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Biocompatible non-leachable antimicrobial polymers with a nonionic hyperbranched backbone and phenolic terminal units†

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This work aimed to develop biocompatible non-leachable antimicrobial polymers without ionic structures. A series of nonionic hyperbranched polymers (HBPs) with an isatin-based backbone and phenolic terminal units were synthesized and characterized. The molecular structures and thermal properties of the obtained HBPs were characterized by SEC, NMR, FTIR, TGA and DSC analyses. Disk diffusion assay revealed significant antibacterial activity of the obtained phenolic HBPs against nine different pathogenic bacteria. The presence of a methoxy or long alkyl group close to the phenolic unit enhanced the antibacterial effect against certain Gram positive and negative bacteria. The obtained nonionic HBPs were blended in polyester poly(hexamethylene terephthalate) films, which showed no noticeable leakage after being immersed in water for 5 days. Finally, these HBPs showed no cytotoxicity effect to MG-63 osteoblast-like human cells according to MTT analysis, and negligible hemolytic effect.

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Introduction

Antimicrobial polymers (APs) have attracted growing attention recently, due to their high efficacy and selectivity, as well as low risk for leaching or lower skin permeation compared to small molecular antimicrobials.^{1–4} In the past decade, a significantly growing number of APs has been approved by the Food and Drug Administration, which highlights the importance and translational potential of this class of materials.^{5–8} Most APs are ionic, which interact with bacterial membranes by ionic interactions.^{9–18} However, the relatively high water solubility of ionic polymers could be a disadvantage for certain applications such as coatings or additives.^{19–21} Therefore, nonionic APs have attracted growing interest particularly in the development of new coating or additives for various materials applications.^{22,23}

Nonionic APs usually interfere with bacteria by certain non-ionic interactions with bacterial membranes (*e.g.* by hydrogen bonding, hydrophobic interactions, or aromatic interactions *etc.*).^{24–28} To enable such interactions, a particularly attractive

strategy is to utilize naturally occurring antimicrobial molecules (*e.g.* aspirin, indole, isatin, *etc.*), which can interact with bacteria. In addition, these molecules have been adopted by the natural ecosystems and thus may have lower environmental impact. This strategy has recently gained increasing attention, and a number of APs with various naturally occurring antimicrobial functionality have been reported, such as those with tropolone, aspirin, curcumin, limonene, astaxanthin, indole, or isatin structures.^{22,29–35}

Phenolic molecules are abundant in nature and many of them are natural antimicrobials, such as phenol,³⁶ catechol,³⁷ guaiacol (a lignin fragment),³⁸ pyrogallol,³⁹ and cardanol derivatives (*e.g.* hydro-cardanol from cashew nut shell liquid).^{40,41} These phenolic molecules are potentially attractive building blocks for the design of new nonionic APs.^{42–44} Various phenolic thermoplastic and thermosetting polymers with antibacterial function have been reported, of which the antimicrobial effect could be measured by various methods (*e.g.* halo zone test, spread plate method, minimum inhibitory concentration, and minimum bactericidal concentration, *etc.*).^{42,45–49} Bio-composites with grafted phenols have also been reported with significant antibacterial activity against various Gram-positive and negative bacteria.⁴³

Highly branched polymers such as dendrimers or hyperbranched polymers (HBPs) form a particularly important class of APs, which have a large number of densely grafted functional groups that can interact with bacteria synergistically.^{22,25,50–53} This can thus enhance their antimicrobial effect.^{50,54–63} In addition, their near spherical structures could enhance the solubility and facilitate their processing in solutions (*e.g.* by spin coating).⁶⁴

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To our knowledge, the potential of dendritic polymers with phenol termini as new antimicrobial materials have not been investigated.

Herein, we report on the synthesis of four potentially bio-based nonionic HBPs with isatin-based backbone and four different phenolic groups (*i.e.* phenol, catechol, guaiacol and hydro-cardanol) by a one-step polymerization of an isatin-based AB₂ monomer followed by grafting various phenol units. The molecular and thermal properties of the obtained phenolic HBPs were characterized, and their antibacterial properties were evaluated and compared to that of small molecular agents. The leaching risk and cytotoxicity of the obtained polymers were also investigated.

Experimental

Materials

4-Hydroxybenzaldehyde (98%), vanillin (99%), syringaldehyde (98%), 2-oxindole (97%), methyl 2-bromoacetate (>97%), mesitylene (98%), dibutyltin oxide (DBTO) (>98%), 1,6-hexanediol (97%), 1,5-pentanediol (>97%), 1,4-butanediol (>99%), 1,3-propanediol (>98%) and sodium sulfate (Na₂SO₄) were purchased from Sigma-Aldrich. Glacial acetic acid (99.8%), hydrochloric acid (37%), *N,N*-dimethylformamide (DMF, ACS, Reag. Ph. Eur.) and ethyl acetate (EtOAc, ACS, Reag. Ph. Eur.) and *n*-heptane were purchased from VWR Chemicals. Methanol was purchased from Honeywell. Chloroform (Analytical grade, stabilized with ethanol) and xylene (Analytical grade, ACS) were purchased from Scharlau. All chemicals and reagents were used as received.

Synthesis

AB₂ Monomer 3. To a 100 mL round-bottom flask equipped with a magnetic stirrer and a reflux condenser, isatin (2.41 g, 16.9 mmol, 1.00 eq.), **2** (4.07 g, 20.2 mmol, 1.20 eq.), K₂CO₃ (3.50 g, 30.3 mmol, 1.50 eq.), and 50 mL MeCN were added and stirred at 83 °C. After 14 h, the reaction mixture was cooled to room temperature, and the solvent was removed under reduced pressure. The residual solid mixture was dissolved in 250 mL EtOAc, washed with water (3 × 50 mL), dried over MgSO₄, and concentrated under reduced pressure. The crude product was purified by recrystallization from ethanol to orange needle-like crystals with a yield of 89%. ¹H NMR (400.13 MHz, DMSO-d₆) δ, ppm: 7.69 (td, 1H), 7.55 (dd, 1H), 7.33 (d, 1H), 7.26 (tq, 2H), 7.14 (td, 1H), 6.92 (tt, 1H), 6.89 (dq, 2H), 4.22 (t, 2H), and 4.08 (t, 2H). ¹³C NMR (100.61 MHz, DMSO-d₆) δ, ppm: 183.48, 158.13, 150.96, 138.37, 137.65, 128.89, 128.87, 127.07, 125.51, 123.70, 117.56, 110.19, 41.88, and 33.74. FT-IR ν (cm⁻¹): 1745 (C=O str.), 1727 (C=O str.), 1613 (Ar C–C str.), 1470 (Ar C–CH in-plane bend. + Ar C–C str.), 1325 (Ar CCH in-plane bend. + C–N str. + Ar C–C str.), 1095 (Ar C–C str. + Ar C–CH in-plane bend. + Ar C–C str.), 751 (Ar C–H out-of-plane bend).

HBP1. TFSA (2.36 mL, 27.0 mmol, 10.0 eq.) was added dropwise to a solution of monomer **3** (0.710 g, 2.70 mmol, 1.00 eq.) in DCM (0.5 mL) placed in a capped 5 mL vial, and the reaction mixture was stirred at room temperature for 15 h.

Afterwards, half of the reaction mixture was saved for the *in situ* synthesis of **HBP-H** (described later), and the other half was directly quenched with methanol (200 mL), forming precipitates that were collected by filtration. The resulting precipitates were re-dissolved in DCM and then precipitated in 200 mL methanol. The precipitates were filtrated, washed with methanol (3 × 50 mL), and dried under vacuum at 50 °C for 24 h, yielding a light-orange solid (0.580 g, 88%). SEC in chloroform, *M*_n = 16.2 × 10³ g mol⁻¹, *M*_w = 33.7 × 10³ g mol⁻¹, PDI = 2.08. ¹H NMR (400.13 MHz, DMSO-d₆) δ, ppm: 7.69–7.42 (br. 2H), 7.42–6.90 (br. 4H), 6.90–6.65 (br. 2H), 4.13 (br. 2H), 4.00 (br. 2H), and 3.36 (br. 3H). ¹³C NMR (100.61 MHz, DMSO-d₆) δ, ppm: 183.48, 177.35, 158.19, 150.95, 142.22, 140.73, 138.38, 136.91, 130.71, 129.04, 128.72, 126.77, 126.17, 125.45, 124.94, 123.67, 122.84, 117.55, 110.22, 61.85, 50.94, 41.84, and 33.43. FT-IR ν (cm⁻¹): 1737, 1712, 1609, 1467, 1351, and 1169.

HBP-P. To a solution of monomer **3** (0.570 g, 2.10 mmol, 1.00 eq.) in DCM (1 mL) in a capped 5 mL vial, TFSA (1.33 mL, 14.2 mmol, 7.00 eq.) was added dropwise, and the reaction mixture was stirred at room temperature for 15 h. Afterwards, TFSA (0.380 mL, 4.20 mmol, 2.00 eq.) and phenol (0.400 mL, 4.20 mmol, 2.00 eq.) were sequentially added, and the reaction vial was re-capped and kept stirring at room temperature for another 24 h. The crude reaction mixture was then poured into 200 mL methanol, and the resulting precipitate was collected by filtration, washed with excess of methanol, and dried at 50 °C under vacuum for 24 h, yielding **HBP-P** as an off-white solid (0.740 g, 74%). SEC (DMAc), *M*_n = 5700 g mol⁻¹, *M*_w = 9900 g mol⁻¹, PDI = 1.74. ¹H NMR (400.13 MHz, DMSO-d₆) δ, ppm: 9.39 (br. 2H), 7.30–6.60 (br. 16H), and 4.14 (br. 4H). ¹³C NMR (100.61 MHz, DMSO-d₆) δ, ppm: 183.48, 177.35, 158.19, 150.95, 142.22, 140.73, 138.38, 136.91, 130.71, 129.04, 128.72, 126.77, 126.17, 125.45, 124.94, 123.67, 122.84, 117.55, 110.22, 61.85, 50.94, 41.84, and 33.43. FT-IR ν (cm⁻¹): 1737, 1712, 1609, 1467, 1351, and 1169.

