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# Rationally designed pure-inorganic upconversion nanoprobes for ultra-highly selective hydrogen sulfide imaging and elimination *in vivo*†

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Lung injury is a hydrogen sulfide (H<sub>2</sub>S)-associated complication with high mortality in acute pancreatitis (AP) cases. Herein, we used Prussian Blue (PB) as a H<sub>2</sub>S-responsive acceptor to develop a novel pure-inorganic upconversion nanoprobe for detecting and eliminating H<sub>2</sub>S, which can be used for diagnosing AP and alleviating lung injury. Upconversion nanoprobes with 5 nm PB shells were optimized to achieve outstanding *in vitro* H<sub>2</sub>S detection capacity (linear range: 0–150 μM, LOD: 50 nM), which met the *in vivo* serum H<sub>2</sub>S range, and thus were feasible for imaging H<sub>2</sub>S *in vivo*. More importantly, when combined with the traditional H<sub>2</sub>S synthetase inhibitor DL-PAG, the nanoprobes also served as a therapeutic agent that synergistically alleviated lung injury. As PB is an FDA-approved drug, our work proposes a potential clinical modality for the early diagnosis of AP, which will decrease lung injury-induced mortality and increase the survival rates of AP cases.

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## Introduction

Hydrogen sulfide (H<sub>2</sub>S) is a newly discovered gaseous signaling molecule, in addition to nitrogen oxide and carbon monoxide, and is an essential player in various physiological processes.<sup>1</sup> In acute pancreatitis (AP) cases, excessive serum H<sub>2</sub>S levels can cause lung injury, which leads to high early mortality rates due to respiratory failure and hypoxemia.<sup>2,3</sup> Therefore, developing a probe that can simultaneously image and eliminate H<sub>2</sub>S from serum would significantly benefit AP patients.

Luminescence probes can be applied to disease diagnostics due to their strong performance in time-resolution imaging and dynamic bioinformatics monitoring.<sup>4–11</sup> Among all phosphors, upconversion nanoparticles emit adjustable luminescence (300–800 nm) under near-infrared (NIR) excitation, and have the advantages of low background luminescence and high stability, which makes them ideal for *in vivo* luminescence imaging.<sup>12–16</sup> Therefore, upconversion nanoparticles are feasible for use as donors in construction of high-performance luminescence nanoprobes.<sup>17–21</sup> Using upconversion nanoparticles as donors and H<sub>2</sub>S-responsive acceptors, some upconversion nanoprobes for H<sub>2</sub>S detection and imaging have been developed based on Förster resonance energy transfer (FRET) and inner filter effects.<sup>22–24</sup> However, the typical H<sub>2</sub>S-responsive acceptors were organic dyes with obvious shortcomings, including low stability and hydrophobicity. In contrast,

inorganic acceptors have no such issues, but are limited by low H<sub>2</sub>S selectivity and potential toxicity to biosystems, which resulted in less research into inorganic acceptors. Thus, an exploration of biocompatible inorganic H<sub>2</sub>S-responsive acceptors with good selectivity and high stability should be conducted with the aim of developing nontoxic hydrophilic H<sub>2</sub>S nanoprobes.

Due to the strong interaction between Fe(II/III) and cyanide, Prussian Blue (PB) is ultra-stable when combined with various biomolecules, which contributes to its outstanding biocompatibility.<sup>25</sup> Nevertheless, a synchronous reaction between Fe(III) and H<sub>2</sub>S may cause the decomposition of PB in a H<sub>2</sub>S solution, which would result in decreased PB absorbance that can be used to colorimetrically detect H<sub>2</sub>S. When applying PB as a H<sub>2</sub>S-responsive acceptor to construct upconversion nanoprobes, the weakened absorbance in the visible and NIR ranges can also lead to upconversion luminescence (UCL) recovery, which can be used for luminescence detection of H<sub>2</sub>S. Conversely, PB can also eliminate free H<sub>2</sub>S in fluid by forming stable sulfur and sulfide compounds, which means that these nanoprobes could be a potential drug for eliminating excessive serum H<sub>2</sub>S. As PB is a US Food and Drug Administration (FDA)-approved drug for clinical use, PB-modified upconversion nanoprobes may be optimal inorganic nanoprobes that simultaneously image and eliminate H<sub>2</sub>S.

Herein, a novel PB-functionalized upconversion nanoprobe was developed for dual-modal colorimetric/luminescence H<sub>2</sub>S detection. The thickness of the PB shell was modulated to achieve the optimal detection capacity within the serum H<sub>2</sub>S concentration range. To ensure safety, the cytotoxicity, biocompatibility, and biobehavior of the as-optimized

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nanoprobes were carefully studied. Ultimately, the feasibility of the nanoprobes for imaging  $\text{H}_2\text{S}$  and alleviating lung injury was confirmed in an AP mouse model.

