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Cite this: *Chem. Sci.*, 2020, **11**, 5238

All publication charges for this article have been paid for by the Royal Society of Chemistry

Received 13th April 2020

Accepted 29th April 2020

DOI: 10.1039/d0sc02060e

rsc.li/chemical-science

Differentiating A β 40 and A β 42 in amyloid plaques with a small molecule fluorescence probe[†]

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Differentiating amyloid beta (A β) subspecies A β 40 and A β 42 has long been considered an impossible mission with small-molecule probes. In this report, based on recently published structures of A β fibrils, we designed iminocoumarin-thiazole (ICT) fluorescence probes to differentiate A β 40 and A β 42, among which A β 42 has much higher neurotoxicity. We demonstrated that ICTAD-1 robustly responds to A β fibrils, evidenced by turn-on fluorescence intensity and red-shifting of emission peaks. Remarkably, ICTAD-1 showed different spectra towards A β 40 and A β 42 fibrils. *In vitro* results demonstrated that ICTAD-1 could be used to differentiate A β 40/42 in solutions. Moreover, our data revealed that ICTAD-1 could be used to separate A β 40/42 components in plaques of AD mouse brain slides. In addition, two-photon imaging suggested that ICTAD-1 was able to cross the BBB and label plaques *in vivo*. Interestingly, we observed that ICTAD-1 was specific toward plaques, but not cerebral amyloid angiopathy (CAA) on brain blood vessels. Given A β 40 and A β 42 species have significant differences of neurotoxicity, we believe that ICTAD-1 can be used as an important tool for basic studies and has the potential to provide a better diagnosis in the future.

Introduction

Amyloid beta (A β) plaques, one of the characteristic biomarkers for Alzheimer's disease (AD), have been discovered for more than 100 years in the postmortem brains of AD patients.^{1,2} However, the role of A β plaques in the pathology of AD has still been heavily debated, because the correlation between plaque burdens (numbers and areas) and the severity of AD is poor.^{3–5} In the plaques, A β 40 and A β 42 peptides are major constituents. Nonetheless, unlike the role of plaque, there is nearly no argument that A β 42 has much higher neurotoxicity than A β 40 does.^{1,2,4,6,7} Conceivably, differentiating A β 40 and A β 42 can considerably clarify the role of plaque in AD pathology. Unfortunately, small-molecule probes with such capacity are scarce.⁷

Due to the small difference in the amino acid sequence of the peptides, discovering small-molecule probes capable of differentiating A β 40 and A β 42 has been considered as an impossible mission. In our previous studies, inspired by the binding principles of antibodies for soluble and insoluble A β s, we designed a series of small fluorescent molecules to

selectively detect soluble A β s,⁸ the likely biomarker for the early stage of AD pathology. Encouraged by the antibody's capability to specifically recognize A β 40 or A β 42 peptides, we hypothesized that it could be possible to differentiate A β 40 and A β 42 with a small molecule probe. Our design strategy is different from most previous studies, which are focused on adjusting optical properties to turn on (off) signals or make larger stokes shifts.^{9–13} Unfortunately, few probes have been designed based on the insights from the A β structures. In this report, we demonstrated that our designed small-molecule fluorescence probe, **ICTAD-1**, has the capacity to spectrally differentiate A β 40 and A β 42 *in vitro* and in the biologically relevant environment. We believe that our strategy could provide a new path for designing A β probes.

Results

Design of fluorescent imaging probes

It is obvious that the C-terminal of A β peptide is the key for designing small-molecule probes to distinguish A β 40 and A β 42. However, this is extremely challenging, due to the difference in only two amino acids (isoleucine–alanine). Nonetheless, it has been routinely performed in numerous laboratories with *anti*-A β 42 antibodies to determine the contents of A β 42 in cell media and brain tissues.^{14–17} These *anti*-A β 42 antibodies were designed based on the epitope of the C-terminal of the peptide. This fact has bolstered us to believe that the properties of the C-terminal can be relied on to design our small molecule probes. In the

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[†] Electronic supplementary information (ESI) available. See DOI: 10.1039/d0sc02060e

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past, X-ray structures of full-length A β s were rare.^{18–20} However, in recent years, several detailed structures of A β fibrils have been published. Particularly, the advanced cryoEM technology has impressively facilitated A β structure studies.^{21–23}

After having carefully surveyed the published structures of A β fibrils, we found several potential binding sites for designing probes for A β fibrils. The sites are A site, which locates in the hydrophilic N-terminal portion, B site, the hydrophobic mid-region, and C site, which is formed by a hydrophobic C-terminal from one A β peptide and a hydrophilic N-terminal from another A β peptide (Fig. 1a). Numerous small molecules have been reported as ligands of A β 40 and A β 42 species, including several sub-species such as soluble oligomers and insoluble fibrils. However, nearly all of the compounds have been designed to interact with the B site, which is the middle region of A β peptides.^{8,10,24–35} Obviously, this is not the suitable region for designing probes to differentiate A β 40 and A β 42. Surprisingly, to the best of our knowledge, no compound has been intentionally designed or validated to target the C-terminal and the C site. Interestingly, we noticed that, for the site C in most cases, multiple pieces of the A β peptide forms a gulf, in which one side consists of hydrophilic amino acids (K28, D1), and another side is hydrophobic of V39, V40, I41, and A42 (isoleucine-alanine), the last two amino acids in A β 42 (Fig. 1b and S1†).

