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# Dual enzyme-like activity of iridium nanoparticles and their applications for the detection of glucose and glutathione†

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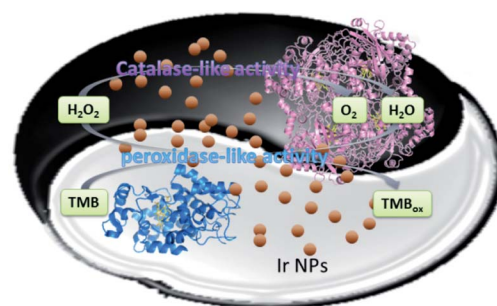
Here we show that iridium nanoparticles (Ir NPs) functionally mimic peroxidase and catalase. The possible mechanism of intrinsic dual-enzyme mimetic activity of Ir NPs was investigated. Based on the excellent peroxidase-like activity of Ir NPs, a new colorimetric detection method for reduced glutathione (GSH) and glucose was proposed.

Recently, nanomaterials with inherent enzyme-like activity have attracted considerable attention due to their simple preparation, storage, and separation, as well as the low cost as compared with natural enzymes. Various nanomaterials have been shown to mimic the activity of oxidase, peroxidase, catalase or superoxide dismutase (SOD), ranging from metals,<sup>1–10</sup> metal oxides,<sup>11–15</sup> and metal coordination complexes<sup>16–21</sup> to carbon-based nanomaterials.<sup>22–26</sup> The ability of these nanomaterials to replace specific enzymes may offer new opportunities for enzyme-based applications. For example, nanozymes with oxidase-like or peroxidase-like activity have shown potential applications in biosensing and immunoassay, such as the detection of H<sub>2</sub>O<sub>2</sub>, glucose, antioxidants, antigens, antibodies and so on.<sup>27</sup> By using nanozymes with peroxidase-like activities, Wei and co-workers recently have developed novel sensor arrays to detect biothiols and proteins as well as discriminate cancer cells owing to the differential nonspecific interactions between the components of the sensor arrays and the analytes, providing a potential approach to discriminate versatile analytes.<sup>8</sup> Nanomaterials with SOD-like or catalase-like activity have exhibited antioxidant activity, thus could protect aerobic cells from oxidative stress, showing potential application in inflammation therapy.<sup>6,28–31</sup> Also, nanozymes with high catalase-like activity was able to produce O<sub>2</sub> at the hypoxic tumor site, serving as efficient agents for cancer therapy.<sup>23,32,33</sup> Very recently, Zhang' group has developed a simple and biocompatible platform to elevate O<sub>2</sub> for improving photodynamic therapeutic efficacy by combining the photosensitizer with Prussian blue

nanomaterials.<sup>34</sup> Prussian blue could catalyze H<sub>2</sub>O<sub>2</sub> to generate O<sub>2</sub>, and then the photosensitizer transforms the O<sub>2</sub> to produce singlet oxygen (<sup>1</sup>O<sub>2</sub>) upon laser irradiation for cancer therapy. Besides, Qu *et al.* have found the porous platinum nanoparticles with catalase-like activity, which greatly enhanced radiotherapy efficacy and overcame the hypoxic tumor microenvironment.<sup>35</sup>

In this work, we demonstrate that Ir NPs exhibited both peroxidase-like and catalase-like activities. As shown in Scheme 1, Ir NPs can catalyze the decomposition reaction of H<sub>2</sub>O<sub>2</sub> into oxygen and water, possessing potential applications in the cancer therapy as catalase mimics. On the other hand, the tiny Ir NPs with the average diameter of 2.4 nm exhibited high peroxidase-like catalytic activity. Furthermore, by using H<sub>2</sub>O<sub>2</sub> as an intermediary, a simple and sensitive colorimetric detection method for GSH and glucose has been designed.

Synthesis of Ir NPs were carried out by a simple chemical reduction process, in which sodium hexachloroiridate(III) hydrate was used as precursor with ascorbic acid as a protecting agent and sodium borohydride as the reducing agent (see Experimental section in ESI†). After heating and stirring at 95 °C for 15 min, the resulting homogeneous light brown Ir NPs dispersion was obtained with good stability and reproducibility.



