

Cite this: *Chem. Sci.*, 2021, 12, 331

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Engineering reversible cell–cell interactions using enzymatically lipidated chemically self-assembled nanorings†

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Multicellular biology is dependent on the control of cell–cell interactions. These concepts have begun to be exploited for engineering of cell-based therapies. Herein, we detail the use of a multivalent lipidated scaffold for the rapid and reversible manipulation of cell–cell interactions. Chemically self-assembled nanorings (CSANs) are formed via the oligomerization of bivalent dihydrofolate reductase (DHFR²) fusion proteins using a chemical dimerizer, bis-methotrexate. With targeting proteins fused onto the DHFR² monomers, the CSANs can target specific cellular antigens. Here, anti-EGFR or anti-EpCAM fibronectin-DHFR² monomers incorporating a CAAX-box sequence were enzymatically prenylated, then assembled into the corresponding CSANs. Both farnesylated and geranylgeranylated CSANs efficiently modified the cell surface of lymphocytes and remained bound to the cell surface with a half-life of >3 days. Co-localization studies revealed a preference for the prenylated nanorings to associate with lipid rafts. The presence of antigen targeting elements in these bifunctional constructs enabled them to specifically interact with target cells while treatment with trimethoprim resulted in rapid CSAN disassembly and termination of the cell–cell interactions. Hence, we were able to determine that activated PBMCs modified with the prenylated CSANs caused irreversible selective cytotoxicity toward EGFR-expressing cells within 2 hours without direct engagement of CD3. The ability to disassemble these nanostructures in a temporally controlled manner provides a unique platform for studying cell–cell interactions and T cell-mediated cytotoxicity. Overall, antigen-targeted prenylated CSANs provide a general approach for the regulation of specific cell–cell interactions and will be valuable for a plethora of fundamental and therapeutic applications.

Received 8th June 2020

Accepted 22nd October 2020

DOI: 10.1039/d0sc03194a

rsc.li/chemical-science

Introduction

Cell-based therapies have demonstrated notable therapeutic success when applied to tissue engineering, regenerative medicine, and cancer immunotherapy.^{1–3} These recent advances have highlighted the significance of controlling the fate and function of therapeutic cells. Typically, the efficacy of therapeutic cells is dependent on their ability to interact directly with other cells. Therefore, techniques that can efficiently regulate cell–cell interactions are regarded as valuable tools for cell-based therapies.^{4–6}

While the engineering of cell–cell interactions has been dominated by genetic methodologies such as chimeric antigen

receptors (CARs), non-genetic cell surface modification is an attractive alternative since the cell surface can be directly modified without the need for genomic alterations or optimization of transfection efficiencies.⁷ Existing cell surface antigens are commonly utilized as handles for subsequent surface modification. For instance, bispecific T cell engagers are well-studied scaffolds that generally decorate the cancer cell surface with antigen-targeting scFvs that can also bind the pan-T cell antigen, CD3.^{8–10} While highly successful, the induced cell–cell interactions by bispecific antibodies are restricted to the binding specificity of the incorporated antibodies. While metabolic labeling can universally incorporate novel functional groups into the plasma membrane, the requisite cell culture steps and bio-orthogonal reactions are time-consuming.¹¹ Finally, some one-step lipid insertion methods can directly anchor targeting molecules on the cell surface through hydrophobic interactions with membrane lipids; however, the modifications are usually stable for mere hours^{12,13} and, in some cases, both cell types must be modified.¹⁴

To address these issues, our lab has developed a multivalent protein scaffold referred to as chemically self-assembled

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† Electronic supplementary information (ESI) available. See DOI: 10.1039/d0sc03194a

nanorings (CSANs).¹⁵ We have previously demonstrated that CSANs can be engineered to stably associate with cell membranes and mediate reversible cell–cell interactions.^{16,17} CSANs are prepared by the oligomerization of bivalent dihydrofolate reductase (DHFR²) fusion proteins using a chemical dimerizer, bis-methotrexate (bisMTX). This results in the formation of a predominantly octameric nanoring structure with uniform size distribution.^{15,16} Importantly, the nanorings can be disassembled by treatment with the FDA-approved antibiotic, trimethoprim, thereby rendering ring formation reversible.¹⁷

Antibody-derived ligands are widely used scaffolds for cell targeting and cell–cell interaction studies. However, their biophysical properties make them less than optimal for many fundamental and clinical applications.¹⁸ As an alternative, our lab has evolved human tenth type III fibronectin (Fn3) domains capable of binding to epidermal growth factor receptor (EGFR) or epithelial cell adhesion molecule (EpCAM).¹⁹ When these Fn3 domains were recombinantly tethered to the DHFR² fusion proteins, the resultant monomers were assembled into CSANs capable of binding to cells that overexpress these carcinoma antigens.²⁰

Previously, we demonstrated that bifunctional CSANs can be installed on cell membranes *via* hydrophobic insertion using either of two approaches: (1) employing a phospholipid-bisMTX conjugate to form lipid-modified CSANs; or (2) first modifying the cell surface with biotinylated or clickable phospholipids, and then treating these cells with CSANs fused to monovalent streptavidin (mSA) or CSANs formed with trivalent azide-bisMTX, respectively.^{20,21} Nevertheless, these methods have significant limitations, as the first approach poses the synthetic challenge of preparing pure phospholipid-bisMTX, while the second approach requires a multi-step process and leaves residual conjugates on the cell surface. Therefore, the development of targeted CSANs that can be enzymatically lipidated would significantly streamline their preparation and hence dramatically expand their utility in engineering cell–cell interactions.

Protein prenyltransferases catalyze the addition of C15 (farnesyl) and C20 (geranylgeranyl) lipids to proteins containing C-terminal CAAX-motifs.^{22–26} Following lipid modification, these prenylated proteins translocate to cellular membranes.²⁷ Since the CAAX-box sequence is the only requirement for prenyltransferase recognition, essentially any protein can be lipidated by genetic fusion of a CAAX-box onto the C-terminus of the protein of interest.^{28,29} Hence, we envisioned that the fusion of a functionalized DHFR² with such a sequence (CVIA) would facilitate the preparation of lipidated proteins suitable for CSAN assembly. This enzymatic process allows lipidation to be accomplished in a single step and is much more efficient than chemical conjugation reactions.^{28,30} Therefore, the resulting prenylated CSANs could directly modify any mammalian cell membrane with multivalent targeting elements through hydrophobic interactions between the isoprenoids and membrane phospholipids (Fig. 1). Moreover, the multivalency of these prenylated CSANs would make them more stable on the

cell membrane than other monomeric lipid-modified constructs.^{31,32}

In this study, we prepared three distinct DHFR² fusion proteins, all of which include the CAAX-box sequence CVIA appended at their C-terminus. Two of these proteins also incorporate an Fn3-based targeting domain at their N-terminus, while the third lacks a targeting ligand and thereby remains agnostic (DHFR²-CVIA). One of the targeted entities utilizes an EGFR-targeting Fn3 (E1-DHFR²-CVIA) and the other uses an EpCAM-targeting Fn3 (Ep-DHFR²-CVIA). We demonstrate that both farnesyl transferase and geranylgeranyl transferase are able to efficiently and quantitatively generate lipid-modified E1-DHFR²-CVIA and Ep-DHFR²-CVIA proteins, and that these monomers easily assemble into nanorings that can modify cell surface membranes in a single step. The modification is stable for days and can direct specific, antigen-targeted cell–cell interactions that can be reversed using trimethoprim. This system was also used to demonstrate that activated T cells modified with prenylated anti-EGFR CSANs will fully initiate cell killing within two hours. Those results highlight the unique ensemble of properties including simplicity, tunability and reversibility that make prenylated CSANs particularly suitable for studying cell–cell interactions.

