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# Last-step $^{18}\text{F}$ -fluorination of supported 2-(aryl-di-*tert*-butylsilyl)-*N*-methyl-imidazole conjugates for applications in positron emission tomography†

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**Aiming for potential applications in positron emission tomography, fully automated productions of  $^{18}\text{F}$ -labelled bioconjugates were achieved using heterogenous precursors obtained by anchoring imidazole-di-*tert*-butyl-arylsilanes to a polystyrene resin. The reactions were performed using either “batch” or “flow” procedures, avoiding both the time-consuming azeotropic drying and HPLC purifications usually required.**

Positron emission tomography (PET) is a powerful imaging technique based on the injection of a radiotracer containing a  $\beta^+$  emitting element.<sup>1</sup> Among the suitable isotopes, fluorine-18 exhibits convenient properties such as a 97% decay by  $\beta^+$  emission (635 keV positrons), a half-life of 109.8 min and the ability to form covalent bonds. For example, [ $^{18}\text{F}$ ]-2-deoxy-2-fluoro-D-glucose ([ $^{18}\text{F}$ ]FDG) has been employed routinely for decades in cancer diagnosis by PET. Looking for efficient and versatile syntheses of biologically specific [ $^{18}\text{F}$ ]tracers, numerous synthetic methods and strategies were developed,<sup>2</sup> such as late-stage  $^{18}\text{F}$ -labelling,<sup>3</sup> “click” conjugations<sup>4</sup> or last-step fluorinations of specific prosthetic groups.<sup>5,6</sup> However, their transfer to clinical applications remains challenging in most cases.<sup>7</sup> Indeed, in addition to the constraints inherent to radiosyntheses, *i.e.* short time of synthesis (production time inferior to 3 half-lives), small scale reactions (typically 10–100 nmol) and the protection of the operator from radiation (reactions performed in closed lead-shielded fumehoods), the procedure should be fully automatable to ensure its reproducibility and operability

by technicians.<sup>1a</sup> Thus, kit-like precursors that can directly deliver the isolated radio-labelled product in one step without cumbersome/time-consuming azeotropic-drying or HPLC-purification steps are greatly preferred. In particular, using precursors grafted on a solid support whose selective cleavage is triggered by the radio-labelling reaction can greatly improve the practicality of the overall process.<sup>8</sup> Indeed, manipulation and packaging of the precursor become more convenient, and it theoretically allows a fast and easy separation of the large excess of the starting material from the radiolabelled tracer using a simple filtration method. When considering the syntheses of PET tracers, simultaneous radio-labelling and cleavage were achieved *via* starting materials anchored on solid supports by either electrostatic interactions, organometallic bonding or covalent linking.<sup>9</sup> For instance, the latter one was applied to the synthesis of a protected [ $^{18}\text{F}$ ]FDG using a resin-linked sulfonate leaving group, but further deprotection was still required to obtain the final radiolabelled product (Scheme 1A(a)).<sup>9f</sup> On the other hand, the last-step  $^{18}\text{F}$ -labelling of supported unprotected substrates still remains extremely challenging. Indeed, heterogeneous reactions lead usually to a reactivity decrease when compared to their homogeneous versions, requiring harsher labelling conditions often non-compatible with sensitive functional groups in biomolecule-based substrates.

Whereas simple [ $^{18}\text{F}$ ]fluoroarenes could be obtained in 3–14% radiochemical yields (RCY) from supported triazene<sup>9a</sup> or iodonium<sup>9i</sup> precursors (Scheme 1A(b and c)), a recent work of Kuhnast *et al.* demonstrated that pyridine-ammonium grafted onto a resin were radiolabelled at room temperature with RCY of 3–8% after filtration on C18 or  $\text{Al}_2\text{O}_3$  cartridges (Scheme 1A(d)).<sup>9f</sup> Interestingly, when linked to a peptide, it also reacted with [ $^{18}\text{F}$ ]F<sup>−</sup> to give in 30 min the desired bioconjugate with a low RCY of 1%, but with an excellent radiochemical purity (RCP) without HPLC purification (>95%).