**Scheme 1** Schematic presentation for dual-enzyme mimetic activity of Ir NPs.

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The obtained Ir NPs were thoroughly characterized by various methods. Transmission electron microscopy (TEM) images indicated that the as-prepared Ir NPs showed a narrow size distribution with the average diameter of  $\sim 2.4$  nm (Fig. 1A–C). UV-vis spectrum of Ir NPs showed an absorption peak at  $\sim 280$  nm (Fig. 1D), in agreement with the value reported earlier,<sup>28</sup> indicating the formation of Ir NPs. XPS spectra of Ir 4f in Ir NPs were presented in the Fig. S1†. A pair of doublet peaks at 61.0 and 64.0 eV were observed, revealing that Ir in Ir NPs is mostly metallic Ir(0).<sup>36</sup> Furthermore, inductively coupled plasma-optical emission spectroscopy (ICP-OES) disclosed that the exact concentration of Ir NPs is  $25 \mu\text{g mL}^{-1}$ .

To investigate the peroxidase-like activity of Ir NPs, the peroxidase coupled assay was employed and the change in absorbance of reaction was monitored using a UV-vis absorbance spectrophotometer. As shown in Fig. 2A, exposure of Ir NPs to a colorless peroxidase substrate 3,3',5,5'-tetramethylbenzidine (TMB) in the presence of  $\text{H}_2\text{O}_2$  resulted in the fast oxidation of TMB to a blue product. However, no color change of the TMB substrate was observed only with Ir NPs or  $\text{H}_2\text{O}_2$ , indicating the intrinsic peroxidase-like activity of Ir NPs. Similar to HRP, the catalytic activity of Ir NPs is dependent on the pH, temperature and catalyst dosage. Fig. S2† showed that the catalytic activity of Ir NPs was much higher in weakly acidic solution and reached its highest at pH 4.0, consistent with those reported for peroxidase-like NPs and HRP.<sup>37–40</sup> In the range of 20–80 °C, the maximum catalytic activity was obtained under 50 °C. For simplicity, we adopted pH 4.0 and room temperature ( $\sim 20$  °C) for subsequent analysis of peroxidase-like activity of Ir NPs. When increasing the dosage of Ir NPs, the catalytic activities of Ir NPs clearly increased as shown in Fig. 2B. Interestingly, some small gas bubbles were observed in the tubes at the same time.

In order to confirm which gas was produced and whether Ir NPs had the intrinsic catalase-like activity, the decomposition

of  $\text{H}_2\text{O}_2$  was further investigated by monitoring the changes of UV-vis absorbance at 240 nm under the basic conditions. As shown in Fig. 2C, the absorbance was obviously decreased as the dosage of Ir NPs increased, and many gas bubbles could be observed in the cuvette, indicating Ir NPs could catalyze the decomposition of  $\text{H}_2\text{O}_2$  into  $\text{O}_2$ . Temperature and pH can also make a big effect on the catalase-like activity of Ir NPs. Under the basic conditions or higher temperature, much more and bigger gas bubbles were produced (Fig. S3†), suggesting higher catalase-like activity of Ir NPs. Obviously, Ir NPs possessed intrinsic catalase-like activity, which could be regulated by adjusting the temperature and pH.

The formation of  $\cdot\text{OH}$  during the reactions was assessed to better understand the mechanism for the dual enzyme-like activity of Ir NPs. Terephthalic acid was adopted here as a fluorescence probe to trap  $\cdot\text{OH}$ . As shown in Fig. 2D, in the absence of Ir NPs, terephthalic acid emitted blue. However, the fluorescence intensity was gradually decreased as the concentration of Ir NPs increased, suggesting that Ir NPs could consume  $\cdot\text{OH}$  radicals rather than generate ones. The reactivity of Ir NPs appears to be different from that of the other peroxidase mimics, where  $\cdot\text{OH}$  mediates the oxidation of organic substrate.

As Ir NPs exhibited the peroxidase-like activity, we monitored the reaction of Ir NPs with  $\text{H}_2\text{O}_2$  and TMB. The apparent steady-state kinetic parameters were determined by changing one substrate concentration while keeping the other substrate concentration constant. The value  $\varepsilon = 39\,000 \text{ M}^{-1} \text{ cm}^{-1}$  (at 652 nm) for the oxidized product of TMB was used here to obtain the corresponding concentration term from the absorbance data. As shown in Fig. S4,† we observed that the oxidation reaction catalyzed by Ir NPs followed the typical Michaelis-Menten behavior toward both substrates. The Michaelis-Menten constant ( $K_m$ ) and the maximum initial velocity ( $V_m$ ) given in Table S1† were obtained by using Lineweaver-Burk plot (Fig. S4B and D†). Compared with the Pd-Ir cubes,<sup>38</sup> Ir NPs presented a similar  $K_m$  for TMB and a very low  $K_m$  for  $\text{H}_2\text{O}_2$ , suggesting that Ir NPs have a higher affinity to  $\text{H}_2\text{O}_2$ . Moreover, Ir NPs presented larger  $V_m$  for both of TMB and  $\text{H}_2\text{O}_2$ , indicating the strong catalytic activity of Ir NPs. What is more important is that Ir NPs showed high stability after long-term storage. After five months of storage at room temperature, the peroxidase-like catalytic activity of Ir NPs maintained 96% (Fig. S5†), significantly expanding their practical applications.

