

Cite this: *RSC Adv.*, 2019, 9, 3946

Co-amorphous palbociclib–organic acid systems with increased dissolution rate, enhanced physical stability and equivalent biosafety†

Man Zhang, Xinnuo Xiong, Zili Suo, Quan Hou, Na Gan, Peixiao Tang, * Xiaohui Ding and Hui Li 

The preparation of co-amorphous drug systems by adding a small molecular excipient is a promising formulation in the modern pharmaceutical industry to improve the solubility, dissolution rate, and bioavailability of poorly soluble drugs. In this study, palbociclib co-amorphous systems with organic acids (succinic, tartaric, citric, and malic acid) at molar ratios of 1 : 1 were prepared by co-milling and characterized by differential scanning calorimetry (DSC), fourier transform infrared spectroscopy (FTIR) and solid-state nuclear magnetic resonance (SS-NMR). These solid-state investigations have confirmed the formation of co-amorphous salts between PAL and organic acids. The solubility, dissolution rate and stability of the four co-amorphous drug systems were significantly improved compared with these of crystalline and amorphous palbociclib. The biosafety of the co-amorphous drug systems was the same as that of palbociclib without affecting the efficacy of the drug and eliciting toxic side effects. These comprehensive approaches for the palbociclib–acid co-amorphous drug systems provided a theoretical basis for its clinical applications.

Received 26th November 2018

Accepted 23rd January 2019

DOI: 10.1039/c8ra09710k

rsc.li/rsc-advances

1. Introduction

Approximately 40% of marketed drugs and 75% of clinical research drugs exhibit limited water solubility,^{1,2} which severely limits the absorption of drugs and increases the side effects of oral drugs.^{3–5} Polymer is usually added to prepare an amorphous solid dispersion, increasing the dissolution rate and stability of the amorphous drug.⁶ Nevertheless, this technique has considerable drawbacks; for instance, the hygroscopicity of many polymers and the limited miscibility of drugs to polymers increases the volume and weight of formulations.^{7–9} Using small molecular ligands to prepare co-amorphous systems rather than drug–polymer combinations has gained considerable interest in the pharmaceutical field.^{10–12} Co-amorphous drug systems are composed of a fixed stoichiometric ratio of API and other small-molecule solid substances (organic acids, amino acids, or drugs) that forming a homogeneous single-phase solid formulation.^{13–15} An active drug and a ligand may interact *via* ionic bonds, hydrogen bonds, or other noncovalent bonds, which overcomes the disadvantages of amorphous drugs that it easily crystallizes, thereby improving the physical properties of drugs.^{16–18} For example, ionic interactions in indomethacin–arginine co-amorphous system remarkably enhanced the

intrinsic dissolution rate and physical stability relative to amorphous indomethacin.¹⁹ Tryptophan bound to carbamazepine *via* hydrogen bonding and π – π interaction.²⁰ Meanwhile, co-amorphous can improve the drug release properties through the precipitation of drug rich phase of nano/micro dimensions.²¹ Since co-amorphous drug systems show an improvement in supersaturation ability, it is a promising drug system for increasing the solubility of poorly soluble drugs and stabilizing amorphous drugs.^{22–24}

Palbociclib (PAL, Fig. 1A) is the first highly selective inhibitor of CDK4/6 approved by the FDA in treating advanced breast cancer.²⁵ PAL inhibits not only the proliferation of breast cancer cells in combination with letrozole but also the proliferations of human hepatocellular carcinoma cells, colon cancer, and mantle cell lymphoma.²⁶ As a heavyweight drug for breast cancer, the effectiveness of oral PAL monotherapy is greatly reduced, and its toxic side effects are increased because of its low solubility and poor bioavailability.^{27,28} Unfortunately, there has not been published any peer reviewed study on solid state forms of PAL such as polymorphs and amorphous solid dispersions in the current research.

In recent years, research on co-amorphous system has focused on the structural characterization, solubility, and dissolution properties.²⁹ Few reports had confirmed the formation of co-amorphous salts between weakly basic APIs and acidic excipients and evaluated the biosafety of co-amorphous formulation compared to the existing formulation in this field. This paper aims to study the co-amorphous drug systems from the perspective of bonding performance and biosafety.

School of Chemical Engineering, Sichuan University, Chengdu, Sichuan, 610065, China. E-mail: lihuilab@sina.com; tangpeixiao@126.com; Fax: +86 028 85401207; Tel: +86 026 85405220

† Electronic supplementary information (ESI) available. See DOI: 10.1039/c8ra09710k

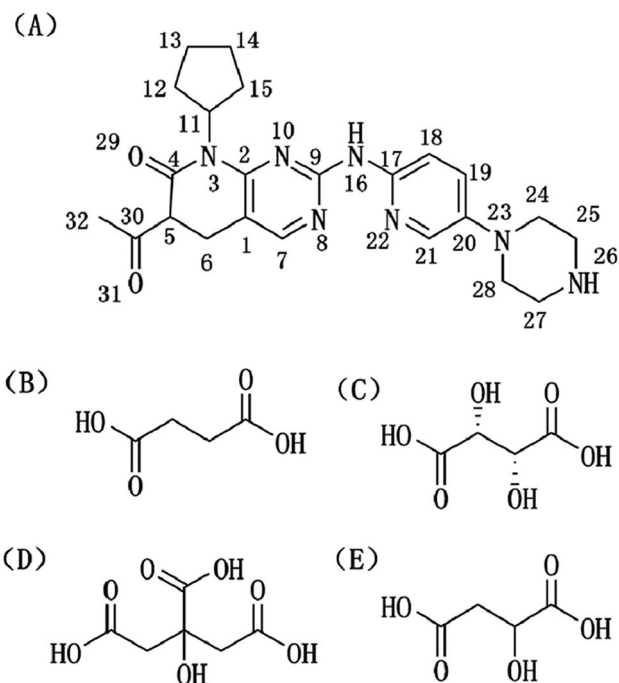


Fig. 1 Molecular structures of (A) palbociclib (PAL), (B) succinic acid (SUC), (C) L-tartaric acid (TAR), (D) citric acid anhydrous (CIT), and (E) D,L-malic acid (MAL).

Four co-amorphous drug systems of PAL and organic acids (succinic, tartaric, citric, and malic acid, Fig. 1B–E) were prepared by co-milling and performed DSC, IR, and SS-NMR to explore the intermolecular bonding properties between PAL and organic acids. The biosafety of the four co-amorphous drug systems was assessed through cytotoxicity experiments. The effects of the addition of several organic acids on normal kidney cells, normal breast cells, and breast cancer cells were evaluated. These researches on the co-amorphous systems presented a safe and effective formulation technology for the development of new PAL solid forms with great dissolution rates, good physical stability, and high bioavailability.

2. Experiments and methods

2.1 Materials

The main drug crystalline PAL (>98%, $\rho_0 = 1.313 \text{ g cm}^{-3}$) was obtained from Chemsky International Co., Ltd. (Shanghai, China). Succinic acid (SUC, $\rho_1 = 1.572 \text{ g cm}^{-3}$), L-tartaric acid (TAR, $\rho_2 = 1.76 \text{ g cm}^{-3}$), citric acid anhydrous (CIT, $\rho_3 = 1.542 \text{ g cm}^{-3}$), and D,L-malic acid (MAL, $\rho_4 = 1.601 \text{ g cm}^{-3}$) were purchased from Kelong Company, Ltd. (Chengdu, China). All of the reagents were of analytical grade. Millipore water was used in the cell experiments.

