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Functionalized gold nanostructures: promising gene delivery vehicles in cancer treatment

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Surface-modified gold nanoparticles are recognized as promising gene delivery vehicles in the treatment of cancer owing to their excellent biocompatibility with biomolecules (like DNA or RNA) and their unique optical and structural properties. In this context, this review article focuses on the diverse transfection abilities of the gene to the targeted cell on the basis of different shapes and sizes of gold nanoparticles in order to promote its effective expression for cancer treatment. In addition, recent trends in gold nanoparticle mediated gene silencing, gene delivery, detection and combinatory therapies are highlighted considering their cytotoxic effects on healthy human cells.

1. Introduction

Cancer, with high incidence and deregulated cell growth, has caused death all over the world. Conventionally, cancer treatment relied mainly upon tumour resection along with chemotherapy, where there is non-specific accumulation of drugs and/or radiotherapy resulting in various side effects. A large number of cancer cells have become drug resistant towards these therapies mostly due to the molecular mechanism. These drawbacks of the traditional approach towards treatment of cancer can be overcome by combining gene therapy with other related therapies such as chemotherapy, photothermal therapy, photodynamic therapy, *etc.*^{1–4} Gene delivery vectors reported in recent years, include polymer-based, lipid-based, and inorganic nanoparticle-based systems.^{5–9} Ideal non-viral gene vectors offer numerous advantages, such as

chemical stability, biocompatibility, effective targeting, stimulus responsiveness and feasibility for combined treatments.^{2–4} Due to irregular signalling pathways and genetic alterations, the concept of novel molecularly targeted therapeutic strategies such as gene-silencing or knockdown therapies have been introduced.^{10–14} RNA interference (RNAi), one of the significant gene therapy approaches followed by tumour resection has fascinated researchers in cancer treatment,¹⁵ where microRNA (miRNA) and plasmid DNA (pDNAs) are frequently utilized because of their higher stability and specificity than those of small interfering RNA (siRNA).^{16,17} Surface-modified gold nanomaterials are acknowledged as favourable gene delivery vehicles,^{18–21} in consequence of their small size, general non-toxicity, ease of functionalization and high surface to volume ratio, localized surface plasmon resonance (LSPR) of gold nanoparticles resulting in improved consideration from non-viral siRNA gene delivery.^{11,22,23} Additionally, these nanoparticles can also be used for imaging of tumours by computed tomography, a leading radiologic technology in the field of biomedical imaging.²⁴

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In continuation of our research work in the field of nanomaterials and cancer treatment,^{25–30} the current review focuses on advanced accomplishments of gene therapy in conjugation with gold nanoparticles that stand out as potential candidates for anti-oncological approaches. In addition, detailed mechanisms like gene silencing, gene delivery along with detection and imaging are discussed both *in vitro* and *in vivo*.

2. Evaluation of gold nanoparticles in gene silencing

The commendable contributions of AuNPs in gene silencing have enhanced the treatment of cancer drastically. Various recent reports have shown effectiveness utilizing this approach as shown in Table 1. Table 1 shows the cellular recognition and entry of the nanoparticles, of different size and shape at tumor

sites for knockdown. RNA interference (RNAi), one of the gene therapy approaches offered has attracted interest in cancer treatment due to its high specificity and efficiency and the relatively minor upshots.^{31,32} Over the decade, a novel strategy for detection and gene knockdown has been introduced using RNA interference.^{33,34} Telomerase which is highly expressed in many types of cancer cells whose activity inhibition using human telomerase reverse transcriptase (hTERT) has been investigated in oncology.³⁵ However, there are challenges that hinder the efficient delivery of hTERTsiRNA at the tissue level as well as the intracellular levels (Fig. 1).^{36–38}

Under the influence of LED radiation, the Chromium-doped zinc gallate nanoparticles $\text{ZnGa}_2\text{xO}_4 : \text{Cr}_x$ (ZGOC) nanofiber emission could be absorbed selectively by gold nanorods (AuNRs), which induces a mild photothermal effect that in turn triggers the liberation of the particles from ZGOC nanofibers, localized drug delivery systems (LDDSS), and enhances the



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cellular uptake and the therapeutic effect. The new therapeutic platform, with LED-amplified gene silencing has therefore inspired another potential system to enhance gene therapy in cancer treatment. The successful RNAi lies in the effective release of siRNA from the endosomes, which can destroy the target mRNA in the cytoplasm and inhibit the expression of the target protein.³⁹ Post conjugation of mRNA, siRNA instigates degradation of mRNA, hence significantly reducing protein expression by targeting the gene.^{34,40} In a study, to therapeutically target eukaryotic elongation factor 2 kinase (eEF-2K), which has been identified as an important oncogenic pathways for promoting breast cancer. Kezban *et al.* synthesized a highly monodisperse and stable nano-formulation using polyethylenimine-modified gold nanoparticles (AuNP-PEI) and conjugated them with eEF-2K siRNA. Hence, down regulation of triple negative breast cancer cells (TNBC) using AuNP-PEI/eEF-2K siRNA was observed *in vitro*.³³

To make sure the better detection and therapeutic effect, anti-miR-21 strands are fully modified by 2'-O-methyl to increase binding affinity with tumor gene and improve stability and resistance to exonucleases to prolonged inhibition of miRNAs.⁴¹ Recent studies have shown that Taxol, a chemotherapeutic drug initially induces apoptosis of cancer cells, but on prolonged treatment, the cancer cells become immune to this drug and to other drugs as well.^{42,43} This resistance of cancer cells towards these chemotherapeutic drugs is called multidrug resistance (MDR).⁴⁴ Various studies have reported that P-glycoprotein (P-gp) is overexpressed in MDR cell lines.⁴⁵ The reduction in the expression of P-gp could be done using hyperthermia.⁴⁶ Also, microRNA-21 (miR-21) a type of miRNA could be downregulated resulting in inhibiting tumor progression and invasion.^{47,48} miRNA, is advantageous in promoting cell invasion by regulating various genes, including programmed cell death 4 (PDCD4) gene, tissue inhibitor of metalloproteinase inhibitor 3 (TIMP3), phosphatase and tensin homolog (PTEN) gene in a variety of tumors, such as lung cancer, glioblastoma, and breast cancer.⁴⁹ AuNPs are functionalized with miRNA-21

inhibitors that are hybridized with fluorophore-labeled DNA molecules named "flares", miRNA-21 inhibitors are 2'-O-methyl modified antisense oligonucleotide that are complementary to the mature miRNA-21 to suppress its function, resulting in cells growth inhibition and apoptotic cells death, as shown in Fig. 2.⁵⁰ Cancer stem cell (CSC) with the mark of CD44 plays an important role in gastric cancer (GC). The transfection of rMETase carried by HA-G5 PAMAM-Au visibly inhibited the escalation and tumor sphere formation of GC cells through promoting METase activity. Elevated level of methionine (MET) promotes self-growth of cancer cells. Suppression of CD44(+) GC resulted because of downregulation of METase activity, which lead to increase of Cyc C and ROS levels. For instance, the p53 and HSV-TK suppressed the proliferation and promoted apoptosis of cancer cells.^{51,52} No effect on healthy cells was observed due to the low concentration of MET.⁵³ Owing to the excellent structural properties (PAMAM) is found to be suitable in conjugation with metallic nanoparticles.⁵⁴ Improvement in efficacy of gene transfecting COS-7 cells and shape maintenance of dendrimers was caused through G5-PAMAM encapsulated gold nanoparticles.⁵⁵ Additionally, hyaluronic acid (HA) was conjugated onto PAMAM for targeting CD44 + gastric cancer stem cells specifically.⁵⁶

Another instance of this approach is demonstrated by the use of folic acid (FA) due to its replication control, cell proliferation, synthesis of proteins and biocompatibility.⁵⁸ Moreover, it has high affinity towards FA receptors which are mainly overexpressed in breast (MCF-7), and cervical (KB) cells.⁵⁹ Gold nanoparticle conjugated generation five dendrimers (Au : G5D) and Au : G5D : FA NPs proved to be highly efficient in combining with pCMV-Luc DNA and transporting it. The pDNA were safeguarded from nucleases corresponding to formation of stable nanocomplexes.⁶⁰ siCOX-2/9R/DG-AuNS (hydrazone) showed best gene silencing and inhibition effect on tumor cell growth amongst siCOX-2/AuNS, siCOX-2/9R-AuNS, siCOX-2/9R/DG-AuNS, and siCOX-2/9R/DG-AuNS (hydrazone) groups in both HepG2 and SGC7901 cells.⁶¹ In comparison to free siRNA,



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Table 1 Surface modified gold nanoparticles as gene delivery vehicles to produce gene silencing effect

