



Cite this: *RSC Chem. Biol.*, 2021, 2, 1692

Received 24th May 2021,
Accepted 1st October 2021

DOI: 10.1039/d1cb00118c

rsc.li/rsc-chembio

Activation of a G protein-coupled receptor through indirect antibody-mediated tethering of ligands†

Ross W. Cheloha, ^{‡*}^a Fabian A. Fischer, [§]^a Thomas J. Gardella^b and Hidde L. Ploegh ^{*}^a

Antibodies raised against many cell surface proteins, including G protein-coupled receptors, remain important tools for their functional characterization. By linking antibodies to ligands for cell surface proteins, such adducts can be targeted to the surface of a cell type of choice. Site-specific functionalization of full-size antibodies with synthetic moieties remains challenging. Here we present new approaches in which single domain antibodies (known as VHJs or nanobodies) that target either cell surface proteins or conventional antibodies are used to indirectly deliver ligands for GPCRs to their sites of action. The combination of high yield production of nanobodies, facile site-specific functionalization, and compatibility with commercially available mouse and rabbit antibodies should enable wide application of this approach.

Introduction

Antibodies remain the gold standard for the selective detection and targeting of proteins in biological applications. Many proteins can be detected with commercially available antibodies, which have become essential tools in biology. Antibodies are often used to block the action of ligands on cell surface proteins. Antibodies can also deliver bioactive compounds to cells that express the relevant antigen. Antibody-drug conjugates (ADCs) are typically composed of an antibody functionalized with cytotoxic compounds. Upon internalization into endosomal compartments and proteolysis, ADCs release cytotoxic payloads that act inside the cell.¹ Ligands for cell surface receptors can also be linked to antibodies; however, such efforts often suffer from a lack of specificity or difficulties in producing active, stable conjugates in sufficient yield.^{2–6}

The use of single domain antibodies (VHJs or nanobodies) can overcome some of these complications.⁷ Nanobodies are the recombinantly expressed variable regions of camelid heavy

chain only antibodies. They are the smallest antibody fragments that retain the capacity to bind antigen. Because nanobodies do not require pairing with the light chain through disulfide linkage, they can be expressed recombinantly in bacteria in high yield. Sortase-mediated labeling offers a straightforward method for site-specifically labeling recombinant proteins, including nanobodies.⁸ Nanobodies have been applied in a variety of settings, including as imaging agents in immuno-positron emission tomography,⁹ as crystallization chaperones,¹⁰ and as inhibitors or agonists of cell surface receptor signaling.^{11–14} The first nanobody-based therapeutic has now been approved for clinical application.¹⁵

Nanobody conjugates have also been used to deliver bioactive compounds to specific cell types. A nanobody was applied as a conventional ADC to deliver a cytotoxic compound to kill murine lymphoma cells *in vitro* and in mice.¹⁶ In an example of targeting cell surface proteins,¹⁷ a conjugate between a green fluorescent protein (GFP)-specific nanobody and a photo-switchable agonist for the metabolic glutamate receptor enabled light-mediated activation of receptor signaling, but required the use of an engineered receptor-GFP fusion.¹⁴ A variant of glucagon-like peptide-1 (GLP1) was fused to a GLP1-receptor-specific nanobody to provide a conjugate with activity in mice.¹⁸ We showed that the conjugation of weakly active fragments of parathyroid hormone (PTH) to nanobodies that bound the receptor or that recognized epitope tags incorporated into type-1 PTH-receptor (PTHR1) augmented the biological activity and receptor specificity of these otherwise sub-optimal fragments.² This approach was dubbed “conjugation of ligands and antibody for membrane protein”, or CLAMP. One of these CLAMPs induced a physiological response in mice, whereas the corresponding free peptide did not.²

^a Program in Cellular and Molecular Medicine, Boston Children's Hospital, 1 Blackfan Circle, Boston, MA, 02115, USA. E-mail: ross.cheloha@nih.gov, hidde.ploegh@childrens.harvard.edu

^b Massachusetts General Hospital and Harvard Medical School, 50 Blossom Street, Boston, MA, 02114, USA

† Electronic supplementary information (ESI) available. See DOI: [10.1039/d1cb00118c](https://doi.org/10.1039/d1cb00118c)

‡ Current affiliation: National Institute of Health, National Institutes of Diabetes, Digestive and Kidney Disease, Laboratory of Bioorganic Chemistry, Bethesda, MD, 20894, USA.

§ Current affiliation: Kennedy Institute of Rheumatology, University of Oxford, OX3 7FY, Oxford, UK.



These applications relied in large part on the use of target-specific nanobodies. While the pool of nanobodies continues to expand,¹⁹ there are many targets for which appropriately specific nanobodies are not available. Here we describe new approaches that rely on nanobodies for delivery of ligands for cell surface receptors independent of the availability of target-specific nanobodies.

Experimental

General

HEK293 cell lines were cultured in DMEM medium containing 10% (v/v) fetal bovine serum and penicillin/streptomycin. Cell lines were routinely tested for mycoplasma infection. LC/MS was performed in the positive ionization mode. Masses for proteins and conjugates were calculated by analysis of multiply charged ions using the MaxEnt feature on MassLynx software. Protein and conjugate concentrations were calculated using absorbance at 280 nm for VHHS. Peptide concentrations were determined gravimetrically, assuming that the weighed mass consisted of ~50% peptide (w/w). Transfections of HEK293 were performed using Lipofectamine2000 (Invitrogen, 11668019) using manufacturer's instructions. Commercial antibodies used in these studies are listed in Table S1 (ESI[†]).

Plasmids and DNA

HEK293-derived cell lines stably expressing human PTHR1 (GP2.3) and PTHR1_{6E} (G6E19) along with a cAMP-responsive luciferase variant have been previously reported.² HEK293 cells expressing only the cAMP-responsive luciferase (GS22a) were transiently transfected with a plasmid encoding PTHR1 lacking its extracellular domain with or without an N-terminal HA-tag extension. Annotated sequence data for all PTHR1 constructs are found in Fig. S1 (ESI[†]). Sequences for nanobodies targeting human β 2-microglobulin (MHC-I), MHC-II, UBC6E (6E tag), α 5 β 1, mouse Igk, and rabbit IgG have been published previously.²⁰⁻²³

Peptide synthesis

Peptides were prepared using conventional solid-phase synthesis methods with Fmoc-protection of backbone amines as described previously.² Synthesis was performed on Rink-amide linker resin to yield C-terminal amides. Identity and purity of peptides were confirmed by LC/MS. All peptides were of a purity of >85%. Purified products were dissolved in water (10 mM stock concentration) and stored at -20 °C. Purified peptides with C-terminal cysteines were functionalized with DBCO-maleimide (Click Chemistry Tools) as described previously.²

Protein expression, purification, and functionalization

The production and purification of VHHS and sortase A pentamutant was performed as described previously.²⁴ VHHS were labeled using sortase A pentamutant as described previously.²⁵

Flow cytometry

Adherent cells were dissociated from the substrate with trypsin, washed and resuspended in PBS, followed by staining for 1 h on

ice in the presence of the indicated concentrations of VHH probes functionalized with biotin. Cells were pelleted by centrifugation and washed with PBS prior to staining with streptavidin-PE (BioLegend, 405204). Cells were again pelleted by centrifugation, washed, and analyzed by flow cytometry (BD Accuri C6).