Results

Anti-EGFR and anti-EpCAM Fn3 proteins were previously generated based on the human tenth type III fibronectin domain.^{19,33} Here, the Fn3 proteins were genetically fused to the N-terminus of DHFR² fusion proteins, while a CVIA sequence was appended to the C-terminus to generate the E1-DHFR²-CVIA and Ep-DHFR²-CVIA fusion proteins (ESI Note 1†). The proteins were expressed in soluble form in *E. coli* and characterized by gel electrophoresis (Fig. 2a). The CVIA-tagged proteins were shown to be substrates for both farnesyl transferase and geranylgeranyl transferase, which modify the C-terminal cysteine with either a farnesyl group or a geranylgeranyl group, respectively. In this manner, the farnesylated DHFR² proteins (E1-DHFR²-Far, Ep-DHFR²-Far, and DHFR²-Far) and geranylgeranylated DHFR² proteins (E1-DHFR²-GG, Ep-DHFR²-GG, and DHFR²-GG) were generated, with modifications confirmed *via* LC-MS (Fig. 2b and S1†).

Upon the addition of a molar excess of the chemical dimerizer, bisMTX, the monomeric DHFR² fusion proteins rapidly self-assembled into ring structures that were similar to previously reported CSANs,³⁴ which was demonstrated by size exclusion chromatography (SEC; Fig. S2†). The hydrodynamic diameter of the nanorings was measured by dynamic light scattering (DLS) (Fig. 2d and S3†). The sizes of both the E1-DHFR²-CVIA CSANs and Ep-DHFR²-CVIA CSANs were found to be similar (24–25 nm) and somewhat larger than the simple DHFR²-CVIA rings (18 nm, Fig. S3†), which lack the added Fn3 targeting domain. Both farnesylated and geranylgeranylated CSANs were found to be modestly larger (33–35 nm) than their non-prenylated counterparts. Cryo-transmission electron microscopy (cryo-TEM) imaging analysis revealed that the morphology and the size of the anti-EGFR and anti-EpCAM



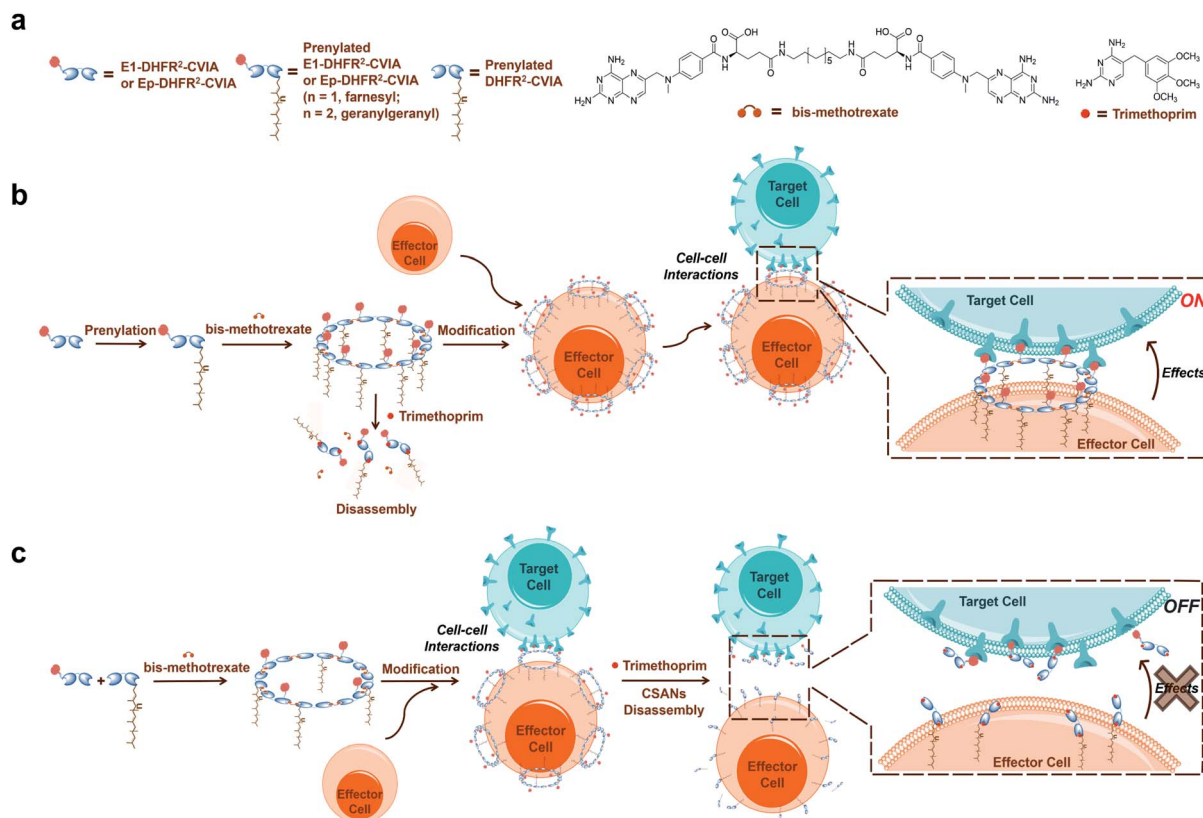


Fig. 1 Approach to directing cell–cell interactions with prenylated CSANs. (a) Components of prenylated CSANs. (b) Anti-EGFR-DHFR²-CVIA (E1-DHFR²-CVIA) or anti-EpCAM-DHFR²-CVIA (Ep-DHFR²-CVIA) proteins can be farnesylated or geranylgeranylated, and these prenylated proteins can form multivalent CSANs in the presence of bisMTX. The prenylated nanorings can modify cell surfaces through hydrophobic interactions with the plasma membrane and then target the modified cells to EGFR⁺ or EpCAM⁺ cells to form cell–cell interactions. (c) Similarly, hybrid prenylated CSANs can be constructed from E1-DHFR²-CVIA (or Ep-DHFR²-CVIA) protein that is not prenylated and pre-prenylated but non-targeted DHFR²-CVIA protein. The hybrid CSANs can mediate cell–cell interactions and can be disassembled on the cell surface using clinically relevant concentrations of trimethoprim, thereby terminating the CSAN-mediated cell–cell interactions.

CSANs were consistent with the results obtained *via* DLS studies (Fig. 2c and S4†).

The B-cell leukemia cell line, Raji, epidermoid carcinoma cell line, A431, and the breast cancer cell line, MCF-7, were used as models to assess the ability of the prenylated CSANs to modify mammalian cell membranes. The CVIA-tagged fusion proteins were farnesylated or geranylgeranylated by farnesyl transferase or geranylgeranyl transferase, respectively and oligomerized into CSANs using bisMTX (Fig. 2c and S4†). Accordingly, Raji cells, A431 cells, and MCF-7 cells were each incubated with prenylated CSANs at room temperature for 1 h and after washing, the membrane-bound CSANs were quantified using the anti-FLAG-PE antibody *via* flow cytometry. As shown, both farnesylated and geranylgeranylated CSANs effectively modified each of the cell surfaces (Fig. 3a).

To gain further insight into the nature of the interaction between prenylated CSANs and cell membranes, confocal microscopy studies were carried out with FITC labeled CSANs (Fig. 3b). Prenylated CSANs (2.5 μ M) were shown to modify the surface of Raji cells in semi-discrete areas. Staining with the lipid raft specific agent, Alexa Fluor 594-conjugated cholera toxin subunit B, revealed co-localization of CSANs and lipid

rafts. Consistent with these findings, previous studies have shown that farnesylation can target H-Ras to lipid rafts on the cytoplasmic membrane.³⁵ Importantly, neither of the prenylated CSAN species were found to be toxic to Raji or MCF-7 cells at concentrations as high as 6 μ M (Fig. S5†).