In this context, we developed recently a new 2-(aryl-di-*tert*-butylsilyl)-*N*-methyl-imidazole tag (Imidazole-Silicon Fluoride Acceptors = ImidSiFA)<sup>10</sup> that could be fluorinated efficiently

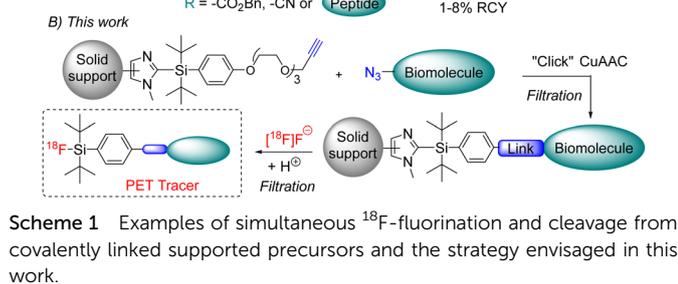
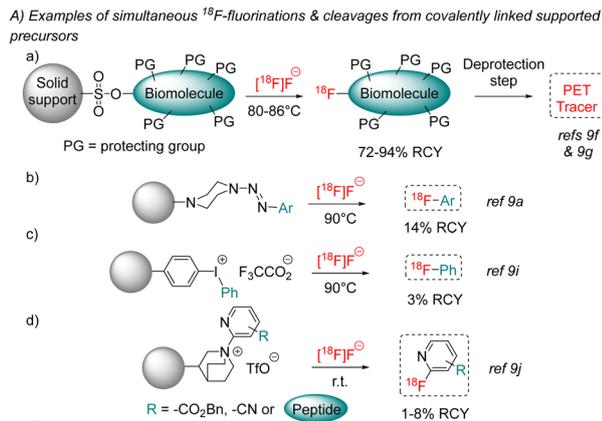
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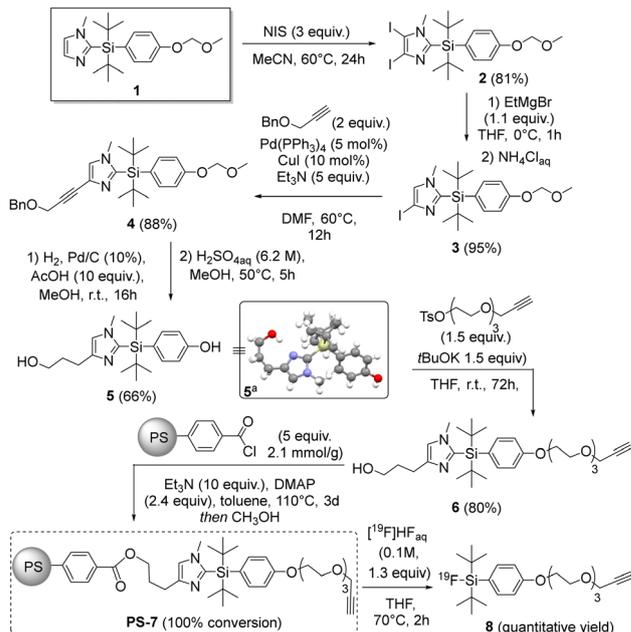
† Electronic supplementary information (ESI) available: Experimental procedures and copies of  $^1\text{H}$ ,  $^{13}\text{C}$ ,  $^{29}\text{Si}$  and  $^{19}\text{F}$  NMR NMR spectra for new compounds. Radio- and UV-HPLC traces for [ $^{18}\text{F}$ ]compounds. CCDC 2169890. For ESI and crystallographic data in CIF or other electronic format see DOI: <https://doi.org/10.1039/d2cc03258a>



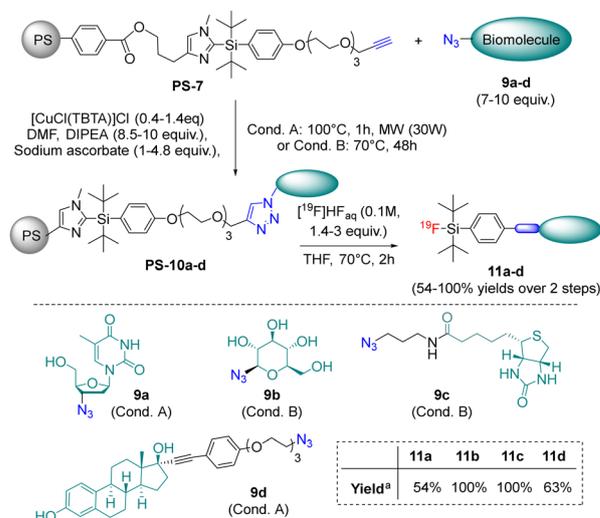


by aqueous  $[\text{}^{18}\text{F}]\text{F}^-$ .<sup>11</sup> Thus, anchoring the imidazole leaving group on a solid support was envisaged as the next step for the full automation of the radiolabelling process. In particular, the possibility to achieve the conjugation after grafting on the solid support was explored using copper-catalysed Huisgen cycloaddition (CuAAC).<sup>12</sup> Indeed, it would enhance the versatility of this method by allowing the preparation of various conjugated precursors from a unique starting resin (Scheme 1B).

