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# A novel ratiometric fluorescent probe for rapid detection of hydrogen peroxide in living cells†

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In this work, we present a new ratiometric fluorescent probe JNY-1 for rapid and convenient detection of  $H_2O_2$ . The probe could selectively and sensitively respond to  $H_2O_2$  within 10 min. In addition, this probe was successfully applied for monitoring and imaging of  $H_2O_2$  in liver cancer HepG2 cells under physiological conditions.

significance.

#### Introduction

Reactive oxygen species (ROS) is a collective term that describes the chemical species that are formed upon incomplete reduction of oxygen and includes the hypochlorous acid/hypochlorite ions (HOCl/OCl), hydrogen peroxide (H2O2), superoxide anion (O<sup>2-</sup>) and the hydroxyl radical (HO'). ROS in the body are generated endogenously from oxygen mainly through the mitochondrial respiration process as well as exogenously by exposure to deleterious conditions including UV light, xenobiotics and infectious agents.1 ROS are classically known as indicators of oxidative stress, which is a fundamental process that operates in a diverse array of human diseases, including Alzheimer's diseases, cardiovascular disorders, and cancer.<sup>2-4</sup> Hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) is one of the most important ROS. Cellular hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) arises primarily as a ubiquitous dismutation product of superoxide. Mounting evidence suggests that H<sub>2</sub>O<sub>2</sub> production drives a broad spectrum of cellular processes. For example, when H<sub>2</sub>O<sub>2</sub> is generated at low concentrations (<0.7 µM) in a regulated fashion, it functions as a ubiquitous intracellular second messenger, regulating a multitude of physiological and pathological processes in cell.<sup>5</sup> Under conditions of stress or stimulation by exogenous chemicals, H<sub>2</sub>O<sub>2</sub> can be generated aberrantly and can be converted to dramatically more "damaging" ROS such as hypochlorous acid (HOCl) and hydroxyl radical (HO') by myeloperoxidase and Fenton reagents, respectively. The resulting ROS can attack cellular structures or biomolecules such as proteins, liposomes, and DNA, which has been associated with aging, Alzheimer's

disease, and cancer.6,7 However, the transient increase of

intracellular H2O2 may be necessary for mitosis.8 Therefore,

development of a rapid and highly selective method for monitoring  $H_2O_2$  level change  $H_2O_2$  in living cells is of great

However, it is challenging to capture and detect  $H_2O_2$  in living cells. This is mainly due to  $H_2O_2$  in the cells possessing

the following characteristics. At first, H<sub>2</sub>O<sub>2</sub> can readily moves out of cells through free diffusion. So, it's difficult to detect

Fluorescence imaging based on small-molecule fluorescent probes has emerged as an efficient methodology to visualize the spatial and temporal distribution of biomolecules in biological specimens due to its real-time, sensitive, and noninvasive characteristics.9-11 Up to now, numerous fluorescent probes for endogenous H2O2 detection that have been elaborated, 12-16 and the detection mechanisms of these H<sub>2</sub>O<sub>2</sub> probes are mainly based on boronate oxidation17 or Baeyer-Villiger-type reactions.18 To some extent, these probes always have some minor defects. Several boronate-based probes react more slowly with H<sub>2</sub>O<sub>2</sub> compared to other reactive species (e.g., peroxynitrite and hypochlorite).19-21 Some of them have been used to detect peroxynitrite<sup>22-24</sup> or benzoyl peroxide<sup>25</sup> instead of H<sub>2</sub>O<sub>2</sub>. On the other hand, the vast majority of these probes are intensity-based turn-on fluorescent probes.26 However, interpretation of the results obtained with turn-on probes could be complex. As the fluorescence intensity is very sensitive to environmental factors such as probe concentration, temperature, medium polarity, and pH and also instrumental set-ups, such intensity-based