## Results and discussion

### Rationally designed upconversion nanoprobes for $\text{H}_2\text{S}$ detection

The PB-functionalized upconversion nanoprobes were rationally designed as a core-shell structure of 20% Er-doped  $\text{NaLuF}_4:\text{Yb,Er,Tm}@/\text{NaLuF}_4$  nanoparticles (UCNPs) coated with a homogeneous PB shell of optimal thickness. Using typical solvothermal methods, uniform core-shell UCNPs were synthesized with a larger size distribution ( $47.2 \pm 4.3$  nm) than that of  $\text{NaLuF}_4:\text{Yb,Er,Tm}$  cores ( $37.2 \pm 3.8$  nm; Fig. 1A and S1A and B†). After inner shell coating, the upconversion

luminescence (UCL) of UCNPs was significantly improved in both visible and NIR regions due to inhibition of multi-phonon relaxation between the emitter and the absorbed ligands (Fig. S1C†). Furthermore, X-ray diffraction (XRD) patterns suggested that the UCNPs were in a highly crystallized hexagonal phase, corresponding to the standard reference card of  $\beta\text{-NaLuF}_4$  (JCPDS: 027-0726; Fig. S2A†). High-resolution transmission electron microscopy (HR-TEM) images of UCNPs with a defined crystallographic plane supported this finding (Fig. 1B).

To obtain the as-designed nanoprobes, a PB shell was coated onto UCNPs (UC-PB) by the ligand-exchange and controllable complexation method.<sup>26</sup> After successful PB coating, the low contrast shell could be identified in both HR-TEM and scanning transmission electron microscopy (STEM) images (Fig. 1C and D). Energy dispersive X-ray analysis (EDXA) line scanning

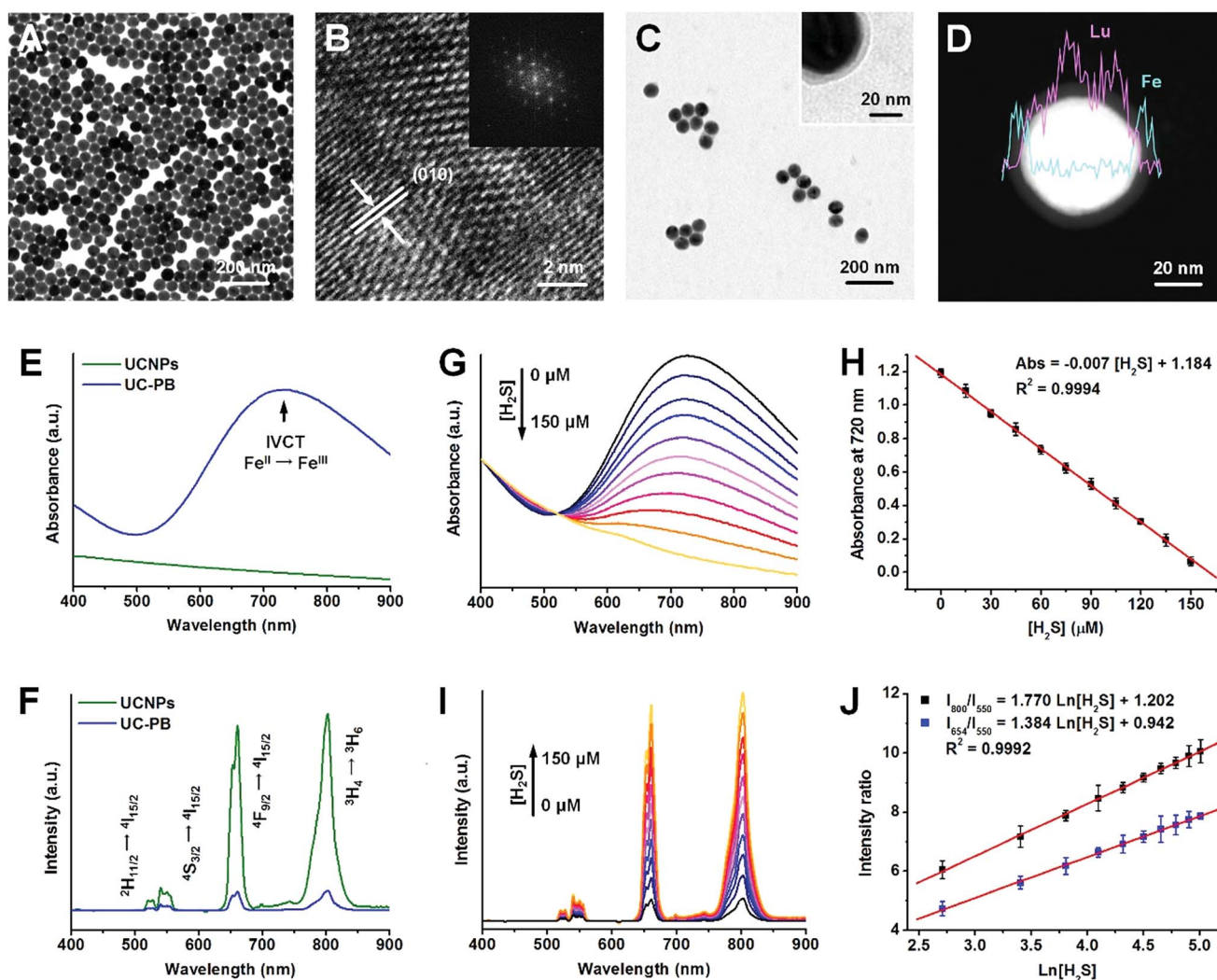


Fig. 1 Characterization and  $\text{H}_2\text{S}$  detection capacities of the UC-PB nanoprobes. TEM image (A) and high-resolution lattice image (B) of UCNPs. Inset: the corresponding fast Fourier transform diffractogram. (C) TEM image of the UC-PB nanoprobes. Inset: TEM image of a single UC-PB nanoprobe. (D) STEM image and EDXA line scan on a single UC-PB nanoprobe. UV-vis-NIR absorbance spectra (E) and UCL spectra (F) of UCNPs and UC-PB nanoprobes. UV-vis-NIR absorbance spectra (G) and UCL spectra (I) of UC-PB nanoprobes in response to various concentrations of  $\text{H}_2\text{S}$ . Linear relationship between absorbance at 720 nm (H) or between the UCL ratio (J) of UC-PB<sub>5</sub> nanoprobes and various concentrations of  $\text{H}_2\text{S}$ . Data are represented as mean  $\pm$  SD.