Firstly, various pathways were screened to introduce a linking moiety on the imidazole leaving group of the ImidSiFA tag, but post-functionalization of the previously described 2-(4-(methoxymethoxy)phenyl-di-*tert*-butylsilyl)-*N*-methyl-imidazole **1**<sup>10</sup> proved to be the most efficient and reliable one (Scheme 2). Indeed, iodination,<sup>13</sup> Sonogashira coupling hydrogenation led to product **5**, exhibiting unprotected alcohol and phenol moieties (45% yield from **1**). Interestingly, **5** was crystallised and analysed by X-ray diffraction,<sup>‡</sup> which confirmed the highly hindered structure of this silane (Scheme 2). Finally, the phenol was alkylated with a PEG chain functionalized by an alkyne moiety, and product **6** was consecutively anchored by esterification onto a polystyrene resin with benzoyl chloride residues to give the supported precursor **PS-7**. The efficiency of the grafting was confirmed by fluorination of a portion of the resin beads in model conditions with aqueous  $[\text{}^{19}\text{F}]\text{F}^-$  (0.1 M, 1.3 equiv., in THF at 70 °C for 2 h), which yielded quantitatively the corresponding fluorosilane **8** based on the theoretical resin loading of **6**. This highly encouraging result led us to explore the conjugation of the **PS-7** resin by CuAAC with azides present on biomolecule derivatives (Scheme 3). Model molecules containing thymidine, glucose, biotine, and estradiol cores (*i.e.* **9a**, **9b**, **9c** and **9d**, respectively) were selected and engaged in the heterogeneous “click” reaction. After optimisation, a Cu(II)



**Scheme 2** Synthesis of the resin supported ImidSiFA bearing a pendant alkyne moiety and  $^{19}\text{F}$ -labelling in model conditions. <sup>‡</sup>Mercury drawing of the crystalline structure of **5** obtained by X-ray diffraction.

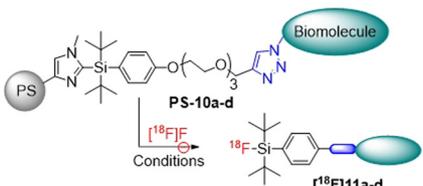
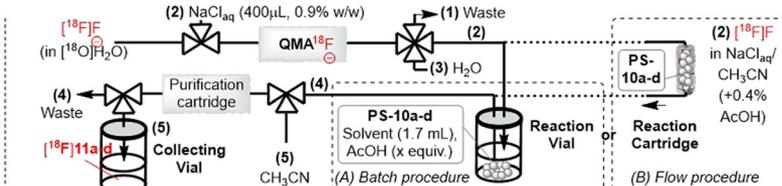


**Scheme 3** Conjugation of the resin supported ImidSiFA **PS-7** and  $^{19}\text{F}$ -labelling in model conditions. <sup>‡</sup>Yields over two steps. For the exact experimental conditions, see the ESI.†

complex with tris(benzyltriazolylmethyl)amine) as ligand (TBTA)<sup>14</sup> was identified as the best catalyst with either classical heating or micro-wave activation depending on the substrate (Scheme 3).

Then, the resulting beads were simply washed and dried, and a fraction of each was subjected to  $^{19}\text{F}$ -fluorination using the model conditions previously described (aqueous HF at 0.1 M in THF for 2 h at 70 °C). In this case, the desired fluorinated bioconjugates were obtained in 54% to 100% yields



