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# A model analysis of centimeter-long electron transport in cable bacteria†

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The recent discovery of cable bacteria has greatly expanded the known length scale of biological electron transport, as these multi-cellular bacteria are capable of mediating electrical currents across centimeter-scale distances. To enable such long-range conduction, cable bacteria embed a network of regularly spaced, parallel protein fibers in their cell envelope. These fibers exhibit extraordinary electrical properties for a biological material, including an electrical conductivity that can exceed  $100 \text{ S cm}^{-1}$ . Traditionally, long-range electron transport through proteins is described as a multi-step hopping process, in which the individual hopping steps are described by Marcus electron transport theory. Here, we investigate to what extent such a classical hopping model can explain the conductance data recorded for individual cable bacterium filaments. To this end, the conductive fiber network in cable bacteria is modelled as a set of parallel one-dimensional hopping chains. Comparison of model simulated and experimental current(*I*)/voltage(*V*) curves, reveals that the charge transport is field-driven rather than concentration-driven, and there is no significant injection barrier between electrodes and filaments. However, the observed high conductivity levels ( $>100 \text{ S cm}^{-1}$ ) can only be reproduced, if we include much longer hopping distances ( $a > 10 \text{ nm}$ ) and lower reorganisation energies ( $\lambda < 0.2 \text{ eV}$ ) than conventionally used in electron relay models of protein structures. Overall, our model analysis suggests that the conduction mechanism in cable bacteria is markedly distinct from other known forms of long-range biological electron transport, such as in multi-heme cytochromes.

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## 1 Introduction

Electron flow through proteins is central to the functioning of living organisms, as it connects the sites where oxidation and reduction half-reactions occur that support vital biochemical processes.<sup>1</sup> The best studied systems in terms of biological electron transport are the membrane complexes that enable photosynthesis in chloroplasts or respiration in mitochondria.<sup>2,3</sup> These protein structures incorporate a series of non-protein cofactors (*e.g.*, hemes, FeS clusters) that act as relay centres for electron transport. Electrons migrate through the electrically insulating protein medium by quantum-mechanical tunneling from one center to the next. As the tunneling rate exponentially decreases with distance, cofactors must be closely spaced ( $<1.4 \text{ nm}$  apart) to allow for sufficiently

fast rates ( $>10^3 \text{ s}^{-1}$  time scale) that can sustain metabolism.<sup>3</sup> Typically, electron transport chains incorporate up to 10–20 cofactors, and so the overall length scale of conduction is limited to  $<20 \text{ nm}$ . This has fueled the idea that biological electron transport takes place at the nanometer scale, and so, any electron current exceeding  $3 \text{ nm}$  in biology is generally referred to as “long-range electron transport”.<sup>2</sup>

The recent discovery that cable bacteria can channel electrical currents across centimeter distances,<sup>4</sup> *i.e.*  $10^6$  times further, thus gives a radically new meaning to the concept of “long-range electron transport”.<sup>5</sup> Cable bacteria are long, motile, filamentous bacteria that thrive in the surface sediments of rivers, lakes, and oceans.<sup>6–9</sup> Their respiratory metabolism couples the oxidation of free sulfide ( $\text{H}_2\text{S}$ ) to the reduction of oxygen ( $\text{O}_2$ ), which is an energetically favorable reaction.<sup>10,11</sup> The remarkable feature is that these two half-reactions are carried out by different parts of the long filaments, and so the sites of oxidation and reduction can be millimetres to centimetres apart.<sup>4</sup> To ensure that the redox half-reactions remain electrically coupled, electrons are internally conveyed through the cable bacterium filaments.<sup>12–14</sup>

To mediate this centimeter-scale electron transport, cable bacteria harbor an electrical grid consisting of thin protein

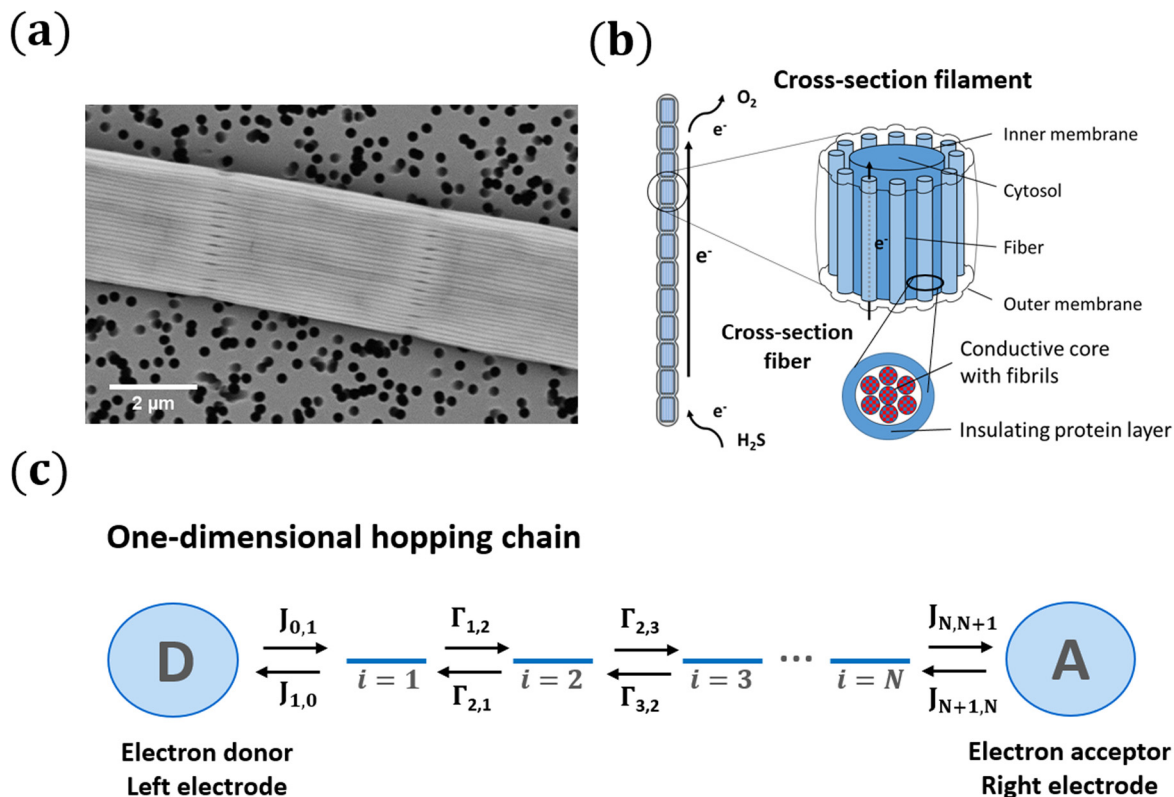
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**Fig. 1** Conduction in cable bacteria is modelled as a set of parallel one-dimensional hopping chains (a) Scanning electron microscope image of a cable bacteria filament. The outer surface shows a set of parallel ridges, each embedding a conductive fibre. (b) Schematic of the conductive structure of cable bacteria based on recent investigations. A filament consists of a long chain of cells. Electrons are uploaded through  $\text{H}_2\text{S}$  oxidation, transported along the filament, and downloaded via  $\text{O}_2$  reduction. The cell envelope incorporates a set of conductive fibres, with diameter  $d_f$ , that consist of thinner fibrils, with diameter  $d_c$ , which each act as a single independent conduction path. (c) A single conduction path is schematically represented as a linear chain of hopping sites (blue stripes). Between two adjacent sites ( $i, i+1$ ), there is a forward transition rate,  $\Gamma_{i,i+1}$ , and a backward transition rate,  $\Gamma_{i+1,i}$ . At the terminal ends, electron exchange occurs with electrodes or donor/acceptor molecules, formally represented by the sites  $i=0$  and  $i=N+1$ .

fibers embedded in the cell envelope<sup>13</sup> (Fig. 1a). Recent studies have resolved the intricate architecture of this highly organized fiber network<sup>15–17</sup> (see Fig. 1b and discussion below). Additionally, it has been shown that these protein fibers display extraordinary electrical properties for a biological material. Electrical measurements demonstrate that the fiber conductivity can reach up to  $100 \text{ S cm}^{-1}$ , which is comparable to that of highly doped conductive polymers.<sup>13,18</sup> Because of this, the protein fibers are regarded as a promising new material for bio-based electronics.<sup>13</sup> Such technological application however necessitates the resolution of some fundamental questions. What mechanism allows for such highly efficient centimeter-scale conduction in proteins? Does the electron transport in cable bacteria bear any similarity to the mechanisms seen in the well-studied protein systems of photosynthesis and respiration?