results found that Fe was well-distributed on the periphery of UCNPs, which further confirmed the existence of the PB shell on UCNP surfaces (Fig. 1D). Furthermore, a new diffraction peak was observed at the 2-theta range of 20–40 degrees, which corresponded to the (2,2,0) and (3,3,1) crystallographic planes of face-centered cubic PB (JCPDS: 52-1907) and indicated PB formation in the as-prepared nanoprobe (Fig. S2B†). The Fe peak in the EDXA spectrum and fabrication of cyanide bonds in the Fourier transform infrared (FTIR) spectrum also illustrated successful PB coating (Fig. S2C and D†). The as-prepared nanoprobe had a strong absorbance peak in the red (600–700 nm) and NIR (700–900 nm) ranges (Fig. S3†), which was attributed to the intervalence charge transfer between Fe(III) and Fe(II) in PB and caused remarkable UCL quenching of UCNPs through both Förster resonance energy transfer (FRET) and inner filter effects (Fig. 1E and F and S4A†). Compared with typical upconversion nanoparticles with relatively low Er dopant concentration (2% Er dopant, UCNPs-L), these UCNPs (20% Er dopant) had stronger UCL in the red and NIR regions, and higher red/green and NIR/green ratios, which were well matched with the absorbance range of PB, and thus were more feasible for constructing PB-functionalized upconversion nanoprobe (Fig. S4B–D†).

As the H<sub>2</sub>S concentration increased, the absorbance of PB decreased and the UCL of UCNPs recovered accordingly, owing to the decomposition of the PB shells in response to H<sub>2</sub>S (Fig. 1G and I). To study and optimize the influence of PB thickness on H<sub>2</sub>S detection performance, nanoprobe with 5 nm (UC-PB<sub>5</sub>), 8 nm (UC-PB<sub>8</sub>), and 11 nm (UC-PB<sub>11</sub>) PB shells were prepared by modulating the reactant ratio (Fig. S5A and B†). As the concentration of serum H<sub>2</sub>S is within the micromolar range (reported previously as 0–150 μM), the nanoprobe was optimized to be within this range. It was found that all three nanoprobe responded to H<sub>2</sub>S, while the UCNP itself had no response (Fig. S5C–E†), which highlighted the essential role of PB in the H<sub>2</sub>S-responsive nanoprobe. As changes in absorbance and UCL were highly correlated with the reacted PB ratio, nanoprobe with thinner PB shells showed higher H<sub>2</sub>S sensitivity. However, low levels of PB limited the detection range due to limiting amounts of the H<sub>2</sub>S responsive agent. When the PB shell was <5 nm, serum H<sub>2</sub>S concentrations were beyond the detection range of the nanoprobe (Fig. S5C–E†). Meanwhile, compared with nanoprobe with thicker shells, UC-PB<sub>5</sub> had larger signal changes and was significantly more sensitive in the same H<sub>2</sub>S concentration range. Therefore, to be within the serum H<sub>2</sub>S concentration ranges while achieving the balance between a wide detection range and high sensitivity, UC-PB<sub>5</sub> nanoprobe was selected. These results also demonstrated that the range and sensitivity of H<sub>2</sub>S detection could be easily modulated by changing the PB shell thickness, which demonstrated the great adaptability of the PB-functionalized nanoprobe.

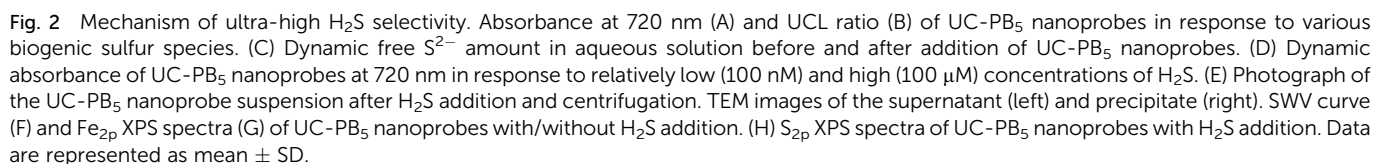
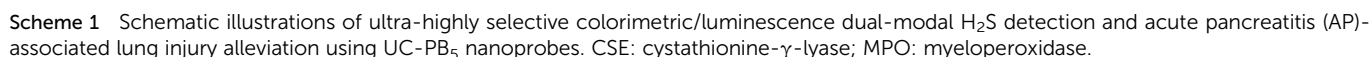
Since UC-PB<sub>5</sub> nanoprobe was optimized for H<sub>2</sub>S detection in clinical applications, a detailed evaluation of their performance was conducted. The concentration and absorbance at 720 nm of UC-PB<sub>5</sub> nanoprobe suspensions were quantified using ultraviolet-visible-near-infrared (UV-vis-NIR) spectra