2.2 Preparation of co-amorphous and physical mixtures

Co-amorphous of PAL-acids systems (SUC, TAR, CIT, MAL) were prepared by co-milling in a ball mill (LNMN-QM 0.4L, Heishan Xinlun Agate Handicrafts Co., Ltd. China) for 4 hours at 25 °C.

A total mass of 1 g of the PAL and four organic acid at molar ratios of 1 : 1 were placed into four agate balls jars (50 cm³) containing 10 agate balls ($\varnothing = 10 \text{ mm}$) and 30 agate balls ($\varnothing = 3 \text{ mm}$). Amorphous PAL was prepared by milling crystalline PAL for 6 hours. The rotation speed of the solar disk was set to 574 rpm, and alternate co-milling periods (typically 10 min) with pause periods (typically 2 min) were applied to limit the mechanical heating of the sample.

Physical Mixtures (PM) were prepared by geometric mixing of crystalline PAL with each acid in 1 : 1 molar ratio using a motor and pestle for a few minutes.

2.3 Analytical techniques

2.3.1 Powder X-ray diffractometry (XRD). XRD measures were performed to confirm the crystalline or amorphous nature of the powder samples at 25 °C by using a diffractometer (X'Pert PRO; PANalytical, Almelo, Netherlands) with a PIXcel 1D detector and Cu K α radiation. The diffraction data were collected in a 2θ range of 4–50° at a step size of 0.01313°.

2.3.2 Scanning electron microscopy (SEM). The morphological characteristics of the studied samples were examined under a SEM (JSM-7500F; JEOL, Tokyo, Japan) at 15.0 kV. Electrically conductive samples were prepared by coating with a thin gold layer in vacuum prior to examination.

2.3.3 Thermogravimetric analysis (TGA). Thermogravimetric analysis (TGA) was performed using an analyzer (TG209F1 Iris; Netzsch, Selb, Germany) in aluminum crucibles at a heating rate of 10 °C min^{−1} from 40 °C to 600 °C under nitrogen purging (60 mL min^{−1}).

2.3.4 Differential scanning calorimetry (DSC). DSC thermograms were obtained using a differential scanning calorimeter Q200 (TA Instruments Co., New Castle, DE, USA). Samples (3–5 mg) were exposed to aluminum pans, heated from 40 °C to the decomposition temperature at a rate of 10 °C min^{−1} under nitrogen purging (50 mL min^{−1}). The heating temperature of PAL-acid CM and PM was lower than the decomposition temperature based on the weight loss of the TGA curve (ESI Fig. S1†). The glass transition temperature (T_g) was determined as the midpoint of onset and end temperature of the heat capacity change at the T_g . The theoretical T_g of the co-amorphous (T_{g12}) was calculated from the Gordon–Taylor eqn (1):³⁰

$$T_{g12} = \frac{w_1 T_{g1} + k w_2 T_{g2}}{w_1 + k w_2} \quad (1)$$

where T_{g1} and T_{g2} are the T_g of drug and acids, respectively; w_1 and w_2 represent the weight fractions of two components; and k is a constant that can be expressed by the following formula (2):³¹

$$k = \frac{T_{g1} \times \rho_1}{T_{g2} \times \rho_2} \quad (2)$$

where ρ_1 and ρ_2 are the densities of the drug and acid, respectively.

2.3.5 Hot-stage polarized optical microscopy (HSM). The HSM method was performed with polarizing microscope (Leica DMLP, Germany) equipped a heating stage (LTS350) and



camera (Power Shot S50). A small amount of amorphous PAL placed on the slide was heated in a hot bench oven from 40 °C to 280 °C at 5 °C min⁻¹. Co-amorphous samples were heated from 40 °C to 80 °C at a heating rate of 5 °C min⁻¹ and from 80 °C to 150 °C at a heating rate of 2 °C min⁻¹.

2.3.6 Fourier transform infrared spectroscopy (FTIR). FTIR spectra were obtained with a Nicolet 6700 Fourier Transform Infrared Spectroscopy spectrometer (Thermo Fisher Scientific, USA). Each sample was dispersed in KBr, ground in mortar and pestle, and disk was prepared by applying pressure about 1000 psig. A total of 64 scans were performed (with a spectral resolution of 4 cm⁻¹) over the range of 4000–400 cm⁻¹. Data analysis was performed using IR solution software.

2.3.7 Nuclear magnetic resonance (NMR). The Solid-State Nuclear Magnetic Resonance (SS-NMR) spectra of the studied samples were obtained on a Bruker AV II-500 MHz NMR operating spectrometer. ¹³C SS-NMR spectra were recorded using a double-tuned cross-polarization magic-angle spinning probe. Approximately 500 mg of the samples was used for each run. ¹H NMR spectra of the samples were obtained at 295 K with a Bruker Avance 400 spectrometer (Germany) at 400 MHz. DMSO-d₆ and D₂O were used to dissolve all the samples, respectively.

2.4 Solubility and dissolution studies

UV-vis spectrophotometer (TU-1901, Peking General Instrument, China) was used to estimate the supersaturation solubility profile. To estimate dissolution kinetics, supersaturated solutions were prepared by adding a large excess of the samples to phosphate buffer (pH = 6.8). The solutions were stirred at 37 °C for a specified amount of time. Each sample was filtered through a 0.45 μm syringe, immediately diluted and concentration was estimated using UV-vis spectroscopy. Powder dissolution studies were conducted in triplicate and the average values have been reported.

Co-amorphous dissolution experiments were conducted using a ZRC-8D dissolution tester (Chuangxing, Tianjin, China) at 100 rpm and 37 ± 0.5 °C (paddle). Powder samples containing 75 mg of PAL equivalent were introduced to the dissolution medium of 900 mL (pH = 6.8 phosphate buffer solution). Then, 5 mL of the eluted sample was withdrawn at 2, 5, 10, 15, 30, 45, 60, 120, 180, and 240 min, filtered through a 0.45 μm syringe, and supplemented with 5 mL of phosphate buffer solution in a buffer vessel. At least triplicate samples were used for each measurement.

2.5 Physical stability test

The stability of the form was investigated at 40 °C under relative humidity (RH) levels of 32%, 57%, and 75%, which were achieved with the saturated salt solutions of MgCl₂, NaBr, and NaCl in desiccators, respectively. The samples were repeatedly analyzed through XRD at 3, 15, 30, and 90 days.

2.6 Cytotoxicity evaluation

The cytotoxicity of PAL and PAL-acid co-amorphous systems on breast cancer cells (MDA-MB-453, MCF-7), normal breast cells

(MCF-10A), and renal epithelial cells (293T) were detected through MTT assay. After the cells were cultured in the logarithmic growth phase at a seeding density of 3.0 × 10³–5.0 × 10³ cells per well for 24 h in a 96-well plate, the drug of the specified concentration gradient (DMSO dissolution, medium dilution) was added, and the test was repeated thrice. The cells were cultured in an incubator at 37 °C, 5% CO₂, and saturated humidity for 48 h. Afterward, 20 μL of MTT (5 mg mL⁻¹) was added to each well. The specimens were further incubated at 37 °C for 4 h, the medium was carefully aspirated, 150 μL of DMSO was added to each well to dissolve the purple crystals, and the shaker was slowly shaken to dissolve the crystals sufficiently. Absorbance at 492 nm was obtained using a microplate reader (Molecular Devices, USA).