S. No.	Type of gold nanoparticles (shape & size)	Type of cancer treated/targeted cells	Delivery vehicle	Targeted Functions	Reference
1	Gold nanoparticles (~50 nm)	Breast cancer	AuNP-PEI/EEF-2K siRNA	Gene knockdown <i>in vitro</i> and <i>in vivo</i> and evaluated antitumor efficacy in a TNBC tumor model	33
2	Gold nanorods (~70 nm × ~30 nm)	HepG2 cancer cells	PEI-Au/siRNA and PEI-Au/siRNA@ZGOC	Protection of siRNA for gene silencing and LDDS gene vector system of PEI-Au/siRNA@ZGOC which binds siRNA for gene silencing	39
3	Gold nanoparticles (~50 nm)	Gastric cancer	HAG5PAMAMAuMETase	Suppressed the growth of tumor <i>via</i> targeting CD44(+) cells	56
4	Gold nanoparticles (65–128 nm)	Breast (MCF-7), and cervical (KB) cells	Au : G5D and Au : G5D : FA NPs	Affords good protection to the pDNA against nucleases	60
5	Gold nanostars (72.5 ± 3.2 nm)	Hepatocellular carcinoma cells (HepG2) and SGC7901 cells	siRNA/9R/DG-AuNS (hydrazine)	Gene silencing and inhibiting the cell growth rate	61
6	Gold nanoclusters (2.6 ± 0.5 nm)	Panc-1 <i>in vitro</i> , pancreatic tumours <i>in vivo</i>	AuNC-siRNA	Suppressed pancreatic tumour progression	62
7	Gold nanostars (AuNS TRITON: 80–90 nm; AuNS LSB: 50–70 nm; shrunk AuNS LSB: 20–30 nm)	MCF-7/Luc cells	AuNS-POLYMER-siRNA	Suppressed luciferase expression	63
8	Gold nanoshells (159 ± 11 nm)	Triple-negative breast cancer	LbL-NS	Suppressed cancer cell growth	64
9	Gold nanorods (48 × 16 nm)	Ovarian cancer cell line (SKOV-3)	DTC-anchored siRNA duplex	Efficient knockdown	66
10	Gold nanoassembly (20–25 nm)	Hela cells	Rf, RfSH and Rf@AuNPs	DNA damage and apoptosis	69
11	Gold nanoparticles (30.42 ± 0.29 nm)	MCF-7 and MDA-MB-453 cells	AuNP@PEG@anti-RAB27A	Gene silencing and decrease of exosome release	74
12	Gold nanoparticles (~6 nm)	A375 human melanoma cells	AuNP-SX/SS/SN-DNA and AuNP-TSX/TSS/TSN-plasmid complexes	To modify cellular protein expression	[81]
13	Gold nanocages (~50 nm)	Hepatocellular carcinoma (HCC) A375 cells	HA/anti-miR-21/PPAuNCs	Reversing MDR (multidrug resistance)	85
14	Gold nanoclusters (103.7 ± 3.8 nm)	Lung cancer, breast cancer, pancreas cancer, skin cancer, ovary cancer	TAT-AuNS/Cas9 protein/sgRNA	Inhibited the tumour growth	93
15	Gold nanoparticles (5.3 nm)		TDDS (Au-TR-DX-si)	Knockdown of erbB2 oncogene <i>in vitro</i> and tumor suppression <i>in vivo</i>	98
16	Gold nanoparticles (65–128 nm)	HEK293, HepG2, Caco-2, MCF-7, KB	Au : G5D, Au : G5D : FA, G5D, G5D : FA	Apoptosis, enhanced transfection efficiency	127

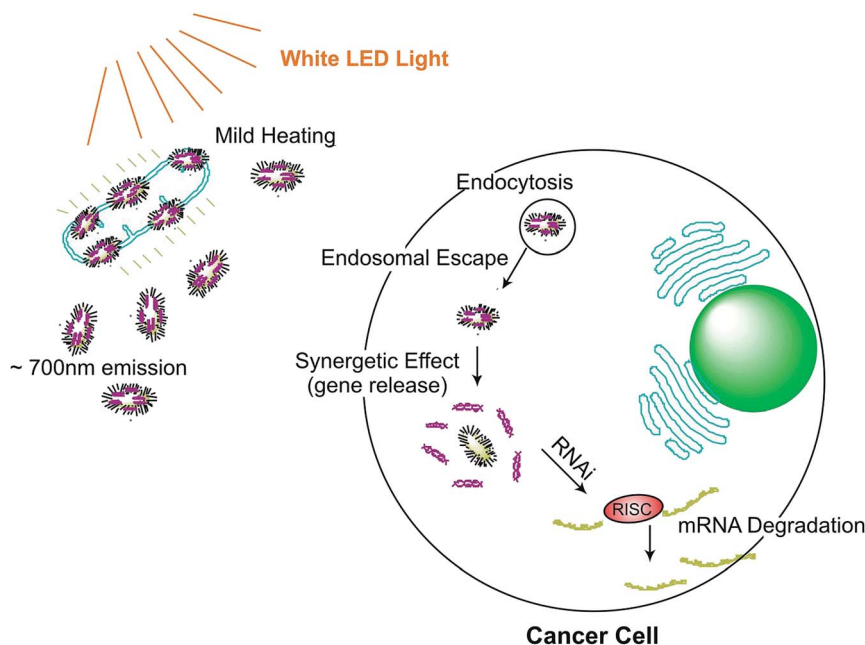


Fig. 1 Gene silencing on targeted cancer cell site using white LED light (~ 700 nm emission). Gold nanorods-assembled ZnGa_2O_4 -Cr nanofibers for LED-amplified gene silencing.³⁹

gold nanocages conjugated siRNA (AuNC-siRNA) entered the Panc-1 cells in much larger quantity, showed lysosomal escape and effective gene silencing. In addition, it enhanced circulation lifetime, increased accumulation on tumour sites showed high safety.⁶² PPE-LA coating showed better gene silencing of MCF-7 cells than AuNS (gold nanostar) coated with SH-PEG3000-NH₂. Although, siRNA complexes coated with AuNS showed better results than siRNA alone.⁶³ Using Western blotting, it was analysed that miR-34a-LbL-NS significantly decreased Bcl-2 and SIRT1 expression in MDA-MB-231 cells in comparison to control groups and also reduced metabolic activities in MDA-MB-231 cells.⁶⁴ Transglutaminase 2 (TG2) plays a vital role in metastasis of recurrent ovarian cancers,

hence becomes a critical target.⁶⁵ Successful gene knockdown by AuNR based DTC-siRNA, was observed using colorimetric assay.⁶⁶ Flavoprotein enzyme assembling is done mainly by riboflavin (Rf) and is overexpressed in prostate and human breast cancers.^{67,68} Abhishek Sau and team prepared thiol-modified riboflavin-gold nanoparticles (RfS@AuNPs), targeting HeLa cells hence causing DNA damage and apoptosis in them.⁶⁹ Exosomes which are found in body fluids, containing protein and nucleic acids, secreted by both normal and malignant cells.⁷⁰⁻⁷² The presence of these in higher content is responsible for tumour growth and evasion.^{71,73} AuNP@PEG@anti-RAB27A silence higher gene expression than that of RAB27A, also inhibiting formation of Rab27, a protein

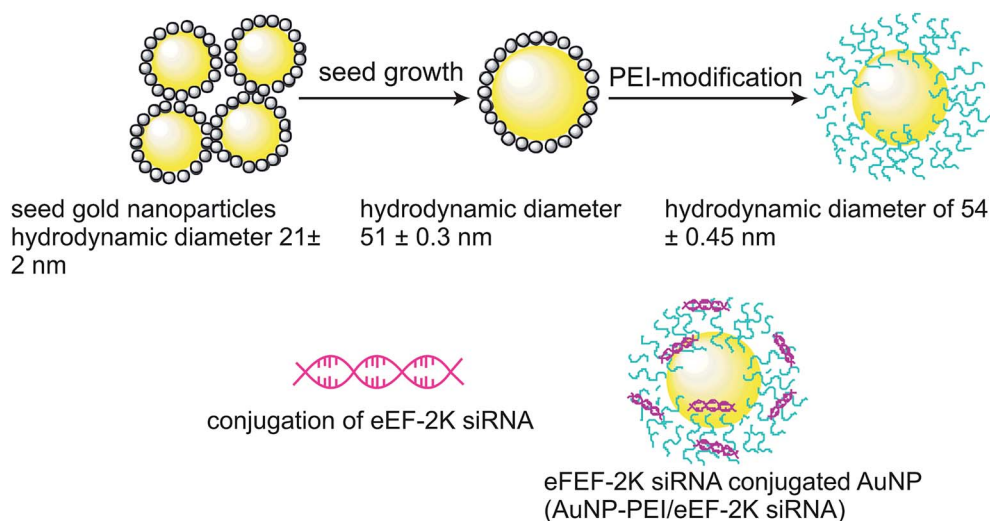


Fig. 2 Schematic illustration for modification of AuNPs via polyethyleneimine.³³



Table 2 Characterization of AuNPs for enhanced gene delivery

S. no.	Type of gold nanoparticles (shape & size)	Type of cancer treated	Delivery vehicle	Targeted functions	Reference
1	Gold nanorods (~30 nm × 10 nm)	HEK293, HepG2 cells	AHP, sm-AHP, CD-PGEA	Apoptosis, enhanced transfection efficiency	75
2	Gold nanoparticles (2.9 nm and 3.1 nm)	EGFP, Luc cells	Au DENPs-mPEG and Au DENPs-PEG-FA	Low immunogenicity and enhanced gene transfection efficiency	142

from RAB27A mRNA.⁷⁴ Xinyan Chen *et al.* used “ship in a bottle strategy” and encapsulated AuNRs inside the hollow cavity of HSN (hollow silica nanoparticles). SF (hydrophobic anti-proliferative and antiangiogenic drug) release was observed due to the detachment of CD-PGEA when NIR radiation was applied, leading to apoptosis in both *in vitro* as well as *in vivo*.⁷⁵