The ability of targeted CSANs to bind to antigen-expressing cell lines was assessed by flow cytometry. The anti-EGFR CSANs bound selectively to the EGFR⁺ cell line, A431, and the anti-EpCAM CSANs bound selectively to the EpCAM⁺ cell line, MCF-7 (Fig. 3c). The binding affinity of the anti-EpCAM and anti-EGFR CSANs towards EpCAM⁺ MCF-7 cells or EGFR⁺ MDA-MB-231 cells, respectively, was also assessed by flow cytometry (Fig. 3d and S6†). The CSANs were shown to bind to their target cells with high affinity (anti-EpCAM CSANs: apparent $K_d = 31 \pm 11$ nM; anti-EGFR CSANs: apparent $K_d = 16 \pm 2.4$ nM). These results are comparable to our previous studies of these fibronectin-based targeting scaffolds.^{19,20,34}

We have previously demonstrated that the apparent affinity of a targeted CSAN can be modulated by mixing different ratios of a targeting monomer with a non-targeting monomer, thereby tuning the valency of the scaffold.³⁶ Accordingly, we chose to explore the effect of various prenylation valencies on



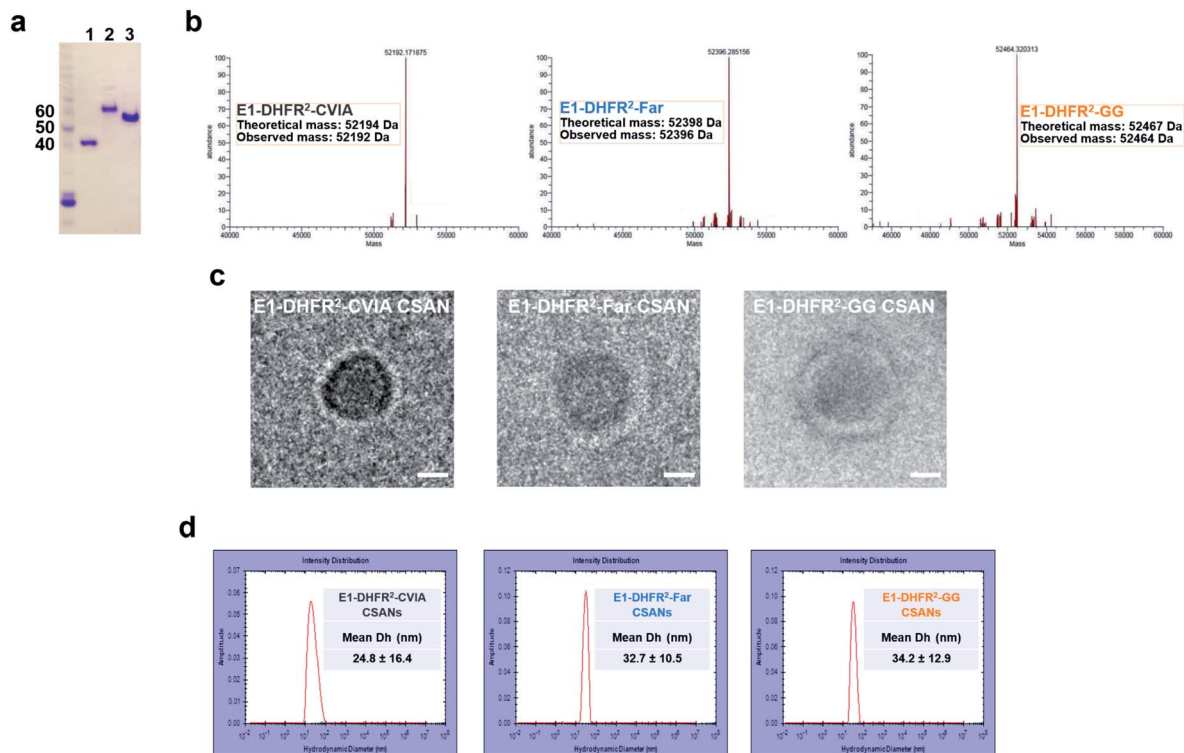


Fig. 2 Characterization of prenylated CSANs. (a) SDS-PAGE gel of DHFR²-CVIA (1), Ep-DHFR²-CVIA (2), and E1-DHFR²-CVIA (3) proteins. (b) LC-MS of E1-DHFR²-CVIA, farnesylated E1-DHFR²-CVIA (E1-DHFR²-Far) and geranylgeranylated E1-DHFR²-CVIA (E1-DHFR²-GG) proteins. Ring formation was confirmed by (c) cryo-TEM imaging of anti-EGFR nanorings (scale bar, 10 nm). (d) Hydrodynamic diameter analysis of anti-EGFR nanorings using dynamic light scattering. The E1-DHFR²-CVIA nanorings have a D_H of 25 ± 16 nm and prenylated nanorings have D_H values of 33 ± 11 nm and 34 ± 13 nm, as shown.

farnesylated and geranylgeranylated CSANs' ability to insert into Raji cell membranes (Fig. 4a). Hybrid CSANs were prepared by oligomerizing prenylated DHFR²-CVIA protein (DHFR²-Far or DHFR²-GG) with unprenylated DHFR²-CVIA at different molar ratios, including 8 : 0, 4 : 4 and 2 : 6. As such, the resultant CSANs contain different numbers of isoprenoids groups in

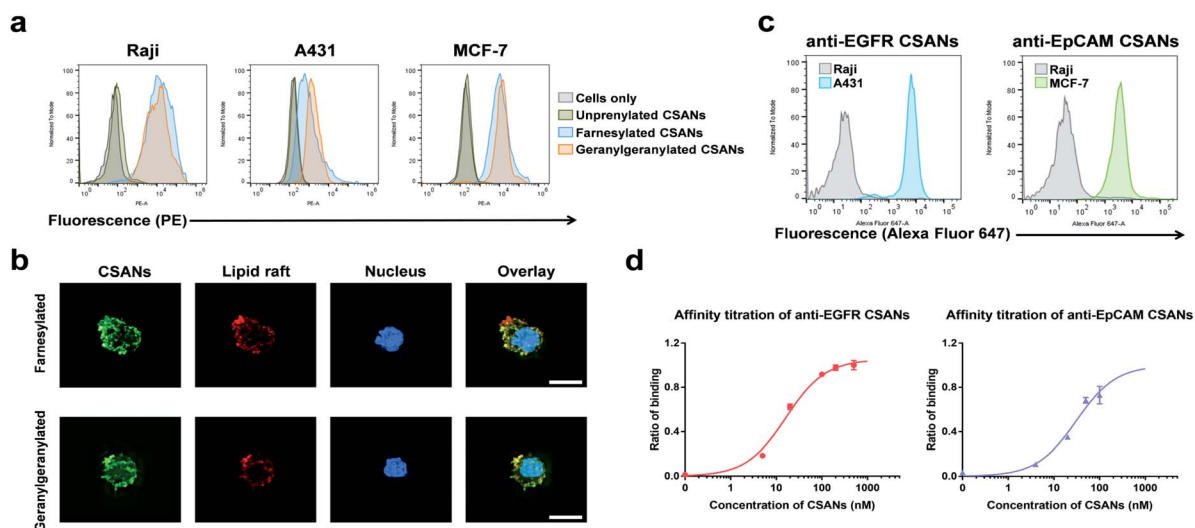


Fig. 3 Prenylated CSANs insert into cell membranes and bind to their target antigens. (a) Flow cytometry demonstrates that prenylated CSANs hydrophobically insert into the cell membrane of Raji, A431, and MCF-7 cells. (b) Fluorescent microscopy shows the prenylated CSANs localized on the plasma membrane of Raji cells. Co-staining demonstrated that the prenylated CSANs localize to membrane lipid rafts, as shown (scale bar, 10 μ m). (c) EGFR- and EpCAM-targeted CSANs bind selectively to EGFR⁺ A431 cells and EpCAM⁺ MCF-7 cells, respectively, via flow cytometry. Raji cells were used as the EGFR⁻/EpCAM⁻ cell line for both assays. (d) The apparent affinity of anti-EGFR (16.3 ± 2.4 nM) and anti-EpCAM CSANs (31.1 ± 11 nM) was assessed by flow cytometry using EGFR⁺ MDA-MB-231 cells and EpCAM⁺ MCF-7 cells, respectively.



