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# Poly(triazolyl methacrylate) glycopolymers as potential targeted unimolecular nanocarriers†

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Synthetic glycopolymers are increasingly investigated as multivalent ligands for a range of biological and biomedical applications. This study indicates that glycopolymers with a fine-tuned balance between hydrophilic sugar pendant units and relatively hydrophobic polymer backbones can act as single-chain targeted nanocarriers for low molecular weight hydrophobic molecules. Non-covalent complexes formed from poly(triazolyl methacrylate) glycopolymers and low molecular weight hydrophobic guest molecules were characterised through a range of analytical techniques – DLS, SLS, TDA, fluorescence spectroscopy, surface tension analysis – and molecular dynamics (MD) modelling simulations provided further information on the macromolecular characteristics of these single chain complexes. Finally, we show that these nanocarriers can be utilised to deliver a hydrophobic guest molecule, Nile red, to both soluble and surface-immobilised concanavalin A (Con A) and peanut agglutinin (PNA) model lectins with high specificity, showing the potential of non-covalent complexation with specific glycopolymers in targeted guest-molecule delivery.

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## Introduction

The development of synthetic single-chain macromolecular devices has been the subject of considerable research effort in recent years. One notable example of this is single-chain polymeric nanoparticles (SCPNs), where polymer chains are designed to fold at predefined points of their repeating unit sequence,<sup>1</sup> mimicking in concept the formation of folded structures in natural proteins. SCPNs can be synthesised following the formation of covalent or non-covalent intramolecular interactions.<sup>2–5</sup> Concerted effort between macromolecular chemists and biophysicists has provided access to increasingly sophisticated single-chain molecular devices with potential applications in catalysis, sensors, nanoreactors, and

nanomedicine.<sup>4–6</sup> For example, Lemcoff,<sup>7–9</sup> Pomposo<sup>10</sup> and Zimmerman's<sup>11</sup> groups engineered single-chain metal-organic nanocatalysts sharing key structural and functional similarity with metalloenzymes.

In biomedical settings, the size of delivery carriers affects their ability to cross biological barriers, and distribute in biological tissues.<sup>12</sup> Whilst sub-100 nm nano-structures are able to permeate hypervascular solid tumours, only those in the sub-50 nm size range can extravasate and penetrate poorly permeable hypovascular cancer tissues.<sup>13,14</sup> Thus, the possibility of scaling the size of specific nanocarriers down to that of individual polymer chains could potentially result in tangible clinical benefits. Outside of the biomedical applications, ultra-small polymer nanoparticles enabled the tuning of the macroscopic properties of polymer nanocomposites (PNCs) over a range inaccessible to conventional PNCs,<sup>15</sup> and access to conjugated polymer nanoparticles (Pdots) with unique fluorescence brightness and intraparticle energy migration efficiencies.<sup>16</sup>

Unimolecular micelles are molecular devices where polymer chains are designed to possess a core-shell morphology mimicking that of the self-assembled micelles.<sup>17,18</sup> Based on the individual polymer chains, unimolecular micelles possess the advantage of not unfolding or disassembling at low concentrations, such as those encountered in clinical settings *in vivo*. This is a key advantage for their potential applications in drug delivery and (bio)imaging, relative to conventional micelles.<sup>12,19–24</sup> Unimolecular micelles frequently include, in a single molecule, a hydrophobic core with a hyperbranched or

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dendrimeric structure which can non-covalently complex hydrophobic drugs, and a hydrophilic periphery, thus, resembling micelles formed by conventional surfactants.<sup>19,21,25,26</sup>

Alternative unimolecular structures have also been described, such as the ‘polysoaps’ assembled by McCormick and co-workers by statistical RAFT copolymerization of 2-acrylamido-2-methylpropane sulfonic acid (AMPS) and *n*-dodecyl acrylamide (DDAM) at specific molar ratios.<sup>27</sup> Recently, Stenzel and Barner-Kowollik’s groups described the synthesis of cross-linked sub-10 nm-sized single chain nanoparticles based on glucose-containing glycopolymers,<sup>28</sup> while Stenzel, Paulusse and co-workers utilised analogous nanomaterials to target GLUT1 and GLUT3 glucose transporters in HeLa cells.<sup>29</sup>

Inspired by these examples, here we explored a minimalistic approach to single-chain vectors, where guest molecules are reversibly incorporated within the individual linear and 4-arm polymer chains – as opposed to self-assembled micelles and/or hyperbranched-like structures – and pendant functionalities are used to provide recognition to specific biological targets.