HBP-C. To a solution of monomer **3** (0.580 g, 2.20 mmol, 1.00 eq.) in DCM (1 mL) in a capped 5 mL vial, TFSA (1.34 mL, 15.4 mmol, 7.00 eq.) was added dropwise, and the reaction mixture was stirred at room temperature for 15 h. Afterwards, TFSA (0.400 mL, 4.40 mmol, 2.00 eq.) and catechol (0.480 g, 4.40 mmol, 2.00 eq.) were sequentially added, and the reaction vial was re-capped and kept stirring at room temperature for another 24 h. Afterwards, the reaction mixture was poured into 200 mL methanol, and stirred for another 1 h. The resulting suspension was concentrated under vacuum until about half volume, and then poured into 200 mL diethyl ether. The resulting precipitate was collected by filtration, washed with diethyl ether (3 × 50 mL), dried under vacuum at 50 °C for 24 h, yielding **HBP-C** as an off-white solid (0.720 g, 68%). ¹H NMR (400.13 MHz, DMSO-d₆) δ, ppm: 8.87 (br. 4H), 7.30–6.30 (br. 14H), and 4.13 (br. 4H). ¹³C NMR (100.61 MHz, DMSO-d₆) δ, ppm: 183.48, 177.35, 158.19, 150.95, 142.22, 140.73, 138.38, 136.91, 130.71, 129.04, 128.72, 126.77, 126.17, 125.45, 124.94, 123.67, 122.84, 117.55, 110.22, 61.85, 50.94, 41.84, and 33.43. FT-IR ν (cm⁻¹): 1737, 1712, 1609, 1467, 1351, and 1169.

HBP-G. To a DCM (1 mL) solution of monomer **3** (0.530 g, 2.00 mmol, 1.00 eq.), TFSA (1.22 mL, 14.0 mmol, 7.00 eq.) was



added and stirred at room temperature in a capped 5 mL vial. After 15 h, TFSA (0.350 mL, 4.00 mmol, 2.00 eq.), and guaiacol (0.430 mL, 4.00 mmol, 2.00 eq.) in DCM (1.50 mL) were sequentially added and the reaction vial re-capped. After 24 h at room temperature, the crude product was poured into 200 mL methanol, and the resulting precipitate was collected by filtration. After dissolving the solid in DCM, the organic solution was precipitated in 200 mL methanol, filtrated and washed with methanol. Drying at 50 °C during 24 h under vacuum produced **HBP-G** as an off-white solid (0.750 g, 75%). SEC in chloroform, $M_n = 10.6 \times 10^3 \text{ g mol}^{-1}$, $M_w = 15.9 \times 10^3 \text{ g mol}^{-1}$, PDI = 1.50. ^1H NMR (400.13 MHz, DMSO- d_6) δ , ppm: 8.96 (br. 2H), 7.30–6.30 (br. 14H), 4.14 (br. 4H), 3.64 (br. 3H), and 3.49 (br. 3H). ^{13}C NMR (100.61 MHz, DMSO- d_6) δ , ppm: 183.48, 177.35, 158.19, 150.95, 142.22, 140.73, 138.38, 136.91, 130.71, 129.04, 128.72, 126.77, 126.17, 125.45, 124.94, 123.67, 122.84, 117.55, 110.22, 61.85, 50.94, 41.84, and 33.43. FT-IR ν (cm^{-1}): 1737, 1712, 1609, 1467, 1351, and 1169.

HBP-H. To a solution of monomer **3** (0.710 g, 2.70 mmol, 1.00 eq.) in DCM (0.5 mL), in a capped 5 mL vial, TFSA (1.67 mL, 18.9 mmol, 7.00 eq.) was added dropwise, and the resulting reaction mixture was stirred at room temperature for 15 h. Afterwards, half of the reaction mixture was directly used for the *in situ* synthesis of **HBP-H**. TFSA (1 mL) and a solution of 3-hydro-cardanol (1.48 g, 4.40 mmol) in DCM (4 mL) were sequentially added, and the reaction vial was capped. After stirring at room temperature for 24 h, the crude reaction mixture was poured into 200 mL methanol, and the resulting precipitate was collected by filtration, re-dissolved in DCM, and re-precipitated in 200 mL methanol. The precipitate was filtrated, washed with methanol ($3 \times 50 \text{ mL}$), and dried under vacuum at 50 °C for 24 h to yield an off-white solid as **HBP-H** (1.36 g, 74%, based on half of the starting material **3**). SEC in chloroform, $M_n = 46.5 \times 10^3 \text{ g mol}^{-1}$, $M_w = 126 \times 10^3 \text{ g mol}^{-1}$, PDI = 2.71. ^1H NMR (400.13 MHz, CDCl_3) δ , ppm: 9.61 (br. 2H), 7.40–6.00 (br. 14H), 4.09 (br. 4H), 2.52–2.35 (br. 4H), 1.57–1.42 (br. 4H), 1.27 (br. 48H), and 0.89 (br. 6H). ^{13}C NMR (100.61 MHz, CDCl_3) δ , ppm: 183.48, 177.35, 158.19, 150.95, 142.22, 140.73, 138.38, 136.91, 130.71, 129.04, 128.72, 126.77, 126.17, 125.45, 124.94, 123.67, 122.84, 117.55, 110.22, 61.85, 50.94, 41.84, and 33.43. FT-IR ν (cm^{-1}): 1737, 1712, 1609, 1467, 1351, and 1169.

Measurements

Nuclear magnetic resonance (NMR) measurements were carried out on a Bruker DRX400 spectrometer at the proton frequency of 400.13 MHz and carbon frequency of 100.61 MHz. Fourier transform infrared (FTIR) spectra were measured with an attenuated total reflection (ATR) setup using a Bruker Alpha FT-IR spectrometer. Twenty-four scans were co-added using a resolution of 4 cm^{-1} . Size exclusion chromatography (SEC) in chloroform was performed with a Viscotek 305 TDA at 35 °C with a flow rate of 1.0 mL min^{-1} , which included a guard column and two Malvern Panalytical general purpose mixed bed columns with an exclusion limit of $20 \times 10^6 \text{ Da}$ for polystyrene. Detection consisted of a conventional dual cell refractive index detector, a four-capillary bridge viscometer, and a light scattering detector operating at 3 mW, at a wavelength of 670 nm, and measurements

angles of 90° and 7°. The three detectors were calibrated with a polystyrene standard (96 kDa) from Polymers Laboratories. Molecular weights were determined by the triple detection method using the OmiSEC 5.12. software (Malvern). Size exclusion chromatography (SEC) in DMAc was performed using Agilent 1100/1200 Infinity HPLC System equipped with three columns (GPC column PSS GRAM 3000 Å, $10 \mu\text{m}$; GPC column PSS GRAM 1000 Å, $10 \mu\text{m}$; GPC column PSS GRAM 30 Å, $10 \mu\text{m}$) connected in sequence at 40 °C in DMAc with LiBr (5 g L^{-1}) at a flow rate of 1 mL min^{-1} . Calibration was carried out with ReadyCal-Kit poly(methyl methacrylate) standards $M_p = 202\text{--}2200 \text{ kDa}$. Differential scanning calorimetry (DSC) measurements were performed using TA Instruments DSC Q2000. The samples were studied with a heating rate of 10 °C min^{-1} under nitrogen with a purge rate of 50 mL min^{-1} . The sequence consisted of a heating ramp from 40 to 300 °C and held at that temperature for 30 s, followed by a cooling ramp to -50 °C and held at that temperature for 3 min, and finally a heating ramp to 300 °C, which was employed to determine the glass transition temperature (T_g). Thermogravimetric analysis (TGA) was performed with a thermogravimetric analyzer TA Instruments Q500 at a heating rate of 10 °C min^{-1} under nitrogen with a purge rate of 50 mL min^{-1} . Water contact angle (θ) was measured in a picture (taken with a Nikon Bellows PB-6 camera) of a single water droplet placed onto the dry polymer film.

Antimicrobial bioassay

Bacteria culture. Nine pathogenic microorganisms including *Escherichia coli* ATCC 25922 (Ec), *Staphylococcus aureus* ATCC 25923 (Sa), *Proteus mirabilis* ATCC 14153 (Pm), *Proteus vulgaris* ATCC13315 (Pv), *Pseudomonas aeruginosa* ATCC 27853 (Pa), *Enterobacter aerogenes* ATCC13048 (Ea), *Bacillus thuringiensis* (Bt), *Salmonella typhimurium* SL 1344 (St) and *Streptococcus mutans* ATCC 25175 (Sm) were used to determine the antibacterial properties of monomer **3**, **HBP1**, **HBP-P**, **HBP-C**, **HBP-G**, and **HBP-H**. All bacteria strains were sub-cultured on (Luria Bertoni) LB agar culture at 37 °C for 24 h.