before being used for detection. We found that the absorbance at 720 nm of a UC-PB<sub>5</sub> nanoprobe suspension was negatively correlated with H<sub>2</sub>S concentration at 0–150 μM (Abs. =  $1.184 - 0.007 \times [\text{H}_2\text{S}]/\mu\text{M}$ ,  $R^2 = 0.9994$ , LOD: 10 nM, Fig. 1H). Moreover, using the 550 nm UCL intensity as a reference, the relative 654 nm (abbreviated  $I_{654}/I_{550}$ ) and 800 nm (abbreviated  $I_{800}/I_{550}$ ) intensities were positively linearly correlated with  $\text{Ln}[\text{H}_2\text{S}]$  within the same range ( $I_{654}/I_{550} = 0.942 + 1.384 \times \text{Ln}[\text{H}_2\text{S}]/\mu\text{M}$ ,  $I_{800}/I_{550} = 1.202 + 1.770 \times \text{Ln}[\text{H}_2\text{S}]/\mu\text{M}$ ,  $R^2 = 0.9992$ , LOD: 10 nM, Fig. 1J). Compared with all previously reported upconversion nanoprobe for H<sub>2</sub>S detection, UC-PB<sub>5</sub> had a favorable detection capacity (Table S1†).<sup>23,24,27,28</sup> It is noteworthy that the reaction between UC-PB<sub>5</sub> and H<sub>2</sub>S reached equilibrium within a very short period (approximately 350 s for the spectra and 20 s for the naked eye, Fig. S6 and Video S1†), which indicated that UC-PB<sub>5</sub> was feasible for dynamic H<sub>2</sub>S detection. More importantly, UC-PB<sub>5</sub> nanoprobe was well-dispersed in various biological fluids and showed high stability after long-term storage (Fig. S7†). Therefore, UC-PB<sub>5</sub> can serve as a dual-modal colorimetric/luminescence probe with favorable biostability and H<sub>2</sub>S detection capacity (Scheme 1).

### Increased H<sub>2</sub>S selectivity from cooperative redox and combination reactions

Apart from its outstanding H<sub>2</sub>S detection capacity and high stability, we also noticed that UC-PB<sub>5</sub> had ultra-high selectivity for H<sub>2</sub>S among other biomolecules, including typical bio-reductants and bio-complexes (Fig. S8 and 9†). Moreover, UC-PB<sub>5</sub> also showed no response to other bio-sulfur species (typically biothiols, S<sub>2</sub>O<sub>3</sub><sup>2-</sup>, and SO<sub>3</sub><sup>2-</sup>), even at high concentrations (15 mM, 100-fold higher than [H<sub>2</sub>S]; Fig. 2A and B). To uncover the mechanism of this ultra-highly selective H<sub>2</sub>S detection, the reaction was monitored and products were characterized. After adding UC-PB<sub>5</sub> into a H<sub>2</sub>S solution, the free S<sup>2-</sup> concentration significantly decreased as a function of time, indicating that H<sub>2</sub>S may have reacted with UC-PB<sub>5</sub> (Fig. 2C). However, because ferrocyanide (also known as Prussian White, reduced PB) can be rapidly oxidized by dissolved oxygen in water, the single redox reaction between UC-PB<sub>5</sub> and H<sub>2</sub>S failed to achieve permanent PB decomposition according to dynamic absorbance spectra (Fig. 2D). Therefore, we concluded that the decomposition of PB by H<sub>2</sub>S involved cooperation of both redox and combination reactions. To confirm this hypothesis, the products were further characterized. TEM images showed that small nanostructures were formed after adding H<sub>2</sub>S, while PB shells were rugged and detached from UCNP surfaces (Fig. 2E). Square-wave voltammetry (SWV) curves and Fe<sub>2p</sub> X-ray photoelectron spectroscopy (XPS) spectra suggested that the Fe(III) in PB was the oxidation reaction center (Fig. 2F and G), while the S<sub>2p</sub> XPS spectra confirmed the existence of both sulfur and ferrous sulfide, demonstrating the simultaneous redox and combination reactions between UC-PB<sub>5</sub> and H<sub>2</sub>S (Fig. 2H). As there were two coordinated Fe(II) in the reduced form of PB (Fe(II)–C≡N– and Fe(II)–N≡C–), the combination reaction center was further identified by studying the reaction between H<sub>2</sub>S and other iron complexes. This showed that only sulfur was produced in the





reaction between ferricyanide (containing  $\text{Fe(III)}-\text{C}\equiv\text{N}^-$  in its reduced form) and  $\text{H}_2\text{S}$ , while both sulfur and ferrous sulfide were produced between ferric isothiocyanate (containing  $\text{Fe(III)}-\text{N}\equiv\text{C}-$  in its reduced form) and  $\text{H}_2\text{S}$ , which was attributed to the stronger coordinative interaction between  $\text{Fe(III)}$  and C than N in the  $-\text{C}\equiv\text{N}-$  structure (Fig. S11†). Above all, the ultra-highly selective  $\text{H}_2\text{S}$  detection using UC-PB<sub>5</sub> contributed to the permanent PB decomposition by the cooperation of redox and combination reactions between  $\text{H}_2\text{S}$  and PB. The nitrogen-coordinated Fe was either the oxidation or combination reaction center in PB that reacted with  $\text{H}_2\text{S}$ , resulting in the  $\text{H}_2\text{S}$ -responsiveness of PB.

