



Cite this: *Green Chem.*, 2022, **24**, 1270

Eco-friendly processes for the synthesis of amorphous calcium carbonate nanoparticles in ethanol and their stabilisation in aqueous media†

Lauriane Chuzeville,^{a,b} Frank Boury,^{id} ^c David Duday,^a Resmi Anand,^a Enzo Moretto^{a,b} and Jean-Sébastien Thomann ^{id} *^a

Amorphous calcium carbonate nanoparticles (ACC NPs) are promising multifunctional materials for healthcare applications. Due to their instability in aqueous media, pure ACC NPs for the biomedical field are increasingly synthesised in absolute ethanol, using the ammonia diffusion method (ADM). Although this method presents the advantage of providing stable ACC NPs without additives, it requires the use of pure ethanol as solvent. New insights into the formation mechanisms of ACC NPs in ethanol using gas diffusion are presented in this article. The optimisation of the process according to these findings can increase the mass concentration of ACC NPs by a factor of 3.5. As a result, the amount of ethanol required to produce a target mass of particles is significantly decreased, reducing the ecological impact of the process. The stabilisation of the resulting ACC NPs in aqueous media is achieved by a short-time process using phospholipids based on the ethanol injection method. By using the natural electrostatic affinity of negatively charged materials for the positive surface of ACC NPs in ethanol, we reduced the process time from 24 h to 2 minutes, compared with the closest state of the art, decreasing the operating time and corresponding energy consumption. The process does not require the use of synthetic PEGylated lipids for steric stabilisation. In addition, a natural egg-sourced phospholipid was identified as an efficient stabiliser for the first time. The upscaling of our process was successfully demonstrated using a 50 L reactor for bulk synthesis, as well as a continuous flow reactor for industrial continuous flow production.

Received 15th September 2021,
Accepted 26th November 2021

DOI: 10.1039/d1gc03396d

rsc.li/greenchem

Introduction

In recent years, there has been increasing interest in calcium carbonate nanoparticles (CaCO₃ NPs) from various industrial fields.^{1–5} Besides their excellent biocompatibility and biodegradability, they present numerous advantages for cosmetic formulations and biomedical applications.^{6–12} For instance, they are intensively investigated for drug delivery, diagnostics and tumour therapy due to their pH responsive and buffering properties.^{6–12} In both fields, nanosize can be of extreme importance, for long-lasting effect and increased stability in cosmetic formulations, or for targeting tumoral and inflamed tissues in biomedical applications for instance.^{13–17}

CaCO₃ exists in three major crystalline polymorphs (vaterite, aragonite and calcite), and in an amorphous phase.^{18,19} The latter presents great advantages for the healthcare and biomedical fields, including a higher porosity and the ease of obtaining highly monodisperse NPs *via facile* processes.^{20–22} The high porosity of the amorphous form (100–200 m² g⁻¹) compared to the other polymorphs (<30 m² g⁻¹) leads to higher capacity of active molecule loading, as well as a higher sensitivity to water. The latter is a key advantage for enhancing burst dissolution at target sites.^{20,22–25} Amorphous CaCO₃ nanoparticles (ACC NPs) are also employed for their highly homogeneous spherical shape, including for the synthesis of core-shell multifunctional nanomaterials.^{26,27}

Due to its transient nature, ACC is the most unstable CaCO₃ form when in contact with water, spontaneously dissolving and crystallising into other CaCO₃ polymorphs, vaterite, calcite and/or aragonite.^{28,29} Despite being an advantage for enhancing burst dissolution, the instability in aqueous media remains a major hindrance to the use of ACC NPs in the fields where the phase and size conservation is critical in aqueous media.^{30,31} This is particularly the case for applications requiring intravenous injection for instance.^{6,20,26}

^aMaterials Research and Technology, Luxembourg Institute of Science and Technology, 5 Avenue des Hauts Fourneaux, Esch/Alzette L-4362, Luxembourg.
E-mail: jean-sebastien.thomann@list.lu

^bUniversity of Luxembourg, Department of Physics & Materials Science, 162a Avenue de la faïencerie, 1511 Luxembourg city, Luxembourg

^cCRCINA-GLIAD Team 17, INSERM, UMRS 1232, Université de Nantes, Université d'Angers, 49933 Angers, France

†Electronic supplementary information (ESI) available. See DOI: 10.1039/d1gc03396d



The synthesis and stabilisation of CaCO₃ colloids at nano-scale is widely described in the literature using one-pot strategies in aqueous media. This includes the synthesis of CaCO₃ with stabilising molecules such as synthetic polymers, lipids or a combination of therapeutic molecules and synthetic polymers.^{5,9,32–40} The phase of the particles is generally not amorphous, with a mean diameter often higher than 300 nm.^{5,9,32,33,35,36} Vidallon *et al.* recently reported the synthesis of a hybrid polydopamine/bovine serum albumin/CaCO₃ NPs stable in aqueous media for contrast-enhanced ultrasound imaging.⁵ The NPs obtained are a polycrystalline mixture of vaterite and calcite, with a mean diameter above 500 nm.⁵ Furthermore, these methods provide hybrid nanoparticles, with a CaCO₃ content lower than pure ACC NPs materials.^{5,9,32–36} Another aqueous strategy consists of the synthesis of CaCO₃ nanoparticles inside liposomes, to control the final size of the particles.^{41–44} These methods use toxic organic solvents to synthesise the liposomes.^{41–43} The size homogeneity and phase control of the CaCO₃ particles obtained is uncontrolled with these methods.^{41–44}

Pure ACC NPs with a size under 150 nm can be easily obtained without synthetic additives *via* a low cost and facile vacuum-assisted process in absolute ethanol developed over the last ten years.^{6,11,20,21,23,26,45–50} This process is the ammonia diffusion method (ADM), usually known for the synthesis of CaCO₃ NPs in water or in a mix water/ethanol.^{32,33,51} In this variation, absolute ethanol is used as unique solvent to limit the amount of water and prevent the crystallisation of ACC NPs into vaterite or calcite without the need for synthetic additives.^{6,20,21} The final nanoparticles are dispersed in ethanol and are stable, with a highly homogeneous size under 150 nm, and a spherical shape.^{6,20} Although this method is becoming increasingly popular in the biomedical field, there are only few studies that briefly discuss the process parameters and the ACC NPs formation mechanism.^{21,49} Therefore, several variations of the methods are found in the literature, highlighting the need for a deeper understanding of ethanol ADM mechanisms for the synthesis of ACC NPs. Indeed, this process uses ethanol as solvent and should be carefully optimised to minimise the quantity of solvent required to synthesise a certain amount of particles.

For applications requiring the dispersion of ACC NPs in aqueous media, the use of an albumin solution or of lipidic additives have been reported to achieve the stabilisation of the particles in presence of water.^{6,11,20,23,26,47} However, stabilisation without the use of synthetic additives and/or harmful solvents remains a challenge.^{7,11,20,37,38,40,52} Hybrid lipid-ACC NPs (LCC NPs) are of particular interest as they combine the advantages of ACC and lipid nanomaterials.^{11,37,38} The major drawback of lipid-based stabilisation is the need for hazardous organic solvents like cyclohexane or chloroform to dissolve the lipids,^{37,38} and/or the use of PEGylated lipids.^{20,39} The work of Wang *et al.* for example uses a mix of ethanol and chloroform to dissolve the lipid mix used as stabilisers.¹¹ Recently, Wang *et al.* successfully developed a method without toxic organic solvent to stabilise ACC NPs in water using phospholipids.²⁰

However, their method requires a 24 h continuous mixing of the ACC NPs/lipid mixture at 37 °C prior to the injection in water, representing a long operating time and energy consumption.²⁰ Furthermore, the lipid mix reported includes PEGylated phospholipids as key stabiliser.²⁰ One of the recent challenges faced by the pharmaceutical and cosmetic industries is the development of more sustainable products and technologies.^{53–56} Therefore, there is a need for the development of PEG-free materials and as PEGs are synthetic and non-biodegradable materials.^{53,54,56} This need is also motivated by the emergence of anti-PEG immune responses due to the extensive use of PEGylated additives in the food, cosmetic and pharmaceutical industries.^{57–62} In the biomedical field, the apparition of anti-PEG IgG and IgM is responsible for efficacy loss and hypersensitivity reactions.^{59,63}

In this work, we report on valuable new insights into the formation mechanisms of ACC NPs by ADM in absolute ethanol by investigating several influential parameters (diffusion of water and ammonia in the ethanol solution of CaCl₂, size of the gas–ethanol interphase, presence or absence of a diffusion barrier) and *in situ* monitoring of the pH in ethanol (pHe) and conductivity during the reaction. These new insights lead to a better understanding of the influence of several reaction parameters, allowing the optimisation of the process efficiency to significantly reduce the amount of ethanol required to synthesise a certain mass of ACC NPs.

Subsequently, this work reports new advances for the stabilisation of the resulting ACC NPs in aqueous media using phospholipids. Similarly to the work of Wand *et al.*, the developed process is based on the ethanol injection method and is not using toxic organic solvents.²⁰ We studied the influence of the phospholipid polar head group on the stabilisation efficiency, and rationally selected the lipids according to their natural electrostatic affinity for calcium ions and ACC NPs. As a result, we were able to significantly reduce the process duration from 24 h to 2 min, decreasing the operating time and energy consumption of the process. The selected lipids are not PEGylated, increasing the sustainability of the process. Lastly, a bio-sourced phospholipid has been identified as suitable stabiliser. CryoTEM imaging is used to investigate the particular structuration behaviour of these lipids around the ACC NPs. This work also presents two different strategies to adapt the process to industrial needs, using a 50 L large scale reactor and a continuous flow reactor.

Experimental

Materials

Calcium chloride hexahydrate (CaCl₂·6H₂O), ammonium bicarbonate (NH₄HCO₃), 1,2-dipalmitoyl-*sn*-glycero-3-phosphocholine (DPPC), 1,2-dioleoyl-3-trimethylammonium-propane (DOTAP), 1,2-dioleoyl-*sn*-glycero-3-phospho-L-serine (DOPS), 1,2-distearoyl-*sn*-glycero-3-phospho-L-serine (DSPS), 1,2-dihexadecanoyl-*sn*-glycero-3-phospho-L-serine (DPPS), 1,2-dimyristoyl-*sn*-glycero-3-phospho-L-serine (DMPS), 1,2-didodecanoyl-*sn*-



glycero-3-phospho-L-serine (DLPS), and 1,2-dipalmitoyl-*sn*-*glycero*-3-phospho-(1'-*rac*-glycerol) (DPPG) were purchased from Sigma Aldrich (Overijse, and Diegem, Belgium). *N*-(Carbonyl-methoxypolyethylene glycol-2000)-1,2-distearoyl-*sn*-*glycero*-3-phosphoethanolamine (DSPE-PEG 2000) was purchased from Avanti (Alabaster, Alabama, United States). Egg phosphatidyl glycerol (1,2-diacyl-*sn*-*glycero*-3-phospho-*rac*-glycerol, sodium salt) (E PG) was purchased from Lipoid (Ludwigshafen, Germany). Absolute Ethanol was purchased from VWR International (Fontenay-sous-Bois, France). The 3 Å molecular sieve was purchased from Sigma Aldrich (Gillingham, United Kingdoms).