Disc diffusion assay. The antimicrobial properties of the prepared compounds against the bacteria were evaluated by a disc diffusion method according to the literature.⁶³ First, the tested samples ($25 \mu\text{g mL}^{-1}$) were dissolved in DMF (**3**, **HBP1**, **HBP-C**, **HBP-P** and **HBP-G**) or chloroform (**HBP-H**). Susceptibility of microorganisms' culture was adjusted by 0.5 McFarland as a reference standard. Microorganism culture suspension ($100 \mu\text{L}$, $10^6 \text{ cells per mL}$) was swabbed onto a plate with Müller-Hinton agar. Filter discs (diameter: 6 mm) were placed on the Petri plate inoculated with microorganisms. Afterward, $20 \mu\text{L}$ of the prepared sample solutions were loaded on the sterile discs. Pure solvents (DMF or chloroform) were used as negative control. The disc containing gentamicin and streptomycin ($25 \mu\text{g per disc}$) was compared to the prepared $25 \mu\text{g mL}^{-1}$ of polymers as a positive control. The Petri plates within bacteria cultures were incubated at 37 °C for 24 h. All experiments were performed in triplicate. The results were expressed as the mean diameter of inhibition zone in $\text{mm} \pm \text{standard deviation}$ (mean \pm SD). Significant differences between two groups of data were



evaluated as p values by t -test using Microsoft Excel. $p < 0.05$ indicates significant difference, while $p \geq 0.05$ indicates insignificant difference.

MTT assay

The MG-63 human osteoblast-like cells were cultured in Dulbecco's Modified Eagle Media (DMEM) supplemented with 10% fetal bovine serum (FBS), 1% penicillin, and 1% streptomycin in a humidified incubator at 37 °C. The medium was replaced every 2 days. Cells were trypsinized and centrifuged at 400g for 4 min to get a concentrated cell pellet when the confluence reached 80%. 1×10^4 cells per well were seeded on a 96-well plate and cultured for 24 h before adding the materials. Test compounds (monomer **3**, and HBPs) dissolved in DMSO (10 mg mL^{-1} , 5 mg mL^{-1} , 1 mg mL^{-1}) were then added to the cells at a final DMSO concentration of 1% (v/v). Fresh culture medium only with 1% DMSO (v/v) was used as negative control, and each sample was replicated in four wells. After being cultured for 24 h, the cell culture medium was discarded and the cells were washed with phosphate buffer. MTT working solution (0.5 mg mL^{-1}) was added to the cells and incubated for 2 h at 37 °C, after which DMSO ($200 \mu\text{L well}^{-1}$) was added to the reaction products for 10 min. The solubilized contents were pipetted and transferred into a clear bottom 96-well plate. Absorbance was determined by spectrophotometry at 600 nm wavelength. To evaluate the possible interaction between polymers and MTT working solution, a control experiment was conducted by using only polymers under same conditions without adding cells.

Hemolysis tests

The HaemoScan Biomaterial Haemolytic Assay (HaemoScan, Netherlands) was used to investigate the cytotoxicity of the monomer **3** and all polymers on human erythrocytes according to the manufacturer's protocol.⁶⁵ Briefly, the erythrocyte was prepared by repeatedly rinsing with different wash buffer (Dilution buffer I, II and III, provided by the manufacturer) and centrifuged at $400 \times g$ for 10 min. Afterward, 5 mL of the Dilution buffer III was added to re-suspend the erythrocytes. 0.5 mL erythrocyte suspension was used to test each sample. The samples were first dissolved in DMSO to form 10 mg mL^{-1} stock solutions. 5 μL of the stock solution was added in 0.5 mL erythrocyte suspension with a final (suspension) concentration of $100 \mu\text{g mL}^{-1}$ for polymers. After 24 h of incubation, the samples were centrifuged at $4500 \times g$ for 1 min and 20 μL of the supernatant pipetted into a 96-well plate along with 180 μL of assay buffer. The absorbance was read at a wavelength of 450 nm. Each polymer has been tested triplicate. DMSO (5 μL , 1% v/v) was used as the negative control (0% hemolysis). Lysis buffer was used as the positive control (100% hemolysis). The hemolysis percentage was calculated by following equation.⁶⁶

Hemolysis %

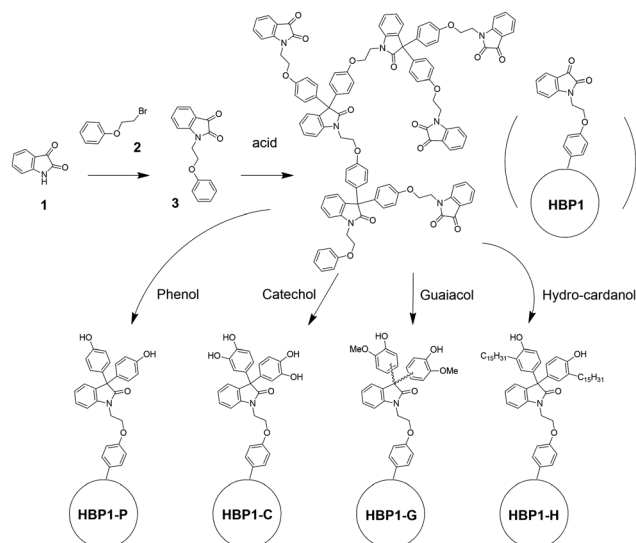
$$= \frac{\text{OD}_{450}(\text{Sample}) - \text{OD}_{450}(\text{negative control})}{\text{OD}_{450}(\text{positive control}) - \text{OD}_{450}(\text{negative control})} \times 100\%$$

Results and discussion

Synthesis and characterization of HBPs

AB₂-monomer **3** was synthesized by a straightforward S_N2 reaction of isatin **1** and β -bromophenethole **2** in 89% yield (Scheme 1). Both starting molecules are potentially bio-based. Isatin (**1**) is widely produced in nature, and its derivatives frequently display biological activities including antimicrobial properties.⁶⁷ The other starting molecule, β -bromophenethole (**2**), can be conveniently obtained by bromination of phenoxyethanol, which is also a bio-based molecule derived from phenol and ethylene carbonate.⁶⁸ Phenoxyethanol is also widely used in industry as solvent, synthetic intermediate, and fixing agent for perfumes.⁶⁹ Monomer **3** is an AB₂ monomer for acid-catalysed Friedel–Crafts type polymerizations (the phenyl group can react twice with the carbonyl group in each monomer),^{70–72} which can yield a non-crosslinked hyperbranched polymer structure with diaryloxindoles backbone.^{73,74} AB₂ monomer **3** was polymerized according to a previously reported polymerization protocol for a similar monomer,⁶³ which was performed at room temperature without solvent, yielding the desired isatin-based precursor **HBP1** after a simple precipitation from methanol. Afterward, **HBP1** was reacted with the phenolic compounds as grafting agents (*i.e.* phenol, catechol, guaiacol and hydro-cardanol), yielding the four corresponding phenolic HBPs (**HBP-P**, **HBP-C**, **HBP-G** and **HBP-H**, respectively).

The chemical structures of the obtained HBPs were characterized by ¹H NMR spectroscopy in either CDCl₃ or DMSO-d₆, depending on their solubility (Fig. 1 and 2). ¹H NMR spectra of monomer **3**, **HBP1**, **HBP-P**, **HBP-C** and **HBP-G** were measured in DMSO-d₆ (Fig. 1). **HBP-H** was insoluble in DMSO-d₆, and its ¹H NMR spectrum was measured in CDCl₃ instead (Fig. 2). First, all the signals for monomer **3** in DMSO-d₆ were unambiguously assigned (Fig. 1(A)). The triplets at 4.08 and 4.22 ppm



Scheme 1 Synthesis of bio-based AB₂ monomer **3**, isatin-based precursor polymer (**HBP1**) and four phenolic HBPs, including **HBP-P** (with phenol), **HBP-C** (with catechol), **HBP-G** (with guaiacol), and **HBP-H** (with hydro-cardanol).



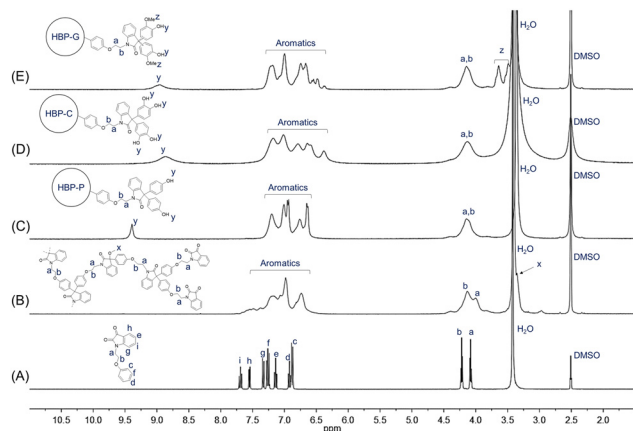


Fig. 1 ^1H NMR spectra of (A) monomer **3**, (B) **HBP1**, (C) **HBP-P**, (D) **HBP-C**, and (E) **HBP-G** in $\text{DMSO}-d_6$. **HBP-H** was insoluble in $\text{DMSO}-d_6$, so its ^1H NMR spectrum was measured in CDCl_3 and compared to that of monomer **3** and **HBP1** in CDCl_3 (Fig. 2).

(*a* and *b*, respectively) were assigned to the methylene protons ($-\text{CH}_2-$). All the aromatic signals were also clearly assigned (*c-i*). When the ^1H NMR spectrum of monomer **3** was measured in CDCl_3 , similar peaks were observed with minor changes in the chemical shifts of the peaks (Fig. 2(A)). After the polymerization of monomer **3**, the ^1H NMR spectrum of the resulting **HBP1** in $\text{DMSO}-d_6$ displayed broader signals, which indicated the occurrence of polymerization (Fig. 1(B)). The protons on the ethylene bridges (*a* and *b*) displayed overlapping resonances at 4.13 and 4.00 ppm, respectively. In addition, a new signal (*x*) appeared at 3.36 ppm (overlapping with the water peak), which was more discernible in the ^1H NMR spectrum in CDCl_3 at 3.54 ppm (*x*, Fig. 2(B)). This signal was attributed to the OCH_3 groups in the polymer structures, which were formed by quenching the intermediate tertiary OH groups (partial reactions during polymerization) with methanol.^{63,75} The aromatic proton signals of **HBP1** were broadened and overlapped at 6.74–7.69 ppm in Fig. 1(B) and 6.45–7.65 ppm in Fig. 2(B).