At present, the molecular structure of the fiber network remains unresolved, and as a result, the conduction mechanism remains elusive. Model analysis, however, allows us to explore potential mechanisms. Nanoscale electron transport across proteins, as seen in multi-heme cytochromes, is conventionally described by the multistep hopping formalism.<sup>19</sup> Here, we investigate whether this same model formalism can

describe the highly efficient, centimeter-scale electron transport in cable bacteria. In the multi-hopping picture, it is assumed that charges are temporarily localized at particular sites, and that electron transport occurs by incoherent “hopping” between consecutive sites along a chain. The electron transfer during a single hop is described by Marcus theory, which requires that the reorganization energy,  $\lambda$ , is significantly larger than electronic coupling,  $H$ , so that localized charge carriers form in the initial and final states.<sup>20</sup> These Marcus-type hopping models comprise the default modelling approach for biological conduction, and have been used previously to describe nanometer scale electron transport in multi-heme cytochromes<sup>21</sup> and protein-based molecular junctions,<sup>22–24</sup> as well as micrometer scale electron transport in the nanowires of metal-reducing bacteria.<sup>25–27</sup>

The distance over which electron transport occurs in cable bacteria is however very different from the length scale for which the Marcus multi-stepping model has been originally developed. To test the validity of the Marcus formalism, we describe the conductive fiber network in cable bacteria as a set of parallel one-dimensional hopping chains. This is the most parsimonious model description, given that the molecular structure of the fibers still remains unresolved. The model



describes the electron transport through the hopping chains when a voltage bias is imposed by connecting electrodes (Fig. 1). In our analysis, we simulate the site occupancy along the chain as well as the resulting current/voltage response, and investigate the relationship between the hopping rate and the electrical conductivity. The model output is compared to an experimental dataset that was recently obtained by detailed electrical characterization of individual fiber networks of cable bacteria.<sup>28</sup>

## 2 Model framework

### 2.1 The conductive structure in cable bacteria

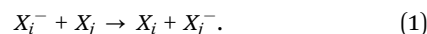
Cable bacteria possess a set of  $N_F$  fibre structures in their cell envelope, which are arranged in parallel and run continuously along the whole length of the centimeter-long cable bacterium filaments (Fig. 1a and b). These fibres consist of a conductive core (diameter  $d_F = 26$  nm), surrounded by an electrically insulating shell,<sup>17</sup> and always appear to have a similar geometry.<sup>15</sup> Thicker cable bacteria simply embed more parallel fibers in the cell envelope ( $N_F$  ranges from 15 to 75<sup>15</sup>). Here, we adopt  $N_F = 60$  as a reference value, which is a characteristic value for *Electrothrix gigas*, the larger strain of cable bacteria<sup>29</sup> that was used in our electrical characterization experiments.

The large ratio of the fiber length ( $10^7$  nm) to the fiber diameter (26 nm) suggests that charge transport in the fibers is largely one-dimensional. Still, the fiber core diameter is considerably larger than the typical spacing between charge carrier sites in metalloproteins<sup>3</sup> ( $\approx 1$  nm). Hence, there could be multiple conduction channels acting in parallel in a single fiber. Here, we assume that each conductive fiber core consists of  $N_C$  parallel conduction paths, each  $d_C = 2$  nm in diameter (Fig. 1b). Assuming a hexagonal packing of cylinders, this implies that each fiber embeds  $N_C = 125$  parallel conduction channels. This large number of conduction channels can be regarded as an upper limit, thus providing a conservative estimate for the conductivity estimated by the model. If less channels are present, then the conductivity of individual channels must be higher. We disregard electron transport between channels, and so the total electrical current through a single bacterial filament is due to electron transport in  $N_P = N_F \cdot N_C = 7500$  parallel one-dimensional conduction channels (see Table 1).

### 2.2 Electron flow in a one-dimensional hopping chain

Each conduction channel is described as a one-dimensional chain of charge carrier sites that spans a length  $L$ . From a

biological perspective, a charge carrier site can be interpreted as a electron-carrying cofactor embedded in a non-conductive protein matrix. Electrons are assumed to be solely transported by hopping, *i.e.*, sequential tunneling through the protein matrix from one cofactor to the next. A site can be in two states: uncharged (carrying no electron;  $X_i$ ) or charged (carrying an electron;  $X_i^-$ ). The resulting electron transfer can be represented by a biomolecular self-exchange reaction between electron carriers



Between any pair of charge carrier sites  $ij$ , the forward transition rate is denoted by  $\Gamma_{ij}$  and the reverse rate is given by  $\Gamma_{ji}$  (Fig. 1c). To keep the analysis tractable, we assume that these transfer rates are only dependent on the present state of the protein complex, and not on past states (Markov assumption). The hopping transitions at different locations are also assumed to be uncorrelated.<sup>30</sup>

When the energies of the departure and destination sites differ ( $U_i \neq U_j$ ), energy must be exchanged with the environment during the electron transfer from  $i$  to  $j$  to ensure energy conservation. If this energy is dissipated to an environment at constant temperature  $T$  (heat bath), the ratio of the transition rates must follow the detailed balance relation:<sup>31,32</sup>

$$\frac{\Gamma_{ij}}{\Gamma_{ji}} = \exp\left(-\frac{U_j - U_i}{k_B T}\right), \quad (2)$$

where  $k_B$  is Boltzmann's constant. The electron flow (*i.e.*, number of electrons transported per unit time) between two sites is given by:

$$J_{ij} = \Gamma_{ij} p_i (1 - p_j). \quad (3)$$

Here,  $p_i$  is the site occupancy. An electron can only jump to a site when it is vacant (Pauli exclusion principle without electron spin). The transition rate is hence weighted by the probability that the starting site is occupied,  $p_i$ , and that the destination site is empty,  $(1 - p_j)$ . The dynamics of the site occupancy is governed by the combined effect of all electron currents that arrive at or leave a given site:

$$\frac{dp_i}{dt} = \sum_j (J_{ji} - J_{ij}). \quad (4)$$

The net electrical current that passes through the chain segment between sites  $i$  and  $i + 1$  becomes:

$$I_{i,i+1} = e \sum_{m=1,\dots,i} p_m \sum_{n=i+1,\dots,N} \Gamma_{m,n} (1 - p_n) - e \sum_{m=i+1,\dots,i} p_m \sum_{n=1,\dots,i} \Gamma_{m,n} (1 - p_n). \quad (5)$$

The quantity  $e = 1.6 \times 10^{-19}$  C is the elementary charge. The first term represents the electrons travelling to the right (*i.e.* the forward currents passing site  $i$ ), while the second term represents the electrons travelling to the left (*i.e.* the backward currents passing site  $i + 1$ ). Our interest is in the steady state situation, where no charge builds up in the hopping chain, and

Table 1 Parameterization of the conductive network in cable bacteria

Parameter	Symbol	Units	Value
Fibre diameter	$d_F$	nm	26
Number of fibres	$N_F$	—	60
Conduction channel diameter	$d_C$	nm	2
Number of conduction channels per fibre	$N_C$	—	125
Total number of parallel conduction channels	$N_P$	—	7500



so the net electron flow from/to a particular hopping site must be zero ( $dp_i/dt = 0$ ). In the steady state, the current must be the same across all segments the chain ( $I_{i,i+1} = I$ ).

### 2.3 Nearest neighbour hopping

Electron tunneling in protein structures is known to have a strong exponential dependence on distance.<sup>33–36</sup> Therefore, the chance that an electron hops to a remote site in the chain is improbable. We can implement this by only allowing transitions between adjacent sites, *i.e.*, nearest neighbour hopping. Moreover, when the protein structure that forms the conduction channel is highly regular, all charge carriers will be identical, and the interdistance and site energy (without an imposed electrical field) will show little variation. As a result, the transition rates between neighbouring sites will be identical throughout the whole chain ( $\Gamma_{i,i+1} = \Gamma_R$  and  $\Gamma_{i+1,i} = \Gamma_L$ ). Assuming nearest neighbour hopping in a regular chain with identical sites, the net chain current (eqn (5)) simplifies to:

$$I = e\Gamma_R p_i(1 - p_{i+1}) - e\Gamma_L p_{i+1}(1 - p_i). \quad (6)$$

Similarly, the site occupancy balance reduces to

$$\begin{aligned} \frac{dp_i}{dt} = & \Gamma_R p_{i-1}(1 - p_i) - \Gamma_L p_i(1 - p_{i-1}) \\ & + \Gamma_R p_i(1 - p_{i+1}) - \Gamma_L p_{i+1}(1 - p_i). \end{aligned} \quad (7)$$