ACC NPs preparation

CaCl₂·6H₂O was dissolved in absolute ethanol in a glass container, at a mass concentration of 4.4 mg mL⁻¹. Optionally, the container can be covered by parafilm punctured with 12 holes of 1 mm diameter. The container is then placed in a desiccator at room temperature, along with excess NH₄HCO₃ distributed in 4 vials (~10 g per vial). The system is placed under vacuum for 2–96 h. The vacuum is set at 200 mbars, then the system is sealed, and the pumping is stopped. At the end of the reaction, the particles were centrifuged at 30 000g for 10 min. The supernatant is discarded, the particles are resuspended in the proper amount of ethanol and dispersed with an ultrasonic bath for few minutes. The resulting solution of ACC NPs in ethanol is stored at 4 °C. ACC NPs growth was monitored with and without 3 Å molecular sieve in the desiccator, to evaluate the influence of ammonia and water on ACC NPs growth.

Stabilisation of ACC NPs in water

The stabilisers (*i.e.* DPPC, DOPS, DSPS, DPPS, DMPS, DLPS DOTAP, E-PG, DPPG, DSPE-PEG2000) were prepared in ethanol at a mass concentration of 0.25 mg mL⁻¹ using an ultrasonic bath.

Then, ACC NPs suspended in ethanol are mixed with the stabiliser at a mass ratio ACC:stabiliser of 1. After a one-minute of homogenisation in an ultrasonic bath, the obtained solution was mixed with deionised water by a one-pot injection at a ratio of ethanol:deionised water 1:9. The injection was followed by a 15-second stirring by vortex (Fig. 1).

Surface charge modulation

Lipid-coated ACC (LCC) using DOPS as stabilisers dispersed in deionised water were mixed with a stock solution of DOTAP in

ethanol, molar ratio DOTAP/DOPS between 1–10. The stock solution of DOTAP was mixed with deionised water by a one-pot injection at a ratio of ethanol:deionised water 1:9. The injection was followed by a 15-second stirring by vortex.

Characterisation

The particle size distribution and zeta potential were measured in ethanol⁶⁴ or in deionized water at pH 7, with a Zetasizer (Nano-ZS90, Malvern Instruments Ltd, UK) based on dynamic light scattering (DLS) or micro-electrophoretic light scattering technique respectively. The nanoparticles suspensions were neither diluted nor filtered prior to the analysis. A minimum of three measurements are performed per sample. The refractive indexes used are 1.681 for pure ACC and LCC NPs, with an absorbance of 0.

The mass concentration of ACC NPs after synthesising was determined by centrifuging 20 mL of solution at 30 000g for 10 min, discarding the supernatant, and drying the pellet under vacuum for 15 minutes. Afterward, the tube was weighed (mass tube). The mass of the empty tube is referred to as “mass tare”.

$$\text{Mass concentration} = \frac{\text{mass tube} - \text{mass tare}}{20 \text{ mL}}$$

The size and surface morphology of the NPs were characterized by Scanning Electron Microscopy (SEM). A droplet of solution was deposited on to copper tape and air-dried. The ACC NPs non coated by lipids were imaged immediately after drying to avoid degradation due to air moisture contamination. SEM images were performed with a Helios Nanolab, 650 Scanning Electron Microscope (FEI Company, Hillsboro, Oregon, United States), operating at a voltage of 2–10 kV and current of 25–100 pA.

The concentration of the nanoparticle suspensions was determined by Nanoparticles Tracking Analysis (NTA), using the Nanosight® NS500, with the temperature control set at 25 °C. The samples were diluted at a ratio 1:1000 in deionised water at pH 7 prior to analysis. A minimum of five measurements were performed by sample.

The XRD measurements were performed on an XRD X'Pert Pro in reflection mode with a Cu K-alpha tube (45 kV, 40 mA). The primary optics contain a programmable divergence slit whereas the secondary optics consist of a PIXcel detector run in 1D mode with a programmable antiscatter slit. Before measuring the sample, the solutions containing the nanoparticles were deposited on to a zero-background holder and covered with a thin Kapton film in order to prevent the solvent from evaporating. During the measurement, the zero-background holder was spun.

Cryogenic transmission electron microscopy (CryoTEM) was performed as follows. Four microliters of sample were deposited on a holey carbon film (Quantifoil type R1.2/1.3), rendered hydrophilic by either a low-power plasma cleaning treatment (Model 1070 NanoClean, Fishione) for the LCC NPs sample or by a negative glow discharge in air (PELCO easiGlow™) for the ACC NPs sample. For the ACC NPs samples, blotting was performed for 2 s with a blot force of 8,

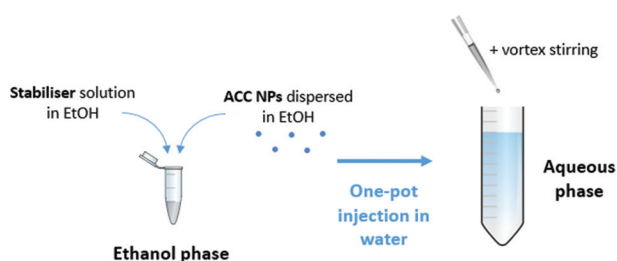


Fig. 1 Process for the stabilisation of ACC NPs in aqueous media.



and for LCC NPs, 0.5 seconds with a blot force of 5. Then, vitrification in liquid ethane was performed using an automated plunger (Vitrobot, FEI Compagny). Blotting was carried out at 10 °C and 90–95% humidity. Images were recorded using the SerialEM software on a FEI Tecnai F30 microscope (FEI Company, Hillsboro, Oregon, United States) operating at a voltage of 100 kV and equipped with a Falcon camera (FEI company).

The helium ion microscope (HIM) images were recorded with an Orion Nanofab Instrument (Zeiss, Peabody, US). Helium ion microscopy was based on the detection, with a conventional Everhart–Thornley (ETD) detector, of the secondary electrons emitted from the sample surface scanned with a focused energetic He⁺ or Ne⁺ ion beam.⁶⁵ With a helium beam resolution of 0.3 nm and a Neon beam resolution of 1.5 nm, this microscope offers Secondary Electron (SE) images with a high contrast for imaging insulator. Compared to the latest generation of Scanning Electron Microscope (SEM), the HIM allows specimens to be probed with a better surface sensitivity, a higher depth of field and the ability to analyse uncoated insulator samples.⁶⁵ In this study, the images were acquired with a 25 keV He⁺ beam of 0.2 pA for a matrix of 1024 × 1024 pixels and a counting time of 40 μs per pixel.

ACC particle size monitoring

Five desiccators containing all the reagents (see ACC NPs preparation) were connected to the vacuum manifold of a Schlenk line (ESI Fig. S1†). The system was placed under vacuum. The 5 desiccators were exposed to the same vacuum conditions. At several time intervals, a desiccator was isolated from the Schlenk line by a valve and opened to measure the nanoparticle size by DLS (see Characterisation).

The particle size after 2 h of reaction time was characterised by SEM, and also by Helium Ion Microscopy (HIM) (see Characterisation) to corroborate the SEM measurements.

pHe and conductivity monitoring during ACC NPs synthesis

A pH probe and a conductivity probe were inserted into a modified plastic desiccator (ESI Fig. S2†), and dipped into the CaCl₂·6H₂O solution in ethanol. The reaction was conducted by following the ACC NPs preparation protocol.

The variation of electrical conductivity (EC) was followed by a USP compliant EC, TDS, NaCl, Resistivity, Temperature Meter from Hanna Instruments (Temse, Belgium), HI98192, with a four-ring conductivity resistivity electrode from Hanna Instruments, HI763123.

The pHe variation was followed by a pH/temperature Bench Meter from Hanna Instruments (Temse, Belgium), HI2002, with a digital, glass body, double junction, conical tip, pH/temperature electrode from Hanna Instruments, HI10530.

Process upscaling for the stabilisation of ACC NPs in water and the surface charge modulation for volumes >50 mL

Stock solutions of stabilisers and charge modulation agent in absolute ethanol were prepared at a mass concentration of 0.25 mg mL⁻¹, using an ultrasonic bath.

The solution of ACC NPs in ethanol was mixed with the stock solution of stabiliser using an ultrasonic bath. The mass ratio of ACC : stabiliser is ranging between 1 and 2. After one minute of mixing, the ethanol solution was added to a large volume of deionised water under magnetic stirring (>500 rpm), at a ratio of ethanol : deionised water 1 : 9. For an Erlenmeyer of 2 L with a bottom diameter of 15 cm, a magnetic bar of 5 cm was used.

The magnetic stirring (>500 rpm) replaced the one-pot injection using a pipette (see Stabilisation of ACC NPs in water), allowing larger volumes to be handled.

Process upscaling for the stabilisation of ACC NPs in water adapted to industrial volumes

50 L reactor: the upscaling was performed using the reactor from Orb Pilot 50 L (Syrrix, Royston, United Kingdom), equipped with a mechanical stirrer, on a 40 L final volume. 36 L of water were put under stirring with a stirring speed of 300 rpm. Then, 4 L of an ethanolic solution of EPG and suspended ACC NPs (mass ratio ACC NPs : EPG of 1) were poured in 13 seconds inside the water phase.

Continuous flow reactor: for the upscaling of the stable ACC NPs in water, we performed a facile continuous flow mixing method using Coflore® Agitated Cell Reactor (ACR) (AM Technology, Cheshire, England). The Coflore ACR is a mechanically agitated plug flow reactor, in which efficient mixing is performed using multiple interlinked cell reactors. The cell reactor was connected to a syringe pump and a peristaltic pump for the continuous supply of reactants. The stabiliser DOPS was prepared in ethanol at a mass concentration of 0.25 mg mL⁻¹ and ACC NPs suspension was mixed with the stabiliser at the mass ratio of 1, followed by homogenization in an ultrasonic bath. Then, the ACC NPs : stabilizer colloidal solution was transferred into a 50 mL syringe connected to a syringe pump. A controlled flow of deionised water to the cell reactor was established using a peristaltic pump. Both reactants were introduced to the Coflore mixing cell at the following conditions: flow rate of ACC NPs : stabilizer 1 mL min⁻¹, flow rate of water 9 mL min⁻¹, agitation of 9 Hz at room temperature.

Results and discussion

ACC NPs formation by ethanol ADM

ACC NPs were prepared by a vacuum-assisted ammonia diffusion method (ADM) in absolute ethanol inspired by the work of S-F. Chen *et al.*²¹ and A. Som *et al.*⁶ (Fig. 2). CaCl₂·6H₂O serves as Ca²⁺ precursor, ammonium bicarbonate as CO₃²⁻ precursor, and absolute ethanol as solvent. The synthesis in ethanol limits the presence of water, preventing the spontaneous aggregation and crystallisation of CaCO₃ NPs without the need for synthetic additives.^{6,11,20,21,23,26,45–50} This method leads to the obtention of pure ACC nanoparticles with a size under 150 nm.