The conversion of **HBP1** into **HBP-P**, **HBP-C**, **HBP-G** and **HBP-H** gave rise to characteristic phenolic proton signals at 9.39, 8.87, and 8.96 (*y*, Fig. 1(C)–(E)), and 9.61 ppm (*y*, Fig. 2(C), inset), respectively. Furthermore, the most downfield aromatic signals for **HBP1** (7.42–7.69 ppm in Fig. 1(B) and 7.43–7.65 ppm in Fig. 2(B)) was not observed in the ^1H NMR spectra of the phenolic HBPs (Fig. 1(C)–(E) and 2(C)), which indicated the complete consumption of precursor polymer **HBP1** after the phenolic grafting reactions. Moreover, the signal corresponded to the OCH_3 groups due to methanol quenching in **HBP1** (*x* in Fig. 1(B) and 2(B)) was not observed after the phenolic functionalization. This was consistent with the fact that these phenolic HBPs were synthesized *in situ* from monomer **3** without methanol quenching for **HBP1**. The ^1H NMR spectrum of **HBP-G** in Fig. 1(E) displayed extra broad signals at 3.49–3.64 ppm (*z*), which were associated with the methoxy protons in the terminal guaiacol groups. Finally, the up-field signals at 0.89, 1.27, 1.46, and 2.40 ppm in the ^1H NMR spectrum of **HBP-H** (Fig. 2(C)) corresponded to

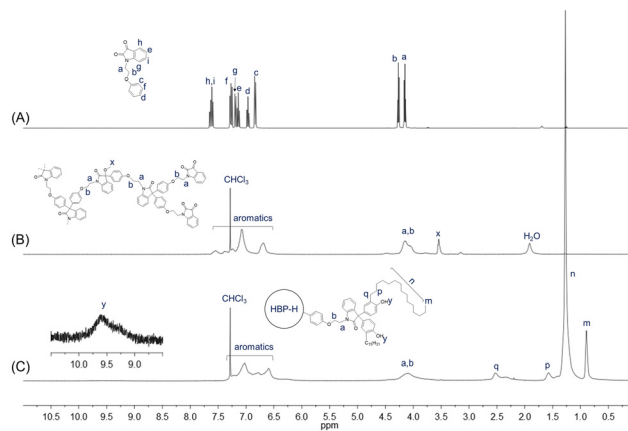


Fig. 2 ^1H NMR spectra of (A) monomer **3**, (B) **HBP1**, and (C) **HBP-H** in CDCl_3 . The inset in (C) showed the signal for phenolic group (*g*).

the aliphatic protons in the terminal hydro-cardanol units (*m*, *n*, *p* and *q*, respectively).

The degree of branching (DB) of **HBP1** was evaluated according to the ^1H NMR signal intensities that corresponded to the linear, dendritic, and terminal units (Fig. S1, ESI†). The DB values of **HBP1** was calculated as 0.51 (calculations shown in ESI†), which suggested that the carbonyl group of AB_2 monomer **3** showed almost the same reactivity as its intermediate with OH group.⁷⁶ This is different from some other reported isatin-based AB_2 monomers, which has much higher reactivity for the second reaction step.^{77,78} The DB values of the phenolic HBPs were expected to remain the same as that of **HBP1**, because they were prepared by post-polymerization functionalization of **HBP1** without changing the backbone. Unfortunately, quantification of the DB values for the phenolic HBPs was unsuccessful due to the difficulty in finding discernible signals corresponding to linear units in the ^1H NMR spectra.

The chemical structures of the new HBPs were further confirmed by FTIR spectroscopy. In the high wave number region (Fig. 3(A)), a broad O–H stretching band was observed at $3570\text{--}3130\text{ cm}^{-1}$ in the FTIR spectra of all the four phenolic HBPs, which was absent in the spectra of monomer **3** and **HBP1**. This confirmed the presence of phenolic OH groups in the polymers, which indicated the success of grafting reactions. In the carbonyl region (Fig. 3(B)), the two carbonyl groups of monomer **3** (1 and 2, Fig. 3(B)) showed an overlapped broad signal centred at $\sim 1728\text{ cm}^{-1}$, which was consistent with other reported isatin derivatives.⁷⁹ After the polymerization of **3**, the resulting **HBP1** showed an additional $\text{C}=\text{O}$ stretching band at 1715 cm^{-1} , which corresponded to the reacted isatin moieties in the backbone (**3**). The unreacted terminal isatin carbonyl units (1 and 2) displayed as a shoulder in the FTIR spectrum. After the phenolic grafting reactions of **HBP1**, the shoulder corresponded to the terminal carbonyl groups (1 and 2) in the FTIR spectrum of **HBP1** disappeared, which confirmed the complete consumption of terminal isatin moieties after phenolic grafting. In addition, a new $\text{C}=\text{O}$ stretching band appeared at $1697\text{--}1671\text{ cm}^{-1}$ in the FTIR spectra of all the phenolic HBPs, which corresponded to the carbonyl group in the resulting



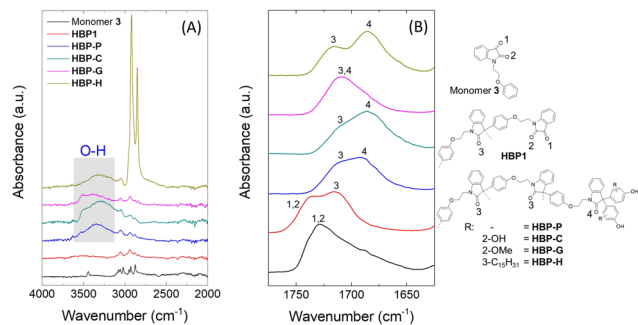


Fig. 3 FTIR spectra of monomer **3** and HBPs in the regions of (A) 4000–2000 cm^{-1} and (B) 1775–1625 cm^{-1} . Numerals 1–4 represent the different carbonyl groups.

diaryloxindole units (4). This also independently confirmed the success of phenolic grafting.

The molecular weight of **HBP1** was conveniently measured by SEC in chloroform ($M_n \sim 16$ kDa and $M_w \sim 34$ kDa, Table 1). After the phenolic grafting, **HBP-H** with long alkyl groups remain soluble in chloroform. SEC results indicated significantly increased molecular weight of **HBP-H** ($M_n \sim 46.5$ kDa and $M_w \sim 126.0$ kDa) compared to its precursor **HBP1**, which is due to the grafted mass. The other three phenolic HBPs were insoluble or only partially soluble in chloroform or DMAc (the two commonly used SEC solvents in our group), but their soluble fraction was measured anyway to provide some insight. **HBP-G** was partially soluble in chloroform, and the SEC measurement of its soluble fraction showed apparently lower molecular weight than that of precursor **HBP1** (Table 1), which indicated that only the low molecular weight fraction was soluble and high molecular weight fraction was insoluble and filtered off prior to SEC measurements. **HBP-P** was completely insoluble in chloroform, but was partially soluble DMAc. According to the SEC results in DMAc, a relatively low molecular weight was obtained (Table 1), which could also be due to the loss of insoluble high molecular weight fraction in DMAc by filtration prior to the SEC measurements. **HBP-C** was completely insoluble in chloroform or DMAc, which were the two solvents allowed for our SEC instruments, so its molecular weight was not measured. The SEC traces of these tested polymers are shown in Fig. S2 (ESI†).

Thermal properties of the obtained HBPs were characterized by DSC and TGA measurements. According to the DSC results,

Table 1 Molecular characterization and thermal properties of the obtained HBPs. M_n , M_w , and D were determined by SEC in chloroform (for **HBP1**, **HBP-G** and **HBP-H**) or DMAc (for **HBP-P**). T_d is the temperature for the maximum decomposition rate, according to TGA derivative curves. Char yield (CY) was obtained by TGA. **HBP-C** was not measured by SEC due to insolubility

HBP	M_n (kDa)	M_w (kDa)	D	T_g ($^{\circ}\text{C}$)	T_5 ($^{\circ}\text{C}$)	T_d ($^{\circ}\text{C}$)	CY (%)
HBP1	16.2	33.7	2.08	188	366	419	42
HBP-P	5.70	9.90	1.73	242	335	409	39
HBP-C	—	—	—	234	353	405	36
HBP-G	10.6	15.9	1.51	200	236	409	33
HBP-H	46.5	126.0	2.71	127	263	430	10

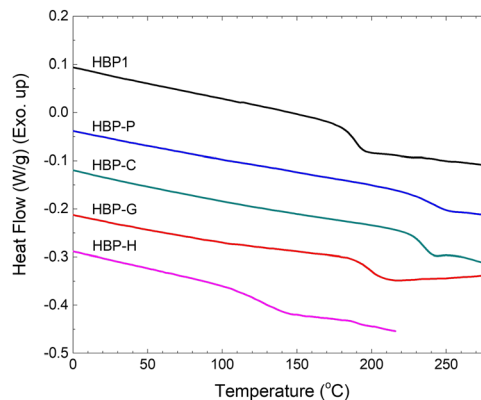


Fig. 4 DSC curves of HBPs (second heating).

the T_g value of **HBP1** was 188 $^{\circ}\text{C}$ (Fig. 4 and Table 1). After phenolic grafting, the resulting HBPs with solely hydroxyl end-groups (*i.e.* **HBP-P** and **HBP-C**) showed higher T_g values ($T_g \sim 242$ and 234 $^{\circ}\text{C}$, respectively) due to the increased rigidity and hydrogen bonding. The T_g value of **HBP-G** ($T_g \sim 200$ $^{\circ}\text{C}$) was higher than that of **HBP1**, but lower than that of **HBP-P** and **HBP-C**. This could be related to the additional flexibility imparted by the methoxy groups of **HBP-G**, which somewhat counter-balanced the enhanced T_g by the increased rigidity and hydrogen bonding endowed by the phenolic units. When even longer aliphatic alkyl chain was incorporated (*i.e.* **HBP-H**), a rather low T_g (~ 127 $^{\circ}\text{C}$) was observed, which was caused by the lubricating effect of the flexible aliphatic alkyl chain. All the HBPs were amorphous under the conditions studied without melting endotherm in the DSC heating curves (Fig. 4).