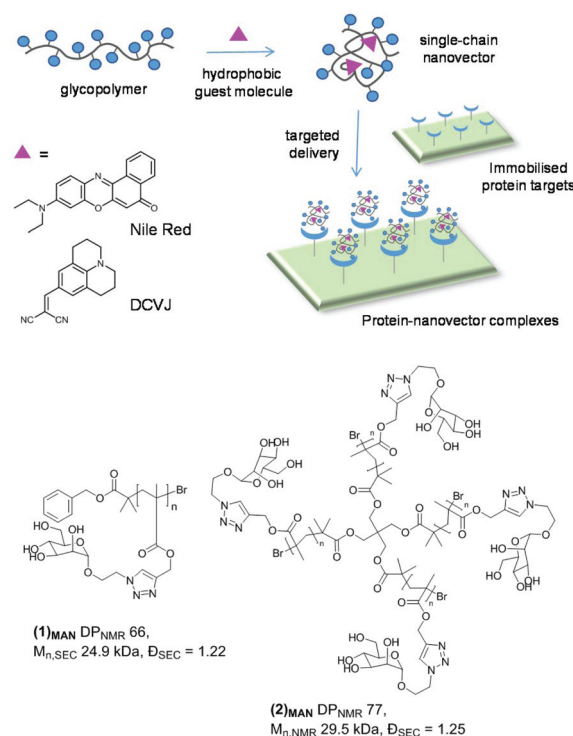
Synthetic glycopolymers are a class of macromolecules which are ideally suited for this aim, as (i) by varying the nature of pendant sugars and polymer backbone, their physico-chemical properties can be precisely controlled, (ii) they can be designed to possess functional groups which enable selective interaction with low molecular weight payloads, (iii) as biologically-inspired macromolecules they can target a variety of biologically relevant carbohydrate-binding proteins – lectins.<sup>30–32</sup>

Accordingly, in this work we investigate the ability of a range of glycopolymers to reversibly interact with model hydrophobic guest molecules, and evaluate the physico-chemical characteristics of the resulting nanocomplexes. Furthermore, we provide a prediction of the atomistic structure of these single-chain nanocomplexes through molecular dynamics simulations, and an initial evaluation of their targeting properties, particularly their interactions with carbohydrate-binding proteins.

## Results and discussion

### Poly(triazolyl methacrylate) glycopolymers: interaction with hydrophobic fluorescent probes

The glycopolymers investigated in this work were prepared by copper-catalysed alkyne–azide cycloaddition (CuAAC) functionalisation of preformed poly(propargyl methacrylate)s with appropriate sugar azides, as first reported by Haddleton and us.<sup>33,34</sup> Through this approach, libraries of glycopolymers were prepared *via* post-polymerization modification of the same parent polymer, leading to families of glycopolymers which only differ in the nature of the pendant carbohydrate units, and share all the other macromolecular characteristics – *i.e.* degree of polymerisation (DP), macromolecular topology (*e.g.* linear *vs.* branched), and molecular weight dispersity ( $\bar{D}$ ). Importantly for this study, this strategy leads to glycopolymers with a relatively hydrophobic polymethacrylate backbone and



**Chart 1** Top: Graphical illustration of glycopolymer single chain-guest molecule interaction, and targeted delivery to protein targets on functional surfaces. Hydrophobic fluorescent probes utilised in this study are Nile red and DCVJ. Bottom: Mannosylated linear (1)<sub>MAN</sub> and 4-arm star (2)<sub>MAN</sub> glycopolymers investigated in this study.

triazolyl linkers, which could potentially allow reversible binding with small hydrophobic guest molecules.