On the basis of the high affinity and catalytic activity of Ir NPs to  $\text{H}_2\text{O}_2$ , the analytes that could consume or produce  $\text{H}_2\text{O}_2$  could be detected indirectly by using the TMB as substrate.<sup>27</sup> Therefore, a simple colorimetric method was developed to detect GSH and glucose using Ir NPs. GSH, which plays an important role in many cellular processes including redox activities, signal transduction, detoxification, and gene regulation,<sup>41,42</sup> can consume  $\text{H}_2\text{O}_2$  and result in the shallowing color of the Ir NPs-TMB- $\text{H}_2\text{O}_2$  system. As presented in Fig. 3A, the absorbance dropped sharply with the addition of GSH. And a linear relationship between the absorbance and logarithmic values of GSH's concentrations was obtained in the range from 200 nM to 100  $\mu\text{M}$  (Fig. 3B). The level changes of GSH have been linked to varieties of diseases, such as diabetes, psoriasis, liver

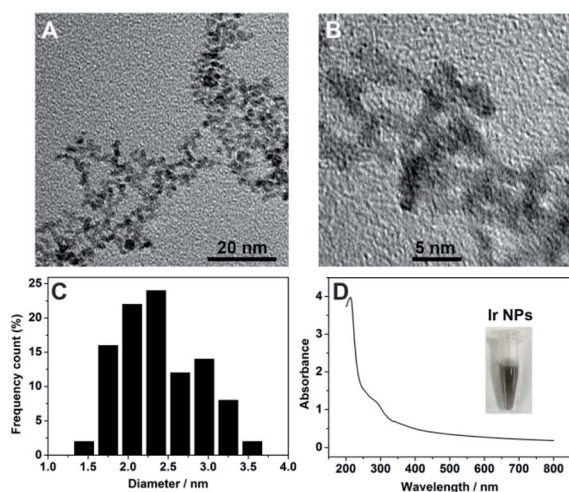


Fig. 1 (A and B) TEM images of Ir NPs at different magnification. (C) Size distribution histogram of Ir NPs. (D) UV-vis absorption spectrum of Ir NPs. The inset shows the photograph of Ir NPs dispersed in the aqueous solution.



