

PAPER

View Article Online
View Journal | View Issue



Cite this: *Environ. Sci.: Nano*, 2021, 8, 1081

Self-decontaminating nanofibrous filters for efficient particulate matter removal and airborne bacteria inactivation†

Zan Zhu,^a Yu Zhang,^a Liang Bao,^b Jianping Chen,^a Shun Duan,^{ac} Sheng-Chieh Chen,^a Ping Xu ^b and Wei-Ning Wang ^{*,a}

With the increased bacteria-induced hospital-acquired infections (HAIs) caused by bio-contaminated surfaces, the requirement for a safer and more efficient antibacterial strategy in designing personal protective equipment (PPE) such as N95 respirators is rising with urgency. Herein, a self-decontaminating nanofibrous filter with a high particulate matter (PM) filtration efficiency was designed and fabricated via a facile electrospinning method. The filters implemented in the electrospun nanofibers were constructed by grafting a layer of antibacterial polymeric quaternary ammonium compound (QAC), that is, poly[2-(dimethyl decyl ammonium) ethyl methacrylate] (PQDMAEMA), onto the surface of metal-organic framework (MOF, UiO-66-NH₂ as a model) to form the active composite UiO-PQDMAEMA. The UiO-PQDMAEMA filter demonstrates an excellent PM filtration efficiency (>95%) at the most penetrating particle size (MPPS) of 80 nm, which is comparable to that of the commercial N95 respirators. Besides, the UiO-PQDMAEMA filter is capable of efficiently killing both Gram-positive (*S. epidermidis*) and Gram-negative (*E. coli*) airborne bacteria. The strong electrostatic interactions between the anionic cell wall of the bacteria and positively charged nitrogen of UiO-PQDMAEMA are the main reasons for severe cell membrane disruption, which leads to the death of bacteria. The present work provides a new avenue for combating air contamination by using the QAC-modified MOF-based active filters.

Received 10th December 2020,
Accepted 22nd March 2021

DOI: 10.1039/d0en01230k

rsc.li/es-nano

Environmental significance

An antibacterial strategy is urgently desired for face mask design because the bio-contaminated surfaces would lead to the risk of secondary transmission of bacterial infection. We herein report a self-decontaminating air filter, where the antibacterial quaternary ammonium compound (QAC) modified metal-organic framework (MOF) nanocrystals were embedded as fillers into the electrospun nanofibers with the assistance of the electrospinning technique. Effective inactivation of airborne bacteria (both Gram-positive and Gram-negative) is achieved by the strong electrostatic interactions between negatively charged bacteria cell walls and positively charged QAC-modified MOF nanocrystals. This work demonstrates a promising strategy for efficient control of indoor air contaminants (e.g., particulate matter and airborne bacteria), which can be extended to other surface decontamination applications.

1. Introduction

Hospital-acquired infections (HAIs), also known as health-associated infections, have been recognized as a major threat to the safety of patients and healthcare workers worldwide.^{1–5}

During the COVID-19 pandemic, numerous cross-infections occurred in the hospitals among healthcare workers and patients, indicating that the adverse effects of HAIs such as mortality, morbidity, and associated costs are enormous.⁶ To reduce the HAIs, face-piece respirators such as N95 respirators and surgical masks are recommended by the United States Centers for Disease Control and Prevention (CDC) as efficient respiratory personal protective equipment (PPE).^{7–9} For convenience, the term ‘face mask’ is used to represent N95 respirators and surgical masks throughout the article. Even though the commercial face masks can provide users with certain degree of protection, there are still intensive researches and efforts to improve their performance in terms of particulate matter (PM) filtration, user-friendliness, and airborne pathogens inactivation.^{10–12}

^a Department of Mechanical and Nuclear Engineering, Virginia Commonwealth University, Richmond, Virginia 23219, USA. E-mail: wnwang@vcu.edu;

Fax: +1 804 827 7030; Tel: +1 804 827 4306

^b Philips Institute for Oral Health Research, Virginia Commonwealth University, Richmond, Virginia, 23298, USA

^c State Key Laboratory of Chemical Resource Engineering, Key Lab of Biomedical Materials of Natural Macromolecules, Ministry of Education, Beijing Laboratory of Biomedical Materials, Beijing University of Chemical Technology, Beijing 100029, China

† Electronic supplementary information (ESI) available. See DOI: 10.1039/d0en01230k



Electrospinning producing nanofibers from a polymer solution is an efficient technique to fabricate filter media with high PM filtration performance, attributing to the small diameters of the nanofibers and fiber charges.^{13–17} To further increase the functionality, *e.g.*, hydrophobicity, breathability, toxic gas removal, *etc.*, of the electrospun filters, metal-organic frameworks (MOFs), a class of porous crystalline polymers, have been embedded into the electrospun polymer to form the MOF-based filters.^{18–23} Endorsed by the hierarchical structures and tunable surface chemistry, the MOF-based nanofibrous filters not only possess different functionalities but also achieve a high PM filtration efficiency and a lower pressure drop^{18,24} which is beneficial to the wearer's comfort in breathing. However, most of these MOF-based filters cannot be used to actively kill microorganisms such as bacteria. To impart the antibacterial properties to the MOF-based filters, the key is to develop a fabrication method for filters with high efficiency for the simultaneous removal of PM and inactivation of bacteria.

Bacteria pathogens are one of the major infectious agents that cause the persistence of HAIs.²⁵ Indirect contact with contaminated surfaces and airborne droplets are two of the most common modes of bacteria transmission.²⁶ Most commercial face masks and electrospun MOF-based filters can only passively block the transmission of airborne bacteria but not be able to kill them *in situ*, *i.e.*, on the mask surface. The bacteria being captured by the face mask may accumulate on the mask surface and can still survive for hours or even days, which would significantly increase the possibility of HAIs through surface contact transmission.^{27,28} Therefore, there is an urgent demand to develop antibacterial filters for face masks. This need can be achieved by incorporating antibacterial materials into face mask filters. Conventional strategies of using antibacterial agents such as Ag ions,²⁹ Cu ions,³⁰ metal oxides,³¹ and photosensitizers³² are not very suitable because most of these materials are toxic to humans and environmentally unfriendly. In particular, when people breathe, talk, cough, or sneeze, the water droplets may condense on the mask surface,³³ which might cause the release of these chemicals.³⁴ As a result, a safer method is demanded to impart the face mask with nonleaking and antibacterial properties.

Quaternary ammonium compounds (QACs) are potent antimicrobials that are widely used as disinfectants because of their low toxicity, the flexibility of molecule structures, the readiness of fixation on the surface, the low probability of antibiotic resistance, and so on.^{35–38} The bactericidal activity of QACs stems from the electrostatic attraction between permanent positively charged nitrogen (N^+) in QACs and negatively charged bacterial membrane,³⁹ which would ultimately lead to cell lysis, namely the burst of cytoplasmic material.⁴⁰ In particular, the polymeric QACs with long alkyl chains exhibited enhanced bactericidal activity because the longer alkyl chains can interact with the lipid cell walls more strongly and destabilize the bacterial membrane more effectively.⁴¹ Even though the recent emerging popular

“grafting from” approach, also known as “surface-initiated polymerization”, has enabled the controllable grafting QACs on the material surfaces,⁴² the immobilization of polymeric QACs onto the face mask filters is still challenging for the following reasons. Firstly, the surface of the filter should be pretreated by plasma or other chemical treatment to allow the fixation of the suitable initiators, which is complicated and time-consuming.⁴² Secondly, the harsh organic solvents would impair the PM filtration efficiency of electret media, which is one of the most important functionalities of the face mask filter.^{17,43,44} Therefore, how to immobilize the polymeric QACs on the face mask filters without compromising the PM filtration efficiency is a prominent quest.

To achieve this goal, this work reports a rational design approach to incorporate a QAC-modified MOF into the electrospun fibers to form an active composite filter. As an important type of MOFs, the amino-derived MOFs provide great platforms to covalently attach functional groups by post-synthetic modification. Herein, a robust UiO-66-NH₂ is used as the base material,^{45,46} which is subsequently decorated with a layer of polymeric QAC, *i.e.*, poly[2-(dimethyl decyl ammonium) ethyl methacrylate] (PQDMAEMA) through a classical atomic transfer radical polymerization (ATRP) approach. With the assistance of the electrospinning technique, the as-synthesized active composite UiO-PQDMAEMA was embedded with the polyacrylonitrile (PAN) solution to produce an antibacterial nanofibrous filter, which also exhibits a high PM filtration performance comparable to a commercial N95 respirator (Scheme 1). The UiO-PQDMAEMA@PAN filter is capable of efficiently killing both Gram-positive (*S. epidermidis*) and Gram-negative (*E. coli*) bacteria by destroying their cell membranes, highlighting that the UiO-PQDMAEMA@PAN can be potentially used as an antibacterial core filter for N95 respirators. We expect that this design of antibacterial filters can also be used for the fabrication of the heating, ventilation, and air conditioning (HAVC) air filter as well as the membrane for waterborne bacteria disinfection.