This work focusses primarily on mannosylated linear and 4-arm star glycopolymers (1)<sub>MAN</sub> and (2)<sub>MAN</sub>, respectively (Chart 1), although analogous materials bearing different pendant carbohydrate units – galactose, lactose and trehalose – were also investigated to identify the general structure–activity relationships of these materials (*vide infra*). Linear (1)<sub>MAN</sub> and star (2)<sub>MAN</sub> glycopolymers were made with similar degrees of polymerisation – DP 66 and 77, respectively – to identify the effect of the macromolecular topology on their physico-chemical properties, and on their ability to interact with guest molecules.

In a previous study,<sup>35</sup> we observed that polarity-responsive extrinsic fluorescent dyes, Nile red and SYPRO-orange, produced highly fluorescent solutions in aqueous media containing triazolyl methacrylate glycopolymers. Both fluorophores possess low quantum yields in aqueous media, resulting in a low fluorescence intensity, which increases in less polar environments.<sup>36,37</sup> Triazolyl methacrylate glycopolymers have been extensively investigated.<sup>33,34,38–47</sup> Yet, to the best of our knowledge, this behaviour, suggestive of their surfactant-like properties and of their ability to non-covalently bind hydrophobic probes under aqueous conditions, has not been described. Thus, the present study investigates the mechanism and modalities of host–guest interactions between glycopoly-



mers and low molecular weight guest-molecules. We further explore the potential of these materials as nanocarriers for receptor specific, targeted delivery.

Here, Nile red was chosen as the hydrophobic guest molecule because, although a possible structure has been suggested,<sup>37</sup> the exact molecular identity of SYPRO-orange has not yet been disclosed. In initial experiments, a solution of Nile red in THF was added to deionised water to achieve a theoretical final concentration of  $20\ \mu\text{g mL}^{-1}$ . In the absence of glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub>, after evaporation of the co-solvent, THF, Nile red was found to form a red-pink precipitate in an otherwise colourless or very lightly pink aqueous phase (Fig. 1A). This is consistent with the very low solubility reported for Nile red in water ( $<1\ \mu\text{g mL}^{-1}$ ).<sup>48</sup> In contrast, in the presence of triazolyl glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> ( $0, 50, 100, 1000\ \mu\text{g mL}^{-1}$ ) a visible pink coloration, with

intensity increasing as the concentration of glycopolymers increased, was observed.