Conventional antibodies were also used for staining cells for flow cytometry as described above, with the following exceptions. In one staining method, primary antibodies (IgGs) were incubated with cells at the indicated concentrations in the presence of a 3 fold molar excess of secondary (anti-IgG) nanobodies site-specifically conjugated with biotin. Biotin was detected with streptavidin-PE as described above. In an alternative method, cells were stained with unlabeled primary antibodies and detected following secondary staining, using commercial secondary anti-IgG antibodies conjugated with AlexaFluor647 (ThermoFisher, A-21235). Data were analyzed using FlowJo version 7.6. The median fluorescence intensity (MFI) of stained cells was used to generate VHH binding dose response curves.

VHH-peptide conjugation reactions

VHH-biotin-azide conjugates were mixed with a three-fold molar excess of PTH-DBCO in TBS with 10% (v/v) glycerol. The reaction mixture was shaken at 22 °C until any unreacted VHH-biotin-azide had been completely consumed. The desired conjugate was purified from free PTH-DBCO using a PD-10 size exclusion column (Cytiva, 17085101). A summary of the characterization of these conjugates by LC/MS is shown in Table S2 (ESI[†]).

Measurement of cAMP response

Assays were performed using a luminescence-based readout with cells expressing cAMP Glosensor as previously described²⁶ with exceptions. A modified protocol was followed for assays that include commercial IgGs. IgG concentrations were calculated based on protein concentrations listed on manufacturer data sheets and assuming an average IgG molecular weight of 150 000 g mol⁻¹. VHH-PTH₁₋₁₁ conjugates were premixed with indicated IgGs at a 3:1 molar ratio and incubated for at least 10 minutes at room temperature prior to addition to cells expressing PTHR1 or variants.

Intercellular receptor activation assays

Murine B cell lymphoma A20 cells (ATCC TIB-208) were incubated with PTH₁₋₃₄ or VHH-PTH₁₋₃₄ conjugates in PBS containing 1% (w/v) bovine serum albumin (BSA) at the indicated concentrations for 1 h on ice. These A20 cells were then washed with additional PBS with BSA and pelleted by centrifugation through four wash cycles. The loaded and washed A20 cells were then distributed (50 000 cells per well) to a 96 well plate containing HEK293 cells expressing PTHR1 and cAMP Glosensor as described above. Luminescence readouts at time points prior to 10 minutes after addition of A20 cells were unreliable, so luminescence was measured between 12–16 minutes after addition of the A20 cells.



Data calculations

Data were processed using Microsoft Excel and GraphPad Prism 6. Data from cAMP dose-response assays were analyzed using a sigmoidal dose-response model with variable slope. Data sets were statistically compared by using one-way ANOVA with multiple comparisons. Statistically significant differences between data sets were inferred at $p < 0.05$.

Results and discussion

Nanobody–ligand conjugates bind surface markers and are capable of indirectly activating PTHR1

Several approaches for tethering ligands for cell surface receptors at or near their site of action are shown in Fig. 1. Previous work from our lab focused on activation of the type-1 parathyroid hormone receptor (PTHR1), which is activated under physiological conditions by the peptide parathyroid hormone (PTH).²⁷ Parathyroid hormone/parathyroid hormone-related protein receptor (PTH/PTHrP type 1 receptor; commonly known as PTHR1) is a family B G-protein-coupled receptor (GPCR) that regulates skeletal development, bone turnover and mineral ion homeostasis.²⁸ Conjugation of weakly active peptide agonists for PTHR1 to VHHS that bind to the same receptor (Fig. 1a) augments the biological activity of the ligand and avoids off-target activation *in vitro* and *in vivo*.²

This observation prompted us to ask whether other mechanisms for tethering ligands for PTHR1 near their site of action through conjugation with nanobodies would also enable activation of PTHR1 (Fig. 1). This scheme depends on the spatial disposition of PTHR1 relative to the target recognized by the relevant nanobody or antibody, as it requires an interaction of the ligand-modified nanobody with a surface molecule other than PTHR1 (Fig. 1c and d).

We used a cell-based system in which human PTHR1 or its variants are stably expressed in HEK293 cells as a test bed for alternative tethering strategies. In the first iteration, VHHS that target cell surface proteins naturally expressed on HEK293 cells were prepared and evaluated (Fig. 1b). We used VHHS that target human β 2-microglobulin, the light chain of cell surface Class I major histocompatibility complex products (VHH_{MHC-I}, previously named Nb30),²⁰ the integrin $\alpha 5\beta 1$ (VHH _{$\alpha 5\beta 1$}), and a short peptide epitope taken from the intracellular protein UBC6E (VHH_{6E}).²² These VHHS were labeled at their C-terminus by means of sortagging with a peptide functionalized with biotin for detection and with an azide for conjugation to appropriately functionalized peptides of choice (Fig. 2a).² Conjugates comprised of VHHS, biotin, and PTH₁₋₁₁ were used to label HEK293 cells, followed by detection with a streptavidin–phycoerythrin conjugate (Fig. 2b–d). The HEK293 cell line (PTHR1-6E-HEK) expresses PTHR1 with the 6E tag inserted into a disordered