When the hopping chain is very long, as is the case for cable bacteria, we can describe the occupancy profile as a continuous function of the position along the chain,  $p_{i\pm 1} = p(x_i \pm a)$ , where  $x_i$  is the center position of site  $i$ , and  $a$  is the center-to-center distance between sites. The total number of sites in the chain hence amounts to  $N = L/a$ . Expansion to second order,

$$p(x_i \pm a) = p(x_i) \pm a \left[ \frac{dp}{dx} \right]_{x_i} + \frac{a^2}{2} \left[ \frac{d^2p}{dx^2} \right]_{x_i}, \quad (8)$$

and substitution into the site occupancy balance (eqn (7)), leads to the differential equation:

$$\frac{d^2p}{dx^2} + \frac{2}{a} \tanh\left(\frac{\Delta}{2k_B T}\right) (2p - 1) \frac{dp}{dx} = 0. \quad (9)$$

Here,  $\Delta = U_i - U_{i+1} = eV(1 - \alpha)/N$  represents the difference in site energy between two sites ( $\alpha = \alpha_L + \alpha_R$  specifies the total voltage drop at the electrodes; see Fig. 2 and below). In a similar fashion, the normalized chain current can be written as (see ESI†):

$$\begin{aligned} \frac{I}{e\Gamma_R} = & \left( 1 - \exp\left(\frac{-\Delta}{k_B T}\right) \right) p(x)(1 - p(x)) \\ & - a \frac{dp}{dx} \left( p(x) + \exp\left(\frac{-\Delta}{k_B T}\right) (1 - p(x)) \right). \end{aligned} \quad (10)$$

For a given temperature  $T$ , site spacing  $a$  and site energy difference  $\Delta$ , the site occupancy profile  $p(x)$  along the chain can be calculated from eqn (9), and then implemented into eqn (10) to provide the current.

### 2.4 Charge transfer to and from the chain

The site occupancy equation (eqn (9)), which governs the electron transport within the hopping chain, requires suitable boundary conditions. For this, we need to consider how electrons are either injected or ejected from the chain at the left and right boundaries. Two different situations can be considered: the metabolic operation of cable bacteria under *in vivo* conditions (in which electrons are supplied and removed through redox half-reactions; Fig. S2 in the ESI†), and the situation under which cable bacteria are electrically investigated in the laboratory (in which electrons are exchanged with electrodes; Fig. 2). The latter will be the focus of our analysis here, as it represents the situation under which the conductance data are collected.

In the laboratory, the conductance of cable bacteria is studied by connecting individual filaments to metal electrodes.<sup>13,18,28</sup> A bias voltage,  $V$ , is applied to the two terminal electrode contacts, and the electrical current,  $I$ , that flows through the cable bacterium segment is recorded (operation of the electrode set-up is illustrated in Fig. 2a). If charge injection from the electrode is non-limiting ( $J \gg \Gamma_{R,L}$ ; see Fig. S3 and additional derivations in ESI†), the occupation probability at the edges reads:

$$\begin{aligned} p_{L,R} = & \frac{1}{\exp\left(\frac{U_{L,R} - \mu_{L,R}}{k_B T}\right) + 1} \\ = & \frac{1}{\exp\left(\frac{U_0 \pm \alpha_{L,R} eV}{k_B T}\right) + 1}. \end{aligned} \quad (11)$$

In this expression,  $U_{L,R}$  is the site energy of the start  $x = 0$  and end  $x = L$  of the hopping chain and  $\mu_{L,R}$  is the chemical potential of the left/right electrode (Fig. 2b). The site energy at the terminal ends is given by  $U_{L,R} = \mu_{L,R} + U_0 \pm \alpha_{L,R} eV$ . In this approximation, the edge occupancies,  $p_{L,R}$ , follow the Fermi-Dirac distribution of the corresponding electrodes. In the general case, an injection barrier,  $U_0$ , is present (difference between Fermi level of the electrodes and the site energy in the hopping chain), and voltage drops ( $\alpha_L$ ,  $\alpha_R$ ) may occur at the interface between filaments and electrodes (see details in Fig. 2).

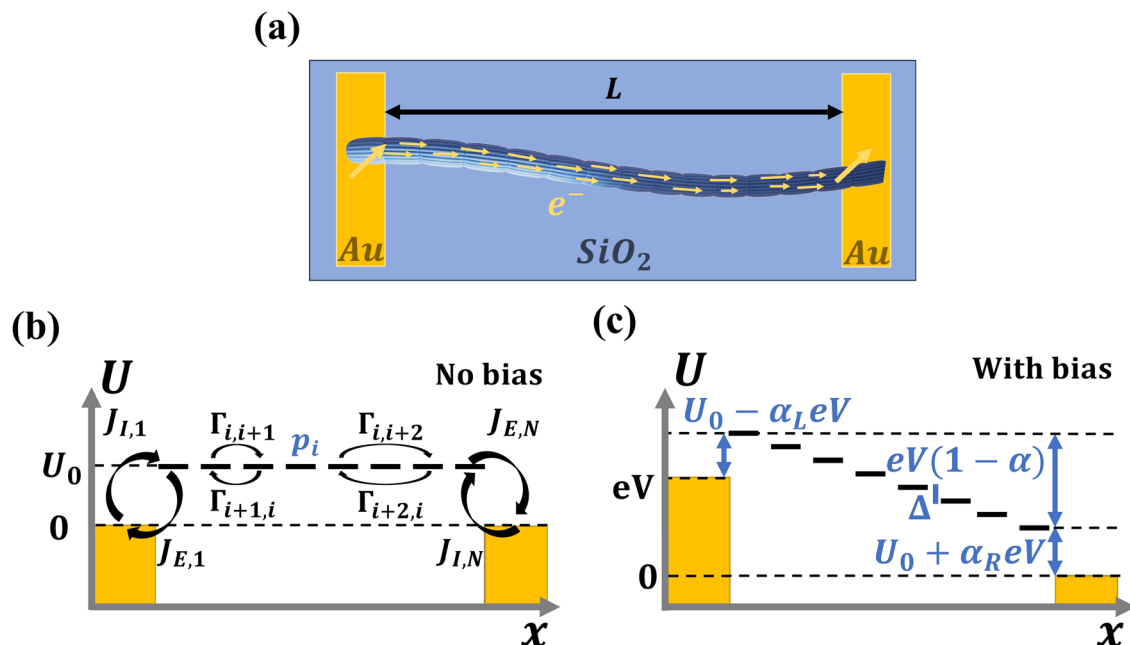
### 2.5 Marcus hopping rate

Semi-classical Marcus theory provides the following expression for the electron transfer rate between two sites in the hopping chain:<sup>20</sup>

$$\Gamma_R = \frac{2\pi}{\hbar} \frac{H^2}{\sqrt{4\pi\lambda k_B T}} \exp\left(-\frac{(\lambda - \Delta)^2}{4\lambda k_B T}\right). \quad (12)$$

Here,  $H$  represents the electronic coupling between the initial and final states, and  $\lambda$  is the reorganisation energy. The Marcus expression only holds for the case of weak electronic coupling, *i.e.*, when  $H \ll \lambda$ .<sup>20,37,38</sup> When the driving force is small compared to the reorganization energy ( $\Delta \ll \lambda$ ), the approximation  $(\lambda - \Delta)^2 \sim \lambda(\lambda - 2\Delta)$  holds, and the Marcus





**Fig. 2** Electrical investigation of cable bacteria filaments between electrodes. (a) Schematic of the electrical characterization approach. A filament is deposited onto insulating silicon dioxide ( $\text{SiO}_2$ ) substrate and connected to two gold (Au) electrodes with a gap length  $L$ . Electrons flow from one side to the other, through the conductive fiber network of the filament. (b) Site energy vs. position along the hopping chain for the case without any voltage bias. Transfer rates between hopping sites are denoted  $\Gamma$ , and injection/ejection rates from electrodes  $J$ . Electron states in the metal electrode (dark yellow) are filled up until the chemical potential, chosen as  $\mu = 0$ . Site energies are equal to the injection barrier ( $U_i = U_0$ ). (c) Site energy vs. position for an electrode bias  $V$ . The left electrode is at chemical potential  $\mu_L = eV$ , and the right electrode at  $\mu_R = 0$ . An electron loses an energy  $\alpha_L eV$  at the biased electrode and  $\alpha_R eV$  at the grounded electrode, while the rest of the energy is lost in the hopping chain ( $eV(1 - \alpha)$  with  $\alpha = \alpha_L + \alpha_R$ ). As long as the voltage drops linearly inside the hopping chain, there is a constant voltage drop between adjacent hopping sites,  $\Delta = eV(1 - \alpha)/N$ . The injection barrier at the left electrode is  $U_0 - \alpha_L eV$ , and the other side, it is  $U_0 + \alpha_R eV$ .

rate can be written as:

$$\Gamma_R = \Gamma_R^0 \exp\left(\frac{\Delta}{2k_B T}\right). \quad (13)$$

The prefactor  $\Gamma_R^0$  represents the unbiased Marcus rate at a given temperature (eqn (12) with  $\Delta = 0$ ). If the electronic coupling  $H$  is only weakly dependent on the driving force, this prefactor can be considered to be independent of the applied voltage bias.