All the obtained HBPs showed fairly high thermal stability according to TGA measurements (Fig. 5 and Table 1). The initial thermal decomposition temperature (T_5 , Table 1) for all the polymers was above 230 $^{\circ}\text{C}$, and the temperature for the maximal decomposition rate (T_d) was higher than 400 $^{\circ}\text{C}$. In addition, the char yield (CY) at 800 $^{\circ}\text{C}$ for all the HBPs was in the range of 33–42%, except for **HBP-H** (CY $\sim 10\%$). These high CY values could be related to their high aromatic content, which suggested possible inherent flame retardance.^{80,81} The exceptionally low CY of **HBP-H** could be attributed to its relatively low aromatic content due to the presence of long alkyl units.^{82,83}

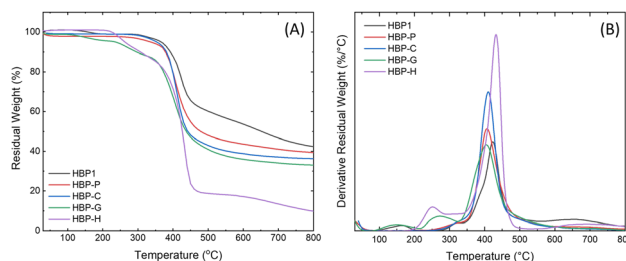


Fig. 5 TGA (A) residual weight and (B) derivative weight loss curves of HBPs.



Film casting and leaching evaluation

The short-time leaching risk of the obtained HBPs from a polymer matrix was preliminarily evaluated by measuring the UV-vis absorption of the aqueous phase after the polymer films blended with HBPs were immersed in water for 5 days. Poly(hexamethylene terephthalate) (PHT, $M_n \sim 13$ kDa, $M_w \sim 21$ kDa) was selected as the matrix for leaching investigations, which is softer than PET and suitable for various applications,^{84–86} particularly bicomponent fibres in nonwoven textiles.⁸⁷ Another potential advantage of PHT is that it is synthesized using 1,6-hexanediol, which could be readily produced from various bio-resources.^{88,89} In this work, PHT powder was synthesized according to our previously reported procedure.^{90,91} The thin films of pure PHT or PHT blended with HBPs were prepared according to a solution-casting protocol.^{92,93} The films of pure PHT or PHT with **HBP1** or **HBP-H** were cast from their chloroform solutions (50 mg mL⁻¹). The PHT films with **HBP-P** and **HBP-G** were cast from their HFIP solutions (50 mg mL⁻¹). PHT film with **HBP-C** could not be prepared due to solubility limitations. **HBP-C** was only soluble in DMSO or DMF, but insoluble in many other commonly used organic solvents for film casting (e.g. chloroform, HFIP, etc.). However, PHT was insoluble in DMSO or DMF. Therefore, there was no common solvent that could dissolve both PHT and **HBP-C**. All the prepared films were immersed in water for 5 days, and the aqueous phase was measured by UV-vis spectroscopy. As shown in Fig. 6, none of the PHT films with HBPs (**HBP1**, **HBP-P**, **HBP-G**, and **HBP-H**) showed noticeable UV-vis absorbance, indicating their non-leachable nature from the polymer films within 5 days. On the contrary, the aqueous phase with the immersed PHT film containing monomer **3** showed significant UV-vis absorption after 5 days, indicating its leakage. This provided a preliminary insight into the non-leaching risk of the obtained polymers in pure water. In the future, it would be interesting to investigate the leaching risks under more specific chemical environment (e.g. pH, salt) for a particular application. Finally, the water contact angles of these PHT films were measured (Fig. S3, ESI[†]), which showed a general increase of

hydrophobicity of the PHT films upon blending with HBPs. Particularly, the PHT film blended with **HBP-H** was the most hydrophobic, which was consistent with the presence of hydrophobic long alkyl chains in **HBP-H**.

Antibacterial activity

The antibacterial activity of the obtained HBPs was evaluated by a straightforward disk diffusion assay (example images in Fig. S4, ESI[†]). The target bacteria include six Gram-negative G(–) bacteria (*Proteus mirabilis*, *Pseudomonas aeruginosa*, *Proteus vulgaris*, *Enterobacter aerogenes*, and *Salmonella typhimurium*, and *Escherichia coli*) and three Gram-positive G(+) bacteria (*Staphylococcus aureus*, *Bacillus thuringiensis* and *Streptococcus mutans*). First, the isatin-functionalized polymer **HBP1** and its corresponding monomer **3** were compared. As shown in Fig. S5 (ESI[†]), **HBP1** showed significantly larger zones of inhibition than monomer **3** for two G(–) bacteria *Ec* and *St* ($p < 0.05$, Table S1, ESI[†]). For the other four tested G(–) bacteria and all the three G(+) bacteria, **HBP1** showed comparable size of inhibition zones as monomer **3** ($p > 0.05$). One should notice that **HBP1** as a polymer has considerably lower solubility and molecular diffusion rate in disk diffusion measurements, yet it showed comparable or even larger zone of inhibition compared to monomer **3**. This indicated the strong antimicrobial effect of **HBP1**, which could be attributed to the synergistic interaction with bacteria by the densely grafted isatin groups in **HBP1**.^{63,94} It should be noted that the zones of inhibition in this work should not be simply compared to those ones we presented in our previous work about another series of isatin-functionalized polymers, due to the different solvents used for sample loading.⁶³ The only exception is **HBP-H**, for which the same solvent (chloroform) was used for sample loading as in our previous work (into the paper disc prior to antimicrobial tests). In general, the inhibition zones of **HBP-H** were smaller than those of the isatin-functionalized polymers in our previous work. This might be related to the higher molecular weight of **HBP-H**, which could reduce its diffusion rate during antimicrobial experiments.^{26,63}

Next, the antibacterial effects of the obtained HBPs (including monomer **3**) were compared to that of two commercial small molecular antibiotics, streptomycin and gentamicin. For simplicity, only those with significant differences ($p < 0.05$, Table S1, ESI[†]) are shown in Fig. 7 and 8. In general, monomer **3** and HBPs exhibited stronger activity ($\Delta > 0$, $p < 0.05$, Table S1, ESI[†]) against most bacteria compared to streptomycin. There are a few exceptions where comparable effect was observed ($p \geq 0.05$, Table S1, ESI[†]), such as for all the HBPs against G(–) bacterium *Ea* (shown as empty column at the corresponding places in the figure).

The comparison of the obtained HBPs with gentamicin was more complex (Fig. 8). In most cases, no significant difference ($p \geq 0.05$, Table S2, ESI[†]) was observed between their zones of inhibition (indicated as the absence of data column, such as for *Pv*). In a few cases, significantly higher ($\Delta > 0$, $p < 0.05$) or lower ($\Delta < 0$, $p < 0.05$) antimicrobial effects of HBPs (or monomer **3**) were observed compared to that of gentamicin.

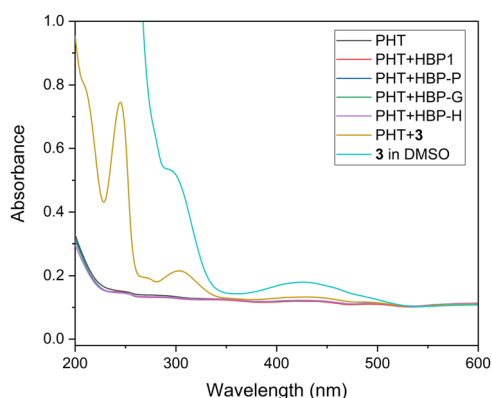


Fig. 6 UV-vis absorbance spectra of the aqueous phase after the pure PHT film or PHT films containing HBPs or monomer **3** were immersed in deionized water for 5 days (photos of the films shown in Fig. S2, ESI[†]). UV-vis absorbance spectrum of monomer **3** in DMSO was presented as a reference.



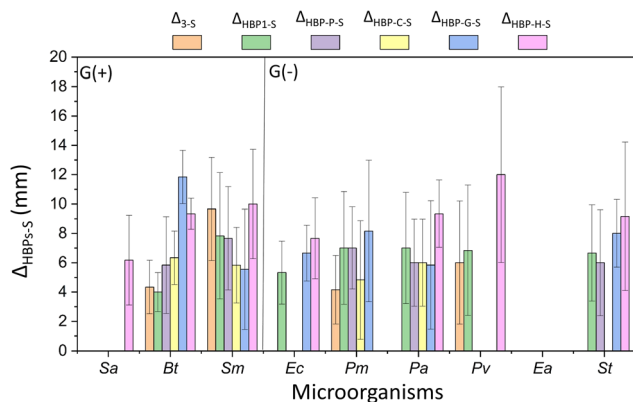


Fig. 7 Difference between the inhibition zones of the obtained polymers (or monomer **3**) and streptomycin (Δ_{x-s} , $x = \mathbf{3}$ or HBPs). Note, only those Δ_{x-s} values with significant differences ($p < 0.05$, Table S1, ESI†) are shown in the figure. Positive Δ_{x-s} values indicate more effective antibacterial effect for the investigated compounds compared with streptomycin. Absence of data column displayed in the corresponding place indicates that the inhibition zones of the monomer **3** or polymer and streptomycin were comparable without significant difference ($p \geq 0.05$, Table S1, ESI†). For instance, there is no data plotted for bacterium *Ea*, which indicates similar antimicrobial effect for this bacterium by the obtained polymers and streptomycin.