This interesting feature of the C site requires its binding ligands to meet the following criteria: (1) although A β 40 and A β 42 only have two amino acids difference, their hydrophobicity is very distinct. It is well known that, compared to A β 40, A β 42 is much stickier and considerably easier to aggregate. This

is the key feature for designing probes to distinguish them, and this key feature requires the designed probes contain a hydrophobic moiety to interact differently with the hydrophobic side of the C-site; (2) in addition to the hydrophobic moiety, the ligand needs to contain a hydrophilic moiety to interact with the polar side; (3) the designed probe has a different binding affinity to A β 40 and A β 42 fibrils; and (4) the probes should have distinct fluorescence spectra and/or binding strength in the presence of A β 40 and A β 42 fibrils.

In terms of the fluorescent properties of small-molecule fluorescent probes, numerous compounds showed blue-shifting (hypsochromic shifting) after interacting with A β s, suggesting they bind to a hydrophobic environment. However, benzothiazole analogues are distinct because they showed fluorescence red-shifting (bathochromic shifting),³⁶ indicating this moiety can bind to a polar environment. The most typical compound is thioflavin T, which has been used as a gold standard for A β plaque staining, and its derivative PIB has been widely used in the clinic as a PET tracer for imaging A β deposits.^{37–43} Thioflavin T provides the classic emission of spectral red-shifting. However, thioflavin T cannot spectrally differentiate the A β fibrils, likely due to its incapacity to differentially interact with the hydrophobic moiety of the C-site. Nonetheless, we consider thioflavin T is a good starting point for probe designing.

Based on the above consideration, the designed probe should be tilted between the hydrophilic and hydrophobic moieties with a vertical arrangement (parallel to the fibril axis) (Fig. 1d), while thioflavin T is too short to touch the hydrophobic moiety and this is why it does not have the differentiating capacity. Conceivably, extending the length of the hydrophobic patch of thioflavin T has the potential to achieve this goal (Fig. 1c). In this regard, we designed **ICTAD-1** (imino-coumarin-thiazole for AD), in which *N,N*-dimethyl-phenyl is for touching the hydrophobic moiety and for adjusting the binding affinity. In addition, iminocoumarin was introduced to stretch the hydrophilic moiety, which can enhance the binding through increasing hydrogen bonds (Fig. 1c). Moreover, the NH group in iminocoumarin could be served as a hydrogen donor to form an intramolecular hydrogen bond with benzothiazole moiety, leading to the enhanced planarity of the two heterocycles, which was distinctly different from the previously reported coumarin derivatives.

To validate this design strategy, molecular docking between **ICTAD-1** and A β s was performed. The molecular docking results **ICTAD-1** with A β 42 (PDB: 5OQV) showed that, indeed, the hydrophilic patch of C-site interacted with the stretched hydrophilic moiety of **ICTAD-1**, and the extended aromatic ring moiety interacted with the hydrophobic patch (Fig. 1d). The hydrophobic interaction between **ICTAD-1** with residues ALA2 and ILE41 of A β 42 was observed. The oxygen atom in iminocoumarin formed an intermolecular hydrogen bonding with the NH of GLY38. Moreover, the intramolecular hydrogen bond was also observed. The docking score for **ICTAD-1** with A β 42 at site C was -8.8476 , which was lower than thioflavin T (-6.8242), indicating **ICTAD-1** might have better binding affinity to A β 42 than thioflavin T. Similar docking results of **ICTAD-1** with other

