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Inkjet assisted fabrication of planar biocompatible memristors

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In this study we address a novel design of a planar memristor and investigate its biocompatibility. An experimental prototype of the proposed memristor assembly has been manufactured using a hybrid nanofabrication method, combining sputtering of electrodes, patterning the insulating trenches, and filling them with a memristive substance. To pattern the insulating trenches, we have examined two nanofabrication techniques employing either a focused ion beam or a cantilever tip of an atomic force microscope. Inkjet printing has been used to fill the trenches with the functional titania ink. The experimental prototypes have qualitatively demonstrated memristive current–voltage behavior, as well as high biocompatibility.

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Introduction

Memristors are passive two-terminal elements of an electric circuit, whose resistance depends on the previously passed electric current. Their history started from the prediction of a hypothetically “missing circuit element” by Leon Chua in 1971¹ and nowadays has reached a slightly revised concept, basically meaning “the resistance switching memory”.² The memory effect of resistive switching is observed in many organic and inorganic nanomaterials, including simple oxides and their modifications.^{3–7} This allows integration of memristors into micro- and nanoelectronic devices using traditional nanofabrication techniques.^{8–10} Nowadays, memristors are considered to be one of the key elements of newly developing neuromorphic electronics,^{11,12} since it functionally mimics the synaptic plasticity of biological neurons^{13–15} and thus is suitable for bioinspired technologies.^{14,16,17}

Neuromorphic electronics was triggered by the discovery of principal electric phenomena in a neuron cell membrane in the early 1950's. In particular, the resistive switching model of the voltage gated ionic channels described by Hodgkin and Huxley in their Nobel prize awarded research¹⁵ gave rise to numerous electrical and computational prototypes of neural networks that were known since early 1960's.^{18,19} Nowadays, there is a growing interest in functional interfaces between biological and

artificial neural networks. This interest arises from two general research trends: adapting digital computational processes to native information processing mechanisms^{20,21} and investigation of the functional reserves of the biological neural networks.^{22,23} From the technological point of view, the electronic resistive switching memory is the common feature belonging to both biological and artificial electrical neurons. As such, it is considered as the frontier of feasible bionano interfaces. The state of the art and future expectations in this field have recently been outlined in a topical review.²⁴

Nowadays, *in vitro* studies of electrical activity in neuronal and other biological cells require special microelectrode arrays²⁵ and thus external wiring is needed to establish connection with a control unit or a memristive device.²⁶ Alternatively, microelectrodes and memristive elements can be integrated into one device. In the most common topological arrangement, memristors are fabricated as a dielectric thin film sandwiched between the transverse arrays of top and bottom electrodes (so-called “crossbar latch”). This configuration is a key architecture proposed for integrated nanoscale electronics.²⁷ Integration of crossbar memristors with the outer microelectrode array for *in vitro* experiments with biological cells or tissues would require an additional insulating layer and conductive channels between the inner and outer electrodes. This can be fabricated using conventional lithography. Alternatively, a layout with planar topology can be designed. Recently, several studies addressed the planar configuration of memristive elements.^{28–30} These elements were technologically performed using photolithography, leaving gaps between the pairs of metallic electrodes and filling them with a memristive composite. The gaps widths were reported to range from 10 μm ^{28,29} to 50–200 μm .³⁰ To achieve the memristive effect

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between so far distant electrodes, the authors used dielectric nanocomposite materials with silver nanoparticles. The use of silver nanoclusters allows for memristive effect based on reversible generation of conductive filaments through the electrically induced diffusive mechanism.³¹ However, the use of silver nanoparticles in biocompatible devices is risky, as their reported cytotoxicity at the cell level may be an issue.³² In this regard, an interesting solution would be the use of other than silver-based compounds with metal nanoclusters capable for realizing the same type of diffusive mechanism of memristivity. Recently, a promising effect of electroforming in gold nanoclusters has been demonstrated on a planar memristor prototype (3 mm × 3 mm) fabricated by supersonic cluster beam deposition.³³

The micrometer-scale resolution for the planar patterning of the diffusive-type memristors can be achieved by the conventional mask lithography. The use of mask lithography is however limited for *in situ* biological studies, so all the operations are allowed only prior to deposition of biological cells.