This method is increasingly employed in the biomedical field to produce highly regular pure ACC NPs in terms of size



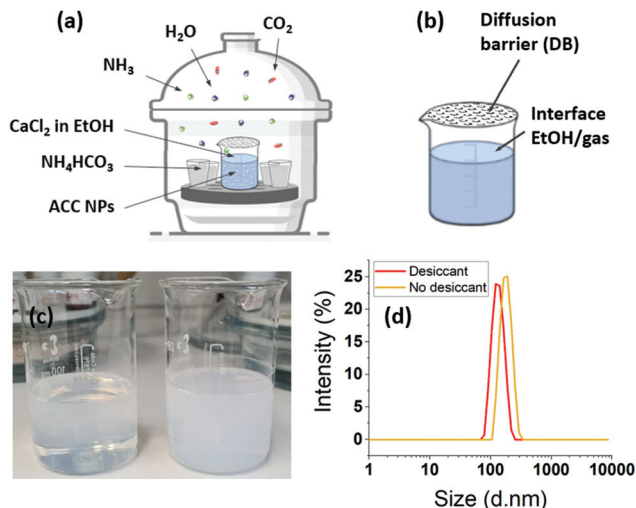
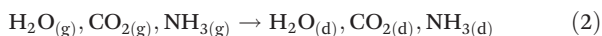
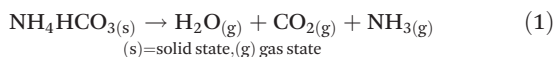


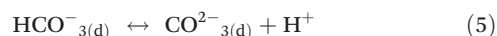
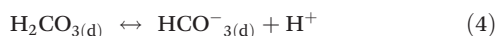
Fig. 2 (a) Schematic representation of the reaction setup. (b) Schematic representation of the diffusion barrier (DB) and the gas–ethanol interface. (c) Final ACC NPs solution obtained with desiccant (left) and without desiccant (right). (d) Size distribution measured by DLS of final ACC NPs obtained with and without desiccant.

and shape.^{6,11,20,23,26,46–50} However, the investigation of ACC NPs formation mechanisms in absolute ethanol using ADM is at its beginning.^{21,49} Therefore, several variations in the process parameters are present in the literature.^{6,11,20,21,23,26,45–50} The following work intends to bring new data and understanding on the ethanol ADM formation of ACC NPs, as a base for process efficiency optimisation. As ethanol is used as only solvent, improving the process efficiency reduces the amount of ethanol needed to synthesise a specific mass of particles, decreasing the ecological impact of the process.

In aqueous ADM, the CaCO_3 formation mechanisms are well known and are described by eqn (1)–(6):⁵¹



(d)=dissolved in the calcium chloride ethanol solution, containing residual water from the solvation of $\text{CaCl}_2 \cdot 6\text{H}_2\text{O}$



Ammonium carbonate or bicarbonate are used as the CO_2 source, and placed in a sealed container with an aqueous solution of calcium chloride. Under vacuum, the decomposition of ammonium carbonate or bicarbonate is spontaneous⁶⁶ and leads to a progressive saturation of the gas phase with CO_2 , NH_3 and H_2O (eqn (1)).⁵¹ These gases diffuse into the calcium chloride solution through the gas–liquid interface (eqn (2)). Once in solution, water molecules react with the dissolved CO_2

to form H_2CO_3 (eqn (3)), in acid–base equilibria with HCO_3^- and CO_3^{2-} (eqn (4) and (5)). The diffusion of ammonia in the solution increases the pH, generating a basic environment where the formation rate of CO_3^{2-} is increased.⁵¹ The final reaction between Ca^{2+} and CO_3^{2-} produces CaCO_3 (eqn (6)).^{51,67} In water, without additives, the amorphous form of CaCO_3 at nano-size is not stable.^{22,28,29}

In absolute ethanol ADM, the generation of H_2O from the decomposition of ammonium carbonate or bicarbonate, is an essential step for the formation of the precursor ions NH_4^+ and CO_3^{2-} .^{46,48,67,68} In our process, water molecules also come from the solvation of $\text{CaCl}_2 \cdot 6\text{H}_2\text{O}$ in ethanol. We verified the influence of the water and ammonia vapours coming from the decomposition of ammonium bicarbonate by placing a 3 Å molecular sieve in the desiccator. A 3 Å molecular sieve has the ability of trapping of water and ammonia without trapping the CO_2 (Fig. 2). The particle size distribution monitored by DLS shows a size of 132 nm with a PDI of 0.008 with the sieve. The size increases to 177 nm without molecular sieve, with a PDI of 0.025. The size dispersion remains narrow with a particle size under 200 nm. These results seem to indicate that the water coming from the decomposition of ammonium bicarbonate do not lead to uncontrolled crystallisation or aggregation. The final mass concentration is 0.6 mg mL^{-1} with sieve, compared to a final mass without sieve of 2.1 mg mL^{-1} . As a consequence, the solution turbidity (Fig. 2c) appears more important without molecular sieve. These results evidence that the initial water content coming from the solvation of $\text{CaCl}_2 \cdot 6\text{H}_2\text{O}$ in absolute ethanol is sufficient to obtain monodisperse ACC NPs. However, the results without sieve show that the diffusion of ammonia and water in ethanol catalyses the formation of ACC NPs, leading to an increase in the final mass concentration by a factor of 3.5. In a similar way to aqueous ADM, the role of water is to generate the aqueous forms of CO_2 , *i.e.* H_2CO_3 , HCO_3^- , CO_3^{2-} (eqn (3)). The role of ammonia is to alkalise the ethanol solution, promoting the precipitation of CaCO_3 NPs by displacing the equilibrium in favour of CO_3^{2-} (eqn (3)–(5)).^{46,48,67,68} The final mass concentration increase by a factor of 3.5 without molecular sieve demonstrates the importance of the diffusion of water and ammonia in the process efficiency. In several studies, drierite is employed to trap the water coming from the decomposition of ammonium bicarbonate.^{6,48} Our results strongly suggest a better process efficiency without trapping these water molecules. Indeed, the increase in final mass concentration observed without drierite could divide by 3.5 the volume of ethanol required to produce the same mass of particles.

We investigated the growth mechanisms of ACC NPs in ethanol ADM. The size of ACC NPs was monitored by DLS at different reaction times (Fig. 3, ESI Fig. S8†). The particle size after 2 h reaction is below the limit of DLS sensitivity and was successfully determined by SEM imaging. Clusters with a mean diameter of 10 nm were observed. The results were confirmed by helium ion microscopy imaging to exclude a possible contamination or artefact from the SEM measurement. Thanks to this observation, we successfully determined that



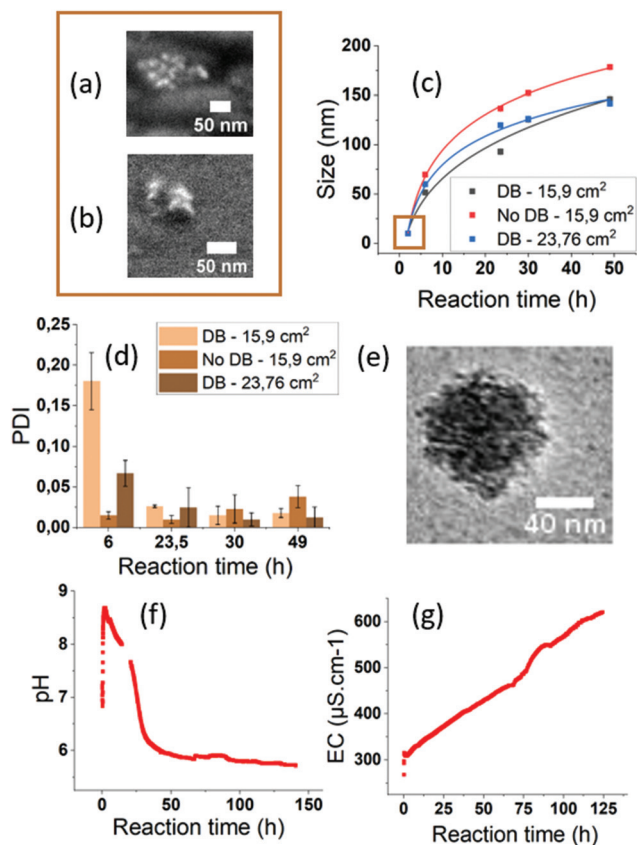


Fig. 3 ACC NPs growth in function of the reaction time. (a) SEM imaging after 2 h reaction. (b) Helium ion beam imaging after 2 h. (c) ACC NPs growth curves, with or without DB, for gas–ethanol interfaces of 15.9 cm² and 23.8 cm². The fitting curves are following a power law $y = a + b \times x^c$. The r^2 are of 0.981 (black), 0.997 (blue) and 0.992 (red). (d) PDI values. (e) CryoTEM imaging of an ACC NP after synthesis. (f) pH monitoring for 140 h. (g) Electric conductivity (EC) monitoring for 140 h.

the growth of ACC NPs followed a classical power law between 2 h and 49 h reaction time in ethanol ADM (Fig. 3c). The nature of the power law variables (temperature, pressure) were not determined in this work, and would require further modelling. The ACC NPs PDI after 49 h reaction time was below 0.05. Such a narrow size distribution suggests a growth mechanism with the nucleation and growth steps occurring separately. A simultaneous nucleation and growth mechanism would lead to polydisperse size dispersions.⁶⁹ The Lamer model was considered, as it is the most common model of the classical nucleation theory describing a burst nucleation followed by a diffusion driven growth.⁶⁹ However, the CryoTEM characterisation of the final ACC NPs revealed an irregular shape of NPs (Fig. 3e). The NPs appeared to be constituted from an aggregation of nuclei, forming an irregular granular structure (Fig. 3e). The SEM and helium beam characterisation at 2 h confirms the granular structure, revealing small clusters with a similar particle constitution of several nuclei (Fig. 3a and b). These observations exclude both diffusion-driven growth and the Lamer model, which would lead to a more homogeneous structure and shape.⁶⁹ Growth by nucleus aggregation was also

excluded by the PDI values <0.05 at 49 h reaction time. These observations led us to consider the hypothesis of a homogeneous nucleation followed by an autocatalytic heterogeneous nucleation & growth on the surface irregularities of the NPs. This hypothesis is consistent with the PDI < 0.05 after 49 h reaction time, and with the irregular granular structure of the nanoparticle revealed by CryoTEM.

The influence of the gas–ethanol interface area (Fig. 3, ESI Fig. S7†) was also investigated. An increase in the gas–ethanol interface area generates a higher gas diffusion rate in the CaCl₂ solution according to the Fick Law.⁷⁰ In our experiment, for a gas–ethanol interface of 15.9 cm², the final mass concentration reached 1.1 mg mL⁻¹, compared to 2.1 mg mL⁻¹ with an interface of 23.8 cm². It represents a final mass concentration increase by a factor of 1.9. No PDI alteration was observed. The results of the present study show an increase in size and mass concentration when the gas–ethanol interface area increases. Hence, process efficiency in terms of end product quantity can be significantly improved by increasing the gas–ethanol interface area.