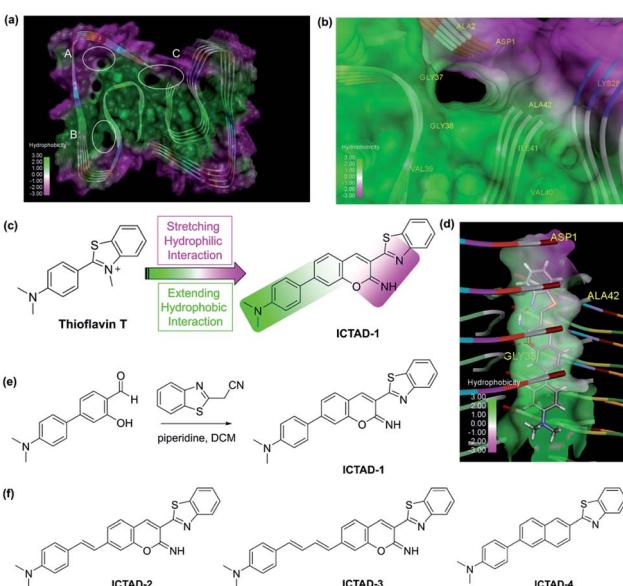


Fig. 1 (a) The possible binding sites of A β 42 protein (PDB: 5OQV); (b) binding site C of A β 42 (PDB: 5OQV); (c) the design strategy of probe **ICTAD-1**; (d) the binding model of probe **ICTAD-1** with A β 42 protein (PDB: 5OQV), the red dashed lines note hydrogen bonds; (e) the synthetic route for probe **ICTAD-1**; (f) the structures of compounds **ICTAD-2**, **ICTAD-3**, and **ICTAD-4**.



$\text{A}\beta 42$ fibrillar structures (PDB: 5KK3 and 2NAO) were achieved (Fig. S2a and b[†]). We also carried out the docking studies of **ICTAD-1** with $\text{A}\beta 40$ fibrillar structures (PDB: 2MVX). The docking results showed **ICTAD-1** could bind to the C site of $\text{A}\beta 40$ through three intramolecular hydrogen bonds with residues HIS6 and GLU11 (Fig. S2c[†]). And it was observed that there were hydrophobic interactions between **ICTAD-1** with residues PHE4 and VAL40. Moreover, the docking score of **ICTAD-1** with $\text{A}\beta 40$ was -8.2130 , which was slightly lower than $\text{A}\beta 42$. Similarly, **ICTAD-1** could also dock into the C sites of other $\text{A}\beta 40$ fibrils (PDB: 2MPZ and 6SHS) (Fig. S2d and e[†]). Considering the difference in the hydrophobic environment at sites C in $\text{A}\beta 40$ and $\text{A}\beta 42$, these results indicated that **ICTAD-1** had the potential to bind and discriminate $\text{A}\beta 40$ and $\text{A}\beta 42$ fibrils.

To investigate whether the iminocoumarin moiety is necessary for binding, we designed **ICTAD-2** by replacing it with a naphthalene ring. In addition, we designed **ICTAD-3** and -4 to further extend the hydrophobic moiety to investigate whether the compounds can better match with the hydrophobic patch in the C-site. The synthesis of **ICTAD-1** is straightforward, and its route is shown in Fig. 1e. The structures and synthetic routes for **ICTAD-2**, -3, and -4 are shown in Fig. 1f and ESI.[†]

Properties of **ICTAD-1**

With the probe in hand, we firstly performed the photostability experiments in DMF to investigate whether **ICTAD-1** is stable under light (1500 joule per minute), and found that there were nearly no changes of fluorescence intensity after irradiating 120 minutes (Fig. 2a and S3a–d[†]), suggesting that **ICTAD-1** has excellent stability to resist photobleaching. To explore **ICTAD-1**'s responses towards different pH media, we titrated it within the range of pH 2–11, and found its absorbance intensity was consistent from pH 6–11. While we found that its fluorescence intensity decreased dramatically from pH 2–5, and its fluorescence is minimal under pH 7 (Fig. 2b and S4[†]), suggesting this

probe has minimal fluorescence background signal and is suitable for *in vivo* imaging. With **ICTAD-1** in hand, we also investigate its absorbance and emission spectra in different solvents. We found that the absorbance is much less dependent (<30 nm changes) on solvent polarity, while its emission could be drastically changed in different solvents, and about 150 nm difference could be found from non-polar hexane to glycol. As we expected, **ICTAD-1** displayed much longer emission in polar solvents such as DMSO and glycol, indicating this probe can interact with a polar environment (Fig. 2c, d and S4[†]). Moreover, **ICTAD-1** exhibited higher quantum yield in the nonpolar solvents, such as hexane and toluene (Table S1[†]).

Responses of **ICTAD-1** to $\text{A}\beta$ fibrils in solutions

To examine **ICTAD-1**'s emission response to $\text{A}\beta$ fibrils, we incubated 250 nM of the probe with different concentrations of $\text{A}\beta 40$ and observed a consistent red-shifting of emission from 1.25 μM to 12.5 μM , suggesting the binding of **ICTAD-1** with $\text{A}\beta$ s is not 1 : 1 stoichiometry (Fig. 3a). Meanwhile, apparent fluorescence intensity increases could be observed with different concentrations of $\text{A}\beta 40$. The largest shift was 47 nm and the largest intensity increase was over 6-fold. We also observed that the fluorescence intensity increased with time and it reached a plateau within 20 minutes (Fig. S5c and d[†]). The turn-on effect of **ICTAD-1** is likely due to twisted intramolecular charge transfer (TICT) upon binding to the fibrils, in which the planar configuration is preferred, and the rotation of the aromatic rings is restricted.^{33,44} From this study, we were also able to calculate a binding constant $K_d = 6.27 \mu\text{M}$ for $\text{A}\beta 40$, while K_d of $\text{A}\beta 42$ was 3.78 μM , suggesting that the binding to $\text{A}\beta 40$ fibrils was weaker than that for $\text{A}\beta 42$ fibrils (Fig. 3a–d). In addition, we found that **ICTAD-1** provided excellent linear correlations with the concentrations of $\text{A}\beta 40$ and $\text{A}\beta 42$ fibrils in the range of 0–4 μM (Fig. S5[†]).