3. Analyzing targeted gene delivery using modified gold nanoparticles

The main goal of gene therapy is to select an acceptable carrier to specifically transport the target gene to the desired target cell and promote its effective expression for treatment. The carrier of gene therapy mainly includes two categories: viral vector and non-viral vector.⁵⁶ Surface-modified Gold nanomaterials are considered as efficient gene delivery vehicles.^{76,77} However, for gene therapy in general, siRNA molecules are phagocytosed and hence need to overcome extracellular and intracellular obstacles and be released from the endosome after being internalized by tumor cells.⁷⁸ Scientists have reported the efficiency of gold nanoparticles in analyzing targeted gene delivery and these are summarized in Table 2. The Covalently coupled nucleic acids (such as single monodentate thiol (SX), bidentate dual thiol (SS), or mixed bidentate thiol plus amine (SN) coordination of nucleic acids) on the surface of gold nanoparticles (AuNP) have been used as an effective gene therapy agent to modify cellular protein expression. It is anticipated that the therapeutic effect depends on length of time the nucleic acid sequence resides in the *endo*-lysosomal pathway once the cell is transfected. It is believed that it depends on the linkage chemistry of the DNA to the AuNP surface.⁷⁹ LDDSS, which are designed to manipulate the tumor microenvironment are normally injected (or implanted), have intrinsic drawbacks in achieving effective gene therapy. Therefore, by combining LDDSS and particulate gene carriers (*i.e.* gold nanorods) unique opportunities might be offered allowing controlled delivery and release of a targeted therapeutic concentration and effective phagocytosis of siRNA molecules for enhanced gene therapy. Polyethyleneimine (PEI) is a well-known non-viral nucleic acid vector with high transfection efficiency both *in vitro* and *in vivo* due to the high density of positively charged amino groups distributed along the backbones of the molecular chains.⁸⁰ The positively-charged polyethyleneimine conjugated gold nanorods (Au-PEI NRs) possess the ability to electrostatically bind to negatively-charged siRNA. The protection of siRNA by PEI-Au/siRNA and PEI-Au/siRNA@ZGOC vectors was further verified by the addition of

RNaseA to mimic the human serum environment. The PEI-Au/siRNA and PEI-Au/siRNA@ZGOC vectors were found to protect the siRNA, effectively, from the degradation effects of RNaseA.³⁹ The permeability barrier imposed by stratum corneum makes an extreme challenge for the topical delivery of plasmid DNA (pDNA), which is widely used in gene therapy.⁸¹ Dendritic macromolecules are highly branch monodisperse macromolecules, presenting a sphere with cavity structure, hence are easy to combine with DNA to form nanoscale complex, which can protect DNA to achieve the purpose of transfection, so as the viral carrier, which is widely used.⁸² A group of researchers performed surface modification on polyamidoamine (PAMAM) dendrimers to decrease cytotoxicity and increase transfection efficiency.⁸³ Hyaluronic acid (HA), with good biocompatibility and aqueous solubility, was reported to be a receptor of CD44.⁸⁴ HA can target the site with high-expression CD44 tumor for targeted drug delivery to CD44-overexpressing cancer cell.⁴⁶ A novel gene delivery vector was developed, hyaluronic acid (HA)-modified, polyethylenimine (PEI)-conjugated PEGylated gold nanocages (AuNCs), which was designated as HA/PPAuNCs. This system possessed relative high photothermal conversion efficiency upon near infrared (NIR) laser irradiation, low cytotoxicity, and high targeted delivery ability. Moreover, anti-miR-21 could be condensed by PEI onto the surface of HA/PPAuNCs and then delivered into target cells. Therefore, HA/anti-miR-21/PPAuNCs might effectively overcome DOX resistance of HCC and provide new insights for cancer treatment.⁸⁵

3.1 Employing gold nanoparticles for gene delivery *in vitro*

Various scientists have studied the role of AuNPs *in vitro* to improve gene delivery in a targeted manner. In this context, modification of AuNPs with cationic polymers bound effectively to negatively surface charged siRNA molecules *via* a layer-by-layer approach has been studied. Due to their unique combination of surface plasmon properties and nanometer-scale dimensions, effective intracellular delivery of Au nanoparticles can be achieved along with transfected siRNA *in vitro*.³⁹ Presently, using multifunctional carrier AuNP, the perforation and transfection effect of pDNAs in the melanoma cells at the subcutaneous site were investigated.⁸¹ Polyethyleneimine (PEI) having abundant surface amine groups is found to be showing high efficacy due to its ability to compact DNA efficiently,^{86,87} however it has high levels of cytotoxicity. Hence, PEG has been used along with gold nanoparticles targeting HeLa.⁸⁸ Cyclooxygenase-2 (COX-2) is a rate-limiting enzyme over-expression of which is a sign of tumorigenesis, promotion of



malignant tumor cells and is expressed in vascular endothelial and adjacent normal tissues.^{89,90} Hongyan Zhu *et al.* have prepared siCOX-2/AuNS, siCOX-2/9R-AuNS, siCOX-2/9R/DG-AuNS, and siCOX-2/9R/DG-AuNS (hydrazone) groups in combination with siRNA to down-regulate COX-2 expression, targeting HepG2 (hepatocellular carcinoma cells) and SGC7901 cells.⁶¹ Plk1 gene is overexpressed in many tumor tissues for *e.g.*, A375 cells, inhibition of which is a good strategy for tumor therapy.^{91,92} Peng Wang *et al.* prepared LGCP (polyethylene glycol-lipid/AuNS/Cas9 protein/sgPlk1 plasmid) to suppress Plk1 gene.⁸⁷ The folate receptor (FR) is overexpressed in abundant of cancers such as: human ovarian, brain, cervical, epithelial, and breast cancer amongst others.⁹⁴ Jude Akinyelu and Moganavelli Singh prepared folic acid (FA) and chitosan (CS) functionalization with Au-PLGA NPs for downregulation of FR.⁹⁵ Heregulin-2 (HER2) is overexpressed in human ovarian cancer cell line and are known to be resistant to chemotherapy and aggressive.^{96,97} Rajesh Kotcherlakota and team prepared TDDS (Au-TR-DX-si) to target the same.⁹⁸ Pancreatic cancer being one of the dangerous cancers, its prominent cause being perineural invasion has its adverse effects such as increased neurite densities.^{99,100} Targeting NGF gene is the most important to tackle pancreatic cancer.⁶² Hence, Yifeng Lei *et al.* synthesized AuNC-siRNA⁶² because siRNA has the ability to cause sequence-specific gene silencing.^{101,102} Carla Sardo and team used a different shape of gold nanoparticle, *i.e.*, gold nanostar and conjugated it with SH-PEG3000-NH2 and PPE-LA targeting MCF-7/Luc cells.⁶³ As depicted in Table 2, AHP has shown better transfection efficiency than sm-AHP in HEK293 and HepG2 cells, which was visualized using enhanced green fluorescent protein (EGFP). This could be due to the shape and size of gold nanorods, and also rough surface of AHP.⁷⁵ miRNA regulates gene expression to control cell metabolic activity.¹⁰³ In an experiment conducted by R. Goyal *et al.*, LbL-NS was developed to deliver miR-34a into triple-negative breast cancer cells.⁶⁴ Poly-L-lysine (PLL) shows good endosomal escape,¹⁰⁴ since loss of expression of miR-34a takes place in TNBC.^{105,106} Therefore, naked miRNA cannot passively target due to its large size and negative charge.¹⁰⁷ In a study carried out by Jianxin Wang *et al.*, DTC-anchored siRNA duplex loaded onto AuNRs was used, which targeted ovarian cancer cell line (SKOV-3). DTC (dithiocarbamates) are resistant to nonspecific desorption reducing off target effects.⁶⁶ Nucleic acid is a great tool for detection as well as treatment purposes.^{108,109} MicroRNA (miRNA) plays vital roles in cell proliferation, differentiation,^{110,111} and tumors,^{112,113} and one of its example is Lethal-7 (Let-7).¹¹⁴ One of its members is Let-7a which can suppress the tumor cell growth and metastasis.^{115,116} Although DNA and RNA are similar compounds, a major difference is in their structure. DNA contains only one hydroxyl group, while RNA contains two hydroxyl groups. So, PBA shows low binding effect for compounds containing one hydroxyl group.¹¹⁷

Isocitrate dehydrogenase 1 (IDH1) which is highly expressed in Glioblastoma multiforme (GBM) is disruptive form found in brain tumors and can be targeted using siRNA.^{118,119} Jun Yue *et al.*, modified the siRNA with AuNPs (stars and spheres) to target the Isocitrate dehydrogenase 1 (IDH1) expression.¹²⁰ The

N/P ratio of 2.5 reveals the best transfection efficiency which was observed using flow cytometry and confocal microscopy. It could be due to the compaction ability and strong interaction of vectors with pDNA.¹⁴²

Baoji Du *et al.*, have used GDD (gold nanoparticles/dimethyldioctadecylammonium bromide (DODAB)/dioleoylphosphatidylethanolamin) and GF (gold nanoparticles/DODAB/DOPE/DOPE-folic acid) with different ratios of DOPE-FA targeting MCF-7 and A549 cells both *in vitro* and *in vivo* which is portrayed in the above figure¹²¹

3.2 *In vivo* delivery of genes via gold nanoparticles

The emerging need to explore recent nanoparticles capable of altering the collective state is worthy of attention;¹²² that is, how such vehicles can be modified for the development of *in vivo* obstacles that AuNPs face.¹²³ Previously, the interaction of small AuNPs with DNA was studied at low [NaCl], concluding that the reversible groove binding interaction was governed by solvation and viscosity factors.¹²⁴ Recently, in the study of the structural characterization of the gold colloid-DNA interaction, it was shown that AuNPs was able to interact with DNA *via* groove binding or intercalation, depending on the ethanol content and the *R* ratio.¹²⁵ According to Elia *et al.* previous structural approach,¹²⁵ their study has demonstrated that ethanol modifies AuNPs/DNA interaction from intercalation to groove binding by two simple mechanisms: gold nanoparticle aggregation and change in DNA conformation from B to C-form.¹²⁶ Particulate systems can be associated with the circulation of excessively high concentrations of drugs *in vivo*. (LDDSSs) offer the potential to target the drug more effectively.¹²⁷ In their work, Xiang *et al.* reported a new type of localized gene delivery system with LED-responsive properties based on the combination of the LDDSSs and nanoparticle gene vectors. In their system, hTERT siRNA was grafted on to AuNRs and these were attached to the surface of electrospun ZGOC nanofibers as depicted in Fig. 3. Au nanorods with an absorption peak of 700 nm matching the emission of ZGOC nanofibers were prepared using a seed growth method. Gold nanorods modified with a cationic polymer (PEI) were electrostatically bound with negatively charged siRNA.³⁹

