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On the stability of peptide secondary structures on the TiO₂ (101) anatase surface: a computational insight†

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The biological activity of proteins is partly due to their secondary structures and conformational states. Peptide chains are rather flexible so that finding ways inducing protein folding in a well-defined state is of great importance. Among the different constraint techniques, the interaction of proteins with inorganic surfaces is a fruitful strategy to stabilize selected folded states. Surface-induced peptide folding can have potential applications in different biomedicine areas, but it can also be of fundamental interest in prebiotic chemistry since the biological activity of a peptide can turn-on when folded in a given state. In this work, periodic quantum mechanical simulations (including implicit solvation effects) at the PBE-D2* level have been carried out to study the adsorption and the stability of the secondary structures (α -helix and β -sheet) of polypeptides with different chemical composition (*i.e.*, polyglycine, polyalanine, polyglutamic acid, polylysine, and polyarginine) on the TiO₂ (101) anatase surface. The computational cost is reduced by applying periodic boundary conditions to both the surface and the peptides, thus obtaining full periodic polypeptide/TiO₂ surface systems. At variance with polyglycine, the interaction of the other polypeptides with the surface takes place with the lateral chain functionalities, leaving the secondary structures almost undistorted. Results indicate that the preferred conformation upon adsorption is the α -helix over the β -sheet, with the exception of the polyglutamic acid. According to the calculated adsorption energies, the affinity trend of the polypeptides with the (101) anatase surface is: polyarginine \approx polylysine > polyglutamic acid > polyglycine \approx polyalanine, both when adsorbed in gas phase and in presence of the implicit water solvent, which is very similar to the trend for the single amino acids. A set of implications related to the areas of surface-induced peptide folding, biomedicine and prebiotic chemistry are finally discussed.

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Introduction

There are many aspects that regulate the activity of a protein: the amino acid sequence, the structure, the pH, the temperature, *etc.* Temperature and pH are properties relatively easy to control, and in the human body they are very well buffered. The

amino acidic sequence, which determines the protein structure (*i.e.*, secondary, tertiary and quaternary), can be modified by applying mutations. In the last years, protein engineering has gained interest because, by means of *de novo* peptide design techniques, one can generate new proteins, not present in nature, exhibiting unique and desired properties.^{1,2} All protein functions depend on their structure, which, in turn, depends on the physical and chemical environmental conditions. Any change of a protein at any structural level, including slight changes in the folding and shape, may render it as non-functional. Examples of how protein structure regulates its activity are hemoglobin and statherin. In the former case, hemoglobin can be in tense (T) or relaxed (R) conformations, each of them exhibiting different affinities to O₂.^{3–5} In the case of statherin (a human salivary protein), while it has a random coil conformation in solution, it adopts an α -helix conformation when adsorbed on hydroxyapatite (the main constituent of tooth enamel), so preventing calcium phosphate precipitation

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† Electronic supplementary information (ESI) available: PBE-D2* optimized structures of the bare TiO₂ surface and of extended, β -sheet and α -helix poly-amino acidic systems, in gas phase and adsorbed on the TiO₂ surface. Extended Tables of the adsorption energies and the relative stabilities between β -sheet and α -helix on TiO₂. AIMD simulations of the GLY- β -sheet-AP/TiO₂ and GLY- β -sheet-P/TiO₂ complexes. Graphics of H-bond pattern analysis of the secondary structures analysed. Fractionary coordinates of the optimized systems. See DOI: <https://doi.org/10.1039/d2cp04395e>



and maintaining a high calcium level in saliva for the remineralisation of the tooth enamel.^{6–9}

The protein structure, and particularly its folding, is regulated by many driving forces. In aqueous solution, folding is essentially dictated by hydrogen-bond (H-bond) and hydrophobic (dispersion dominated) interactions.^{10,11} In solution, proteins fold by exposing the hydrophilic lateral chains to the polar solvent, while the hydrophobic residues are buried in the core of the protein. Peptide chains are rather flexible so that finding efficient ways that force the protein folding in a well-defined state has an increasing interest. To be folded, a protein needs extra-interactions that compensate the entropy loss due to moving from the random coil state to the folded state. Solvation/desolvation processes also play a crucial role in the entropic budget.

The adoption of the “surface science model for catalysis” approach, based on the interplay among materials preparation methods, spectroscopic measurements and quantum mechanical simulations, has been very useful to characterize surface molecular events relevant for heterogeneous catalysis.^{12–16} Inspired on by the same underlying idea, in the last years, combination of surface science with molecular biology has led to the “surface science model for biology”,^{17–19} in which the interactions of a biological molecule with an inorganic substrate are investigated. In this last years, the interaction of proteins with inorganic surfaces has demonstrated to be an effective strategy to stabilize selected folded states.²⁰ Different studies on this topic can be found using, for example, gold nanoparticles,^{21–23} silica,^{24,25} and hydroxyapatite.^{26,27} The surface-induced peptide folding is a promising tool to: (i) obtain peptide monolayers exhibiting free-interacting sequences that may display specific biochemical recognition phenomena; and (ii) induce a specific bioactivity of the protein, which is missing in its unfolded state. Both issues have several important applications in biosensing, biotechnology, biocatalysis, biomaterials, tissue engineering, nanotechnology, and proteomics. Moreover, the peptide folding induced by naturally-occurring surfaces and the subsequent activation of a potentially “hidden” bioactivity might have triggered the first biocatalytic reactions in a primordial Earth (in absence of life), hence giving rise to the emergence of the metabolic cycles, a crucial aspect for the origin of life.^{28,29} On the other hand, surface-induced peptide folding can have implications in the pathogenesis of Alzheimer disease. It has been shown that TiO₂ nanoparticles significantly enhance the rate of amyloid- β (A β) fibrillation,^{30,31} which can be related to the enhanced stabilization of β -sheets assemblies, the common structure of polypeptide chains in fibrillary aggregates.³²

The capability of a surface to induce a given peptide folding state is dictated by the structure-specific binding properties of the interacting components. Thus, detailed knowledge of the interactions between the peptide and the surface is of fundamental relevance. Experimental techniques such as X-ray diffraction, which is hitherto the most accurate techniques to accurately determine the molecular structure at atomic resolution fails to characterize peptide/surface interactions, due to a drastic drop of resolution when passing from a 3D

to a 2D system.³³ Other spectroscopic techniques such as Fourier-transform infrared spectroscopy (FTIR),³⁴ or atomic force microscopy (AFM)³⁵ can provide useful information on the interaction of biologic molecules with inorganic surfaces,³⁶ but they are still far from providing atomic resolution details. However, recent works have proven that solid state nuclear magnetic resonance (ssNMR) couple with cryo-electron tomography and cryo-electron microscopy techniques is capable to get closer to the atomistic resolution, even if these characterization techniques could be further improved.^{37–39} Computer simulations, and in particular molecular/surface modelling, are thus useful complementary tools to obtain the missing atomic-scale information. For instance, full characterization of the glycine/nanohydroxyapatite interactions was achieved by combining spectroscopic measurements with accurate quantum mechanical (QM) calculations.⁴⁰ Quite obviously, most of the computational studies involving proteins (with thousands of atoms) have been performed with classical molecular dynamics (MD) simulations,^{41,42} focusing on the dynamic behaviour of proteins in water and when docked to the surfaces. The adoption of classical force fields (FF), forced by the large system size, inevitably lowers the accuracy of the results, as FF: (i) cannot cope with the likely bond breaking/making between the side chains and the surfaces (with the exception of reactive force fields like ReaxFF⁴³); (ii) may be inaccurate when dealing with interactions involving hybrid inorganic/organic systems for which the parametrization is usually grossly estimated. QM simulations are, thus, the obvious choice to keep well-balanced accuracy for a large variety of chemical environments. However, these studies are rare due to the enormous complexity of the considered systems.^{44,45} Consequently, to apply full QM simulations, one is forced to design simplified systems, reducing the biological component to single amino acids or very small oligopeptides in interaction with the surfaces.^{27,46}