We then performed similar experiments to study the emission changes of **ICTAD-1** with $\text{A}\beta 42$ fibrils and found consistent red-shifts. Remarkably, we observed that the degrees of emission peak shifting were different, and $\text{A}\beta 40$ provided much larger red-shifting (Fig. 3e and f). This is expected because $\text{A}\beta 42$ provided tight binding due to its higher hydrophobicity and crowded space, while $\text{A}\beta 40$ is less crowded and provides loose binding. This is consistent with **ICTAD-1**'s binding constants for $\text{A}\beta 40/42$. Interestingly, in the solutions of $\text{A}\beta 40/42$ mixture, we found that the normalized spectral peaks shifted from shorter wavelengths (blue) to longer wavelengths (red) with the increasing ratio of $\text{A}\beta 40$ component, and the shifted wavelength number was linear to the ratio of $\text{A}\beta 40/42$ (Fig. S6[†]). In addition, we found that **ICTAD-1** had excellent selectivity over metal ions and other proteins, such as bovine serum albumin (BSA) and human serum albumin (HSA) (Fig. S7[†]).

To examine whether a naphthalene ring can be used to replace the iminocoumarin moiety in **ICTAD-1**, we performed similar solution tests with **ICTAD-2**, and found that **ICTAD-2** provided a slight red-shifting and a slight intensity decrease (Fig. S8a[†]), suggesting the hydrophilic iminocoumarin moiety is necessary for binding to the hydrophilic patch in $\text{A}\beta$

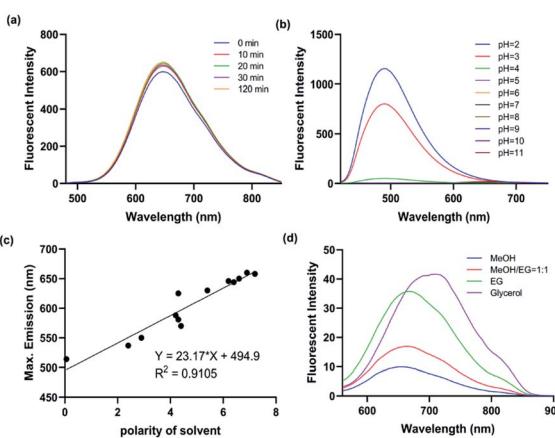


Fig. 2 (a) The fluorescent spectra changes of **ICTAD-1** (10 μM) in DMF under the irradiation of daylight lamp for 120 min; (b) the fluorescent spectra of **ICTAD-1** (10 μM) in different pH aqueous solutions (1% DMF); (c) the linear relationship between the polarity of solvent and the maximum emission wavelength; (d) the fluorescence spectra of **ICTAD-1** (10 μM) in solvents of different viscosity, EG: ethylene glycol.