## 2.6 Numerical approach

The solution of the occupancy balance equation (eqn (4)) with suitable boundary conditions (eqn (11)) fully describes the electron transport through the hopping chain. To solve this differential equation, we implemented a numerical solution procedure (see ESI†) that calculates the site occupancy profile,  $p(x)$ , as a function of the position along the chain  $x$  and the applied bias voltage  $V$ . Subsequently the normalized chain current  $I/(e\Gamma_R)$  is calculated, and this is then combined with the Marcus expression (eqn (12)) to simulate the full  $I(V)$  curve (see Fig. S1, ESI†). We also derived a set of analytical expressions for the occupancy profile and normalized chain current for the case when there's a symmetric voltage drop at the electrodes ( $\alpha_L = \alpha_R$ ). Expressions are derived for the absence ( $U_0 = 0$ ) or presence ( $U_0 > 0$ ) of an injection barrier. These analytical expressions allow to identify how different end-member transport regimes influence the shape of the  $I/V$  curve.

The details of the derivations are given in the ESI† and the resulting expressions are summarized in Tables S1 and S2.

## 3 Results

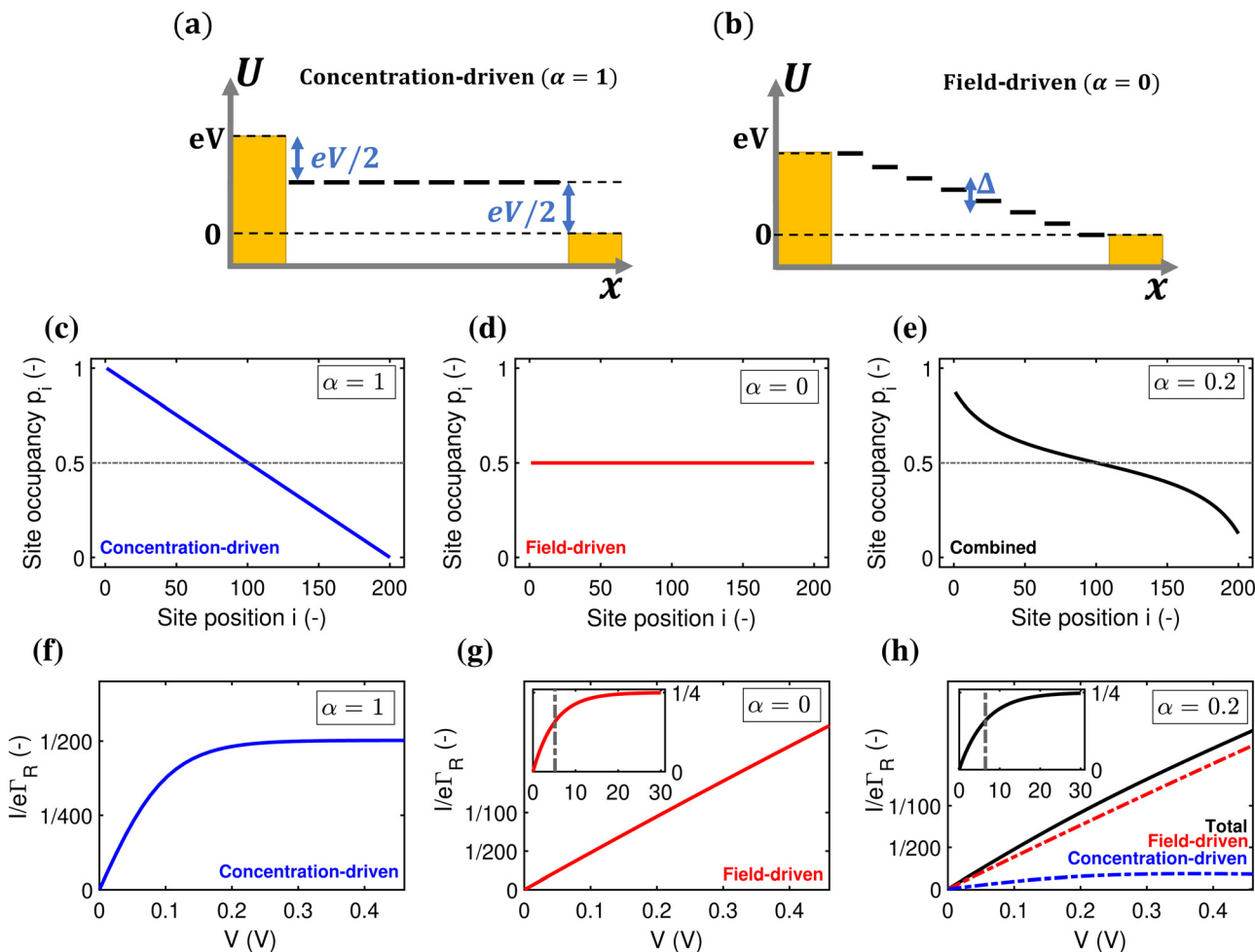
The mapping of the electrical current,  $I$ , as a function of the applied bias voltage,  $V$ , forms a key analysis in the electrical characterisation of materials. As a baseline and reference situation, we simulated a hopping chain with following parameters:  $N = 200$ , transport is predominantly field-driven ( $\alpha = 0.2$ ), resides in the resonant regime ( $U_0 = 0$ ), and has a reorganisation energy,  $\lambda = 200$  meV, and electronic coupling,  $H = 16$  meV. Subsequently, we systematically varied each parameter individually to verify its impact on the  $I(V)$  curve. We also compared the output of the model simulations to an extensive experimental dataset, consisting of  $I(V)$  curves collected at different temperatures ( $T = 80\text{--}300$  K) for cable bacterium filaments of different length. The data collection procedure is presented in detail elsewhere.<sup>28</sup> Fig. 5 displays relevant  $I(V)$  curves for three segments of different length ( $L = 4, 40, 300$   $\mu\text{m}$ ).

### 3.1 Concentration-driven versus field-driven regime

A first question is whether the electron transport in cable bacteria is concentration-driven or field-driven. These regimes correspond to two limiting cases for the







**Fig. 3** Concentration-driven versus field-driven electron transport. (a) and (b) Energy vs. position diagram in the concentration-driven end-member ( $\alpha = 1$ ) and field-driven end-member ( $\alpha = 0$ ). (c) Site occupancy,  $p_i$  vs. site position,  $i$ , in the concentration-driven limit ( $\alpha = 1$ ). (d) Site occupancy,  $p_i$  vs. site position,  $i$ , in the field-driven limit ( $\alpha = 0$ ). (e) Site occupancy,  $p_i$  vs. site position,  $i$ , in the combined scenario ( $\alpha = 0.2$ ). (f) Normalized chain current,  $I/(e\Gamma_R)$  as a function of the applied voltage,  $V$ , in the concentration-driven limit ( $\alpha = 1$ ). (g). Same graph in the field-driven limit ( $\alpha = 0$ ). The inset shows higher-voltage regime, with a vertical line plotted at  $eV = Nk_B T$ . (h). Same in the combined scenario ( $\alpha = 0.2$ ), with the field- and concentration-driven terms (red and blue respectively). The inset shows higher-voltage regime, with a vertical line plotted at  $eV(1 - \alpha) = Nk_B T$ .

behaviour of the electrical field at the electrode interfaces (see Fig. 3); either the applied voltage completely drops over the electrode interfaces ( $\alpha = 1$ ), or there is no voltage drop at the electrodes ( $\alpha = 0$ ). In our simulations, we assume that the voltage drop is similar at both electrodes ( $\alpha_L = \alpha_R = \alpha/2$ ).

When the current is exclusively concentration-driven, the entire voltage drop occurs at the interface of the electrodes ( $\alpha = 1$ , Fig. 3a), and there is no electric field or electric potential gradient present in the hopping chain ( $\Delta = 0$ ). As a result, all sites reside at the same site energy, and the detailed balance relation (eqn (2)) implies that the forward and backward transition rates must be equal. In this regime, the electron transport is purely “diffusive”, *i.e.*, driven by the difference in site occupation probability along the chain. The differential equation describing the occupancy profile (eqn (9)), becomes the stationary

diffusion equation and has a linear solution (Fig. 3c):

$$p(x) = p_L - (p_L - p_R) \frac{x}{L}, \quad (14)$$

with  $p_L = p(x = 0)$  and  $p_R = p(x = L)$ . The normalized chain current shows an hyperbolic tangent dependence on the applied voltage (Fig. 3f, derivation in ESI†):

$$\frac{I}{e\Gamma_R} = \frac{1}{N} \tanh\left(\frac{eV}{4k_B T}\right). \quad (15)$$

Because there is no electric field within the hopping chain ( $\Delta = 0$ ), the transition rate matches the unbiased Marcus rate ( $\Gamma_R = \Gamma_R^0$ ), and so the  $I/V$  curve attains the form:

$$I = N p \frac{e\Gamma_R^0}{N} \tanh\left(\frac{eV}{4k_B T}\right). \quad (16)$$

The current starts out linearly ( $I \propto V$ ), and saturates



around  $eV \approx 4k_B T$ , as the occupancy gradient approaches its maximum ( $p_L = 1$ ;  $p_R = 0$ ). At room temperature, this saturation should occur around  $V = 0.1$  V. The experimental  $I(V)$  curves (Fig. 5a–c), however, do not show this saturation effect. When the bias voltage is increased beyond 0.1, the  $I(V)$  curve still remains linear. Therefore, the electron transport in fiber network of cable bacteria does not appear to be concentration-driven.