In the present work, we have studied the stability of secondary structures (α -helix and β -sheet) on the TiO₂ (101) anatase surface by means of periodic QM simulations, in both dry and aqueous environments, this latter by adopting an implicit solvation model. To assess the influence of the lateral chains in the adsorption properties, different polypeptide model systems differing in their chemical functionalities have been used: polyglycine (the reference case), polyalanine (nonpolar), polyglutamic acid (polar/acidic), and polylysine and polyarginine (polar/basic). To model the peptide/TiO₂ surface systems, the same strategy used in a previous work by us using polyglycine as a test case⁴⁷ has also been adopted here, *i.e.*, the periodicity applied to the surface has also been applied to the peptide. This strategy allowed using relatively small unit cells (up to 500 atoms) keeping, at the same time, the desired secondary structure of the considered polypeptides. Clearly, this strategy cannot provide information on the conformational space of the whole protein/surface system, providing, instead, easy reproducibility of the results due to its well-defined strategy and adopted computational tools. Nonetheless, it can provide enough information on the relative role of different peptide composition as well as elucidate the basic interactions



causing the preference of a secondary structural motif of the adsorbed peptide.

Methodology

Computational details

All the periodic DFT local geometry optimizations have been done with the Vienna *Ab initio* Simulation Package (VASP).^{48–51} The calculations were performed with the Perdew–Burke–Ernzerhof (PBE) functional,⁵² including the Grimme's D2^{53,54} empirical correction for dispersion, modified for extended systems (D2*),⁵⁵ which has proven to provide good results on these kinds of systems.^{56,57} VASP uses the projector-augmented wave (PAW) pseudopotentials⁵⁸ to describe the ionic cores and a plane wave basis set for the valence electrons. For the present work, the energy cutoff was set to 500 eV, the self-consistent field (SCF) iterative procedure was converged to a tolerance in total energy of $\Delta E = 10^{-5}$ eV, and the tolerance on gradients for local geometry optimization was set to 0.01 eV Å⁻¹ for each atom in each direction. For all the calculations involving the TiO₂ surface, only the internal atomic positions were freely optimized, keeping the cell parameters fixed to the experimental values of the bulk structure. For the isolated secondary structures, both the atomic positions and the cell parameters were optimized, thus including in the calculations of the adsorption energies the deformation cost of the biological part to adapt to the surface cell. Solvent effects were also considered through the polarizable continuous model (PCM) as implemented in the VASP package,^{59,60} optimizing the gas phase systems within this implicit solvent model. The *k*-points mesh was set to (3, 3, 1) for the adsorption of the extended primary structures and β -sheets, and to (2, 2, 1) for α -helix adsorptions.

Visualization and manipulation of computed structures were done with the MOLDRAW⁶¹ and VMD⁶² packages. Figures have been rendered with the POV-Ray program,⁶³ using MOLDRAW to build up the input file.

Polypeptide/surface and mathematical models

As in our previous work on the modelling of periodic polyglycine secondary structures and their adsorption on the anatase TiO₂ (101) surface,⁴⁷ a full periodic approach has also been applied to model the structures of the polypeptides studied here. The structures of the periodic isolated polypeptide systems are available in the ESI.† The starting complexes were built using the polyglycine systems in ref. 47 by substituting the H atom on the α -carbon with the proper side chain of interest. Then, the side chains were moved in order to maximize the interactions with the surface by forcing the formation of dative and H-bonds, thus following the principle of the maximum electrostatic interactions (the starting structures are available in the ESI† as well). In addition to the α -helix and β -sheet secondary structures, in this work we also modelled the extended primary structures (i.e. the peptides unfolded forming a linear chain). The above-mentioned structures (i.e. the extended primary linear polymer) do not have physical meaning and have

been used as reference to calculate the adsorption energies (see below).

The TiO₂ (101) slab model has unit cell parameters of $a = 7.569$ Å, $b = 10.239$ Å, $\gamma = 90$ degrees. The surface slab model presents, at the outermost positions, penta coordinated Ti atoms (Ti_{5c}, which can act as acidic Lewis sites) and bridge O atoms (O_{br}, which can act as basic Lewis sites) that bonds among two Ti_{5c}. The structure of the bare surface is available in ESI.† All the polypeptide β -sheet structures were adsorbed on a 1×1 unit cell resulting, under the periodic approach, in 2D-periodic surface slab systems. In contrast, α -helices are 1D-periodic polymer systems (the periodic direction being very close to the surface *b* cell axis) and, accordingly, the *a* parameter must be large enough to avoid lateral interactions among adjacent unit cells. To this end, different supercells were used, depending on the size of the polypeptide lateral chains: for polyglycine and polyalanine, a 2×1 supercell ($a = 15.138$ Å, $b = 10.239$) was used, ensuring a distance of ~ 10 Å between neighbouring helices, while for the other peptides (i.e., polyglutamic acid, polylysine and polyarginine), a 3×1 supercell ($a = 22.707$ Å, $b = 10.239$) was used. The *c* parameter was set to 40 Å, to ensure negligible interactions among fictitious slab replicas.

To calculate the adsorption energies between the polypeptide secondary structures and the TiO₂ (101) anatase surface, and the energetics of the interconversion between β -sheet and α -helix on the surface, the same strategy of our previous paper has been adopted.⁴⁷

Adsorption energies normalized to the amino acid residues per unit cell ($\Delta E_{\text{ADS/unit}}$) were calculated as:

$$\Delta E_{\text{ADS/unit}} = \frac{1}{N(\text{EXT}/\alpha/\beta)} \left[E_{\text{CPLX}}^{(\text{EXT}/\alpha/\beta)} - \left(\frac{N(\text{EXT}/\alpha/\beta)}{N_{\text{EXT}}} \right) E_{\text{EXT}} - E_{\text{SURF}} \right] \quad (1)$$

where (EXT/ α / β) refers to the extended primary (EXT), α -helix (α) and β -sheet (β) structures of the polypeptides, E_{CPLX} is the total energy of a given polypeptide/surface complex, E_{EXT} is the total energy of the isolated extended primary polypeptide, N is the number of amino acid units of the corresponding polypeptide structures in the unit cell, the normalization factor “2” is the number of amino acid units of the primary extended structures in the unit cell (i.e., 2 for all the cases of polyamino acidic systems), and E_{SURF} is the total energy of the isolated surface (considering the corresponding unit cell sizes). By using this expression, the energetics associated with forming a secondary structure upon adsorption (which is a balance between the energy gain due to the formation of the H-bond patterns of the secondary structures and the energy cost due to the deformation of the secondary structures upon adsorption) is already considered, because the reference system is the extended primary polypeptide structure. These energetic terms, moreover, have been computed as:

$$\Delta E_{\text{H/unit}} = \frac{1}{N(\alpha/\beta)} \left[E_{\text{PP}}^{(\alpha/\beta)} - \left(\frac{N(\alpha/\beta)}{N_{\text{EXT}}} \right) E_{\text{EXT}} \right] \quad (2)$$



$$\Delta E_{\text{def/unit}} = \frac{1}{N^{(\alpha/\beta)}} \left[E_{\text{PP/CPLX}}^{(\alpha/\beta)} - E_{\text{PP}}^{(\alpha/\beta)} \right] \quad (3)$$

where $\Delta E_{\text{H/unit}}$ and $\Delta E_{\text{def/unit}}$ are the abovementioned H-bond gain and the deformation cost (normalized per amino acidic residue), E_{PP} is the total energy of the corresponding isolated secondary structure and $E_{\text{PP/CPLX}}$ is the total energy of the corresponding isolated secondary structure but in their optimized geometry on the surface. The sum of the two terms gives the energy balance of the H-bond gain and the deformation energy when the polypeptide secondary structures adsorb on the surface with respect to the extended primary structure:

$$\Delta E_{\text{H+def/unit}} = \Delta E_{\text{H/unit}} + \Delta E_{\text{def/unit}} \quad (4)$$