3. Results and discussion

3.1 Preparation of co-amorphous drug systems

We recorded peak changes at various milling times by XRD measurements (Fig. 2). The diffraction peaks of the four systems and PAL itself gradually weaken as the milling time increases, eventually becoming an amorphous halo. However, the four ligand organic acids remained crystalline during the corresponding milling time. The phenomenon initially indicated the formations of amorphous PAL and PAL-acid co-amorphous mixtures (CM). We utilized four organic acids: succinic (SUC), tartaric (TAR), citric (CIT), and malic acid (MAR) to increase the stability of amorphous PAL. The pK_a and ΔpK_a values of the acids are summarized in Table 1. According to the empirical pK_a rule, the salt formation can be distinguished from the co-crystals when the ΔpK_a (pK_a(base) – pK_a(acid)) is greater than 3.^{32,33} Since the pK_a values are reflections in the aqueous solution,³⁴ it is difficult to accurately assess molecular interactions of PAL-acid co-amorphous systems based on ΔpK_a values.

3.2 Micromorphology analysis

The micromorphological characteristics and particle size of the amorphous samples at μm scale were observed through scanning electron microscopy. The crystalline and amorphous PAL presented regular prismatic or rod-like structures (Fig. 3a and b). The columnar structure was more favorable for the mixing uniformity of PAL with organic acids than the tabular structure. Amorphous PAL showed needle morphology at a magnification of 20 000×. This structure was much smaller than that of crystalline PAL. Four free organic acids appeared in large block morphology at a 100 μm magnification scale (Fig. S3†). Compared with amorphous PAL, the micromorphological of four co-amorphous had changed. The block structures of the four co-amorphous particles were larger than PAL, and the surface of the former was smoother than that of the latter (Fig. 3c–f).

3.3 Thermal analysis

The Gordon–Taylor equation assumes that no specific interaction occurs between the two molecules.²⁰ Consequently, the deviation between the experimental T_g value and the theoretical



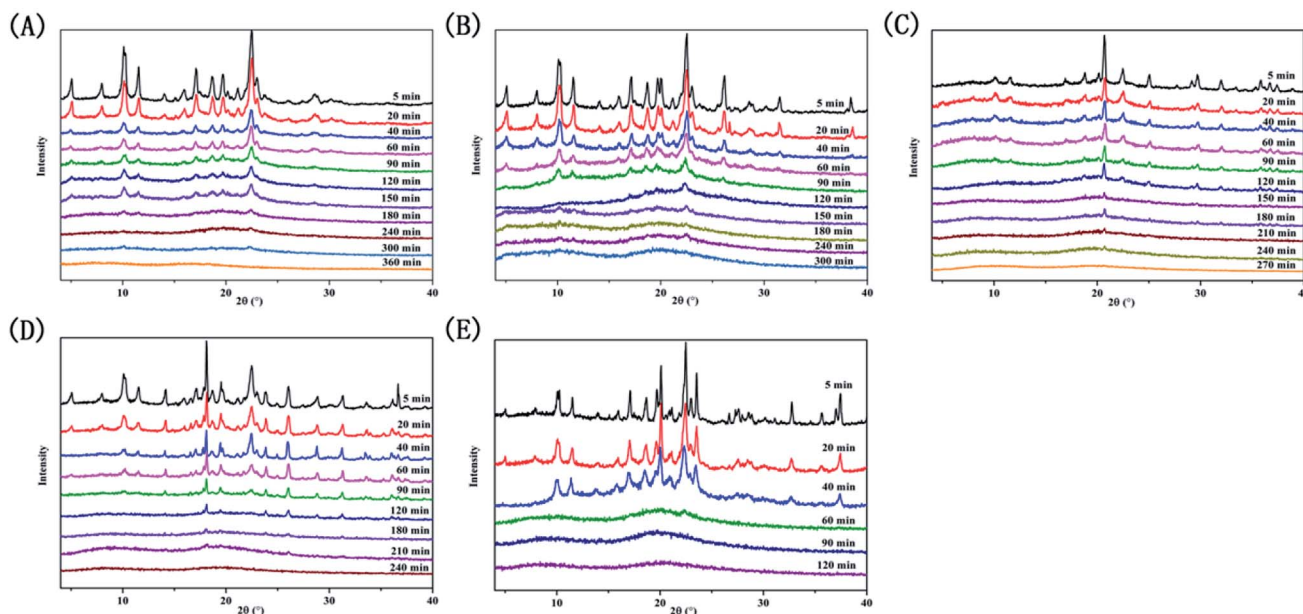


Fig. 2 X-ray powder diffraction patterns at selected time intervals. (A) PAL, (B) PAL-SUC CM, (C) PAL-TAR CM, (D) PAL-CIT CM, and (E) PAL-MAL CM.

T_g value represents the intensity of the molecular interaction. The determination of the glass transition temperature (T_g) of the co-amorphous systems is a reliable method to evaluate intermolecular interaction.^{7,8}

Unfortunately, the amorphization of four organic acids were not obtained by ball milling (Fig. S2†) and only the T_g value of CIT was reported as 11 °C, which resulted in the difficulty of predicting the T_g of co-amorphous systems.² In case of co-

amorphous PAL-SUC, PAL-TAR, and PAL-MAL, it assumed that the T_g values of the organic acid were equal to $0.67 \times T_m$ (melting point) according to the empirical formula.³⁵ Although this formula was incompletely accurate, it provided a basis for calculating T_g values of acid and then calculated the T_g value of co-amorphous system.³⁶ The calculated T_g values of SUC, TAR, and MAL were 37, 24, and -2 °C, respectively.

The experimental T_g value of amorphous PAL was approximately 50 °C, whereas the addition of the four organic acids led to a significant increase in T_g values of the co-amorphous systems (Fig. 4 and Table 2). The experimental T_g value of co-amorphous PAL-CIT was 70 °C, much higher than the calculated one. When ΔT_g (experimental T_g value – theoretical T_g value) was higher, stronger interactions, such as ionic bonds, may exist between drugs molecules and organic acid molecules.³⁴ Meanwhile, the experimental T_g values of the other three systems were also higher than the calculated ones. ΔT_g values predicted the formation of co-amorphous salts between PAL and organic acids in these four systems. This strong electrostatic interaction between PAL and the acid molecules greatly interfered with the short-range order of the amorphous PAL molecule and consequently inhibited the tendency of the PAL-acid co-amorphous to recrystallize.

HSM was applied to monitor the recrystallization of amorphous PAL and co-amorphous products.^{37,38} As shown in Fig. 5, amorphous PAL recrystallized at approximately 100 °C and began to melt at 250 °C, which was consistent with the DSC result in Fig. 4 (98 °C for recrystallization and 260 °C for melting). The birefringence observed in the four co-amorphous forms of HSM at 80–100 °C corresponded to the recrystallization peak in DSC (Fig. 5c–f). However, only PAL-SUC and PAL-MAL systems clearly showed the obvious needle crystalline forms under HSM. The co-amorphous PAL-TAR and PAL-CIT observed in HSM became yellow needle-like or block near the

Table 1 Acids used in co-amorphous systems^a

	pK_{a1} , acid	$\Delta pK_a = pK_{a1}$, PAL – pK_{a1} , acid
Succinic acid	4.2	3.2
Tartaric acid	2.9	4.5
Citric acid	3.1	4.3
Malic acid	3.5	3.9

^a The pK_{a1} of the most acidic site in each acid.^{31,32}

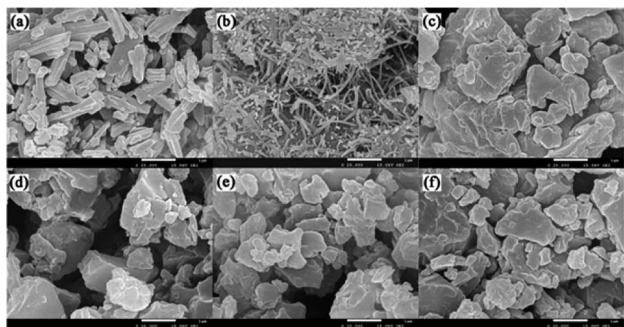


Fig. 3 SEM images of powder sample: (a) crystalline PAL, (b) amorphous PAL, (c) PAL-SUC CM, (d) PAL-TAR CM, (e) PAL-CIT CM, and (f) PAL-MAL CM. The images were magnified at 20 000×.