For example, **HBP-H** was more effective ($\Delta > 0$, $p < 0.05$, Table S2, ESI†) than gentamicin against two G(+) bacteria (*Sa*, *Bt*) and one G(−) bacterium (*Pa*). **HBP-G** was more effective ($\Delta > 0$, $p < 0.05$, Table S2, ESI†) than gentamicin against one G(+) bacterium *Bt*. Monomer **3** and **HBP-C** were less effective than gentamicin against two G(−) bacteria *Ec* and *St*.

Furthermore, the four obtained phenolic HBPs (*i.e.* **HBP-P**, **HBP-C**, **HBP-G** and **HBP-H**) were compared with the isatin-functionalized **HBP1** in terms of their zones of inhibition

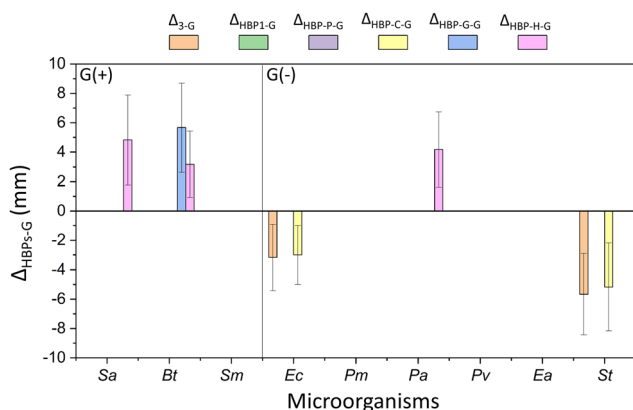


Fig. 8 Comparison of the inhibition zones of HBPs (or monomer **3**) and gentamicin (Δ_{x-g} , $x = \mathbf{3}$ or HBPs). Only those Δ_{x-g} values with significant differences ($p < 0.05$, Table S2, ESI†) are displayed. Positive or negative Δ_{x-g} values indicate stronger or weaker antibacterial effect for the investigated compounds compared with gentamicin, respectively. The absence of data column in the corresponding place indicates that the inhibition zones of the HBPs (or monomer **3**) and gentamicin were comparable ($p \geq 0.05$, Table S2, ESI†). For instance, for bacteria *Pm*, *Pv* and *Ea*, no data column was displayed, which indicated that for these bacteria the antimicrobial effect of the obtained polymers was comparable to that of gentamicin.

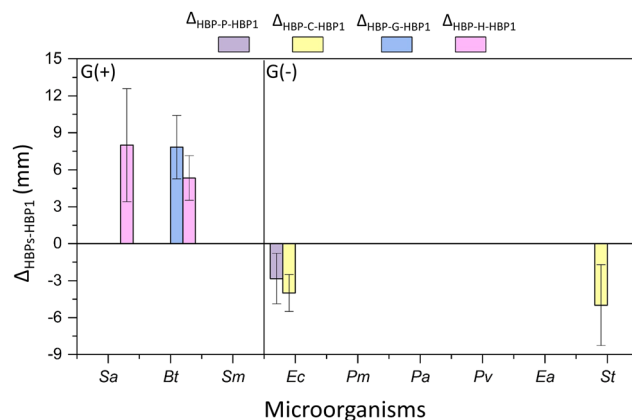


Fig. 9 Difference between the inhibition zones of HBPs and **HBP1** (Δ_{x-HBP1} , $x = \mathbf{HBP-P}$, **HBP-C**, **HBP-G**, or **HBP-H**). Note, only those Δ_{x-HBP1} values with significant differences ($p < 0.05$, Table S3, ESI†) are shown in the figure. Positive Δ_{x-HBP1} values indicate more effective antibacterial effect for the investigated HBPs compared with **HBP1**. Negative Δ_{x-HBP1} values indicate less effective antibacterial effect for the investigated compounds HBPs compared with **HBP1**. Absence of data column displayed in the corresponding place indicates that the inhibition zones of HBPs compared with **HBP1** were comparable without significant difference ($p \geq 0.05$, Table S3, ESI†). For instance, for bacteria *Sm*, *Pm*, *Pa*, *Pv*, and *Ea*, there is no data plotted, which indicates that for these bacteria the effect of the obtained polymers was very similar (no significant difference) to that of **HBP1**.

(Fig. 9). As a result, most phenolic HBPs showed comparable zones of inhibition as **HBP1** (indicated by the absence of data columns in Fig. 9). Interestingly, there were three cases for G(+) bacteria, where significantly larger ($\Delta > 0$, $p < 0.05$) inhibition zones were observed for phenolic HBPs. For instance, **HBP-G** with guaiacol moiety containing methoxy group was more effective ($\Delta > 0$, $p < 0.05$, Table S3, ESI†) than **HBP1** against *Ec*. Similarly, **HBP-H** with hydro-cardanol moiety containing a long alkyl group was more effective than **HBP1** against *Sa* and *Bt*. These observations indicated that the presence of a methoxy or a long alkyl group could enhance the interactions with certain G(+) bacterial membranes. For certain G(−) bacteria, significantly smaller ($\Delta < 0$, $p < 0.05$) inhibition zones were observed for those phenolic HBPs without ether or alkyl groups (*i.e.* **HBP-P** and **HBP-C**). For instance, **HBP-P** showed lower activity against *Ec* than **HBP1**, while **HBP-C** showed lower activity against both *Ea* and *St* than **HBP1**. This could suggest that the ether or alkyl groups of phenolic HBPs could enhance their molecular interaction with the membrane of certain G(−) bacteria, which presumably could be related to their enhanced structural hydrophobicity.^{64,95}

Cytotoxicity

The cytotoxicity to MG-63 osteoblast-like human cells of the obtained monomer **3** and HBPs were evaluated using a standard MTT assay.^{23,96} As illustrated in Fig. 10, the cell viability of monomer **3** at 100, 500 and 1000 $\mu\text{g mL}^{-1}$ were less than 40% (21, 24, and 31% respectively), indicating its significant toxicity to the tested cells. Compared to monomer **3**, all HBPs exhibited significantly higher cell viability. For **HBP-P** and **HBP-H**, the



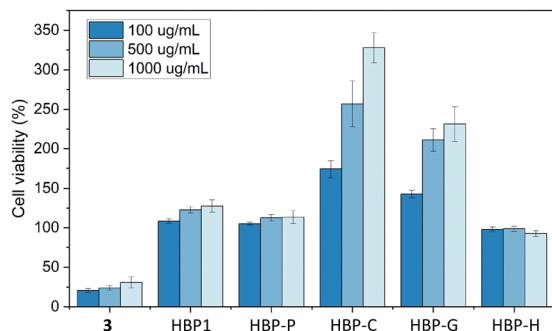


Fig. 10 Cytotoxicity of monomer **3** and HBPs against osteoblast-like human cells at three concentrations (100, 500 and 1000 $\mu\text{g mL}^{-1}$). The results were presented as relative percent viability of the treated cells compared to that of untreated control (100% of cell viability, not shown in the graph).

observed cell viability values were generally in the range of 90–100%, which indicated non-toxicity. For **HBP1**, **HBP-C** and **HBP-G**, the observed cell viability values were higher than 100% with an increasing trend upon increased concentration. This indicated that these polymers not only were non-toxic to MG-63 osteoblast-like human cells, but also could promote their growth. Such a result was consistent with some other previously reported polymeric materials (e.g. chitosan derivatives), which could be desirable for tissue engineering and wound healing applications.^{97–100} To address whether the higher cell viability was related to reaction between polymers and MTT solution, control experiments were performed under the same condition without adding cells. As a result, (Fig. S6, ESI[†]), no significant absorbance was observed at 600 nm with all the three concentrations (as compared to the absorbance for the MTT measurements with cells), indicating no significant interaction with the MTT working solution. The exact reason for the increased cell viability remained to be unravelled. It was reported in the literature that natural polymers like chitosan could mimic the glycosaminoglycan structures in extracellular matrix, and thus could facilitate cell adhesion, migration and proliferation.⁹⁹

More investigations are needed to evaluate whether synthetic HBPs may have similar effect.

Hemolytic activity

The *in vitro* toxicity on human erythrocytes of monomer **3** and all HBPs was evaluated using the Haemoscan Hemolytic Assay (HaemoScanbv, Groningen, Netherlands) according to the manufacturer's protocol.⁶⁵ As shown in Fig. 11, all polymers showed low hemolytic effect (<5%) after 24 h of cultivation with the human erythrocytes, while monomer **3** showed more significant hemolytic effect (~10%). This indicates hemocompatibility of these polymers, which may facilitate potential biomedical applications.

Conclusions

Four aromatic hyperbranched polymers (HBPs) with phenolic terminal groups and isatin-based backbone were synthesized via a facile solvent-free polymerization followed by functionalization with various bio-based phenolic structures. The high aromatic content of the resulting HBPs resulted in high char yields after TGA measurements, which may indicate inherent flame retardancy. As expected, the phenolic HBPs showed significant antibacterial activity against 9 different pathogenic bacteria, as well as negligible leakage from polyester films into water. Interestingly, we discovered that the presence of a methoxy or long alkyl group close to the phenolic unit could enhance the antibacterial effect for certain Gram positive or negative bacteria. Finally, these bio-based HBPs were non-cytotoxic to the MG-63 osteoblast-like human cells, neither did they show any significant hemolytic activity. These results indicated that these new polymers could be potentially suitable antimicrobial materials for various biomedical applications. In the future, synthetic work toward more structural variations is planned to better understand the structure-property relationship of this new class of sustainable antimicrobial materials.