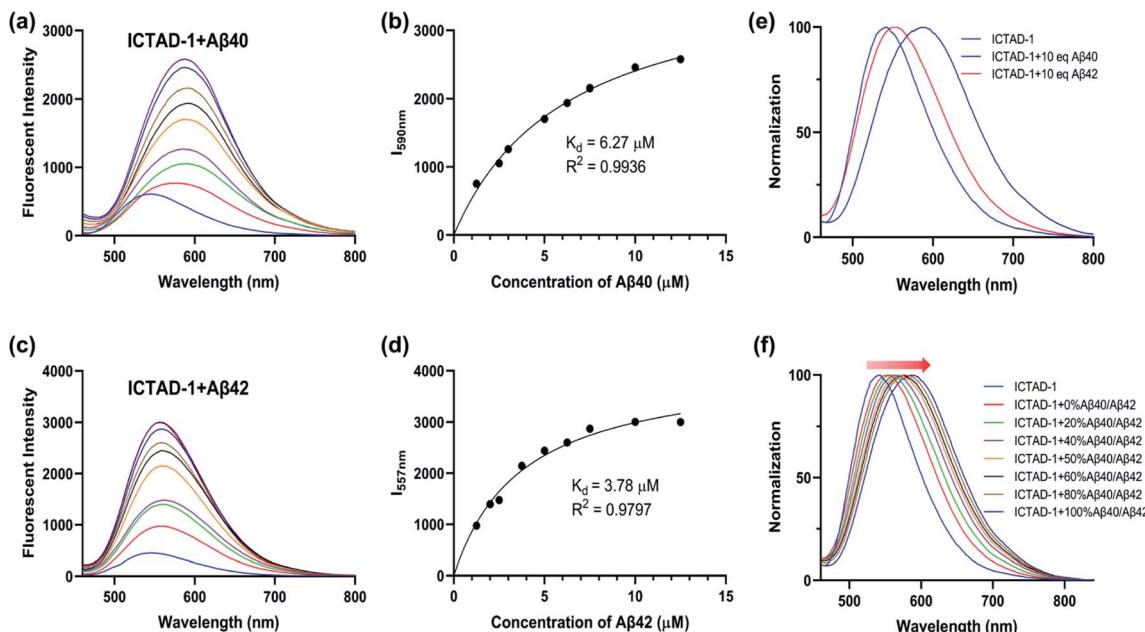


Fig. 3 The fluorescent spectra of ICTAD-1 (250 nM) in the absence and presence of A β 40 (a) or A β 42 (c); the binding curve of ICTAD-1 (250 nM) with A β 40 (b) or A β 42 (d); (e) normalization fluorescent spectra of ICTAD-1 (250 nM) with A β 40 or A β 42 (10 eq., 2.5 μ M); (f) normalization fluorescent spectra of ICTAD-1 (250 nM) with different percent of A β 40 in A β 42 (10 eq., 2.5 μ M).

fibrils. Different from **ICTAD-1**, **ICTAD-3** showed no apparent red-shifting, while it showed a slight intensity increase (Fig. S8b†). **ICTAD-4** showed an observable blue-shifting and a moderate intensity increase (Fig. S8c†). Since **ICTAD-2**, -3, and -4 didn't have favorable properties for differentiating A β 40/42, we didn't perform further investigation for these compounds.

Differentiating A β 40 and A β 42 with ICTAD-1 *via* spectral unmixing imaging

To explore whether **ICTAD-1** can be used to quantify the amount of A β 40 and A β 42 fibrils, spectral unmixing with mixtures of these fibrils was performed (Fig. S9†). First, we used pure A β 40 and A β 42 fibrils solutions to establish the spectra on a 96-well plate. The linear relationships could be observed for both fibrils (Fig. S10†), suggesting that spectral unmixing is feasible to quantify the contribution of each component in the mixture. The detection limitations are 3.3 nM and 28.3 nM for A β 40 fibrils and A β 42 fibrils respectively. Then we conducted library-based spectral unmixing to separate the ratios of these two fibrils. Indeed, we found that it was feasible to deconvolute the signals with the characteristic spectra of free **ICTAD-1** (green), **ICTAD-1** with A β 40 fibrils (red), and A β 42 fibrils (blue) (Fig. 4a and b).

Next, to investigate whether spectral unmixing is feasible in a biologically relevant environment, we performed the above experiments in the presence of bovine serum albumin (BSA) and mouse brain homogenate (BH). As we expected, spectral unmixing could be used to deconvolute the signals from the free probe (green), binding with BSA or BH (cyan), binding with A β 40 (red) and A β 42 (blue) (Fig. 4c–e), suggesting it is possible

to spectrally differentiate the A β fibrils in biologically relevant environments.

Tissue staining and spectral unmixing with **ICTAD-1**

We first explored whether **ICTAD-1** could provide a high quality of plaque staining, and found that plaques on brain slides of 5xFAD mice can be sharply visualized after the slide was incubated with the probe for 15 minutes (Fig. 5a), and the labeled plaque showed excellent colocalization with 6E10 antibody staining (Fig. 5a), which is specific to A β s. This result suggested that **ICTAD-1** was able to specifically label A β plaques.

The previous results inspired us to explore the capability of **ICTAD-1** in differentiating A β 40 and A β 42 fibrils in the plaques. Then we relied on confocal imaging that has been equipped with a spectral unmixing function. Interestingly, the spectra from the core most closely resembled the one for A β 42 *in vitro* studies, whose peak wavelength was shorter. Meanwhile, the spectra from the periphery were similar to the one from A β 40 fibrils *in vitro*, whose peak has a longer wavelength (Fig. 5b–e and S11†). The peak wavelength difference from the two spectra was 12 nm (Fig. 5e). Reportedly, A β 42 is the dominant species in the core of plaques,^{45–48} which is consistent with our spectral unmixing results. Taken together, these results suggested that **ICTAD-1** could be used to quantify the contents of A β 42/A β 40 from brain slides. This also indicates that it is possible to quantify the subspecies in human brain tissue, which is very important to clarify the contributions of A β 42 fibrils to the AD pathology.