The relative stability of the secondary structures on the surface has been calculated by comparing their adsorption energies for each polypeptide system according to the energy cycle of Fig. 1A

$$\Delta \Delta E_{\text{surf/unit}} = \Delta E_{\text{ADS/unit}}^{(\beta\text{-PP})} - \Delta E_{\text{ADS/unit}}^{(\alpha\text{-PP})} \quad (5)$$

Similarly, it is also possible to refer the adsorption energies with respect to the secondary structures already formed:

$$\Delta E_{\text{ADS/unit}}^{(\alpha/\beta)} = \left[E_{\text{CPLX}}^{(\alpha/\beta)} - E_{\text{PP}}^{(\alpha/\beta)} - E_{\text{SURF}} \right] \times \frac{1}{N^{(\alpha/\beta)}} \quad (6)$$

where the reference $E_{\text{PP}}^{(\alpha/\beta)}$ is the total energy of the isolated β -sheet/ α -helix structures at their optimized geometries. Consequently, the energetic cycle becomes as depicted in Fig. 1B:

$$\Delta \Delta E_{\text{surf/unit}} = \Delta E_{\text{ADS/unit}}^{(\beta)} - \Delta E_{\text{ADS/unit}}^{(\alpha)} + \Delta \Delta E_{\text{iso/unit}} \quad (7)$$

and $\Delta \Delta E_{\text{iso/unit}}$ is the energy associated with the α -helix \rightarrow β -sheet conversion for the secondary structures in their isolated states:

$$\Delta \Delta E_{\text{iso/unit}} = \frac{E_{\text{PP}}^{(\beta)}}{N^{(\beta)}} - \frac{E_{\text{PP}}^{(\alpha)}}{N^{(\alpha)}} \quad (8)$$

in which the total energies ($E_{\text{PP}}^{(\beta)}$ and $E_{\text{PP}}^{(\alpha)}$) are normalized by the amino acid units of each structure, *i.e.*, $N^{(\beta)} = 4$ and $N^{(\alpha)} = 7$. Eqn (2) and (4) must give the same results by definition.

Results and discussion

The polyglycine case – brief summary of our previous work

In our previous work,⁴⁷ the adsorption and the relative stability of the polyglycine α -helix and β -sheet structures was assessed by using the same modelling strategies applied here. The optimized geometries of the polyglycine secondary structures adsorbed on TiO_2 are reported in ESI,[†] Table 1 reports the calculated $\Delta E_{\text{ADS/unit}}$ values (and related terms), and Table 2 the relative stabilities of the α -helix and β -sheet structures on the surfaces.

The effect of the TiO_2 surface (and also of the implicit solvation) is to stabilize the α -helix folding over the β -sheet one. This can be explained by analysing the energy contributions to the adsorption energy reported in Table 1 (more details on their calculation can be found in the ESI[†]). While the $\Delta E_{\text{ADS/unit}}$ adsorption energies are fairly similar for all the cases (between -30 and -34 kJ mol^{-1} in the gas phase), the deformation energies due to the adsorption is very different for each secondary structure (between 14 and 23 kJ mol^{-1} , see $\Delta E_{\text{def/unit}}$ in Table 1), being minor in the α -helix (which moreover goes in opposite direction with respect to the adsorption energy). Because of that, α -helix is the most stable secondary structure upon TiO_2 adsorption. Further proofs of this enhanced stability of the α -helix were provided by *ab initio* molecular dynamics simulations (AIMDs). They were run to assess if dynamic effects (*i.e.*, temperature and entropy) could induce denaturation of the secondary structures, as the backbone C=O groups directly interact with the surface through $\text{C=O} \cdots \text{Ti}_{5c}$ dative bonds. After the AIMDs, the resulting α -helix structure was found, although more distorted, more stable (after optimising the geometry) than the non-distorted structure, hence increasing the stability of the α -helix/ TiO_2 complex. However, this was not the case for β -sheets structures: by starting the AIMDs with

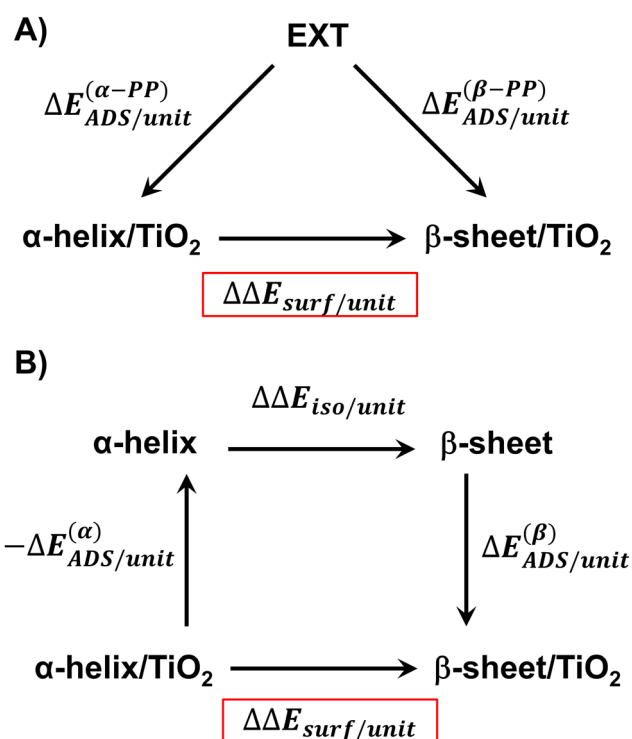


Fig. 1 Energy cycles to compute the reaction energy associated with the conversion process of α -helix/ $\text{TiO}_2 \rightarrow \beta$ -sheet/ TiO_2 : (a) based on the energy balance between the normalized adsorption energies of the α -helix and β -sheet to the surfaces from the periodic isolated extended primary structures; (b) based on an energy cycle adopting a three-step process: (i) desorption of the α -helix from the surface into its periodic isolated state, (ii) conformational change from α -helix to β -sheet in their periodic isolated states, and (iii) adsorption of the β -sheet to the surface from its periodic isolated state.