To facilitate the skin penetration of pDNA deeply into the melanoma tissues, Jiang *et al.* presented a cell penetrating peptide and cationic polymer (PEI) conjugated gold nanoparticle (AuNP) that can compact the pDNAs into cationic nanocomplexes and penetrate through the intact stratum corneum without any additional enhancement used. Moreover, the AuNP is highly efficient in stimulating the intracellular uptake and nuclear targeting of the pDNAs in cells, which guarantees the effective transfection. It was shown that not only miR-222 but also miRNA-221 reduces viability and induce apoptosis mediated by the KIT, AKT and BCL2 signaling cascade.¹²⁸ miRNA-221 has been proposed as a potential tumor suppressor for melanoma therapy. Moreover, topical delivery miRNA-221 inhibitor gene can avoid or decrease reticulo endothelial system (RES) uptake, reduce systemic toxicity, and provide targeted gene delivery to the tumor site located at the skin



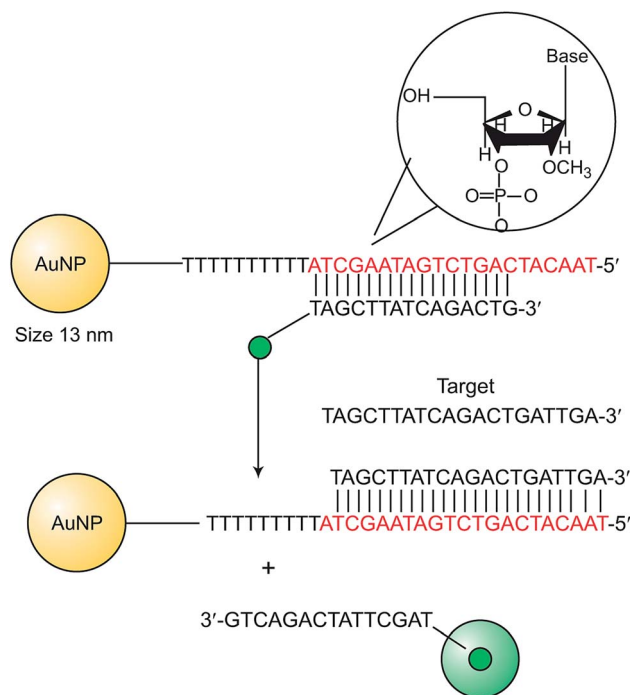


Fig. 3 Schematic representation for miRNA detection using AuNP – 2'-OMe-DNA probes.⁵⁷

subcutaneous layer. However, stratum corneum always poses a formidable challenge to biomacromolecules penetration. To circumvent these problems that confront the current methods, herein, for the first time, they presented a novel strategy for the cutaneous melanoma therapy by topical delivery a pDNA encoded with miRNA-221 inhibitor gene through HIV-1 twinarginine translocation peptide (TAT) conjugated cationic gold nanoparticles.³³

4. Combinatory therapies in cancer treatment using modified gold nanoparticles

In general, ideal non-viral gene vectors offer characteristics, such as chemical stability, biocompatibility, effective targeting, stimulus responsiveness and feasibility for combined treatments (*i.e.* chemotherapy, photothermal therapy, photodynamic therapy, *etc.*).^{38,78,144} Gene delivery vectors reported in the recent years, include polymer-based, lipid-based, and inorganic nanoparticle-based systems.^{129,130} Surface-modified Au

nanomaterials are recognized as promising gene delivery vehicles.^{76,77} The anti-cancer effects of the PEI-Au/siRNA and PEI-Au/siRNA@ZGOC samples were assessed *via in vitro* cell culture for 48 h and 72 h, using exposure to LED light. LED radiation did not appear to induce any clear effect on the PEI-Au/siRNA group but, in contrast the PEI-Au/siRNA@ZGOC group showed a significant decrease in cell viability under LED irradiation.⁸¹ pAuNPs revealed to have high photothermal effect and loading capacity by Au-thiol linkage. Hence, FAM-Dz/TAT-pAuNPs was prepared to target hepatitis C virus (HCV) human hepatocarcinoma cells using hyperthermic treatment *via* photothermal therapy. The loading was successful which proved to be biocompatible and resulted in low cytotoxicity.¹³¹ Combinatorial approach using gene therapy and chemotherapeutic drugs has been successfully done in combination with AuNPs which successfully lead to tumor suppression and ErbB2 gene silencing.⁹⁸

5. Role of modified gold nanoparticles in detection and imaging of tumors

One of the major aspects in treating cancer is accurate detection and imaging of oncogenic cells which enables various therapeutic techniques to eliminate them effectively, many of which are discussed in Table 3. Various gold nanoparticles of different shapes like, gold nanospheres and sizes have been depicted, which illustrate the cellular uptake by cell lines. Cellular uptake is usually observed using confocal microscopy, flow cytometry, Western blot analysis, TEM. Deep tissue imaging with a long period has been achieved *in vivo* using repeated excitation with low-energy LEDs.^{132–134} Several cellular uptake detections can be done using the confocal laser scanning microscopy (CLSM) as mentioned in few examples. A comparison between the cellular uptake of PEI and PEG-Au PENPs has been done using the confocal laser scanning microscopy (CLSM), proving that L25/pDNA polyplex has almost the same cellular uptake as that of PEI/pDNA polyplex.⁸⁸ Also, siRNA/9R/DG-AuNS (hydrazine)-treated cells showed greater fluorescence intensity amongst AuNS, 9R-AuNS, 9R/DG-AuNS and 9R/DG-AuNS (hydrazine).⁶¹ LGCP was successfully detected using confocal microscopy indicating the successful endosomal escape of the LGCP as the separation of the green/red fluorescence from the blue fluorescence took place.⁹³ Transfection analysis of FA-CS-PLGA NPs, CS-PLGA NPs, Au-CS-PLGA NPs and FA-Au-CSPLGA NPs only to be proven that Au functionalized has high cellular uptake than

Table 3 Detection and imaging of tumor cells *via* modified gold nanoparticles

S. no.	Type of gold nanoparticles (shape & size)	Type of cancer treated	Delivery vehicle	Inference	Reference
1	Gold nanoparticles (L25, L50, L100, L200)	HeLa cells	PEG-Au PENPs	L25 has high cellular uptake	88
2	Gold nanoparticles (199.4 ± 25.2 nm)	MCF-7, HepG2 and HEK293 cells	Au-CS-PLGA NPs and FA-Au-CSPLGA NPs	High cellular uptake	95
3	Gold nanosphere (~13 and 50 nm), star (~40 nm)	U87 cells	siRNA	High cellular uptake	118
4	Gold nanoparticles (~10 nm)	MCF-7, A549 cells	GDD, GF	Enhanced cellular uptake	119



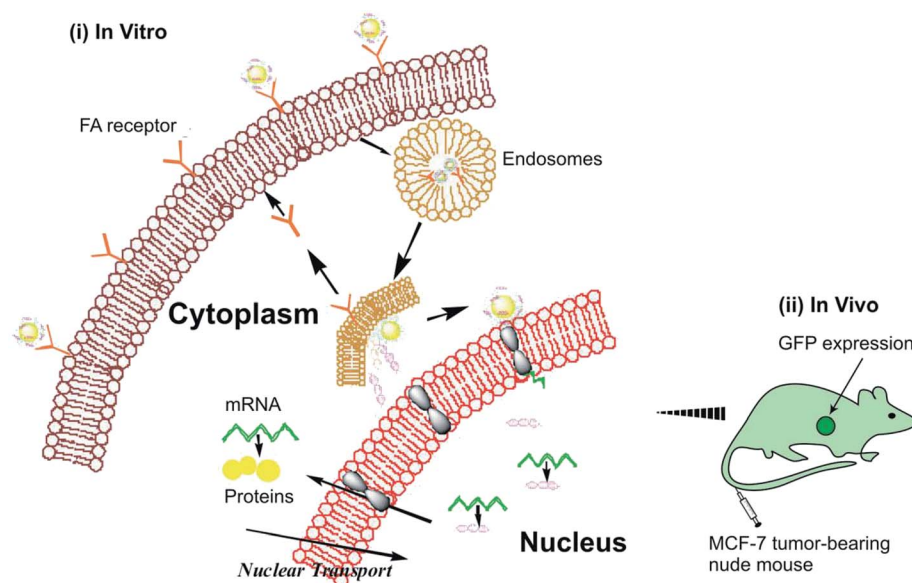


Fig. 4 Depiction of targeted gene delivery of GF/DNA (i) *in vitro* and (ii) *in vivo*.¹²¹

others because it has high atomic number hence easily identified using TEM.¹³⁵ Also it has high zeta potential indicating its stability and increased adsorption of FA and chitosan onto the PLGA.⁶⁰ Direct sequencing method which is used for traditional detection of gene mutations has various setbacks such as complexity, time-consuming, and expensive.^{136,137} So in an experiment done by Xihong Zhao and Chii-Wann Lin., they used colorimetric assays to detect various PNA/DNA complex in AuNPs solution. When PNA is added, colour of the AuNP solution changes from brick-red wine colour to dark purple, on addition of PNA–DNAcomp complex it retains its colour back to brick-red wine colour, and on adding PNA–DNAnc mixture it shows purple colour.¹³⁸ Furthermore, Rajesh Kotcherlakota *et al.*, used confocal microscopy to detect the effect of TDDS on SKOV-3 (HER2+) and MDA-MB-231 (HER2-) cells.⁹⁸ Endosomal escape was also observed using TEM.⁹⁸ Siyu Qian *et al.*, reported an experiment in which they used PBA-AuNPs for detection of miRNA using SPR sensing system as illustrated in Fig. 4.¹³⁹ RNA induces low response in SPR detection as it has lower mass,

hence AuNPs are used to produce effective results for detection as it has high mass.^{140,141}