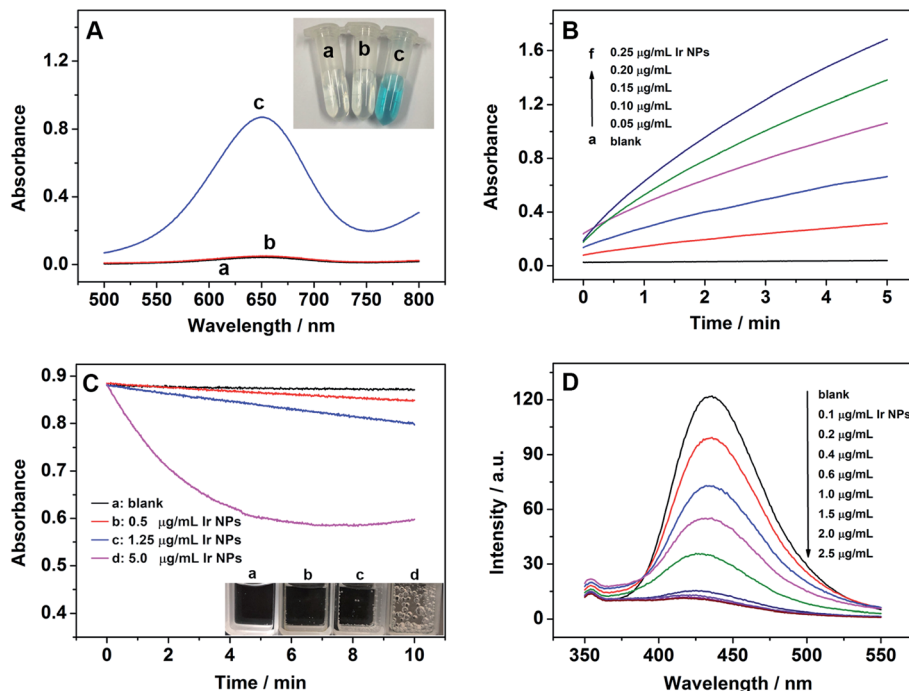


Fig. 2 (A) The absorption spectra and digital photos of different colorimetric reaction systems: (a) TMB + H<sub>2</sub>O<sub>2</sub>, (b) TMB + Ir NPs, and (c) TMB + H<sub>2</sub>O<sub>2</sub> + Ir NPs. (B) Time-dependent absorbance changes at 652 nm of TMB reaction solutions catalyzed by the different concentrations of Ir NPs. (C) Time-dependent absorbance changes at 240 nm of 20 mM H<sub>2</sub>O<sub>2</sub> catalyzed by the different concentrations of Ir NPs incubated in 0.1 M HAC–NaAc buffer (pH 9.0). (D) The effect of concentration of Ir NPs on the formation of hydroxyl radical with terephthalic acid as a fluorescence probe. Reaction condition: 0.1 M HAC–NaAc buffer (pH 6.0).

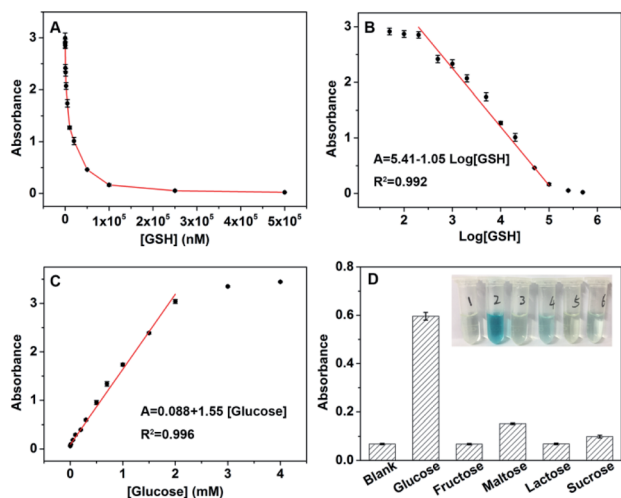


Fig. 3 (A) Dose–response curve for GSH detection at 652 nm. (B) Linear relationship between the absorbance and logarithmic values of GSH's concentrations in the range from 200 nM to 100 μM. (C) Dose–response curve for glucose detection at 652 nm. (D) Determination of the selectivity of glucose detection (from left to right: blank, 0.3 mM glucose, 3 mM fructose, 3 mM maltose, 3 mM lactose and 3 mM sucrose). Inset: the color change with the different solutions. The error bars represents the standard deviation of four measurements.

damage and Parkinsons.<sup>43,44</sup> The proposed colorimetric biosensor provided a sensitive method to monitor GSH. Furthermore, because H<sub>2</sub>O<sub>2</sub> is the main product of the glucose

oxidase (GOx)-catalyzed reaction; glucose could be detected based on the combination of GOx. Fig. 3C shows typical glucose concentration–response curves with the linear range of 10 μM to 2 mM. According to the principle of S/N = 3, the calculated detection limit was 5.8 μM. Table S2† was listed to compare the sensing performance of Ir NPs with other nanomaterials. Ir NPs are superior to other nanomaterials in lower detection limit and wider detection range for colorimetric determination of glucose.

To explore the selectivity of above glucose sensor, 10 times concentration of control samples including fructose, maltose, lactose and sucrose were tested as shown in Fig. 3D. The color difference could be distinguished by the naked eye, suggesting the high selectivity of the biosensing system for glucose detection. Using this method, we detected glucose in 50-fold dilution fetal bovine serum to demonstrate the feasibility of this biosensor for practical applications, and the results are listed in Table S3.† As can be seen, the recoveries of glucose fall in the range of 93.3–104% by using the standard addition method. The proposed biosensor was also applied for determining glucose concentrations in blood samples donated by healthy and diabetic persons (Fig. S6†). According to the calibration curve, the concentration of glucose from different samples was 7.0 mM and 14.4 mM, which agrees well with that measured in the local hospital, 6.8 mM and 14.4 mM. Therefore, this colorimetric method is suitable and satisfactory for glucose analysis of real samples with high sensitivity and selectivity.

In summary, Ir NPs synthesized by a simple chemical reduction process exhibited both of peroxidase-like and catalase-like activity. Moreover, the dual enzyme-like activity could be regulated by adjusting the temperature and pH. On the one hand, Ir NPs could consume  $\cdot\text{OH}$  radicals exhibiting potential applications in the antioxidant therapeutics as antioxidant nanozymes. On the other hand, as peroxidase mimics, Ir NPs were successfully applied in the construction of colorimetric biosensors to detect GSH and glucose. This work will facilitate the utilization of intrinsic dual-enzyme activity and other catalytic properties of Ir NPs in analytical chemistry, biotechnology, and medicine.

## Conflicts of interest

There are no conflicts to declare.

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