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# Multifunctional, histidine-tagged polymers: antibody conjugation and signal amplification†

Yichuan Zhang,<sup>†ab</sup> Alessia Gambardella,<sup>‡a</sup> Muhammed Üçüncü,<sup>†ac</sup>  
Jin Geng,<sup>†ab</sup> Jessica Clavadetscher,<sup>a</sup> Mark Bradley<sup>†\*a</sup> and  
Annamaria Lilienkamp<sup>†\*a</sup>

**A polymer scaffold, with multiple reactive centres, was synthesised by RAFT polymerisation and conjugated to the antibody herceptin. A hexahistidine RAFT agent enabled the rapid and simple purification of polymer–protein conjugates, while the tetrazine conjugation strategy allows myriad cargos to be attached and amplified.**

The ability to amplify reporter signals and cargos is important in a number of areas ranging from fluorescent imaging to radiotherapy and is of particular importance with low abundance targets. Several signal enhancement methods have been developed with numerous techniques associated with the polymerase chain reaction and variants.<sup>1</sup> Non-nucleic acid based amplification methods include horseradish peroxidase-driven signal amplification of tyramide-conjugates<sup>2</sup> or luminol,<sup>3</sup> and alkaline phosphatase driven amplification.<sup>4</sup> Although these enzyme-based amplification methods work well, they typically require the use of secondary antibodies and bespoke substrates, with colorimetric or fluorescent outputs often able to diffuse away from the site of generation. Non-enzymatic fluorescence amplification techniques include *e.g.* the recruitment of antibody-GFP fusion proteins to a target protein tagged with multiple copies of the antibody epitope,<sup>5</sup> Avidin-conjugated viral capsids loaded with dyes for the detection of biotinylated targets,<sup>6</sup> and biological self-assembly of biotin and streptavidin surface engineered quantum dots.<sup>7</sup>

Synthetic polymers are an attractive approach to biomolecule labelling and fluorescence or mass-tag signal amplification.<sup>8</sup> Conjugation of polymers to proteins can be categorised as “grafting-from” and “grafting-to” approaches,<sup>9</sup> the former starting with the formation of a “macro-activator” (*i.e.*, linkage of an

initiator or a chain transfer agent to a protein), followed by polymerisation; however, this approach is limited by the need to avoid protein denaturation and the restricted choice of suitable functional monomers.<sup>10</sup> The “grafting-to” approach uses pre-synthesised polymers for bioconjugation but suffers from complications, such as how to separate conjugated proteins from non-conjugated materials.<sup>11</sup>

Here, we report a rapid amplification approach, based on poly(acrylamide)–antibody conjugates bearing norbornene reactive centres for both “switch-on” of quenched tetrazine-linked fluorophores and cargo amplification in the form of metal ions (Fig. 1). The polymers were synthesised through reversible addition–fragmentation chain transfer (RAFT) polymerisation, using the synthesised chain transfer agent **2** that contained the ubiquitous hexahistidine tag (His-Tag), designed to allow rapid polymer–antibody conjugate purification by metal affinity chromatography. Upon treatment with a quenched BODIPY–tetrazine conjugate, rapid “switch-on” and amplification in fluorescence were observed.

Five polymers with different molecular weights and densities of the norbornene reactive centres were synthesised (**P1–P5**) to explore how composition affected conjugation, antibody binding affinity, and the level of cargo amplification (Fig. 2a). *N,N*-Dimethylacrylamide (DMA) was used due to its low cytotoxicity and the high water solubility of its polymers,<sup>12</sup> with the norbornene-based acrylamide **1** (Scheme S1, ESI†) providing the site for tetrazine ligation. The polymers were efficiently synthesised by RAFT polymerisation with the desired molecular weights (7–30 kDa) with polydispersities between 1.2–1.8 (Table S1 and Fig. S1, ESI†) using a His-Tag-RAFT agent **2** (synthesised on solid-phase<sup>13</sup> in high yield/purity, Scheme S2, ESI†), which allowed the widely used method of metal ion affinity chromatography to be applied to polymer-conjugate purification.