Western Blot and Nano Tracking Analysis (NTA) were the techniques used for AuNP@PEG@anti-RAB27A to evaluate the exosomes release. Consequence of it was the reduction of exosomes secretion and also exported the nanoparticles to recipient cells, hence decrease of the exosome release.⁷⁴ Confocal microscopy and flow cytometry (FCM) were used to evaluate the gene transfection abilities of GDD and GFs.¹¹⁹ Results showed that GF2.5 showed higher gene transfection efficiency for MCF-7 cells due to enhanced cellular uptake efficiency mediated by the FA targeting ability, but did not so in A549 (FA-receptor-negative cells) (Fig. 5 and 6).¹¹⁹

Confocal microscopy and flow cytometry were used to assess the cellular uptake of both Au DENPs-mPEG and Au DENPs-PEG-FA, implying that FA modification and enhanced the cellular uptake.¹⁴² EGFP (Enhanced green fluorescent protein) was performed to visualize the gene transfection of AHP in HepG2 cells, hence demonstrating it to have highest

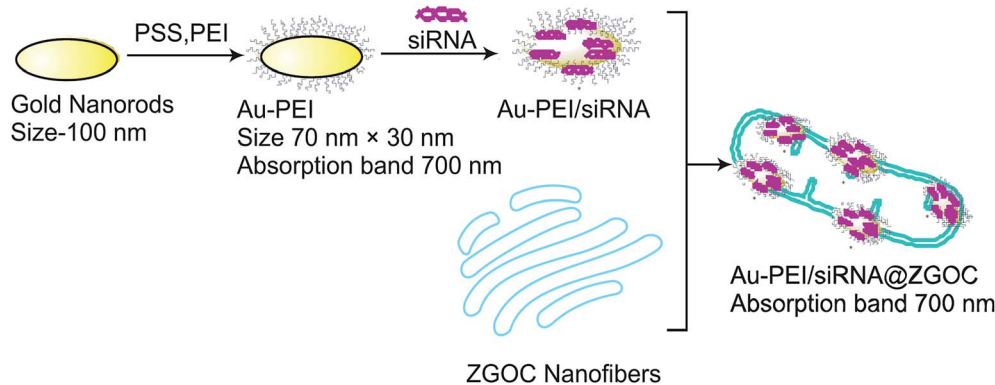


Fig. 5 Schematic illustration of PEI-Au/siRNA onto ZGOC nanofibers.³⁹



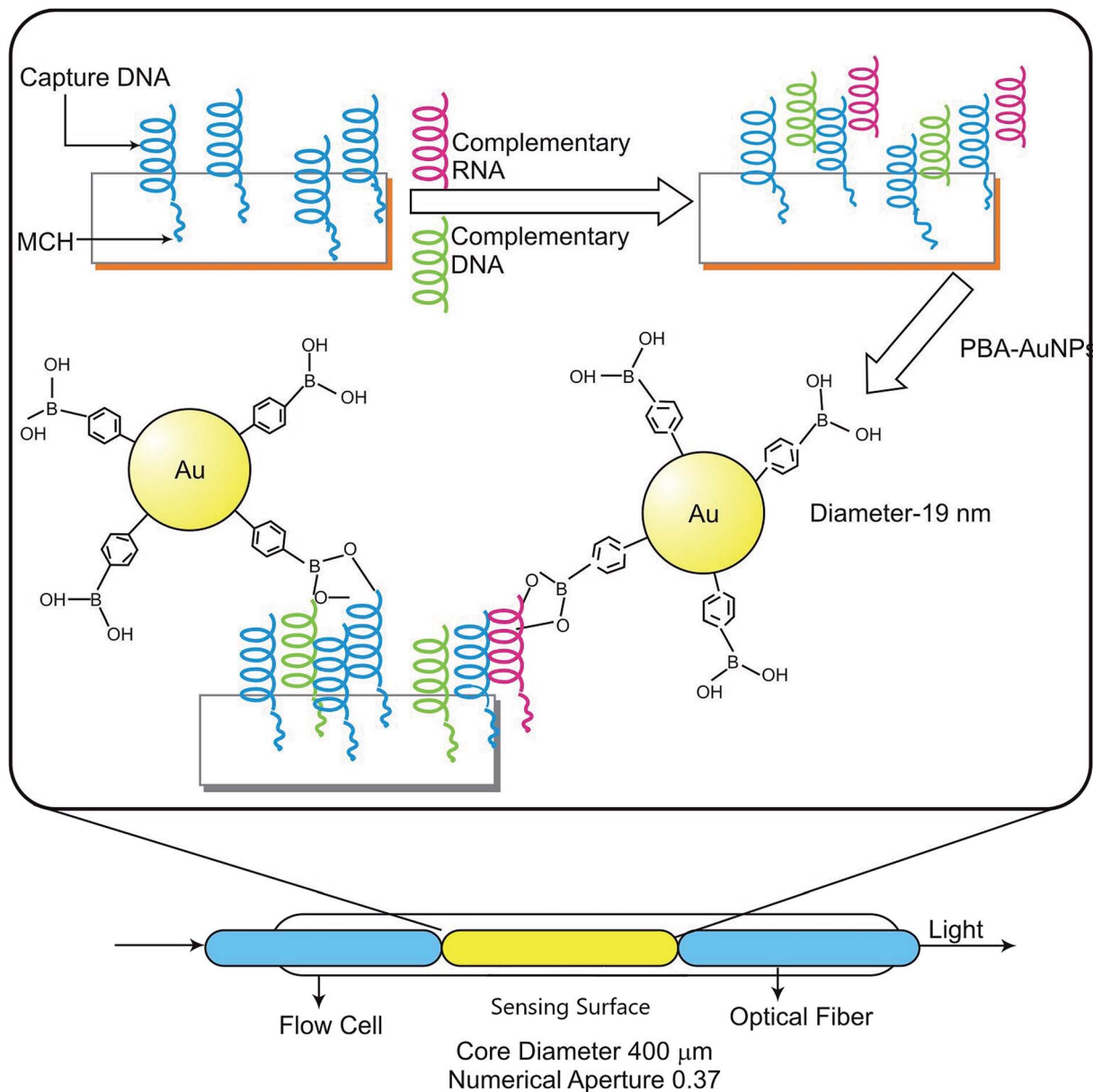


Fig. 6 Combinatorial therapy representing schematic illustration of SPR sensing system for detecting miRNA.¹³⁹

transfection amongst CD-PGEA and PEI.⁷⁵ Also, flow cytometry assay was used to further evaluate the cellular uptake and revealed AHP to have the highest trends.⁷⁵

6. Cytotoxic assays of gene delivery vectors on healthy cells

The detection of cytotoxic effects of gene vectors and nanoparticles for both tumor and normal cells is critical for their translation to clinics. This indicates biocompatibility of gene delivery vehicles and nanoparticles for gene delivery. Haematological and biochemical parameters are main indicators to assess the cytotoxic effects of nanoparticles. Various methods for detection of cytotoxicity levels are MTT assay, cell counting kit-8

(CCK-8), cell viability test, and many more. Moreover, the HA-G5 PAMAM-Au-METase could markedly inhibit the tumor sphere formation rather than HA-G5 PAMAM-METase.⁵⁶ The cytotoxicity assay in an experiment conducted by Aijun Li and team was carried out using Cell Counting Kit-8 (CCK-8) assay, proving that polyethylenimine (PEI) alone is more cytotoxic than PEG-Au PENPs at different concentrations. Cytotoxic levels were found to be in the order $\text{PEI} > \text{L25} > \text{L50} > \text{L100} > \text{L200}$.⁸⁸ Another method used is detection using MTT reduction assay showing that all FA-CS-PLGA NPs, CS-PLGA NPs, Au-CS-PLGA NPs and FA-Au-CSPLGA NPs are non-toxic.⁹⁵ MTT assay tested the cytotoxicity of Au : G5D : DNA, Au : G5D : FA : DNA, G5D : DNA and G5D : FA : DNA and found Au : G5D : DNA, Au : G5D : FA : DNA to be less toxic than G5D : DNA and G5D : FA : DNA.⁶⁰ MTT assay was used to evaluate the cytotoxicity of GDD and GFn,



Table 4 Various other combinatory characteristic features of gold nanoparticles

S. No.	Type of gold nanoparticles (shape & size)	Type of cancer treated/targeted cells	Delivery vehicle	Targeted Functions	Reference
1	Gold nanoparticles (13 nm \pm 2 nm)	Breast cancer	AuNP-2'-OMe-DNA probes	miRNA-21 detection and inhibition leading to apoptotic cells death	57
2	Gold nanoplates	HCV genomic human hepatocarcinoma	TAT/FDz-pAuNPs	To investigate the synergistic effect of NIR irradiation with pAuNPs-based chemotherapy	123
3	Gold nanobeacon (~13 nm)	Colorectal carcinoma	Thiol-DNA-hairpin Cy3 sequences: antisense gold nanobeacon: nonsense gold nanobeacon	To detect and inhibit KRAS gene for a theranostic approach in colorectal carcinoma cells	143

GF2.5 demonstrated to be least cytotoxic.¹¹⁹ CCK-8 assay was used to evaluate the cell viability of non-viral vectors indicating the reduction of cytotoxicity using both Au DENPs-mPEG and Au DENPs-PEG-FA.¹⁴² Using MTT assay it was evaluated that cell viabilities of HEK293 and HepG2 cell lines was above $\approx 60\%$, suggesting the compromised cytotoxicity of AHP.⁷⁵ Many combinatory aspects of employing AuNPs are depicted in Table 4.