2. Experimental section

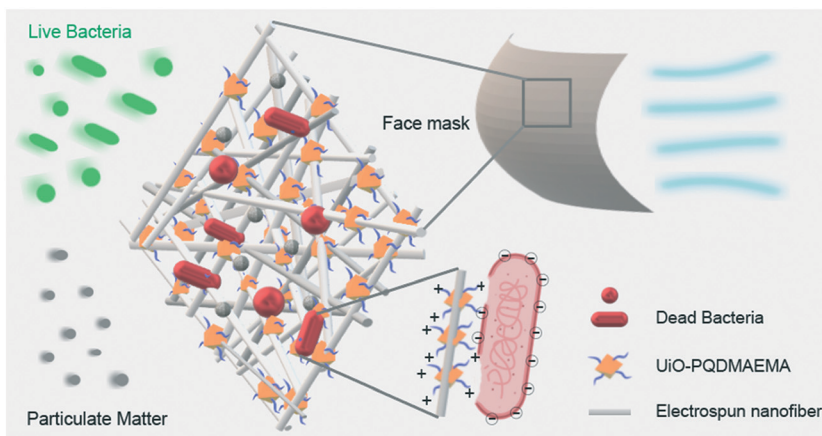
2.1 Preparation of UiO-66-NH₂, UiO-BIBB, and UiO-PQDMAEMA

The synthetic procedures for UiO-PQDMAEMA preparation are schematically depicted in Scheme 2. In general, the raw UiO-66-NH₂ was firstly decorated with initiator 2-bromoisobutryl bromide (BIBB) *via* covalent bonding to form UiO-66-BIBB. Then, the monomer 2-(dimethyl decyl ammonium) ethyl methacrylate (QDMAEMA) was polymerized and grafted on the surface of UiO-66-BIBB through the ATRP process to obtain the final product, which is denoted as UiO-PQDMAEMA. The details of material synthesis processes can be seen in S1.†

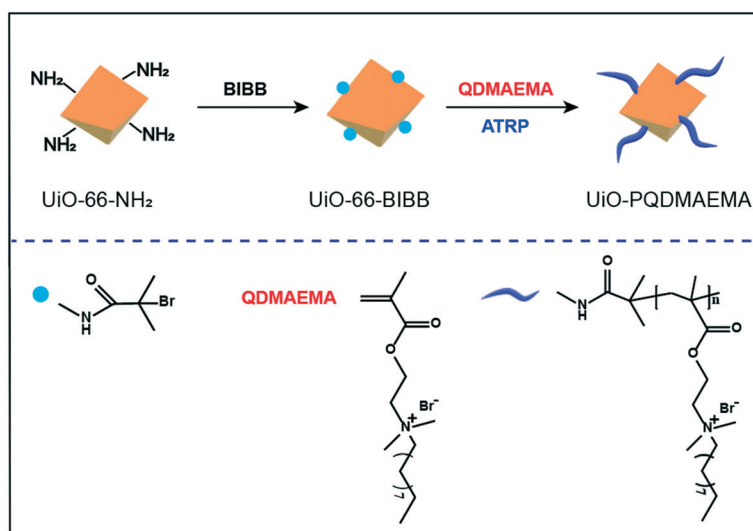
2.2 Fabrication of face mask filter

The face mask filter was fabricated *via* the facile electrospinning method, where the electric force is generated





Scheme 1 The schematic illustration of UiO-PQDMAEMA@PAN filter towards PM capture and airborne bacteria inactivation.



Scheme 2 Schematic preparation route for UiO-PQDMAEMA.

by a high voltage to draw threads of polymer solutions to fibers with diameters in the order of hundred nanometers.⁴⁷ The experimental details are summarized here. Four different DMF (*N,N*-dimethylformamide) solutions of PAN (6 wt% PAN loading), UiO-66-NH₂@PAN (60 wt% MOF loading), UiO-PQDMAEMA@PAN (60 wt% UiO-PQDMAEMA loading), and Cu@PAN (60 wt% Cu(NO)₃·3H₂O loading) were used as the precursors for the nanofibers. The electrospinning process was operated at a precursor flow rate of 0.5 ml per hour. A high voltage of 17 kV was applied and the distance between the collector and spinneret was set at 17 cm. The obtained fibers were collected on the substrate of stainless-steel mesh (from McMaster-Carr). The temperature and relative humidity (RH) were kept at 50 °C and 10%, respectively.

2.3 Materials characterization

The surface functional groups of the samples were analyzed by a Fourier transform infrared (FT-IR) spectrometer (Nicolet

iS50). X-ray diffraction (XRD) patterns were collected by the PANalytical X'Pert Pro MPD. Morphologies of the samples were observed by SEM (scanning electron microscopy, Su-70, Hitachi) and TEM (transmission electron microscopy, JEOL JEM-F200). Thermogravimetric analysis (TGA) was conducted with a TA Q500 under nitrogen gas flow with a heating rate of 10 °C min⁻¹. The gas adsorption experiments were carried out using Autosorb iQ (Quantachrome Instrument). The fluorescence images were obtained by the Zeiss Axiovert 200M fluorescence microscope. The surface compositions were determined by the X-ray photoelectron spectrometer (XPS, Thermo Scientific ESCALAB 250).

2.4 Particulate filtration tests

The particle filtration tests were conducted based on the ISO standard (ISO 21083-1:2018) for the flat sheet media and the experimental system is shown in Fig. 1a.⁴⁸ The particle filtration efficiency of as-synthesized filters was tested under



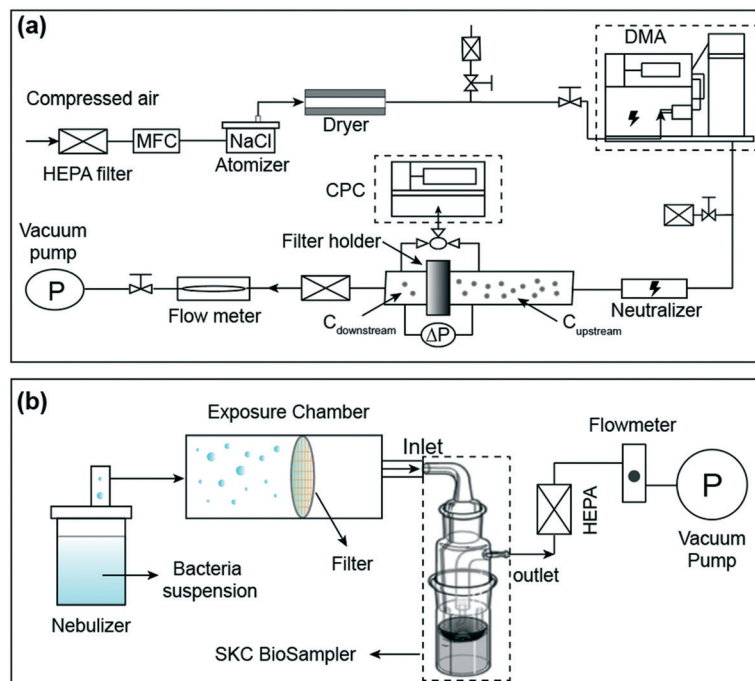


Fig. 1 Schematic diagram of the experimental setup for particle filtration measurements (a) and bacteria filtration tests (b).

9.3 cm s⁻¹ face velocity which is within the media face velocity ranges in the N95 test (~5–10 cm s⁻¹).^{49,50} In brief, monodisperse sodium chloride (NaCl) particles were generated by an atomizer (TSI model 9302, TSI Inc.) and classified by a differential mobility analyzer (DMA, Model 3082, TSI Inc.) with sizes of 20, 30, 50, 80, 100, 150, 200, 300, 400, and 500 nm. Before challenging the filter media, the classified monodisperse particles were neutralized by a Po²¹⁰ neutralizer to minimize the particle charge for mimicking the charging condition of ambient particles, which are normally in Boltzmann equilibrium.⁴⁴ An ultrafine condensation particle counter (UCPC, Model 3776, TSI Inc.) operated at 1.5 L min⁻¹ and a three-way valve were used to measure the upstream and downstream particle number concentrations of the filter media. For comparison, the filtration performance of a commercial N95 respirator from VWR (Makrite®) was also tested, in which a relatively flat portion of the respirator was cut out to form a flat sheet and the aforementioned same filtration procedure was applied.

The size-fractionated penetration, $P(d_x)$, representing the fraction of particles with diameter d_x can go through the filter medium, is defined as:

$$P(d_x) = \frac{C(d_x)_{\text{downstream}}}{C(d_x)_{\text{upstream}}} \quad (1)$$

where $C(d_x)_{\text{downstream}}$ and $C(d_x)_{\text{upstream}}$ are the downstream and upstream number concentrations of d_x particles, respectively. The size-fractionated filtration efficiency, $\text{PFE}(d_x)$, of the filter is thus calculated as:

$$\text{PFE}(d_x) = 1 - P(d_x) \quad (2)$$

The correction of $\text{PFE}(d_x)$ due to particle diffusion loss was also carried out and the method is described in the S2.† The upstream and downstream particle concentrations were measured for at least three times to obtain the representative filtration results. The standard deviation ($\sigma(d_x)$) was calculated using the following equation:

$$\sigma(d_x) = \frac{C(d_x)_{\text{downstream}}}{C(d_x)_{\text{upstream}}} \sqrt{\left(\frac{\sigma_{\text{downstream}}}{C(d_x)_{\text{downstream}}}\right)^2 + \left(\frac{\sigma_{\text{upstream}}}{C(d_x)_{\text{upstream}}}\right)^2} \quad (3)$$

where $\sigma_{\text{downstream}}$ and σ_{upstream} are the standard deviations at the downstream and upstream of the filter holder, respectively.⁵¹

2.5 Bacteria filtration tests

A system for bacteria filtration tests was also developed in this study (Fig. 1b). Specifically, two representative bacteria *S. epidermidis* (Gram-positive) and *E. coli* (Gram-negative) suspensions with a density at 10⁷ CFU mL⁻¹ in phosphate-buffered saline (PBS) solution were used as precursors. Then, the suspensions were atomized by an ultrasonic nebulizer operated at 2.4 MHz to generate bioaerosols to challenge the filters at a flow rate of 12.5 L min⁻¹ for 1 minute. A BioSampler (SKC Inc.) containing 20 ml sterile PBS solution was used to collect the escaped bioaerosol. After collection, the escaped bacteria concentrations were determined by the standard plate counting method. The plates were incubated at 37 °C for 20 hours, and the number of colonies was



enumerated through visual inspection. The bacterial filtration efficiency (BFE) of the filter is defined as follows:

$$\text{BFE} = 1 - \frac{C_f}{C_{\text{total}}} \quad (4)$$

where C_f (CFU mL⁻¹) is the bacteria concentration in the Biosampler with a face mask filter operation; C_{total} (CFU mL⁻¹) is the bacteria concentration in the Biosampler without a mask filter operation.