For the synthesis of ACC NPs by ADM in water or ethanol, a diffusion barrier (DB) constituted of parafilm punctured with small holes is generally placed on the CaCl₂ solution container (Fig. 2b). These DB are known to act as reaction regulators.⁵¹ We investigated the influence of and need for such a DB barrier in a process in absolute ethanol. Indeed, the literature suggests that performing the reaction in absolute ethanol is sufficient to limit the amount of water and prevent the spontaneous aggregation and crystallisation of CaCO₃ NPs.^{49,71,72} We compared the size, dispersion and mass concentration between an uncovered container, and a container covered by a parafilm tape punctured with small holes. A difference in size and mass was observed between the two samples (Fig. 3, ESI Fig. S6†). The final mass concentration without a DB reached 1.2 mg mL⁻¹, compared to 0.5 mg mL⁻¹ with a DB, which represents a final mass increase by a factor of 2.4. The PDI of both samples were under 0.1 after 49 h reaction time (Fig. 3). Without a DB, the diffusion rate of CO₂, NH₃ and H₂O in the CaCl₂ solution increases. Hence, this may generate a faster concentration increase of the precursor ion CO₃²⁻ in solution, and therefore lead to higher particle concentration without alteration of the particle size dispersion. These results strongly suggest that a regulation with DBs is not required in ethanol ADM to generate monodisperse ACC NPs. Furthermore, they demonstrate that the removal of the DB lead to a significantly higher efficiency in terms of final mass concentration of ACC NPs.

The conductivity and pH were monitored during the synthesis for 96 h inside the chamber to get a better understanding of the formation mechanisms of ACC NPs in ethanol ADM. The trends observed were confirmed by a second monitoring up to 140 h of synthesis (Fig. 3f, ESI Fig. S9†). The size measured by DLS after 96 h reaction was 150.8 nm with a PDI of 0.066. These values were similar to the sizes obtained after 49 h reaction (Fig. 3c). Hence, the size of ACC NPs seems to reach a maximum close to 150 nm. After 140 h reaction, white



aggregates were visually observed in the solution, with a polydisperse size distribution characterised by DLS (ESI Fig. S10†).

In ADM, pH is a critical parameter known to govern the balance between the different aqueous carbonate species.⁵¹ The pHe monitoring of our reaction showed an initial burst up to a pHe of 8.75 after 5 minutes, followed by a progressive decrease and a stationary phase at pH 5.7 (Fig. 3f). The pHe burst is probably a consequence of ammonia and water diffusion in the ethanol solution, following the decomposition of ammonium bicarbonate. Indeed, in aqueous or ethanol ADM, ammonia is known to cause a pH increase favouring the existence of CO_3^{2-} .^{46,48,67,68} However, the pHe evolution we observed in ethanol was surprisingly different from pH studies conducted in aqueous ADM.⁵¹ With water as the solvent, the pH increases during 5 to 30 minutes before reaching a maximum value between 9.8 and 10.5.⁵¹ Afterwards, in water, the pH mildly decreased to reach a stationary phase at pH 9.8.⁵¹ The differences in the pH and pHe variation rate and amplitude observed between aqueous and ethanol ADM could originate from the differences in ionic solubility and the solvation limit between the two solvents. The presence of CO_2 in ethanol or in water is known to decrease the pHe or the pH.^{51,67,73} CO_2 has a higher solubility in ethanol compared to water.⁶⁷ On the other hand, ammonia is less soluble in ethanol compared to water.^{74,75} These two differences could explain the amplitude of the pHe decrease in ethanol compared to water ADM. As the pHe decreases, the equilibrium between the different forms of hydrated CO_2 will progressively be displaced in disfavour of the formation of CO_3^{2-} . As a result, the formation of ACC NPs will progressively slow down (Fig. 3c). A stationary phase is reached at pHe 5.7 in our solution. At such pHe, CO_3^{2-} becomes a minority. This stationary phase is reached close to 48 h, when the growth of ACC NPs becomes negligible, with the maximum size of 150 nm observed by DLS at 50 h and 96 h reaction time.

The conductivity was also monitored to follow the ionic and water content of the CaCl_2 ethanol solution. In absolute ethanol, the conductivity is negligible ($0.06 \mu\text{S cm}^{-1}$). The initial conductivity measured in the $\text{CaCl}_2 \cdot 6\text{H}_2\text{O}$ ethanol solution is significantly higher, with values reaching $290 \mu\text{S cm}^{-1}$. This increase evidences the presence of Ca^{2+} , Cl^- and water coming from the solvation of $\text{CaCl}_2 \cdot 6\text{H}_2\text{O}$. The follow up of conductivity shows a burst when the vacuum is set, followed by a steady and linear increase along the reaction. This increase is linear up to the end of the 140 h monitoring. The initial burst when the vacuum is set might result from the significant bubbling occurring in the solution during the vacuum pumping, as the conductivity electrode is very sensitive to air bubbles. However, it might also be a consequence of the gas diffusion in the ethanol solution following the decomposition of ammonium bicarbonate. The steady increase testifies to a regular generation of ionic species in the solution. Despite Ca^{2+} and CO_3^{2-} being involved in the formation of ACC NPs, NH_4^+ and Cl^- also exist in the solution and contribute to the final ionic content. In contrast with pHe and size evolution, no maximum or stationary phase was observed. Besides the ionic

content evolution, the linear increase of conductivity strongly suggests a continuous diffusion of water inside the ethanol solution. An increase of water content would certainly explain the aggregation of ACC NPs occurring between 96 h and 140 h reaction, through dissolution/crystallisation catalysed by the slightly acidic environment.^{28,29}

The XRD spectrum of the final ACC NPs shows two wide peaks centred on 2θ values of 25° and 40° respectively, characteristic of amorphous CaCO_3 NPs (Fig. 4a).⁷⁶ The typical porosity and granular structure of ACC are visible by CryoTEM (Fig. 4b). The size dispersion characterized by DLS evidences monodisperse spherical NPs with a polydispersity index (PDI) under 0.05 (Fig. 4c). SEM imaging corroborate monodisperse nanoparticles with spherical and porous structure, characteristic of non-crystalline CaCO_3 NPs with an average diameter of 70 nm (Fig. 4d). The size dispersion in DLS is centred on 127 nm, a higher value compared to SEM measurement, due to the hydrodynamic diameter of ACC NPs in ethanol.⁶

ACC NPs size and shape in the presence of water have been characterised by DLS and SEM to evaluate the influence of water on the size and crystallinity of the particles (Fig. 4e and f). Both analyses clearly evidenced the instability of ACC NPs in aqueous media. The DLS size distribution is larger with PDI above 0.25 and centred on micrometre scale values $>1 \mu\text{m}$.

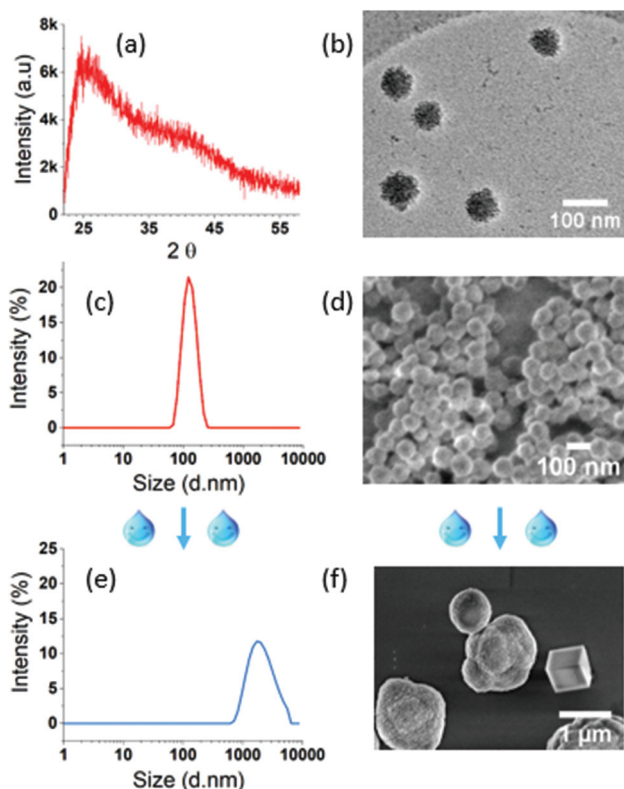


Fig. 4 ACC NPs characterisation in ethanol and water. In ethanol: (a) XRD spectra. (b) CryoTEM imaging. (c) Size distribution characterized by DLS. (d) SEM characterisation. (e) Particle size distribution of ACC NPs in presence of water. (f) SEM images of ACC NPs after water exposition.



SEM characterisation confirms the presence of large microparticles, with characteristic shapes of crystalline polymorphs, typically vaterite aggregates and trigonal rhombohedral calcite.⁷⁷ These results testify to the instability of ACC NPs in the presence of water, and strongly suggest a crystalline transition to calcite through vaterite intermediates. This behaviour is inherent to the transient nature of non-stabilised ACC NPs in the presence of water.⁷⁸

The following section presents a facile green process to preserve the amorphous structure and nanosize of ACC NPs in aqueous media. This process is exclusively using a water-ethanol mix and non-PEGylated phospholipids. The process was optimised by rationalising the selection of phospholipids according to their polar head structure.

PEG-free lipid stabilisation of ACC NPs in water

Up to this day, the greenest strategy for the stabilisation in aqueous media of ACC NPs synthesised using ethanol ADM has been reported by Wang *et al.*²⁰ The process is based on solvent exchange using ethanol and water, a well-known method used for the synthesis of liposomes and more commonly known as the ethanol injection method.^{20,79,80} A mix of PEGylated lipids and phosphatidylcholine (PC) phospholipids is used for the stabilisation.²⁰ The lipids are put in contact with ACC NPs for 24 h under continuous magnetic stirring before injection in a large volume of water. Lipids self-organise around the ACC NPs when they come into contact with water.²⁰

Our work aimed to lower the contact time between the lipids and the ACC NPs to lower the amount of energy and operating time required for the process. The objective is also to employ more sustainable stabilisers and provide an effective stabilisation without using PEGylated lipids. To achieve these goals, we rationalised the phospholipid selection according to the polar head structure. Indeed, the polar head group affinity for Ca^{2+} ions is likely to influence the stabilisation efficiency, as ACC NPs have a positive surface charge in ethanol⁶⁴ (Fig. 5d). 1,2-Dioleoyl-*sn*-glycero-3-phospho-L-serine (DOPS), a negatively charged phospholipid was selected for the proof of concept. Phosphatidylserine (PS) phospholipids are known to interact strongly with calcium by non-covalent electrostatic interactions, resulting in the formation of dehydrated complexes.^{81–83} According to some studies, PS polar head groups are more rigid than PC head groups, and have a stronger ability to interact with each other by electrostatic interactions or hydrogen bonds.^{84,85} As a result, membranes composed of PS phospholipids are more condensed in the presence of Ca^{2+} ions compared to other phospholipid membranes.^{84–86} PS lipids, due to their negative net charge are likely to self-organise more rapidly and efficiently around ACC NPs. They should provide an effective protective layer against water without the need for PEGylated lipids, due to their condensed structural arrangement in the presence of Ca^{2+} ions. In our process, ACC NPs are put into contact with DOPS in ethanol for 1–2 minutes, followed by a one-pot injection into water with 15 seconds vortex at a ratio ethanol:water 1:9.