An alternative choice of planar memristive elements is represented by various metal oxides, whose memristance is based on the ionic drift mechanism.^{4,34–36} However, their realization requires much thinner dielectric layer, as the theoretical memristance of the ionic drift system is shown to be inverse square dependent on the distance between the electrodes.⁴ In this case, however, the use of conventional mask lithography meets aberration challenges and thus becomes costly.

In this study, we propose a hybrid nanofabrication method for planar memristors, comprising the nanoscale patterning of insulating trenches by atomic force microscopy (AFM) and inkjet printing of the functional ink. This combination allows accurate manipulations at ambient environment and as such is prospective for designing, engineering, and prototyping electrical circuits with biological cells or tissues, both prior to and after their deposition. A prototype device with a series of memristor elements has been manufactured accordingly and thoroughly investigated. In order to investigate the biocompatibility of the materials used in the prototype, an assay for their biocompatibility has been performed using both neuronal (IMR-32, neuroblastoma) and non-neuronal (PHF, postnatal human fibroblasts) cell lines. Next, we report the main processing features for the elaborated prototype, the functional behaviour, and discuss the applicability, challenges, and further prospects of the proposed fabrication technique.

Materials and methods

Device outline

The concept of the proposed planar memristor element is as follows: a thin layer of metallic electrode is deposited on a glass substrate. The shape of the electrode has a narrow bottleneck area in the middle, where a thin trench across the electrode is formed. The depth of the trench overcomes the electrode thickness, so that the resulting narrow gap splits the original electrode into two terminals. Then the gap is filled by a memristive dielectric substance.

In our prototype samples, five memristor elements with planar Au–TiO₂–Au sandwiches were fabricated on the surface of glass substrates (size 76 mm × 25 mm × 1 mm, roughness <0.15 μm, Levenhuk, Russia). The electrodes were deposited by gold sputtering, while their shapes were profiled by photolithography. The electrode separating trenches were made by scratching with a cantilever tip of an atomic force microscope (AFM). In addition, a reference series of memristive elements were prepared with trenches made by focused ion beam (FIB) milling. The resulting gaps between the electrodes were filled with titanium dioxide ink, using a laboratory scale inkjet printer. The AFM-based fabrication process is schematically shown in Fig. 1. In the following subsections, the main processing steps will be described in detail.

Electrode fabrication. The glass substrate was washed with a detergent, deionized water, and acetone, and then dried in oven at 110 °C for 30 min. A sequence of 3 nm chromium and 30 nm gold layers were sputtered on the substrate. The chromium intermediate layer was used for improving adhesion between gold and glass. The shapes of the electrodes were formed using photolithography. A positive photoresist (AZ 1505) was spin-coated on the gold surface. The surface patterning was performed using G-line lithography with a wavelength of 436 nm. The unprotected part of the gold layer was removed by wet etching in a 1 wt% aqueous KCN solution for 20 s at 25 °C. The remaining chromium layer was etched in a Cr etchant (CR-7) for 10 s at 25 °C. The protecting layer of the photoresist was removed in a bath with photoresist remover (AZ400T) taken at 50 °C for 1 h. The result is shown in Fig. 2.

Trench forming. The electrode separating gaps were formed as thin trenches crossing the gold layers at their narrowest “bottleneck” areas.

The trenches of the first type were made mechanically, by scratching the gold surface with a cantilever tip of a scanning probe microscope (SPM) Ntegra Aura (NT-MDT, Russia), operating in the AFM contact mode. The cantilever was chosen with a hardness of 22 N m^{−1} (NT-MDT, Russia) and a tip curvature radius of 10 nm. The scratching force was estimated as:

$$F = \Delta Zk$$

where ΔZ is the deflection of the probe between two fixed points, and k is the stiffness of the cantilever. A calibration

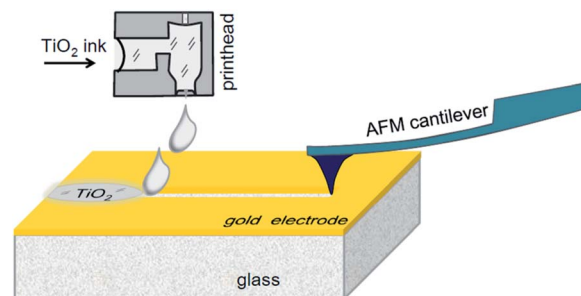


Fig. 1 Scheme for hybrid fabrication of a planar memristor.