2.6 Bacteria inactivation assessments

The bacteria inactivation assessments were carried out as follows. After being challenged by the bioaerosol for 1

minute, the filter was sealed in a petri dish and placed in the dark for 2 hours to allow the interaction between the filter surface and captured bacteria. Subsequently, the filter was vortexed at 5000 rpm for 5 minutes to resuspend the captured bacteria in the 20 ml PBS solution. Then, the suspension was diluted with PBS, and 3 μ L of each decimal dilution was dropped in the sterile nutrient agar culture plates. The agar plates with the bacteria suspensions were incubated at 37 °C for 20 hours to give the visible colonies, which were enumerated to calculate the number of living bacteria. The bacteria inactivation efficiency (BIE) was calculated by the following equation:

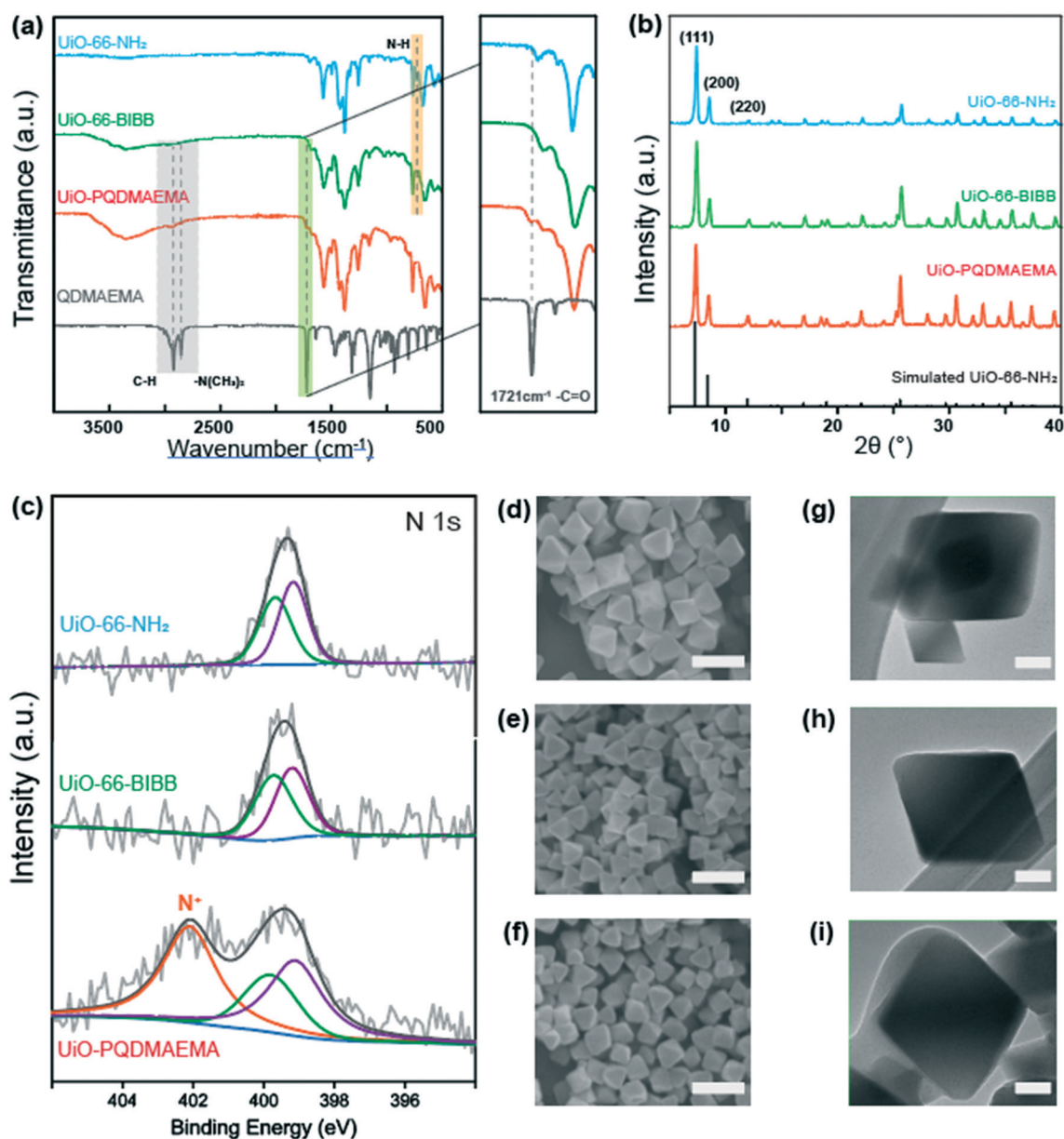


Fig. 2 FT-IR spectra (a) and XRD patterns (b), high-resolution N 1s XPS spectra (c), SEM images (d–f), and TEM images (g–i) of UiO-66-NH₂, UiO-66-BIBB, and UiO-PQDMAEMA, respectively (top to bottom). Scale bars in (d–f): 500 nm; scale bars in (g–i): 50 nm.



$$\text{BIE} = 1 - \frac{C_{\text{live}}}{C_{\text{total}}} \quad (5)$$

where C_{live} is the concentration of live bacteria remaining on the filter. Additionally, after being placed in the dark for 2 hours, the filter was cultured in the nutrient agar at 37 °C for 20 hours for residual analysis of remained viable cells.

Fluorescence microscopy is a useful technique to examine the viability of bacterial cells before and after contacting the filter. To perform this analysis, 1 ml bacteria cell suspension was centrifuged and resuspended in 10 μL of PBS solution, which was subsequently stained by a live/dead staining kit (Molecular Probes, Invitrogen) in the dark for 1 hour. Bacterial cells with intact cell membranes (live) were stained by SYTO 9 and fluorescent green, whereas propidium iodide (PI) penetrates only damaged membranes and stains the dead bacteria, which presented red fluorescence.

3. Results and discussion

3.1 Characterization of UiO-66-NH₂, UiO-BIBB, and UiO-PQDMAEMA

The surface chemistry of UiO-66-NH₂, UiO-66-BIBB, UiO-PQDMAEMA, and monomer QDMAEMA were analyzed by FT-IR as shown in Fig. 2a. It is found that the peak at 768 cm^{-1} in the raw UiO-66-NH₂, attributed to the N-H wagging vibrations,⁵² disappears in UiO-66-BIBB after modifications. This indicates that the initiator BIBB is successfully anchored on the -NH₂ group of UiO-66-NH₂ *via* covalent bonding. After ATRP reaction, an emerging peak at 1721 cm^{-1} is found in UiO-PQDMAEMA, which originates from the C=O stretching vibration of ester groups from QDMAEMA;⁵³ besides, two additional peaks at 2822 cm^{-1} and 2770 cm^{-1} are also observed in UiO-PQDMAEMA, which are assigned to the -N(CH₃)₂ symmetric and asymmetric vibrations from QDMAEMA, respectively.⁵⁴ Therefore, it can be concluded that PQDMAEMA is successfully grafted onto UiO-66-NH₂ *via* ATRP.

In addition to the surface chemistry, the crystalline structures of UiO-66-NH₂, UiO-66-BIBB, and UiO-PQDMAEMA were examined by XRD. As shown in Fig. 2b, the XRD pattern of the as-synthesized UiO-66-NH₂ is well consistent with the simulated one, where the characteristic peaks at 7.4° and 8.8° are attributed to the (111) and (200) crystal planes, respectively.⁵⁵ It is noted both UiO-66-BIBB and UiO-PQDMAEMA share almost the same XRD patterns as UiO-66-NH₂, indicating that the crystalline structure of UiO-66-NH₂ is maintained after BIBB treatment and polymerization. The unchanged crystalline structure of UiO-66-NH₂ throughout the entire synthesis procedures also implies that the UiO-66 modified materials are very stable, which is favorable for the post-processing and applications.

To further elucidate the evolution of nitrogen from the -NH₂ group in UiO-66-NH₂, the near-surface elemental information was determined by the XPS measurements.

Fig. 2c shows the deconvoluted N 1s core-level peaks of UiO-66-NH₂, UiO-66-BIBB, and UiO-PQDMAEMA. The XPS spectra of UiO-66-NH₂ and UiO-66-BIBB exhibit two nitrogen peaks at 398.9 eV and 399.8 eV, which are assigned to N-H and C-N, respectively.⁵⁶ A new peak at 402.0 eV is found in UiO-PQDMAEMA, which is attributed to the C-N⁺ component from the monomer QDMAEMA, confirming that an outer quaternized surface layer is formed.³⁵ Based on the XPS spectra in Fig. 2c, the quaternization degree (QD) of UiO-PQDMAEMA was estimated to be 48% (see ESI† for details).⁵⁷

The morphologies of UiO-66-NH₂, UiO-66-BIBB, and UiO-PQDMAEMA were also observed by SEM. As shown in Fig. 2(d, e, g and h), UiO-66-BIBB has similar crystal shapes to that of UiO-66-NH₂ with an average particle size of ~265 nm. After the ATRP reaction, the surface of UiO-PQMAEMA becomes smooth (Fig. 2f), and an obvious polymer shell can be observed in its TEM image (Fig. 2i). Understandably, the core contour and size are similar to those of unmodified UiO-66-NH₂, which is well consistent with the XRD results in Fig. 2b. According to the TGA results, the percentage of polymer in UiO-PQDMAEMA was estimated at 9.93% (Fig. S1†). All the above results once again confirm the successful grafting of PQDMAEMA onto UiO-66-NH₂.

3.2 Fabrication of UiO-PQDMAEMA@PAN filter *via* electrospinning

To fabricate composite nanofibers by using the electrospinning approach, a precursor solution of polymer and filler particles is generally used, resulting in the production of composite nanofibers where the filler particles are uniformly distributed inside the polymer backbone.¹⁹ This homogeneous structures are often undesirable as the functionality of the embedded fillers cannot be fully exploited. This is especially true in this work. To take full advantages of the surface properties of UiO-PQDMAEMA for efficient contact-killing bactericidal assays, the UiO-PQDMAEMA particles should be exposed on the surface of the polymer fibers. However, selective coating of the UiO-PQDMAEMA particles on the PAN fiber surface by using a single-step electrospinning method is challenging. In this work, we developed an engineering approach to rationally tune the diameter of the backbone support PAN fibers smaller than that of the filler UiO-PQDMAEMA particles ($d \cong 213$ nm, Fig. 2f) to expose them on the surface of the PAN fiber. Because the terminal fiber diameter (d_f) in electrospinning is determined by an equilibrium between the repulsive electrostatic force and liquid's surface tension, it can be predicted by the following equation:⁵⁸

$$d_f \sim \left(\gamma \frac{Q^2}{I^2} \right)^{\frac{1}{3}} w_p^{\frac{1}{2}} \quad (6)$$

where γ is the surface tension of the polymer solution, Q is the feeding flowrate, I is the electric current in the system, and w_p is the polymer volume fraction. Besides, the surface



tension is also a function of temperature, which can be expressed as:⁵⁹

$$\gamma = \gamma^0 \left(1 - \frac{T}{T_c}\right)^n \quad (7)$$

where γ^0 is the constant for each liquid, n is a positive empirical factor, T_c is the critical temperature and T is the actual temperature. To obtain thinner fibers, we rationally decrease the γ of PAN/DMF solution by increasing the working temperature to 50 °C, given that Q , I , and w_p are all fixed in our system. Furthermore, the working RH was kept at a low level of 10% to generate the thinner

nanofibers because a lower RH would favor the solvent evaporation and thus the solidification rate of the jet.⁶⁰ Not surprisingly, the defect-free and uniform nanofibers are observed in the pure PAN filter (Fig. 3a). The average diameter of pure PAN fibers is measured to be ~139 nm (Fig. 3c), which is thinner than those fabricated at room temperature (25 °C) and higher RH of 35% with an average diameter size of 242 nm (Fig. S2†). Fig. 3b shows the morphology of the UiO-PQDMAEMA@PAN filter, where the UiO-PQDMAEMA particles are well decorated on the PAN fiber surface with an overall average diameter of 368 nm (Fig. 3d). The exposure of the UiO-PQDMAEMA particles to