In vivo two-photon imaging with **ICTAD-1**

To validate whether **ICTAD-1** can be used for *in vivo* imaging, we performed two-photon microscopic imaging with 15 month old

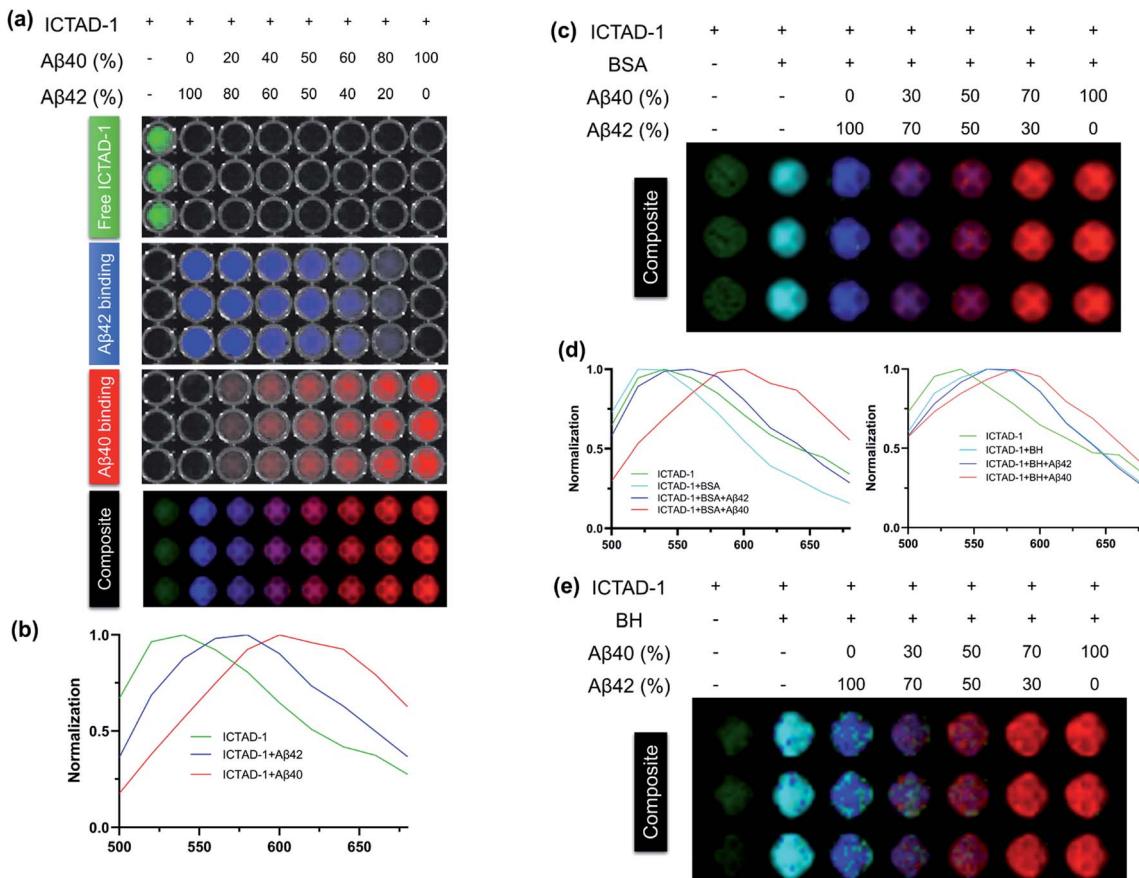


Fig. 4 (a) Plate imaging of ICTAD-1 (250 nM) in the presence of different ratios of A β 40/A β 42 (2.5 μ M, 10 eq.) in 96-wells plate after unmixing. $E_x = 430$ nm, $E_m = 500$ –680 nm. (b) Normalized unmixing spectra of ICTAD-1 (250 nM) with or without A β 40 and A β 42; (c) plate imaging of ICTAD-1 (250 nM) in the presence of different ratios of A β 40/A β 42 (2.5 μ M, 10 eq.) in 96-wells plate after unmixing in the presence of BSA; (d) normalized unmixing spectra of ICTAD-1 (250 nM) with or without A β 40 and A β 42 in the presence of BSA or mouse brain homogenate (BH); (e) plate imaging of ICTAD-1 (250 nM) in the presence of different ratios of A β 40/A β 42 (2.5 μ M, 10 eq.) in 96-wells plate after unmixing in the presence of mouse brain homogenate.

5xFAD mice. We first intravenously (iv) injected the mouse with FITC-dextran as the contrast agent for blood vessels. After 5 minutes, we iv injected **ICTAD-1** (1 mg kg⁻¹), and imaged the mouse at 5 minutes post-injection of **ICTAD-1**. As expected, the plaques can be easily identified, due to the excellent contrast (Fig. 6a-c), suggesting that the probe can cross the brain-blood barrier (BBB) and can label plaques *in vivo*. Interestingly, we experienced some difficulties to identify cerebral amyloid angiopathy (CAA) on the vessels, which can be found from its auto-fluorescence (blue in Fig. 6d and e). These results indicated that **ICTAD-1** has weak capacities to label CAAs, in which A β 40 is the dominant species.^{49,50} This result could be possibly explained with our *in vitro* K_d data, which indicated that **ICTAD-1** had much stronger binding to A β 42, while it showed weaker binding to A β 40. This *in vivo* data also suggested that differentiating A β 40 and A β 42 *in vivo* via different binding strength (K_d) was feasible.