### Ultra-highly selective ratiometric imaging of $\text{H}_2\text{S}$

By virtue of the fact that luminescence signals are essential resources for bioimaging, UC-PB<sub>5</sub> was a potential  $\text{H}_2\text{S}$ -responsive nanophosphor for imaging  $\text{H}_2\text{S}$  in cells and *in vivo*. The signal intensity obtained from luminescence imaging was also useful for evaluating the concentration of  $\text{H}_2\text{S}$  in regions or samples of interest. Before applying UC-PB<sub>5</sub> to further experimentation, its cytotoxicity and biocompatibility were carefully studied though the PB and upconversion nanoparticles were previously reported to be safe for bioapplications.<sup>29,30</sup> Both cell viability assays and SYTO-9/propidium iodide staining suggested that UC-PB<sub>5</sub> had no obvious cytotoxicity. It had relatively high  $\text{IC}_{50}$  values of  $4.05 \text{ mg kg}^{-1}$  and  $3.44 \text{ mg kg}^{-1}$  at 24 and 48 h, respectively (Fig. S12†). Furthermore, serological tests and tissue sections also suggested that UC-PB<sub>5</sub> had no negative influence on organ function or morphology, demonstrating its good *in vivo* biocompatibility (Fig. S13 and 14†). These results ensured the safety of UC-PB<sub>5</sub> in the subsequent studies.

It is known that  $\text{H}_2\text{S}$  can be produced from thiol-containing amino acids under the enzymatic catalysis of cystathionine- $\gamma$ -lyase (CSE).<sup>31</sup> However, DL-propargylglycine (DL-PAG) can irreversibly inhibit CSE by attacking the active-site Tyr<sup>114</sup> with its deprotonated  $\beta$ -position, resulting in reduced  $\text{H}_2\text{S}$  production.<sup>32</sup> In contrast, L-cysteine (L-Cys) and NaHS, which can serve as the substrate and product of this reaction, respectively, can correspondingly alter intracellular  $\text{H}_2\text{S}$  levels (Fig. S15A†). Thus, these biomolecules can modulate intracellular  $\text{H}_2\text{S}$  concentrations by simulating the environment and regulatory processes. Due to the correlation between the UCL ratio of nanoprobes and  $\text{H}_2\text{S}$  concentration, UC-PB<sub>5</sub> was feasible for evaluating changes in intracellular  $\text{H}_2\text{S}$  levels.

After incubation with UC-PB<sub>5</sub>, strong UCL was observed in the cytoplasm of living cells, which demonstrated that UC-PB<sub>5</sub> could be taken up by cells, which then accumulated  $\text{H}_2\text{S}$ -generated electrolytes (Fig. 3A). Dynamic imaging of intracellular  $\text{H}_2\text{S}$  also demonstrated that UC-PB<sub>5</sub> could rapidly and sensitively respond to changes in the  $\text{H}_2\text{S}$  concentration (Fig. 3B). By obtaining UCL intensities from the green ( $550 \pm 20 \text{ nm}$ , Abbr. G) and red ( $650 \pm 15 \text{ nm}$ , Abbr. R) channels of cells without pretreatment, a standard R/G ratio was calculated and set as the normal intracellular  $\text{H}_2\text{S}$  concentration ( $\text{R/G} = 6.28 \pm 0.36$ , Fig. S15B and C†), which corresponded to previous findings. Compared with cells without pretreatment, the R/G ratio ( $5.49 \pm 0.13$ ) in DL-PAG-pretreated cells was significantly lower.