Oppositely, when the current is exclusively field-driven ( $\alpha = 0$ , Fig. 3b), the site occupancy does not show a gradient ( $p_i = 1/2$ , Fig. 3d). In this field-driven scenario, electron transport is solely “drift” based, *i.e.*, it is driven by the difference in the forward and backward transition rates. The normalized chain current becomes (Fig. 3g, derivation in ESI†):

$$\frac{I}{e\Gamma_R} = \frac{1}{4} \left[ 1 - \exp\left(\frac{-eV}{Nk_B T}\right) \right]. \quad (17)$$

This relation predicts that the normalized chain current becomes constant ( $I/(e\Gamma_R) = 1/4$ ), when the applied voltage becomes sufficiently high, *i.e.*, when  $eV/N > k_B T$  (inset in Fig. 3g). Yet, when the chain includes many hopping sites, this transition voltage  $V = Nk_B T/e$  is very large. For example, for a long cable bacterium segment ( $\sim 2$  mm) and a short hopping distance ( $\sim 1$  nm), the number of hopping sites becomes  $N = 2 \times 10^6$ , and so the corresponding transition voltage at room temperature ( $k_B T \approx 25$  meV) equals  $V = 50 \times 10^3$  V. This explains why the transition is not seen in the experimental  $I/V$  data.

When the voltage bias is sufficiently small compared to the reorganization energy ( $eV/N < \lambda$ ), we can use the Marcus rate expression, eqn (13), and so the  $I/V$  curve attains the form:

$$I = N_P \frac{e\Gamma_R^0}{2} \sinh\left(\frac{eV}{2Nk_B T}\right) \approx N_P \frac{e\Gamma_R^0}{4} \frac{eV}{Nk_B T}. \quad (18)$$

The experimentally recorded  $I(V)$  curves closely fit the temperature-dependent response that is predicted by the above relation (Fig. 5d–f). When the temperature is high and the bias is sufficiently small, *i.e.*, when  $eV/N < k_B T$ , the approximation in eqn (18) is valid and the  $I/V$  becomes linear. Such linear  $I/V$  curves are indeed observed near room temperature. Moreover, when the temperature is lowered, the experimental  $I/V$  curves become more non-linear and adopt a hyperbolic sinus shape, as predicted by eqn (18). This hence suggests that conduction in cable bacteria is field-driven.

When  $\alpha = 0.2$ , the site occupancy profile adopts a non-linear shape, which lies in between the linear concentration-driven and flat field-driven profile (Fig. 3e). Likewise, it can be shown that the resulting  $I(V)$  curve can be decomposed into the sum of a field-driven and a concentration-driven contribution (Fig. 3h; see derivation in ESI†). At higher voltages, the field-driven current becomes dominant (Fig. S5, ESI†).

### 3.2 Resonant versus off-resonant transport

A second question is whether the electron transport in the conductive fibers of cable bacteria is affected by an injection barrier,  $U_0$ , or not. When the charge transport is not hampered

by the barrier, it resides in the resonant regime. Oppositely, when the injection barrier is slowing down the transport, it is off-resonant. Fig. 4 shows the transition from the off-resonant to resonant transport regime for the reference parameters, but with  $U_0 = 0.1$  eV instead of zero. Analytical expressions can be derived for the occupancy profile and the normalized chain current (see ESI†). For low bias voltages, transport is off-resonant ( $\alpha_L eV < U_0$ ), and the site occupancy stays low throughout the chain (Fig. 4a). As the bias voltage increases, the conduction enters the resonant regime when  $\alpha_L eV = U_0$  and the occupancy profile evolves towards a static tangent-shaped profile (Fig. 4a, similar to that displayed in Fig. 3e). The normalized  $I(V)$  curve shows the transition from off-resonant to resonant transport, which occurs at  $V = U_0/(e\alpha_L)$  (Fig. 4b). At low bias, in the off-resonant regime, the normalized chain current is non-linear, while in the resonant regime, the current increases linearly with the applied voltage bias.

In the off-resonant regime, the temperature has a large effect on the site occupancy profile, and induces an overall decrease of the site occupancy upon cooling. In contrast, in the resonant regime, the occupancy profile is only marginally influenced by the temperature (Fig. 4c). Overall, the full  $I(V)$  curves show the same strong non-linear shape as the normalized  $I(V)$  (Fig. 4d). The experimental  $I(V)$  curves do not display this strong non-linearity (Fig. 5). This indicates that there is no significant injection barrier present, when the cable bacterium filaments are interfaced to gold electrodes.

### 3.3 Length dependence of the $I(V)$ curve

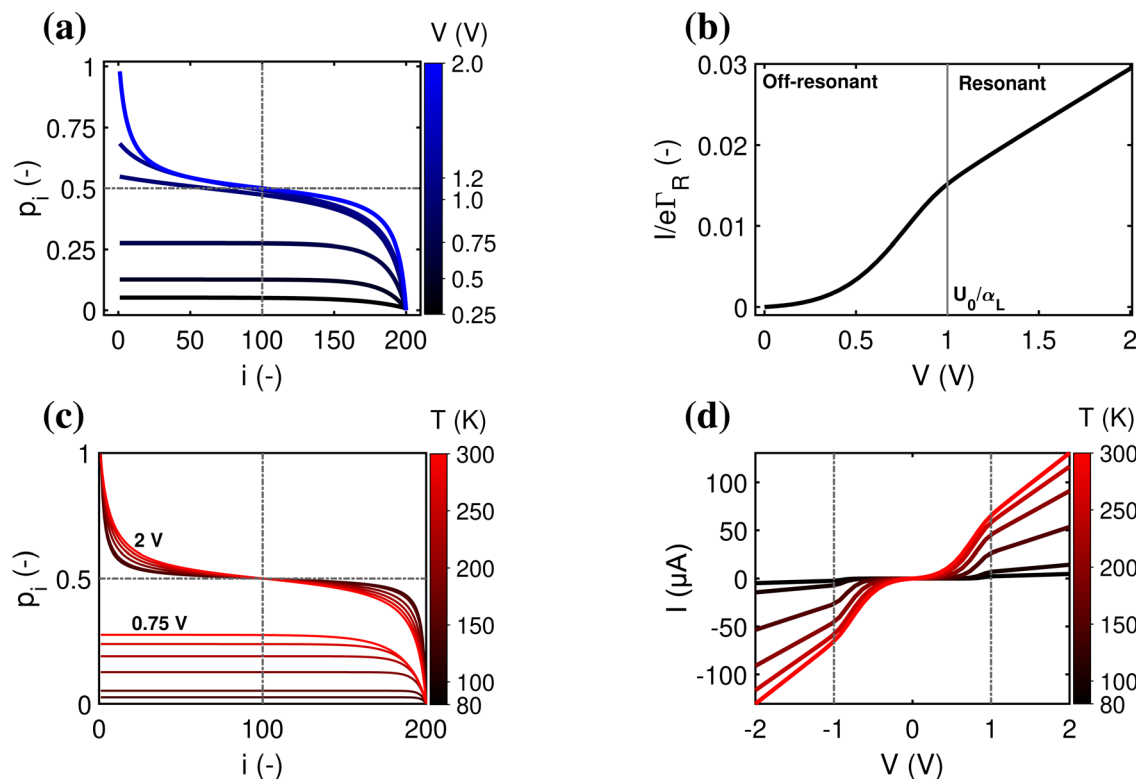
A third aspect relates to the impact of the hopping chain length on the  $I(V)$  curve. As clearly seen in the experimental data (Fig. 5a–c), the shape of the  $I(V)$  curve becomes more linear as the length of the investigated segment increases. This phenomenon is well represented by eqn (18), which predicts that the  $I(V)$  curve becomes more linear as the number of sites  $N$  increases (simulated  $I/V$  curves are displayed in Fig. 5d–f). The explanation is rather straight forward: as the number of sites  $N$  decreases, the site energy difference  $\Delta = eV/N$  increases at a given fixed voltage. When  $\Delta$  increases, the expression for the normalized current (eqn (17)) becomes non-linear, while also the Marcus rate (eqn (13)) adds to the non-linearity. As a result, the full  $I(V)$  curve becomes increasingly hyperbolic, when the temperature decreases and/or the segment length decreases (Fig. 5).