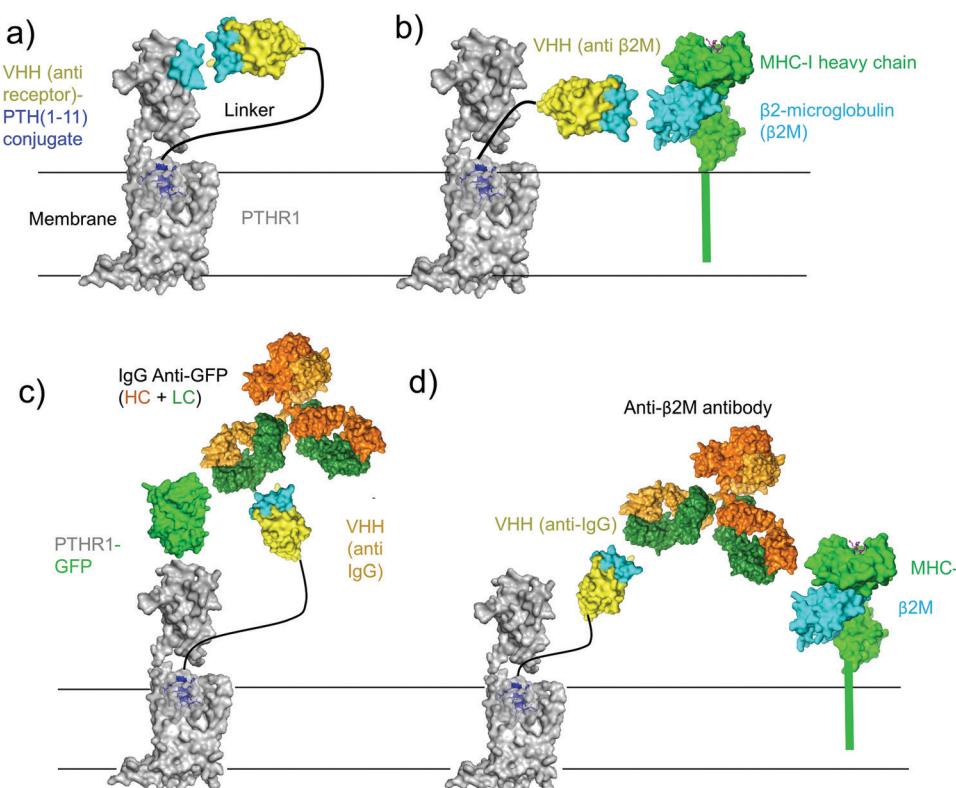


Fig. 1 Schematic of methods for receptor activation using ligand-nanobody fusions with PTHR1 as an example. (a) Direct tethering of ligand to its target with a VHH as previously described.² (b) Indirect targeting using a VHH that binds another protein (MHC-I) on the cell surface. (c) Antibody-mediated direct tethering using a receptor-specific (or fusion protein-specific) full-size antibody (IgG) and a VHH that binds IgG. (d) Antibody-mediated indirect tethering using a full-size antibody that binds another protein (MHC-I) on the cell surface and a VHH that binds IgG.



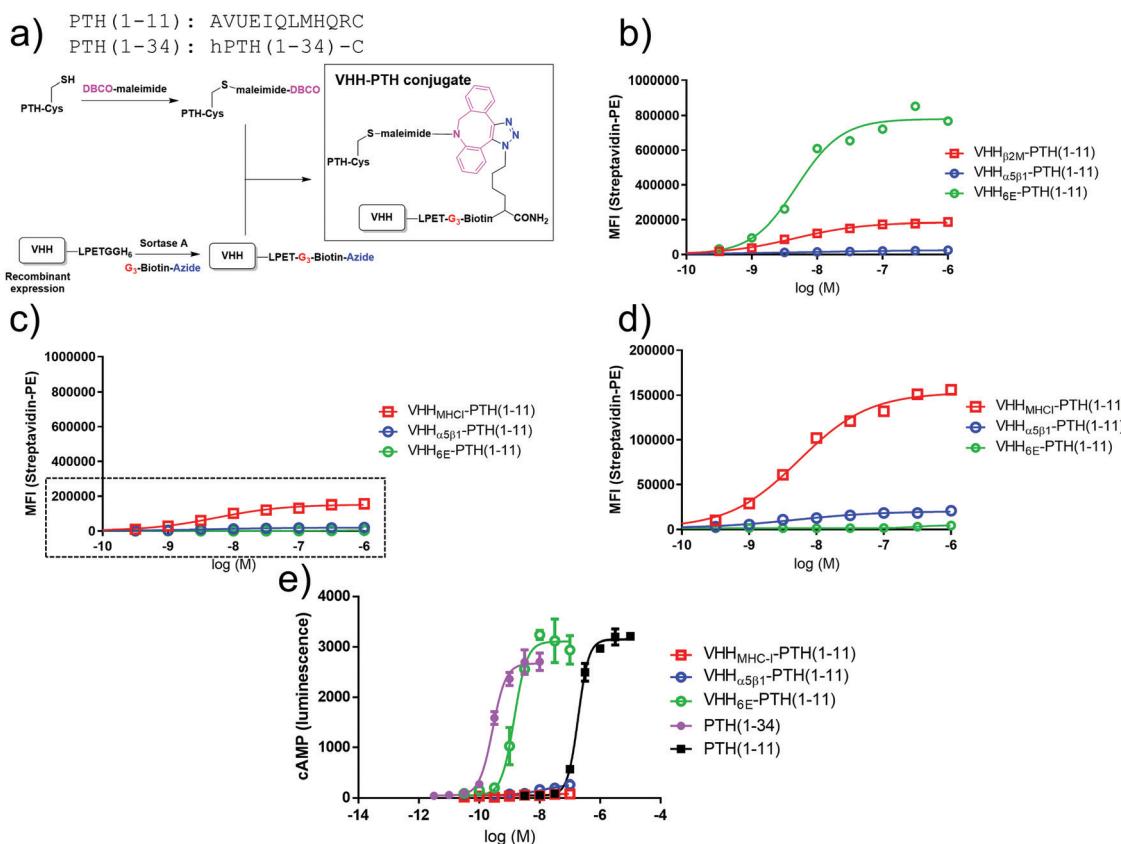


Fig. 2 Synthesis and evaluation of PTH–nanobody conjugates. (a) Synthetic scheme for production of PTH–nanobody conjugates. PTH-peptide synthesis and functionalization, VHH production and functionalization, and conjugation was performed as described in methods. (b) Representative (one of three experiments) dose–response curve for binding of VHH–biotin–PTH conjugates to PTHR1-6E-HEK cells. The plots were produced by fitting a sigmoidal dose–response curve. Staining, detection, and quantitation were performed as described in methods. Representative data from one of three independent experiments is shown, with compiled data shown in Table 1. (c) Binding of VHH–biotin–PTH conjugates to neg-HEK cells with a zoomed inset (boxed region) shown in panel d. Representative data from one of three independent experiments is shown with compiled data shown in Table 1. (e) Representative dose–response assay for induction of cAMP responses in PTHR1-6E-HEK cells. Error bars correspond to standard deviation from replicate conditions in a single experiment. Plots were generated by fitting a sigmoidal dose–response curve. Representative data from one of three independent experiments is shown with compiled data shown in Table 1.