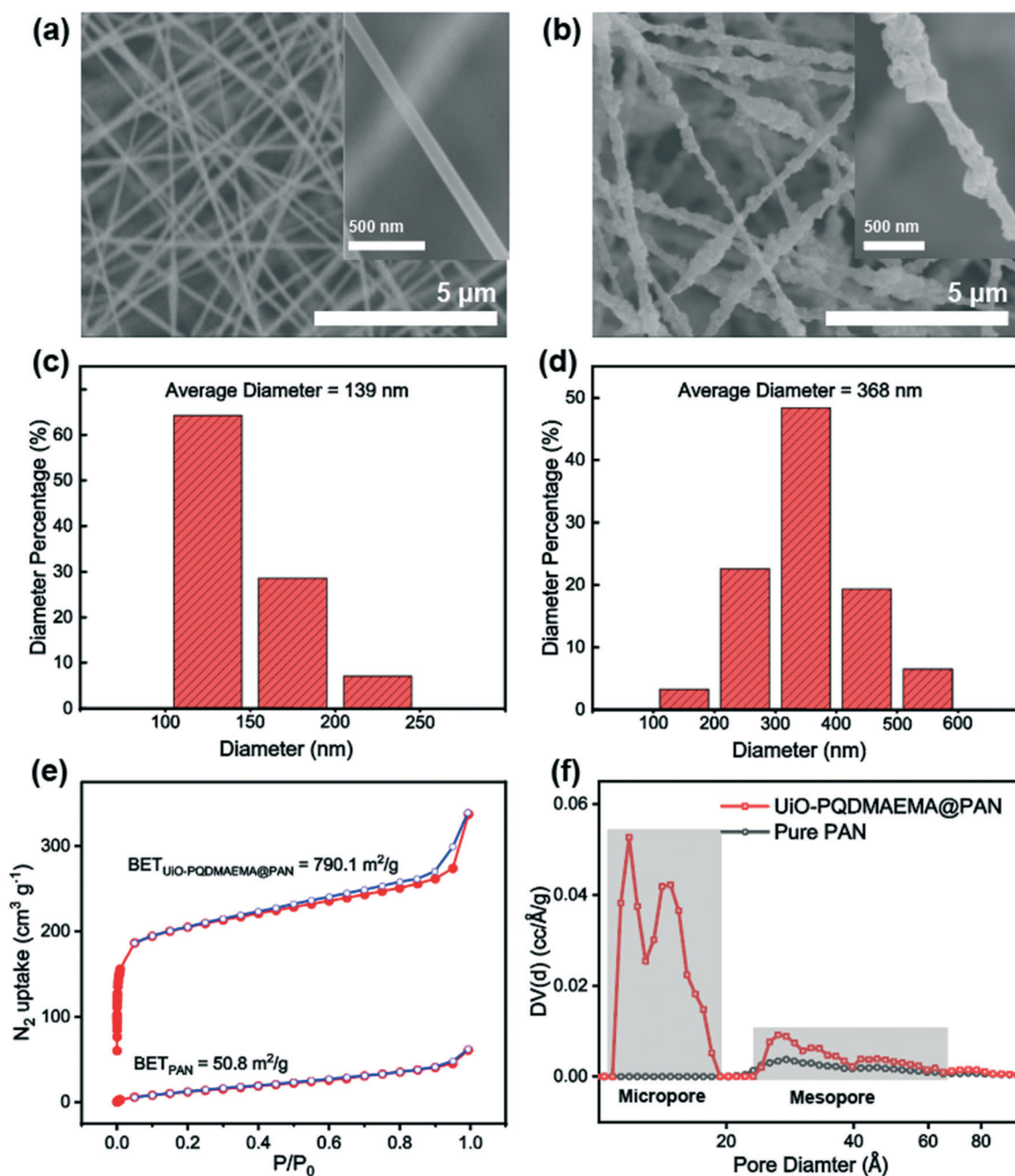


Fig. 3 SEM images, fiber diameter distribution, and BET analysis of pure PAN filter (a, c, e and f) and UiO-PQDMAEMA@PAN filter (b and d-f).



the environment (Fig. 3b) gives them more contacting opportunities with captured bacteria. The nitrogen sorption isotherms of the pure PAN and UiO-PQDMAEMA@PAN filters are shown in Fig. 3e. With the successful integration of porous UiO-PQDMAEMA into the PAN fibers, the BET surface area is increased to $790.1 \text{ m}^2 \text{ g}^{-1}$, which is much higher than the pure PAN filter of $50.8 \text{ m}^2 \text{ g}^{-1}$. For UiO-PQDMAEMA@PAN, the rapid increase in N_2 uptake at a low relative pressure ($P/P_0 < 0.01$) indicates the abundance of micropores (pore size $< 20 \text{ \AA}$), which is due to the existence of UiO-PQDMAEMA, while the slight increase at high relative pressure and the existence of hysteresis suggest the presence of mesopores ($200 \text{ \AA} > \text{pore size} > 20 \text{ \AA}$).⁶¹ Compared to the pure PAN with only mesopores, the UiO-PQDMAEMA@PAN filter exhibits a hierarchical structure containing the characteristics of both micropores and mesopores (Fig. 3f). Moreover, XRD and FT-IR analyses indicate that the crystalline structure and surface chemistry of the UiO-PQDMAEMA are retained after the electrospinning process (Fig. S3(a and b)†).

3.3 Evaluation of particle filtration performance

The particle filtration performances of the UiO-PQDMAEMA@PAN filter (shown in Fig. 4a) and the N95 (shown in Fig. 4b) were tested by the experimental setup shown in Fig. 1a. It should be noted that the particle filtration efficiency measured throughout the study is the

initial particle filtration efficiency as the challenging particles were low concentration monodisperse particles due to the classification of DMA. Thus, the loading effects can be neglected.^{62,63} According to the classic filtration theory,⁶⁴ when the particles pass through the fibrous filter, they are captured by the fiber through a combination of mechanisms including direct interception, inertial impaction, Brownian diffusion, gravitational settling, and electrostatic attraction. For the particles captured at a specific size, the predominant mechanisms vary based on the properties of the tested filters.⁶⁵ Therefore, each filter often has a specific size-fractionated efficiency curve. Fig. 4c compares the efficiency curves amongst the pure PAN, UiO-PQDMAEMA@PAN, and N95 filters. It is seen that the particle filtration efficiency decreases with particle size until it reaches the most penetrating particle size (MPPS) at around 80 nm, and subsequently increases for particles greater than 80 nm. By controlling the volume of the precursors, the thickness of the UiO-PQDMAEMA@PAN filter is adjusted to $16 \mu\text{m}$ (Fig. S3c†), and the minimum filtration efficiency of as-synthesized UiO-PQDMAEMA@PAN filter at 80 nm is measured to be $\sim 95.1\%$. The filtration performance is comparable to that of a commercial N95 respirator, which makes the UiO-PQDMAEMA@PAN a potential candidate for an N95 respirator filter medium. It is noted that as compared to the pure PAN filter tested under the same pressure drop (52.3 Pa), a higher filtration efficiency is obtained for the UiO-PQDMAEMA@PAN filter. This is probably due to the higher

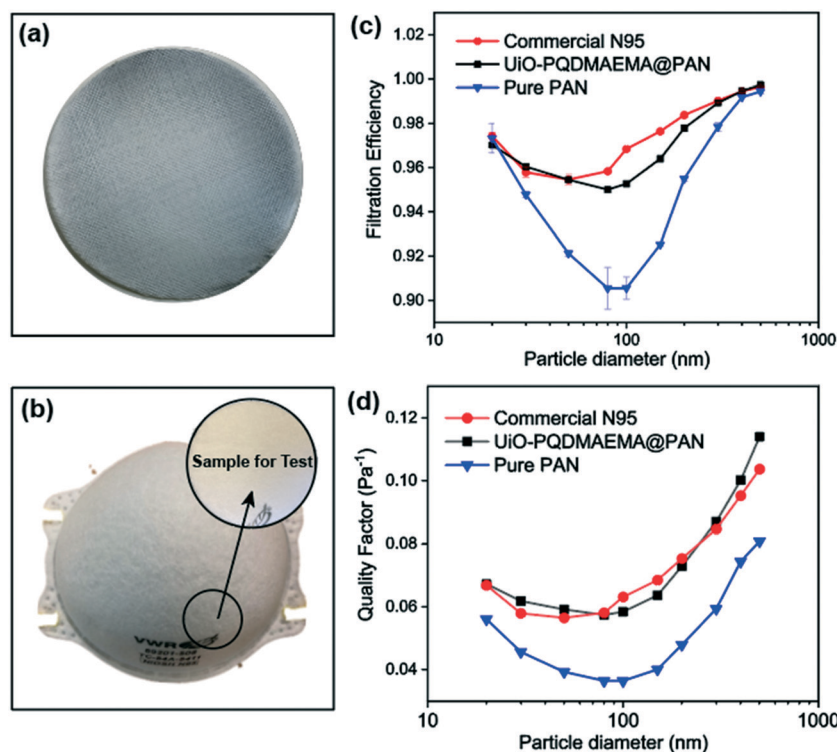


Fig. 4 Digital images of as-synthesized UiO-PQDMAEMA@PAN filter (a) and commercial N95 respirator (b); inset image in (b) is a relatively flat sheet cut out from the commercial N95 respirator for particle filtration test; particle filtration efficiency (c) and quality factor (d) tested by NaCl particles of 20–500 nm at a face velocity at 9.3 cm s^{-1} towards pure PAN filter, UiO-PQDMAEMA@PAN filter, and commercial N95 respirator.



fiber charge, chaotic airflow and larger local fiber diameter favorable for interception and diffusion depositions by the hierarchical MOF particles within the electrospun fibers.^{66–68} As shown in Fig. 3f, the UiO-PQDMAEMA@PAN filter is endowed with hierarchical structures, which contain both micropores and mesopores by embedding the porous UiO-PQDMAEMA particles in the electrospun fibers.