each nanoring, with overall valencies ranging from 8–2. Cells were treated with the hybrid prenylated CSANs and incubated for 1 h at room temperature. The membrane insertion of the prenylated CSANs was then characterized by flow cytometry (Fig. S7†), and the K_d for each type of CSANs determined (Fig. 4b, c and Table S1†). In each case, CSANs composed of 100% prenylated monomers exhibited the highest membrane binding affinity, with geranylgeranylated CSANs exhibiting a higher membrane affinity (48 ± 22 nM) than farnesylated CSANs (150 ± 6.2 nM). As can be seen from Table S1,† a reduction in valency directly corresponded to a proportional reduction in the apparent affinity. Thus, although geranylgeranylated CSANs exhibited greater binding affinity, the cumulative cost per lipid loss on membrane binding was similar. It is noteworthy that the relationship between the apparent K_d values of prenylated CSANs and the prenylation valency (N) follows the equation:

$$\text{Apparent } K_{d,N} = \frac{K_{d,1}}{\text{valency}^2}$$

in which $K_{d,1}$ represents the binding affinity of the monomeric ligand (Fig. 4d). This relationship between valency and affinity is consistent with previous analyses of multivalent CSANs and the relationship between binding affinity, ligand valency, and antigen expression.³⁶

Previously, we have demonstrated that octameric phospholipid-based CSANs are stable on the cell membrane for

>72 h.^{20,21} To assess the cell surface stability of prenylated CSANs, we stained Raji cells with CellTrace Violet (CTV) and then treated them with farnesylated or geranylgeranylated CSANs prepared from prenylated DHFR²-CVIA monomers. The CSAN-modified cells were then returned to culture for 0–72 h. Every 24 h, an aliquot of cells was taken for analysis, and the remaining culture media was refreshed to partially stimulate physiologic clearance. Samples were stained using an anti-FLAG-PE antibody to label remaining cell surface CSANs before analysis by flow cytometry. The quantification of surface-bound CSANs was corrected for the dilution effect of cell division over this time period, as dictated by the CTV labeling. The results revealed that, similar to the studies utilizing phospholipid attachment, the half-life for the association of the farnesylated and geranylgeranylated CSANs was >72 h (Fig. 4e). Within this extended time frame, farnesylated CSANs appear to dissociate from the cell membrane more rapidly than the geranylgeranylated counterparts. Indeed, this difference in membrane longevity was more pronounced when comparing the farnesylated and geranylgeranylated DHFR²-CVIA monomers (Fig. 4e).

As previously reported, the treatment of CSANs with the FDA-approved antibiotic and DHFR antagonist, trimethoprim, results in rapid CSANs disassembly and a corresponding decrease in their cell membrane stability.^{20,21} To demonstrate this, Raji cells modified with CSANs were treated with a 20-fold molar excess of trimethoprim. Within 24 h, greater than 60% of

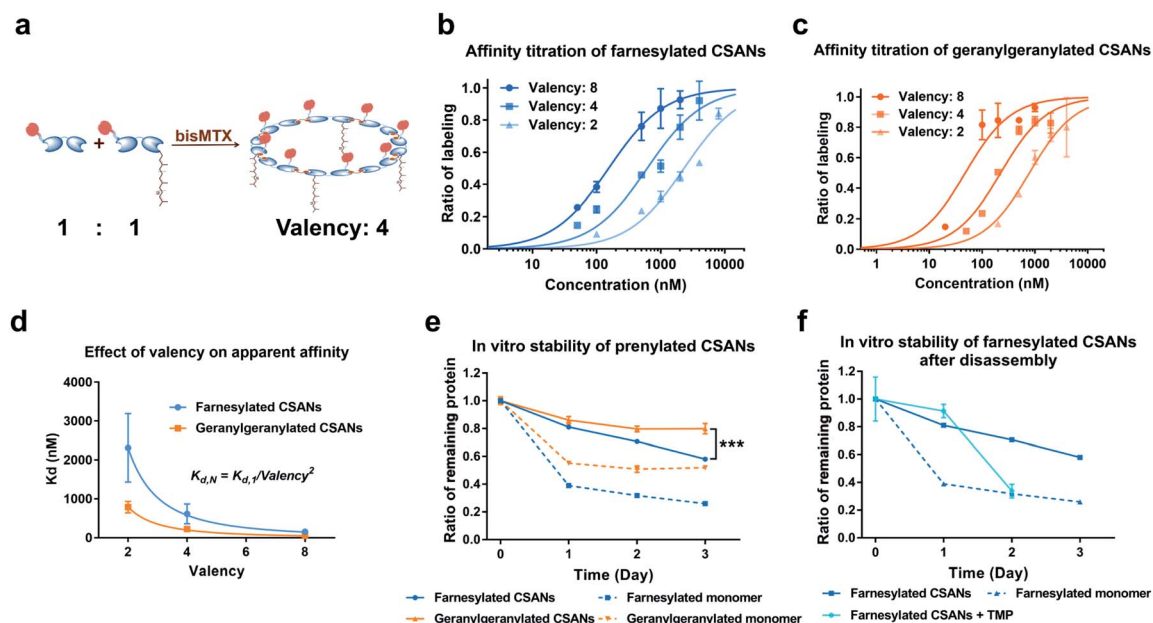


Fig. 4 Affinity and stability study of prenylated CSANs. (a) The number (valency) of isoprenoids groups in the hybrid CSANs can be tuned by assembling different molar ratios of monomeric subunits. The apparent affinity of (b) farnesylated and (c) geranylgeranylated CSANs for the plasma membrane varies directly with isoprenoid valency, as demonstrated by flow cytometry. (d) The apparent K_d values of the prenylated CSANs for membrane binding exhibited an inverse relationship with the square of the valency ($K_{d,N} = K_{d,1}/\text{valency}^2$, $R^2 > 0.997$ for both prenylated CSANs). (e) Multivalent prenylated CSANs exhibit a longer cell surface half-life (>72 hours) compared to the monomeric prenylated proteins *in vitro*. (f) The membrane residence half-life of the farnesylated CSANs decreases significantly (<20 hours) upon scaffold disassembly with trimethoprim. Significance in (e) (data on Day 3) was tested using a two-tailed, unpaired *t*-test. And is indicated as *** $P < 0.001$. Data in panels (b), (c), (e), and (f), are represented as the mean \pm standard deviation from $n = 3$ independent trials. For panel (d), data are shown as the mean $K_d \pm$ standard error (from $n = 3$ independent samples). In some instances, small error bars are obscured by the symbols denoting the mean value.