Discussion

$\text{A}\beta$ plaques have been discovered for more than 100 years, however, their roles in AD pathology are still poorly defined. The

complicated dynamics and contributions of each component are the likely factors for the perplex. It is well documented that A β 40 and A β 42 are the major components of the plaques. Nonetheless, it is not clear what is the contribution weight of each A β subspecies to the pathology, and whether the content of A β 42 in plaques has better correlations with the severity of the disease. With our probe, it is possible to partially solve the mysteries, and we may have the capacity to quantify how much A β 42 is in each plaque, each brain slide, and specific brain areas. Conceivably, it is also possible to quantify A β 42 contents for a whole-brain through serial slide imaging. With such a tool, we will be well equipped to answer those basic mechanism questions and will clarify the questions around postmortem plaques, which will provide more diagnostic information.

Thioflavin T reportedly showed slight difference of fluorescence lifetimes in pure solutions for A β 40 and A β 42 fibrils,⁵¹ however, it remains unknown whether the differences can be applied under physiological conditions. Kung *et al.*⁵² reported that radioligand [^{125}I]DMTZ had certain preference for A β 42-positive cerebral amyloid angiopathy (CAA). However, it is not clear whether it has the capacity to differentiate A β 40/42 in the plaques.

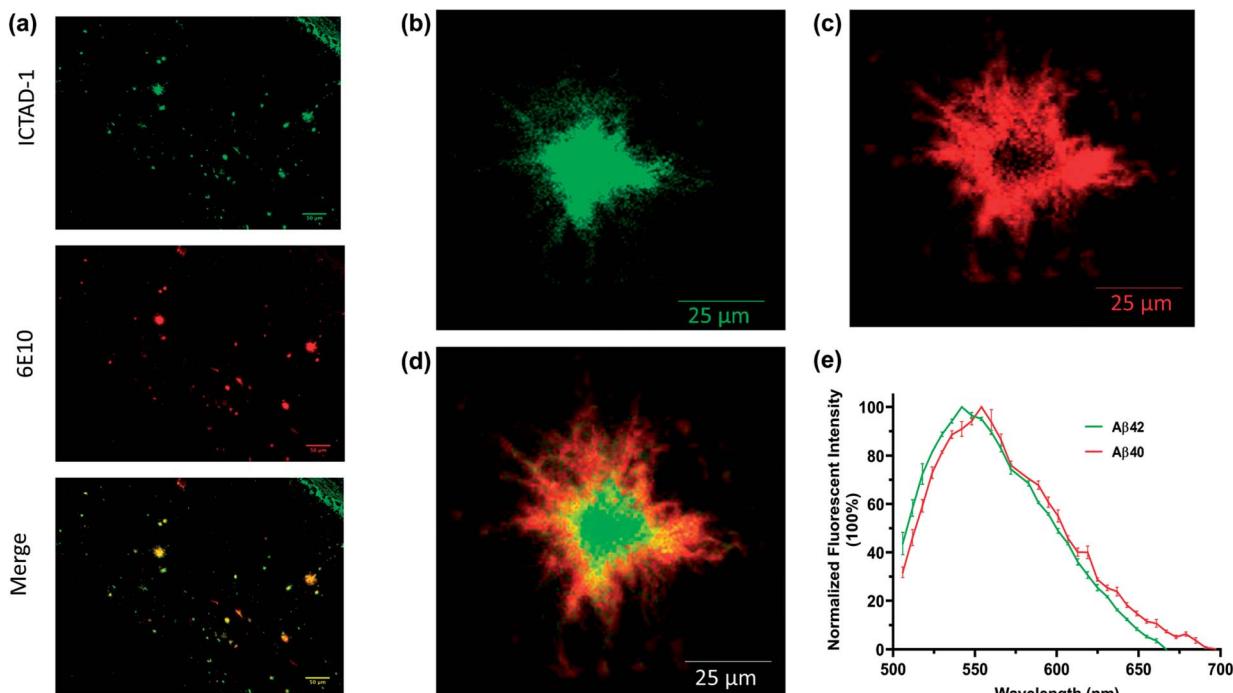


Fig. 5 (a) The brain tissues from 5xFAD mice were co-stained with ICTAD-1 and antibody 6E10; (b) the core of A_β plaque stained with ICTAD-1; (c) the periphery of A_β plaque stained with ICTAD-1; (d) merged image of (b) and (c); (e) the normalized unmixing fluorescent spectra of A_β plaques stained with ICTAD-1 ($n = 3$).