The pressure drop is another very important parameter, as breathing air behind the face mask requires significant pressure or energy provided by the users, which is highly related to wearer's comfort and health during breath. Therefore, a low-pressure drop is always a desirable filter property. The quality factor (QF), a comprehensive parameter, is used to evaluate the filtration performance of the filter media, which takes both efficiency and pressure into account. The QF is defined as:⁶⁹

$$QF = -\frac{\ln(1 - PFE)}{\Delta P} \quad (8)$$

where PFE and ΔP are the particle filtration efficiency and pressure drop across the filter, respectively. The higher the QF, the better the filter is. Given that the higher QF values are obtained as compared to the pure PAN, the UiO-PQDMAEMA@PAN filter has a much better filtration performance because of the incorporation of UiO-PQDMAEMA in the electrospun nanofibers. Additionally, the minimum QF value of the UiO-PQDMAEMA@PAN filter is calculated to be 0.058 at MPPS of 80 nm, which is comparable to that of 0.056 for the commercial N95 respirator at 50 nm, indicating that the UiO-PQDMAEMA@PAN filter demonstrates a satisfactory filtration performance.

3.4 Evaluation of bacteria filtration performance

The bacteria filtration performance of the UiO-PQDMAEMA@PAN filter is evaluated by challenging with the bioaerosols containing *S. epidermidis* (Gram-positive bacteria) and *E. coli* (Gram-negative bacteria). The schematic diagram of the experimental setup for the bioaerosol filtration is shown in Fig. 1b. The BioSampler (SKC Inc) which combines impingement with centrifugal motion is used for the escaped

bacteria collection. Specifically, there are three collection nozzles positioned at a specific angle above the collection sterile PBS solution during the sampling, and the air stream with bacteria is directed to the wall of the sampling where a liquid film is formed due to the centrifugal motion of the liquid.⁷⁰ This design lowers the microorganism stress as compared to the conventional impinger and ensures the viability of the collected bacteria, which makes SKC BioSampler a reliable and *de facto* reference sampler in bioaerosol studies.⁷¹ The recommended air flowrate for the N95 respirator test is 28.3 L min⁻¹ by the U.S. Food and Drug Administration (FDA),⁷² where the face velocity is calculated to be 3.1 cm s⁻¹.⁷² In our system, the face velocity of the tested filter is calculated to be 10.5 cm s⁻¹, given that the working flowrate of the BioSampler should be fixed at 12.5 L min⁻¹ to ensure the accuracy of the bacteria collection.⁷³ As shown in Fig. 5(a and b), no bacteria of *S. epidermidis* and *E. coli* are found after passing through the UiO-PQDMAEMA@PAN filter as well as the commercial N95 respirator, which indicates that all the airborne bacteria are completely captured by the filter even at a high face velocity of 10.5 cm s⁻¹. The reason for the airborne bacteria that cannot pass through the UiO-PQDMAEMA@PAN filter is mainly due to their sizes. Both *S. epidermidis* and *E. coli* have sizes in the range from 0.5 to 2 μ m, which is much larger than the MPPS (<100 nm) as discussed above. Therefore, the bacteria filtration of these filters is much more efficient. In summary, the as-synthesized UiO-PQDMAEMA@PAN filter demonstrates an excellent performance towards bacteria capture, which could be potentially used to protect user's safety by blocking out the routes of airborne bacteria transmission.

3.5 Bactericidal evaluation of UiO-PQDMAEMA@PAN filter

The bacteria inactivation performance of the UiO-PQDMAEMA@PAN filter was also evaluated towards both *S. epidermidis* and *E. coli*. Control experiments of pure PAN filter and UiO-66-NH₂@PAN filter were also conducted for comparison. As shown in Fig. 6(a and b), both pure PAN and UiO-66-NH₂@PAN filters show limited capabilities of killing bacteria while the UiO-PQDMAEMA@PAN filter has a

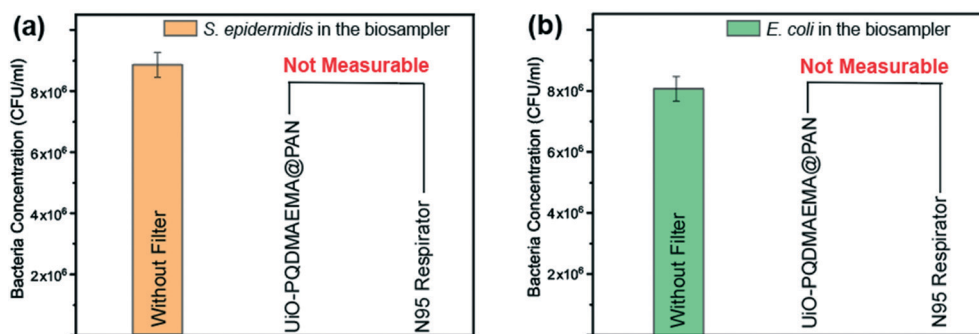


Fig. 5 Collected *S. epidermidis* (a) and *E. coli* (b) concentration in the SKC BioSampler after the airborne bacteria passing through the UiO-PQDMAEMA@PAN filter and commercial N95 respirator.



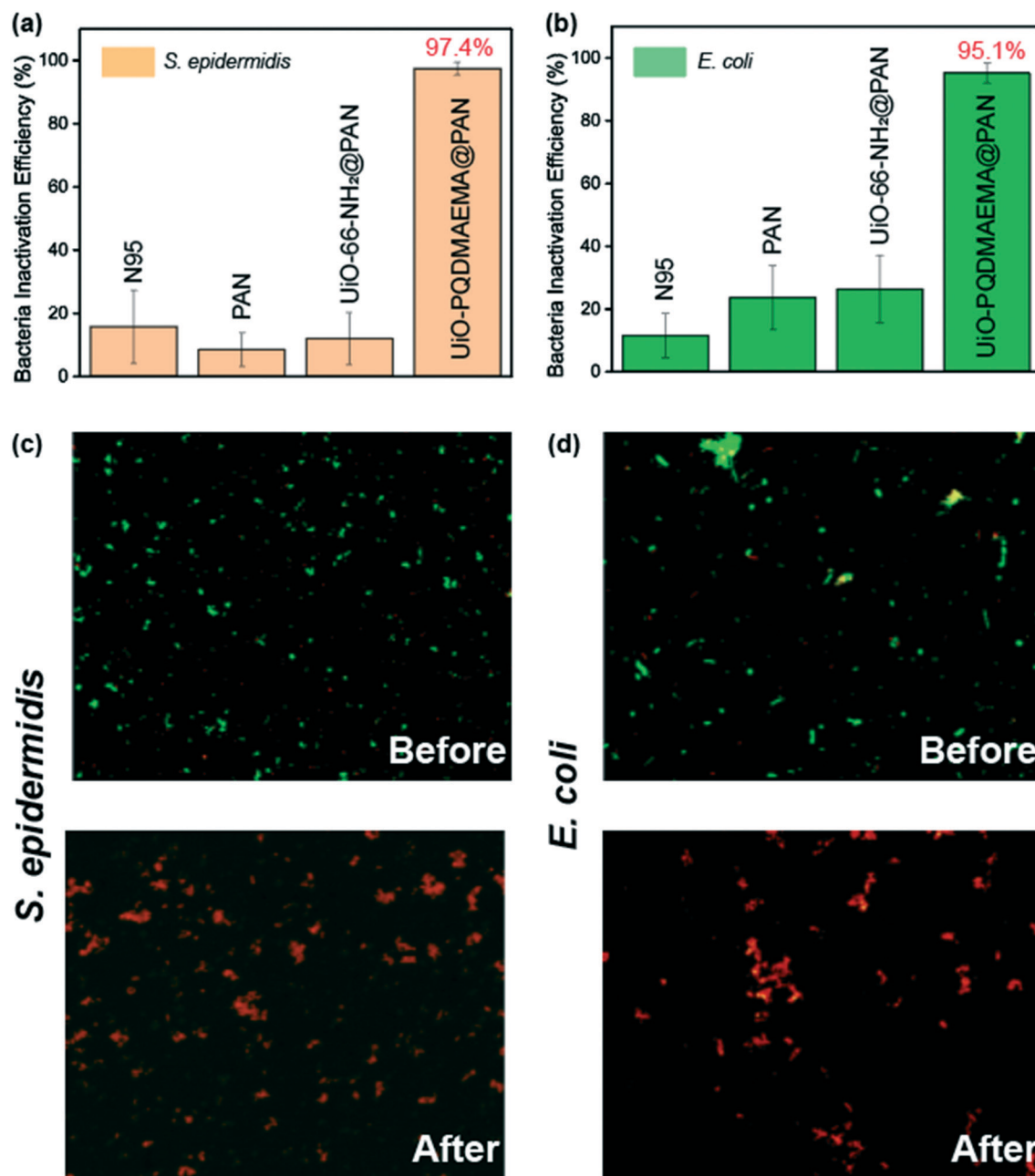


Fig. 6 *S. epidermidis* (a) and *E. coli*. (b) Inactivation performance towards commercial N95 respirator filter, PAN, UiO-66-NH₂@PAN, and UiO-PQDMAEMA@PAN filter; fluorescence images of the collected *S. epidermidis* (c) and *E. coli*. (d) Before and after contacting the UiO-PQDMAEMA@PAN filter.

significant inactivation efficiency of ~97.4% of *S. epidermidis* and ~95.1% of *E. coli*, indicating that the grafted UiO-PQDMAEMA on the surface of PAN fibers enables the filter to have efficient bactericidal behaviors. Further live/dead bacteria fluorescence assays using LIVE/DEAD kit were also conducted to investigate the bactericidal effects of the UiO-PQDMAEMA@PAN filter. Before conducting the experiments, most bacteria were alive and stained by SYTO 9, therefore, numerous green dots are observed in Fig. 6(c and d). However, the number of dead bacteria, which emit the red fluorescence was increased significantly after contacting the

surface of the UiO-PQDMAEMA@PAN filter, implying that the membrane integrity of bacterial cells is disrupted. Meanwhile, the ratio of live and dead bacteria in fluorescence images shows almost no change in the control group of pure PAN and UiO-66-NH₂@PAN filters once again confirming the bactericidal behaviors of the UiO-PQDMAEMA@PAN filter. (Fig. S4†) The commercial N95 respirator was also tested towards bactericidal performance. As shown in Fig. 6(a and b) and S4†, negligible bacterial inactivation efficiencies can be obtained for *S. epidermidis* and *E. coli*, indicating that most of the adhered bacteria are still alive,



which is the main reason that the contaminated respirator could be the source of HAIs transmission. As compared to the commercial N95 respirator, the as-synthesized UiO-PQDMAEMA@PAN filter demonstrates an efficient and rapid bacteria inactivation performance, which makes it a promising candidate for the antibacterial filter in the N95 level respirator.