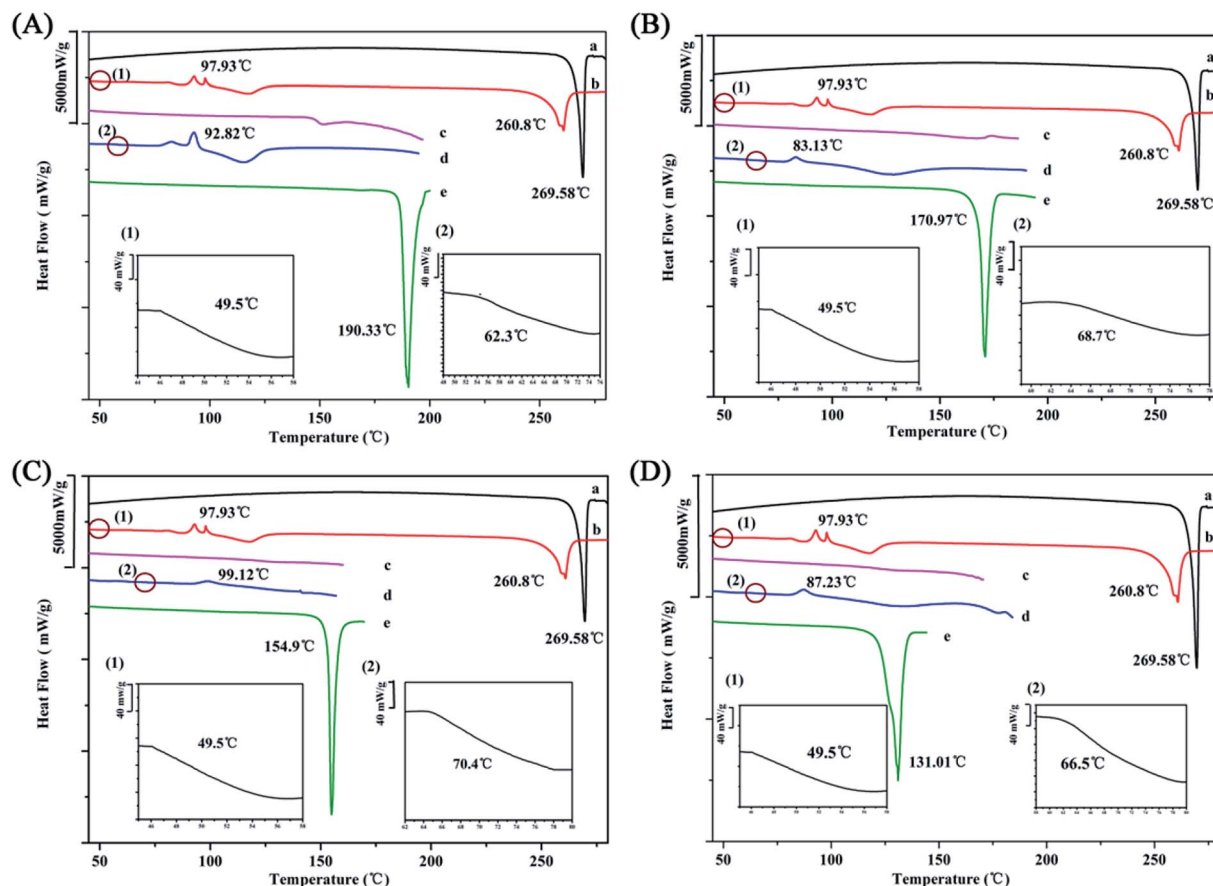


Fig. 4 DSC curves of (A) PAL-SUC, (B) PAL-TAR, (C) PAL-CIT, and (D) PAL-MAL. Each picture from top to bottom: (a) crystalline PAL, (b) amorphous PAL, (c) PAL-acid PM, (d) PAL-acid CM, and (e) crystalline organic acid. Images (1) and (2) were partially enlarged views of amorphous PAL and PAL-acid CM near T_g , respectively.

Table 2 Experimental and Calculated T_g of the PAL-acid Co-amorphous Systems

	Experimental T_g (°C)	Calculated T_g (°C)	ΔT_g (°C)
PAL	49 ± 1.8	—	—
PAL-SUC	62.3 ± 1.4	47	15
PAL-TAR	68.7 ± 0.9	41	27
PAL-CIT	70.4 ± 0.8	25	45
PAL-MAL	66.5 ± 1.2	-11	77

recrystallization temperature compared with that in the absence of refraction at 40 °C (Fig. S4†). The results showed that the co-amorphous samples were easily converted into crystals when the temperature was higher than 80 °C because amorphous PAL and co-amorphous PAL-acid in high-energy states lack a long-range disordered structure, which absorbed energy during heating, and the disorderly molecular orientation moves for recrystallization.³⁹

3.4 Spectroscopic characterization

The bonding properties between PAL and four organic acids were characterized through FTIR and SS-NMR. The results are shown in Fig. 6 and 7. No significant change was observed in the

carbonyl vibration in the 1900–1650 cm^{-1} region of the IR spectra. As such, the N–H stretching region was mainly compared in these four systems. The N–H stretching of pure amorphous PAL exhibited a bathochromic shift from 3421.24 cm^{-1} to 3413.79 cm^{-1} , whereas the N–H bending vibration (at 1556.09 and 1553.48 cm^{-1} in the crystalline PAL) merged and shifted to 1549.67 cm^{-1} (Fig. 6A). Co-amorphous

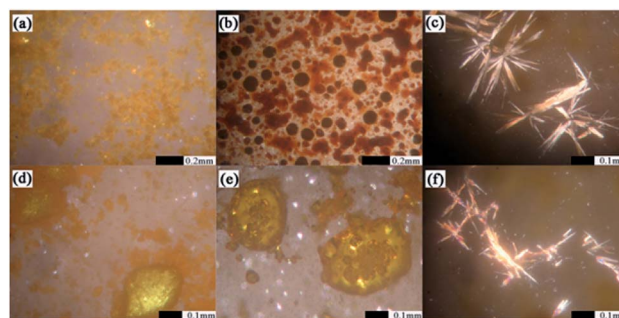


Fig. 5 HSM of amorphous solid sample: (a) amorphous PAL at 100 °C, begin to appear with birefringence; (b) amorphous PAL at 250–270 °C, gradually begin to melt; (c) PAL-SUC CM at 85–95 °C; (d) PAL-TAR CM at 80–90 °C; (e) PAL-CIT CM at 95–105 °C; and (f) PAL-MAL CM at 85–100 °C.



PAL-SUC had a broad peak at 2492.68 cm^{-1} and a sharp peak at 2867.04 cm^{-1} compared with its physical mixture. The same peak changes were observed in PAL-TAR, PAL-CIT, PAL-MAL co-amorphous systems, whereas these shifts were not detected in the corresponding physical mixtures (Fig. 6B–E). The appearances of these new peaks around 2490 and 2860 cm^{-1} were attributed to the stretching vibration of amine salt. These findings confirmed the formation of co-amorphous salts between PAL and the organic acids.