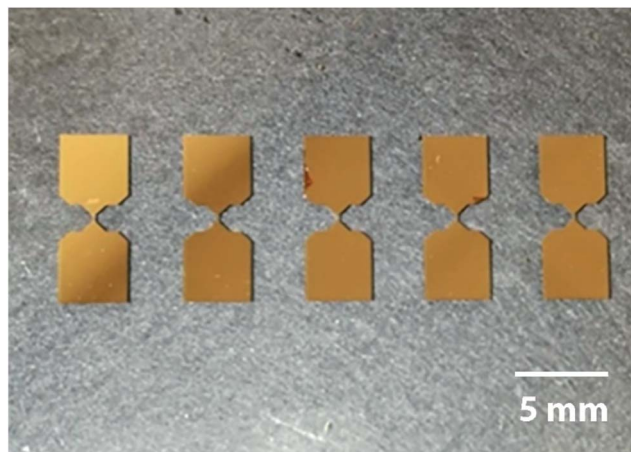


Fig. 2 Gold-sputtered electrodes.

routine³⁷ with standard silicon semi-contact probes was performed prior to main operations.

The trenches of the second type were etched by a focused ion beam of Ga using a Carl Zeiss Neon 40 Cross-Beam workstation. Acceleration voltage and current in the beam column were 30 kV and 10 pA, correspondingly.

Trench filling. The trenches separating the electrodes were filled with titania (TiO₂) nanoparticles dispersed in a sol and deposited by inkjet printing. Titania nanoparticles were derived by sol-gel process. The sol was obtained by hydrolysis of titanium(IV) isopropoxide (TIP) (97%, Sigma-Aldrich) in deionized water (<5 μS cm⁻¹) under vigorous stirring (1000 rpm), while nitric acid (65%, Sigma-Aldrich) was used for protonating. The whole processing route is described in detail elsewhere.³⁸ The resulting colloid was stable, with typical characteristics of zeta potential *ca.* 20 mV and the average hydrodynamic radius of particles 9.2 ± 0.9 nm, in agreement with the previous report.³⁹

The synthesized sol was processed in a rotary evaporator until the solid TiO₂ phase was obtained. Then the ink was derived by diluting TiO₂ nanoparticles in deionized water and adding ethylene glycol and a surfactant DX4000 in order to adjust the surface tension and viscosity of the ink solution. The ink rheological properties were adjusted to comply with the technological printing environment (the printhead nozzle diameter and the desirable droplet volume).

The phase composition and crystallinity of the prepared titania ink were characterized by X-ray diffraction and gas sorption methods, using a Rigaku SmartLab 3 diffractometer (CuKα radiation, λ = 1.5418 Å) and a Quantachrome Nova 1200e surface area analyser, respectively. The surface area and the average pore diameters were estimated using the models by Brunauer–Emmett–Teller (BET) and Barrett–Joyner–Halenda, (BJH) respectively.

The prepared TiO₂ ink was decanted into a cartridge and inkjet deposited onto the trenches by inkjet printing. A Fujifilm Dimatix materials printer DMP-2831 with a 10 pL cartridge was used. The printing conditions were set as follows: temperature of the substrate 35 °C, nozzle driving voltage 22 mV, drop spacing 25 μm, and 1 mm sample-to-printhead distance.

Annealing. The prepared films were dried for 1 day at room temperature, then annealed in an air oven at 200 °C for 2 hours, as suggested in previous studies.^{40,41}

Characterization

The quality of trench forming was controlled by the means of atomic force microscopy (AFM) and scanning electron microscopy (SEM), while the final device prototypes were subjected to electric characterization, as well as to cell viability assay, using the standard methylthiazol tetrazolium (MTT) test protocol.

AFM and SEM imaging. The AFM images were obtained using a scanning probe microscope (SPM) Ntegra Aura (NT-MDT, Russia) operating in the AFM contact mode.