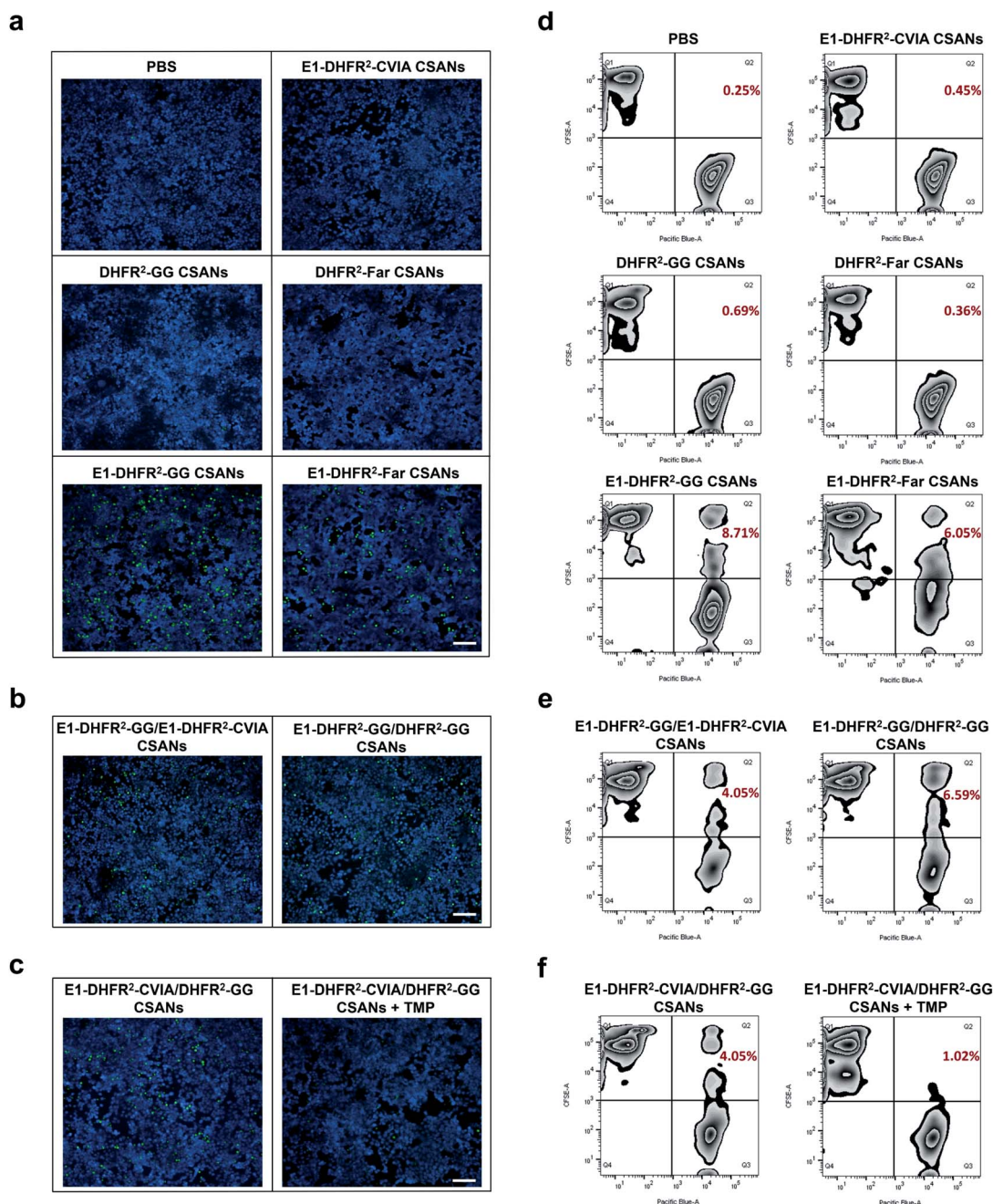


Fig. 5 Prenylated CSANs mediate reversible cell–cell interactions. (a) Fluorescent microscopy demonstrates that prenylated anti-EGFR CSANs can mediate reversible cell–cell interactions in the fluorescent microscopy imaging experiment (scale bar, 100 μ m). Raji cells were stained by CFSE, while EGFR⁺ A431 cells were plated on the coverslips and stained by CellTrace Violet (CTV). The E1-DHFR²-GG CSANs and E1-DHFR²-Far CSANs maintained the cell–cell interactions, which were shown by the remaining green Raji cells on the coverslip after PBS wash, while the CSANs without targeting elements or isoprenoids groups (E1-DHFR²-CVIA, DHFR²-GG and DHFR²-Far CSANs) failed to mediate cell–cell interactions. (b) The hybrid CSANs with 50% molar isoprenoids groups (E1-DHFR²-GG/E1-DHFR²-CVIA CSANs) or 50% molar anti-EGFR domains (E1-DHFR²-GG/DHFR²-GG CSANs) were able to mediate cell–cell interactions (scale bar, 100 μ m). (c) The cell–cell interactions were shown to be dissociated by the disassembly of the hybrid prenylated anti-EGFR CSANs (E1-DHFR²-CVIA/DHFR²-GG CSANs) through TMP treatment (scale bar, 100 μ m). (d) The cell–cell interactions were also investigated using flow cytometry, where the CFSE-stained Raji cells were modified with CSANs and incubated with CTV-stained A431 cells. The resulting CFSE⁺/CTV⁺ cell pairs were then quantified by flow cytometry. Both prenylated and geranylgeranylated CSANs induced cell–cell interactions, though the latter was more efficient. (e) Reduction of isoprenoids groups or EGFR-targeting domains by 50% in the CSANs diminished cell–cell interactions. (f) TMP was shown to significantly interrupt the cell–cell interactions mediated by E1-DHFR²-CVIA/DHFR²-GG CSANs.