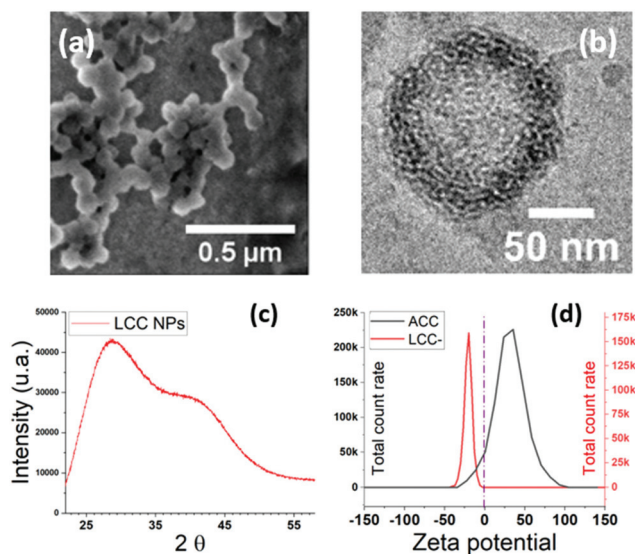


Fig. 5 Characterisation of DOPS LCC NPs. (a) SEM imaging of LCC NPs. (b) CryoTEM imaging of LCC NPs in water. (c) XRD spectra of LCC NPs in water. (d) Zeta potential of ACC NPs in ethanol (black) and LCC NPs in water.

Compared to the state of the art,²⁰ the contact time between ACC NPs and the lipids is reduced from 24 h to 1–2 min before injection into water. SEM images of the resulting LCC NPs reveal monodisperse particles with an average size of 90 nm. An average size increase of 20 nm compared to absolute ACC NPs is observed (Fig. 4d and 5a), testifying from the structuration of DOPS around ACC NPs.

A monitoring of zeta potential at pH 7 before and after stabilisation shows a switch from positive to negative values, corroborating the presence of DOPS at the surface of the NPs⁸⁷ (Fig. 5d). ACC NPs are not stable in aqueous media. Therefore, the zeta potential measurement is performed in ethanol.⁶⁴ CryoTEM imaging (Fig. 5b) reveals a singular structuration of the lipids around the LCC core, with interconnected lipid multi-assemblies. Studies using “one-pot” injection method for the stabilisation of ACC NPs using phospholipids suggest a lipid structuration in a supported lipid bilayer around the ACC NPs.^{20,39} Our study suggests that the structuration of PS phospholipids around ACC NPs does not lead to a supported lipid bilayer but to several lipid layers that are interconnected probably through hemi-fusion mechanisms⁸⁸ (Fig. 5b). Indeed, on the CryoTEM image, the multilayers are not concentric and are not separated by a water layer.⁸⁹ The fusion or hemi-fusion of PS membrane in the presence of Ca^{2+} ions is a well-known phenomenon.^{90,91} It seems that some layers are infiltrated into the first few nanometres of the porous structure of ACC NPs. The XRD spectrum confirmed the conservation of the amorphous structure of the LCC NPs core (Fig. 5c). Two wide peaks centred on 2θ values of 27° and 42° are observed, characteristics from amorphous CaCO_3 .⁷⁶

The increase of the DOPS/ CaCO_3 molar ratio leads to a size increase in the resulting LCC NPs (Fig. 6a and b). The size and



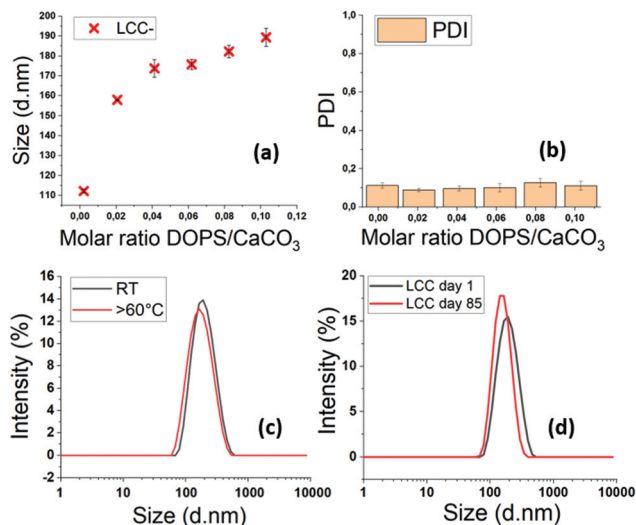


Fig. 6 (a) LCC size evolution according to the molar ratio DOPS/CaCO₃ characterized by DLS. 6 measurements were performed by sample. (b) Corresponding PDI values. (c) LCC size evolution after exposure to a temperature of 60–80 °C for 1 h, characterized by DLS. (d) LCC size dispersion at day 1 and day 85 characterized by DLS.

PDI of each sample were measured by DLS six times in a 15 min period, to ensure that the particles were stable. The minor standard deviations testify to the stability of the LCC NPs after injection in water. The PDI values around 0.1 evidence monodisperse size dispersions, even at low molar ratios DOPS/CaCO₃ (Fig. 6b). With DOPS as stabiliser, LCC NPs remain stable in water with significant variations in temperature, up to 60 °C (Fig. 6c). The stability in time is up to several months in water, which is really promising in terms of *in vivo* circulation time, storage conditions, handling and transport resistance.

The influence of the lipid polar head structure on stabilisation efficiency was investigated. Several lipids with cationic (trimethylammonium-propane (TAP)), zwitterionic (PC), or anionic head group phosphatidylglycerol (PG) were selected (Table 1). The particle size and PDI measured by DLS, as well

Table 1 Effect of the lipid head group on the stabilisation efficiency. LCC size and polydispersity index are measured by DLS, and the particle concentration (particle per mL) is measured by Nanoparticle Tracking Analysis (NTA)

Stabiliser	Size (nm)	PDI	Concentration (particles per mL)
18 : 1 PS (DOPS)	162.5	0.18	1.46×10^{11}
18 : 1 TAP	104.3	0.246	6.38×10^{10}
16 : 0 PS	139.3	0.102	2.31×10^{11}
16 : 0 PC	326.4	0.322	1.25×10^{11}
16 : 0 PC + DSPE-PEG (80/20 w/w)	Out of quality range		5.71×10^{11}
16 : 0 PG	142.7	0.017	2.07×10^{11}
E-PG ^a	148.7	0.022	1.88×10^{11}

^a Egg-PH composition: 95% mixed C₁₆–C₁₈ saturated and unsaturated (~50–50).

as the concentration monitored by Nanoparticle Tracking Analysis (NTA) of the resulting LCC NPs, were compared to the values obtained with PS phospholipids, which were used as a reference. Samples were synthesised at a constant mass of lipid and ACC NPs.

An effective stabilisation was also observed using negatively charged lipids with a PG polar head. The LCC NPs sizes and concentrations using PG phospholipids were comparable with the values obtained with PS phospholipids of a similar aliphatic chain length (Table 1). PDIs were inferior to 0.1, evidencing monodisperse size populations.

On the contrary, the comparison between 18 : 1 TAP and 18 : 1 PS lipids showed a PDI increase from 0.18 to 0.246, and a concentration drop from 1.46×10^{11} NPs per mL to 6.38×10^{10} NPs per mL when using TAP lipids as stabilisers. This evidenced a lack of stabilisation, leading to polydisperse samples and concentration drop.

Using 16 : 0 PS as a reference, the comparison between the PC and PS head groups showed a PDI increase from 0.102 to 0.322, and a size increase from 139.3 nm to 326.4 nm when using PC lipids as stabilisers. This evidences a lack of stabilisation leading to polydisperse samples, with larger particles which may result from aggregation and/or crystallisation.^{28,29}

A mix of PC and DSPE-PEG phospholipids was also tested with proportions similar to the work of C. Wang *et al.*, to investigate the influence of the addition of PEGylated lipids on the NPs stabilisation with a reduced contact time between ACC NPs and lipids.²⁰ PEGylated lipids could restore the stabilisation by providing steric stabilisation to the ACC NPs.⁹² However, with our process, this lipid mix did not lead to efficient stabilisation. The size and PDI could not be monitored as the values were out of the quality range of the DLS, due to excessive polydispersity of the sample (Table 1).

To summarise, these results evidence an efficient stabilisation with negatively charged lipids, and a deficient stabilisation when using zwitterionic and cationic lipids. The addition of PEGylated lipids did not provide efficient steric stabilisation with our process when using a mix of PC + DSPE-PEG. These results demonstrated the correlation between the stabilisation efficiency and the phospholipid head structure. The lipid affinity for calcium ions is a determinant parameter for a short process using a one-pot ethanol injection. A reduction of the process time from 24 h to 2 min has been achieved compared with the closest state of the art using the ethanol injection method.²⁰ This achievement could lead to significant optimisations in the future in terms of process efficiency, operating time reduction and corresponding energy saving for the stabilisation of ACC NPs in aqueous media.

This affinity of PG lipids for ACC NPs led us to consider egg PG (E-PG), a bio-sourced phospholipid, as a stabiliser. E-PG is a mix of PG with different aliphatic chain lengths and unsaturation degrees. The size dispersion of E-PG LCC NPs characterized by DLS is narrow, with a PDI of 0.022 for a mean diameter of 148.7 nm, evidencing an efficient stabilisation (Table 1). Using E-PG as exclusive stabiliser, we achieved in this work the stabilisation of ACC NPs in water with a size



under 150 nm using only a bio-sourced phospholipid. Replacing the use of synthetic or hemi-synthetic phospholipids by E-PG could lead to the development of a more sustainable process compared with the closest state of the art, using a PEGylated phospholipid in the stabilising mix.²⁰ Furthermore, the cost of bio-sourced highly purified natural phospholipids from soybeans or egg yolk suitable for injectable applications is becoming comparable with the price of PEGylated phospholipids. Hence, the use of egg-sourced PG represents a promising green alternative in terms of process cost to the use of synthetic stabilisers for calcium carbonate nanoparticles in aqueous media. A comparative table of the different existing methods to stabilize CaCO₃ NPs in aqueous media is presented in the ESI (Fig. S12†) to illustrate the benefits of our process in terms of sustainability and stabilisation efficiency.

A test was performed in phosphate buffer solution 0.1 M with DOPS, to evaluate the stability of LCC NPs in a media suitable for biological applications (ESI Fig. S13†). The size dispersion of the DOPS-LCC NPs in PBS was characterised by DLS, showing a PDI of 0.21 for a mean diameter of 187.3 nm. The control in water presented a PDI of 0.15 for a mean diameter of 168.5 nm. Despite an increase in mean diameter and polydispersity, particles stabilise in PBS present a narrow size distribution and a mean diameter below 200 nm. The difference observed in PBS might come from the ions existing in PBS, interfering with the interaction phospholipid/ACC NPs. For possible biological application, the 10% ethanol remaining in the solution can be evaporated by rotavapor if necessary.

LCC NPS surface charge modulation

The stabilisation of ACC NPs using cationic lipids was not efficient (Table 1). However, the surface charge modulation of the LCC NPs could be achieved by the post-insertion of cationic lipids in a solution of LCC NPs. Hence, there is an electrostatic affinity between the negatively charged phospholipids used for the stabilisation of ACC NPs in water and positively charged lipids.

An ethanolic solution of 18 : 1 TAP cationic lipids is injected at room temperature in an aqueous solution of LCC NPs stabilised by DOPS (Fig. 7a). The injection is followed by high intensity mixing using a vortex. The zeta potential shifted from negative values to positive values, testifying from the structuration of the cationic lipids around the LCC NPs (Fig. 7b).