portion of the receptor extracellular domain² (Fig. 2b), whereas HEK293 serves as a negative control (neg-HEK) (Fig. 2c and d). VHH_{MHC-I} and VHH_{α5β1} conjugates labeled PTHR1-6E-HEK and neg-HEK cells at low concentrations, indicating tight binding. VHH_{MHC-I} labeling provided a higher maximal intensity of staining (approximately 10 fold) than VHH_{α5β1} (Table 1).²⁹ Staining of PTHR1-6E-HEK cells with the VHH_{6E} conjugate provided a stronger signal than staining with VHH_{MHC-I} (Table 1), consistent with a high level of expression of PTHR1-6E on PTHR1-6E-HEK cells. We then evaluated whether the VHH–PTH conjugates shown to bind to PTHR1-6E-HEK cells stimulated receptor activation and the production of cyclic adenosine monophosphate (cAMP), a second messenger produced upon PTHR1 activation. Consistent with previous results, VHH_{6E}-PTH₁₋₁₁ potently stimulated cAMP responses on PTHR1-6E-HEK cells (Fig. 2e and Table 1).² VHH_{MHC-I}-PTH₁₋₁₁ was essentially inactive in stimulating cAMP responses, whereas VHH_{α5β1}-PTH₁₋₁₁ induced a weak but detectable response. This observation was unexpected given that staining of HEK cell lines was stronger with VHH_{MHC-I} than VHH_{α5β1}. The origin of this difference is unknown, but it may

relate to the larger size and expanded flexibility of the extracellular portions of α5β1 relative to β2-microglobulin as a more compact subunit of MHC-I. Another possibility is that PTHR1 may localize to membrane domains closer to α5β1 relative to the β2-microglobulin-MHC-I complex. In this context, the use of a longer flexible linker between the receptor agonist and nanobody may improve activation efficacy. A conjugate consisting of a nanobody and ligand that both target the same receptor was relatively insensitive to inclusion of a short polyethylene glycol linker.² Collectively, VHH–PTH conjugates that directly target other proteins on the cell surface (MHC-I, α5β1) are only weak agonists of PTHR1.

Combination of primary antibodies with VHH_{mIg}-PTH₁₋₁₁ strongly increases PTHR1 activation

We also tested whether targeting a receptor of interest using a conventional monoclonal antibody (immunoglobulin, Ig) and a nanobody–PTH conjugate in which the nanobody binds to Ig could serve to activate the receptor (Fig. 1c). We used a nanobody (previously²³ named TP1170, named here VHH_{mIg}) that

Table 1 Summary of VHH-PTH binding and receptor activation. Binding and signaling assays were performed as described in methods. Values listed are the mean and standard deviation from three independent experiments. EC₅₀ values result from fitting a four-parameter sigmoidal dose-response model to the data. Max. stain for binding assays is provided by the top plateau value from the dose-response models. These values are normalized to the top plateau value recorded for VHH_{MHC-I} binding in each experiment. The maximal cAMP signal is computed by normalizing the response recorded at the highest concentration tested for that compound in each assay to the background in that same assay. This normalization method was used because some compounds were too weak to generate reliable dose-response curves

Binding EC ₅₀		Max. stain	
	nM	SD	Intensity (relative to MHC-I)
PTHR1-6E-HEK			SD
VHH _{6E} -PTH ₁₋₁₁	5.1	0.3	5.6
VHH _{MHC-I} -PTH ₁₋₁₁	3.2	1.2	1
VHH _{a5b1} -PTH ₁₋₁₁	4.6	3.3	0.11
Signaling cAMP EC ₅₀		Max. cAMP signal	
PTHR1-6E-HEK	nM	SD	Normalized (fold over no ligand)
PTH ₁₋₃₄	0.18	0.090	120
PTH ₁₋₁₁	132	51	150
VHH _{6E} -PTH ₁₋₁₁	0.71	0.64	104
VHH _{MHC-I} -PTH ₁₋₁₁	> 100 nM		3.8
VHH _{a5b1} -PTH ₁₋₁₁	> 100 nM		33
Binding EC ₅₀		Max. stain	
Neg-HEK	nM	SD	Intensity (relative to MHC-I)
VHH _{6E} -PTH ₁₋₁₁	ND ^a	ND	0.020
VHH _{MHC-I} -PTH ₁₋₁₁	4.3	1.7	1.0
VHH _{a5b1} -PTH ₁₋₁₁	3.0	2.8	0.10

^a The maximal staining for VHH_{6E}-PTH₁₋₁₁ on HEK-neg cells was very weak, so binding EC₅₀ values were not determined (ND).

binds to the kappa light chain found in 95% of mouse IgGs.²³ We prepared VHH_{mIg}-PTH₁₋₁₁ and evaluated its agonist activity on HEK293 cells that stably express PTHR1 fused to GFP³⁰ in the presence or absence of a mouse monoclonal IgG antibody specific for GFP (α -GFP). As a control we used non-specific polyclonal mouse IgG (isotype) in place of α -GFP. We mixed VHH_{mIg}-PTH₁₋₁₁ at a 3:1 molar ratio with mouse IgGs prior to addition to HEK293 cells and then recorded cAMP responses at VHH_{mIg}-PTH₁₋₁₁ doses of 100 nM and 10 nM (Fig. 3a and b). The combination of VHH_{mIg}-PTH₁₋₁₁ and α -GFP led to a robust cAMP response at 100 nM and a weak response at 10 nM, whereas the combination of VHH_{mIg}-PTH₁₋₁₁ and isotype was inactive. The combination of VHH_{mIg}-PTH₁₋₁₁ and α -GFP was more potent than PTH₁₋₁₁ alone. In a separate experiment, we used versions of PTHR1 in which the extracellular portion of the receptor was absent or replaced with the HA-epitope tag (Fig. S2, ESI†).³¹ The combination of VHH_{mIg}-PTH₁₋₁₁ and α -HA mouse monoclonal IgG lead to a cAMP response that far exceeded the response seen with PTH₁₋₁₁ alone, whereas the combination of VHH_{mIg}-PTH₁₋₁₁ and isotype mouse IgG was inactive. These data show that indirect targeting of PTHR1 using an Ig-specific nanobody-PTH conjugate and a bridging

IgG (Fig. 1c) can augment the biological activity of a weakly active ligand.

The ability to use antibodies to target proteins on the cell surface other than the receptor of interest (Fig. 1d) provides opportunities for the delivery of ligands to cell types of choice, based on the presence of an IgG-recognized surface marker. As a proof of concept, we deployed commercial antibodies that target β 2-microglobulin (α - β 2M) as a component of cell surface MHC-I, a ubiquitously expressed type I membrane protein. This also allowed a direct comparison with the use of a nanobody that targets β 2-microglobulin (Fig. 1a and 2). Because we were targeting PTHR1 indirectly, we used a HEK293 cell line that stably expresses wild-type PTHR1. The combination of VHH_{mIg}-PTH₁₋₁₁ and mouse α - β 2M induces a robust cAMP response at a concentrations of 100 nM whereas the combination of VHH_{mIg}-PTH₁₋₁₁ and a control antibody ("isotype") was inactive (Fig. 3c and d). The use of a control nanobody-PTH conjugate that targets the 6E epitope tag (VHH_{6E}-PTH₁₋₁₁) in combination with α - β 2M was also inactive. Neither the binding of IgG to PTHR1 nor the presence of an irrelevant VHH-PTH₁₋₁₁ conjugate leads to activation. The combination of VHH_{mIg}-PTH₁₋₁₁ and α - β 2M was more potent than PTH₁₋₁₁ alone. Indirect targeting (as in Fig. 1d) can therefore substantially increase the biological activity of a weakly active ligand. This stands in sharp contrast to parallel efforts with conjugates that comprise nanobodies that target β 2M, which failed to activate PTHR1 (Fig. 1b and 2). The cause of this divergence is unclear but may be related to the additional flexibility and/or distance provided by the bridging full-size antibody.