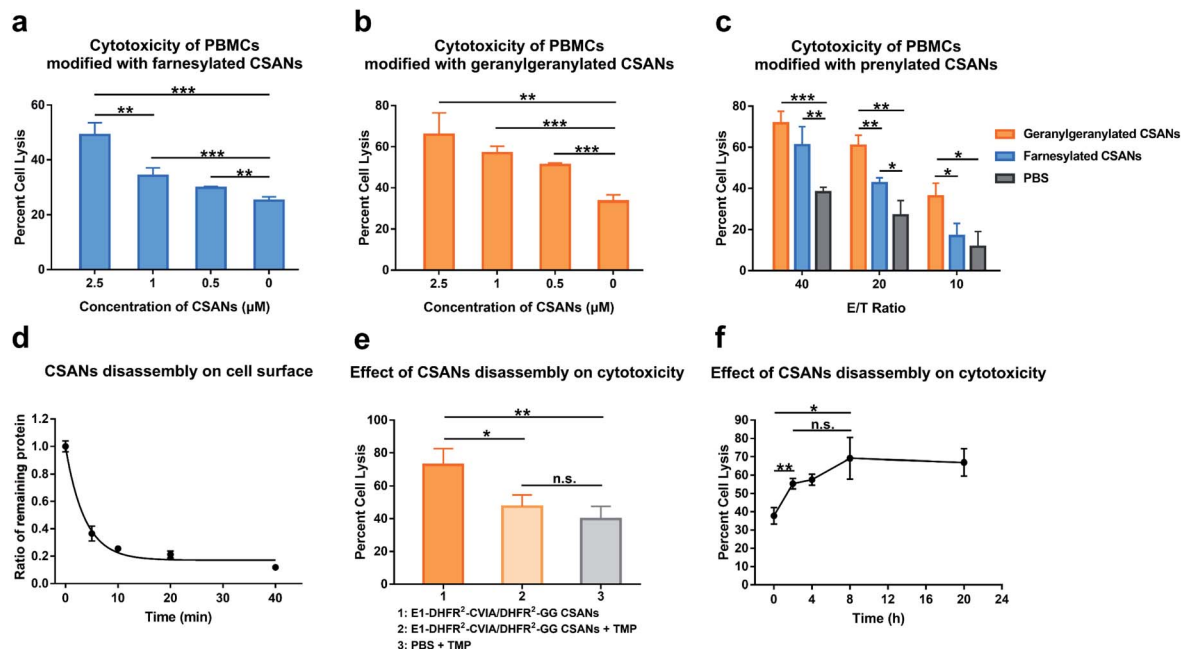


Fig. 6 Prenylated CSANs enhance cytotoxicity towards EGFR⁺ target cells. The cytotoxicity of PBMCs against EGFR⁺ A431 cells after modification with (a) farnesylated anti-EGFR CSANs (E1-DHFR²-Far CSANs) or (b) geranylgeranylated anti-EGFR CSANs (E1-DHFR²-GG CSANs) was studied using an LDH release assay. Both prenylated CSANs enhanced the cytotoxicity of PBMCs in a concentration-dependent manner. (c) The impact of different effector : target (E/T) ratios on the cytotoxicity of CSAN-modified PBMCs was also assessed using an LDH release assay. (d) Kinetic study of CSAN disassembly on cell surface. Raji cells were modified with the hybrid E1-DHFR²-CVIA/DHFR²-GG CSANs, and the E1-DHFR²-CVIA protein was disassociated from the cell surface using trimethoprim. The remaining E1-DHFR²-CVIA protein was then quantified via flow cytometry. The half-life of CSAN disassembly is 3.5 min. (e) CSAN disassembly was shown to significantly reduce the cytotoxicity of PBMCs modified with the hybrid E1-DHFR²-CVIA/DHFR²-GG CSANs, as expected. (f) The E1-DHFR²-CVIA/DHFR²-GG CSANs were disassembled at different time points (0 h, 2 h, 4 h, 8 h, 20 h) during the co-culture of CSAN-modified PBMCs and A431 cells, and the cytotoxicity of the PBMCs was studied after the CSANs disassembly. Significance in (a), (b), (c), (e) and (f) was tested using a two-tailed, unpaired t-test. And is indicated as ** $P < 0.01$ or * $P < 0.05$. For panel (d), data are shown as the mean \pm standard deviation from $n = 3$ independent samples. Error bars in (a), (b), (c), (e) and (f) denote the standard error calculated from $n = 3$ independent trials and each trial has $n = 3$ independent samples.

the farnesylated CSANs had been lost from the cell surface, with the presumed monomeric species exhibiting similar stability on the cell membrane as the parental monomeric farnesylated DHFR²-CVIA (Fig. 4f). Thus, these observations confirm that the stability of the CSANs and their multivalent nature can be pharmacologically altered on the cell membrane by treatment with trimethoprim.

To study the cell-cell interactions mediated by prenylated CSANs, CFSE-stained Raji cells were modified with prenylated anti-EGFR CSANs or incubated with control solutions and then co-cultured with CTV-stained A431 cells that were plated on glass coverslips. After washing off unbound Raji cells, the cells were fixed and imaged via fluorescence microscopy. Both farnesylated and geranylgeranylated anti-EGFR CSANs were able to efficiently mediate cell-cell interactions, as shown by the adherence of CFSE-labeled Raji cells to the CTV-labeled A431 cells (Fig. 5a, b and S8a†). In contrast, the prenylated DHFR²-CVIA CSANs or unprenylated E1-DHFR²-CVIA CSANs that lack the targeting moiety or the prenyl group, respectively, were unable to induce cell-cell interactions and did not significantly differ from the PBS control group (Fig. 5a). As illustrated in Fig. 1c, the disassembly of the hybrid prenylated anti-EGFR CSANs was expected to completely terminate the CSAN-mediated cell-cell interactions. Treatment of the co-cultures

with trimethoprim (TMP) for 1 h was shown to significantly reduce the amount of cell-cell interactions induced by the hybrid anti-EGFR CSANs constructed from prenylated DHFR²-CVIA and unprenylated E1-DHFR²-CVIA protein (Fig. 5c and S8b†), consistent with the disassembly of the CSANs by TMP.

To quantitatively characterize the cell-cell interactions mediated by the prenylated anti-EGFR CSANs, CFSE-stained Raji cells were labeled with CSANs and incubated with EGFR⁺ A431 cells in PBS, followed by flow cytometry analysis. The CFSE⁺/CTV⁺ double-positive cell population, which represents induced Raji/A431 cell clusters, was quantified as the indicator of cell-cell interactions. Specifically, both prenylated anti-EGFR CSANs induced cell-cell interactions, though the geranylgeranylated anti-EGFR CSANs were shown to induce 44% more cell-cell interactions than comparable farnesylated CSANs (Fig. 5d). When hybrid CSANs formed from a 1 : 1 molar mixture of E1-DHFR²-CVIA and prenylated E1-DHFR²-CVIA were used, a 50% decrease in the percentage cell-cell interactions was observed (Fig. 5e and S9a†). Consistent with these observations, the hybrid CSANs prepared from a 1 : 1 molar mixture of prenylated E1-DHFR²-CVIA and prenylated DHFR²-CVIA also exhibited a reduction in the percentage of cell-cell interactions (Fig. 5e and S9a†). Moreover, the cell clusters induced by the hybrid prenylated anti-EGFR CSANs, whether



geranylgeranylated or farnesylated, were greatly reduced in number after treatment with trimethoprim (Fig. 5f and S9b†). Thus, this data indicates that these strong and reversible cell-cell interactions are mediated by prenylated anti-EGFR CSANs.

Finally, as an alternative antigen, the cell-cell interactions mediated by prenylated anti-EpCAM CSANs were also investigated through analogous imaging and flow cytometry experiments using EpCAM⁺ MCF-7 cells as the target cells. Consistent with our observations described above for the prenylated anti-EGFR CSANs, both types of prenylated anti-EpCAM CSANs efficiently mediated the cell-cell interactions, with the geranylgeranylated CSANs again providing more robust interactions (Fig. S10 and S11†).

We next assessed the ability of prenylated CSANs to direct PBMc-mediated lysis of target cells using a lactate-dehydrogenase (LDH) release assay. Activated PBMcs were modified with prenylated anti-EGFR CSANs (E1-DHFR²-Far or E1-DHFR²-GG CSANs) and incubated with EGFR⁺ A431 cells. The CSAN-functionalized PBMcs exhibited dose-dependent lysis of the target cells that was significantly higher than the cytotoxicity observed for unmodified control PBMcs (Fig. 6a and b). In addition, the prenylated anti-EGFR CSANs failed to enhance the cell lysis of EGFR-MCF-7 cells, by CSAN-modified PBMcs, further demonstrating the specificity of the prenylated anti-cancer CSANs (Fig. S12†). Consistent with the cell-cell interactions and membrane stability studies, geranylgeranylated anti-EGFR CSANs induced a significantly greater amount of cellular toxicity than farnesylated anti-EGFR CSANs, even at effector/target cell ratios (E/T) as high as 20 : 1 (Fig. 6c).

As was demonstrated above, treatment with trimethoprim can disassemble prenylated CSANs, resulting in their loss from the cell surface. When Raji cells modified with geranylgeranylated anti-EGFR CSANs were treated with a 20-fold excess of trimethoprim, approximately 80% of the nanorings were disassembled on the cellular membrane within 10 min, yielding a half-life of 3.5 min (Fig. 6d). To facilitate complete dissociation of the lipidated subunit from the targeting ligand, thereby ensuring that no cross-links between the cells would remain upon scaffold disassembly, we prepared geranylgeranylated anti-EGFR CSANs from E1-DHFR²-CVIA (unprenylated) and non-targeted geranylgeranylated DHFR²-CVIA. Treatment with trimethoprim at time zero (right after mixing between CSAN-modified PBMcs and A431 cells) was shown to abolish the ability of the modified PBMcs to induce target cell cytotoxicity (Fig. 6e).

To further study the effects of CSANs disassembly timing on induced cytotoxicity, PBMcs were modified with the hybrid geranylgeranylated anti-EGFR CSANs (E1-DHFR²-CVIA/DHFR²-GG CSANs), mixed with target A431 cells, and then treated with trimethoprim at various time points. The level of targeted cytotoxicity was then determined at the end of 20 h for each time point. As can be seen from Fig. 6f, cytotoxicity is initiated within the first few minutes with maximum cytotoxicity observed after at least 2 h. Thus, the initiation of target tumor cell apoptosis and likely necrosis can be abolished if interrupted early but is irreversible past this time point.