### 3.4 Conductivity

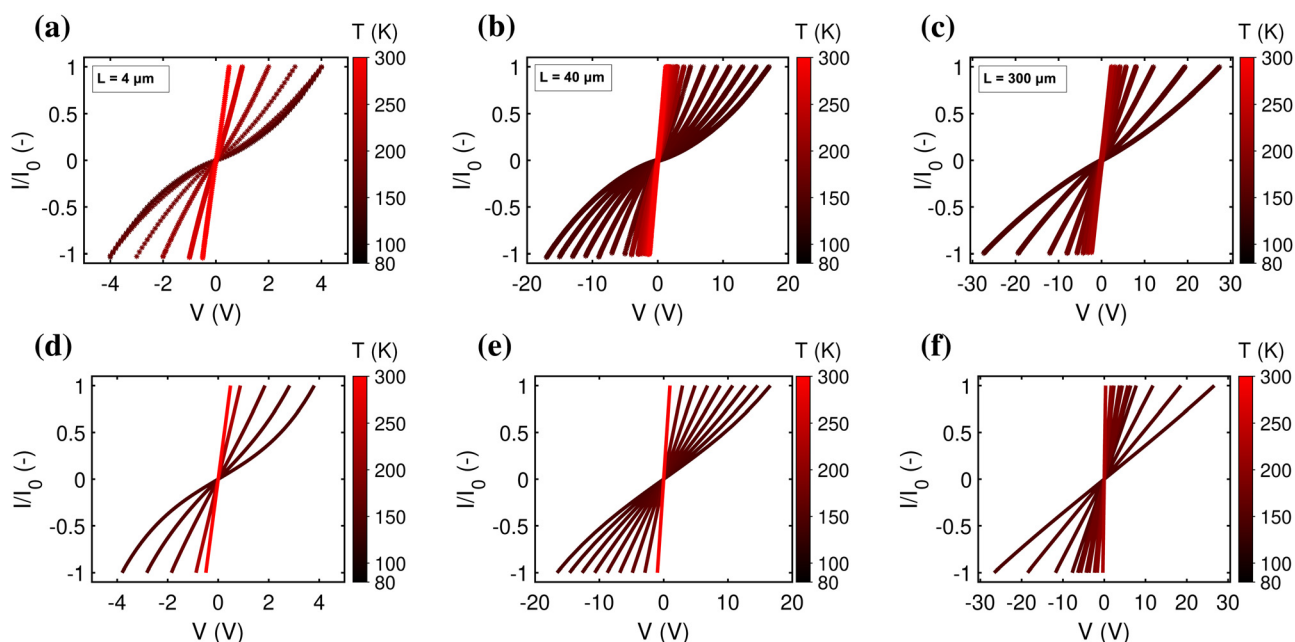
Overall, the multistep hopping model appears to adequately simulate the experimental  $I(V)$  curves, in the field-driven regime with no significant injection barrier. Therefore, a prominent question is whether the model can also reproduce the conductivity of the cable bacteria fibers, which is extremely high for a biological system (reaching up to  $>100$  S cm $^{-1}$  at room temperature). To this end, we now investigate the relationship between the hopping rate and the electrical conductivity.

Assuming a suitably long chain (such that the low-bias limit  $eV/N \ll k_B T$  holds), and adopting field-driven transport ( $\alpha = 0$ )





**Fig. 4** Resonant and off-resonant electron transport in a hopping with an injection barrier. Model parameters are:  $N = 200$ ,  $U_0 = 0.1$  eV,  $\alpha = 0.2$ ,  $T = 300$  K. (a) Simulated occupancy profile for six different voltages (as indicated by numbers next to the colour bar). The dashed lines indicate the crossing at  $p_{N/2} = 1/2$ . (b) Normalized chain current,  $I/e\Gamma_R$ , plotted as a function voltage bias,  $V$ . The transition from off-resonant to resonant occurs at  $eV = U_0/\alpha_L = 1$  V. (c) Occupancy profile at two fixed voltages (off-resonant  $V = 0.75$  V and resonant  $V = 2$  V) for six different temperatures (indicated by numbers next to the colour scale). (d) Simulated current–voltage response for six different temperatures, using the Marcus rate (eqn (12)) with parameters  $H = 16$  meV and  $\lambda = 0.2$  eV.



**Fig. 5** Dependence of  $I(V)$  curves on temperature in the range 80–300 K. (a)–(c) Experimental data showing the rescaled current,  $I/I_0$ , as a function of voltage,  $V$ . The current,  $I$ , is rescaled to its maximum value,  $I_0$ , per  $I(V)$ -trace, to illustrate the shape of the curve. The three panels (a)–(c) correspond to three different segment lengths ( $L = 4$   $\mu\text{m}$ ,  $L = 40$   $\mu\text{m}$ , and  $L = 300$   $\mu\text{m}$ ). (d)–(f) Simulated  $I(V)$ 's with  $N = 70$  (d),  $N = 450$  (e) and  $N = 3000$  (f). The other parameters are:  $U_0 = 0$ ,  $\alpha = 0$ ,  $H = 16$  meV and  $\lambda = 0.2$  eV.





and no injection barrier ( $U_0 = 0$ ), we can use eqn (18) to express the conductivity of a fiber of length  $L$  and cross-section  $A$ :

$$\sigma = \frac{I L}{V A} = \frac{e^2 \Gamma_R^0}{4k_B T \pi (d_C/2)^2} \frac{a}{\Gamma_R^0} \quad (19)$$

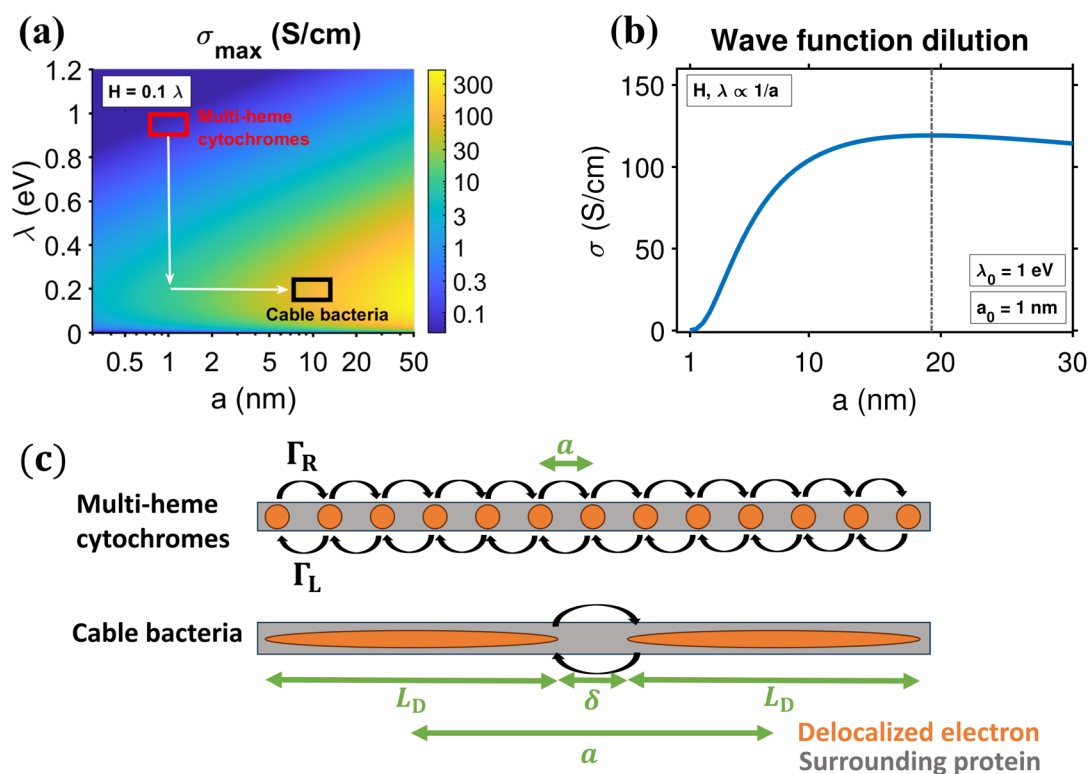
This expression is insightful, because it has the familiar form,  $\sigma = ne\mu$ , with the charge carrier density  $n = 1/(4a\pi(d_C/2)^2)$  and mobility,  $\mu = e\Gamma_R^0 a^2/(k_B T)$ . The factor 1/4 in the charge carrier density  $n$  arises from the occupation factor  $p(1-p)$  with  $p = 1/2$  the site occupancy in the resonant, field-driven regime (Fig. 4).

