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Optical control of nanobody-mediated protein activity modulation with a photocleavable fluorescent protein†

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Antibodies are crucial in various biological applications due to their specific binding to target molecules, altering protein function and structure. The advent of single-chain antibodies such as nanobodies has paved the way for broader applicability in both research and therapies due to their small size and efficient tissue penetration. Recently, several approaches have been reported to optically control the antigen-binding affinity of nanobodies. Here, we show an alternative strategy for creating photo-activatable nanobodies. By fusing the photocleavable protein PhoCl with the N-terminus of the nanobody (named optoNb60), we successfully demonstrated light-dependent restoration of the antigen-binding ability and the following modulation of the activity of a target protein, the beta-2 adrenergic receptor. Moreover, the activation of optoNb60 was monitored by the fluorescence changes upon photoconversion. The compatibility of the uncaging design with the previously reported optogenetic molecules using nanobodies will contribute to the further optimization of the response capabilities of existing optogenetic tools, thereby expanding their applicability.

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Introduction

The unique ability of antibodies to specifically bind to target molecules with high affinity is indispensable in various biological applications, including protein activity modulation.^{1,2} By selectively binding to specific regions of target proteins, antibodies activate or inactivate protein functions by altering protein conformations and blocking active sites. In contrast to conventional antibodies, which typically exist as tetrameric structures with large molecular weights, the emerging use of single-chain antibodies, such as nanobodies,³ has recently gained significant attention.^{4–9} The remarkably small size of nanobodies enables exceptional tissue-penetrating capabilities, which allow them to access target molecules within tissues more effectively than traditional antibodies. Nanobodies are also used for the modulation of protein functions; for instance, a nanobody called Nb60 binds to the beta-2 adrenergic receptor (β 2AR) and inhibits ligand-dependent β 2AR-mediated signaling.¹⁰ The versatility of nanobodies as modulators for protein functions has led to their widespread use in research and therapeutics, underscoring their impor-

tance in understanding and manipulating biological processes at the molecular level.

Various strategies have been developed to regulate the antigen-binding affinities of nanobodies. One such approach involves employing chemogenetic control by integrating circularly permuted bacterial dihydrofolate reductase (cpDHFR)¹¹ into complementary-determining region 3 (CDR3) of the nanobody, named ligand-modulated antibody fragments (LAMAs).¹² This allows for the modulation of antigen binding by administration of the DHFR inhibitor trimethoprim. Alternatively, chemical induction of protein–protein interactions has been utilized to reassemble split nanobody fragments.¹³ Furthermore, a split-protein system has been combined with a light-inducible protein–protein interaction system, known as an optobody, utilizing optical dimerization tools called Magnets.¹⁴ Another optogenetic strategy akin to LAMAs involves the incorporation of a light-responsive LOV domain into the non-CDR loop, which enables reversible modulation of the affinity.¹⁵ Although these design strategies enable the artificial control of antigen binding, the activation of modified antibodies cannot be confirmed until the analysis of target protein functions.

In the present study, we aimed to develop a new design for generating photo-activatable caged nanobodies by genetically fusing a photocleavable protein called PhoCl¹⁶ with the N-terminal side of the nanobody locating an antigen-binding region. PhoCl undergoes photoconversion upon 405 nm

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illumination and then irreversibly cleaves into two fragments. By fusing PhoCl with the N-terminus of Nb60 (optoNb60), light-dependent uncaging of the fused nanobody was achieved, which enabled the subsequent modulation of β 2AR function. Moreover, the activation of the caged nanobody can be monitored using the photoconversion of fluorescence originating from the fused PhoCl. The present uncaging design will contribute to the precise control of target protein functions by tracking the photoconversion fluorescence, thereby expanding their applicability such as quantitative control of biological phenomena.

Materials and methods

Plasmid construction

The cDNAs of SNAPf tag, Halo tag, and PhoCl were amplified from pSNAPf-ADRB2 (NEB), p53-HaloTag (Promega), and PC-cadherin,¹⁷ respectively. The cDNA of Nb60 was generated by PCR. The PCR products were subcloned into the pcDNA4/myc-His B vector (Thermo Fisher Scientific, CA, USA).