Discussion

Cell-cell interactions play vital roles in many aspects of physiological and pathological processes; therefore, the ability to manipulate such interactions is valuable for fundamental studies of cellular biology and for potential therapeutic applications. To streamline the preparation of CSANs designed to bind to membranes *via* non-covalent interactions, we explored here the use of enzymatic methods to append naturally occurring lipids onto the desired nanostructured targets. An important advantage of such an approach is that it capitalizes on the catalytic efficiency afforded by enzymatic conjugation. Such methods allow protein attachment to occur with high conversion even at low concentrations driven by the formation of an energetically favorable enzyme-substrate complex. Moreover, the use of natural substrates obviates the need for complex synthetic methods, thus enhancing the ease of implementation.

Accordingly, we explored the potential of enzymatically labeling the monomeric protein component of the CSANs to directly install a natural C15 or C20 lipid, which upon multivalent display, would result in high-affinity membrane binding. We designed DHFR²-CVIA monomers that would be substrates for either farnesyl transferase or geranylgeranyl transferase, thus allowing enzymatic lipidation with either farnesyl or geranylgeranyl moieties, respectively. The DHFR²-CVIA monomers were easily expressed in *E. coli* and quantitatively enzymatically labeled with either farnesyl or geranylgeranyl groups. Despite being prenylated, the rings did not aggregate and were found to be stable for days in solution. Moreover, the prenylated CSANs quickly and stably ($T_{1/2} > 72$ h) labeled the cell membrane, with longer geranylgeranyl modifications exhibiting significantly more longevity than the shorter farnesyl groups. Since the number of displayed isoprenoids groups on the rings can be tuned by varying the ratio of prenylated to non-prenylated protein components prior to oligomerization, we were able to demonstrate that both fully farnesylated and geranylgeranylated CSANs yielded the highest membrane binding affinity. The appending of an anti-EGFR or anti-EpCAM fibronectin targeting domain did not affect membrane binding and allowed labeled cells to form direct contact with EGFR-expressing or EpCAM-expressing cells respectively *in vitro*.

In addition, significant differences were observed between the ability of fully farnesylated or geranylgeranylated CSANs to promote targeted cell-cell interactions, with geranylgeranylated CSANs forming significantly more cell-cell interactions than the farnesylated counterparts. When the valency of either isoprenoid groups or targeting ligands incorporated into the CSAN was reduced, a corresponding reduction of cell-cell interactions was observed. Consistent with previously reported CSANs, each construct was readily disassembled by treatment with a non-toxic excess of trimethoprim. Given the lower affinity of the farnesylated DHFR² monomers, there may be an advantage to employing the farnesylated CSANs over geranylgeranylated CSANs, since dissociation of the resulting farnesylated monomers from the cell surface is likely to be faster than geranylgeranylated monomers due to the lower affinity of the



shorter lipid for the membrane. Interestingly, similar to observations for prenylated proteins on the cytoplasmic membrane, the prenylated CSANs were shown to preferentially concentrate in lipid rafts. The differences in the ability of, for example, A431 and MCF-7 cells to bind to the prenylated CSANs may reflect differences in their lipid raft composition. Further studies with a range of cell lines and well characterized level of lipid rafts should shed light on the selectivity of prenylated CSANs to associate with lipid rafts over other regions of the cell membrane.

The T cell receptor in complexation with CD3, CD4, and CD8 has been found to be highly associated with and dependent on lipid rafts for the propagation of Lck based signaling.^{37,38} Consequently, we evaluated the ability of prenylated anti-EGFR CSANs, to direct T cell-targeted killing of an EGFR-overexpressing epidermoid carcinoma line, A431 cells. Activated PBMCs, which are 90% T cells, were treated with geranylgeranylated anti-EGFR CSANs. The modified T cells were shown to induce targeted killing of A431 cells. Given that we were employing activated T cells and that trimethoprim treatment can lead to rapid disassembly of the CSANs, we chose to investigate the time frame within which T cell killing is initiated once the targeted tumor cells have been engaged by dosing with excess trimethoprim at various time points and measuring the amount of induced cytotoxicity that occurred prior to CSAN abrogation. Our results indicate that similar to CAR-T cells at a similar E : T ratio, cytotoxicity is induced within the first two hours, after which removal of the CSANs has no effect on the targeted cytotoxicity.³⁹ Whether the structure of the cytotoxic immune synapse is similar to CAR-T cells or BiTcs remains to be determined, since there is no direct binding or engagement of CD3.^{40,41} Given the complex order and processes engaged by TCRs through the immune synapse, it is surprising that simply associating the T cell surface with the target cell through the prenylated CSANs results in T cell induced cytotoxicity. Ongoing studies of the engineering of interactions between the T cells and the target cells by prenylated CSANs should expand our understanding of the constraints or lack of constraints governing T cell-mediated cytotoxicity. The ability to study the time-dependence of T cell target engagement highlights the utility of the lipidated CSANs described here. The unique reversibility and tunability of the CSAN-based constructs described here make them particularly versatile tools for the study of cell-cell interactions in general. Given the complex order and processes engaged by TCRs through the immune synapse, it is interesting that the prenylated anti-EGFR CSANs are able to induce T cell-targeted cell killing.

Conclusions

In summary, we developed the multivalent prenylated chemically self-assembled nanorings (CSANs) for mediating reversible cell-cell interactions. Prenylated CSANs offer a facile one-step approach for the stable membrane labeling of virtually any cell type, providing accessible and pharmacologically reversible cell-cell interactions for a range of fundamental scientific and therapeutic applications.

Author contributions

C. R. W., M. D. D., and Y. W. designed the project. O. K. designed the E1-DHFR²-CVIA (initial version) protein, and C. M. C. designed the Ep-DHFR² proteins. Y. W. designed and generated the Ep-DHFR²-CVIA, E1-DHFR²-CVIA and DHFR²-CVIA proteins based on the protein scaffolds from O. K. and C. M. C. Y. W. prepared the farnesyl transferase. S. A. and J. L. H. prepared the geranylgeranyl transferase. Y. W. performed all the experiments and analyses presented in the paper. Y. W. wrote the manuscript and all authors provided edits and comments.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

This work was supported by GM084152 (M. D. D.), CA185627 (C. R. W.), CA247681 (CRW) and NSF Grant ECCS-2025124 to the Minnesota Nano Center. We thank Dr Robert Hafner for his help with the cryo-TEM experiments, and these experiments were carried out in the Characterization Facility, University of Minnesota, which receives partial support from NSF through the MRSEC program. We thank Dr Yingchun Zhao for his help with the LC-MS experiments that were conducted in the Masonic Cancer Center's Analytical Biochemistry Shared Resource. We thank Dr Mark Sanders for his help with the fluorescent imaging experiments, which were carried out in the University Imaging Center, University of Minnesota. We thank Dr Barry Finzel and William McCue for their assistance with the DLS analysis. We thank Dr Lakmal Rozumalski for the help with the manuscript.