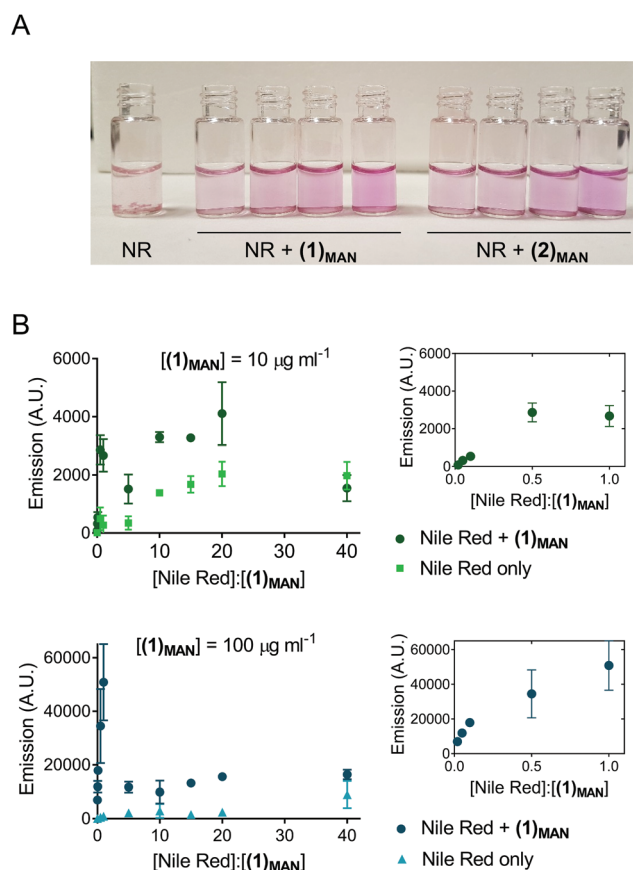
Following these initial observations, increasing concentrations of Nile red ( $50\text{--}1000\ \mu\text{g mL}^{-1}$ ) were added to solutions of (**1**)<sub>MAN</sub> in deionised water ( $10$  and  $100\ \mu\text{g mL}^{-1}$ ). The measured fluorescence was found to reach its maximum at approximately  $0.5\text{--}1$  molecules of Nile red per polymer chain (Fig. 1B). Interestingly, in the samples with a higher concentration of glycopolymer (**1**)<sub>MAN</sub> ( $100\ \mu\text{g mL}^{-1}$ ) a lower fluorescence was observed at high [Nile red]:[(**1**)<sub>MAN</sub>] ratios. This could be explained with the fact that in aqueous media Nile red can form non-emissive H-type dimers and larger aggregates through  $\pi\text{--}\pi$  stacking interactions,<sup>49,50</sup> and this phenomenon would become predominant at high concentrations of the dye. This effect was more evident in the set of samples with a higher concentration of glycopolymer (**1**)<sub>MAN</sub> ( $100\ \mu\text{g mL}^{-1}$ ), which requires larger amounts of Nile red to achieve the same [Nile red]:[(**1**)<sub>MAN</sub>] ratios. Analogous fluorescence vs. concentration profiles were observed when a more biologically relevant medium, PBS, was employed as the dispersing medium (Fig. S2†).

#### Sugar poly(triazolyl methacrylates): unimolecular micelles vs. higher order assemblies

Our initial experiments suggested that the poly(triazolyl methacrylate) glycopolymer could, rather unexpectedly, solubilise in water the otherwise poorly soluble hydrophobic probe Nile red. To gain mechanistic insight into this phenomenon, the propensity of polymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> to self-assemble under aqueous conditions was initially assessed by surface tension analysis.

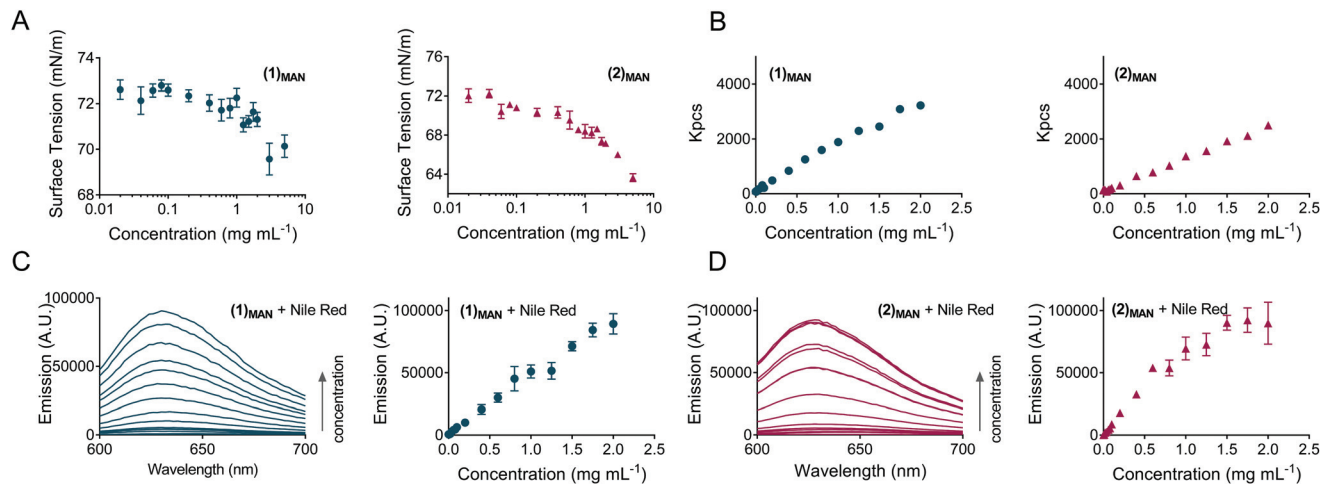
The surface tension ( $\gamma$ ) of aqueous solutions is reduced in the presence of chemical species which adsorb at the air/water interface, *i.e.* surfactants.<sup>51</sup> Typical  $\gamma$  vs. [surfactant] plots are sigmoidal curves with three distinct zones. At low concentrations, the air/water interface is scarcely populated by surfactant molecules, which in turn induces only relatively small changes of surface tension.<sup>51,52</sup> As the concentration of the surfactant increases, cooperativity among the adsorbed surfactant molecules at the interface induces a sharp decrease of  $\gamma$ , until saturation (or quasi-saturation) of the interface is reached.<sup>51,52</sup> After this point – the onset of aggregation (critical micellar concentration, CMC, if micelles are formed) – subsequent addition of the surfactant results in the formation of supramolecular assemblies, and will not induce any further significant decrease of surface tension. Thus, surface tension analysis is routinely used to determine the CMC of surfactants.<sup>27,52–54</sup>