An additional visualization of microstructure was obtained using a scanning electron microscope (SEM) Tescan Vega 3 with a beam accelerating voltage of 20 kV, operating with a secondary electron detector.

Electrical characterization. Electrical characterization of the planar memristor elements was performed using a Sub-Femtoamp Remote SourceMeter Keithley 6430 operating in standard two-point regime and KickStart Instrument Control Software Version 2.0.6 (Tektronix). The measurements of electric current were taken by applying a dc voltage sweep from 0 to 5 V stepwise, with a step value of 0.05 V and a settling time of 0.01 s. All the electrical characterizations were performed at room temperature and normal atmospheric conditions.

Cytotoxicity assay. To assess the cytotoxicity of materials used in the memristor device, a series of samples coated with sputtered Au, as well as samples coated with TiO₂ ink were prepared separately and placed into clear 96-well flat-bottom plates (Eppendorf). An additional empty plate was reserved for the control test. The cells of neuroblastoma (IMR-32, ATCC® CCL-127™, USA) and postnatal human fibroblast (PHF, Institute of Cytology RAS, Russia) lines were taken each in a quantity of 5 × 10³ and seeded in the prepared 96-well plates with the samples, as well as in the control one. The cell viability was measured using the standard methylthiazol tetrazolium (MTT) assay.⁴² In brief, the cells were incubated for 72 h at 37 °C. The incubated product was tested by adding 0.2 mL of MTT (5 mg mL⁻¹) for 2 hours, then the MTT-formazan product was dissolved in 0.2 mL of DMSO and the optical absorbance was measured at 570 nm using a plate reader Infinite F50 (Tecan). To improve cells visibility, trypan blue solution (0.4 wt%) was added as cell stain. The experimental reproducibility was provided with three individual batches prepared for each of the experimental tests.

Results and discussion

Topology

Profiling of the trench by an AFM cantilever tip requires adjustment of scratching force and speed towards the optimal regime. In this study we have investigated the relationships between the applied scratching force and the profile of the resulting trench in the gold layer. The results are shown in Fig. 3. Fig. 3a illustrates the AFM images for a series of trenches



obtained at forces of 2, 5, 8, 12, 15, and 20 μN , while the corresponding depth profiles are shown in Fig. 3b. The topology parameters of obtained trenches are listed in Table 1. The results demonstrate that the scratching efficiency changes drastically when the applied force is sufficient to break through the whole layer. In the case of 30 nm gold film, this was achieved at 20 μN .

The optimal scratching speed of 3 $\mu\text{m s}^{-1}$ has been found empirically. At a higher speed, scratching was accompanied with a ploughing effect, while speed lowering only resulted in longer processing time.

Fig. 4 compares the trenches obtained by AFM scratching (Fig. 4a) and FIB etching (Fig. 4b). It is noteworthy that the shape of the AFM-processed trench is strongly affected by the geometry of the cantilever tip, so that it is narrow at the bottom (*ca.* 150–200 nm) and broadening towards the top (*ca.* 700–800 nm). In contrast, the FIB-etched trench has regular rectangularly shaped profile, *ca.* 400 nm width (Fig. 4b).

Dielectric layer

Sol-gel synthesis of TiO_2 nanoparticles is a low temperature process with a possibility to control the phase ratio of different polymorphs as well as the morphology by adjusting parameters of acidic peptization in an aqueous solution.³⁹ In this study we used the regime of synthesis previously adjusted to meet the rheological requirements for inkjet printing.^{38,43} XRD pattern of the derived ink is shown in Fig. 5. The synthesized nanoparticles are predominantly identified as anatase (JSPDS card #21-1272), while some traces of brookite have also been detected (JSPDS card #29-1360); no rutile (JSPDS card #21-1276) is observed. Anatase is the well suitable TiO_2 polymorph for memristive application that has been demonstrated in a series of theoretical⁴⁴ and experimental^{45–47} studies. The average crystallite size by Scherer's equation was *ca.* 6 nm upon heat treatment at 50 $^\circ\text{C}$ and *ca.* 7 nm after treatment at 200 $^\circ\text{C}$. The BET