7. Conclusion

Gene therapy is a tool for treatment of cancer and genetic diseases. In this review, recent research work done in the field of cancer treatment using gene therapy, *via* surface modified gold nanoparticles has been discussed. There are numerous more therapies like radiotherapy, chemotherapy, immunotherapy, targeted therapy, and hormone therapy. For future prospects, these therapies in combination with gene therapy have better and safer treatments against cancer. Combinatory therapies along with gene therapy using AuNPs as delivery vehicles can be used effectively for the treatment of cancer since most cancers are recurring or have become immune to single therapies used. Also, therapies like chemotherapy and radiotherapy have various side effects which in synergy with gene therapy could reduce their cytotoxicity. Viral and non-viral vectors are commonly used for transfection of therapeutic genes to tumor. Since, viral vectors have less loading capacity, limited mass production, are cytotoxic and show strong unwanted immune activity. Hence, non-viral vectors have wider scope in the future. Their advantages include low cytotoxicity, good binding ability to nucleic acids, nucleic acids release controlling ability, strong binding efficiency to nucleic acids and high cellular uptake. Transfections of nucleic acids and various biomolecules in conjugation with gold nanoparticles to tumor sites have proven to inhibit tumor growth. This suggests the translational approaches toward cancer gene therapy *via* gold nanostructures. Higher cellular uptake, biocompatibility, low cytotoxicity and detection are some of the parameters required for biomolecules as well as gold nanoparticles for translation to clinics. Currently, some of the liposome based nanoparticles are in clinical trials for gene silencing.

Conflicts of interest

There are no conflicts to declare.

References

- 1 S. Duarte, G. Carle, H. Faneca, M. C. P. de Lima and V. Pierrefite-Carle, *Cancer Lett.*, 2012, **324**, 160–170.
- 2 H. J. Kim, A. Kim, K. Miyata and K. Kataoka, *Adv. Drug Deliv. Rev.*, 2016, **104**, 61–77.
- 3 H. Kim and W. J. Kim, *Small*, 2014, **10**, 117–126.
- 4 C. Ma, L. Shi, Y. Huang, L. Shen, H. Peng, X. Zhu and G. Zhou, *Biomater. Sci.*, 2017, **5**, 494–501.
- 5 S. Rietwyk and D. Peer, *ACS Nano*, 2017, **11**, 7572–7586.
- 6 M. W. Amjad, P. Kesharwani, M. C. I. Mohd Amin and A. K. Iyer, *Prog. Polym. Sci.*, 2017, **64**, 154–181.
- 7 J. Li, C. W. T. Leung, D. S. H. Wong, J. Xu, R. Li, Y. Zhao, C. Y. Y. Yung, E. Zhao, B. Z. Tang and L. Bian, *ACS Appl. Mater. Interfaces*, 2019, **11**(25), 22074–22084.
- 8 D. Lee, K. Upadhye and P. N. Kumta, *J. Mater. Sci. Eng. B*, 2012, **177**, 289–302.
- 9 C. Zhang, Y. Yong, L. Song, X. Dong, X. Zhang, X. Liu, Z. Gu, Y. Zhao and Z. Hu, *Adv. Healthcare Mater.*, 2016, **5**, 2776–2787.
- 10 D. Bumcrot, M. Manoharan, V. Kotliansky and D. W. Sah, *Nat. Chem. Biol.*, 2006, **2**(12), 711–719.
- 11 R. Shahbazi, B. Ozpolat and K. Ulubayram, *Nanomedicine*, 2016, **11**(10), 1287–1308.
- 12 B. Ozpolat, A. K. Sood and G. Lopez-Berestein, *J. Intern. Med.*, 2010, **267**(1), 44–53.
- 13 M. E. Davis, J. E. Zuckerman, C. H. J. Choi, D. Seligson, A. Tolcher, C. A. Alabi, Y. Yen, J. D. Heidel and A. Ribas, *Nature*, 2010, **464**(7291), 1067–1070.
- 14 A. Fire, S. Xu, M. K. Montgomery, S. A. Kostas, S. E. Driver and C. C. Mello, *Nature*, 1998, **391**(6669), 806–811.
- 15 K. V. Morris and D. J. Looney, *Science*, 2004, **305**, 1289–1292.
- 16 V. Winstel, P. Kuhner, B. Krismer, A. Peschel and H. Rohde, *Appl. Environ. Microbiol.*, 2015, **81**, 2481–2488.
- 17 L. Smith, M. Wloch, M. Ye, L. Reyes, S. Boutsaboualoy, C. Dunne, J. Chaplin, D. Rusalov, A. Rolland, C. Fisher, M. Al-Ibrahim, M. Kabongo, R. Steigbigel, R. Belshe, E. Kitt, A. Chu and R. Moss, *Vaccine*, 2010, **28**, 2565–2572.