Since typical bactericidal activities of QAC-based polymers are based on the contact killing mechanism, where the electrostatic interactions between negatively charged bacteria cell wall and positively charged QAC-based molecules are mainly responsible for the disruption of bacteria membrane, two prerequisites should be satisfied to endow the materials to have efficient antibacterial performance.^{42,74} One is the enough contacting time between bacteria and QAC-modified surfaces, and the other is that a threshold of charge density should be reached.⁷⁵ In this study, when the airborne bacteria are captured by the filter, they are trapped by multiple nanofibers containing numerous contacting sites of positively charged UiO-PQDMAEMA (N^+). (Scheme 1 and Fig. 2c) From the time course of bacteria inactivation in Fig. S5,† the UiO-PQDMAEMA@PAN filters exhibit limited bactericidal performance within the first 30 minutes, which is probably due to the insufficient interactions between bacterial cell wall and UiO-PQDMAEMA particles. When the contacting time extended to 2 hours, 97.4% of *S. epidermidis* and 95.1% *E. coli* were finally killed. Compared to the Gram-positive bacteria *S. epidermidis*, the Gram-negative bacteria *E. coli* exhibited a relatively greater resistance to contact disinfection, as shown in Fig. 6, indicating a difference in physicochemical interaction with the UiO-PQDMAEMA@PAN. The discrepancy in the antibacterial efficiency could be caused by various cell structures between the Gram-positive bacteria and the Gram-negative bacteria. The Gram-positive bacterial cell wall is composed of a simple layer of peptidoglycan. This layer has numerous pores, which allow the QAC molecules to readily penetrate the thick cell wall and reach the cytoplasmic membrane.⁷⁶ However, the cell wall of the Gram-negative bacteria *E. coli* is comprised of two membranes reinforced by the expression of lipopolysaccharide on the cellular surface, which provides an additional protective property.⁷⁷ Therefore, a more efficient antibacterial performance was obtained towards *S. epidermidis* than *E. coli*.

The positive charge density of outer layer is another key parameter to define antibacterial efficacy.⁷⁵ For *S. epidermidis* and *E. coli* inactivation, the prerequisite charge density should be above the critical threshold of 1×10^{12} – $10^{14} N^+$ per cm^2 .^{78,79} To calculate the charge density of UiO-PQDMAEMA, we used the crystal in Fig. 2i (also Fig. S6†) for further estimation. The crystal in red contour is the initial UiO-66- NH_2 , which is decorated by a layer of QAC polymer. Assuming that charges were uniformly distributed within the polymer layer, the charge density (CD) can be determined by the following equation:

$$CD = \frac{Q}{A} \quad (9)$$

where Q is the surface charge and A is the surface area. The CD of UiO-PQDMAEMA was calculated to be $3 \times 10^{14} N^+$ per cm^2 (see S8† for details). Therefore, UiO-PQDMAEMA in this work is expected to exhibit effective antibacterial actions. Besides, the monomer DMAEMA is quaternized by 1-bromodecane to impart the QDMAEMA with 10 carbon atoms in the alkyl chains. (Scheme 2) The relatively long alkyl chains in UiO-PQDMAEMA could interact strongly with the peptidoglycan cell wall and, finally, bacteria are killed by the lysis of their cytoplasm.⁴¹

To further unravel the interactions between UiO-PQDMAEMA@PAN filter and bacteria, the morphologies of *S. epidermidis* and *E. coli* were observed by SEM. As shown in Fig. 7(a and c), the cells of *S. epidermidis* and *E. coli* maintained intact upon initial contact with the UiO-PQDMAEMA filter. After contacting treatment for 2 hours, the shapes of both *S. epidermidis* and *E. coli* are deformed, and the cell membranes are severely damaged (Fig. 7(b and d)), which indicates that the QAC modified MOF enables the electrospun filter with efficient antibacterial capability against both Gram-negative and Gram-positive bacteria.

3.6 Leakage evaluation

The leakage of the antibacterial agent during the filtration and antimicrobial activity is a serious issue because improper intake of these chemicals would result in severe health issues.⁸⁰ Among the commercial antimicrobial face masks and respirators, Ag^+ and Cu^{2+} are the two most frequently used metal ions in the filter media to inactivate microorganisms.⁸¹ Herein, we fabricated a Cu^{2+} -loaded PAN

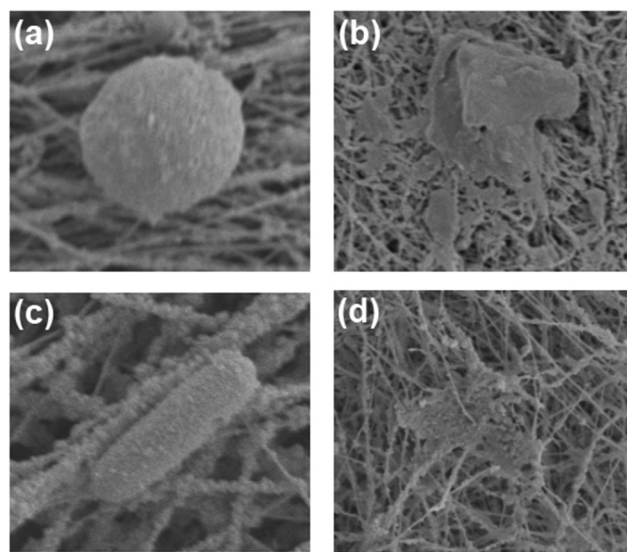


Fig. 7 SEM images of UiO-PQDMAEMA@PAN filter with *S. epidermidis* (a and b) and *E. coli*. (c and d) After contacting treatment for 0 and 2 hours.



filter (Cu@PAN) for comparison. To examine the leakage behaviors, both UiO-PQDMAEMA@PAN and Cu@PAN filters were immersed in the 100 ml DI water for 2 hours. Then, 1 ml AgNO_3 (1 mM) and Na_2S (1 mM) were added into UiO-PQDMAEMA@PAN and Cu@PAN solutions, respectively. The rationale for designing the leakage test is as follows. For the UiO-PQDMAEMA@PAN filter, there might be some Br^- released from the 1-bromodecane ($\text{C}_{10}\text{H}_{21}\text{Br}$) in the UiO-PQDMAEMA particles (see Scheme 2 for details). If Br^- is leaked from the filter, it would react quickly with Ag^+ to form a yellow precipitate, AgBr . Similarly, the Cu^{2+} released from Cu@PAN filter would combine with S^{2-} in the Na_2S solution to produce CuS precipitates. As shown in Fig. S8,† no color change is observed in the UiO-PQDMAEMA@PAN beaker after AgNO_3 titration, indicating there is negligible Br^- leakage. While the solution turned to be brown in the Cu@PAN beaker, which is caused by the formation of a low concentration of CuS precipitates. As compared to the Cu@PAN filter, negligible leakage was found in the UiO-PQDMAEMA@PAN immersed in the water, indicating that the UiO-PQDMAEMA@PAN filter is safe for humans and environmentally friendly.

4. Conclusion

In summary, we designed an antibacterial filter where the QAC modified MOF (UiO-PQDMAEMA) was incorporated into the electrospun PAN fibers. The antibacterial agent polymeric QACs (PQDMAEMA) was grafted onto the surface of UiO-66- NH_2 via ATRP. To partially expose the surface of the UiO-PQDMAEMA particles, the backbone electrospun PAN nanofibers were produced at an enhanced working temperature of 50 °C and low RH of 10%. The as-synthesized UiO-PQDMAEMA@PAN filter exhibited a satisfactory performance towards PM filtration and bacterial blockage, which is comparable to those of the commercial N95 respirator. In particular, the UiO-PQDMAEMA@PAN filter demonstrated excellent bactericidal activities towards both Gram-positive *S. epidermidis* and Gram-negative *E. coli* via a contact-killing mechanism. The incorporated UiO-PQDMAEMA particles with positively charged nitrogen (N^+) in the long alky chain resulted in the deformation and damage of cells after electrostatic interactions between UiO-PQDMAEMA and bacteria. The current work indicates that the UiO-PQDMAEMA@PAN could be a comprehensive protection core filter for the N95 respirator against PM and airborne bacteria. This study also sheds light on the design of QAC modified antibacterial materials and paves a way for the application of these materials in air cleaning.

Author contributions

Z. Zhu worked in conceptualization, methodology, formal analysis, investigation, and validation. Y. Zhang and S.-C. Chen took part in filtration measurements, data curation, and formal analysis. L. Bao worked in formal analysis of bacteria

inactivation. J. Chen assisted in material synthesis. S. Duan helped with conceptualization and methodology. W.-N. Wang and P. Xu worked in funding acquisition and supervision. Z. Zhu and W.-N. Wang wrote the paper. All authors have read and agreed to the published version of the manuscript.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The authors acknowledge the financial support from National Science Foundation (CMMI-1727553), the Center for Innovative Technology (CIT) through the Commonwealth Research Commercialization Fund (CRCF) program, as well as the VCU COVID-19 Rapid Research Funding Program.

References

- 1 A. Y. Peleg and D. C. Hooper, Hospital-Acquired Infections Due to Gram-Negative Bacteria, *N. Engl. J. Med.*, 2010, **362**, 1804–1813.
- 2 S. S. Magill, E. O'Leary, S. J. Janelle, D. L. Thompson, G. Dumyati, J. Nadle, L. E. Wilson, M. A. Kainer, R. Lynfield, S. Greissman, S. M. Ray, Z. Beldavs, C. Gross, W. Bamberg, M. Sievers, C. Concannon, N. Buhr, L. Warnke, M. Maloney, V. Ocampo, J. Brooks, T. Oyewumi, S. Sharmin, K. Richards, J. Rainbow, M. Samper, E. B. Hancock, D. Leaptrot, E. Scalise, F. Badrun, R. Phelps and J. R. Edwards, Changes in Prevalence of Health Care-Associated Infections in U.S. Hospitals, *N. Engl. J. Med.*, 2018, **379**, 1732–1744.
- 3 S. S. Magill, J. R. Edwards, W. Bamberg, Z. G. Beldavs, G. Dumyati, M. A. Kainer, R. Lynfield, M. Maloney, L. McAllister-Hollod, J. Nadle, S. M. Ray, D. L. Thompson, L. E. Wilson and S. K. Fridkin, Multistate Point-Prevalence Survey of Health Care-Associated Infections, *N. Engl. J. Med.*, 2014, **370**, 1198–1208.
- 4 P. W. Stone, Economic burden of healthcare-associated infections: an American perspective, *Expert Rev. Pharmacoecon Outcomes Res.*, 2009, **9**, 417–422.
- 5 A. Marchetti and R. Rossiter, Economic burden of healthcare-associated infection in US acute care hospitals: societal perspective, *J. Med. Econ.*, 2013, **16**, 1399–1404.
- 6 B. Carter, J. T. Collins, F. Barlow-Pay, F. Rickard, E. Bruce, A. Verduri, T. J. Quinn, E. Mitchell, A. Price, A. Vilches-Moraga, M. J. Stechman, R. Short, A. Einarsson, P. Braude, S. Moug, P. K. Myint, J. Hewitt, L. Pearce, K. McCarthy and C. S. Collaborators, Nosocomial COVID-19 infection: examining the risk of mortality. The COPE-Nosocomial Study (COVID in Older PEople), *J. Hosp. Infect.*, 2020, **106**, 376–384.
- 7 L. Rosenstock, 42 CFR Part 84: Respiratory Protective Devices Implications for Tuberculosis Protection, *Infect. Control Hosp. Epidemiol.*, 1995, **16**, 529–531.
- 8 Centers for Disease Control and Prevention (CDC), Laboratory performance evaluation of N95 filtering facepiece respirators, 1996, *Morb. Mortal. Wkly. Rep.*, 1998, **47**, 1045–1049.