To achieve simultaneous “switch-on” and amplification of fluorescence by the polymer–protein conjugates, two fluorogenic BODIPY–tetrazines were synthesised (Fig. 2b). Tetrazine-quenched fluorophores, that are activated *via* an inverse electron-demand Diels–Alder reaction (*INVDA*), have found use in fluorescent

<sup>a</sup> EaStCHEM School of Chemistry, University of Edinburgh, EH9 3FJ, Edinburgh, UK. E-mail: mark.bradley@ed.ac.uk, annamaria.lilienkamp@ed.ac.uk

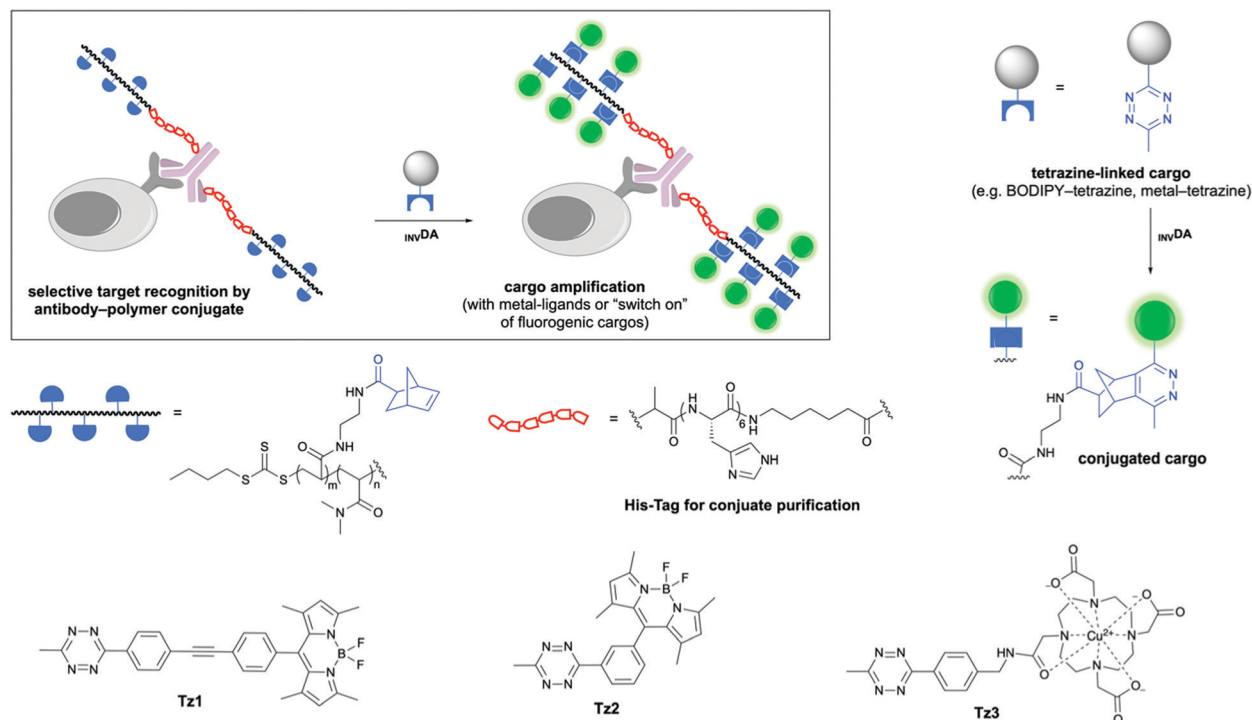
<sup>b</sup> Shenzhen Institutes of Advanced Technology, Chinese Academy of Sciences, Shenzhen, China

<sup>c</sup> Department of Analytical Chemistry, Faculty of Pharmacy, Izmir Katip Celebi University, Izmir, Turkey

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‡ These authors contribute equally.





**Fig. 1** Signal amplification using a polymer–protein conjugate. The antibody herceptin was conjugated to a polymer scaffold that carried multiple norbornenes (for signal amplification *via* tetrazine ligation) and was synthesised using a hexahistidine tagged-RAFT agent. Subsequent treatment with a tetrazine-quenched fluorophore or a metal-bearing tetrazine, “switches-on” and/or amplifies the signal.

imaging,<sup>14–18</sup> allowing direct target visualisation without extensive washing steps. **Tz1** was synthesised as reported previously,<sup>14</sup> whereas the published route to **Tz2**<sup>15</sup> could not be reproduced and instead was synthesised from 3-formylbenzonitrile, *via* the tetrazine aldehyde **S9**,<sup>16</sup> which was treated with 2,4-dimethylpyrrole, followed by oxidation with DDQ and complexation with  $\text{BF}_3 \cdot \text{OEt}_2$  to give the BODIPY–tetrazine **Tz2** in high yield (Scheme S3, ESI†).<sup>17</sup> The metal chelating tetrazine **Tz3** was synthesised by coupling the DOTA–NHS ester to an amino-functionalised tetrazine,<sup>19</sup> followed by Cu(II) loading (Scheme S4, ESI†).