Molecular interactions between PAL and four organic acids were further investigated through SS-NMR. Amorphous samples were broader than crystalline PAL and PAL-acid physical

mixtures because of a wide range of molecular orientations. No significant shifts were observed in the four co-amorphous ^{13}C and ^{31}P of carbonyl groups, and the ^{15}N on the pyrimidine ring (corresponding to crystalline PAL 165.86, 205.71, and 161.86 ppm, respectively, Fig. S5†). Therefore, the most potential site in PAL was ^{26}N located in piperazine ring, and the strength of the PAL-acid interaction was determined by studying the displacement of ^{24}C – ^{25}C .

The studied amorphous solids corresponding to the crystalline samples with 29–36 ppm multiple peaks on SS-NMR broadened and merged into one or two peaks with a small shift because of the anisotropy of chemical shift and the

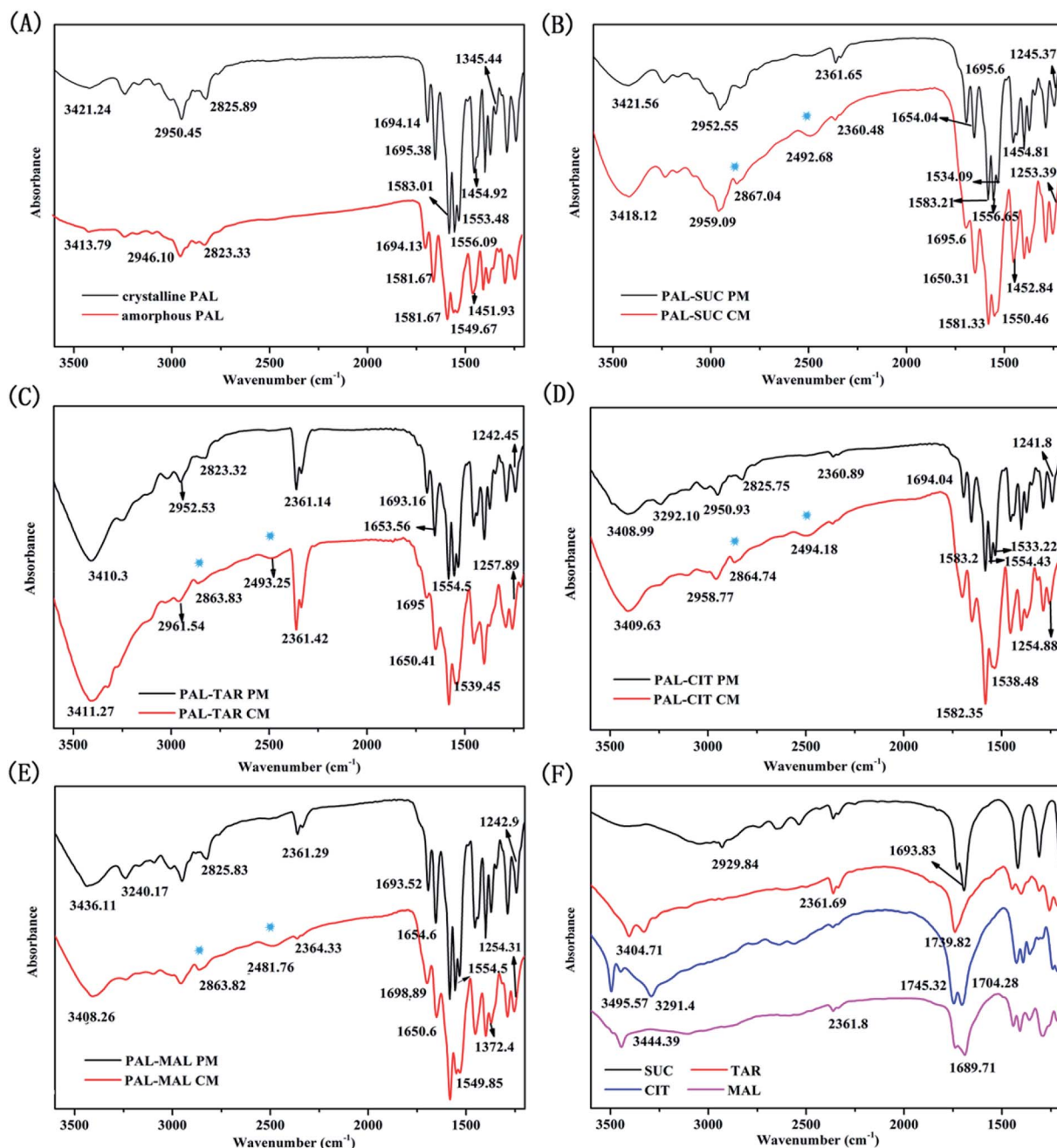
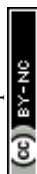


Fig. 6 FT-IR spectra of (A) crystalline PAL and amorphous PAL; (B) PAL-SUC PM and PAL-SUC CM; (C) PAL-TAR PM and PAL-TAR CM; (D) PAL-CIT PM and PAL-CIT CM; (E) PAL-MAL PM and PAL-MAL CM; and (F) four organic acids.



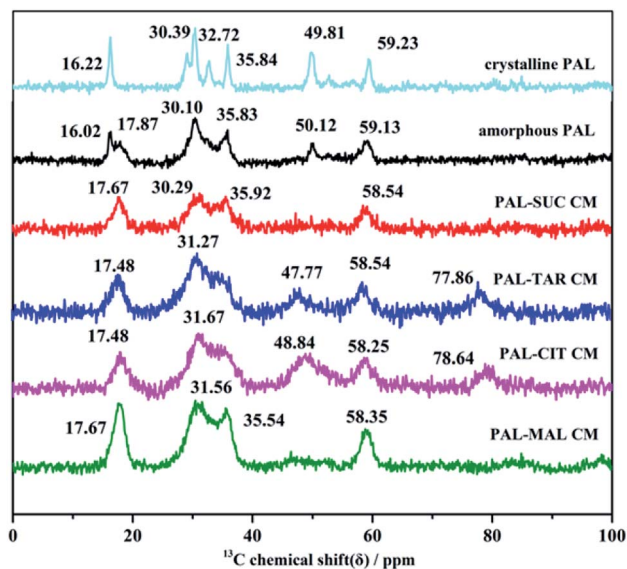


Fig. 7 Solid-state ^{13}C NMR spectra of crystalline PAL, amorphous PAL, and four co-amorphous PAL–acid systems (CM).

interaction between amorphous molecules. The chemical shifts of ^{24}C in the four PAL–acid PM were approximately 59.42 ppm, which corresponded to the resolved peak in crystalline PAL observed at 59.23 ppm. This peak in PAL–acid CM had a change in the chemical shift of 1.0–0.7 ppm, moving to approximately 58.35 ppm (Fig. 7). The protonation of ^{26}N increased the shielding effect on the piperazine ring, thereby exhibiting a slight variation. The results of SS-NMR further confirmed that the four co-amorphous drug systems were the structure of co-amorphous salts. ^1H NMR spectra of the samples proved that actual chemical composition of the co-amorphous particles is the salt of the drug PAL and the acid at a molar ratio of 1 : 1 (Fig. S6†).