The DLS characterisation showed a narrow size distribution, with a mean diameter shifting from 95.4 nm to 105.3 nm after the injection of 18 : 1 TAP lipids at a ratio DOPS : TAP of 1 (Fig. 7c). When the DOPS : TAP ratio is increased to 10, the mean diameter shift is larger, with a shift from 115.4 nm to 152.8 nm following the injection of 18 : 1 TAP lipids (Fig. 7d). The variation in mean diameter shift in accordance with the 18 : 1 TAP concentration increase also evidences the structuration of the cationic lipids around the already formed LCC NPs stabilised by DOPS.

These results prove the possibility of post-inserting cationic lipids after the stabilisation of ACC NPs in water using DOPS in water. This post-insertion technique allows to effectively

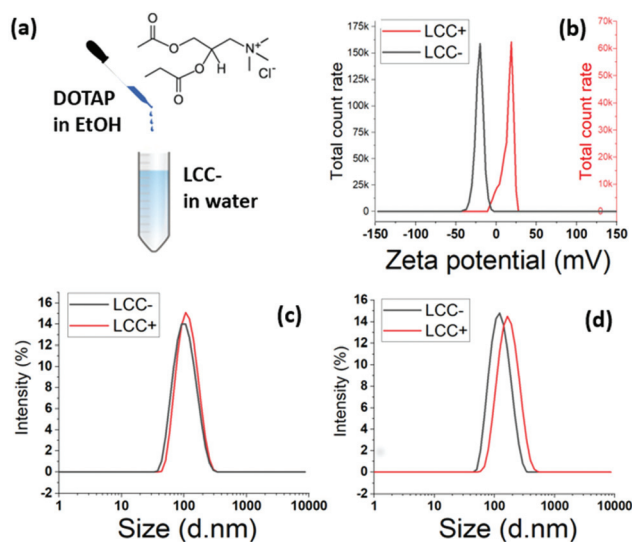


Fig. 7 Post-insertion of DOTAP to modulate the charge of LCC NPs. (a) Schematic synthesis process. (b) Zeta potential of DOPS LCC NPs (black) and DOPS/DOTAP LCC NPs (red). (c) DLS characterisation of DOPS LCC NPs before (black) and after (red) the injection of DOTAP. Molar ratio DOTAP/DOPS = 1. (d) DLS characterisation of DOPS LCC NPs before (black) and after (red) the injection of DOTAP. Molar ratio DOTAP/DOPS = 10.

tively tune the surface charge of the final LCC NPs and could pave the way for the modulation of other surface properties.

Upscaling

The ratio ethanol/water (1/9) used for the stabilisation of ACC NPs in water with the ethanol injection technique²⁰ plays an important role in the final concentration of LCC NPs. This final concentration of LCC NPs after injection is limited. The synthesis of larger amounts of LCC NPs leads to larger volumes of the water phase and of the ethanol phase. According to our experiments, the pipette injection method is efficient up to a volume of 40 mL of LCC NPs, using a 10 mL pipette for the injection of a 4 mL ethanol phase. Above this volume, we observed that the injection strength became weaker, which strongly affected the lipid structuration around the particles. We tested on a 2 L volume the replacement of the injection method by a magnetic stirring of the water phase above 500 rpm. The size dispersion of the particles remains narrow, with PDI < 0.1, and a comparable particle stability is obtained compared with the pipette injection method (ESI Fig. S14†).

These results showed injection can be replaced by strong stirring of the water phase. We tested two different upscaling techniques suitable for industrial transfer. The first one is a 50 L reactor with mechanical stirring, and the second one is a continuous mixing flow process allowing continuous flow production of the stabilised nanoparticles (Fig. 8a and b).

In the 50 L reactor we performed a synthesis on a 40 L final volume, using egg PG as stabiliser. 4 L of an ethanolic solution containing ACC NPs and egg PG was poured into 36 L of water



under strong mechanical mixing. A 5 mL control was also performed using ethanol injection method. The DLS and SEM results show highly homogeneous nanoparticles, stable in water. The size increase between the control and the upscaled sample is neglectable, under 10 nm in mean diameter (Fig. 8b and c). This experiment demonstrates the ability to upscale our process for industrial needs using large scale mechanical stirring reactors. The concern with this method was the one-pot addition of the ethanolic phase containing the ACC NPs and the stabiliser. Indeed, the addition time with larger volumes can increase. However, despite the increase of addition time from 3 s (5 mL control) to 13 s (40 L volume), the nanoparticles obtained were stable and homogeneous in size and shape.

To overcome the potential limitation of the one-pot addition of large volumes, we investigated the possibility of industrial flow production with our process. We developed a facile continuous flow mixing method using Coflore® Agitated Cell Reactor (ACR). This continuous flow reactor performs efficient mechanical agitation using multiple interlinked cell reactors (Fig. 9a). The upscaling proof of concept was performed on a final volume of 250 mL using DOPS as stabiliser. The fluxes of the ethanol phase containing ACC NPs and DOPS, and of the water phase were determined according to the ratio water:ethanol 9:1 used for the injection method. The flux of the ethanol phase is 1 mL min^{-1} , and the flux of water of 9 mL min^{-1} , in order to obtain a ratio 9:1 of water:ethanol at the mixing points. The final nanoparticles are stable in aqueous media and highly homogeneous in size and

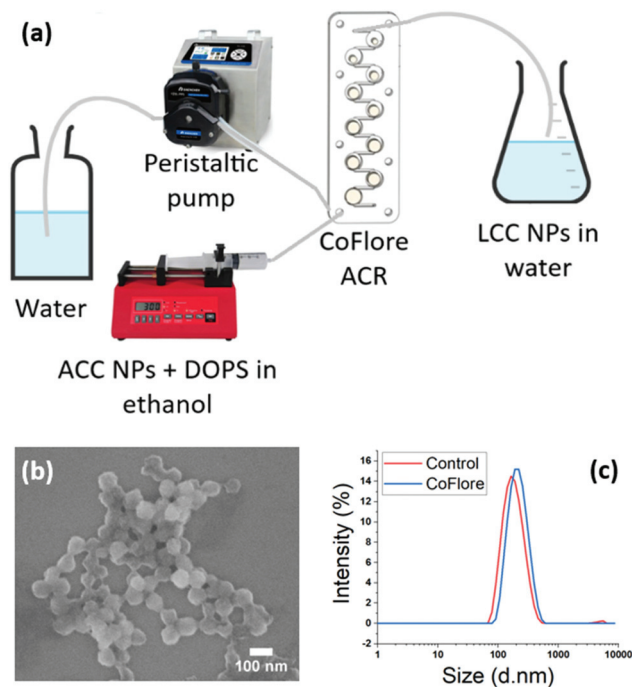


Fig. 9 Upscaling stabilisation ACC NPs by DOPS in aqueous media using the CoFloRE continuous flow reactor. (a) Schematic representation of the reactor and of the process. (b) SEM imaging of the resulting LCC NPs in aqueous media. (c) DLS characterisation of the resulting LCC NPs size dispersion with a control performed by ethanol injection in a volume of 5 mL.

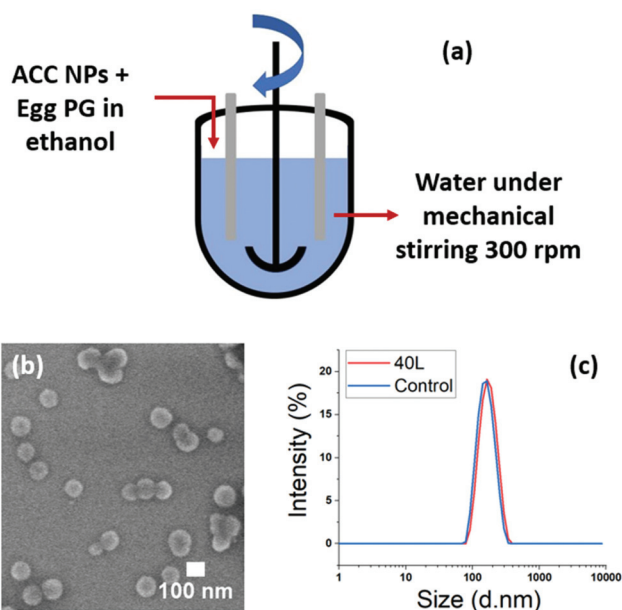


Fig. 8 Upscaling stabilisation ACC NPs by egg PG in aqueous media using a 50 L chemical reactor, for a final volume of 40 L LCC NPs. (a) Schematic representation of the reactor. (b) SEM imaging of the resulting LCC NPs in aqueous media. (c) DLS characterisation of the resulting LCC NPs size dispersion with a control performed by ethanol injection in a volume of 5 mL.

shape, with a mean size of 70 nm measured on the SEM picture (Fig. 9b and c). A control was performed on 5 mL using the ethanol injection method, showing no significant difference in size and dispersity. These results demonstrate the feasibility of switching from bulk injection and stirring to a continuous flow production using agitated cell mixing. This method has a great potential for industrial upscaling as a continuous flow process, allowing the continuous production of stabilised LCC NPs with a high control and reproducibility of the mixing conditions. High volumes can be produced with this technique. With these fluxes, 25 min are required to synthesise 250 mL.

Conclusions

ACC NPs synthesised using ethanol as solvent are monodispersed with a mean diameter under 150 nm without the need for synthetic additives. The particle size growth follows a power law between 2 h and 49 h reaction, maintaining a narrow size dispersion with PDI values under 0.05. Combined with the porous granular structure of ACC NPs, these results suggest a formation of ACC NPs by a first homogeneous nucleation event, followed by a growth by autocatalytic heterogeneous nucleation happening on the ACC NPs surface irregularities. We demonstrated the importance of the diffusion of water and ammonia to catalyse the formation of ACC NPs in



ethanol. Consequently, we observed that the removal of the DB and of drierite increased the process efficiency by a factor of 3.5. Therefore, the volume of ethanol required to produce a determined mass of ACC NPs can be divided by 3.5, reducing the ecological impact of the process.

Subsequently, our works focussed on the stabilisation in aqueous media of the resulting ACC NPs for biomedical and healthcare applications. The adaptation of the ethanol injection process using phospholipids represents to this date the greenest process for the stabilisation of ACC NPs in water. We rationalised the selection of the phospholipids according to their natural electrostatic affinity for ACC NPs and were able to reduce the process time from 24 h to 2 min. The use of PS and PG phospholipids provides an efficient electrostatic stabilisation of the ACC NPs, without the need for additional PEGylated lipids. Compared with the state of the art, the absence of PEGylated lipids increases the sustainability of the process and the biotolerance of the final particles. The reduction of the process duration consequently decreases its operating time and energy consumption. The obtained LCC NPs were highly monodisperse, with an excellent stability in temperature (up to 60 °C) and time (up to three months) variations. The efficiency of PG lipids led to the identification of an egg-sourced phospholipid as a suitable bio-sourced stabiliser. Our process was demonstrated suitable for industrial large-scale production in one pot using a 50 L chemical reactor with mechanical stirring, and in continuous flow production using the Coflore® Agitated Cell Reactor.