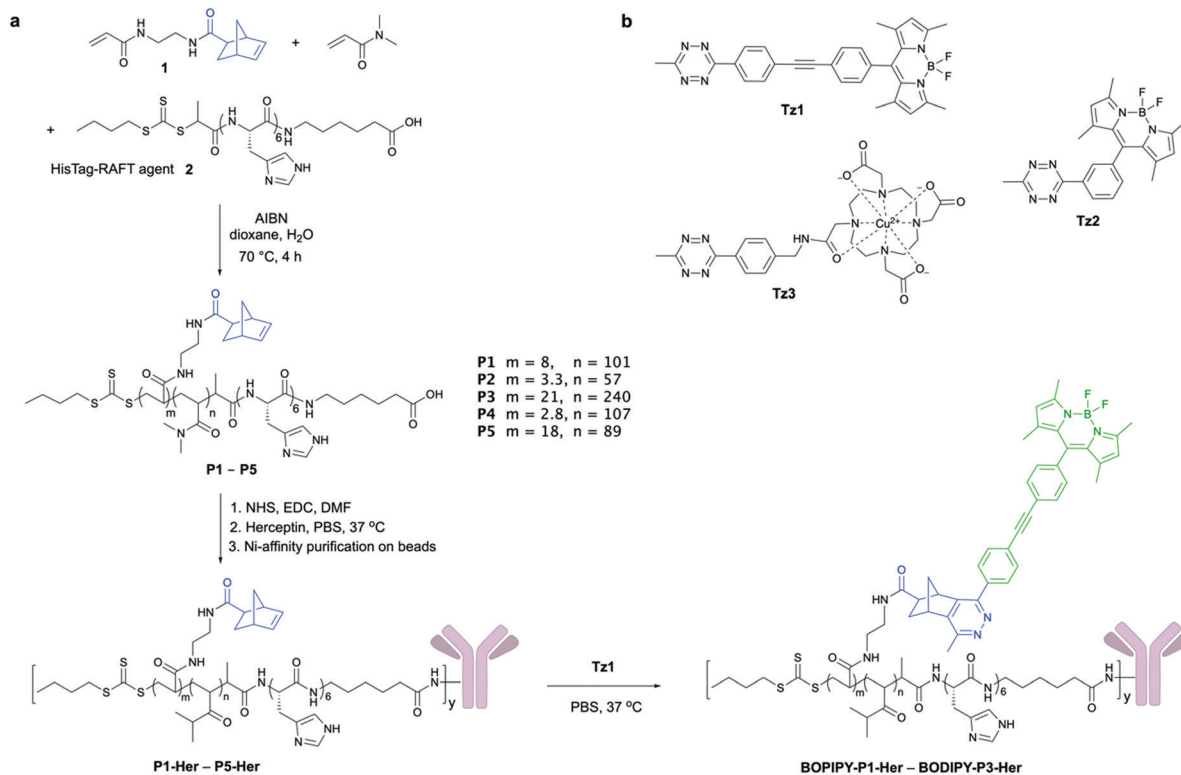
The reactivity of the norbornene-decorated polymer **P1** (12  $\mu\text{M}$ ) with the tetrazines **Tz1** and **Tz2** (1  $\mu\text{M}$ ) was investigated by monitoring the time-dependent increase in fluorescence, triggering fluorescence increases of 21 and 9-fold respectively, in PBS after 30 min (Fig. S3 and S4, ESI†). However, stability studies showed that although **Tz1** and **Tz2** were robust in PBS and serum-free media, **Tz2** underwent undesired tetrazine hydrolysis in serum, while in contrast, **Tz1** showed good stability and was thus used in preference for all investigations (Fig. S5, ESI†).

The antibody herceptin facilitates tyrosine kinase receptor HER2 degradation and is used clinically to treat aggressive breast cancer,<sup>20</sup> and was used here to demonstrate both cell labelling<sup>21</sup> and cargo amplification. Polymers conjugated to herceptin (**P1-Her**–**P5-Her**) were purified in 45–88% yields utilising the His-Tag (Fig. 2a and Table S2, ESI†), with SDS PAGE showing successful conjugation (Fig. S9, ESI†). When **P1-Her** was treated with tetrazine **Tz1** (Fig. 2a), intense fluorescent labelling of the antibody resulted, with selectivity between