Table 1  $^{18}\text{F}$ -Fluorination of supported precursors **PS-10a-d**



| Entry (number of runs)      | Substrate (mass)      | Conditions <sup>a</sup>                                       | RCY of [ $^{18}\text{F}$ ]11 <sup>b</sup> (%) (RCP in %) <sup>c</sup> |
|-----------------------------|-----------------------|---|---|
| 1 <sup>d</sup> ( $n = 1$ )  | <b>PS-10a</b> (5 mg)  | THF (1.7 mL), AcOH (10 equiv.), 100 °C, 15 min                | 8 (81)  |
| 2 <sup>d</sup> ( $n = 1$ )  | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (10 equiv.), 100 °C, 15 min | 16 (67)   |
| 3 <sup>d</sup> ( $n = 1$ )  | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 17 (65)   |
| 4 <sup>d</sup> ( $n = 1$ )  | <b>PS-10a</b> (10 mg) | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 14 (71)   |
| 5 <sup>d</sup> ( $n = 1$ )  | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 30 min | 19 (76)   |
| 6 ( $n = 1$ )               | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 12 (97)   |
| 7 ( $n = 3$ )               | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (10 equiv.), 100 °C, 15 min | 13 ± 3 (97 ± 3)   |
| 8 ( $n = 3$ )               | <b>PS-10b</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 17 ± 2 (> 98)   |
| 9 ( $n = 3$ )               | <b>PS-10c</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 13 ± 1 (86 ± 7)   |
| 10 ( $n = 3$ )              | <b>PS-10d</b> (5 mg)  | CH <sub>3</sub> CN (1.7 mL), AcOH (60 equiv.), 100 °C, 15 min | 9 ± 4 (71 ± 11)   |
| 11 <sup>e</sup> ( $n = 2$ ) | <b>PS-10a</b> (5 mg)  | CH <sub>3</sub> CN (4.0 mL) +0.4% AcOH over 15 min, 100 °C    | 7 ± 1 (87 ± 3)  |

<sup>a</sup> Using the batch procedure otherwise indicated. <sup>b</sup> Calculated as the activity in the collected vial (corrected by the decay) divided by the activity of the reaction vial before heating, and multiplied by the RCP, mean ± standard deviation of the  $n$  experiments, see the ESI for details. <sup>c</sup> Determined by radio-HPLC. <sup>d</sup> Experiments performed from a batch of **PS-10a** with only 80% conversion for the CuAAC step. <sup>e</sup> Using the “flow procedure”.

over the conjugation/fluorination steps after simple filtration. § Moreover, no fluorinated alkyne **8** was detected by  $^1\text{H}$  NMR and HPLC analyses in the isolated products, which confirmed full conversions for the CuAAC reactions after optimisation.

With these precursors in hands,  $^{18}\text{F}$ -fluorination was then examined using an AllinOne automated PET tracer synthesizer (see the ESI† for details). The [ $^{18}\text{F}$ ]fluoride obtained from the cyclotron (in solution in  $\text{H}_2[^{18}\text{O}]\text{O}$ ) was firstly purified and concentrated by trapping onto a quaternary ammonium cartridge (QMA) and further eluted by an aqueous solution of sodium chloride (Step (1), Table 1). Then, in a first set-up (“batch procedure”, Table 1), the resulting [ $^{18}\text{F}$ ]F<sup>-</sup> saline solution was transferred to the reaction vial previously loaded with a supported precursor **PS-10**, the organic solvent and a small quantity of acetic acid to activate the imidazole leaving group (Step (2), Table 1). After heating the suspension, the corresponding labelled compound [ $^{18}\text{F}$ ]11 was purified by adding water in the reaction vial (Step (3), Table 1) and filtering the resulting mixture through a Sep-Pak C18 cartridge in order to remove the unreacted [ $^{18}\text{F}$ ]fluoride (Step (4), Table 1). Finally, the radiotracer was isolated by elution with acetonitrile in a collecting vial (Step (5), Table 1). The activity was measured to calculate the RCY, and the radiochemical purity (RCP) was determined by radio HPLC. It should be noted that the optimisation of the conditions was performed with a batch of **PS-10a** with a conversion of  $\approx 80\%$  for the CuAAC step. ¶ In a first experiment (entry 1, Table 1), the conditions developed for the homogenous  $^{18}\text{F}$ -labelling of ImidSiFAs were employed (*i.e.* THF, 10 equiv. of AcOH and heating at 100 °C for 15 min).<sup>10</sup>

Interestingly, the desired [ $^{18}\text{F}$ ]11a was obtained with promising 8% RCY and 81% RCP. Moreover, switching the solvent to acetonitrile doubled the radiochemical yield to 16% (entry 2, Table 1), while only slightly lowering the radiochemical purity to 67%. On the contrary, increasing the quantities of AcOH or