- 9 L. Liao, W. Xiao, M. Zhao, X. Yu, H. Wang, Q. Wang, S. Chu and Y. Cui, Can N95 Respirators Be Reused after Disinfection? How Many Times?, *ACS Nano*, 2020, **14**, 6348–6356.
- 10 G.-H. Zhang, Q.-H. Zhu, L. Zhang, F. Yong, Z. Zhang, S.-L. Wang, Y. Wang, L. He and G.-H. Tao, High-performance particulate matter including nanoscale particle removal by a self-powered air filter, *Nat. Commun.*, 2020, **11**, 1653.
- 11 H. Zhong, Z. Zhu, P. You, J. Lin, C. F. Cheung, V. L. Lu, F. Yan, C.-Y. Chan and G. Li, Plasmonic and Superhydrophobic Self-Decontaminating N95 Respirators, *ACS Nano*, 2020, **14**, 8846–8854.
- 12 Y. Bai, C. B. Han, C. He, G. Q. Gu, J. H. Nie, J. J. Shao, T. X. Xiao, C. R. Deng and Z. L. Wang, Washable Multilayer Triboelectric Air Filter for Efficient Particulate Matter PM2.5 Removal, *Adv. Funct. Mater.*, 2018, **28**, 1706680.
- 13 A. Charvet, Y. Gonthier, E. Gonze and A. Bernis, Experimental and modelled efficiencies during the filtration of a liquid aerosol with a fibrous medium, *Chem. Eng. Sci.*, 2010, **65**, 1875–1886.
- 14 M. Tebyetekerwa, Z. Xu, S. Yang and S. Ramakrishna, Electrospun Nanofibers-Based Face Masks, *Advanced Fiber Materials*, 2020, **2**, 161–166.
- 15 Y. Cheng, C. Wang, J. Zhong, S. Lin, Y. Xiao, Q. Zhong, H. Jiang, N. Wu, W. Li, S. Chen, B. Wang, Y. Zhang and J. Zhou, Electrospun polyetherimide electret nonwoven for bi-functional smart face mask, *Nano Energy*, 2017, **34**, 562–569.
- 16 R. S. Barhate and S. Ramakrishna, Nanofibrous filtering media: Filtration problems and solutions from tiny materials, *J. Membr. Sci.*, 2007, **296**, 1–8.
- 17 S. Ullah, A. Ullah, J. Lee, Y. Jeong, M. Hashmi, C. Zhu, K. I. Joo, H. J. Cha and I. S. Kim, Reusability Comparison of Melt-Blown vs Nanofiber Face Mask Filters for Use in the Coronavirus Pandemic, *ACS Appl. Nano Mater.*, 2020, **3**, 7231–7241.
- 18 N. Wang, X. Wang, B. Ding, J. Yu and G. Sun, Tunable fabrication of three-dimensional polyamide-66 nano-fiber/nets for high efficiency fine particulate filtration, *J. Mater. Chem.*, 2012, **22**, 1445–1452.
- 19 Y. Zhang, S. Yuan, X. Feng, H. Li, J. Zhou and B. Wang, Preparation of Nanofibrous Metal–Organic Framework Filters for Efficient Air Pollution Control, *J. Am. Chem. Soc.*, 2016, **138**, 5785–5788.
- 20 Y. Bian, R. Wang, S. Wang, C. Yao, W. Ren, C. Chen and L. Zhang, Metal–organic framework-based nanofiber filters for effective indoor air quality control, *J. Mater. Chem. A*, 2018, **6**, 15807–15814.
- 21 M. Wen, G. Li, H. Liu, J. Chen, T. An and H. Yamashita, Metal–organic framework-based nanomaterials for adsorption and photocatalytic degradation of gaseous pollutants: recent progress and challenges, *Environ. Sci.: Nano*, 2019, **6**, 1006–1025.
- 22 S. Feng, X. Li, S. Zhao, Y. Hu, Z. Zhong, W. Xing and H. Wang, Multifunctional metal organic framework and carbon nanotube-modified filter for combined ultrafine dust capture and SO₂ dynamic adsorption, *Environ. Sci.: Nano*, 2018, **5**, 3023–3031.
- 23 Y. Zhang, X. He, Z. Zhu, W.-N. Wang and S.-C. Chen, Simultaneous removal of VOCs and PM_{2.5} by metal-organic framework coated electret filter media, *J. Membr. Sci.*, 2021, **618**, 118629.
- 24 Y. Bian, C. Chen, R. Wang, S. Wang, Y. Pan, B. Zhao, C. Chen and L. Zhang, Effective removal of particles down to 15 nm using scalable metal-organic framework-based nanofiber filters, *Appl. Mater. Today*, 2020, **20**, 100653.
- 25 R. A. Weinstein, R. Gaynes, J. R. Edwards and N. N. I. S. System, Overview of Nosocomial Infections Caused by Gram-Negative Bacilli, *Clin. Infect. Dis.*, 2005, **41**, 848–854.
- 26 J. D. Siegel, E. Rhinehart, M. Jackson and L. Chiarello, 2007 Guideline for Isolation Precautions: Preventing Transmission of Infectious Agents in Health Care Settings, *Am. J. Infect. Control*, 2007, **35**, S65–S164.
- 27 L. Zhiqing, C. Yongyun, C. Wenxiang, Y. Mengning, M. Yuanqing, Z. Zhenan, W. Haishan, Z. Jie, D. Kerong, L. Huiwu, L. Fengxiang and Z. Zanjing, Surgical masks as source of bacterial contamination during operative procedures, *J. Orthop. Translat.*, 2018, **14**, 57–62.
- 28 S. B. Jeong, H. S. Ko, S. C. Seo and J. H. Jung, Evaluation of filtration characteristics and microbial recovery rates of commercial filtering facepiece respirators against airborne bacterial particles, *Sci. Total Environ.*, 2019, **682**, 729–736.
- 29 M. Wu, B. Ma, T. Pan, S. Chen and J. Sun, Silver-Nanoparticle-Colored Cotton Fabrics with Tunable Colors and Durable Antibacterial and Self-Healing Superhydrophobic Properties, *Adv. Funct. Mater.*, 2016, **26**, 569–576.
- 30 J. M. Mazurkow, N. S. Yüzbaşı, K. W. Domagala, S. Pfeiffer, D. Kata and T. Graule, Nano-Sized Copper (Oxide) on Alumina Granules for Water Filtration: Effect of Copper Oxidation State on Virus Removal Performance, *Environ. Sci. Technol.*, 2020, **54**, 1214–1222.
- 31 D. Lv, R. Wang, G. Tang, Z. Mou, J. Lei, J. Han, S. De Smedt, R. Xiong and C. Huang, Ecofriendly Electrospun Membranes Loaded with Visible-Light-Responding Nanoparticles for Multifunctional Usages: Highly Efficient Air Filtration, Dye Scavenging, and Bactericidal Activity, *ACS Appl. Mater. Interfaces*, 2019, **11**, 12880–12889.
- 32 W. Tong, Y. Xiong, S. Duan, X. Ding and F.-J. Xu, Phthalocyanine functionalized poly(glycidyl methacrylate) nano-assemblies for photodynamic inactivation of bacteria, *Biomater. Sci.*, 2019, **7**, 1905–1918.
- 33 R. J. Roberge, E. Bayer, J. B. Powell, A. Coca, M. R. Roberge and S. M. Benson, Effect of Exhaled Moisture on Breathing Resistance of N95 Filtering Facepiece Respirators, *Ann. Occup. Hyg.*, 2010, **54**, 671–677.
- 34 A. Haider, S. Kwak, K. C. Gupta and I.-K. Kang, Antibacterial Activity and Cytocompatibility of PLGA/CuO Hybrid Nanofiber Scaffolds Prepared by Electrospinning, *J. Nanomater.*, 2015, **2015**, 832762.
- 35 Y. Zhang, X. Zhang, Y.-Q. Zhao, X.-Y. Zhang, X. Ding, X. Ding, B. Yu, S. Duan and F.-J. Xu, Self-adaptive antibacterial surfaces with bacterium-triggered antifouling-bactericidal switching properties, *Biomater. Sci.*, 2020, **8**, 997–1006.