Table 1 Calculated adsorption energies normalized per amino acidic unit ($\Delta E_{\text{ADS/unit}}$) for each studied complex, both in the gas phase (bare values) and under PCM conditions (values in parenthesis). Other energetic terms of interest are also included: the energetic gain due to the secondary structure formation with respect to the extended primary polymeric structure ($\Delta E_{\text{H/unit}}$), the deformation energy of the secondary structure due to the adsorption ($\Delta E_{\text{def/unit}}$), and the sum of these two terms ($\Delta E_{\text{H+def/unit}}$). See the text for details on the definition of the energy terms. Energy units are in kJ mol^{-1}

System	AA units	$\Delta E_{\text{ADS/unit}}$	$\Delta E_{\text{H/unit}}$	$\Delta E_{\text{def/unit}}$	$\Delta E_{\text{H+def/unit}}$
GLY_β-sheet_AP/TiO ₂	4	−30.2 (−0.1)	−23.6 (−9.1)	23.0 (19.7)	−0.6 (10.6)
GLY_β-sheet_P/TiO ₂	4	−28.9 (−0.9)	−18.5 (−38)	19.6 (13.8)	1.1 (10.0)
GLY_α-helix/TiO ₂	7	−33.7 (−11.5)	−21.5 (−9.9)	14.1 (9.4)	−7.4 (−0.5)
ALA_β-sheet_AP/TiO ₂	4	−17.4 (3.8)	−27.4 (−14.5)	22.2 (21.5)	−5.2 (6.9)
ALA_β-sheet_P/TiO ₂	4	−15.5 (4.2)	−20.9 (−9.8)	17.2 (18.5)	−3.7 (8.7)
ALA_α-helix/TiO ₂	7	−26.6 (−11.3)	−23.2 (−11.9)	5.2 (5.1)	−18.0 (−6.8)
GLU_β-sheet_AP/TiO ₂	4	−57.1 (−18.8)	−37.6 (−20.9)	34.9 (36.1)	−2.7 (15.2)
GLU_β-sheet_P/TiO ₂	4	−65.5 (−23.4)	−36.8 (−10.2)	30.0 (22.5)	−6.8 (12.3)
GLU_α-helix/TiO ₂	7	−59.0 (−20.2)	−31.6 (−15.1)	12.4 (10.7)	−19.3 (−4.4)
LYS_β-sheet_AP/TiO ₂	4	−67.7 (−34.3)	−39.3 (−22.3)	29.1 (25.7)	−10.2 (3.4)
LYS_β-sheet_P/TiO ₂	4	−71.7 (−38.7)	−36.4 (−19.7)	24.2 (21.4)	−12.1 (1.6)
LYS_α-helix/TiO ₂	7	−84.2 (−46.2)	−23.3 (−10.1)	9.8 (11.1)	−13.5 (1.0)
ARG_β-sheet_AP/TiO ₂	4	−67.9 (−28.5)	−60.9 (−29.1)	59.0 (43.5)	−1.9 (14.4)
ARG_β-sheet_P/TiO ₂	4	−71.8 (−35.1)	−74.8 (−30.0)	64.2 (34.1)	−10.6 (4.1)
ARG_α-helix/TiO ₂	7	−82.6 (−38.6)	−23.5 (−8.8)	3.8 (8.0)	−19.7 (−0.9)

Table 2 Values of the reaction energies of the α-helix → β-sheet conformational change of the isolated secondary structures ($\Delta\Delta E_{\text{iso/unit}}$) and on the TiO₂ (101) anatase surface ($\Delta\Delta E_{\text{surf/unit}}$), including the involved energy terms according to the energy cycle shown in Fig. 1 (see the text for details on the definition of the energy terms), both in the gas phase (bare values) and under PCM conditions (values in parenthesis). Energy units are in kJ mol^{-1}

Reaction	$\Delta E_{\text{ADS/unit}}^{(\beta)}$	$\Delta E_{\text{ADS/unit}}^{(\alpha)}$	$\Delta\Delta E_{\text{iso/unit}}$	$\Delta\Delta E_{\text{surf/unit}}$
GLY_α-helix/TiO ₂ → GLY_β-sheet_AP/TiO ₂	−6.6 (9.0)	−12.2 (−1.6)	−2.1 (0.8)	3.5 (11.4)
GLY_α-helix/TiO ₂ → GLY_β-sheet_P/TiO ₂	−10.4 (2.9)	−12.2 (−1.6)	3.0 (6.1)	4.8 (10.6)
ALA_α-helix/TiO ₂ → ALA_β-sheet_AP/TiO ₂	10.0 (18.7)	−3.3 (0.5)	−4.2 (−2.6)	9.2 (15.5)
ALA_α-helix/TiO ₂ → ALA_β-sheet_P/TiO ₂	5.5 (13.6)	−3.3 (0.5)	2.3 (2.1)	11.1 (15.2)
GLU_α-helix/TiO ₂ → GLU_β-sheet_AP/TiO ₂	−19.6 (2.1)	−27.3 (−5.1)	−5.9 (−5.8)	1.8 (1.4)
GLU_α-helix/TiO ₂ → GLU_β-sheet_P/TiO ₂	−28.7 (−13.2)	−27.3 (−5.1)	−5.2 (5.0)	−6.5 (−3.2)
LYS_α-helix/TiO ₂ → LYS_β-sheet_AP/TiO ₂	−28.4 (−12.0)	−60.9 (−36.1)	−16.0 (−12.2)	16.5 (11.9)
LYS_α-helix/TiO ₂ → LYS_β-sheet_P/TiO ₂	−35.4 (−19.0)	−60.9 (−36.1)	−13.1 (−9.7)	12.5 (7.5)
ARG_α-helix/TiO ₂ → LYS_β-sheet_AP/TiO ₂	−7.0 (0.6)	−59.1 (−29.8)	−37.4 (−20.3)	14.7 (10.1)
ARG_α-helix/TiO ₂ → LYS_β-sheet_P/TiO ₂	3.0 (−5.1)	−59.1 (−29.8)	−51.3 (−21.1)	10.8 (3.5)

distorted β-sheet structures, they reverted to the actual β-sheet ones during the AIMDs.

Polyamino acid secondary structures: alanine, glutamic acid, lysine and arginine

In this work, we apply the same modelling strategy to other peptide secondary structure models, with the aim to expand this study and provide more general information on the interaction of proteinaceous secondary structures with TiO₂ nanoparticles. In the present study, however, we have not run AIMD simulations since as it will be shown below, polypeptide-surface interactions take place through the side chains and not through the C=O backbone, leaving the secondary structure almost undistorted.

Starting from the isolated polyglycine (GLY) structures, we model the other polypeptide systems (hereafter referred to as non-GLY systems) by replacing one of the two hydrogen atoms

of the α-carbon with the corresponding lateral chains (taking caution to form the correct biogenic L enantiomer). Polyalanine (ALA) was chosen as a representative structure for non-polar residues, polyglutamic acid (GLU) for acidic residues, and polylysine (LYS) and polyarginine (ARG) for basic chains. The resulting isolated systems adopting the extended primary, β-sheet (parallel P, and antiparallel AP) and α-helix structures are available in the ESI.† The complexes resulting from the adsorption of the secondary structures for ALA, GLU, LYS and ARG on the TiO₂ (101) anatase surface are shown in Fig. 2–5, respectively. For the sake of comparison, the adsorption complexes of GLY can be found in ESI.† Note that for polyglutamic acid, we have only considered the non-deprotonated form, since as shown for the adsorption of glutamic amino acid on anatase TiO₂ surface⁶⁴ this is the preferred situation.