Cell culture and transfection

Human embryonic kidney (HEK) 293 cells (CRL-1573, ATCC) and COS7 (CRL-1651, ATCC) were cultured in Dulbecco's modified Eagle's medium (DMEM, high glucose; Wako Pure Chemical Industries Ltd, Japan) supplemented with 10% fetal bovine serum (FBS; Gibco, CA, USA), 100 unit mL⁻¹ penicillin and 100 μ g mL⁻¹ streptomycin (Gibco) at 37 °C in 5% CO₂. HEK293 cells stably expressing β 2AR were cultured in DMEM supplemented with 10% FBS, 100 units mL⁻¹ penicillin, 100 μ g mL⁻¹ streptomycin (Gibco), 0.8 μ g μ L⁻¹ G418 sulfate (Millipore Sigma), and 0.05 μ g μ L⁻¹ ZeocinTM selection reagent (Thermo Fisher Scientific). HEK293 cells and COS7 cells were transiently transfected with expression vectors using the TransIT-LT1 transfection reagent (Mirus) or polyethylenimine "Max" (*M_w* 40 000) – high potency linear PEI (Cosmo Bio Co., Ltd), respectively, according to the manufacturer's protocol.

Western blot analysis

Cells were stimulated with 405 nm LED light (6 mW cm⁻² at 405 nm, 30 s min⁻¹, TH-160X120VL405-M1, CCS) for 30 min before cell collection. The cells were collected in lysis buffer (10 mM Tris-HCl, 150 mM NaCl, 5 mM EDTA, 50 mM NaF, and 0.5% (v/v) NP-40) and boiled with 5 \times sample buffer (50 mM Tris-HCl, 2% sodium dodecyl sulfate (SDS), 5% glycerol, 1% 2-mercaptoethanol, and 0.004% bromophenol blue) at 95 °C for 5 min.

For immunoprecipitation analysis, samples were lysed with mild lysis buffer (20 mM HEPES, 100 mM NaCl, and 0.5% maltose-neopentyl glycol). Insoluble materials were removed by centrifugation (14 000*g* for 5 min). Halo- β 2AR-myc was immunoprecipitated with Myc-Trap[®] agarose (Proteintech Group).

The samples were separated by SDS polyacrylamide gel electrophoresis and transferred onto a nitrocellulose membrane

(GE Healthcare). The membrane was blocked with 5% skim milk in Tris-buffered saline containing Tween-20 (TBS-T; 150 mM NaCl, 0.05% Tween-20, 50 mM Tris-HCl, pH 8.0). The membrane was incubated with the indicated primary antibodies and the appropriate secondary antibodies labelled with horseradish peroxidase (ESI Table S2[†]). Immunoblot bands were detected using the SuperSignal West Femto substrate (Thermo Scientific, IL, USA) with an image analyzer (LAS-4000 mini; Fuji Photo Film Co. Ltd, Tokyo, Japan).

Microscopy observation

Transiently transfected cells seeded on a 35 mm glass bottom dish (IWAKI) were stained with the HaloTag TMR ligand (Promega) and/or SNAP-Cell 647-SiR (New England Biolabs) according to the manufacturer's protocol. The cells were observed with an observation medium (Dulbecco's modified Eagle's medium (high glucose)) without L-glutamine and phenol red (FUJIFILM Wako Pure Chemical Corp.) and 10% fetal bovine serum under a confocal fluorescence microscope (IX-81, FV-1000D, Olympus). The acquired images were analyzed using ImageJ software (NIH).¹⁸

Bioluminescence assay

For the cAMP assay, the cells were transiently transfected with the plasmids of the caged nanobody and the pGloSensorTM-22F cAMP plasmid (Promega). The cells were seeded in a 96-well multiplate (Corning). The seeded cells were stimulated with 405 nm LED light (7.2 mW cm⁻² at 405 nm, 30 s min⁻¹, TH-160X120VL405-M1, CCS) for 30 min before the assay. The medium was exchanged with a measurement medium (Dulbecco's modified Eagle's medium (high glucose) with L-glutamine and phenol red, 10% fetal bovine serum, 1% penicillin-streptomycin, and 2% GloSensorTM cAMP reagent stock solution (Promega)), and then incubated in the dark for 2 h. The cells were then stimulated with 1 nM isoproterenol. The bioluminescence was measured using a microplate reader TriStar LB941 (Berthold).

Results

Photocleavage of the caged nanobody

The complementary-determining region of Nb60, which is the binding interface of the target β 2AR, is located on the N-terminal side. To modulate the binding ability of Nb60, candidate molecules were generated by fusing the C-terminus of the photocleavable protein, called PhoCl,¹⁷ with Nb60 at Gln² or Val³, directly or *via* glycine linkers (Gly, Gly-Gly, Gly-Gly-Gly) (Fig. 1, Fig. S1a[†]). For the following characterization, the FLAG tag (DYKDDDDK) and SNAPf tag were attached to the C-terminus. Nb60 fused with the SNAPf tag and an anti-GFP nanobody (GFPNb) fused with the SNAPf tag were also prepared as controls. Upon photocleavage of PhoCl by 405 nm light illumination, optoNb60 possibly binds to β 2AR and inhibits ligand-induced signalling (Fig. 1b).