- 36 H. Sun, Y. Du, C. Gao, Iftikhar, J. Long, S. Li and L. Shao, Pressure-assisted in-depth hydrophilic tailoring of porous membranes achieving high water permeability, excellent fouling resistance and superior antimicrobial ability, *J. Membr. Sci.*, 2020, **604**, 118071.
- 37 M. Ping, X. Zhang, M. Liu, Z. Wu and Z. Wang, Surface modification of polyvinylidene fluoride membrane by atom-transfer radical-polymerization of quaternary ammonium compound for mitigating biofouling, *J. Membr. Sci.*, 2019, **570–571**, 286–293.
- 38 Z. K. Zander, P. Chen, Y.-H. Hsu, N. Z. Dreger, L. Savariau, W. C. McRoy, A. E. Cerchiari, S. D. Chambers, H. A. Barton and M. L. Becker, Post-fabrication QAC-functionalized thermoplastic polyurethane for contact-killing catheter applications, *Biomaterials*, 2018, **178**, 339–350.
- 39 W. W. Wilson, M. M. Wade, S. C. Holman and F. R. Champlin, Status of methods for assessing bacterial cell surface charge properties based on zeta potential measurements, *J. Microbiol. Methods*, 2001, **43**, 153–164.
- 40 M. C. Jennings, K. P. C. Minbiole and W. M. Wuest, Quaternary Ammonium Compounds: An Antimicrobial Mainstay and Platform for Innovation to Address Bacterial Resistance, *ACS Infect. Dis.*, 2015, **1**, 288–303.
- 41 G. Gozzelino, C. Lisanti and S. Beneventi, Quaternary ammonium monomers for UV crosslinked antibacterial surfaces, *Colloids Surf., A*, 2013, **430**, 21–28.
- 42 Y. Jiao, L.-n. Niu, S. Ma, J. Li, F. R. Tay and J.-h. Chen, Quaternary ammonium-based biomedical materials: State-of-the-art, toxicological aspects and antimicrobial resistance, *Prog. Polym. Sci.*, 2017, **71**, 53–90.
- 43 M. H. Chua, W. Cheng, S. S. Goh, J. Kong, B. Li, J. Y. C. Lim, L. Mao, S. Wang, K. Xue, L. Yang, E. Ye, K. Zhang, W. C. D. Cheong, B. H. Tan, Z. Li, B. H. Tan and X. J. Loh, Face Masks in the New COVID-19 Normal: Materials, Testing, and Perspectives, *Research*, 2020, **2020**, 7286735.
- 44 M. Tang, D. Thompson, S.-C. Chen, Y. Liang and D. Y. H. Pui, Evaluation of different discharging methods on HVAC electret filter media, *Build. Environ.*, 2018, **141**, 206–214.
- 45 K. Xie, Q. Fu, Y. He, J. Kim, S. J. Goh, E. Nam, G. G. Qiao and P. A. Webley, Synthesis of well dispersed polymer grafted metal–organic framework nanoparticles, *Chem. Commun.*, 2015, **51**, 15566–15569.
- 46 H. Sun, B. Tang and P. Wu, Development of Hybrid Ultrafiltration Membranes with Improved Water Separation Properties Using Modified Superhydrophilic Metal–Organic Framework Nanoparticles, *ACS Appl. Mater. Interfaces*, 2017, **9**, 21473–21484.
- 47 J. Xue, T. Wu, Y. Dai and Y. Xia, Electrospinning and Electrospun Nanofibers: Methods, Materials, and Applications, *Chem. Rev.*, 2019, **119**, 5298–5415.
- 48 EN, ISO 21083-1:2018, *Test method to measure the efficiency of air filtration media against spherical nanomaterials — Part 1: Size range from 20 nm to 500 nm*, 2018.
- 49 C.-Y. Tien, J.-P. Chen, S. Li, Z. Li, Y.-M. Zheng, A. S. Peng, F. Zhou, C.-J. Tsai and S.-C. Chen, Experimental and theoretical analysis of loading characteristics of different electret media with various properties toward the design of ideal depth filtration for nanoparticles and fine particles, *Sep. Purif. Technol.*, 2020, **233**, 116002.
- 50 NIOSH, *Approval of Respiratory Protective Devices, Code of Federal Regulations Title 42, Part 84*, NIOSH, Cincinnati, OH, USA, 1995, vol. 16, pp. 529–531.
- 51 W. Hao, G. Xu and Y. Wang, Factors influencing the filtration performance of homemade face masks, *J. Occup. Environ. Hyg.*, 2021, **18**, 128–138.
- 52 S. Saebo, L. Farnell, N. V. Riggs and L. Radom, Molecular structure, rotational constants, and vibrational frequencies for ethynamine (NH₂-C≡CH): a possible interstellar molecule, *J. Am. Chem. Soc.*, 1984, **106**, 5047–5051.
- 53 X. Tang, J. Wei, Z. Kong, H. Zhang and J. Tian, Introduction of amino and rGO into PP nonwoven surface for removal of gaseous aromatic pollutants and particulate matter from air, *Appl. Surf. Sci.*, 2020, **511**, 145631.
- 54 C. Greve, N. K. Preketes, R. Costard, B. Koeppe, H. Fidler, E. T. J. Nibbering, F. Temps, S. Mukamel and T. Elsaesser, N–H Stretching Modes of Adenosine Monomer in Solution Studied by Ultrafast Nonlinear Infrared Spectroscopy and Ab Initio Calculations, *J. Phys. Chem. A*, 2012, **116**, 7636–7644.
- 55 A. Schaate, P. Roy, A. Godt, J. Lippke, F. Waltz, M. Wiebecke and P. Behrens, Modulated Synthesis of Zr-Based Metal–Organic Frameworks: From Nano to Single Crystals, *Chem. – Eur. J.*, 2011, **17**, 6643–6651.
- 56 Q. Xiao, Y. Liang, F. Zhu, S. Lu and S. Huang, Microwave-assisted one-pot synthesis of highly luminescent N-doped carbon dots for cellular imaging and multi-ion probing, *Microchim. Acta*, 2017, **184**, 2429–2438.
- 57 J.-W. Xu, Y. Wang, Y.-F. Yang, X.-Y. Ye, K. Yao, J. Ji and Z.-K. Xu, Effects of quaternization on the morphological stability and antibacterial activity of electrospun poly(DMAEMA-co-AMA) nanofibers, *Colloids Surf., B*, 2015, **133**, 148–155.
- 58 S. V. Fridrikh, J. H. Yu, M. P. Brenner and G. C. Rutledge, Controlling the Fiber Diameter during Electrospinning, *Phys. Rev. Lett.*, 2003, **90**, 144502.
- 59 N. K. Adam, *The Physics and Chemistry of Surfaces*, Oxford University Press, 1941.
- 60 X. Wang, B. Ding, J. Yu and J. Yang, Large-scale fabrication of two-dimensional spider-web-like gelatin nano-nets via electro-netting, *Colloids Surf., B*, 2011, **86**, 345–352.
- 61 S. Lowell, J. E. Shields, M. A. Thomas and M. Thommes, *Characterization of porous solids and powders: surface area, pore size and density*, Springer Science & Business Media, 2012.
- 62 D.-Q. Chang, S.-C. Chen and D. Y. H. Pui, Capture of Sub-500 nm Particles Using Residential Electret HVAC Filter Media-Experiments and Modeling, *Aerosol Air Qual. Res.*, 2017, **16**, 3349–3357.
- 63 S.-C. Chen, J. Wang, Y. K. Bahk, H. Fissan and D. Y. H. Pui, Carbon Nanotube Penetration Through Fiberglass and Electret Respirator Filter and Nuclepore Filter Media: Experiments and Models, *Aerosol Sci. Technol.*, 2014, **48**, 997–1008.



- 64 W. C. Hinds and W. C. Hinds, *Aerosol Technology: Properties, Behavior, and Measurement of Airborne Particles*, Wiley, 1999.
- 65 T.-H. Kao, S.-K. Su, C.-I. Su, A.-W. Lee and J.-K. Chen, Polyacrylonitrile microscavolds assembled from mesh structures of aligned electrospun nanofibers as high-efficiency particulate air filters, *Aerosol Sci. Technol.*, 2016, **50**, 615–625.
- 66 H. Wan, N. Wang, J. Yang, Y. Si, K. Chen, B. Ding, G. Sun, M. El-Newehy, S. S. Al-Deyab and J. Yu, Hierarchically structured polysulfone/titania fibrous membranes with enhanced air filtration performance, *J. Colloid Interface Sci.*, 2014, **417**, 18–26.
- 67 Z. Wang, Y. Zhang, X. Y. D. Ma, J. Ang, Z. Zeng, B. F. Ng, M. P. Wan, S.-C. Wong and X. Lu, Polymer/MOF-derived multilayer fibrous membranes for moisture-wicking and efficient capturing both fine and ultrafine airborne particles, *Sep. Purif. Technol.*, 2020, **235**, 116183.
- 68 X. Dai, X. Li and X. Wang, Morphology controlled porous poly(lactic acid)/zeolitic imidazolate framework-8 fibrous membranes with superior PM2.5 capture capacity, *Chem. Eng. J.*, 2018, **338**, 82–91.
- 69 C. Liu, P.-C. Hsu, H.-W. Lee, M. Ye, G. Zheng, N. Liu, W. Li and Y. Cui, Transparent air filter for high-efficiency PM2.5 capture, *Nat. Commun.*, 2015, **6**, 6205.
- 70 G. Mainelis, Bioaerosol sampling: Classical approaches, advances, and perspectives, *Aerosol Sci. Technol.*, 2020, **54**, 496–519.
- 71 C. W. Haig, W. G. Mackay, J. T. Walker and C. Williams, Bioaerosol sampling: sampling mechanisms, bioefficiency and field studies, *J. Hosp. Infect.*, 2016, **93**, 242–255.
- 72 S. Rengasamy, R. Shaffer, B. Williams and S. Smit, A comparison of facemask and respirator filtration test methods, *J. Occup. Environ. Hyg.*, 2017, **14**, 92–103.
- 73 J. Li, A. Leavey, Y. Wang, C. O'Neil, M. A. Wallace, C.-A. D. Burnham, A. C. M. Boon, H. Babcock and P. Biswas, Comparing the performance of 3 bioaerosol samplers for influenza virus, *J. Aerosol Sci.*, 2018, **115**, 133–145.
- 74 S. Wessels and H. Ingmer, Modes of action of three disinfectant active substances: A review, *Regul. Toxicol. Pharmacol.*, 2013, **67**, 456–467.
- 75 R. Kaur and S. Liu, Antibacterial surface design – Contact kill, *Prog. Surf. Sci.*, 2016, **91**, 136–153.
- 76 R. Krieger, *Hayes' handbook of pesticide toxicology*, Academic press, 2010.
- 77 G. Wickham, An investigation into the relative resistances of common bacterial pathogens to quaternary ammonium cation disinfectants, *Biosci. Horiz.*, 2017, **10**, hzx008.
- 78 E. Koufakis, T. Manouras, S. H. Anastasiadis and M. Vamvakaki, Film Properties and Antimicrobial Efficacy of Quaternized PDMAEMA Brushes: Short vs Long Alkyl Chain Length, *Langmuir*, 2020, **36**, 3482–3493.
- 79 R. Kügler, O. Bouloussa and F. Rondelez, Evidence of a charge-density threshold for optimum efficiency of biocidal cationic surfaces, *Microbiology*, 2005, **151**, 1341–1348.
- 80 M. Mercury, *International programme on chemical safety*, 1990, vol. 118.
- 81 J. Zhou, Z. Hu, F. Zabihi, Z. Chen and M. Zhu, Progress and Perspective of Antiviral Protective Material, *Advanced Fiber Materials*, 2020, **2**, 123–139.