Any attempt to apply VHH_{mIg} conjugates in mice would likely be stymied by the high concentration of mIgs found in the mouse blood stream. To circumvent this problem, we turned to a nanobody (previously²³ named TP897, named here VHH_{rig}) that binds to rabbit IgGs, but not mouse. We prepared a VHH_{rig}-PTH₁₋₁₁ conjugate as described above and evaluated its performance in PTHR1 activation assays. VHH_{rig}-PTH₁₋₁₁ activated PTHR1 signaling when combined with rabbit α - β 2M but not mouse α - β 2M (Fig. 3e and f). This finding offers a path towards using this approach *in vivo* in mice.

These findings raised the question whether targeting other cell surface proteins for antibody tethering would likewise facilitate receptor activation. We therefore expanded the approach described above by inclusion of monoclonal antibodies that target the cell surface markers CD63 and CD81, both widely expressed. CD63 and CD81 are members of the tetraspanin family of proteins, naturally expressed on HEK293 cells and on most other cell types, at modest levels.^{32,33} We confirmed by flow cytometry that these monoclonal antibodies bound to HEK293 cells (Fig. S3, ESI†). The α -CD63 and α -CD81 antibodies labeled HEK293 cells following secondary staining with either α -mouse Ig-alexafluor 647 or with VHH_{mIg}-biotin and streptavidin-phycoerythrin (streptavidin-PE, Fig. S3, ESI†). However, neither of the α -CD63 and α -CD81 antibodies stained HEK293 cells as strongly as the anti β 2M antibody, consistent with the high level of β 2M found on most cells (Fig. S3, ESI†).²⁹ We then tested whether the α -CD63 and α -CD81 antibodies

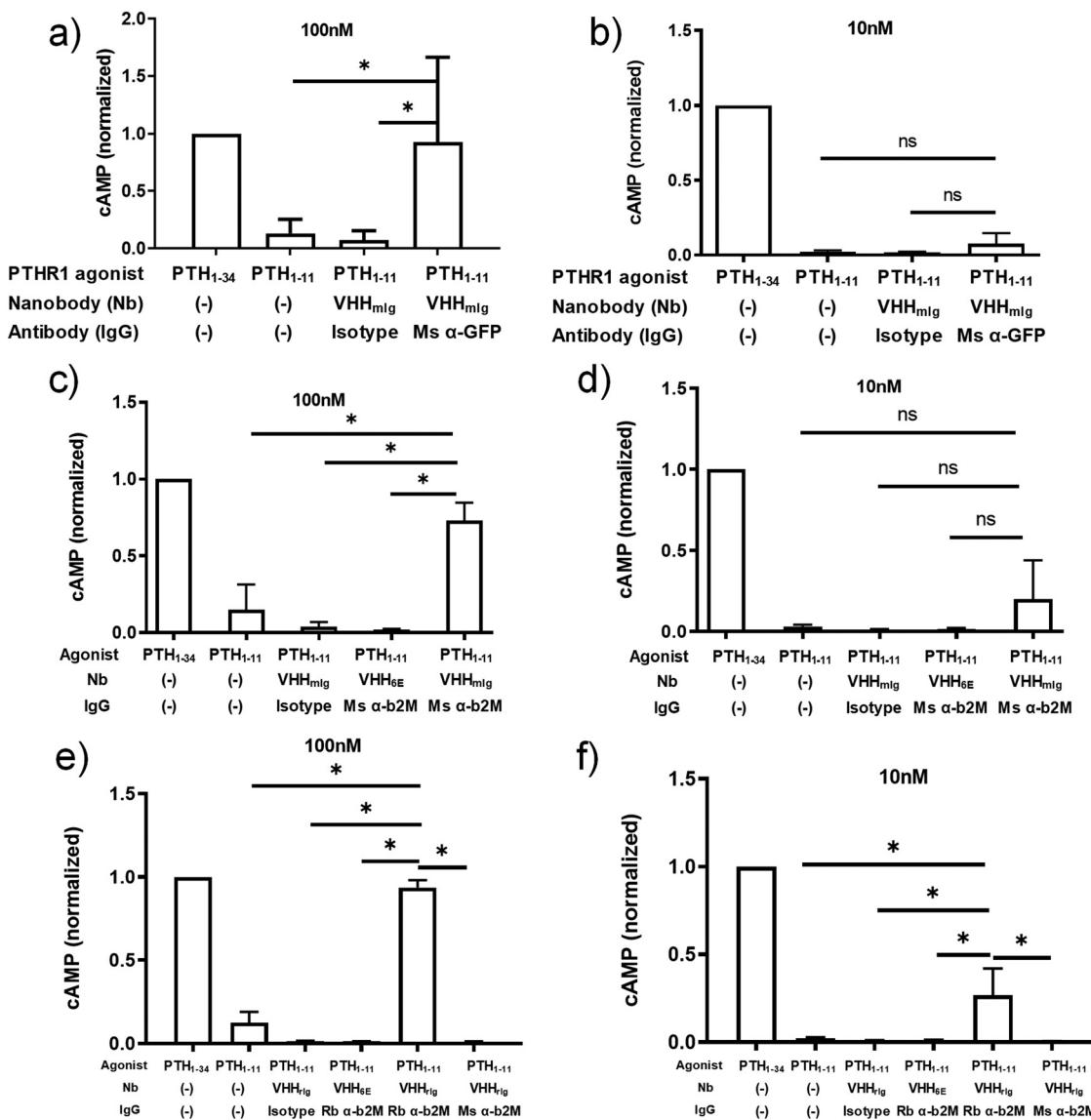


Fig. 3 Assessment of tethered VHH-PTH conjugates in activating PTHR1 signaling. PTH peptides or conjugates prepared as described in Fig. 2a were either mixed with commercially available full-size antibodies or added directly to HEK293 cells that express PTHR1 or its variant as described in methods. Data sets were compared for statistically significant differences using one-way ANOVA with multiple comparisons; * $p < 0.05$. (a and b) HEK293 cells expressing a GFP-PTHR1 fusion protein (see Fig. S1, ESI†) were treated with PTH agonist peptides (columns 1 + 2) or VHH-PTH conjugates mixed with commercial antibodies (columns 3 + 4). PTH agonist peptides and VHH-PTH conjugates were applied at a dose of 100 nM (panel a) or 10 nM (panel b). VHH-PTH conjugates were used a 3 fold molar excess over commercial antibodies. 'Isotype' refers to a polyclonal mouse IgG preparation. The magnitude of the cAMP responses is normalized to that of PTH₁₋₃₄. (c and d) Experiments were performed as in panels a and b, except that HEK293 cells expressed WT hPTHR1. Bars and error bars represent mean \pm SD from 6 independent experiments. (e and f) HEK293 cells expressing WT hPTHR1 were treated with PTH agonist peptides (columns 1 + 2) or VHH-PTH conjugates mixed with commercial antibodies (columns 3–6). "Rb" indicates a monoclonal antibody derived from rabbit. "Ms" indicates monoclonal antibody derived from mouse. Isotype refers to a polyclonal IgG antibody preparation derived from WT mouse. Bars and error bars represent mean \pm SD from 3 independent experiments.