In this report, we also demonstrated that **ICTAD-1** could be used to separate A_β40/42 using spectral properties *in vitro* and binding strength *in vivo*. The spectral unmixing is easy to perform on a regular confocal microscope, suggesting our

method can be easily adapted by other biological-oriented laboratories. From the slide spectral unmixing, the separation of emission peaks of A_β40/42 was 12 nm, which may indicate that the separation of A_β40/42 is imperfect. However, it is

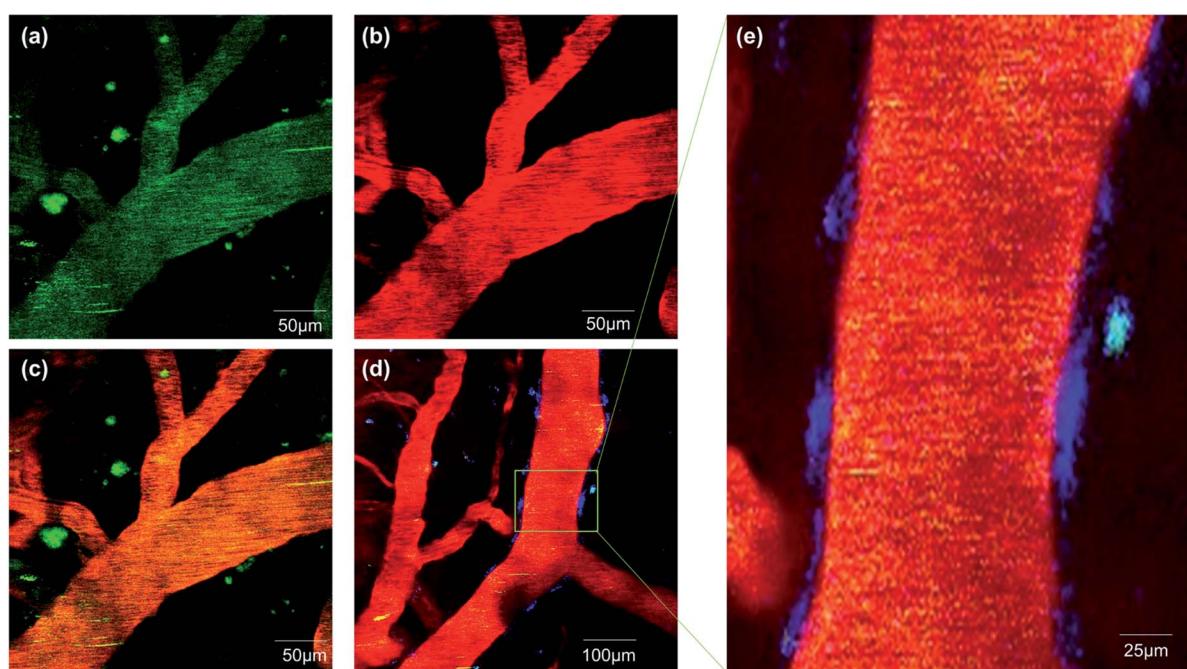


Fig. 6 Two-photon fluorescent images in 5xFAD mice after tail intravenous injected with ICTAD-1 and FITC-dextran. (a) The fluorescence from ICTAD-1 in emission channel of 570–620 nm; (b) the fluorescence from FITC-dextran in emission channel of 500–550 nm; (c) the merged image of (a) and (b); (d) fluorescence imaging of A_β plaques, CAA and blood vessel; (e) partial enlarged detail of (d).



possible to achieve a cleaner separation (a larger difference in the emission peak) if a better algorithm is developed.

The difference of K_d for A β 40/42 could be utilized for designing PET tracers that have much high specificity for A β 42, the most toxic species. Our *in vivo* two-photon imaging indicated that **ICTAD-1** had certain binding preference towards A β 42, and this could be considered as clues for designing for A β 42 specific PET tracers. In addition, it is also tremendously important if we can differentiate CAA and plaques with a PET tracer, which is not currently available. Reportedly, A β 40 is the major component of CAAs.^{49,50} Our data from this report suggests that our probe and its analogues may have the potential to differentiate plaques and CAAs. With such a probe, we will be able to dissect the vascular CAA contribution and plaque contribution to AD pathology.

Our studies also pointed to several possible directions for future AD research. First, we may have the capacity to monitor therapy that is prone to reduce A β 42. Second, it is possible to design drugs that specifically target A β 42. Lastly, we will be able to investigate whether the specific reduction of A β 42 is a validated approach for future drug development.

Conclusions

In summary, we demonstrated that **ICTAD-1** was able to spectrally differentiate A β 40/42 in solutions, in plasma and in brain tissues. **ICTAD-1** has the potential to dissect the toxicity contributions of A β 40 and A β 42, and could be considered as a lead compound for developing A β 42 specific PET tracers.

Ethical statement

All animal experiments were performed in strict accordance with the NIH guidelines for the care and use of laboratory animals (NIH Publication No. 85-23 Rev. 1985) and was approved by the Institutional Animal Care and Use Committee at Massachusetts General Hospital.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

This work was supported by NIH R01AG055413, R21AG065826 and R21AG059134 awards (C. R.). The authors would like to thank Pamela Pantazopoulos, B. S. for proofreading this manuscript.

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