Table 1 Topology of trenches at various forces

Scratch number, Fig. 3a	Force, μN	Width at middle, nm	Depth, nm
1	2	300 ± 100	1.5 ± 0.5
2	5	400 ± 100	8.5 ± 0.5
3	8	400 ± 100	8.5 ± 0.5
4	12	500 ± 100	8.5 ± 0.5
5	15	500 ± 100	8.5 ± 0.5
6	20	500 ± 100	30.0 ± 2.0

surface area was evaluated as 159 $\text{m}^2 \text{g}^{-1}$ and 144 $\text{m}^2 \text{g}^{-1}$ with the BJH average pore diameters 3.2 nm and 3.5 nm for the samples treated at 50 $^\circ\text{C}$ and 200 $^\circ\text{C}$, respectively.

Fig. 6 demonstrates the result of trench filling by inkjet deposition, followed by annealing. As visible in Fig. 6a, the titania ink droplets are deposited precisely on the trenches. The SEM image shown in Fig. 6b demonstrates the droplet morphology. It forms a compact film with little roughness.

Electric characterization

The planar $\text{Au}/\text{TiO}_2/\text{Au}$ memristors were characterized by current-voltage dependencies at several measurement cycles with stepwise increasing and decreasing driving voltage. The results are shown in Fig. 7. All the memristive elements demonstrated rather very low current response, ranging from a few to hundreds nanoamperes, which may be a result of incomplete or loose filling of the narrow trenches with TiO_2 ink and the relatively low crystallinity of titania. Despite this, the U-I dependencies demonstrate the qualitatively memristive behaviour with gradually increasing conductivity at each subsequent unipolar cycle of the applied dc voltage. No electric response

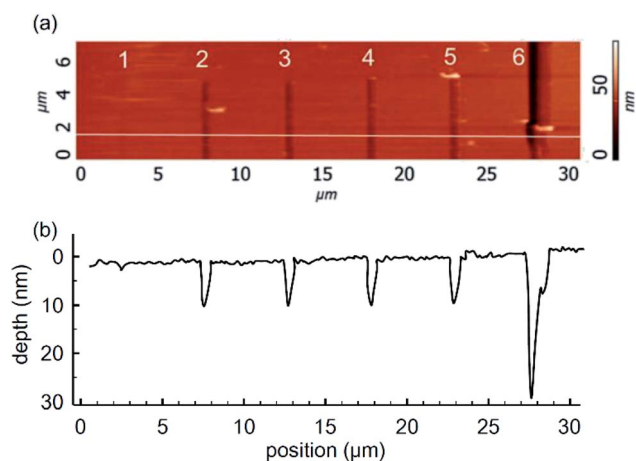


Fig. 3 (a) AFM images of trenches formed with cantilever forces of 2, 5, 8, 12, 15, and 20 μN ; and (b) the corresponding depth profiles.

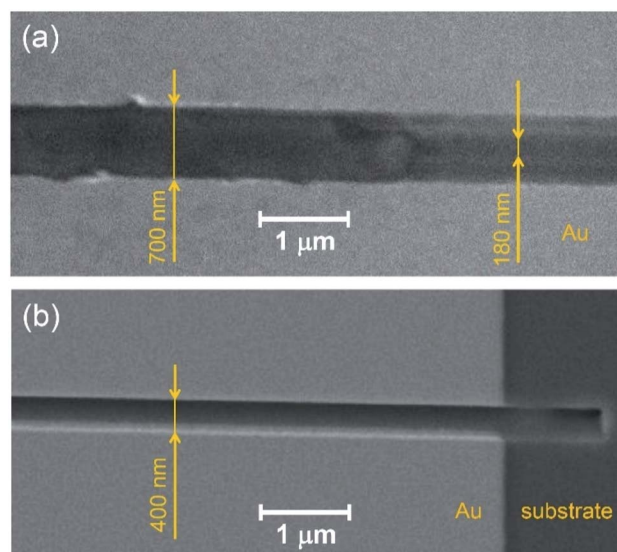


Fig. 4 SEM images of trenches prepared by (a) AFM scratching and (b) FIB etching.