**PS-10a** gave no significant improvement (RCY of 17% and 14%, respectively, entries 3 and 4, Table 1). Furthermore, as heating the reaction mixture for 30 min only improved the radiochemical yield by 3% (entry 5 compared to entry 2, Table 1), a reaction time of 15 min was preferred for the consecutive experiments in order to shorten as much as possible the overall procedure. With these optimised conditions in hand, the last-step radio-labelling was performed using a fully conjugated batch of supported precursors **PS-10a**, yielding [ $^{18}\text{F}$ ]11a in satisfactory 12% RCY using 60 equivalents of AcOH (entry 6) or 13 ± 3% RCY ( $n = 3$ ) with 10 equivalents of AcOH (entry 7). || Moreover, in both cases, an excellent radiochemical purity of 97% was determined without the need for an HPLC purification, which fully demonstrated the advantage of supported ImidSiFA. Then,  $^{18}\text{F}$ -fluorination was performed for supported precursors **PS-10b**, **PS-10c** and **PS-10d** using similar conditions to evaluate the versatility of this supported tag. Interestingly, the glucose-based bioconjugate [ $^{18}\text{F}$ ]11b was produced smoothly with a radiochemical yield of 17 ± 2% ( $n = 3$ ) and an excellent radiochemical purity (> 98%) for each experiment (entry 8). A similar result was observed for the synthesis of the biotin-based tracer from resin beads **PS-10c**, [ $^{18}\text{F}$ ]11c being obtained in 13 ± 1% RCY ( $n = 3$ ) with a good radiochemical purity of 86 ± 7% (entry 9, Table 1). Finally, the radiosynthesis employing the estradiol-based precursor **PS-10d** yielded compound [ $^{18}\text{F}$ ]11d in 9 ± 4% RCY ( $n = 3$ ), while the radiochemical purity was slightly lower and less reproducible in this case (71 ± 11%, entry 10, Table 1). However, taken together, these results confirmed the versatility of the alkyne-functionalized **PS-7** by easily producing various [ $^{18}\text{F}$ ]bioconjugates from the same starting resin.

Then, the set-up was modified to perform the  $^{18}\text{F}$ -fluorination in flow through a pre-packed “reaction cartridge” in stainless steel filled with the supported precursor **PS-10a** and a packing resin (see



the ESI<sup>+</sup> for details). In this case, the [<sup>18</sup>F]F<sup>-</sup> saline solution was firstly diluted with CH<sub>3</sub>CN (+0.4% AcOH) and consecutively injected through the column over 15 min while heating it at 100 °C. The downstream solvent was diluted with H<sub>2</sub>O, and filtered through the Sep-Pack C18 cartridge, and the desired radiolabelled compound was recovered by elution with acetonitrile. This fully automated procedure provided [<sup>18</sup>F]11a in a slightly lower RCY of 7 ± 1% (*n* = 2), but with a good radiochemical purity (87 ± 3, entry 11, Table 1), which established the proof-of-concept for potentially developing kit set-ups using this technology.

To conclude, anchoring the imidazole-di-*tert*-butyl-silane **6** onto a polystyrene resin provided the versatile platform **PS-7**, while its pendant alkyne moiety was directly functionalized by CuAAC. Using aqueous [<sup>18</sup>F]F<sup>-</sup>, the various heterogeneous precursors were simultaneously radio-labelled and cleaved from the resin as the last-step of the radiosynthesis. Thymidine-, glucose-, biotin- and estradiol-based conjugates [<sup>18</sup>F]11a-d were produced with automated “batch” or “flow” set-ups in RCY up to 19%. Good to excellent RCP were obtained in most cases after a simple filtration through the Sep-Pack C18 cartridge and consecutive elution. Removing the need for HPLCs, this “supported-ImidSIFA” method is highly promising for the development of <sup>18</sup>F-fluorination kits for automated syntheses of PET tracers. Other types of “click” bioconjugations are currently explored to widen synthetic and biological application scopes.

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## Conflicts of interest

M. S., G. B., S. R. and C. A. are Sanofi employees and may hold shares and/or stock options in the company.

## Notes and references

‡ Crystallographic data for this structure has been deposited with the Cambridge Crystallographic Data Centre as supplementary publication no. CCDC 2169890.

§ Calculated by hypothesising a 100% grafting in the **6** → **PS-7** step and multiplying by the mass ratios at each step.

¶ The side-product [<sup>18</sup>F]8 was recovered with [<sup>18</sup>F]11a (see ESI<sup>+</sup>).

|| An indirect labelling was attempted for comparison, *i.e.* synthesis of [<sup>18</sup>F]8 and consecutive CuAAC conjugation with **9a**, but product [<sup>18</sup>F]11a was isolated in only 2% RCY (see ESI<sup>+</sup>).

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