cluding most important, there are many isting in the living system which the ROS. H<sub>2</sub>O<sub>2</sub>. Thus, high selectivity is a detection of H<sub>2</sub>O<sub>2</sub>. Therefore, of temporal accuracy is of great studies of H<sub>2</sub>O<sub>2</sub>-related biology. Fluorescence imaging based probes has emerged as an efficient spatial and temporal distribution specimens due to its real-time characteristics.  $^{9-11}$  Up to now, not sent the results of the probability of the results of the resu

intracellular H<sub>2</sub>O<sub>2</sub> *in situ*. Second, H<sub>2</sub>O<sub>2</sub> easily reacts with biosubstances to form other ROS. Therefore, in order to accurately detect H<sub>2</sub>O<sub>2</sub>, the methods require a fast response time. Last but most important, there are many ROS with high reactivity coexisting in the living system which can interfer the detection of H<sub>2</sub>O<sub>2</sub>. Thus, high selectivity is also expected to be achieved for detection of H<sub>2</sub>O<sub>2</sub>. Therefore, detection of H<sub>2</sub>O<sub>2</sub> with spatialtemporal accuracy is of great significance for mechanistic

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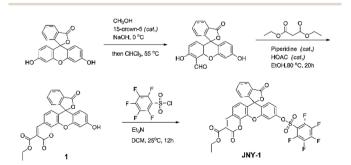
probes are not suitable for quantitative analysis. In this context, ratiometric probes that have an internal correction capability are in great demand. Ratiometric probes provided two separate signals for the probe itself and for its reaction product with the analyte or its analyte bound form, which can normalize the interference. Thus, ratiometric probes with high response rate, excellent selectivity, and good sensitivity should be developed for fulfilling the stringent issues of biological examination.

To address this issue, we herein report a novel ratiometric fluorescent probe JNY-1 (Scheme 1) for detection of H<sub>2</sub>O<sub>2</sub> with high selectivity and sensitivity. In this work, we choose an integration of fluorescein and coumarin fluorophores as the fluorogen because of its' tunable fluorescent properties which could be used for design ratiometric response probes. The pentafluorobenzenesulfonyl group was selected as the reaction unit. As we all known, it is more stable to hydrolysis than ester bond, and the pentafluorobenzene ring enhances the reactivity of the sulfonates toward H2O2, which can contribute to enhance the selectivity and sensitivity of probe towards to H<sub>2</sub>O<sub>2</sub>.<sup>27</sup>. As shown in Fig. 1, in the absent of  $H_2O_2$ , probe **INY-1** is present in spirocyclic form only with coumarin-like emission. After selectively deprotecting the pentafluorobenzenesulfonyl group by H<sub>2</sub>O<sub>2</sub>, probe JNY-1 is present in its strongly fluorescent quinoid form and the fluorescence shift from 440 nm (coumarin-like emission) to 540 nm (fluorescein-like emission).

#### Results and discussion

The synthetic route of probe **JNY-1** is shown in Scheme 1. First, an aldehyde-functionalized fluorescein was prepared according to previous reports.<sup>28,29</sup> The further reaction of fluorescein monoaldehyde with diethyl malonate afforded a coumarin hybrid **1**, which can be treated with 2,3,4,5,6-pentafluorobenzene-1-sulfonyl chloride, eventually resulting in the formation of probe **JNY-1**, which was characterized by <sup>1</sup>H, <sup>13</sup>C NMR and mass spectra.

With the probe **JNY-1** in hand, we then tested its spectroscopic properties. The fluorescence and absorption spectra were measured in DMF/phosphate buffer (30 : 70 v/v, 10 mM, pH 7.4) system at room temperature (25 °C). As displayed in Fig. 1b, the probe **JNY-1** itself showed the maximal absorbance centered at 340 nm. With the excitation at 340 nm, the probe **JNY-1** offered fluorescence emission centered at 440 nm, which is belong to coumarin-like emission. Upon the addition of  $\rm H_2O_2$ , the



Scheme 1 The synthsize route of probe JNY-1.