Conflicts of interest

There are no conflicts to declare.

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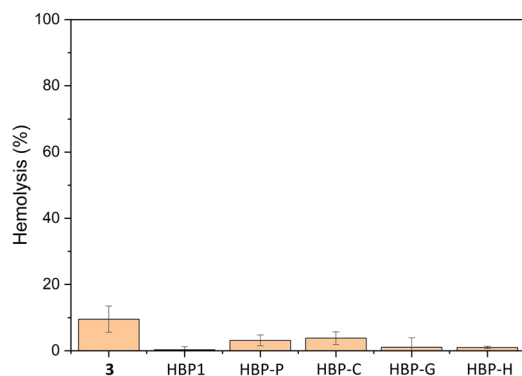


Fig. 11 Hemolytic activity of monomer **3** and HBPs (100 $\mu\text{g mL}^{-1}$). DMSO (1% v/v) was used as the negative control (0% hemolysis). Lysis liquid provided by the manufacture was used as the positive control (100% hemolysis).



References

- 1 K. Peng, T. Zou, W. Ding, R. Wang, J. Guo, J. J. Round, W. Tu, C. Liub and J. Hu, *RSC Adv.*, 2017, **7**, 24903–24913.
- 2 W. Chin, G. Zhong, Q. Pu, C. Yang, W. Lou, P. F. De Sessions, B. Periaswamy, A. Lee, Z. C. Liang, X. Ding, S. Gao, C. W. Chu, S. Bianco, C. Bao, Y. W. Tong, W. Fan, M. Wu, J. L. Hedrick and Y. Y. Yang, *Nat. Commun.*, 2018, **9**, 1–14.
- 3 T. Zhu, Y. Sha, J. Yan, P. Pageni, M. A. Rahman, Y. Yan and C. Tang, *Nat. Commun.*, 2018, **9**, 917.
- 4 A. L. Hook, C. Y. Chang, J. Yang, J. Luckett, A. Cockayne, S. Atkinson, Y. Mei, R. Bayston, D. J. Irvine, R. Langer, D. G. Anderson, P. Williams, M. C. Davies and M. R. Alexander, *Nat. Biotechnol.*, 2012, **30**, 868–875.
- 5 G. N. Tew, R. W. Scott, M. L. Klein and W. F. DeGrado, *Acc. Chem. Res.*, 2010, **43**, 30–39.
- 6 T. Chemistry and S. Review, *Biomacromolecules*, 2007, **8**, 1359–1384.
- 7 I. Banerjee, R. C. Pangule and R. S. Kane, *Adv. Mater.*, 2011, **23**, 690–718.
- 8 F. Siedenbiedel and J. C. Tiller, *Polymers*, 2012, **4**, 46–71.
- 9 D. Raafat and H. Sahl, *Microb. Biotechnol.*, 2009, **2**, 186–201.
- 10 G. Li and J. Shen, *J. Appl. Polym. Sci.*, 2000, 676–684.
- 11 F. Ferrero, M. Periolatto and S. Ferrario, *J. Cleaner Prod.*, 2015, **96**, 244–252.
- 12 V. W. L. Ng, J. P. K. Tan, J. Leong, Z. X. Voo, J. L. Hedrick and Y. Y. Yang, *Macromolecules*, 2014, **47**, 1285–1291.
- 13 N. D. Koromilas, G. C. Lainioti, G. Vasilopoulos, A. Vantarakis and J. K. Kallitsis, *Polym. Chem.*, 2016, **7**, 3562–3575.
- 14 Y. Jiao, L. Niu, S. Ma, J. Li, F. Tay and J. Chen, *Prog. Polym. Sci.*, 2017, **7**, 53–90.
- 15 E.-R. Kenawy and Y. R. Abdel-Fattah, *Macromol. Biosci.*, 2002, **2**, 261–266.
- 16 E. F. Palermo, K. Lienkamp, E. R. Gillies and P. J. Ragnogna, *Angew. Chem., Int. Ed.*, 2019, **58**, 3690–3693.
- 17 A. Kuroki, A. Kengmo Tchoupa, M. Hartlieb, R. Peltier, K. E. S. Locock, M. Unnikrishnan and S. Perrier, *Biomaterials*, 2019, **217**, 119249.
- 18 B. Wang, G. Feng, M. Seifrid, M. Wang, B. Liu and G. C. Bazan, *Angew. Chem., Int. Ed.*, 2017, **56**, 16063–16066.
- 19 R. Costa, J. L. Pereira, J. Gomes, F. Gonçalves, D. Hunkeler and M. G. Rasteiro, *Chemosphere*, 2014, **112**, 177–184.
- 20 K. Lewandowska, *J. Solution Chem.*, 2013, **42**, 1654–1662.
- 21 K. Izutsu and K. Shigeo, *Phys. Chem. Chem. Phys.*, 2000, **2**, 123–127.
- 22 S. Karpagam and S. Guhanathan, *Prog. Org. Coat.*, 2014, **77**, 1901–1910.
- 23 X. Li, I. Sedef, J. A. Linares-pasten, Y. Liu, D. B. Raina, D. Demircan and B. Zhang, *Biomacromolecules*, 2021, **22**, 2256–2271.
- 24 M. B. Patel, S. A. Patel, A. Ray and R. M. Patel, *J. Appl. Polym. Sci.*, 2002, **89**, 895–900.
- 25 D. Demircan and B. Zhang, *Carbohydr. Polym.*, 2017, **157**, 1913–1921.
- 26 E.-R. Kenawy, S. D. Worley and R. Broughton, *Biomacromolecules*, 2007, **8**, 1359–1384.
- 27 W. S. Moon, K. H. Chung, D. J. Seol, E. S. Park, J. H. Shim, M. N. Kim and J. S. Yoon, *J. Appl. Polym. Sci.*, 2003, **90**, 2933–2937.
- 28 L. Martin, P. Gurnani, J. Zhang, M. Hartlieb, N. R. Cameron, A. M. Eissa and S. Perrier, *Biomacromolecules*, 2019, **20**, 1297–1307.
- 29 R. J. Cornell and L. G. Donaruma, *J. Med. Chem.*, 1965, **8**, 388–390.
- 30 L. Erdmann and K. E. Uhrich, *Biomaterials*, 2000, **21**, 1941–1946.
- 31 R. Jabara, N. Chronos and K. Robinson, *Catheter. Cardiovasc. Interv.*, 2008, **72**, 186–194.
- 32 N. Shpaisman, L. Sheihet, J. Bushman, J. Winters and J. Kohn, *Biomacromolecules*, 2012, **13**, 2279–2286.
- 33 H. Tang, C. J. Murphy, B. Zhang, Y. Shen, E. A. Van Kirk, W. J. Murdoch and M. Radosz, *Biomaterials*, 2010, **31**, 7139–7149.
- 34 O. Hauenstein, S. Agarwal and A. Greiner, *Nat. Commun.*, 2016, **7**, 1–7.
- 35 S. Weintraub, T. Shpigel, L. G. Harris, R. Schuster, E. C. Lewis and D. Y. Lewitus, *Polym. Chem.*, 2017, **8**, 4182–4189.
- 36 J. J. Lucchini, J. Corre and A. Cremieux, *Res. Microbiol.*, 1990, **141**, 499–510.
- 37 E. Y. Jeong, J. H. Jeon, C. H. Lee and H. S. Lee, *Food Chem.*, 2009, **115**, 1006–1010.
- 38 H. Liu, B. Lepoittevin, C. Roddier, V. Guérineau, L. Bech, J. M. Herry, M. N. Bellon-Fontaine and P. Roger, *Polymer*, 2011, **52**, 1908–1916.
- 39 K. K. Gaikwad, S. Singh and Y. S. Lee, *J. Coat. Technol. Res.*, 2019, **16**, 147–157.
- 40 M. C. Lubi and E. T. Thachil, *Des. Monomers Polym.*, 2012, **3**, 123–153.
- 41 P. Boonsai, P. Phuwapraisirisan and C. Chanchao, *Int. J. Med. Sci.*, 2014, **11**, 327–336.
- 42 T. Nonaka, Y. Uemura, K. Ohse, K. Jyono and S. Kurihara, *J. Appl. Polym. Sci.*, 1997, **66**, 1621–1630.
- 43 H. M. N. Iqbal, G. Kyazze, I. C. Locke, T. Tron and T. Keshavarz, *Green Chem.*, 2015, **17**, 3858–3869.
- 44 L. Bouarab-Chibane, V. Forquet, P. Lantéri, Y. Clément, L. Léonard-Akkari, N. Oulahal, P. Degraeve and C. Bordes, *Front. Microbiol.*, 2019, **10**, 829.
- 45 K. Huang, X. Fan, R. Ashby and H. Ngo, *Prog. Org. Coat.*, 2021, **155**, 106228.
- 46 K. Huang, R. Ashby, X. Fan, R. A. Moreau, G. D. Strahan, A. Nuñez and H. Ngo, *Prog. Org. Coat.*, 2020, **141**, 105536.
- 47 G. Elegir, A. Kindl, P. Sadocco and M. Orlandi, *Enzyme Microb. Technol.*, 2008, **43**, 84–92.
- 48 A. Nagaraja, Y. M. Puttaiahgowda, A. Kulal, A. M. Parambil and T. Varadavenkatesan, *Macromol. Res.*, 2019, **27**, 301–309.
- 49 E. S. Park, W. S. Moon, M. J. Song, M. N. Kim, K. H. Chung and J. S. Yoon, *Int. Biodeterior. Biodegrad.*, 2001, **47**, 209–214.