could provide tethering to facilitate activation of PTHR1 signaling (Fig. 4). Whereas α -CD81 facilitated activation comparable to α - β 2M at both concentrations tested, α -CD63 failed to promote activation above background levels. The source of this difference between the α -CD81 and α -CD63 antibodies in these assays is not clear, but it may be related to differences in target expression levels or differences in membrane protein localization.³³ These findings open the door to identifying other cell surface markers, potentially expressed specifically on cell types of interest,

that could allow cell-type specific activation of widely expressed receptors.

Cell-bound nanobody-PTH conjugates can activate adjacent cells in co-culture experiments.

Finally, we tested whether antibody-based ligand tethering could bridge the space between distinct cells (Fig. 5a). In this approach the antibody targeting portion of the CLAMP binds to one cell type (targeting cell) and the ligand targets a receptor

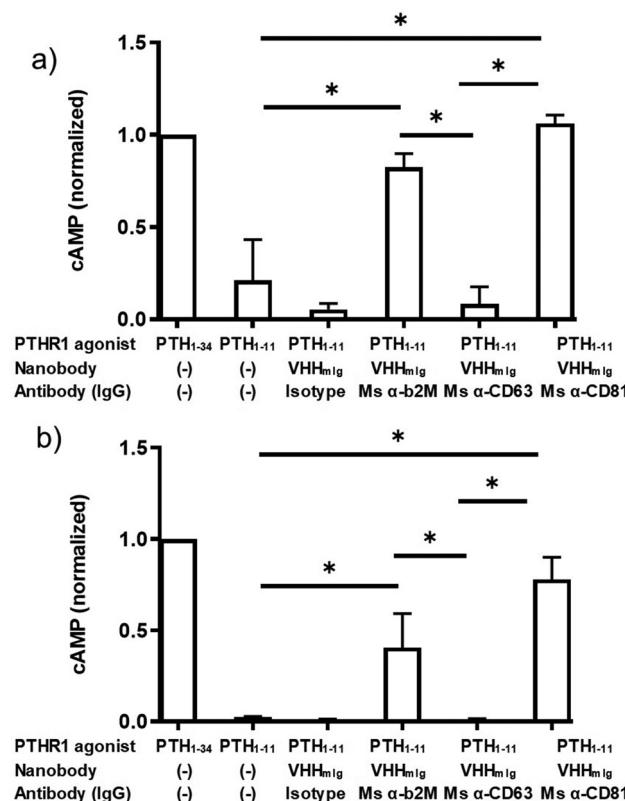


Fig. 4 Assessment of indirect activation efficiency through targeting varied surface proteins. PTH peptides or conjugates prepared as described in Fig. 2a were either mixed with commercially available antibodies or added directly to HEK293 cells expressing PTHR1 or its variant as described in methods. (a and b) HEK293 cells that express PTHR1 were treated with PTH agonist peptides (columns 1 + 2) or VHH-PTH conjugates mixed with commercial antibodies (columns 3–6). PTH agonist peptides and VHH-PTH conjugates were applied at a dose of 100 nM (panel a) or 10 nM (panel b). VHH-PTH conjugates were used at a 3 fold molar excess over commercial antibodies. ‘Isotype’ refers to a polyclonal mouse IgG preparation. The magnitude of the cAMP responses is normalized to that of PTH₁₋₃₄. Bars and error bars represent mean \pm SD from 3 independent experiments that are distinct from those shown in Fig. 3. Data sets were compared for statistically significant differences using one-way ANOVA with multiple comparisons; * p < 0.05.

expressed on another cell type (receptor cell). We combined HEK293 cells that express PTHR1 (receptor cell) and a murine B cell lymphoma line, A20, which expresses high levels of class II major histocompatibility complex (MHC-II, targeting cell³³). Of note, A20 are cells in suspension in contrast to HEK293 cells, which grow adherently. We used a well-characterized VHH that binds murine MHC-II (VHH_{MHC-II}, previously¹⁷ called VHH7). We predicted that intercellular tethering would prove more challenging than intracellular tethering, so we used a larger, more potent PTHR1 peptide agonist (PTH₁₋₃₄), instead of PTH₁₋₁₁, in the CLAMPs that we tested.

PTH₁₋₃₄ can be conjugated to a nanobody with only a minor impact on PTHR1 agonist activity.² We confirmed this: CLAMPs consisting of PTH₁₋₃₄ were conjugated to VHHs that target either GFP³⁴ (VHH_{GFP}-PTH₁₋₃₄) or MHC-II (VHH_{MHC-II}-PTH₁₋₃₄) using the chemistry described in Fig. 2a. These CLAMPs

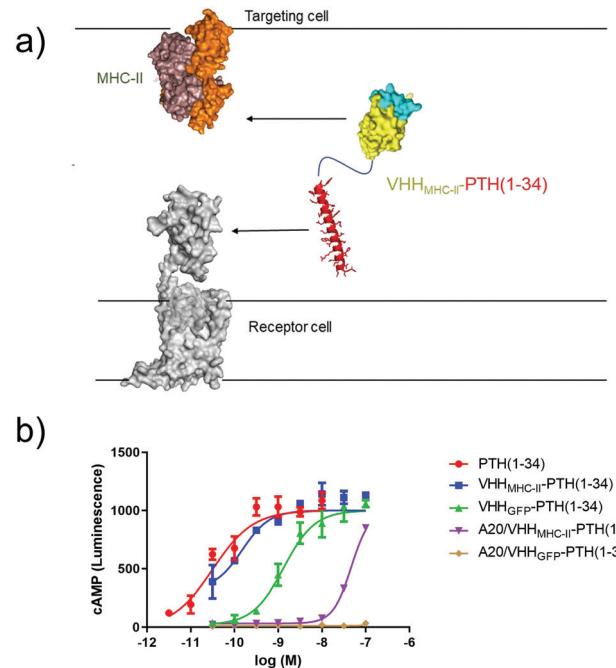


Fig. 5 Intercellular activation of GPCR signaling. (a) Schematic of intercellular antibody tethering. (b) Representative dose–response assay for induction of cAMP responses in PTHR1-6E-HEK cells. Error bars correspond to standard deviation from replicate conditions in a single experiment. Data were fitted to a sigmoidal dose–response model with variable slope. Representative data from one of three independent experiments is shown.