This work aims to contribute to the transition toward sustainable processes in the development of ACC NPs technologies suitable for biomedical and cosmetic applications.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The authors acknowledge the Fonds National de la Recherche (FNR) of Luxembourg for supporting this work through the projects MASSENA PRIDE/15/10935404. The authors also acknowledge the support and the use of resources of the French Infrastructure for Integrated Structural Biology FRISBI ANR-10-INBS-05 and of Instruct-ERIC. They particularly thank Corinne Crucifix for her help with CryoTEM sample preparation and images collection. From the Luxembourg Institute of Science and Technology, the authors acknowledge J. N. Audinot for insightful discussions and the acquisition of the HIM data, Y. Fleming from the Characterization Platform for performing the XRD measurements and his valuable help with the analysis of the results, and S. Krishnamoorthy for his valuable insights on the writing. The authors acknowledge the programs Nanofar (EMJD Europ) and Nanofar+ (Pays de la

Loire, France) for their help and support in the first author training.

Notes and references

- 1 A. Syafiq, *et al.*, Facile synthesize of transparent hydrophobic nano-CaCO₃ based coatings for self-cleaning and anti-fogging, *Mater. Chem. Phys.*, 2020, **239**, 121913.
- 2 N. Farghal and H. Elkafrawy, The effects of activated charcoal and calcium carbonate based toothpastes on surface properties of composite resin restorative materials, *Egypt. Dent. J.*, 2020, **66**, 2431–2438.
- 3 E. T. Hwang, *et al.*, Highly Stable and Fine-Textured Hybrid Microspheres for Entrapment of Cosmetic Active Ingredients, *ACS Omega*, 2020, **5**, 29577–29584.
- 4 A. D. Woldetsadik, S. K. Sharma, S. Khapli, R. Jagannathan and M. Magzoub, Hierarchically porous calcium carbonate scaffolds for bone tissue engineering, *ACS Biomater. Sci. Eng.*, 2017, **3**, 2457–2469.
- 5 M. L. P. Vidallon, *et al.*, Gas-Generating, pH-Responsive Calcium Carbonate Hybrid Particles with Biomimetic Coating for Contrast-Enhanced Ultrasound Imaging, *Part. Part. Syst. Charact.*, 2020, **37**, 1900471.
- 6 A. Som, *et al.*, Monodispersed calcium carbonate nanoparticles modulate local pH and inhibit tumor growth in vivo, *Nanoscale*, 2016, **8**, 12639–12647.
- 7 P. Zhao, *et al.*, Enhancing anti-tumor efficiency in hepatocellular carcinoma through the autophagy inhibition by miR-375/sorafenib in lipid-coated calcium carbonate nanoparticles, *Acta Biomater.*, 2018, **72**, 248–255.
- 8 M. d'Amora, F. Liendo, F. A. Deorsola, S. Bensaid and S. Giordani, Toxicological profile of calcium carbonate nanoparticles for industrial applications, *Colloids Surf., B*, 2020, **190**, 110947.
- 9 N. M. Elbaz, A. Owen, S. Rannard and T. O. McDonald, Controlled synthesis of calcium carbonate nanoparticles and stimuli-responsive multi-layered nanocapsules for oral drug delivery, *Int. J. Pharm.*, 2020, **574**, 118866.
- 10 N. I. Hammadi, *et al.*, Formulation of a sustained release docetaxel loaded cockle shell-derived calcium carbonate nanoparticles against breast cancer, *Pharm. Res.*, 2017, **34**, 1193–1203.
- 11 C. Wang, *et al.*, Mitoxantrone-preloaded water-responsive phospholipid-amorphous calcium carbonate hybrid nanoparticles for targeted and effective cancer therapy, *Int. J. Nanomed.*, 2019, **14**, 1503.
- 12 R. K. Thapa, *et al.*, Progressive slowdown/prevention of cellular senescence by CD9-targeted delivery of rapamycin using lactose-wrapped calcium carbonate nanoparticles, *Sci. Rep.*, 2017, **7**, 1–11.
- 13 A. K. Iyer, G. Khaled, J. Fang and H. Maeda, Exploiting the enhanced permeability and retention effect for tumor targeting, *Drug Discovery Today*, 2006, **11**, 812–818.
- 14 H. Nehoff, N. N. Parayath, L. Domanovitch, S. Taurin and K. Greish, Nanomedicine for drug targeting: strategies



- beyond the enhanced permeability and retention effect, *Int. J. Nanomed.*, 2014, **9**, 2539.
- 15 G. Fytianos, A. Rahdar and G. Z. Kyzas, Nanomaterials in cosmetics: Recent updates, *Nanomaterials*, 2020, **10**, 979.
 - 16 F. Carrouel, S. Viennot, L. Ottolenghi, C. Gaillard and D. Bourgeois, Nanoparticles as anti-microbial, anti-inflammatory, and remineralizing agents in oral care cosmetics: a review of the current situation, *Nanomaterials*, 2020, **10**, 140.
 - 17 J. Marto, *et al.*, Pickering Emulsions Stabilized by Calcium Carbonate Particles: A New Topical Formulation, *Cosmetics*, 2020, **7**, 62.
 - 18 F. A. Andersen and L. Brecevic, Infrared spectra of amorphous and crystalline calcium carbonate, *Acta Chem. Scand.*, 1991, **45**, 1018–1024.
 - 19 N. H. de Leeuw and S. C. Parker, Surface structure and morphology of calcium carbonate polymorphs calcite, aragonite, and vaterite: an atomistic approach, *J. Phys. Chem. B*, 1998, **102**, 2914–2922.
 - 20 C. Wang, *et al.*, Facile preparation of phospholipid–amorphous calcium carbonate hybrid nanoparticles: toward controllable burst drug release and enhanced tumor penetration, *Chem. Commun.*, 2018, **54**, 13080–13083.
 - 21 S.-F. Chen, H. Cölfen, M. Antonietti and S.-H. Yu, Ethanol assisted synthesis of pure and stable amorphous calcium carbonate nanoparticles, *Chem. Commun.*, 2013, **49**, 9564–9566.
 - 22 C. Wang, S. Chen, Q. Yu, F. Hu and H. Yuan, Taking advantage of the disadvantage: employing the high aqueous instability of amorphous calcium carbonate to realize burst drug release within cancer cells, *J. Mater. Chem. B*, 2017, **5**, 2068–2073.
 - 23 C. Wang, *et al.*, Lipase-triggered water-responsive “Pandora’s Box” for cancer therapy: Toward induced neighboring effect and enhanced drug penetration, *Adv. Mater.*, 2018, **30**, 1706407.
 - 24 D. Gebauer, X. Liu, B. Aziz, N. Hedin and Z. Zhao, Porous tablets of crystalline calcium carbonate via sintering of amorphous nanoparticles, *CrystEngComm*, 2013, **15**, 1257–1263.
 - 25 R. Sun, *et al.*, Amorphous calcium carbonate constructed from nanoparticle aggregates with unprecedented surface area and mesoporosity, *ACS Appl. Mater. Interfaces*, 2018, **10**, 21556–21564.
 - 26 Y. Zhao, *et al.*, A preloaded amorphous calcium carbonate/doxorubicin@ silica nanoreactor for pH-responsive delivery of an anticancer drug, *Angew. Chem., Int. Ed.*, 2015, **54**, 919–922.
 - 27 Y. Nakashima, C. Takai, H. Razavi-Khosroshahi, W. Suthabanditpong and M. Fuji, Synthesis of ultra-small hollow silica nanoparticles using the prepared amorphous calcium carbonate in one-pot process, *Adv. Powder Technol.*, 2018, **29**, 904–908.
 - 28 J. Xiao, Z. Wang, Y. Tang and S. Yang, Biomimetic mineralization of CaCO₃ on a phospholipid monolayer: from an amorphous calcium carbonate precursor to calcite via vaterite, *Langmuir*, 2010, **26**, 4977–4983.
 - 29 Q. Shen, *et al.*, Properties of amorphous calcium carbonate and the template action of vaterite spheres, *J. Phys. Chem. B*, 2006, **110**, 2994–3000.
 - 30 G.-B. Cai, G.-X. Zhao, X.-K. Wang and S.-H. Yu, Synthesis of polyacrylic acid stabilized amorphous calcium carbonate nanoparticles and their application for removal of toxic heavy metal ions in water, *J. Phys. Chem. C*, 2010, **114**, 12948–12954.
 - 31 A. Barhoum, *et al.*, Effect of cationic and anionic surfactants on the application of calcium carbonate nanoparticles in paper coating, *ACS Appl. Mater. Interfaces*, 2014, **6**, 2734–2744.
 - 32 C.-F. Dai, *et al.*, Methotrexate intercalated calcium carbonate nanostructures: synthesis, phase transformation and bioassay study, *Mater. Sci. Eng. C*, 2016, **69**, 577–583.
 - 33 C.-F. Dai, W.-Y. Wang, S.-P. Li and X.-D. Li, Synthesis of nanostructured calcium carbonate/methotrexate@ silica and its application in cancer therapy, *RSC Adv.*, 2016, **6**, 68335–68340.
 - 34 C. Xu, *et al.*, Biodegradable Nanoparticles of Polyacrylic Acid-Stabilized Amorphous CaCO₃ for Tunable pH-Responsive Drug Delivery and Enhanced Tumor Inhibition, *Adv. Funct. Mater.*, 2019, **29**, 1808146.
 - 35 K. H. Min, *et al.*, pH-controlled gas-generating mineralized nanoparticles: a theranostic agent for ultrasound imaging and therapy of cancers, *ACS Nano*, 2015, **9**, 134–145.
 - 36 J. Lee, *et al.*, Theranostic gas-generating nanoparticles for targeted ultrasound imaging and treatment of neuroblastoma, *J. Controlled Release*, 2016, **223**, 197–206.
 - 37 S. K. Kim, M. B. Foote and L. Huang, Targeted delivery of EV peptide to tumor cell cytoplasm using lipid coated calcium carbonate nanoparticles, *Cancer Lett.*, 2013, **334**, 311–318.
 - 38 P. Zhao, *et al.*, MiR-375 delivered by lipid-coated doxorubicin-calcium carbonate nanoparticles overcomes chemoresistance in hepatocellular carcinoma, *Nanomedicine*, 2017, **13**, 2507–2516.
 - 39 J. Q. Peng, *et al.*, Targeted co-delivery of protein and drug to a tumor in vivo by sophisticated RGD-modified lipid-calcium carbonate nanoparticles, *J. Controlled Release*, 2019, **302**, 42–53.
 - 40 J. Peng, *et al.*, One-step formation of lipid-polyacrylic acid-calcium carbonate nanoparticles for co-delivery of doxorubicin and curcumin, *J. Drug Targeting*, 2017, **25**, 704–714.
 - 41 C. C. Tester, *et al.*, In vitro synthesis and stabilization of amorphous calcium carbonate (ACC) nanoparticles within liposomes, *CrystEngComm*, 2011, **13**, 3975–3978.
 - 42 C. C. Tester, C.-H. Wu, S. Weigand and D. Joester, Precipitation of ACC in liposomes—a model for biomineralization in confined volumes, *Faraday Discuss.*, 2012, **159**, 345–356.
 - 43 A. Szczeńś, Effects of DPPC/Cholesterol liposomes on the properties of freshly precipitated calcium carbonate, *Colloids Surf., B*, 2013, **101**, 44–48.
 - 44 A. Szczeńś and D. Sternik, Properties of calcium carbonate precipitated in the presence of DPPC liposomes modified