Eqn (19) provides a direct relation between the hopping rate and the conductivity, and readily illustrates the problem of explaining the high conductance in cable bacteria. If we assume that multistep hopping in cable bacteria occurs over a similar length scale as in multi-heme cytochromes,<sup>21</sup> the center-to-center distance between sites would be  $a \sim 1$  nm. Using this value in eqn (19), the required hopping rate for a conductivity of  $100 \text{ S cm}^{-1}$  becomes  $\Gamma_R \approx 2 \times 10^{13} \text{ s}^{-1}$ . This value exceeds by far the fastest hopping rate reported in literature for a biological protein structure ( $10^9 \text{ s}^{-1}$ ).<sup>39,40</sup> More problematically, it also exceeds the typical relaxation rate of vibrational modes in cofactors,  $\sim 10^{13} \text{ s}^{-1}$ , which is considered as a “speed limit” for hopping conduction.<sup>41</sup> The relaxation

rate of vibrational modes must be higher than the hopping rate itself, so that the electron has time to dissipate energy before hopping onwards (see ESI† ‘Non-adiabatic constraint’ for further detail).

To examine the maximum conductivity that a hopping model for cable bacteria can support, we can evaluate the theoretical limits of the Marcus rate expression eqn (12). Marcus theory requires that the inter-site electronic coupling  $H$  is weak,<sup>20</sup> so that it remains small with respect to the reorganisation energy ( $H \ll \lambda$ ). When  $H \approx \lambda$  or beyond, the electron will no longer be localised on the hopping site.<sup>37,38,42</sup> To quantitatively evaluate the maximum conductivity allowed by the Marcus formalism, we adopt the working assumption that the maximum electronic coupling is  $H_{\text{max}} = 0.1\lambda$  (see ESI† for additional discussion of this ‘weak coupling’ constraint).

As a result, the conductivity in eqn (19) only varies with the reorganisation energy  $\lambda$  and the center-to-center distance  $a$ . The resulting model simulations are shown in Fig. 6a. For parameters representing electron transport through multi-heme cytochromes<sup>21</sup> ( $\lambda = 0.8 \text{ eV}$ ,  $a = 1 \text{ nm}$ ), a hopping rate of  $5 \times 10^{10} \text{ s}^{-1}$  and a conductivity level of  $0.2 \text{ S cm}^{-1}$  form the theoretical maximum within the Marcus framework. Note however that this conductivity limit is based upon an



**Fig. 6** Idealized hopping conductivity and mobility within the one-dimensional hopping chain, using Marcus rates (eqn (12)). (a) Conductivity colour map, under the constraint  $H = 0.1\lambda$ , as a function of reorganisation energy  $\lambda$  and center-to-center distance between hopping sites  $a$ . The red and black square are indicators for the typical reorganisation energy and center-to-center distance in hemes and cable bacteria, respectively (see panel (c)). Directions for increased conductivity compared to cytochromes are drawn in white. (b) Conductivity,  $\sigma$ , as a function of center-to-center hopping distance,  $a$ , for a biological system that improves on heme-to-heme hopping with distance  $a_0 = 1$  nm, reorganisation  $\lambda_0 = 1$  eV and electronic coupling  $H_0 = 0.1\lambda_0 = 100$  meV, by wave function dilution ( $H, \lambda \propto 1/a$ ). (c) Scheme of heme-to-heme transport (red) and the proposed hopping mechanism in cable bacteria (black), with center-to-center distance,  $a$ , between regions in which the electron is unobstructed (orange, zero resistance) with repetitive surrounding protein structure (grey). Electrons hop between repeated structures with hopping rates  $\Gamma_{R,L}$ .



unrealistically high electronic coupling,  $H \approx \lambda/10 = 80$  meV. As known from experimental and theoretical assessments,  $H = 10$  meV is already on the high side for multi-heme cytochromes.<sup>21</sup> Adopting the latter value lowers the maximum allowed conductivity to  $4 \text{ mS cm}^{-1}$  (hopping rate:  $8 \times 10^8 \text{ s}^{-1}$ ).

We conclude that a multi-step hopping model with cytochrome-like parameters cannot explain the conductivities measured in cable bacteria. As illustrated in Fig. 6a, there are two ways to achieve a higher conductivity. A first way is to reduce the reorganisation energy, and effectively, cable bacteria appear to do this. Recent studies<sup>18,28</sup> indicate that the reorganisation energy of conductance in cable bacteria is remarkably low ( $\lambda = 0.2 \text{ eV}$ ), *i.e.*, a factor 4 lower compared to heme-to-heme transport in multi-heme cytochromes.

Still, a reduction of the reorganization energy alone is not enough to explain the high conductivity in cable bacteria. With  $\lambda = 0.2 \text{ eV}$  and  $a = 1 \text{ nm}$ , we can only reach a hopping rate of  $2 \times 10^{12} \text{ s}^{-1}$  and a conductivity level of  $10 \text{ S cm}^{-1}$  (vertical arrow in Fig. 6a). Therefore, a second way is to increase increase conductivity is to increase the center-to-center distance  $a$ , thus lowering the number of hopping steps. To attain a conductivity of  $\sigma = 100 \text{ S cm}^{-1}$  as reported for cable bacterium fibers, we need to increase the hopping distance to  $a \approx 10 \text{ nm}$ , under the constraint  $H_{\text{max}} = 0.1\lambda$  with  $\lambda = 0.2 \text{ eV}$  (horizontal arrow in Fig. 6a). This provides a hopping rate  $2.2 \times 10^{12} \text{ s}^{-1}$ , which is still high, but below the “speed limit” for hopping conduction.<sup>41</sup> For more stringent constraints with lower  $H/\lambda$  ratios, higher  $a$  values are required (see Fig. S10 and additional results in ESI†).

The predicted electron mobility accompanying  $\lambda = 0.2 \text{ eV}$  and  $a = 10 \text{ nm}$  is  $\mu = 80 \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$  (Fig. S10, ESI†). This mobility value is high and similar to that of metals ( $\sim 50 \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$ ). Metals are highly conductive because many electrons contribute to transport ( $n \approx 10^{22} \text{ cm}^{-3}$ ), but their charge carrier mobilities are not exceptionally high, since electrons frequently collide with the crystal lattice. The predicted charge carrier density in the one-dimensional hopping chain model with  $a = 10 \text{ nm}$ , is  $n = 1/(4a\pi(d_c/2)^2) \approx 8 \times 10^{18} \text{ cm}^{-3}$ , which is much lower than for metals, thus explaining why the conductivity in cable bacteria is 4 orders of lower than in metals.

## 4 Discussion and conclusions

We have developed a one-dimensional hopping model to describe the extremely long-range electron transport in the periplasmic fiber network of cable bacteria. When filaments are connected to metal electrodes, we propose that the edge occupation probabilities in the hopping chain can be treated as if they were part of the electrode (see eqn (11)). This allows simplified analytical expressions to be derived for the current-voltage characteristics in the field- and concentration-driven regimes (Tables S1 and S2, ESI†). For more general cases,  $I/V$  curves can be numerically simulated.

The conductive fiber network in cable bacteria has been shown to consist of a metalloprotein that incorporates a nickel

cofactor.<sup>17</sup> Yet, the detailed molecular structure of this cofactor remains unresolved, and consequently, any model of charge transport in cable bacteria remains somehow speculative. Still, the model analysis here allows to exclude certain transport models, while at the same time, it provides guidance for further experimental investigations and theoretical developments.

### 4.1 The shape of the $I/V$ curve

When cable bacterium filaments are connected to electrodes and electrically investigated at room temperature, the resulting  $I/V$  curves are conspicuously linear.<sup>13,18,28</sup> Comparison of our model results to these experimentally recorded  $I/V$  curves, shows that the model adequately reproduces the impact of segment length and temperature on the shape of the  $I/V$  curve, provided that we adopt a field-driven regime with no significant injection barrier (Fig. 5).

The linearity is explained by the fact that the filaments investigated are long, and so the charge transfer involves a large number of charge transfer steps  $N$ . As a result, the driving force  $\Delta = eV/N$  remains small compared to the thermal energy scale ( $\Delta \ll k_B T$  and so eqn (17) becomes valid). Moreover, the driving force also stays well below the reorganization energy ( $\Delta \ll \lambda$ ), implying that the electron transfer rate  $\Gamma_R$  remains largely independent of the applied voltage bias (see eqn (12)). These conditions generate linear  $I/V$  curves near room temperature, which become increasingly non-linear (sinus hyperbolic) for lower temperatures and shorter segments, as seen in the experimental data (Fig. 5). Note that the condition ( $\Delta \ll \lambda$ ) also implies that the charge transport well remains within the normal Marcus regime (and hence does not enter into the inverted regime).