performed similarly to PTH₁₋₃₄ itself in cAMP stimulation assays on HEK293 cells (receptor cells) that express human PTHR1 (Fig. 5). This assay was also run using A20 cells (targeting cells) treated with CLAMPs and then washed to remove unbound ligand. Application of targeting cells pre-treated with VHH_{MHC-II}-PTH₁₋₃₄ but not VHH_{GFP}-PTH₁₋₃₄ stimulated robust cAMP responses. These responses were observed when loading A20 cells with CLAMP concentrations of >10 nM. VHH_{MHC-II} binds to MHC-II with half-maximal staining at concentrations of approximately 50 nM.³⁵ This similarity in concentrations suggests a correlation between the amount of CLAMP loaded on the target cell and the extent of receptor activation on the receptor cell. Whether CLAMPs can simultaneously bind to both a targeting cell and receptor cell, or if receptor activation first requires dissociation from the targeting cell, is not clear from this study, although past work with immunocytokines suggests that such dissociation is not required.³ This type of correlation may provide guidelines for future efforts to use intercellular antibody tethering.

Conclusions

We have demonstrated several approaches for activation of GPCR signaling with CLAMPs that do not rely on direct targeting of the receptor. The ability to use conventional monoclonal antibodies as tethering agents should allow expansion of the CLAMP methodology to a variety of targets. This approach is of practical value, as it avoids the need for target-specific nanobodies.



Efforts to identify nanobodies that bind to the exposed extracellular face of GPCRs have been successful in some cases^{11,36–40} but for many cell surface targets nanobodies of appropriate specificity do not yet exist. In contrast, there is a wide array of commercially available monoclonal antibodies that recognize cell surface proteins in mouse and man. Seen from this perspective, the ability to use tethering by commercially available antibodies to activate a receptor of interest only on those cell types that express the antibody target is a major asset. This could offer a means to engineer “AND” logic gates⁴¹ that target receptor signaling only in a subset of cells. The availability of a nanobody that selectively targets rabbit IgG, but not mouse IgGs, provides a path to extend this approach *in vivo* in mice. Intercellular tethering could further expand applications of this approach to interrogate cell-to-cell signaling within a given organ or biological compartment.

Author contributions

Project conceptualization (R. W. C., F. A. F., H. L. P.), research resources (R. W. C., T. J. G., H. L. P.), funding acquisition (R. W. C., T. J. G., H. L. P.), laboratory experimentation (R. W. C., F. A. F., T. J. G.), data visualization (R. W. C., F. A. F.), methodology development (R. W. C., F. A. F.), and manuscript writing (R. W. C., F. A. F., T. J. G., H. L. P.).

Conflicts of interest

R. W. C., T. J. G., and H. L. P. have filed a patent on the use of nanobodies to target GPCRs for signaling (US application number 16810783).

Acknowledgements

Funding was provided by the National Institutes of Health grant numbers P01-DK011794 (T. J. G.), 1DP1AI150593 (H. L. P.) and R01-AI087879 (H. L. P.). R. W. C. was supported in part by funding from the Cancer Research Institute Irvington Postdoctoral Fellowship. We acknowledge Thomas Dean at Massachusetts General Hospital for technical assistance with cell bioassays.

References

- 1 A. Beck, L. Goetsch, C. Dumontet and N. Corvaia, *Nat. Rev. Drug Discovery*, 2017, **16**, 315–337.
- 2 R. W. Cheloha, F. A. Fischer, A. W. Woodham, E. Daley, N. Suminski, T. J. Gardella and H. L. Ploegh, *Nat. Commun.*, 2020, **11**, 2087.
- 3 A. Tzeng, B. H. Kwan, C. F. Opel, T. Navaratna and K. D. Wittrup, *Proc. Natl. Acad. Sci. U. S. A.*, 2015, **112**, 3320–3325.
- 4 L. Sweeny, Y. E. Hartman, K. R. Zinn, J. R. Prudent, D. J. Marshall, M. S. Shekhani and E. L. Rosenthal, *Oral Oncol.*, 2013, **49**, 991–997.
- 5 D. J. Marshall, S. S. Harried, J. L. Murphy, C. A. Hall, M. S. Shekhani, C. Pain, C. A. Lyons, A. Chillemi, F. Malavasi, H. L. Pearce, J. S. Thorson and J. R. Prudent, *Mol. Ther.*, 2016, **24**, 1760–1770.
- 6 A. C. Cheng, E. M. Doherty, S. Johnstone, E. F. DiMauro, J. Dao, A. Luthra, J. Ye, J. Tang, T. Nixey, X. Min, P. Tagari, L. P. Miranda and Z. Wang, *Sci. Rep.*, 2018, **8**, 7570.
- 7 R. W. Cheloha, T. J. Harmand, C. Wijne, T. U. Schwartz and H. L. Ploegh, *J. Biol. Chem.*, 2020, **295**, 15307–15327.
- 8 N. Pishesha, J. R. Ingram and H. L. Ploegh, *Annu. Rev. Cell Dev. Biol.*, 2018, **34**, 163–188.
- 9 T. J. Harmand, A. Islam, N. Pishesha and H. L. Ploegh, *RSC Chem. Biol.*, 2021, **2**, 685.
- 10 E. Pardon, T. Laeremans, S. Triest, S. G. F. Rasmussen, A. Wohlköning, A. Ruf, S. Muyldermans, W. G. J. Hol, B. K. Kobilka and J. Steyaert, *Nat. Protoc.*, 2014, **9**, 674–693.
- 11 R. Heukers, T. W. M. De Groot and M. J. Smit, *Curr. Opin. Cell Biol.*, 2019, **57**, 115–122.
- 12 Y. Ma, Y. Ding, X. Song, X. Ma, X. Li, N. Zhang, Y. Song, Y. Sun, Y. Shen, W. Zhong, L. A. Hu, Y. Ma and M.-Y. Zhang, *Sci. Adv.*, 2020, **6**, eaax7379.
- 13 C. McMahon, D. P. Staus, L. M. Wingler, J. Wang, M. A. Skiba, M. Elgeti, W. L. Hubbell, H. A. Rockman, A. C. Kruse and R. J. Lefkowitz, *Proc. Natl. Acad. Sci. U. S. A.*, 2020, **117**, 20284–20291.
- 14 H. Ren, J. Li, N. Zhang, L. A. Hu, Y. Ma, P. Tagari, J. Xu and M.-Y. Zhang, *Commun. Biol.*, 2020, **3**, 146.
- 15 C. Morrison, *Nat. Rev. Drug Discovery*, 2019, **18**, 485–487.
- 16 T. Fang, J. N. Duarte, J. Ling, Z. Li, J. S. Guzman and H. L. Ploegh, *Angew. Chem., Int. Ed.*, 2016, **55**, 2416–2420.
- 17 T. Fang, C. H. M. J. Van Elssen, J. N. Duarte, J. S. Guzman, J. S. Chahal, J. Ling and H. L. Ploegh, *Chem. Sci.*, 2017, **8**, 5591–5597.
- 18 H. Pan, Y. Su, Y. Xie, W. Wang, W. Qiu, W. Chen, W. Lu, Z. Lu, W. Wang and A. Shang, *Artif. Cells, Nanomed., Biotechnol.*, 2020, **48**, 854–866.
- 19 E. E. Wilton, M. P. Opyr, S. Kailasam, R. F. Kothe and H.-J. Wieden, *ACS Synth. Biol.*, 2018, **7**, 2480–2484.
- 20 K. Domanska, S. Vanderhaegen, V. Srinivasan, E. Pardon, F. Dupeux, J. A. Marquez, S. Giorgetti, M. Stoppini, L. Wyns, V. Bellotti and J. Steyaert, *Proc. Natl. Acad. Sci. U. S. A.*, 2011, **108**, 1314–1319.
- 21 M. Rashidian, E. J. Keliher, A. M. Bilate, J. N. Duarte, G. R. Wojtkiewicz, J. T. Jacobsen, J. Cagnolini, L. K. Swee, G. D. Victora, R. Weissleder and H. L. Ploegh, *Proc. Natl. Acad. Sci. U. S. A.*, 2015, **112**, 6146–6151.
- 22 J. Ling, R. W. Cheloha, N. McCaul, Z.-Y. J. Sun, G. Wagner and H. L. Ploegh, *Mol. Immunol.*, 2019, **114**, 513–523.
- 23 T. Pleiner, M. Bates and D. Görlich, *J. Cell Biol.*, 2018, **217**, 1143–1154.
- 24 R. W. Cheloha, Z. Li, D. Bousbaine, A. W. Woodham, P. Perrin, J. Volarić and H. L. Ploegh, *ACS Chem. Biol.*, 2019, **14**, 1836–1844.
- 25 J. N. Duarte, J. J. Cagnolini, L. K. Swee, A. M. Bilate, J. Bader, J. R. Ingram, A. Rashidfarrokhi, T. Fang, A. Schiepers, L. Hanke and H. L. Ploegh, *J. Immunol.*, 2016, **197**, 4838–4847.
- 26 R. W. Cheloha, A. Maeda, T. Dean, T. J. Gardella and S. H. Gellman, *Nat. Biotechnol.*, 2014, **32**, 653–655.