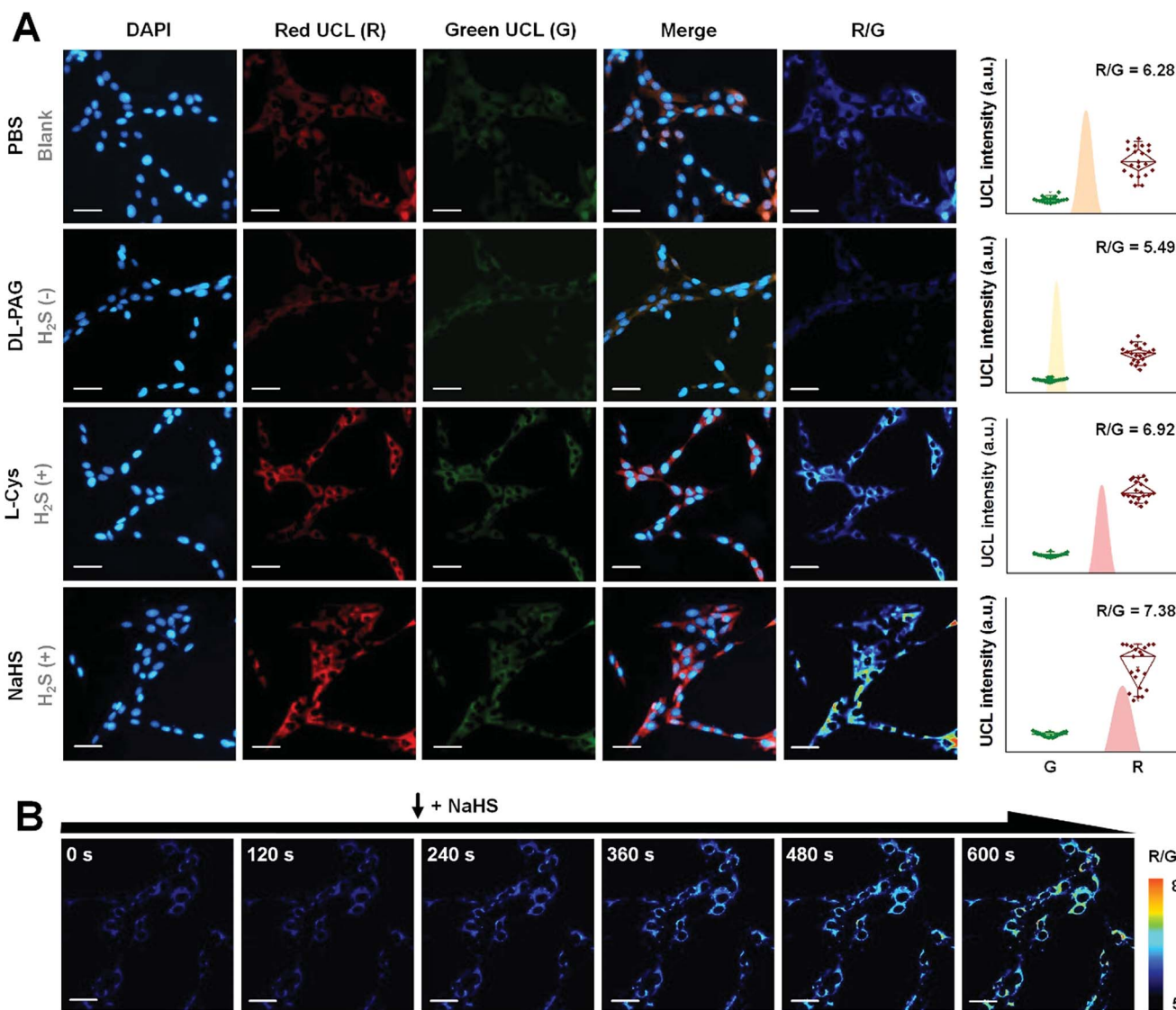
In contrast, L-Cys and NaHS pretreated cells had higher R/G ratios ( $6.92 \pm 0.35$  for L-Cys and  $7.38 \pm 0.59$  for NaHS) than non-pretreated cells (Fig. S15B†). Importantly, we also found that co-pretreated cells also had a lower  $\text{H}_2\text{S}$  concentration ( $\text{R/G} = 5.97 \pm 0.28$ ,  $^{**}p < 0.01$ ) than non-pretreated cells. These results confirmed that UC-PB<sub>5</sub> was applicable for the ratiometric imaging of intracellular  $\text{H}_2\text{S}$  and could evaluate intracellular  $\text{H}_2\text{S}$  concentrations *via* UCL ratios.

As excessive serum  $\text{H}_2\text{S}$  levels can be a potential factor for diagnosing AP, an AP mouse model was established and ratiometric UCL imaging was conducted to evaluate serum  $\text{H}_2\text{S}$  concentrations *in vivo* to verify the feasibility of the developed nanoprobes (Fig. 4A and B and S16†).<sup>33</sup> A strong UCL signal was observed in mice that received intravenous injections of UC-PB<sub>5</sub> (Fig. 4C). The UCL images of dissected organs suggested that UC-PB<sub>5</sub> primarily accumulated in the reticuloendothelial system of mice (Fig. S17†), which corresponded to the bio-distribution and metabolic pathway of UC-PB<sub>5</sub> (Fig. S18†). It was clear that the UCL signals collected in both the NIR ( $800 \pm 12 \text{ nm}$ , Abbr. N) and green ( $550 \pm 20 \text{ nm}$ , Abbr. G) ranges from AP mice were higher than those from normal mice. The N/G ratio of AP mice was also significantly higher than that of normal mice ( $\text{N/G} = 9.28 \pm 0.69$  vs.  $7.26 \pm 0.75$ ,  $^{***}p < 0.001$ ; Fig. 4D). The strong UCL signal and high N/G ratio found in AP mice were attributed to the UCL recovery caused by the reaction between UC-PB<sub>5</sub> and high serum  $\text{H}_2\text{S}$  levels, which suggested that UC-PB<sub>5</sub> was a potential tool for diagnosing AP. More importantly, the CSE-inhibition effect of DL-PAG was also observed by UCL imaging *in vivo*. At 12 h post-injection of DL-PAG, the N/G ratio was decreased ( $\text{N/G} = 7.89 \pm 0.86$ ,  $^{***}p < 0.001$ ) and significantly different compared with that of AP mice that received PBS. These results were in accordance with the studies of cultured cells and indicated that CES activity in AP mice could be effectively inhibited by DL-PAG. These results demonstrated the feasibility of using UC-PB<sub>5</sub> nanoprobes to evaluate  $\text{H}_2\text{S}$  concentration in cells and *in vivo* by ratiometric imaging, as well as their potential for diagnosing AP.