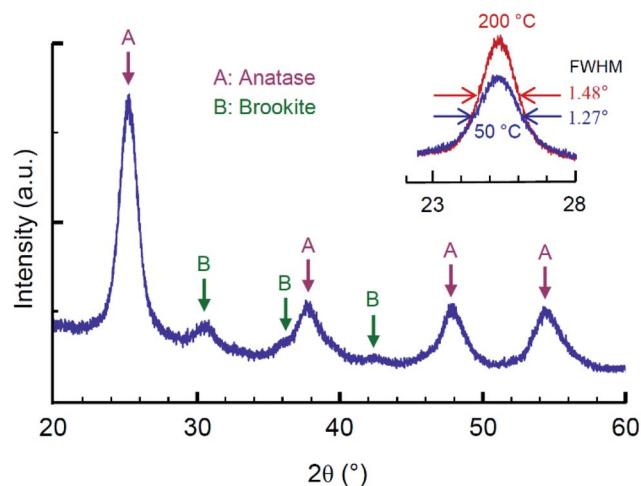


Fig. 5 XRD pattern for sol-gel derived TiO_2 ink; the inset shows peaks for materials thermally annealed at 50 °C and 200 °C.

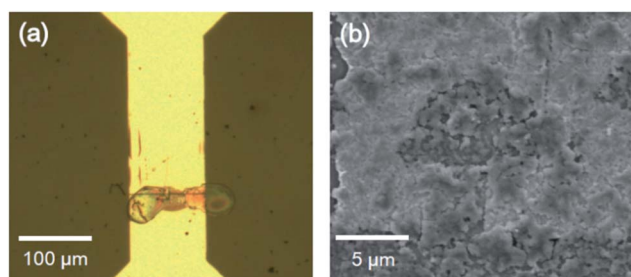


Fig. 6 Images of TiO_2 droplets deposited on trench: (a) optical microscopy; and (b) SEM.

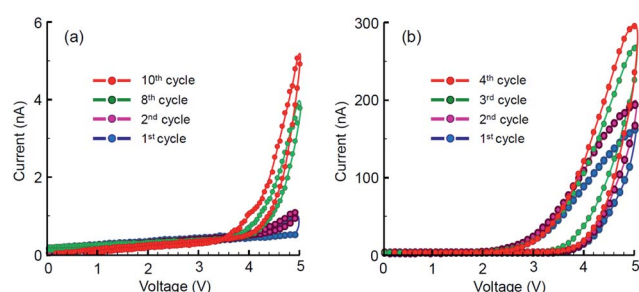


Fig. 7 Current-voltage potentiation curves for a sequence of unipolar cycles applied to memristors prepared with: (a) AFM-scratched trench and (b) FIB-etched trench.

was detected prior to filling the trench with titania ink. The threshold voltages igniting the memristive potentiation were 4.2 V in the case of AFM-made trench (Fig. 7a) and 3.0 V in the case of FIB-made trench (Fig. 7b), which correspond to the difference in their widths (Fig. 4a and b). Owing to proper rectangular shape of the FIB-made trench, the threshold potentiation electric field can be calculated and is thus evaluated as 75 kV cm^{-1} .

Biocompatibility

The fabrication method proposed in this study implies deposition of Au and TiO_2 on the substrate surface. In order to assess biocompatibility of all the materials, they have been deposited separately on a series of glass substrates and subjected to MTT cytotoxicity assays using IMR-32 and PHF cell lines. The experimental results are shown in Fig. 8. The diagram of cell viability is shown in Fig. 8a and demonstrates that none of the materials caused any notable cytotoxic effect on the IMR-32 and PHF cells. Indeed, the cell survival rates for IMR-32 and PHF on Au and TiO_2 were 97.37% for IMR-32/ TiO_2 , 95.86% for PHF/ TiO_2 , 95.93% for IMR-32/Au, and 95.05% for PHF/Au with respect to the control solely incubated batch. In this assay, all the cells were cultivated for 72 hours, the time sufficient for 3 cycles of cell divisions, and no apparent morphological or metabolic changes have been observed, as illustrated in Fig. 8b–e for all the combinations of the cells and materials addressed in the study. Thus, the memristor elements fabricated by the proposed hybrid planar technology and using Au and TiO_2 as constituting materials have demonstrated high biocompatibility.