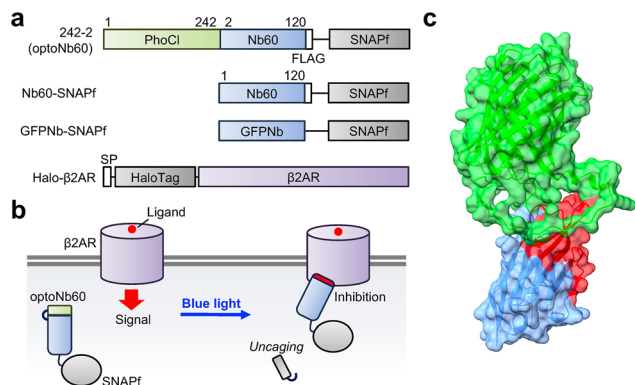


Fig. 1 Schematics for the inhibition of β 2AR by light-induced uncaging of optoNb60. (a) Domain structure of molecules used in this study. The numbers above boxes signify the amino acid numbers of the respective proteins. FLAG: FLAG epitope tag. SP: Signal peptide from HTR3A. (b) Schematic diagram for the strategy of the inhibition of β 2AR by light-induced uncaging of optoNb60. (c) The predicted structure of optoNb60. The structure of PhoCl fused with Nb60 was predicted by AlphaFold2. Green: PhoCl, Blue: Nb60, Red: the antigen-binding region of Nb60.

To examine the photocleavage of PhoCl in the candidate molecules upon blue light illumination, HEK293 cells transiently expressing the molecules were stimulated with blue light (405 nm) for 30 min and then subjected to western blotting (Fig. S1b†). The immunoblotted data clearly showed a light-dependent appearance of the band at around 37 kDa in candidate molecules where PhoCl was fused with Nb60 at Gln² directly (242-2) or *via* Gly (242-G-2) or fused at Val³ *via* Gly (242-G-3). The band size corresponded to the estimated molecular weight of Nb60 fused with the FLAG and SNAPf tags. Considering that the position of PhoCl should be close enough to cover the antigen-binding surface, the candidate molecule 242-2, which showed clear photocleavage and the shortest linker length between PhoCl and Nb60, was named optoNb60. Indeed, the antigen-binding surface of optoNb60 was partially hindered by the fused PhoCl according to the 3D structure predicted by AlphaFold2¹⁹ (Fig. 1c). The incomplete photocleavage might be improved by future optimization under illumination conditions or using the improved version of PhoCl.²⁰ Based on these results, we conclude that PhoCl fused with Nb60 detached from Nb60 upon illumination, which could be regarded as light-dependent uncaging.

Light-dependent recovery of optoNb60's antigen-binding ability

To confirm the photoconversion of PhoCl in optoNb60 in living cells, it was analyzed using fluorescence emitted by excitation light at 488 nm and 559 nm (Fig. 2a). Before photoconversion by illumination at 405 nm, the fluorescence was detected upon 488 nm excitation. Upon illumination at 405 nm, the fluorescence emitted by excitation at 488 nm gradually disappeared within 10 min (Fig. 2b). In contrast, the fluorescence emitted by excitation at 559 nm transiently

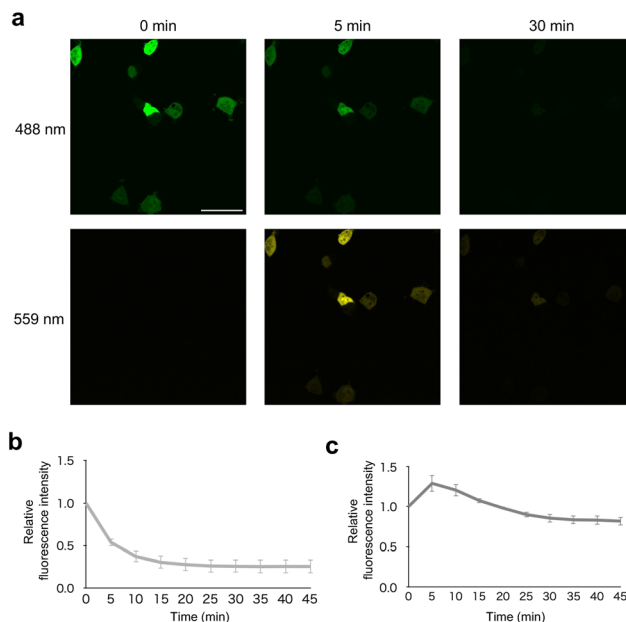


Fig. 2 Photoconversion of optoNb60. (a) The fluorescence emitted from PhoCl in optoNb60 during photoconversion. The numbers on the left side of the images indicate the wavelength of the excitation light. Scale bar: 50 μ m. (b and c) Quantitative analysis of the fluorescence intensities excited at 488 nm (b) and 559 nm (c) during the photoconversion. The fluorescence intensity was normalized by that at the onset of illumination ($t = 0$). Error bar: 95% confidence interval ($n = 3$).