3.5 Solubility and dissolution rate tests

Since the PAL–acid co-amorphous drug systems were developed to increase its aqueous solubility, powder dissolution studies and dissolution rate experiments were conducted. Four co-amorphous systems had the desired spring and parachute supersaturation profile, in the absence of crystallisation inhibitors. A crystallization behavior involves the development of supersaturation, nucleation and the subsequent.¹⁷ The concentration of the drug in the supersaturated solution is much greater than its solubility, which may cause the reprecipitation of dissolved drug in dissolution medium.²³ Just as expected, crystalline PAL had a slow and low dissolution in pH = 6.8 buffer solution, and the supersaturation solubility after 24 h was only $35.27\ \mu\text{g mL}^{-1}$ (Fig. 8A). For amorphous PAL, its supersaturated dissolution profile showed that the maximum solubility was $181.53\ \mu\text{g mL}^{-1}$ after 15 min and then the dissolution began to fall. It was possible that the amorphous PAL may gradually recrystallize for 15 min, and then transform into the crystalline drug itself after one hour. Fig. 8A showed that the co-amorphous PAL–SUC reached the highest level of supersaturation ($1034.06\ \mu\text{g mL}^{-1}$) after 5 minutes. Meanwhile,

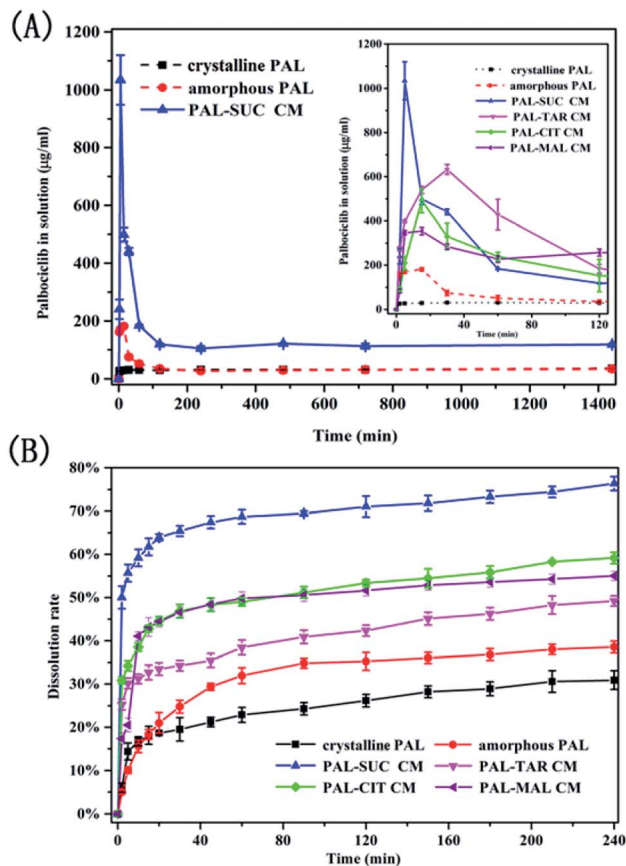


Fig. 8 Supersaturated dissolution profile (A) and dissolution rate curves (B) of crystalline PAL, amorphous PAL, and PAL–acid CM.

The supersaturated dissolution profile of the other three co-amorphous systems was also significantly higher than the API itself.

It could be seen from Fig. 8B that the drug dissolved approximately 31% for crystalline PAL and 38% for amorphous PAL after 4 h. Four co-amorphous forms showed faster dissolution rates and higher cumulative dissolutions compared with the crystalline PAL. Among them, PAL–SUC displayed the most fast dissolution rate which released 50% of the drug within 2 min. Moreover, the cumulative dissolution of PAL–SUC after 4 h was 76%, representing a greater than 2-fold increase than that of amorphous PAL (Fig. 8B). The improvement in the dissolution rates of the co-amorphous system were attributed to co-amorphous salts between PAL and acid, since corresponding PAL–acid physical mixtures had a similar dissolution rate as crystalline PAL (Fig. S7†). These results suggested that four co-amorphous systems had solubility and dissolution advantages while PAL–SUC showed optimal properties and it might be in favour of its oral bioavailability.

3.6 Physical stability

This study explored the effects of temperature and humidity on amorphous PAL and co-amorphous PAL–acid. The pure amorphous PAL converted to crystalline state at $40\ ^\circ\text{C}$ for 3 days (Fig. 9B, S8 and S9†). Co-amorphous PAL–SUC and PAL–MAL



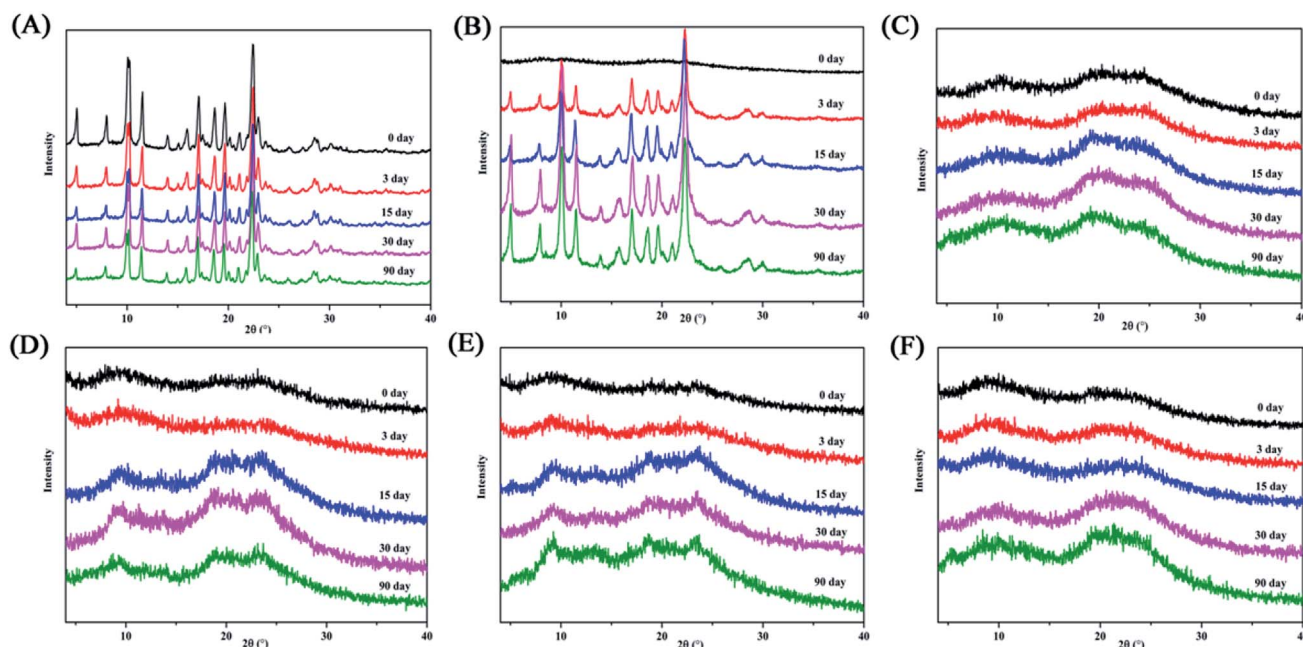


Fig. 9 XRD diffractograms for (A) crystalline PAL, (B) amorphous PAL, (C) PAL-SUC CM, (D) PAL-TAR CM, (E) PAL-CIT CM, and (F) PAL-MAL CM stored at 40 °C/RH 75% over a specified period.