Discussion

The fabrication method addressed in this study has a limited range of applicability, though it has certain favourable advantages for designing *in vitro* experiments with biological tissues and cells at the lab scale. Indeed, the atomic force microscopy is a well-recognized tool for nanoscale materials patterning and engineering,^{48,49} just as much as for bioengineering, investigations in biochemistry and cell biology.^{50,51} Inkjet printing is a cost-efficient nanofabrication method, especially for the lab-scale prototyping.^{52,53} It typically operates with a picolitre droplet volume and 10–20 μm spatial resolution⁵² of the droplet depositing. This is sufficient for integration of the printable microcircuits with biological cells, as long as the cell sizes (*ca.*

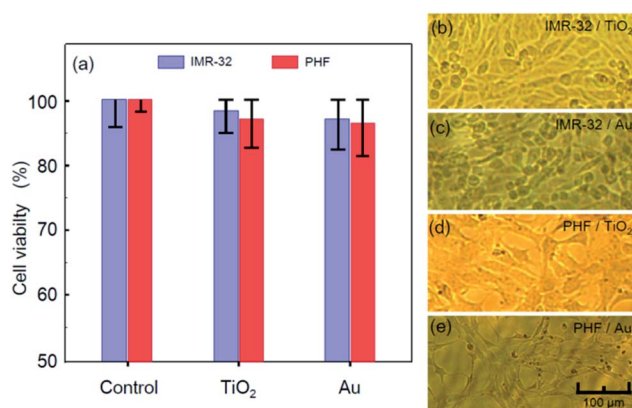


Fig. 8 Viability of IMR-32 and PHF cells incubated solely (control) and on substrates of TiO_2 and Au: (a) chart for percentage of viable cells; and (b–e) optical microscope images of cells after 72 hours of incubation: (b) IMR-32 on TiO_2 , (c) IMR-32 on Au, (d) PHF on TiO_2 , and (e) PHF on Au.



100 μm , e.g. Fig. 8d and e) surpass the printing resolution limit. Furthermore, the inkjet bioprinting is rapidly developing nowadays,^{54,55} thus enabling precise positioning and arrangement of biological and inorganic elements on the substrate.

The nano- and microfabrication methods based on physical (FIB)⁵⁶ or chemical (mask lithography)^{28,29} treatment provide better reproducibility,⁵² though they cannot be considered for conducting *in situ* experiments with biological cells or tissues. In these cases, the combination of AFM and inkjet patterning shall be a justified choice. Their combination allows for *in situ* circuit manipulations even in the case with the integrated biological substances.

Seemingly, the major challenge in the proposed design of planar memristors is the relatively low current response experimentally achieved at this stage (Fig. 7a). Nonetheless, we believe that further development of the functional inks shall lead to better performance. Firstly, a more careful adjustment of the ink crystallinity is needed. Technologically, it is feasible for sol-gel^{38,57} and other⁵⁸ processing routes. Secondly, as the concentration of oxygen vacancies in the functional layer significantly affects the memristive performance,⁴⁴ the optimal level of oxygen nonstoichiometry can be achieved by an appropriate doping or by thermal treatment in an inert atmosphere. And thirdly, other biocompatible memristive compositions can be considered besides TiO_2 .

Conclusion

In summary, we have designed, fabricated, and investigated a novel planar configuration of a memristive element. The proposed hybrid nanofabrication method allows patterning the insulating trenches in the gold-sputtered electrodes and filling them with functional inks using the AFM and inkjet printing techniques, correspondingly. The combination of these methods allows for operational versatility for designing *in vitro* experiments with biological cells and tissues. The fabricated planar memristors have demonstrated a memristive behaviour qualitatively, upon U-I characterization. However the electrical response was rather weak, possibly due to incomplete filling of the trench or low density of the filling material. Thus the proposed fabrication technique requires further elaboration. Finally, the materials used in the fabrication have demonstrated reasonable biocompatibility, not causing any apparent cytotoxic effect on IMR-32 and PHF cells.

Conflicts of interest

There are no conflicts to declare.

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