- 18 J. Shen, H. C. Kim, C. Mu, E. Gentile, J. Mai, J. Wolfram, L. N. Ji, M. Ferrari, Z. W. Mao and H. Shen, *Adv. Healthcare Mater.*, 2014, **3**, 1629–1637.
- 19 Z. Yang, T. Liu, Y. Xie, Z. Sun, H. Liu, J. Lin, C. Liu, Z. W. Mao and S. Nie, *Acta Biomater.*, 2015, **25**, 194–204.
- 20 J. H. Choi, H. J. Hwang, S. W. Shin, J. W. Choi, S. H. Um and B. K. Oh, *Nanoscale*, 2015, **7**, 9229–9237.
- 21 B. K. Wang, X. F. Yu, J. H. Wang, Z. B. Li, P. H. Li, H. Wang, L. Song, P. K. Chu and C. Li, *Biomaterials*, 2016, **78**, 27–39.
- 22 E. Boisselier and D. Astruc, *Chem. Soc. Rev.*, 2009, **38**(6), 1759–1782.
- 23 M. S. Draz, B. A. Fang, P. Zhang, Z. Hu, S. Gu, K. C. Weng, J. W. Gray and F. F. Chen, *Theranostics*, 2014, **4**(9), 872–892.
- 24 M. Shilo, T. Reuveni, M. Motiei and R. Popovtzer, *Nanomedicine*, 2012, **7**(2), 257–269.
- 25 R. K. Sharma, S. Gulati and S. Mehta, *J. Chem. Educ.*, 2012, **89**, 1316–1318.
- 26 R. K. Sharma, S. Sharma, S. Gulati and A. Pandey, *Anal. Methods*, 2013, **5**, 1414–1426.
- 27 P. Pant, R. Bansal, S. Gulati, S. Kumar and R. Kodwani, *Journal of Nanostructures in Chemistry*, 2016, **6**, 145–157.
- 28 S. Kumar, *Anti-Cancer Agents Med. Chem.*, 2016, **16**, 200–211.
- 29 B. Madan, S. Batra and B. Ghosh, *Mol. Pharmacol.*, 2000, **58**, 526–534.
- 30 M. Sardana, V. Agarwal, A. Pant, V. Kapoor, K. C. Pandey and S. Kumar, *Asian Pac. J. Trop. Biomed.*, 2018, **8**(5), 268–272.
- 31 K. V. Morris and D. J. Looney, *Science*, 2004, **305**, 1289–1292.
- 32 L. Aagaard and J. J. Rossi, *Adv. Drug Delivery Rev.*, 2007, **59**, 75–86.
- 33 R. Shahbazi, E. Asik, N. Kahraman, M. Turk, B. Ozpolat and K. Ulubayram, *Nanomedicine*, 2017, **12**, 16.
- 34 R. Shahbazi, B. Ozpolat and K. Ulubayram, *Nanomedicine*, 2016, **11**(10), 1287–1308.
- 35 Y. Xie, H. Qiao, Z. Su, M. Chen, Q. Ping and M. Sun, *Biomaterials*, 2014, **35**, 7978–7991.
- 36 Y. Deng, C. C. Wang, K. W. Choy, Q. Du, J. Chen, Q. Wang, L. Li, T. K. Chung and T. Tang, *Gene*, 2014, **538**, 217–227.
- 37 S. J. Lee, M. J. Kim, I. C. Kwon and T. M. Roberts, *Adv. Drug Deliv. Rev.*, 2016, **104**, 2–15.
- 38 R. Acharya, S. Saha, S. Ray, S. Hazra, M. K. Mitra and J. Chakraborty, *Mater. Sci. Eng., C*, 2017, **76**, 1378–1400.
- 39 L. Qin, P. Yan, C. Xie, J. Huang, Z. Ren, X. Li, S. Best, X. Cai and G. Hana, *Nanoscale*, 2018, **10**, 13432–13442.
- 40 P. Resnier, T. Montier, V. Mathieu, J. P. Benoit and C. Passirani, *Biomaterials*, 2013, **34**(27), 6429–6443.
- 41 G. Meister, M. Landthaler, Y. Dorsett and T. Tuschl, *RNA*, 2004, **10**, 544–550.
- 42 R. H. Wang, J. Bai, J. Deng, C. J. Fang and X. Chen, *ACS Appl. Mater. Interfaces*, 2017, **9**(7), 5828–5837.
- 43 Q. Cheng, L. Du, L. Meng, S. Han, T. Wei, X. Wang, Y. Wu, X. Song, J. Zhou, S. Zheng, Y. Huang, X. J. Liang, H. Cao, A. Dong and Z. Liang, *ACS Appl. Mater. Interfaces*, 2016, **8**(7), 4347–4356.
- 44 Y. Zhao, M. L. Huan, M. Liu, Y. Cheng, Y. Sun, H. Cui, D. Z. Liu, Q. B. Mei and S. Y. Zhou, *Sci. Rep.*, 2016, **6**, 35267.
- 45 Y. Zhao, X. Qi, J. Chen, W. Wei, C. Yu, H. Yan, M. Pu, Y. Li, L. Miao, C. Li and J. Ren, *Cancer Lett.*, 2017, **408**, 102–111.
- 46 J. Kim, C. Jeong and W. J. Kim, *Adv. Drug Deliv. Rev.*, 2016, **98**, 99–112.
- 47 M. Sandbothe, R. Buurman, N. Reich, L. Greiwe, B. Vajen, E. Gurlevik, V. Schaffer, M. Eilers, F. Kuhnel, A. Vaquero, T. Longerich, S. Roessler, P. Schirmacher, M. P. Manns, T. Illig, B. Schlegelberger and B. Skawran, *J. Hepatol.*, 2017, **66**(5), 1012–1021.
- 48 X. Su, H. Wang, W. Ge, M. Yang, J. Hou, T. Chen, N. Li and X. Cao, *Cancer Res.*, 2015, **75**(14), 2875–2885.
- 49 L. Giunti, R. M. Da, S. Vinci, S. Gelmini, A. L. Iorio, A. M. Buccoliero, S. Cardellicchio, F. Castiglione, L. Genitori and M. M. De, *Am. J. Cancer Res.*, 2015, **5**(1), 231–242.
- 50 H. Li, Y. Mu and J. Lu, *Anal. Chem.*, 2014, **86**, 3602–3609.
- 51 C. C. Harris, *J. Natl. Cancer Inst.*, 1996, **88**, 1442–1455.
- 52 D. Naor, *Front. Immunol.*, 2016, **7**, 39.
- 53 D. M. Kokkinakis, A. G. Brickner, J. M. Kirkwood, X. Liu, J. E. Goldwas-ser, A. Kastrama, C. Sander, D. Bocangel and S. Chada, *Mol. Cancer Res.*, 2006, **4**, 575–589.
- 54 S. P. Chaplot and I. D. Rupenthal, *J. Pharm. Pharmacol.*, 2014, **66**, 542.
- 55 Y. Shan, T. Luo, C. Peng, R. Sheng, A. Cao, X. Cao, M. Shen, R. Guo, H. Tomás and X. Shi, *Biomaterials*, 2012, **33**, 3025–3035.
- 56 Y. F. Li, H. T. Zhang and L. Xin, *J. Cancer Res. Clin. Oncol.*, 2018, **12**, 16.
- 57 J. Lia, J. Huang, X. Yanga, Y. Yang, K. Quan, N. Xie, Y. Wu, C. Ma and K. Wang, *Talanta*, 2018, **183**, 11–17.
- 58 Q. Chen, K. Li, S. Wen, H. Liu, C. Peng, H. Cai, M. Shen, G. Zhang and X. Shi, *Biomater.*, 2013, **34**, 5200.
- 59 S. Mansouri, Y. Cuie, F. Winnik, Q. Shi, P. Lavigne, M. Benderdour, E. Beaumont and J. C. Fernandes, *Biomater.*, 2006, **27**, 2060.
- 60 L. S. Mbatha and M. Singh, *J. Nanosci. Nanotechnol.*, 2019, **19**, 1959–1970.
- 61 H. Zhu, W. Liu, Z. Cheng, K. Yao, Y. Yang, B. Xu and G. Su, *Int. J. Mol. Sci.*, 2017, **18**, 2029.
- 62 Y. Lei, L. Tang, Y. Xie, Y. Xianyu, L. Zhang, P. Wang, Y. Hamada, K. Jiang, W. Zheng and X. Jiang, *Nat. Commun.*, 2017, **8**, 15130.
- 63 C. Sardo, B. Bassib, E. F. Craparo, C. Scialabba, E. Cabrinib, G. Dacarrob, A. D'Agostinob, A. Tagliettib, G. Giammonaa, P. Pallavicinib and G. Cavallaro, *Int. J. Pharm.*, 2017, **519**, 113–124.
- 64 R. Goyal, C. H. Kapadia, J. R. Melamed, R. S. Riley and E. S. Day, *Cell. Mol. Bioeng.*, 2018, **11**(5), 383–396.
- 65 A. Verma and K. Mehta, *Curr. Cancer Drug Targets*, 2007, **7**, 559–565.
- 66 J. Wang, M. Thomas, P. Lin, J. X. Cheng, D. E. Matei and A. Wei, *Bioconjugate Chem.*, 2019, **30**(2), 443–453.
- 67 S. M. Mantovani and B. S. Moore, *J. Am. Chem. Soc.*, 2013, **135**, 18032–18035.
- 68 V. Nandwana, I. Samuel, G. Cooke and V. M. Rotello, *Accounts Chem. Res.*, 2012, **46**, 1000–1009.