When using gold electrodes, there appears to be no injection barrier involved in the charge transport. This absence of an injection barrier is intriguing, and requires further experimental examination. The work function, which directly influences the barrier, varies among metals (the energy to bring an electron from the electrode to vacuum of the electrode).<sup>43,44</sup> Therefore, it could be that for electrode materials other than gold, there is a sizable injection barrier.

### 4.2 Impact of reorganization on conductivity

Our model analysis demonstrates that a low reorganization energy is key to achieving a high conductivity in cable bacteria (Fig. 6a). Recent studies have shown that the reorganisation energy in cable bacteria is indeed considerably lower than in other conductive protein systems.<sup>18,28</sup> Yet at present, the molecular structure of the conductive fibers in cable bacteria remains largely unresolved, and therefore, it is not understood why the reorganisation energy of cable bacteria is so small. One potential explanation could be delocalization along the electron transport path, as would result from an ordered aggregation or tight stacking of cofactors. Recently, an extension of Marcus theory has been developed that accounts for charge transfer between so-called donor and acceptor “aggregates”, in which the charge is no longer localized on a single cofactor, but delocalized across a cluster of multiple cofactor molecules.<sup>45</sup>



It was shown that such delocalization can substantially reduce the reorganization energy below what is possible with a single donor and a single acceptor. For example, for a donor aggregate with a fully delocalized state of  $N$  identical donors, the reorganisation energy is decreased  $N$ -fold.<sup>45</sup> For example, if we assume that the reorganization energy  $\lambda$  between a single donor and a single acceptor would be similar to that between consecutive hemes in multi-heme cytochromes, the observed 4 times reduction in  $\lambda$  for cable bacteria as compared to multi-heme cytochromes<sup>18,28</sup> then would imply a delocalization of the charge across  $\sim 4$  cofactor molecules. Yet, to verify whether such a delocalization mechanism is truly at play, we need a better insight into the actual identity and structure of the cofactor molecules in cable bacteria.

### 4.3 A tentative model of charge transport in cable bacteria

Our model analysis reveals that the high conductivity recorded in the conductive fibers of cable bacteria ( $>100 \text{ S cm}^{-1}$ ) can only be explained by a Marcus-type hopping model, unless the number of hopping steps is substantially reduced and the center-to-center distance  $a$  becomes very large (Fig. 6a). Clearly, a hopping distance of  $a \approx 10 \text{ nm}$  exceeds by far the known hopping distances in metalloproteins such as multi-heme cytochromes. If electrons are transported by quantum mechanical tunneling, the center-to-center distance  $a$  must be lower than  $1.4 \text{ nm}$  to attain metabolically relevant electron transport rates (see Moser *et al.*<sup>3</sup>). How can such a large value for  $a$  be reached?

A tentative model is depicted in Fig. 6c. The key difference with classical hopping models of biological transport (*e.g.* heme-based electron transport) is the amount of delocalization, as reflected by the size of the charge carrier sites. Instead of being localized on a small cofactor molecule, electrons are delocalized across wide “relay segments” (distance  $L_D \sim 10 \text{ nm}$ ) that are connected through small non-conductive bridges (distance  $\delta$ ). The electron transport through this protein connection is the rate limiting process, and follows a Marcus-type hopping mechanism. In contrast, the electron transport in the delocalized segments is very fast, and needs to have a far higher mobility than the hopping transport. These relay segments could either be large conjugated molecules, as seen in  $\pi$ -conjugated polymers and graphene nanoribbons,<sup>46</sup> or alternatively, they could involve sets of tightly stacked cofactor molecules that induce electron delocalization (the donor and acceptor “aggregates” discussed above).

This model immediately provokes the question of how biology can synthesize such a structure. Clearly, to ensure high charge transport rates, the “relay segments” should be carefully positioned and oriented, which hence requires a precise coordination by ligating proteins. Furthermore, it is known that delocalized regions are particularly sensitive to disorder effects, as impurities and defects will induce Anderson localisation of electrons,<sup>47</sup> and hence reduce the conductivity. Effectively, the latter phenomenon may help explaining the observation that the conductivity in cable bacteria fibers is variable (ranging from  $0.1$  to  $>100 \text{ S cm}^{-1}$ ; see ref. 13). Differences in levels of

defects/impurities may induce variability in conductance between filaments.

### 4.4 Impact of delocalization on conductivity

As detailed above, the conductivity can be increased by lowering the reorganization energy and increasing the center-to-center distance (Fig. 6a). To quantitatively assess the conjoint impact of both factors, we can introduce reference values for the hopping distance ( $a_0 \sim 1 \text{ nm}$ ) and reorganization energy ( $\lambda_0 \sim 1 \text{ eV}$ ) for conventional biological electron transport. We can now increase  $a$  while keeping  $\delta$  constant, thus simulating the process of wave function dilution (Fig. 6c). When  $a$  becomes much larger than  $a_0$ , we can approximate the delocalization length  $L_D \approx a$  and write the reorganisation energy as  $\lambda = \lambda_0(a_0/a)$  and the electronic coupling as  $H = H_0(a_0/a)$ , where  $\lambda_0$  is the original reorganisation energy and  $H_0$  the original electronic coupling. With these constraints, the ratio between  $H$  and  $\lambda$  stays constant, and so the transport remains within the Marcus regime. Moreover, the conductivity can be calculated as a sole function of the center-to-center distance:

$$\sigma(a) \propto a^{-1/2} \exp\left(-\frac{a_0}{a} \frac{\lambda_0}{4k_B T}\right). \quad (20)$$

The impact of wave function dilution on conductivity is shown in Fig. 6b. With increasing  $a$ , the conductivity first increases, after which it reaches a maximum at  $a = a_0\lambda_0/(2k_B T) = 19 \text{ nm}$ , which is equivalent to  $\lambda = 2k_B T$ . At higher values of  $a$ , the impact of  $\lambda$  fades and the influence of  $H$  becomes dominant, and as a result, the conductivity decreases again. This analysis demonstrates that delocalization may indeed form a mechanism that can substantially increase the conductivity in cable bacteria.

### 4.5 Hopping versus band transport?

In our model analysis, we described the electron transport in cable bacteria as thermally assisted hopping, as this is the default modelling approach employed to describe long-range biological conduction. Is there a possibility that the charge transport is not due to hopping, but rather acts as a form of band transport? In a hopping regime, the charge carrier is localized on a single molecule whereas in the band regime, the charge carrier (wave function) is delocalized over the entire system. In order to achieve a band regime, one must have a highly ordered structure with only a few defects or impurities, and a large electronic coupling between adjacent sites. In highly purified molecular single crystals such as pentacene, transport at low temperature can be described within a band picture.<sup>48</sup> However, at higher temperatures, the charge carriers get localized over single polymer strands and transport operates by a thermally activated hopping mechanism between adjacent polymer chains.<sup>49</sup>

As impurities, disorder and structural defects seem hard to avoid in the cm-long fiber structures in cable bacteria, a hopping regime is expected to operate at room temperature, as in organic crystals. Nevertheless, the models investigated here consider only one electronic state in a given “relay segment”. This leaves the possibility that there is more than



one electronic state in a given “relay segment”. Recall that the driving force behind localisation in our model is a weak electronic coupling at the edge of the hopping site ( $H < \lambda$ ). If a relay segment would be composed of  $N$  tightly stacked molecules, these must all be strongly coupled with an interaction energy,  $t > \lambda$ , if not, the electron would localise in a smaller region.<sup>37</sup> According to the tight binding model, this results in multiple electronic states lying in an energy band of width  $4t$ .<sup>26,50</sup> Within a 10 nm wide “relay segment”, and assuming a stacking distance of 0.35 nm (a typical intermolecular distances in organic conjugated crystals and films), each molecule ( $N = 30$ ) would add a single state to an energy band with an expected level spacing  $4t/N \sim 4\lambda/N \approx 27$  meV. At room temperature, the majority of states would contribute to the conductance (thermal window  $k_B T \approx 25$  meV). Therefore, while pure band transport is not expected in the conductive fiber network of cable bacteria, future studies should consider more elaborate model approaches that allow the existence of multiple electronic states within “relay segments”.

## Author contributions

J. R. V. performed numerical simulations and model analysis. Y. M. B., H. S. J. Z., F. J. R. M. and J. R. V. conceptualized the model analysis, and S. V. validated the simulation approach. J. R. V. and F. J. R. M. wrote the manuscript, with additional input from H. S. J. Z., Y. M. B. and S. V.

## Conflicts of interest

There are no conflicts to declare.

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