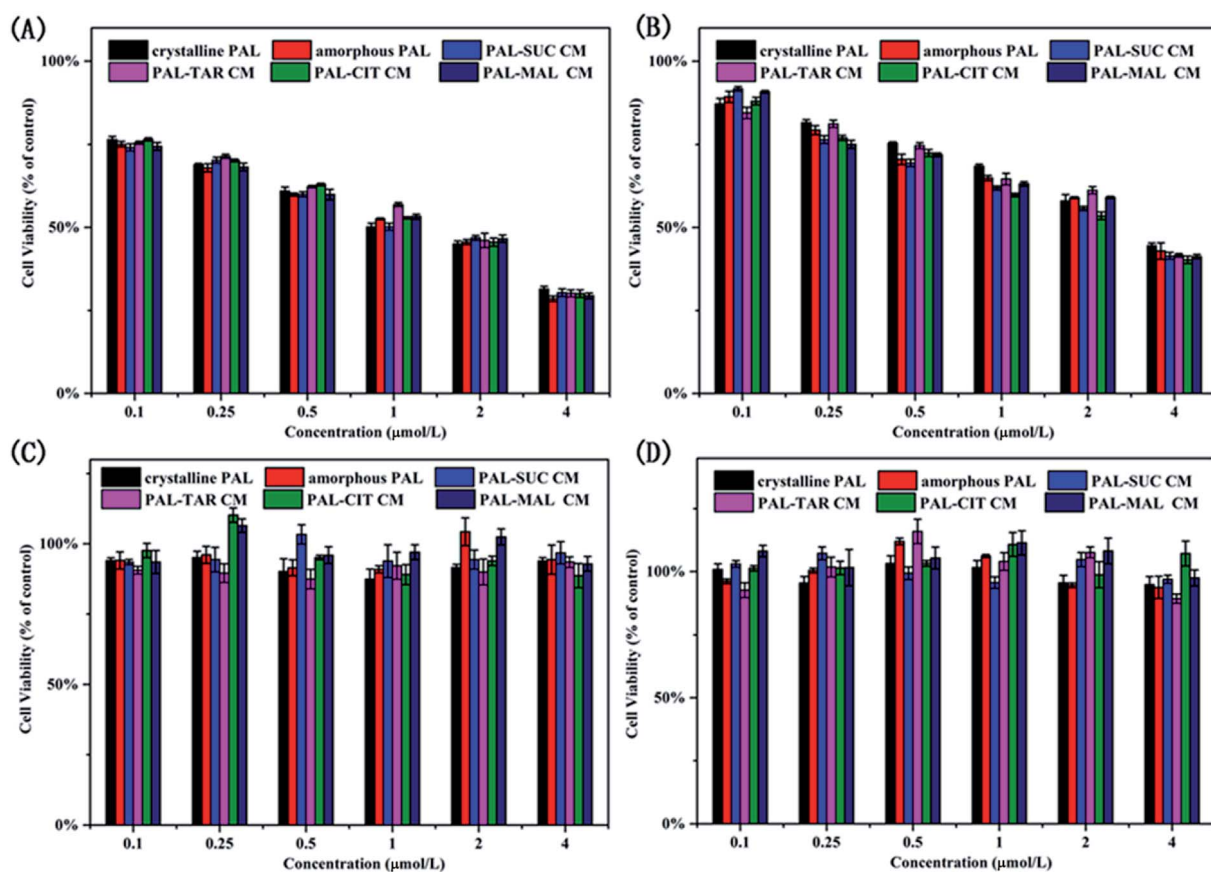
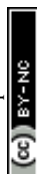


Fig. 10 Proliferation inhibition of (A) MDA-MB-453, (B) MCF-7, (C) MCF-10A, and (D) 293T treated with crystalline PAL, amorphous PAL, and PAL-acid CM.



systems maintained an amorphous halo after 3 months under accelerated conditions (40 °C, 75% RH), while co-amorphous PAL-TAR and PAL-CIT had a tendency to recrystallize after half a month (Fig. 9C–F). Four co-amorphous samples were stable at 40 °C storage conditions. The stability test under 40 °C temperature and various humidity conditions revealed that co-amorphous PAL-acid forms were more stable than amorphous PAL. Among them, co-amorphous PAL-SUC and PAL-MAL were more stable systems. The stabilizing effect of organic acids on amorphous drugs may due to the interaction of carboxylic acid groups with drugs, thereby interfering with the interaction between drug molecules and enhancing the stability of systems.

3.7 Cytotoxicity evaluation

In view of biosafety considerations, we investigated the toxic effects of the co-amorphous drug system on the cells and the drug efficacy, although the four organic acids used in co-amorphous systems are recognized as safer ligands. We utilized two breast cancer cells and two normal cells to explore a co-amorphous biosafety. The effects of the addition of several organic acids on normal kidney cells, normal breast cells, and breast cancer cells were evaluated. Four ligand acids did not influence the growth of cells. The results of cell experiments with four small molecule ligands also demonstrated that the four organic acids used in the co-amorphous drug systems had no toxic side effects on normal cells and breast cancer cells (Fig. S10†).

From Fig. 10A and B, the inhibition rate on MDA-MB-453 cells was higher than that of MCF-7 cells, and the addition of organic acid did not change the PAL efficacy on breast cancer cells. The co-amorphous systems had an equivalent inhibition rate for cancer cells compared with that of the drug substance. PAL formed three hydrogen bonds between ^8N , ^{16}N with CDK6-cyclin V101 and $^{31}\text{C}=\text{O}$ with DFG-D163 N–H to inhibit cancer cell growth,²⁵ the co-amorphous forms displayed an ionic bond between ^{26}N on the piperazine ring with a carboxyl group in acid. The action sites of the pharmacophore and the co-amorphous binding are inconsistent, thereby the formation of the co-amorphous salt did not affect the drug effect, which was also proved by cell experiments. Meanwhile, the studied samples were not cytotoxic to normal breast cancer cells (MCF-10A) and renal epithelial cells (293T) (Fig. 10C and D).

Overall, the results demonstrated that the biosafety of the co-amorphous systems was the same as that of PAL without affecting the efficacy of the drug and without eliciting toxic side effects.

4. Conclusion

In this study, four PAL-acid co-amorphous systems were successfully prepared by co-milling and characterized through XRD, SEM, DSC, HSM, FTIR, and SS-NMR. Our results revealed that ionic bond interaction existed between PAL and four organic acids. Crystalline PAL had a low dissolution and the supersaturation solubility after 24 h was only $35.27\ \mu\text{g mL}^{-1}$, while the co-amorphous PAL-SUC reached the highest level of

supersaturation ($1034.06\ \mu\text{g mL}^{-1}$) after 5 minutes. The solubility and dissolution rate of the co-amorphous PAL-acid systems were higher than that of the crystalline and amorphous PAL forms, and it might be in favour of its oral bioavailability. The stability of four co-amorphous systems was greatly improved under various temperature and humidity conditions compared with the extremely unstable amorphous PAL. The biosafety of the co-amorphous forms was similar to that of PAL. Cytotoxicity experiments explored the effect of adding small molecules on cell inhibition rate. PAL-acid co-amorphous drug systems did not elicit toxic side effects on 293T and MCF-10A and did not affect the efficacy of the PAL on MDA-MB-453 and MCF-7. Four organic acids could be used as the promising excipients to optimize drug properties, and the biosafety of the co-amorphous systems was the same as that of PAL. These comprehensive investigations for the PAL-acid co-amorphous drug systems developed a safe and effective formulation technology, providing a promising approach to improve the dissolution rate of crystalline drugs and the stability of amorphous drugs.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

This work was supported by the Applied Basic Research Project of Sichuan Province (Grant No. 2014JY0042). We are grateful to the Analytical Testing center of Sichuan University for providing solid nuclear magnetic and scanning electron microscopy.