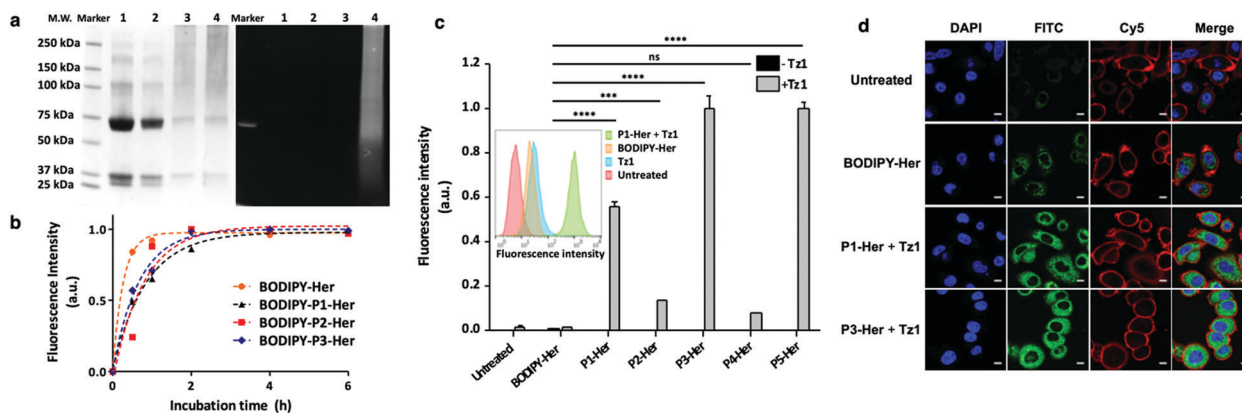
the polymer-tagged antibody and the unmodified variant observed (Fig. 3a, lane 2 *vs.* 4). In addition, SDS-PAGE analysis indicated that the majority of polymer conjugation took place on the heavy chains of the antibody. The influence of the polymers on the antibody's binding affinity was investigated by flow cytometry analysis of the labelling efficiency of the polymer–antibody conjugates on HER2 receptor positive breast cancer cells (SK-BR-3) with **BODIPY-P1-Her**, **BODIPY-P2-Her** and **BODIPY-P3-Her** and **BODIPY-Her**. Incubation of SK-BR-3 cells with small molecule labelled **BODIPY-Her** (Scheme S5, ESI†) resulted in rapid labelling of the cells with fluorescence saturation of cells observed after 2 h. Similar labelling and fluorescence saturation of cells was also observed by polymer conjugated antibodies **BODIPY-P2-Her** and **BODIPY-P3-Her**, whereas **BODIPY-P1-Her** showed slower labelling with fluorescence saturation reached after 4 h incubation (Fig. 3b). MCF-7 cells, which do not express the HER2 receptor, showed no significant changes in fluorescence intensity when incubated with the polymer–herceptin conjugates (Fig. S10, ESI†). None of the polymer–antibody conjugates (**P1-Her** to **P5-Her**), **BODIPY-Her** or **Tz1** showed cellular toxicity at 10 nM, 10 nM and 1  $\mu\text{M}$ , respectively (Fig. S11, ESI†).

The fluorescence “turn-on” and signal amplification with the polymer–antibody conjugates and tetrazine **Tz1** was demonstrated in live SK-BR-3 cells by flow cytometry and microscopy (Fig. 3c and d). Cells treated with **BODIPY-Her** (4 h, 10 nM) showed a moderate increase in fluorescence intensity; however, treatment with the conjugates **P1-Her** to **P5-Her** (4 h, 10 nM), followed by the quenched fluorophore **Tz1** (30 min, 1  $\mu\text{M}$ )





**Fig. 2** (a) Synthesis of the multifunctional polymers **P1–P5** and the ratios of **1**, **2** and DMA found in the synthesised polymers (based on  $^1\text{H}$  NMR analysis). All polymers were synthesised as random copolymers (see ESI† Table S1 for full characterisation). Polymer synthesis was followed by their antibody conjugation (10 eq. polymer per antibody added) and metal-affinity chromatography purification of the polymer–antibody conjugates (**P1-Her–P5-Her**) and subsequent  $\text{Cu}(\text{I})$  mediated dequenching to give the fluorescent conjugates. The NHS-conjugation strategy produces heterogenous polymer–antibody population, with multiple conjugation sites possible; however, only one modification site on the antibody is shown for clarity. (b) The tetrazines explored for signal amplification.