- 69 A. Sau, S. Sanyal, K. Bera, S. Sen, A. K. Mitra, U. Pal, P. K. Chakraborty, S. Ganguly, B. Satpati, C. Das and S. Basu, *ACS Appl. Mater. Interfaces*, 2018, **10**(5), 4582–4589.
- 70 C. Bang and T. Thum, *Int. J. Biochem. Cell Biol.*, 2012, **44**, 2060–2064.
- 71 C. Roma-Rodrigues, A. R. Fernandes and P. V. Baptista, *BioMed Res. Int.*, 2014, **2014**, 1–10.
- 72 J. Zhang, S. Li, L. Li, M. Li, C. Guo, J. Yao and S. Mi, *J. Proteomics Bioinf.*, 2015, **13**, 17–24.
- 73 B. N. Hannafon and W. Q. Ding, *Int. J. Mol. Sci.*, 2013, **14**, 14240–14269.
- 74 C. Roma-Rodrigues, F. Pereira, A. P. A. de Matos, M. Fernandes, P. V. Baptista and A. R. Fernandes, *Nanomed. Nanotechnol. Biol. Med.*, 2017, **13**(4), 1389–1398.
- 75 X. Chen, Q. Zhang, J. Li, M. Yang, N. Zhao and F. J. s Xu, *ACS Nano*, 2018, **12**(6), 5646–5656.
- 76 J. H. Choi, H. J. Hwang, S. W. Shin, J. W. Choi, S. H. Um and B. K. Oh, *Nanoscale*, 2015, **7**, 9229–9237.
- 77 B. K. Wang, X. F. Yu, J. H. Wang, Z. B. Li, P. H. Li, H. Wang, L. Song, P. K. Chu and C. Li, *Biomaterials*, 2016, **78**, 27–39.
- 78 H. J. Kim, A. Kim, K. Miyata and K. Kataoka, *Adv. Drug Deliv. Rev.*, 2016, **104**, 61–77.
- 79 K. J. F. Carnevale and G. F. Strouse, *Bioconjugate Chem.*, 2018, **29**(10), 3429–3440.
- 80 Z. Zhang, L. Wang, J. Wang, X. Jiang, X. Li, Z. Hu, Y. Ji, X. Wu and C. Chen, *Adv. Mater.*, 2012, **24**, 1418–1423.
- 81 J. Niu, Y. Chua, Y. F. Huang, Y. S. Chong, Z. H. Jiang, Z. W. Mao, L. H. Peng and J. Q. Gao, *ACS Appl. Mater. Interfaces*, 2017, **9**(11), 9388–9401.
- 82 J. R. Baker Jr, *Hematol Am Soc Hematol Educ Program*, 2009, **1**, 708–719.
- 83 J. Deng, N. Li, K. Mai, C. Yang, L. Yan and L. M. Zhang, *J. Mater. Chem.*, 2011, **21**, 5273–5281.
- 84 V. M. Platt and F. C. Szoka, *Mol. Pharm.*, 2008, **5**, 474–486.
- 85 W. Wang, S. Huang, J. Yuan, X. Xu, H. Li, Z. Lv, W. Yu, S. Duan and Y. Hu, *Mol. Pharm.*, 2018, **15**(9), 3767–3776.
- 86 O. Boussif, F. Lezoualc'h, M. A. Zanta, M. D. Mergny, D. Scherman, B. Demeneix and J. P. Behr, *Proc. Natl. Acad. Sci. U. S. A.*, 1995, **92**, 7297–7301.
- 87 U. Lungwitz, M. Breunig, T. Blunk and A. Göpferich, *Eur. J. Pharm. Biopharm.*, 2005, **60**, 247–266.
- 88 A. Li, J. Qiu, B. Zhou, B. Xu, Z. Xiong, X. Hao, X. Shi and X. Cao, *Arabian J. Chem.*, 2018, DOI: 10.1016/j.arabj.2018.06.009.
- 89 D. Wang and R. N. DuBois, *Oncogene*, 2010, **29**, 781.
- 90 W. K. K. Wu, J. J. Y. Sung, C. W. Lee, J. Yu and C. H. Cho, *Cancer Lett.*, 2010, **295**, 7–16.
- 91 X. Z. Yang, J. Z. Du, S. Dou, C. Q. Mao, H. Y. Long and J. Wang, *ACS Nano*, 2012, **6**, 771.
- 92 L. Zhang, W. Zheng, R. Tang, N. Wang, W. Zhang and X. Jiang, *Biomaterials*, 2016, **104**, 269.
- 93 P. Wang, L. Zhang, Y. Xie, N. Wang, R. Tang, W. Zheng and X. Jiang, *Adv. Sci.*, 2017, **4**, 1700175.
- 94 Y. G. Assaraf, C. P. Leamon and J. A. Reddy, *Drug Resist. Updates*, 2014, **17**, 89.
- 95 J. Akinyelu and M. Singh, *J. Nanosci. Nanotechnol.*, 2018, **18**(7), 4478–4486.
- 96 M. F. Press, G. Sauter, L. Bernstein, I. E. Villalobos, M. Mirlacher, J. Y. Zhou, R. Wardeh, Y. T. Li, R. Guzman, Y. Ma, J. Sullivan-Halley, A. Santiago, J. M. Park, A. Riva and D. J. Slamon, *Clin. Cancer Res.*, 2005, **11**, 6598–6607.
- 97 A. Berchuck, R. Whitaker, G. Olt, J. T. Soper, D. L. Clarke-Pearson, A. Kamel, R. C. Bast Jr and S. Yin, *Cancer Res.*, 1990, **50**, 4087–4091.
- 98 R. Kotcherlakotaa, D. J. Srinivasanb, S. Mukherjeea, M. M. Haroonb, G. H. Darb, U. Venkatramanb, C. R. Patra and V. Gopal, *J. Mater. Chem. B*, 2017, **5**, 7082–7098.
- 99 A. A. Bapat, G. Hostetter and D. D. Von Hoff, *Nat. Rev. Cancer*, 2011, **11**, 695–707.
- 100 G. O. Ceyhan, I. E. Demir, U. Rauch, F. Bergmann, M. W. Müller, M. W. Büchler, H. Friess and K. H. Schäfer, *Am. J. Gastroenterol.*, 2009, **104**, 2555–2565.
- 101 P. D. Zamore, T. Tuschl, P. A. Sharp and D. P. Bartel, *Cell*, 2000, **101**, 25–33.
- 102 S. M. Hammond, E. Bernstein, D. Beach and G. J. Hannon, *Nature*, 2000, **404**, 293–296.
- 103 L. A. MacFarlane and P. R. Murphy, *Curr. Genom.*, 2010, **11**, 537–561.
- 104 Z. W. Wu, C. T. Chien, C. Y. Liu, J. Y. Yan and S. Y. Lin, *J. Drug Target.*, 2012, **20**, 551–560.
- 105 K. A. Avery-Kiejda, S. G. Braye, A. Mathe, J. F. Forbes and R. J. Scott, *BMC Cancer*, 2014, **14**, 51.
- 106 L. Li, L. Yuan, J. Luo, J. Gao, J. Guo and X. Xie, *Clin. Exp. Med.*, 2013, **13**, 109–117.
- 107 D. Ben-Shushan, E. Markovsky, H. Gibori, G. Tiram, A. Scamparin and R. Satchi-Fainaro, *Drug Delivery Transl. Res.*, 2014, **4**, 38–49.
- 108 H. Dong, J. Lei, L. Ding, Y. Wen, H. Ju and X. Zhang, *Chem. Rev.*, 2013, **113**(8), 6207–6233.
- 109 D. Sidransky, *Science*, 1997, **278**(5340), 1054–1058.
- 110 D. P. Bartel, *Cell*, 2004, **116**(2), 281–297.
- 111 A. Shenoy and R. H. Blelloch, *Nat. Rev. Mol. Cell Biol.*, 2014, **15**(9), 565–576.
- 112 M. Jin, T. Zhang, C. Liu, M. A. Badeaux, B. Liu, R. Liu, C. Jeter, X. Chen, A. V. Vlassov and D. G. Tang, *Cancer Res.*, 2014, **74**(15), 4183–4195.
- 113 G. A. Calin and C. M. Croce, *Nat. Rev. Cancer*, 2006, **6**(11), 857–866.
- 114 B. J. Reinhart, F. J. Slack, M. Basson, A. E. Pasquinelli, J. C. Bettinger, A. E. Rougvie, H. R. Horvitz and G. Ruvkun, *Nature*, 2000, **403**(6772), 901–906.
- 115 B. Li, P. Chen, Y. Chang, J. Qi, H. Fu and H. Guo, *Biochem. Biophys. Res. Commun.*, 2016, **478**(2), 739–745.
- 116 H. Lee, S. Han, C. S. Kwon and D. Lee, *Protein Cell*, 2016, **7**(2), 100–113.
- 117 D. J. Li, Y. Chen and Z. Liu, *Chem. Soc. Rev.*, 2015, **44**(22), 8097–8123.
- 118 D. Sturm, S. Bender, D. T. W. Jones, P. Lichter, J. Grill, O. Becher, C. Hawkins, J. Majewski, C. Jones, J. F. Costello, A. Iavarone, K. Aldape, C. W. Brennan, N. Jabado and S. M. Pfister, *Nat. Rev. Cancer*, 2014, **14**, 92–107.
- 119 L. Galluzzi, O. Kepp, M. G. Vander Heiden and G. Kroemer, *Nat. Rev. Drug Discov.*, 2013, **12**, 829–846.



- 120 J. Yue, T. J. Feliciano, W. Li, A. Lee and T. W. Odom, *Bioconjugate Chem.*, 2017, **28**(6), 1791–1800.
- 121 B. Du, X. Gu, X. Han, G. Ding, Y. Wang, D. Li, E. Wang and J. Wang, *ChemMedChem*, 2017, **12**, 1768–1775.
- 122 K. Zagorovsky, L. Y. T. Chou and W. C. M. Chan, *Proc. Natl. Acad. Sci. U. S. A.*, 2016, **113**, 13600–13605.
- 123 L. Y. Chou, K. Zagorovsky and W. C. Chan, *Nat. Nanotechnol.*, 2014, **9**, 148–155.
- 124 R. Prado-Gotor and E. Grueso, *Phys. Chem.*, 2011, **3**, 1479–1489.
- 125 E. Grueso, P. Perez-Tejeda, R. Prado-Gotor and C. Cerrillos, *J. Phys. Chem. C*, 2014, 4416–4428.
- 126 E. Grueso, P. Perez-Tejeda, R. M. Giráldez-Pérez, R. Prado-Gotor and F. Muriel-Delgado, *J. Colloid Interface Sci.*, 2018, **529**, 65–76.
- 127 J. B. Wolinsky, Y. L. Colson and M. W. Grinstaff, *J. Controlled Release*, 2012, **159**, 14–26.
- 128 M. Ihle, M. Trautmann, H. Kuenstlinger, S. Huss, C. Heydt, J. Fassunke, E. Wardelmann, S. Bauer, H. Schildhaus, R. Buettner and S. Merkelbach-Bruse, *Mol. Oncol.*, 2015, **9**, 1421–1433.
- 129 S. Rietwyk and D. Peer, *ACS Nano*, 2017, **11**, 7572–7586.
- 130 C. Zhang, Y. Yong, L. Song, X. Dong, X. Zhang, X. Liu, Z. Gu, Y. Zhao and Z. Hu, *Adv. Healthcare Mater.*, 2016, **5**, 2776–2787.
- 131 S. Kang, K. Kang, H. Huh, H. Kim, S. J. Chang, T. Jung Park, Ki S. Chang, D.-H. Min and H. Jang, *ACS Appl. Mater. Interfaces*, 2017, **9**(40), 35268–35278.
- 132 Z. Zhou, W. Zheng, J. Kong, Y. Liu, P. Huang, S. Zhou, Z. Chen, J. Shi and X. Chen, *Nanoscale*, 2017, **9**, 6846–6853.
- 133 W. Fan, N. Lu, C. Xu, Y. Liu, J. Lin, S. Wang, Z. Shen, Z. Yang, J. Qu, T. Wang, S. Chen, P. Huang and X. Chen, *ACS Nano*, 2017, **11**, 5864–5872.
- 134 J. Shi, M. Sun, X. Sun and H. Zhang, *J. Mater. Chem. B*, 2016, **4**, 7845–7851.
- 135 R. Yuvakkumar, V. Elango, V. Rajendran and N. Kannan, *Digest Journal of Nanomaterials and Biostructures*, 2011, **6**, 1771.
- 136 X. Zhao, J. Zhong, C. Wei, C. W. Lin and T. Ding, *Front. Microbiol.*, 2017, **8**, 580.
- 137 X. Zhao, C. W. Lin, J. Wang and D. H. Oh, *J. Microbiol. Biotechnol.*, 2014, **24**, 297–312.
- 138 X. Zhao and C. W. Lin, *RSC Adv.*, 2017, **7**, 48554–48560.
- 139 S. Qian, M. Lin, W. Ji, H. Yuan, Y. Zhang, Z. Jing, J. Zhao, J. F. Masson and W. Peng, *ACS Sens*, 2018, **3**(5), 929–935.
- 140 L. He, M. D. Musick, S. R. Nicewarner, F. G. Salinas, S. J. Benkovic, M. J. Natan and C. D. Keating, *J. Am. Chem. Soc.*, 2000, **122**(38), 9071–9077.
- 141 S. Szunerits, J. Spadavecchia and R. Boukherroub, *Rev. Anal. Chem.*, 2014, **33**, 153.
- 142 B. Xu, A. Li, X. Hao, R. Guo, X. Shi and X. Cao, *RSC Adv.*, 2018, **8**, 1265.
- 143 Y. Li, H. Wang, K. Wang, Q. Hu, Q. Yao, Y. Shen, G. Yu and G. Tang, *Small*, 2017, **13**, 1602697.
- 144 C. Ma, L. Shi, Y. Huang, L. Shen, H. Peng, X. Zhu and G. Zhou, *Biomater. Sci.*, 2017, **5**, 494–501.