- 50 H. Bakhshi, S. Agarwal, T. Hayashi, N. Zhu, X. Ni, Z. Shen, F. Padella, H. Wang, J. Soliveri, R. Gómez and F. J. de la Mata, *J. Mater. Chem. B*, 2017, **5**, 6827–6834.
- 51 D. Konkolewicz, M. J. Monteiro and S. Perrier, *Macromolecules*, 2011, **44**, 7067–7087.
- 52 D. Wang, T. Zhao, X. Zhu, D. Yan and W. Wang, *Chem. Soc. Rev.*, 2015, **44**, 4023–4071.
- 53 P. Zhao, F. Mecozzi, S. Wessel, B. Fieten, M. Driesse, W. Woudstra, H. J. Busscher, H. C. Van Der Mei and T. J. A. Loontjens, *Langmuir*, 2019, **35**, 5779–5786.
- 54 C. Z. Chen and S. L. Cooper, *Biomaterials*, 2002, **23**, 3359–3368.
- 55 S. Sathiyaraj, A. Shanavas, K. A. Kumar, A. Sathiyaseelan, J. Senthilselvan, P. T. Kalaichelvan and A. S. Nasar, *Eur. Polym. J.*, 2017, **95**, 216–231.
- 56 P. Ortega, J. L. Copa-Patiño, M. A. Muñoz-Fernandez, J. Soliveri, R. Gomez and F. J. de la Mata, *Org. Biomol. Chem.*, 2008, **6**, 3264.
- 57 C. Abid and S. Chattopadhyay, *J. Appl. Polym. Sci.*, 2010, **116**, 1640–1649.
- 58 S. Charles, N. Vasanthan, D. Kwon and G. Sekosan, *Tetrahedron Lett.*, 2012, **53**, 6670–6675.
- 59 D. Gangadharan, N. Dhandhala and D. Dixit, *J. Appl. Polym. Sci.*, 2012, **124**, 1384–1391.
- 60 E. Fuentes-Paniagua, J. M. Hernández-Ros, M. Sánchez-Milla, M. A. Camero, M. Maly, J. Pérez-Serrano, J. L. Copa-Patiño, J. Sánchez-Nieves, J. Soliveri, R. Gómez and F. Javier de la Mata, *RSC Adv.*, 2014, **4**, 1256–1265.
- 61 H. Bakhshi and S. Agarwal, *Polym. Chem.*, 2016, **7**, 5322–5330.
- 62 J. Lin, S. Qiu, K. Lewis and A. M. Klivanov, *Biotechnol. Bioeng.*, 2003, **83**, 168–172.
- 63 C. R. Arza, S. Ilk, D. Demircan and B. Zhang, *Green Chem.*, 2018, **20**, 1238–1249.
- 64 X. Li, X. Wang, S. Subramaniyan, Y. Liu, J. Rao and B. Zhang, *Biomacromolecules*, 2022, **23**, 150–162.
- 65 K. V. Nemani, K. L. Moodie, J. B. Brennick, A. Su and B. Gimi, *Mater. Sci. Eng., C*, 2013, **33**, 4453–4459.
- 66 H. Yu, L. Liu, H. Yang, R. Zhou, C. Che, X. Li, C. Li, S. Luan, J. Yin and H. Shi, *ACS Appl. Mater. Interfaces*, 2018, **10**, 39257–39267.
- 67 H. Guo, *Eur. J. Med. Chem.*, 2019, **164**, 678–688.
- 68 P. Ziosi, T. Tabanelli, G. Fornasari, S. Cocchi, F. Cavani and P. Righi, *Catal. Sci. Technol.*, 2014, **4**, 4386–4395.
- 69 Y. Teruo, I. Shigeru and I. Yoshiharu, *Bull. Chem. Soc. Jpn.*, 1973, **46**, 553–556.
- 70 D. A. Klumpp, K. Y. Yeung, G. K. S. Prakash and G. A. Olah, *J. Org. Chem.*, 1998, **63**, 4481–4484.
- 71 J. Khan, A. Tyagi, N. Yadav, R. Mahato and C. K. Hazra, *J. Org. Chem.*, 2021, **86**, 17833–17847.
- 72 H. M. Colquhoun, M. G. Zolotukhin, L. M. Khalilov and U. M. Dzhemilev, *Macromolecules*, 2001, **34**, 1122–1124.
- 73 M. L. Yang, Y. X. Wu, Y. Liu, J. J. Qiu and C. M. Liu, *Polym. Chem.*, 2019, **10**, 6217–6226.
- 74 Y. Zheng, S. Li and C. Gao, *Chem. Soc. Rev.*, 2015, **44**, 4091–4130.
- 75 J.-Y. Chen, Z.-L. Xiang, F. Yu, B. F. Sels, Y. Fu, T. Sun, M. Smet and W. Dehaen, *J. Polym. Sci., Part A: Polym. Chem.*, 2014, **52**, 2596–2603.
- 76 C. J. Hawker, R. Lee and J. M. J. Frechet, *J. Am. Chem. Soc.*, 1991, **113**, 4583–4588.
- 77 M. Smet and E. Schacht, *Angew. Chem., Int. Ed.*, 2002, **41**, 4729–4732.
- 78 Y. Fu, J. Chen, H. Xu, C. Van Oosterwijck, X. Zhang, W. Dehaen and M. Smet, *Macromol. Rapid Commun.*, 2012, **33**, 798–804.
- 79 A. Bigotto and V. Galasso, *Spectrochim. Acta*, 1979, **35**, 725–732.
- 80 X. L. Wang, T. Fu, D. M. Guo, J. N. Wu, X. L. Wang, L. Chen and Y. Z. Wang, *Polym. Chem.*, 2016, **7**, 1584–1592.
- 81 N. Warlin, E. Nilsson, Z. Guo, S. V. Mankar, N. G. Valsange, N. Rehnberg, S. Lundmark, P. Jannasch and B. Zhang, *Polym. Chem.*, 2021, **12**, 4942–4953.
- 82 N. M. Barkoula, B. Alcock, N. O. Cabrera and T. Peijs, *Polym. Polym. Compos.*, 2008, **16**, 101–113.
- 83 S. Sen, S. Patil and D. S. Argyropoulos, *Green Chem.*, 2015, **17**, 4862–4887.
- 84 N. González-Vidal, A. M. de Ilarduya, S. Muñoz-Guerra, P. Castell and M. T. Martínez, *Compos. Sci. Technol.*, 2010, **70**, 789–796.
- 85 N. González-Vidal, A. M. De Ilarduya, V. Herrera and S. Muñoz-Guerra, *Macromolecules*, 2008, **41**, 4136–4146.
- 86 X. Lefèbvre, M. H. J. Koch, H. Reynaers and C. David, *J. Polym. Sci., Part B: Polym. Phys.*, 1999, **37**, 1–18.
- 87 Z. Guo, N. Warlin, S. V. Mankar, M. Sidqi, M. Andersson, B. Zhang and E. Nilsson, *ACS Sustainable Chem. Eng.*, 2021, **9**, 16778–16785.
- 88 E. Kovács, G. Turczel, L. Szabó, R. Varga, I. Tóth, P. T. Anastas and R. Tuba, *ACS Sustainable Chem. Eng.*, 2017, **5**, 11215–11220.
- 89 J. He, S. P. Burt, M. Ball, D. Zhao, I. Hermans, J. A. Dumesic and G. W. Huber, *ACS Catal.*, 2018, **8**, 1427–1439.
- 90 S. V. Mankar, M. N. Garcia Gonzalez, N. Warlin, N. G. Valsange, N. Rehnberg, S. Lundmark, P. Jannasch and B. Zhang, *ACS Sustainable Chem. Eng.*, 2019, **7**, 19090–19103.
- 91 N. Warlin, M. N. Garcia Gonzalez, S. Mankar, N. G. Valsange, M. Sayed, S. H. Pyo, N. Rehnberg, S. Lundmark, R. Hatti-Kaul, P. Jannasch and B. Zhang, *Green Chem.*, 2019, **21**, 6667–6684.
- 92 P. Wang, C. R. Arza and B. Zhang, *Polym. Chem.*, 2018, **9**, 4706–4710.
- 93 C. R. Arza and B. Zhang, *ACS Omega*, 2019, **4**, 15012–15021.
- 94 R. C. Goy, S. T. B. Morais and O. B. G. Assis, *Rev. Bras. Farmacogn.*, 2016, **26**, 122–127.
- 95 T. Nonaka, L. Hua, T. Ogata and S. Kurihara, *J. Appl. Polym. Sci.*, 2003, **87**, 386–393.
- 96 X. Li, S. İlç, Y. Liu, D. B. Raina, D. Demircan and B. Zhang, *Polym. Chem.*, 2022, **13**, 2307–2319.
- 97 B. Duan, X. Yuan, Y. Zhu, Y. Zhang, X. Li, Y. Zhang and K. Yao, *Eur. Polym. J.*, 2006, **42**, 2013–2022.
- 98 W. Y. Chuang, T. H. Young, C. H. Yao and W. Y. Chiu, *Biomaterials*, 1999, **20**, 1479–1487.
- 99 D. O. Zamora, S. Natesan and R. J. Christy, *J. Visualized Exp.*, 2012, 1–7.
- 100 J. Sun, Y. Fan, W. Ye, L. Tian, S. Niu, W. Ming, J. Zhao and L. Ren, *Chem. Eng. J.*, 2021, **417**, 128049.