**Fig. 3** (a) SDS-PAGE showing successful conjugation and fluorescence “switch-on”. Lane 1 herceptin; lane 2 herceptin (2.5  $\mu\text{M}$ ) incubated with **Tz1** (25  $\mu\text{M}$ ); lane 3 **P1-Her** and lane 4 **P1-Her** (2.5  $\mu\text{M}$ ) incubated with **Tz1** (25  $\mu\text{M}$ ) (reaction mixtures were purified using centrifugal size exclusion filters prior to analysis). (b) Polymer–herceptin conjugate labelling of SK-BR-3 cells (quantified by flow cytometry with fluorescence intensity normalised to fluorescence saturated cells,  $n = 3$ ) compared to the traditional small molecule labelled herceptin BODIPY-Her (Scheme S5, ESI†). (c) Fluorescence intensity of HER2 receptor positive SK-BR-3 cells treated first with the polymer–herceptin conjugates (10 nM) followed by **Tz1** (1  $\mu\text{M}$ ) (normalised to cells treated with **P3-Her** followed by **Tz1**). The increase in fluorescence intensity between BODIPY-Her and BODIPY-labelled **P1–P5-Her** was 45, 10, 83, 6 and 83-fold, respectively. Inset: The flow cytometry histograms of SK-BR-3 cells treated with BODIPY labelled herceptin BODIPY-Her or **Tz1**, or the polymer–antibody conjugate **P1-Her** followed by **Tz1** (green). Data were analysed using one-way ANOVA with Dunnett post-test (ns, not significant,  $***P < 0.001$ ,  $****P < 0.0001$ ). (d) Confocal fluorescence microscopy images of SK-BR-3 cells treated with BODIPY-labelled herceptin BODIPY-Her (10 nM), and polymer–antibody conjugates **P1-Her** and **P3-Her** (10 nM) followed by **Tz1** (1  $\mu\text{M}$ ). The cell nucleus was stained with Hoechst 33342 (blue,  $\lambda_{\text{ex/em}} = 353/483$  nm) and the plasma membrane stained with CellMask™ Deep Red (red,  $\lambda_{\text{ex/em}} = 649/666$  nm). “Switched-on” BODIPY from **Tz1** is shown in green ( $\lambda_{\text{ex/em}} = 488/512$  nm). Scale bar = 10  $\mu\text{m}$ . The norbornene content and monomer ratios for **P1–P5** (based on  $^1\text{H}$  NMR analysis) are given in Fig. 2.



resulted in remarkable increases in cellular fluorescence (83-fold increase for **P3-Her** and **P5-Her**, compared to **BODIPY-Her**). The fluorescence intensity could be tuned by either changing the molecular weight of the polymers (45, 10 and 83-fold increases for **P1-Her**, **P2-Her** and **P3-Her**, respectively) or the density of the reactive centres (6 and 83-fold increase for **P4-Her** and **P5-Her**, bearing 2.8 and 18 norbornes per polymer chain, respectively). Confocal microscopy images of the cells treated with **P1-Her** and **P3-Her**, which had different numbers of reactive centres (8 vs. 21), followed by **Tz1** showed much brighter fluorescence ( $\lambda_{\text{ex/em}} = 488/512 \text{ nm}$ ) than **BODIPY-Her** treated cells, although with similar cellular localisations, i.e., cytoplasm and membrane (Fig. 3d and Fig. S12, ESI†).

This amplification method could also be translated to amplifying the loading density of radioisotopes.<sup>22</sup> As a proof of concept, **P5-Her** was pre-labelled with **Tz3** (Fig. 2a, Fig. S11 and Scheme S6, ESI†) bearing Cu(II) on a DOTA ligand (copper was used as a model as <sup>64</sup>Cu is widely used in nuclear medicine<sup>23</sup>). The amplified metal loading on SK-BR-3 cells was confirmed by inductively coupled plasma-mass spectrometry (ICP-MS) where the Cu(II) loaded polymer-antibody conjugate **Cu-P5-Her** showed a 6-fold higher copper loading (1.6 pg per cell) in comparison to the conventionally radiolabelled antibody **Cu-Her** (Fig. S14 and Scheme S7, ESI†).

In summary, a linear poly(acrylamide) scaffold bearing norbornenes and a His-Tag was synthesised, conjugated to a clinically used antibody herceptin, and used for fluorescence and metal amplification. Compared to the standard small molecule fluorophore labelled antibody, the polymer-antibody conjugates gave up to an 83-fold increase in fluorescence without affecting antibody binding. This approach of receptor targeted polymer conjugates enables simultaneous “switch-on” and amplification of fluorescent signal with possible contributions to fluorescence-guided surgery and other fluorescence-based applications, especially those where signals are inherently weak due to low numbers of receptors. The approach was applied to the amplification of metal loading with possible uses in nuclear medicine, but the designed polymer scaffold would also enable the “multiplication” of other molecules (e.g. drugs). The new His-Tag-RAFT agent provides a powerful new approach to access various functional polymers with an endogenous purification handle to enable the rapid and simple purification of both “graft-to” or “graft-from” polymer-conjugates.

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## Conflicts of interest

There are no conflicts to declare.

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