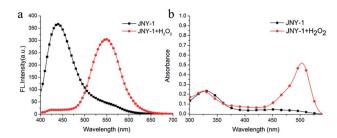


Fig. 1 Fluorescence (a) and UV/Vis absorption (b) spectra of **JNY-1** (10  $\mu$ M) in the absence and presence of H<sub>2</sub>O<sub>2</sub> (100  $\mu$ M).

reaction of **JNY-1** and  $H_2O_2$  happened and resulted the dissociation of the pentafluorobenzenesulfonyl group from **JNY-1**. Obviously, this detection process is not reversible. Thus, a new absorbance centered at 480 nm emerged. Correspondingly, the fluorescein-like emission centered at 540 nm was observed.

As shown in Fig. 2, the time course of the fluorescent emission of probe JNY-1 (10  $\mu$ M) at 540 nm in the presence of  $H_2O_2$  (10 equiv.) was studied. By examining the kinetic data for  $H_2O_2$ , it is apparent that it would take no more than 10 minutes to reach the equilibrium. Generally, it needs 30 min or more to reach the reaction equilibrium between arylboronate based probes and  $H_2O_2$ . JNY-1 showed faster response to  $H_2O_2$  mainly due to the pentafluorobenzene ring enhances the reactivity of the sulfonates toward  $H_2O_2$ . The rapid response time is favorable for detection and imaging of  $H_2O_2$  in the complex biological systems.

Next, the detailed emission titration experiments of probe **JNY-1** (10  $\mu$ M) with various concentrations of H<sub>2</sub>O<sub>2</sub> were also carried out in the DMF/phosphate buffer (30 : 70 v/v, 10 mM, pH 7.4) system. As shown in Fig. 3, when the probe **JNY-1** was treated with different concentrations of H<sub>2</sub>O<sub>2</sub> (0–200  $\mu$ M), the emission band at 440 nm decreased progressively, while a new emission peak around 540 nm was observed. Importantly, as shown in Fig. 4, the ratio of emission intensities ( $I_{540 \text{ nm}}$  :  $I_{440}$ 

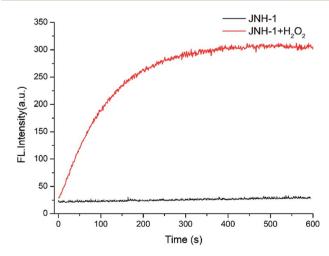


Fig. 2 The time course of the emission intensity of JNY-1 (10  $\mu$ M) at 540 nm in the presence and absence of H<sub>2</sub>O<sub>2</sub> (100  $\mu$ M) with  $\lambda_{ex}=$  340 nm.

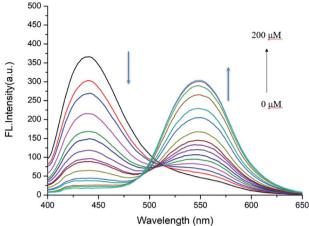


Fig. 3 Fluorescence responses of probe JNY-1 (10  $\mu$ M) toward different concentrations of H<sub>2</sub>O<sub>2</sub> (0–200  $\mu$ M) with  $\lambda_{ex}=380$  nm.

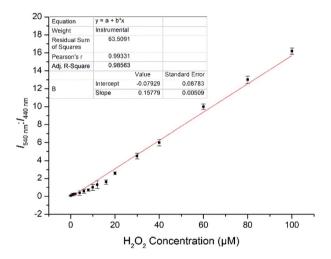


Fig. 4 Fluorescence intensity ratio ( $l_{540~nm}$ :  $l_{440~nm}$ ) of probe JNY-1 versus H<sub>2</sub>O<sub>2</sub> concentration (0–100  $\mu$ M) with  $\lambda_{ex}=380$  nm, error bars, SD (n=3).

nm) increased by nearly 180-fold and exhibited good linear correlation with the amount of  $\rm H_2O_2$  (0–100 μM,  $R^2$  = 0.98563). The detection limit was calculated to be 0.08 μM (3 $\rm S/m$ , in which  $\rm S$  is the standard deviation of blank measurements, n = 11, and  $\rm m$  is the slope of the linear equation). As shown in Fig. S4,† with addition of  $\rm H_2O_2$  (0–200 μM), the initial absorption peak centered at 340 nm decreased slightly, along with a simultaneous emergence of the red shifted new absorption peaks at 500 nm. Correspondingly, JNY-1 displayed distinct color changes from colorless to orange, which could be easily observed by the naked eye (Fig. S6†).