27 R. W. Cheloha, S. H. Gellman, J.-P. Vilardaga and T. J. Gardella, *Nat. Rev. Endocrinol.*, 2015, **11**, 712–724.

28 T. J. Gardella and J.-P. Vilardaga, *Pharmacol. Rev.*, 2015, **67**, 310–337.

29 T. Geiger, A. Wehner, C. Schaab, J. Cox and M. Mann, *Mol. Cell. Proteomics*, 2012, **11**, M111.014050.

30 M. J. Mahon, *Adv. Biosci. Biotechnol.*, 2011, **2**, 132–137.

31 M. D. Luck, P. H. Carter and T. J. Gardella, *Mol. Endocrinol.*, 1999, **13**, 670–680.

32 M. D. Kalemera, J. Cappella-Pujol, A. Chumbe, A. Underwood, R. A. Bull, J. Schinkel, K. Sliepen and J. Grove, Optimised cell systems for the investigation of hepatitis C virus E1E2 glycoproteins, *Microbiology*, 2020, **102**(1).

33 F. Fordjour, S. Owiredu, H. Muendlein, J. Plange, J. Morrell, J. Han and S. Gould, *Matters*, 2016, DOI: 10.19185/matters.201604000004.

34 A. Kirchhofer, J. Helma, K. Schmidthals, C. Frauer, S. Cui, A. Karcher, M. Pellis, S. Muylldermans, C. S. Casas-Delucchi, M. C. Cardoso, H. Leonhardt, K.-P. Hopfner and U. Rothbauer, *Nat. Struct. Mol. Biol.*, 2010, **17**, 133–138.

35 M. Rashidian, E. Keliher, M. Dougan, P. K. Juras, M. Cavallari, G. R. Wojtkiewicz, J. Jacobsen, J. G. Edens, J. M. G. Tas, G. Victora, R. Weissleder and H. Ploegh, *ACS Cent. Sci.*, 2015, **1**, 142–147.

36 D. Maussang, A. Mujić-Delić, F. J. Descamps, C. Stortelers, P. Vanlandschoot, M. Stigter-van Walsum, H. F. Vischer, M. van Roy, M. Vosjan, M. Gonzalez-Pajuelo, G. A. M. S. van Dongen, P. Merchiers, P. van Rompaey and M. J. Smit, *J. Biol. Chem.*, 2013, **288**, 29562–29572.

37 S. Jähnichen, C. Blanchetot, D. Maussang, M. Gonzalez-Pajuelo, K. Y. Chow, L. Bosch, S. De Vrieze, B. Serruys, H. Ulrichs, W. Vandervelde, M. Saunders, H. J. De Haard, D. Schols, R. Leurs, P. Vanlandschoot, T. Verrips and M. J. Smit, *Proc. Natl. Acad. Sci. U. S. A.*, 2010, **107**, 20565–20570.

38 X. Peyrassol, T. Laeremans, V. Lahura, M. Debulpaep, H. El Hassan, J. Steyaert, M. Parmentier and I. Langer, *Front. Endocrinol.*, 2018, **9**, 153.

39 P. Scholler, D. Nevoltris, D. de Bundel, S. Bossi, D. Moreno-Delgado, X. Rovira, T. C. Møller, D. El Moustaine, M. Mathieu, E. Blanc, H. McLean, E. Dupuis, G. Mathis, E. Trinquet, H. Daniel, E. Valjent, D. Baty, P. Chames, P. Rondard and J.-P. Pin, *Nat. Commun.*, 2017, **8**, 1967.

40 C. Hong, N. J. Byrne, B. Zamlynny, S. Tummala, L. Xiao, J. M. Shipman, A. T. Partridge, C. Minnick, M. J. Breslin, M. T. Rudd, S. J. Stachel, V. L. Rada, J. C. Kern, K. A. Armacost, S. A. Hollingsworth, J. A. O'Brien, D. L. Hall, T. P. McDonald, C. Strickland, A. Brooun, S. M. Soisson and K. Hollenstein, *Nat. Commun.*, 2021, **12**, 815.

41 J. Z. Williams, G. M. Allen, D. Shah, I. S. Sterin, K. H. Kim, V. P. Garcia, G. E. Shavey, W. Yu, C. Puig-Saus, J. Tsoi, A. Ribas, K. T. Roybal and W. A. Lim, *Science*, 2020, **370**, 1099–1104.