Notes and references

- 1 T. N. Yamamoto, R. J. Kishton and N. P. Restifo, *Nat. Med.*, 2019, **25**, 1488–1499.
- 2 M. De Luca, A. Aiuti, G. Cossu, M. Parmar, G. Pellegrini and P. G. Robey, *Nat. Cell Biol.*, 2019, **21**, 801–811.
- 3 A. Golchin and T. Z. Farahany, *Stem Cell Rev. Rep.*, 2019, **15**, 166–175.
- 4 C. A. Custódio and J. F. Mano, *ChemNanoMat*, 2016, **2**, 376–384.
- 5 M. Rothbauer, H. Zirath and P. Ertl, *Lab Chip*, 2018, **18**, 249–270.
- 6 D. J. Irvine and E. L. Dane, *Nat. Rev. Immunol.*, 2020, **20**, 321–334.
- 7 C. M. Csizmar, J. R. Petersburg and C. R. Wagner, *Cell Chem. Biol.*, 2018, **25**, 931–940.
- 8 S. R. Frankel and P. A. Baeuerle, *Curr. Opin. Chem. Biol.*, 2013, **17**, 385–392.
- 9 M. Ciof, J. Dorado, P. A. Baeuerle and C. Heeschen, 2012, 465–475.
- 10 J. Wu, J. Fu, M. Zhang and D. Liu, *J. Hematol. Oncol.*, 2015, **1**, 7.



- 11 Y. L. Huang and A. Chen, *Advances in Proteomics Research*, 2012.
- 12 M. Takeo, C. Li, M. Matsuda, H. Nagai, W. Hatanaka, T. Yamamoto, A. Kishimura, T. Mori and Y. Katayama, *J. Biomater. Sci., Polym. Ed.*, 2015, **26**, 353–368.
- 13 Y. Bagheri, S. Chedid, F. Shafiei, B. Zhao and M. You, *Chem. Sci.*, 2019, **10**, 11030–11040.
- 14 Y. Teramura, H. Chen, T. Kawamoto and H. Iwata, *Biomaterials*, 2010, **31**, 2229–2235.
- 15 J. C. T. Carlson, S. S. Jena, M. Flenniken, T. F. Chou, R. A. Siegel and C. R. Wagner, *J. Am. Chem. Soc.*, 2006, **128**, 7630–7638.
- 16 Q. Li, C. R. So, A. Fegan, V. Cody, M. Sarikaya, D. A. Vallera and C. R. Wagner, *J. Am. Chem. Soc.*, 2010, **132**, 17247–17257.
- 17 J. Shen, D. A. Vallera and C. R. Wagner, *J. Am. Chem. Soc.*, 2015, **137**, 10108–10111.
- 18 M. Gebauer and A. Skerra, *Curr. Opin. Chem. Biol.*, 2009, **13**, 245–255.
- 19 L. A. Stern, C. M. Csizmar, D. R. Woldring, C. R. Wagner and B. J. Hackel, *ACS Comb. Sci.*, 2017, **19**, 315–323.
- 20 C. M. Csizmar, J. R. Petersburg, A. Hendricks, L. A. Stern, B. J. Hackel and C. R. Wagner, *Bioconjugate Chem.*, 2018, **29**, 1291–1301.
- 21 K. Gabrielse, A. Gangar, N. Kumar, J. C. Lee, A. Fegan, J. J. Shen, Q. Li, D. Vallera and C. R. Wagner, *Angew. Chem., Int. Ed.*, 2014, **53**, 5112–5116.
- 22 K. T. Lane and L. S. Beese, *J. Lipid Res.*, 2006, **47**, 681–699.
- 23 T. Scott Reid, K. L. Terry, P. J. Casey and L. S. Beese, *J. Mol. Biol.*, 2004, **343**, 417–433.
- 24 T. C. Turek-Etienne, C. L. Strickland and M. D. Distefano, *Biochemistry*, 2003, **42**, 3716–3724.
- 25 Y. Wang, J. K. Dozier, L. S. Beese and M. D. Distefano, *ACS Chem. Biol.*, 2014, **9**(8), 1726–1735.
- 26 J. L. Hougland, K. A. Hicks, H. L. Hartman, R. A. Kelly, T. J. Watt and C. A. Fierke, *J. Mol. Biol.*, 2010, **395**, 176–190.
- 27 E. Choy, V. K. Chiu, J. Silletti, M. Feoktistov, T. Morimoto, D. Michaelson, I. E. Ivanov and M. R. Phillips, *Cell*, 1999, **98**, 69–80.
- 28 Y. Zhang, M. J. Blanden, C. Sudheer, S. A. Gangopadhyay, M. Rashidian, J. L. Hougland and M. D. Distefano, *Bioconjugate Chem.*, 2015, **26**, 2542–2553.
- 29 B. P. Duckworth, J. Xu, T. A. Taton, A. Guo and M. D. Distefano, *Bioconjugate Chem.*, 2006, **3**, 967–974.
- 30 M. Rashidian, S. C. Kumarapperuma, K. Gabrielse, A. Fegan, C. R. Wagner and M. D. Distefano, *J. Am. Chem. Soc.*, 2013, **135**, 16388–16396.
- 31 T. J. Kean, L. Duesler, R. G. Young, A. Dadabayev, A. Olenyik, M. Penn, J. Wagner, D. J. Fink, A. I. Caplan and J. E. Dennis, *J. Drug Targeting*, 2012, **20**, 23–32.
- 32 J. De Kruif, M. Tijmens, J. Goldsein and T. Logtenberg, *Nat. Med.*, 2000, **6**, 223–227.
- 33 S. L. Emanuel, L. J. Engle, G. Chao, R. R. Zhu, C. Cao, Z. Lin, A. Yamniuk, J. Hosbach, J. Brown, E. Fitzpatrick, J. Gokemeijer, P. Morin, B. Morse, I. M. Carvajal, D. Fabrizio, M. C. Wright, R. Das Gupta, M. Gosselin, D. Cataldo, R. P. Ryseck, M. L. Doyle, T. W. Wong, R. T. Camphausen, S. T. Cload, H. N. Marsh, M. M. Gottardis and E. S. Furfine, *mAbs*, 2011, **3**, 38–48.
- 34 O. Kilic, M. R. de Souza, A. A. Almotlak, Y. Wang, J. M. Siegfried, M. D. Distefano and C. R. Wagner, *J. Med. Chem.*, 2020, **63**, 10235–10245.
- 35 I. A. Prior, A. Harding, J. Yan, J. Sluimer, R. G. Parton and J. F. Hancock, *Nat. Cell Biol.*, 2001, **3**, 368–375.
- 36 C. M. Csizmar, J. R. Petersburg, T. J. Perry, L. Rozumalski, B. J. Hackel and C. R. Wagner, *J. Am. Chem. Soc.*, 2019, **141**, 251–261.
- 37 R. Fragoso, D. Ren, X. Zhang, M. W.-C. Su, S. J. Burakoff and Y.-J. Jin, *J. Immunol.*, 2003, **170**, 913–921.
- 38 A. Larbi, G. Dupuis, A. Khalil, N. Douziech, C. Fortin and T. Fülöp, *Cell. Signalling*, 2006, **18**, 1017–1030.
- 39 K. Fousek, J. Watanabe, S. K. Joseph, A. George, X. An, T. T. Byrd, J. S. Morris, A. Luong, M. A. Martínez-Paniagua, K. Sanber, S. A. Navai, A. Z. Gad, V. S. Salsman, P. R. Mathew, H. N. Kim, D. L. Wagner, L. Brunetti, A. Jang, M. L. Baker, N. Varadarajan, M. Hegde, Y. M. Kim, N. Heisterkamp, H. Abdel-Aziz and N. Ahmed, *Leukemia*, 2020, DOI: 10.1038/s41375-020-0792-2.
- 40 A. J. Davenport, R. S. Cross, K. A. Watson, Y. Liao, W. Shi, H. M. Prince, P. A. Beavis, J. A. Trapani, M. H. Kershaw, D. S. Ritchie, P. K. Darcy, P. J. Neeson and M. R. Jenkins, *Proc. Natl. Acad. Sci. U. S. A.*, 2018, **115**, E2068–E2076.
- 41 S. Offner, R. Hofmeister, A. Romaniuk, P. Kufer and P. A. Baeuerle, *Mol. Immunol.*, 2006, **43**, 763–771.