For all non-GLY cases, the secondary structure backbones do not interact directly with the surface (note that this was not the



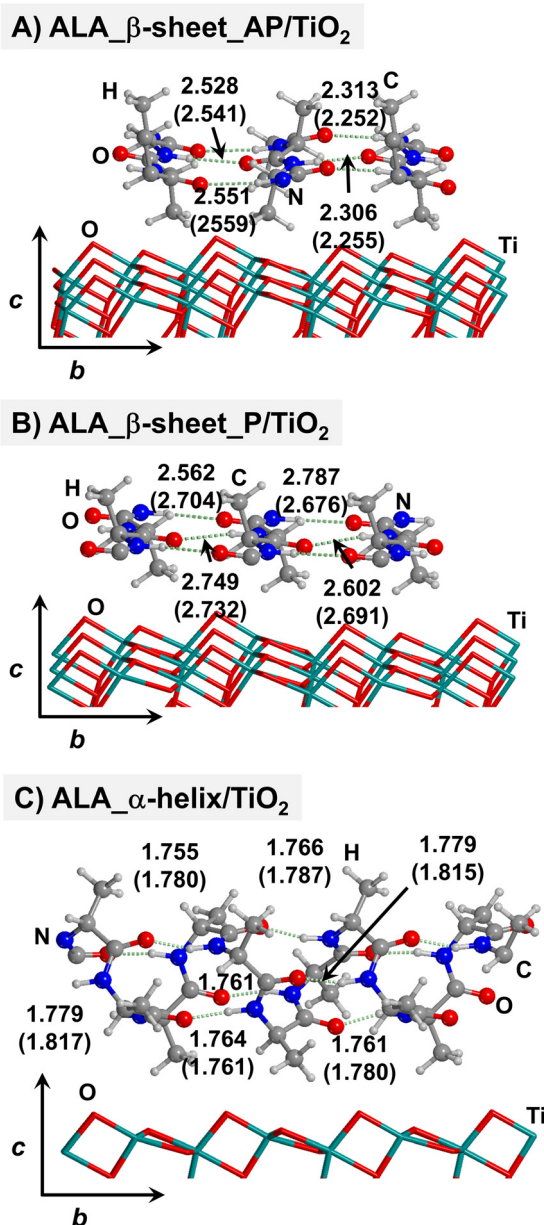


Fig. 2 PBE-D2* optimized structures of antiparallel (a) and parallel (b) polyaniline β -sheets, and polyaniline α -helix (c) adsorbed on the TiO₂ (101) anatase surface. Numbers in parenthesis refer to values in implicit solvation, while numbers without parenthesis refer to values in the gas phase. Bond lengths are in Å.

case for GLY, in which the interaction was direct through $\text{C}=\text{O} \cdots \text{Ti}_{5c}$ bonds). Accordingly, the β -sheet and α -helix secondary structure patterns do not become distorted upon adsorption with respect to the isolated states. However, a comparison of the secondary structure H-bond distances among the isolated and adsorbed states indicates that in β -sheet structures (both in parallel and antiparallel conformation) the H-bonds are notably weaker when on the surface than in the isolated states (*i.e.*, with H-bond distances of ≈ 2.0 – 2.3 Å in the isolated states and ≈ 2.5 – 3.0 Å in the adsorbed states), while in the α -helix structures they are similar (H-bond distances of ≈ 1.8 – 2.0 Å) or even slightly

shorter. For GLU, the interaction takes place between the COOH lateral chain functionality and the surface, in which both a $\text{C}=\text{O} \cdots \text{Ti}_{5c}$ dative covalent bond and a $\text{OH} \cdots \text{O}_{br}$ H-bond are established. Similar interactions take place for LYS and ARG, although for these cases through $\text{N} \cdots \text{Ti}_{5c}$ dative bonds and $\text{NH}_2 \cdots \text{O}_{br}$ H-bonds. For ALA, neither dative interactions nor H-bonds can be formed. In this case, the interaction with the surface is due to dispersive forces, in which the CH_3 group points towards the surface but without establishing any direct interaction.

According to the calculated $\Delta E_{\text{ADS/unit}}$ values (reported in Table 1), ALA is the polypeptide presenting the smallest $\Delta E_{\text{ADS/unit}}$ values (from -15.5 to -26.6 kJ mol⁻¹, values in the gas phase). The trend is then followed by GLU, with a range of $\Delta E_{\text{ADS/unit}}$ from -57.1 to -65.5 kJ mol⁻¹. Finally, LYS and ARG present very similar $\Delta E_{\text{ADS/unit}}$ values (from -67.7 to -84.2 kJ mol⁻¹ and from -67.9 to -82.6 kJ mol⁻¹, respectively). These values are in full consistency with the driving forces responsible of the adsorption. ALA complexes are held by dispersive interactions, and hence this system is the least bound. GLU, LYS and ARG complexes, all form dative covalent bonds and H-bonds. However, dative interactions in GLU are weaker than in LYS and ARG because in the former the dative bond is through an O atom while in the later through N atoms, the Lewis basic character being larger in N than in O. Interestingly, the differences in the computed adsorption energies, support our consideration that it is not necessary to explore all the 20 possible polypeptide models; it is enough to consider classes of amino acidic residues. Thus, we do not expect significant difference (either structural or energetic) between glutamic acid and aspartic acid, or between alanine and leucine or isoleucine. Moreover, the choice was guided from our previous works on the adsorption of amino acids on TiO₂ anatase and rutile surfaces^{64,65} in which, remarkably, the affinities of the lateral chains with the surfaces follow the same trend as the one find here for the polypeptides.

If solvation effects are accounted for with PCM, calculated $\Delta E_{\text{ADS/unit}}$ values drop down by a large amount, because solvation competes with adsorption. However, the energetic ranking among the different amino acids is not altered, apart for GLY and ALA, whose stability is swapped with respect to the gas phase. Therefore, a global sequence of increasing adsorption energy is $\text{ALA} \approx \text{GLY} < \text{GLU} < \text{LYS} \approx \text{ARG}$. We would like to highlight that no calculations with explicit water molecules have been performed, and, accordingly, specific solvent interactions (H-bonding) have not been considered. The above-mentioned ranking can, therefore, be affected if explicit solvent is considered. It is worth mentioning, however, that in our previous work we also simulated a TiO₂ surface covered by a water monolayer in order to simulate an explicit water mediated adsorption.⁴⁷ Results showed that, for GLY, PCM infers slight changes with respect to the gas-phase. Nonetheless, for the non-GLY systems, stronger effects arising from explicit solvation are expected, in particular for those cases possessing acidic or basic lateral chains, which in water can be protonated or deprotonated, depending on the environmental pH. Putting this argument on a solid ground, however, merits a



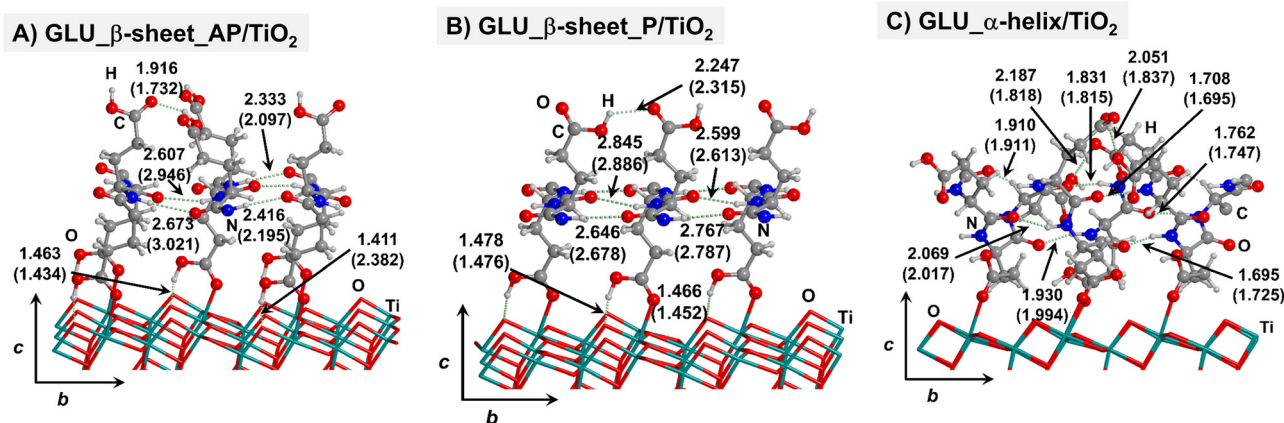


Fig. 3 PBE-D2* optimized structures of antiparallel (a) and parallel (b) polyglutamic acid β -sheets, and polyglutamic acid α -helix (c) adsorbed on the TiO_2 (101) anatase surface. Numbers in parenthesis refer to values in implicit solvation, while numbers without parenthesis refer to values in the gas phase. Bond lengths are in Å.