To verify the selectivity of **JNY-1** for  $H_2O_2$ , we also measured the ratiometric signals change upon addition of a panel of ROS, reactive nitrogen species (RNS), and the representative biological species. As shown in Fig. 5, only  $H_2O_2$  could trigger a large ratiometric response. However, the ratiometric signals showed no or very minor changes for other species, including  ${}^1O_2$ ,

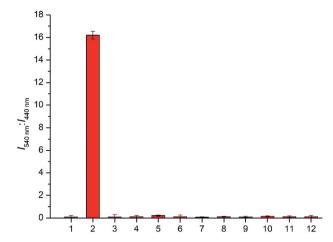


Fig. 5 Fluorescence responses  $I_{540~\rm nm}$ :  $I_{440~\rm nm}$  of JNY-1 (10  $\mu$ M) with various analytes. (1) Free probe; (2)  $H_2O_2$ ; (3)  $^1O_2$ ; (4) ONOO<sup>-</sup>; (5) NO; (6) ClO<sup>-</sup>; (7) *tert*-butyl hydroperoxide (TBHP); (8) ·OH; (9)  $O_2$ <sup>--</sup>; (10) GSH; (11) ascorbic acid and (12) glucose. Each spectrum was recorded at 10 min after the addition, error bars, SD (n=3).

ONOO $^-$ , NO, ClO $^-$ , tert-butyl hydroperoxide (TBHP), ·OH, O $_2$ . GSH, ascorbic acid, and glucose. This result indicated that probe **JNY-1** exhibited remarkably high selectivity for  $H_2O_2$ .

To further evaluate the ability of probe JNY-1 for detection of  $\rm H_2O_2$  in living cells, we conducted the cell imaging experiments. As shown in Fig. 6, the liver cancer HepG2 cells in group A and B were incubated with 10  $\mu$ M of JNY-1 at 37 °C for 15 min before fluorescence imaging. Group A was the control and group B was added 100  $\mu$ M of  $\rm H_2O_2$ . As described in Fig. 6A, HepG2 cells incubated with 10.0  $\mu$ M JNY-1 show fluorescence in blue channel, but there is negligible fluorescence signal through green channel. On the contrary, the probe-loaded cells appear clear cellular profiles with bright green fluorescence when treated with 100  $\mu$ M  $\rm H_2O_2$  for 10 min, the original fluorescence signal in the blue channel weakened accordingly. These imaging results indicate that JNY-1 shows pleasurable cell-permeability and could be applied in dual-color fluorescence imaging of intracellular  $\rm H_2O_2$ .

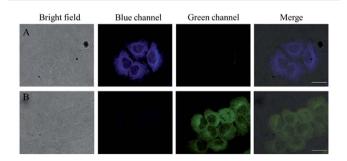


Fig. 6 Confocal fluorescence images of the liver cancer HepG2 cells with probe JNH-1. Fluorescence images were obtained before and after incubation for 10 min without (A) or with (B) 100  $\mu$ M H<sub>2</sub>O<sub>2</sub>. The images were collected at 425–465 nm (blue channel) and 520–560 nm (green channel) upon excitation at 405 nm. Scale bar: 20  $\mu$ m.

#### Conclusions

In summary, we have described the design and synthesis of a new ratiometric fluorescent probe **JNY-1** for detection of  $H_2O_2$ . The probe could selectively and sensitively respond to  $H_2O_2$  within 10 min without interferences of other reactive oxygen species (ROS), reactive nitrogen species (RNS), and biologically relevant species. This probe was successfully applied for monitoring and imaging of  $H_2O_2$  in liver cancer HepG2 cells under physiological conditions. The combination of ratiometric capability, sensitivity, specificity, and rapid response property makes the probe a candidate for various potential applications.

#### Conflicts of interest

There are no conflicts to declare.

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