- with the phospholipase A 2, *J. Therm. Anal. Calorim.*, 2016, **123**, 2357–2365.
- 45 H. S. Lee, T. H. Ha and K. Kim, Fabrication of unusually stable amorphous calcium carbonate in an ethanol medium, *Mater. Chem. Phys.*, 2005, **93**, 376–382.
- 46 H. Zhou, *et al.*, Co-precipitation of calcium carbonate and curcumin in an ethanol medium as a novel approach for curcumin dissolution enhancement, *J. Drug Delivery Sci. Technol.*, 2019, **51**, 397–402.
- 47 Z. Dong, *et al.*, CaCO₃ nanoparticles as an ultra-sensitive tumor-pH-responsive nanoplatfrom enabling real-time drug release monitoring and cancer combination therapy, *Biomaterials*, 2016, **110**, 60–70.
- 48 A. Som, *et al.*, Calcium carbonate nanoparticles stimulate tumor metabolic reprogramming and modulate tumor metastasis, *Nanomedicine*, 2019, **14**, 169–182.
- 49 C. Rao, *et al.*, In vitro preparation and characterization of amorphous calcium carbonate nanoparticles for applications in curcumin delivery, *J. Mater. Sci.*, 2019, **54**, 11243–11253.
- 50 S. F. Lam, K. W. Bishop, R. Mintz, L. Fang and S. Achilefu, Calcium carbonate nanoparticles stimulate cancer cell reprogramming to suppress tumor growth and invasion in an organ-on-a-chip system, *Sci. Rep.*, 2021, **11**, 1–12.
- 51 J. Ihli, P. Bots, A. Kulak, L. G. Benning and F. C. Meldrum, Elucidating Mechanisms of Diffusion-Based Calcium Carbonate Synthesis Leads to Controlled Mesocrystal Formation, *Adv. Funct. Mater.*, 2013, **23**, 1965–1973.
- 52 M. Mantilaka, R. Rajapakse, D. Karunaratne and H. Pitawala, Preparation of amorphous calcium carbonate nanoparticles from impure dolomitic marble with the aid of poly (acrylic acid) as a stabilizer, *Adv. Powder Technol.*, 2014, **25**, 591–598.
- 53 S. Bom, *et al.*, Replacing Synthetic Ingredients by Sustainable Natural Alternatives: A Case Study Using Topical O/W Emulsions, *Molecules*, 2020, **25**, 4887.
- 54 N. Hadjesfandiari and A. Parambath, in *Engineering of Biomaterials for Drug Delivery Systems*, ed. A. Parambath, Woodhead Publishing, 2018, pp. 345–361.
- 55 L. Simon, *et al.*, Polyoxazolines based mixed micelles as PEG free formulations for an effective quercetin anti-oxidant topical delivery, *Int. J. Pharm.*, 2019, **570**, 118516, DOI: 10.1016/j.ijpharm.2019.118516.
- 56 I. M. Banat, Q. Carboué, G. Saucedo-Castañeda and d. J. Cázares-Marinero, J. Biosurfactants: The green generation of speciality chemicals and potential production using Solid-State fermentation (SSF) technology, *Bioresour. Technol.*, 2021, **320**, 124222, DOI: 10.1016/j.biortech.2020.124222.
- 57 P. Zhang, F. Sun, S. Liu and S. Jiang, Anti-PEG antibodies in the clinic: Current issues and beyond PEGylation, *J. Controlled Release*, 2016, **244**, 184–193.
- 58 Q. Yang and S. K. Lai, Anti-PEG immunity: emergence, characteristics, and unaddressed questions, *Wiley Interdiscip. Rev.: Nanomed. Nanobiotechnol.*, 2015, **7**, 655–677.
- 59 G. Kozma, T. Shimizu, T. Ishida and J. Szebeni, Anti-PEG antibodies: Properties, formation and role in adverse immune reactions to PEGylated nano-biopharmaceuticals, *Adv. Drug Delivery Rev.*, 2020, **154–155**, 163–175.
- 60 T. T. Hoang Thi, *et al.*, The Importance of Poly(ethylene glycol) Alternatives for Overcoming PEG Immunogenicity in Drug Delivery and Bioconjugation, *Polymers*, 2020, **12**, 298.
- 61 P. Sellaturay, S. Nasser and P. Ewan, Polyethylene Glycol-Induced Systemic Allergic Reactions (Anaphylaxis), *J. Allergy Clin. Immunol.*, 2021, **9**, 670–675, DOI: 10.1016/j.jaip.2020.09.029.
- 62 F. Cox, K. Khalib and N. Conlon, PEG That Reaction: A Case Series of Allergy to Polyethylene Glycol, *J. Clin. Pharmacol.*, 2021, **61**, 832–835, DOI: 10.1002/jcph.1824.
- 63 R. S. Lane, F. M. Haller, A. A. Chavarroche, A. Almond and P. L. DeAngelis, Heparosan-coated liposomes for drug delivery, *Glycobiology*, 2017, **27**, 1062–1074.
- 64 M. E. Labib and R. Williams, The use of zeta-potential measurements in organic solvents to determine the donor–acceptor properties of solid surfaces, *J. Colloid Interface Sci.*, 1984, **97**, 356–366.
- 65 T. Wirtz, O. De Castro, J.-N. Audinot and P. Philipp, Imaging and analytics on the helium ion microscope, *Annu. Rev. Anal. Chem.*, 2019, **12**, 523–543.
- 66 J. Zernike and Q. J. Ahmed, Three-phase curve of ammonium bicarbonate, *Recl. Trav. Chim. Pays-Bas*, 1954, **73**, 95–101.
- 67 K.-S. Seo, C. Han, J.-H. Wee, J.-K. Park and J.-W. Ahn, Synthesis of calcium carbonate in a pure ethanol and aqueous ethanol solution as the solvent, *J. Cryst. Growth*, 2005, **276**, 680–687.
- 68 E. Peh, A. Taubert and K. Tauer, Ammonium carbonate gas diffusion crystallization in a continuous organic medium leads to dendritic calcium carbonate, *Matters*, 2017, **3**, e201706000012.
- 69 N. T. Thanh, N. Maclean and S. Mahiddine, Mechanisms of nucleation and growth of nanoparticles in solution, *Chem. Rev.*, 2014, **114**, 7610–7630.
- 70 D. Jaynes and A. Rogowski, Applicability of Fick's law to gas diffusion, *Soil Sci. Soc. Am. J.*, 1983, **47**, 425–430.
- 71 N. Koga, Y. Yamane and T. Kimura, Thermally induced transformations of calcium carbonate polymorphs precipitated selectively in ethanol/water solutions, *Thermochim. Acta*, 2011, **512**, 13–21.
- 72 M. Farhadi-Khouzani, D. M. Chevrier, P. Zhang, N. Hedin and D. Gebauer, Water as the key to proto-aragonite amorphous CaCO₃, *Angew. Chem., Int. Ed.*, 2016, **55**, 8117–8120.
- 73 S. R. Golisz, J. S. Yang and R. D. Johnson, Understanding the effect of CO₂ on the pHe of fuel ethanol, *Fuel*, 2017, **199**, 1–3.
- 74 T. K. Sherwood, Solubilities of sulfur dioxide and ammonia in water, *Ind. Eng. Chem.*, 1925, **17**, 745–747.
- 75 L.-J. Huang, W.-L. Xue and Z.-X. Zeng, The Solubility of ammonia in ethanol between 277.35 K and 328.15 K, *Fluid Phase Equilib.*, 2011, **303**, 80–84.



- 76 A. Radha, T. Z. Forbes, C. E. Killian, P. Gilbert and A. Navrotsky, Transformation and crystallization energetics of synthetic and biogenic amorphous calcium carbonate, *Proc. Natl. Acad. Sci. U. S. A.*, 2010, **107**, 16438–16443.
- 77 G.-T. Zhou, Q.-Z. Yao, S.-Q. Fu and Y.-B. Guan, Controlled crystallization of unstable vaterite with distinct morphologies and their polymorphic transition to stable calcite, *Eur. J. Mineral.*, 2010, **22**, 259–269.
- 78 Y. Politi, T. Arad, E. Klein, S. Weiner and L. Addadi, Sea urchin spine calcite forms via a transient amorphous calcium carbonate phase, *Science*, 2004, **306**, 1161–1164.
- 79 Z. Yaari, *et al.*, Theranostic barcoded nanoparticles for personalized cancer medicine, *Nat. Commun.*, 2016, **7**, 1–10.
- 80 M. Pons, M. Foradada and J. Estelrich, Liposomes obtained by the ethanol injection method, *Int. J. Pharm.*, 1993, **95**, 51–56.
- 81 H. Hauser, E. Finer and A. Darke, Crystalline anhydrous Ca-phosphatidylserine bilayers, *Biochem. Biophys. Res. Commun.*, 1977, **76**, 267–274.
- 82 R. Dluhy, D. G. Cameron, H. H. Mantsch and R. Mendelsohn, Fourier transform infrared spectroscopic studies of the effect of calcium ions on phosphatidylserine, *Biochemistry*, 1983, **22**, 6318–6325.
- 83 M. Roux and M. Bloom, Calcium binding by phosphatidylserine headgroups. Deuterium NMR study, *Biophys. J.*, 1991, **60**, 38–44.
- 84 J. L. Browning and J. Seelig, Bilayers of phosphatidylserine: a deuterium and phosphorus nuclear magnetic resonance study, *Biochemistry*, 1980, **19**, 1262–1270.
- 85 G. Büldt and R. Wohlgemuth, The headgroup conformation of phospholipids in membranes, *J. Membr. Biol.*, 1981, **58**, 81–100.
- 86 A. Melcrová, *et al.*, The complex nature of calcium cation interactions with phospholipid bilayers, *Sci. Rep.*, 2016, **6**, 38035.
- 87 M. H. Derkani, *et al.*, Mechanisms of surface charge modification of carbonates in aqueous electrolyte solutions, *Colloids Interfaces*, 2019, **3**, 62.
- 88 X. Banquy, K. Kristiansen, D. W. Lee and J. N. Israelachvili, Adhesion and hemifusion of cytoplasmic myelin lipid membranes are highly dependent on the lipid composition, *Biochim. Biophys. Acta, Biomembr.*, 2012, **1818**, 402–410.
- 89 H. L. Scott, *et al.*, On the mechanism of bilayer separation by extrusion, or why your LUVs are not really unilamellar, *Biophys. J.*, 2019, **117**, 1381–1386.
- 90 N. Düzgüne, *et al.*, Calcium-and magnesium-induced fusion of mixed phosphatidylserine/phosphatidylcholine vesicles: effect of ion binding, *J. Membr. Biol.*, 1981, **59**, 115–125.
- 91 Z. D. Schultz, I. M. Pazos, F. K. McNeil-Watson, E. N. Lewis and I. W. Levin, Magnesium-induced lipid bilayer microdomain reorganizations: implications for membrane fusion, *J. Phys. Chem. B*, 2009, **113**, 9932–9941.
- 92 J. Zhai, *et al.*, Lipid-PEG conjugates sterically stabilize and reduce the toxicity of phytantriol-based lyotropic liquid crystalline nanoparticles, *Langmuir*, 2015, **31**, 10871–10880.