### Alleviating AP-associated lung injury *in vivo* by $\text{H}_2\text{S}$ elimination

Excessive serum  $\text{H}_2\text{S}$  levels in AP lead to various complications that can be even worse than AP itself.<sup>34</sup> Among these complications,  $\text{H}_2\text{S}$ -induced lung injury, including pneumonitis and acute respiratory distress syndrome, are the most serious and are directly responsible for the high early mortality rates in AP cases.<sup>35</sup> Therefore, simultaneously inhibiting  $\text{H}_2\text{S}$  production and eliminating  $\text{H}_2\text{S}$  serum could improve early survival rates.<sup>36</sup> However, traditional  $\text{H}_2\text{S}$  synthetase inhibitors like DL-PAG are slow-acting and cannot eliminate  $\text{H}_2\text{S}$  from serum.<sup>37</sup> To meet the requirements of clinical practice and overcome the limitations of  $\text{H}_2\text{S}$  synthetase inhibitors, it is essential to develop drugs with rapid  $\text{H}_2\text{S}$  elimination capacity. According to the results obtained from  $\text{H}_2\text{S}$  detection *in vitro* and  $\text{H}_2\text{S}$  imaging *in vivo*, the as-designed UC-PB<sub>5</sub> nanoprobes could rapidly react with  $\text{H}_2\text{S}$ , and thus are expected to eliminate serum  $\text{H}_2\text{S}$  within a short period with high efficiency, which would be



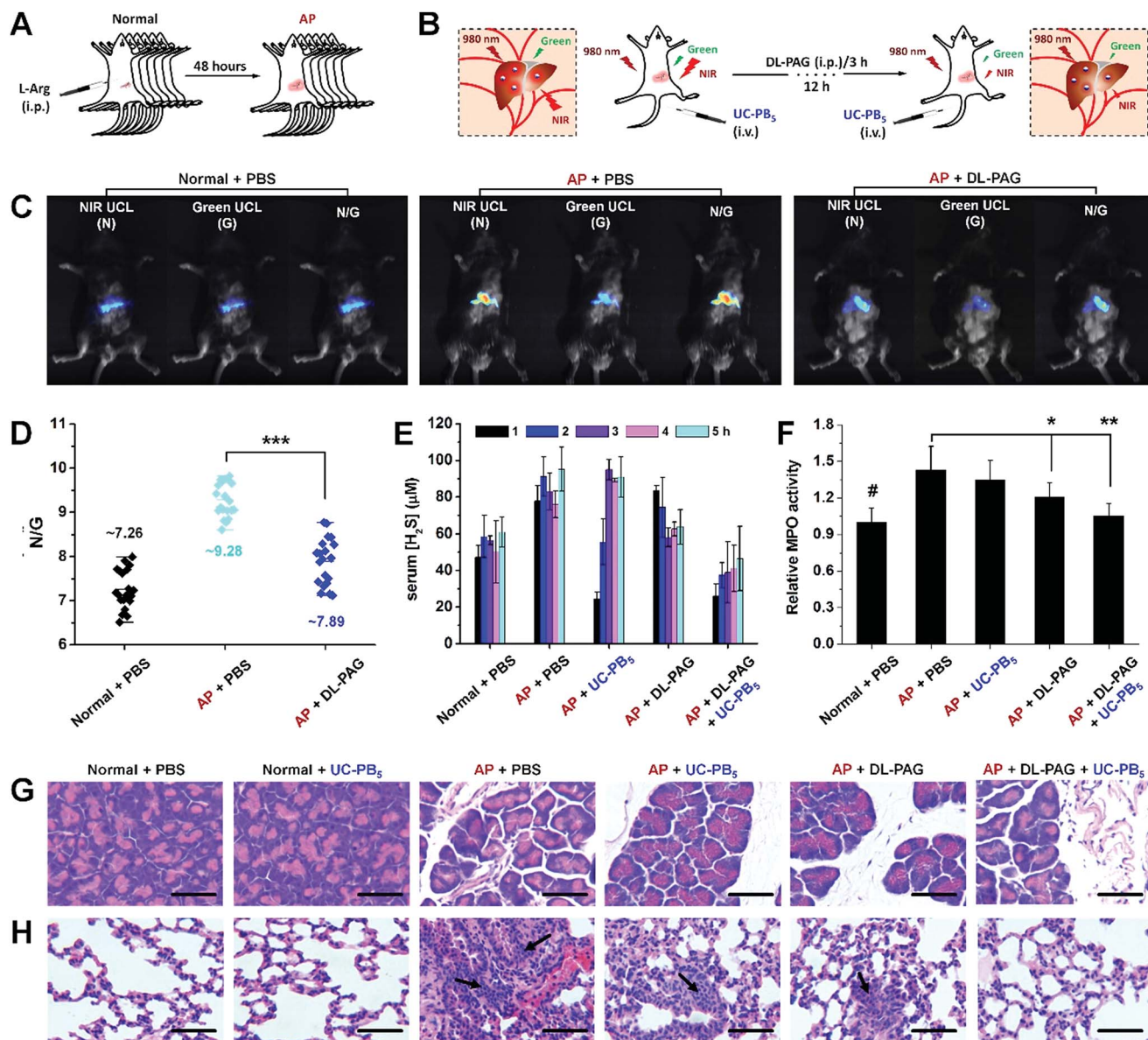


**Fig. 3** Evaluation of the intracellular H<sub>2</sub>S level by ultra-highly selective ratiometric imaging. (A) Luminescence images of A549 cells after various pre-treatments and incubation with UC-PB<sub>5</sub> nanoprobes. The nucleus was stained with commercial DAPI staining solution. The ratiometric luminescence images and R/G ratios were calculated from signals collected from the red channel (R) and green channel (G). The corresponding statistics of UCL signal intensity and calculated R/G ratios are also presented. (B) Dynamic ratiometric luminescence images of A549 cells incubated with UC-PB<sub>5</sub> nanoprobes before and after NaHS addition. The scale bar was 20  $\mu$ m.