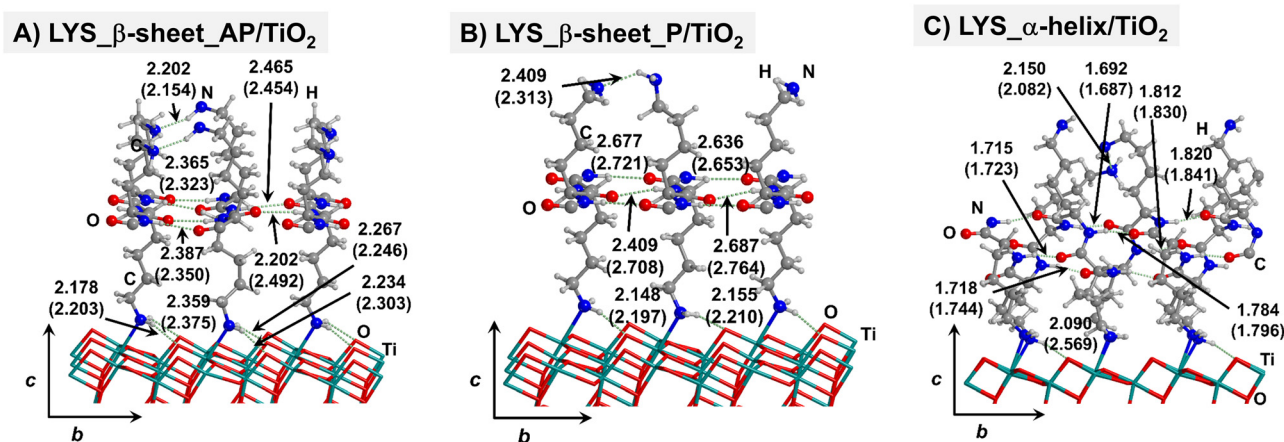


Fig. 4 PBE-D2* optimized structures of antiparallel (a) and parallel (b) polylysine β -sheets, and polylysine α -helix (c) adsorbed on the TiO_2 (101) anatase surface. Numbers in parenthesis refer to values in implicit solvation, while numbers without parenthesis refer to values in the gas phase. Bond lengths are in Å.

separate and extensive study. That is, each system should be studied individually in the presence of a complete solvation sphere and performing AIMDs with long timescales to take into account all the possible polypeptide/solvent/surface degrees of freedom. Such simulations are currently unaffordable and would require cheaper methodologies.

Table 2 reports the relative stability between the α -helix and β -sheets structures of the polypeptide model systems, both in their isolated and adsorbed states. Considering the isolated structures in gas phase, it turns out that, in all the non-GLY cases, the most stable secondary structure is the β -sheet one; for ALA, GLU and LYS adopting the antiparallel orientation, and for ARG the parallel one.

When implicit solvation is taken into account, for all the cases, the α -helix conformation stabilizes by some amount, although the β -sheet structures still dominate. Depending on the amino acid residue constituting the non-GLY polypeptide, the implicit solvation effect can be much more prominent

(the ARG case is that presenting the largest α -helix stabilisation) but no stability inversion over β -sheet is observed. In contrast, and interestingly, the adsorption on the TiO_2 surface goes mostly into the direction to stabilize the α -helix over β -sheet (also for GLY), which is even more accentuated in PCM. GLU is the only outlaw case, as the parallel β -sheet structure is found to be most stable secondary structure on the surface. Therefore, speaking in general, the adsorption of polypeptide secondary structures on the anatase (101) TiO_2 surface revert the relative stability of the isolated ones, rendering α -helix as the most stable adsorbed state. This surface-induced overstability of the α -helix structures can be explained by accounting for the deformation energy ($\Delta E_{\text{def/unit}}$) of the biological parts upon adsorption. Indeed, α -helix structures present deformation energies that are significantly lower than the β -sheet ones (see Table 1). This is because, as mentioned above, the interaction with the surface induces a significant elongation of the backbone H-bond distances in the β -sheet structures, while in



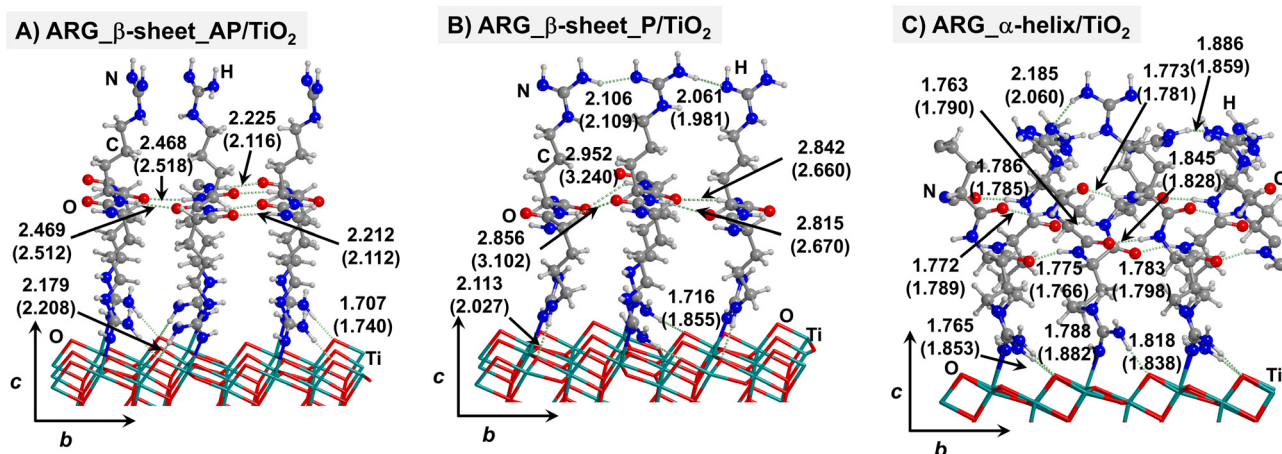


Fig. 5 PBE-D2* optimized structures of antiparallel (a) and parallel (b) polyarginine β -sheets, and polyarginine α -helix (c) adsorbed on the TiO_2 (101) anatase surface. Numbers in parenthesis refer to values in implicit solvation, while numbers without parenthesis refer to values in the gas phase. Bond lengths are in Å.

the α -helix ones they remain almost unperturbed, if not slightly strengthened, and hence the formers are destabilized. Interestingly, the same trend in the deformation energies was observed for GLY (and hence that the α -helix was also found to be more stable than the β -sheet structures), although for this polypeptide, the backbone was actually distorted on the surface because of the direct $\text{C}=\text{O} \cdots \text{Ti}_{5c}$ interactions.

Thus, the deformation of the side chains during the adsorption, and in particular, the degree of variation of the backbone H-bond distances, play a fundamental role in the stabilization of the α -helix structures, in detriment of the β -sheet. The case of GLU, in which the parallel β -sheet has been found to be more stable than the α -helix, can also be explained by the calculated deformation energies. Among the non-GLY systems, GLU is the one presenting the largest (and positive) $\Delta E_{\text{def/unit}}$ value for the α -helix. That is, while for the other systems $\Delta E_{\text{def/unit}}$ values span the 3.8–9.8 range, for GLU it reaches 12.4. Additionally, the β -sheet structures for GLU present a higher H-bond gain on the surfaces than the other non-GLY systems (see values of $\Delta E_{\text{H/unit}}$ of Table 1), as due to the formation of strong H-bonds between the lateral chains. These differences make the parallel β -sheet structure for GLU to be the most stable one on the TiO_2 surface.