increased around 5 min after the onset of illumination and slowly decayed within 20 min (Fig. 2c). These results suggest that the photoconversion of PhoCl in optoNb60 occurred within 5 min, followed by dissociation of the cleaved fragments over 20 min under the illumination conditions.

To examine where the interaction between Nb60 and β 2AR occurs inside the cells, their intracellular localization was investigated. In cells without β 2AR expression, both GFPNb and Nb60 labelled with SNAP-Cell 647-SiR showed cytosolic expression (Fig. 3a). In contrast, Nb60 showed localization on the plasma membrane in cells transiently expressing β 2AR labelled with HaloTag TMR, which also localized on the plasma membrane (Fig. 3b). Taken together, these results confirmed that the interaction between Nb60 and β 2AR occurred on the plasma membrane.

To investigate the antigen-binding ability of optoNb60 before and after 405 nm illumination, the localization of optoNb60 was analyzed by fluorescence from the labelled dye linked *via* the SNAPf tag (Fig. 3c). Before photoconversion, the caged nanobody was expressed in the cytosol, suggesting the absence of interaction with β 2AR located on the plasma membrane. Upon 405 nm illumination, the fluorescence from optoNb60 increased around the plasma membrane and reached a plateau around 25 min after the onset of illumination (Fig. 3d), whereas the fluorescence in the cytosol gradually decreased (Fig. 3e). The interaction between β 2AR and photo-cleaved optoNb60 was also detected by immunoprecipitation (Fig. S2†). These results indicate that the antigen-binding



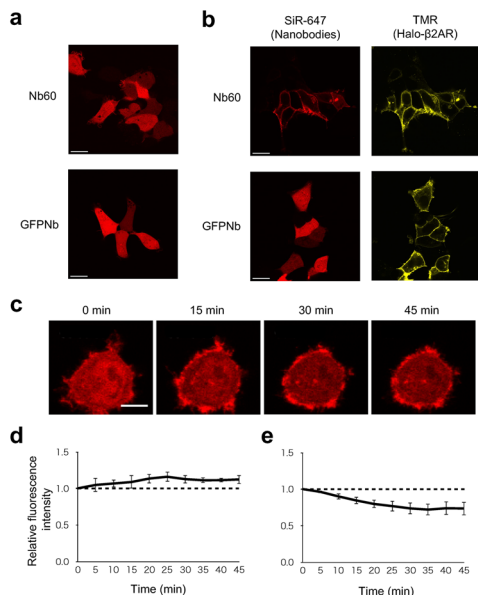


Fig. 3 Light-induced recovery of optoNb60's antigen-binding ability. (a) Intracellular localization of nanobodies. Scale bar: 20 μm . (b) Analysis of interaction between Nb60 and $\beta 2\text{AR}$ by their intracellular localization. 647-SiR and TMR fluorescence indicates the localization of nanobodies (GFPNb, Nb60, optoNb60) and $\beta 2\text{AR}$, respectively. Scale bar: 20 μm . (c) The fluorescence images of the localization of optoNb60 during 405 nm illumination. Scale bar: 10 μm . (d and e) Quantitative analysis of the fluorescence intensities in intracellular compartments. The fluorescence intensities in the plasma membrane (d) or in the cytosol (e) was normalized by that at the onset of illumination ($t = 0$). Error bar: 95% confidence interval ($n = 3$).

ability of Nb60 was inhibited by the fusion of PhoCl with optoNb60 and was recovered upon photoconversion and subsequent dissociation of PhoCl by 405 nm illumination.