Notes and references

- 1 K. Xu, S. Zheng, L. Guo, S. Li, L. Wang, P. Tang, J. Yan, D. Wu and H. Li, *RSC Adv.*, 2015, **5**, 96392–96403.
- 2 H. Ueda, W. Wu, K. Lobmann, H. Grohgan, A. Mullertz and T. Rades, *Mol. Pharmaceutics*, 2018, **15**, 2036–2044.
- 3 A. Newman, S. M. Reutzel-Edens and G. Zografi, *J. Pharm. Sci.*, 2018, **107**, 5–17.
- 4 K. Xu, S. Zheng, L. Guo, S. Li, L. Wang, P. Tang, J. Yan, D. Wu and H. Li, *RSC Adv.*, 2015, **5**, 96392–96403.
- 5 P. Tang, Q. Sun, L. Zhao, H. Pu, H. Yang, S. Zhang, R. Gan, N. Gan and H. Li, *Carbohydr. Polym.*, 2018, **198**, 418–425.
- 6 S. Mohapatra, S. Samanta, K. Kothari, P. Mistry and R. Suryanarayanan, *Cryst. Growth Des.*, 2017, **17**, 3142–3150.
- 7 K. Lobmann, H. Grohgan, R. Laitinen, C. Strachan and T. Rades, *Eur. J. Pharm. Biopharm.*, 2013, **85**, 873–881.
- 8 K. Lobmann, R. Laitinen, H. Grohgan, K. C. Gordon, C. Strachan and T. Rades, *Mol. Pharmaceutics*, 2011, **8**, 1919–1928.
- 9 R. Ojarinta, A. T. Heikkinen, E. Sievanen and R. Laitinen, *Eur. J. Pharm. Biopharm.*, 2017, **112**, 85–95.
- 10 R. B. Chavan, R. Thipparaboina, D. Kumar and N. R. Shastri, *Int. J. Pharm.*, 2016, **515**, 403–415.
- 11 H. Ueda, N. Muranushi, S. Sakuma, Y. Ida, T. Endoh, K. Kadota and Y. Tozuka, *Pharm. Res.*, 2016, **33**, 1018–1029.



- 12 I. Petry, K. Lobmann, H. Grohgan, T. Rades and C. S. Leopold, *Eur. J. Pharm. Biopharm.*, 2018, **133**, 151–160.
- 13 Y. Pan, W. Pang, J. Lv, J. Wang, C. Yang and W. Guo, *J. Pharm. Biomed. Anal.*, 2017, **138**, 302–315.
- 14 J. M. Skienah, I. Sathisaran, S. V. Dalvi and S. Rohani, *Cryst. Growth Des.*, 2017, **17**, 6273–6280.
- 15 L. Arnfast, M. Kamruzzaman, K. Lobmann, J. Aho, S. Baldursdottir, T. Rades and J. Rantanen, *Pharm. Res.*, 2017, **34**, 2689–2697.
- 16 R. Laitinen, K. Lobmann, H. Grohgan, C. Strachan and T. Rades, *Mol. Pharmaceutics*, 2014, **11**, 2381–2389.
- 17 J. Wang, R. Chang, Y. Zhao, J. Zhang, T. Zhang, Q. Fu, C. Chang and A. Zeng, *AAPS PharmSciTech*, 2017, **18**, 2541–2550.
- 18 S. Qian, W. Heng, Y. Wei, J. Zhang and Y. Gao, *Cryst. Growth Des.*, 2015, **15**, 2920–2928.
- 19 M. Fung, K. R. Be Rzis and R. Suryanarayanan, *Mol. Pharmaceutics*, 2018, **15**, 1862–1869.
- 20 S. J. Dengale, H. Grohgan, T. Rades and K. Lobmann, *Adv. Drug Delivery Rev.*, 2016, **100**, 116–125.
- 21 V. Sai Krishna Anand, S. D. Sakhare, K. S. Navya Sree, A. R. Nair, K. Raghava Varma, K. Gourishetti and S. J. Dengale, *Eur. J. Pharm. Sci.*, 2018, **123**, 124–134.
- 22 Y. Bi, D. Xiao, S. Ren, S. Bi, J. Wang and F. Li, *J. Pharm. Sci.*, 2017, **106**, 3150–3155.
- 23 Y. Gao, J. Liao, X. Qi and J. Zhang, *Int. J. Pharm.*, 2013, **450**, 290–295.
- 24 G. Kasten, H. Grohgan, T. Rades and K. Lobmann, *Eur. J. Pharm. Sci.*, 2016, **95**, 28–35.
- 25 R. Roskoski Jr, *Pharmacol. Res.*, 2016, **107**, 249–275.
- 26 Y. Katsumi, T. Iehara, M. Miyachi, S. Yagyu, S. Tsubai-Shimizu, K. Kikuchi, S. Tamura, Y. Kuwahara, K. Tsuchiya, H. Kuroda, T. Sugimoto, P. J. Houghton and H. Hosoi, *Biochem. Biophys. Res. Commun.*, 2011, **413**, 62–68.
- 27 A. Ruiz-Garcia, A. Plotka, M. O'Gorman and D. D. Wang, *Cancer Chemother. Pharmacol.*, 2017, **79**, 527–533.
- 28 W. Sun, K. J. Klamerus, L. M. Yuhas, S. Pawlak, A. Plotka, M. O'Gorman, L. Kirkovsky, M. Kosa and D. Wang, *Cancer Chemother. Pharmacol.*, 2017, **6**, 614–626.
- 29 J. Mishra, K. Lobmann, H. Grohgan and T. Rades, *Int. J. Pharm.*, 2018, **552**, 407–413.
- 30 M. K. Riekes, A. Engelen, B. Appeltans, P. Rombaut, H. K. Stulzer and G. Van den Mooter, *Pharm. Res.*, 2016, **33**, 1259–1275.
- 31 J. A. Baird and L. S. Taylor, *Adv. Drug Delivery Rev.*, 2012, **64**, 396–421.
- 32 B. Swapna and A. Nangia, *Cryst. Growth Des.*, 2017, **17**, 3350–3360.
- 33 L. Orola, I. Sarcevic, A. Kons, A. Actins and M. V. Veidis, *J. Mol. Struct.*, 2014, **1056–1057**, 63–69.
- 34 M. H. Fung, M. DeVault, K. T. Kuwata and R. Suryanarayanan, *Mol. Pharmaceutics*, 2018, **15**, 1052–1061.
- 35 D. Elliott, R. Dawson, W. Elliott and K. Jones, *Data for biochemical research*, Clarendon Press, Oxford, 1959, p. 221.
- 36 S. M. Moinuddin, S. Ruan, Y. Huang, Q. Gao, Q. Shi, B. Cai and T. Cai, *Int. J. Pharm.*, 2017, **532**, 393–400.
- 37 Z. Zhou, H. M. Chan, H. H. Sung, H. H. Tong and Y. Zheng, *Pharm. Res.*, 2016, **33**, 1030–1039.
- 38 B. Zhu, J.-R. Wang and X. Mei, *Cryst. Growth Des.*, 2015, **15**, 4959–4968.
- 39 J. Sibik, K. Lobmann, T. Rades and J. A. Zeitler, *Mol. Pharmaceutics*, 2015, **12**, 3062–3068.