Conclusions

In this work, the adsorption and stability of different peptide models (*i.e.*, polyglycine, polyalanine, polyglutamic acid, polylysine and polyarginine) adopting the secondary (α -helix and β -sheet) structures on the (101) TiO_2 anatase surface have been theoretically studied with PBE-D2* periodic simulations, also considering the effect of implicit water solvation (PCM).

At variance with polyglycine (studied in a previous work),⁴⁷ the interaction of the other polypeptide systems with the surface occurs through the lateral chain functional groups, this way keeping almost intact the secondary structure determined

by the H-bond patterns. The interactions are mainly dictated by dative bonds between lateral chain NH_2 (polylysine and polyarginine) and $\text{C}=\text{O}$ (polyglutamic acid) groups and surface Ti_{5c} atoms, or by dispersive interactions between the CH_3 lateral chain (polyalanine) and the surface. Because of the nature of these interactions, and based on the calculated adsorption energies, a trend on the affinity of the polypeptide systems with the anatase (101) surface has been established, which is (from higher to lower affinity): polylysine \approx polyarginine $>$ polyglutamic acid $>$ polyglycine \approx polyalanine. The inclusion of water implicit solvation does not change the affinity scale obtained in gas phase, despite all the interaction energies become significantly reduced.

The most stable secondary structure on TiO_2 is the α -helix, with the exception of polyglutamic acid, preferring the β -sheet.

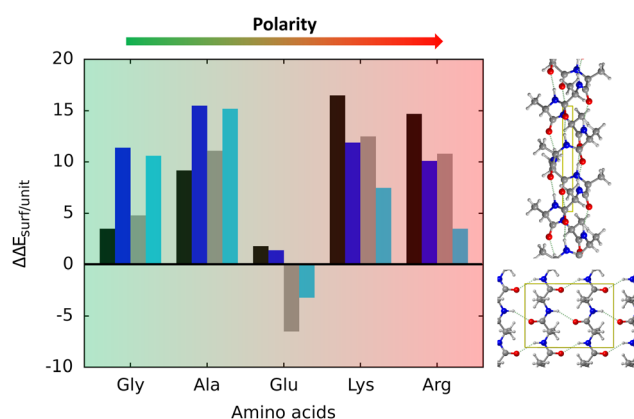


Fig. 6 Graphical summary of all the poly amino acidic systems adsorbed on the (101) anatase TiO_2 . $\Delta\Delta E_{\text{surf/unit}}$ (in kJ mol^{-1}) is calculated according to the following reaction: $\text{AA-}\alpha\text{-helix/TiO}_2 \rightarrow \text{AA-}\beta\text{-sheet}_{\text{AP}}/\text{TiO}_2$ and $\text{AA-}\alpha\text{-helix/TiO}_2 \rightarrow \text{AA-}\beta\text{-sheet}_{\text{P}}/\text{TiO}_2$, where AA corresponds to the amino acids reported on the x axis. Black/grey bars correspond to values calculated in gas phase, while dark/light blue bars in pcm. Black and dark blue bars refer to α -helix \rightarrow antiparallel β -sheet, while grey and light blue bars to α -helix \rightarrow parallel β -sheet.



A graphical summary of all the simulated adsorption processes is shown in Fig. 6. It has been found that the relative stabilities are dictated by the deformation energy of the structures upon adsorption, lower for the α -helix compared to the β -sheet because, in the latter, the adsorption induces a weakening of the backbone H-bond network, not occurring in the former. For the case of polyglutamic acid, the β -sheet folding is more stable because additional H-bonds can be established among side chains, this way providing an extra-stabilization of this structure.

All the results reported in the previous section, even if obtained on model systems, and without considering entropic effects, may give interesting insights at an atomistic level. Indeed, TiO₂ (101) anatase nanoparticles may induce the formation and/or stabilization of specific polypeptide folded secondary structures. Our results indicate that α -helix and β -sheet structures presented in this work are more stable (having larger adsorption energies) and much well-defined on the anatase surface in comparison to polyglycine, for which the deformation of the backbone is larger with respect to other amino acids studied (Ala, Glu, Lys, Arg). This is due to the fact that in the case of polyglycine the backbone is in direct contact with the surface, while for the other amino acids the interaction is mediated by the side chains, thus leaving the secondary structure undistorted. Results from this study may provide atomistic clues on the role of TiO₂ anatase surface on relevant processes such as Ab fibrillation, one of the hallmarks of Alzheimer's disease,^{30,31,66} as well as on the formation of peptides and their conformation in prebiotic chemistry.^{67,68}

Author contributions

Conceptualization: AR, MS. Data curation: SP, AR. Formal analysis: SP, AR. Funding acquisition: MS. Writing – original draft: SP. Writing – review & editing: AR, MS, PU.

Conflicts of interest

There are no conflicts to declare.

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References

- R. J. Leatherbarrow and A. R. Fersht, *Protein Eng.*, 1986, **1**, 7–16.
- R. E. Offord, *Protein Eng.*, 1987, **1**, 151–157.
- C. Xu, D. Tobi and I. Bahar, *J. Mol. Biol.*, 2003, **333**, 153–168.
- S. Park, T. Yokoyama, N. Shibayama, Y. Shiro and J. R. H. Tame, *J. Mol. Biol.*, 2006, **360**, 690–701.
- L. Vitagliano, A. Vergara, G. Bonomi, A. Merlino, C. Verde, G. Prisco, B. D. Howes, G. Smulevich and L. Mazzarella, *J. Am. Chem. Soc.*, 2008, **130**, 10527–10535.
- E. C. Moreno, K. Varughese and D. I. Hay, *Calcif. Tissue Int.*, 1979, **28**, 7–16.
- K. Makrodimitris, D. L. Masica, E. T. Kim and J. J. Gray, *J. Am. Chem. Soc.*, 2007, **129**, 13713–13722.
- M. Ndao, J. T. Ash, N. F. Breen, G. Goobes, P. S. Stayton and G. P. Drobny, *Langmuir*, 2009, **25**, 12136–12143.
- D. L. Masica and J. J. Gray, *Biophys. J.*, 2009, **96**, 3082–3091.
- S. Deechongkit, H. Nguyen, E. T. Powers, P. E. Dawson, M. Gruebele and J. W. Kelly, *Nature*, 2004, **430**, 101–105.
- C. N. Pace, B. A. Shirley, M. McNutt and K. Gajiwala, *FASEB J.*, 2017, **10**, 75–83.
- J. J. H. Sinfelt, *Surf. Sci.*, 2002, **500**, 923–946.
- G. Ertl, M. Weiss and S. B. Lee, *Chem. Phys. Lett.*, 2013, **589**, 18–20.
- R. Schlögl, *Angew. Chem., Int. Ed.*, 2003, **42**, 2004–2008.
- B. Hammer and J. K. Nørskov, *Adv. Catal.*, 2000, **45**, 71–129.
- G. Ertl, *Adv. Catal.*, 2000, **45**, 1–69.
- B. Kasemo, *Surf. Sci.*, 2002, **500**, 656–677.
- V. Puddu and C. C. Perry, *ACS Nano*, 2012, **6**, 6356–6363.
- V. Puddu and C. C. Perry, *Langmuir*, 2014, **30**, 227–233.
- Z. Zhuang, A. I. Jewett, S. Kuttimalai, G. Bellesia, S. Gnanakaran and J. Shea, *Biophys. J.*, 2011, **100**, 1306–1315.
- D. Aili, K. Enander, J. Rydberg, I. Lundström, L. Baltzer and B. Liedberg, *J. Am. Chem. Soc.*, 2006, **128**, 2194–2195.
- D. Aili, K. Enander, L. Baltzer and B. Liedberg, *Nano Lett.*, 2008, **8**, 2473–2478.
- J. M. Slocik, A. O. Govorov and R. R. Naik, *Nano Lett.*, 2011, **11**, 701–705.
- A. Altunbas, N. Sharma, M. S. Lamm, C. Yan, R. P. Nagarkar, J. P. Schneider and D. J. Pochan, *ACS Nano*, 2010, **4**, 181–188.
- J. E. Baio, A. Zane, V. Jaeger, A. M. Roehrich, H. Lutz, J. Pfaendtner, G. P. Drobny and T. Weidner, *J. Am. Chem. Soc.*, 2014, **136**, 15134–15137.
- L. A. Capriotti, T. P. Beebe and J. P. Schneider, *J. Am. Chem. Soc.*, 2007, **129**, 5281–5287.
- A. Rimola, M. Aschi, R. Orlando and P. Ugliengo, *J. Am. Chem. Soc.*, 2012, **134**, 10899–10910.
- G. Wachtershauser, *Proc. Natl. Acad. Sci. U. S. A.*, 1990, **87**, 200–204.
- G. D. Cody, N. Z. Boctor, T. R. Filley, R. M. Hazen, J. H. Scott, A. Sharma and J. Yoder, *Science*, 2000, **289**, 1337–1339.
- W. H. Wu, X. Sun, Y. P. Yu, J. Hu, L. Zhao, Q. Liu, Y. Fen Zhao and Y. Mei Li, *Biochem. Biophys. Res. Commun.*, 2008, **373**, 315–318.
- L. Fei and S. Perrett, *Int. J. Mol. Sci.*, 2009, **10**, 646–655.
- R. Nelson, M. R. Sawaya, M. Balbirnie, A. Madsen, C. Riekel, R. Grothe and D. Eisenberg, *Nature*, 2005, **435**, 773–778.
- I. K. Robinson and D. J. Tweet, *Rep. Prog. Phys.*, 1992, **55**, 599–651.