Modulation of $\beta 2\text{AR}$ activity by the caged nanobody

$\beta 2\text{AR}$ couples to the stimulatory G protein (G_s), which stimulates the effector adenylyl cyclase to transiently produce cAMP.^{21,22} To investigate ligand-induced activation of $\beta 2\text{AR}$, cytosolic cAMP levels were monitored using GloSensor-22F.²³ HEK293 cells stably expressing $\beta 2\text{AR}$ were transiently cotransfected with GloSensor-22F and optoNb60. The transfected cells were illuminated with 405 nm LED light (7.2 mW cm^{-2} , 30 s min^{-1}) or kept in the dark for 30 min, and then stimulated with 10 nM isoproterenol. Ligand-induced changes in cAMP levels were monitored using the bioluminescence of GloSensor-22F (Fig. 4a, Fig. S3†). Considering that the expression level of $\beta 2\text{AR}$ was suppressed by the cotransfected proteins (Fig. S3b†), the bioluminescence of GloSensor-22F was normalized by that before stimulation in each condition in independent experiments. In cells expressing optoNb60, the cAMP level increased upon ligand activation by 1.90-fold in the dark compared to that in non-stimulated cells. In contrast, ligand-induced cAMP level changes in the cells stimulated with 405 nm light decreased 1.43-fold over the non-stimulated cells. In cells expressing GloSensor-22F and Nb60-SNAPf or

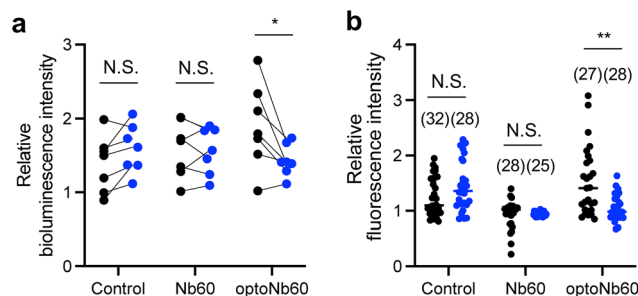


Fig. 4 Light-dependent inhibition of $\beta 2\text{AR}$ by optoNb60. (a) Optical inhibition of cAMP signaling. Black datapoints indicate dark samples, whereas the blue ones show illuminated samples. Control: no expression of any nanobodies. The bioluminescence of GloSensor-22F after ligand stimulation was normalized by that before stimulation in the independent experiments ($n = 7$). The statistical difference was analyzed by a paired t -test. N.S., $P > 0.05$, $*P < 0.05$. (b) Optical inhibition of Ca^{2+} signaling. The fluorescence signal of R-GECO was normalized by that before stimulation in each cell. The statistical difference was analysed by a paired t -test. Numbers in the parentheses indicate the numbers of analysed cells. N.S., $P > 0.05$, $**P < 0.01$.

expressing only GloSensor-22F, ligand-induced changes in cAMP levels were not affected by light illumination at 405 nm. Additionally, $\beta 2\text{AR}$ mobilizes Ca^{2+} via activation of phospholipase C, which is independent of the cAMP pathway.²⁴ To further confirm the inhibitory effect of optoNb60 on $\beta 2\text{AR}$ activity, the intracellular Ca^{2+} level was monitored by R-GECO.²⁵ HEK293 cells stably expressing $\beta 2\text{AR}$ were transiently cotransfected with R-GECO and optoNb60. The cells were stimulated with light and then subjected to Ca^{2+} level analysis under a confocal microscope (Fig. 4b). In control cells, the intracellular Ca^{2+} level increased in response to ligand stimulation, which was inhibited by Nb60 expression. In cells expressing optoNb60 in the dark, the Ca^{2+} level increased upon ligand activation by 1.52-fold compared to that in non-stimulated cells. In contrast, ligand-induced Ca^{2+} level changes in the cells stimulated with 405 nm light decreased 1.06-fold over the non-stimulated cells. These results demonstrate that optoNb60 inhibits $\beta 2\text{AR}$ activity by light-induced uncaging.

Conclusions

In this study, we developed a genetically encoded caged nanobody named optoNb60, whose antigen-binding ability against $\beta 2\text{AR}$ was optically controlled by light-dependent uncaging of N-terminally fused PhoCl. We confirmed that the fused PhoCl undergoes photoconversion and cleaves upon 405 nm illumination, which results in the recovery of the antigen-binding ability of the nanobody. The optically uncaged nanobody allows binding to $\beta 2\text{AR}$ on the plasma membrane and inhibits ligand-dependent activation of downstream signaling. The activation of the caged nanobody can also be monitored by the photoconversion of fused PhoCl, whose fluorescence emitted by excitation at 559 nm transiently increased upon photoconversion. The improvement in the photocleavage efficiency will



further enhance the inhibitory effect. The present uncaging design will contribute to the precise control of target protein functions by tracking the photoconversion fluorescence, thereby expanding their applicability, such as the quantitative control of biological phenomena.

Author contributions

M. E. and T. O. conceived the project, M. E., Q. K. and S. T. performed the experiments, and M. E. and T. O. wrote the manuscript.

Conflicts of interest

There are no conflicts to declare.

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