complementary to inhibitor-based drugs (Fig. S19A†). To test the H<sub>2</sub>S-elimination effect of UC-PB<sub>5</sub>, serum H<sub>2</sub>S concentrations were determined in AP mice that received UC-PB<sub>5</sub> nanoprobe injections. These data showed that serum H<sub>2</sub>S levels in AP mice that received DL-PAG decreased continuously over the first 3 h and remained lower than those in untreated AP mice for the next 2 h. Furthermore, serum H<sub>2</sub>S levels in AP mice that received UC-PB<sub>5</sub> were significantly reduced over the first 2 h of post-injection, which suggested that UC-PB<sub>5</sub> rapidly affected serum H<sub>2</sub>S levels after intravenous injection (Fig. 4E). To test for synergistic effects of UC-PB<sub>5</sub> and DL-PAG on H<sub>2</sub>S levels, AP mice were co-injected with the two agents. Interestingly, serum H<sub>2</sub>S levels were close to the levels in control mice over the study period, which demonstrated that UC-PB<sub>5</sub> and DL-PAG synergistically eliminated H<sub>2</sub>S from serum.

In most cases, H<sub>2</sub>S-induced lung injury is associated with abnormal myeloperoxidase (MPO) activation in the lungs, which results in the overproduction of hypochlorous acids and oxidative damage.<sup>38</sup> Thus, pulmonary MPO activity was also determined to further illustrate the synergy between UC-PB<sub>5</sub> and DL-PAG in alleviating lung injury (Fig. 4F). These data demonstrated that MPO activity was significantly decreased in the lungs of AP mice that received both treatments compared with those that received no or single treatment (UC-PB<sub>5</sub> nanoprobes or DL-PAG), and was correlated with the decreased serum H<sub>2</sub>S levels; hematoxylin and eosin-stained sections also supported these findings (Fig. 4G and H). Lungs harvested from mice that received both treatments had reduced inflammatory reactions and milder pulmonary interstitial edema at the same time points compared with the other mice (Fig. S19B†). These





**Fig. 4** Evaluation of the serum  $\text{H}_2\text{S}$  level and alleviation of AP-associated lung injury *in vivo*. Schematic illustrations of AP model establishment (A) and theranostics experiments (B). Luminescence images (C) and UCL ratio (D) obtained from mice after various pre-treatments and intravenous injection of UC-PB<sub>5</sub> nanoparticles. (E)  $\text{H}_2\text{S}$  concentration in serum of mice that received various treatments in the course of 5 h. (F) Relative MPO activity in the lungs of mice that received various treatments. H&E-stained sections of pancreases (G) and lungs (H) harvested from mice that received various treatments. Statistical significance was determined from one-way *t* tests. \**p* < 0.05, \*\**p* < 0.01, and \*\*\**p* < 0.001. The scale bar was 50  $\mu\text{m}$ . L-Arg: L-arginine; #: the group as the standard of normalization. Data are represented as mean  $\pm$  SD.

results suggested that co-treatment with UC-PB<sub>5</sub> and DL-PAG synergistically alleviated AP-associated lung injury by eliminating  $\text{H}_2\text{S}$  from serum and inhibiting  $\text{H}_2\text{S}$  production, respectively.

## Conclusion

In summary, rationally designed pure-inorganic upconversion nanoparticles using PB as a  $\text{H}_2\text{S}$ -responsive acceptor were developed for sensitive and ultra-highly selective  $\text{H}_2\text{S}$  detection, imaging, and elimination. To meet the serum  $\text{H}_2\text{S}$  concentration range, upconversion nanoparticles with 5 nm PB shells

(UC-PB<sub>5</sub>) were optimized for *in vivo* studies. The UC-PB<sub>5</sub> nanoparticles not only possessed outstanding  $\text{H}_2\text{S}$  detection capacity *in vitro* (linear range: 0–150  $\mu\text{M}$ , LOD: 50 nM), but were also feasible for  $\text{H}_2\text{S}$  imaging in cells and in an AP mouse model. Moreover, the rapid  $\text{H}_2\text{S}$  elimination by UC-PB<sub>5</sub>, in cooperation with the long-term inhibition of  $\text{H}_2\text{S}$  production by DL-PAG, effectively inhibited  $\text{H}_2\text{S}$ -associated MPO activation, which further reduced the oxidative stress in the lungs, alleviating AP-associated lung injury. As PB is an approved drug, our work highlights its great potential for clinical AP treatment by alleviating lung injury, which could reduce the early mortality rate of AP.



## Author contributions

Y. L. and J. Z. conceived the project, analyzed the results, and wrote the original manuscript. All authors contributed to the preparation of the original and revised manuscripts. Y. L., Q. J., and X. Z. synthesized the UC-PB nanoprobles. Y. L., A. J., and F. M. investigated the characteristics of the UC-PB nanoprobles. Y. L. and X. Z. performed UCL imaging *in vitro* and *in vivo*. Y. L. and Q. J. conducted the other experiments.

## Conflicts of interest

There are no conflicts to declare.

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