- 34 C. Wu, A. B. Kjanikaev, R. Adato, N. Arju, A. A. Yanik, H. Altug and G. Shvets, *Nat. Mater.*, 2012, **11**, 69–75.
- 35 O. H. Willemsen, M. M. E. Snel, A. Cambi, J. Greve, B. G. De Grooth and C. G. Figdor, *Biophys. J.*, 2000, **79**, 3267–3281.
- 36 J. J. Gray, *Curr. Opin. Struct. Biol.*, 2004, **14**, 110–115.
- 37 J. Xu, N. Dayan, A. Goldbourt and Y. Xiang, *Proc. Natl. Acad. Sci. U. S. A.*, 2019, **116**, 5493–5498.
- 38 F. Deligey, M. A. Frank, S. H. Cho, A. Kirui, F. Mentink-Vigier, M. T. Swilius, B. T. Nixon and T. Wang, *Biomacromolecules*, 2022, **23**(6), 2290–2301.
- 39 M. E. H. El Nokab, M. H. Habib, Y. A. Alassmy, M. M. Abduljawad, K. M. Alshamrani and K. O. Sebakhy, *Polymers*, 2022, **14**(5), 1049.
- 40 A. Rimola, Y. Sakhno, L. Bertinetti, M. Lelli, G. Martra and P. Ugliengo, *J. Phys. Chem. Lett.*, 2011, **2**, 1390–1394.
- 41 A. Andersen, P. N. Reardon, S. S. Chacon, N. P. Qafoku, N. M. Washton and M. Kleber, *Langmuir*, 2016, **32**, 6194–6209.
- 42 A. C. Deymier, A. K. Nair, B. Depalle, Z. Qin, K. Arcot, C. Drouet, C. H. Yoder, M. J. Buehler, S. Thomopoulos, G. M. Genin and J. D. Pasteris, *Biomaterials*, 2017, **127**, 75–88.
- 43 A. C. T. Van Duin, S. Dasgupta, F. Lorant and W. A. Goddard, *J. Phys. Chem. A*, 2001, **105**, 9396–9409.
- 44 A. Calzolari, G. Cicero, C. Cavazzoni, R. Di Felice, A. Catellani and S. Corni, *J. Am. Chem. Soc.*, 2010, **132**, 4790–4795.
- 45 R. Di Felice and S. Corni, *J. Phys. Chem. Lett.*, 2011, **2**(13), 1510–1519.
- 46 M. D. Piane, M. Corno, R. Orlando, R. Dovesi and P. Ugliengo, *Chem. Sci.*, 2016, **7**, 1496–1507.
- 47 S. Pantaleone, A. Rimola, P. Ugliengo and M. Sodupe, *J. Chem. Inf. Model.*, 2021, **61**, 5484–5498.
- 48 G. Kresse and J. Hafner, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 1993, **47**, 558–561.
- 49 G. Kresse and J. Hafner, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 1994, **49**, 14251–14269.
- 50 G. Kresse and J. Furthmüller, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 1996, **54**, 11169–11186.
- 51 G. Kresse and J. Furthmüller, *Comput. Mater. Sci.*, 1996, **6**, 15–50.
- 52 J. Perdew, K. Burke and M. Ernzerhof, *Phys. Rev. Lett.*, 1996, **77**, 3865–3868.
- 53 S. Grimme, *J. Comput. Chem.*, 2006, **27**, 1787–1799.
- 54 S. Grimme, *J. Comput. Chem.*, 2004, **25**, 1463–1473.
- 55 B. Civalleri, C. M. Zicovich-Wilson, L. Valenzano and P. Ugliengo, *CrystEngComm*, 2008, **10**, 368–376.
- 56 L. Gundelach, T. Fox, C. S. Tautermann and C. K. Skylaris, *Phys. Chem. Chem. Phys.*, 2021, **23**, 9381–9393.
- 57 M. Cutini, I. Bechis, M. Corno and P. Ugliengo, *J. Chem. Theory Comput.*, 2021, **17**, 2566–2574.
- 58 G. Kresse and D. Joubert, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 1999, **59**, 1758–1775.
- 59 K. Mathew, R. Sundararaman, K. Letchworth-Weaver, T. A. Arias and R. G. Hennig, *J. Chem. Phys.*, 2014, **140**, 084106.
- 60 K. Mathew, V. S. C. Kolluru, S. Mula, S. N. Steinmann and R. G. Hennig, *J. Chem. Phys.*, 2019, **151**, 234101.
- 61 P. Ugliengo, D. Viterbo and G. Chiari, *Z. Kristallogr. – Cryst. Mater.*, 1993, **207**, 9–23.
- 62 W. Humphrey, A. Dalke and K. Schulten, *J. Mol. Graphics*, 1996, **14**, 33–38.
- 63 POV-Ray, The Persistence of Vision Raytracer, <http://www.povray.org/>.
- 64 S. Pantaleone, A. Rimola and M. Sodupe, *J. Phys. Chem. C*, 2017, **121**, 14156–14165.
- 65 S. Pantaleone, A. Rimola and M. Sodupe, *Phys. Chem. Chem. Phys.*, 2020, **22**, 16862–16876.
- 66 A. Fardanesh, S. Zibaie, B. Shariati, F. Attar, F. Rouhollah, K. Akhtari, K. Shahpasand, A. A. Saboury and M. Falahati, *Int. J. Nanomed.*, 2019, **14**, 901–911.
- 67 S. Pantaleone, P. Ugliengo, M. Sodupe and A. Rimola, *Chem. – Eur. J.*, 2018, **24**, 16292–16301.
- 68 G. Martra, C. Deiana, Y. Sakhno, I. Barberis, M. Fabbiani, M. Pazzi and M. Vincenti, *Angew. Chem., Int. Ed.*, 2014, **53**, 4671–4674.