In this study, for glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> no CMC could be observed, as the surface tension of their aqueous solutions steadily decreased as the polymer concentration increased throughout the range of concentrations tested ( $0.020\text{--}5.0\ \text{mg mL}^{-1}$ ), without reaching a plateau (Fig. 2A). This suggested that, under these experimental conditions, glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> exist in aqueous solution as individual polymeric chains.



**Fig. 1** Interaction of triazolyl methacrylate glycopolymers with hydrophobic fluorescent probes: (A) Left: Nile red (NR),  $20\ \mu\text{g mL}^{-1}$  in DI H<sub>2</sub>O. Centre and right:  $20\ \mu\text{g mL}^{-1}$  NR + linear (**1**)<sub>MAN</sub> (centre) and 4-arm star (**2**)<sub>MAN</sub> (right) at increasing concentration of glycopolymers ( $0, 50, 100, 1000\ \mu\text{g mL}^{-1}$ ). (B) Fluorescence readings ( $\lambda_{\text{ex}} 550\ \text{nm}$ ,  $\lambda_{\text{em}} 630\ \text{nm}$ ) of Nile red – (**1**)<sub>MAN</sub> samples at variable [Nile red]:[polymer chains] molar ratios, in DI H<sub>2</sub>O. Concentration of (**1**)<sub>MAN</sub> is kept constant at either  $10$  or  $100\ \mu\text{g mL}^{-1}$ , while [Nile red] is gradually increased. [Nile red]:[(**1**)<sub>MAN</sub>] refers to the molar ratio between Nile red and polymer (**1**)<sub>MAN</sub> used in each sample. 'Nile red only' refers to control samples identical to ones described above, except that no glycopolymer (**1**)<sub>MAN</sub> was added. Insets: Magnification of the  $0\text{--}1.0$  [Nile red]:[(**1**)<sub>MAN</sub>] region.





**Fig. 2** A: Surface tension of solutions of linear (1)<sub>MAN</sub> and 4-arm star (2)<sub>MAN</sub> glycopolymers in DI H<sub>2</sub>O at increasing concentrations ( $n = 2$ , triplicate). B: Scattered light intensity as a function of glycopolymer concentration, for (1)<sub>MAN</sub> and (2)<sub>MAN</sub>. C: Left: Emission spectra of samples containing Nile red (equivalent to a theoretical final dye concentration of 2.0  $\mu\text{M}$ , 0.64  $\mu\text{g mL}^{-1}$ ) and solutions of (1)<sub>MAN</sub> at increasing polymer concentrations, 0.0050–2.0  $\text{mg mL}^{-1}$  – corresponding to a [polymer]:[dye] = 0.10–40 for (1)<sub>MAN</sub>. Right: Emission ( $\lambda_{\text{em}} = 630 \text{ nm}$ ) vs. concentration profiles for these samples. D: Left: Emission spectra of samples containing Nile red (equivalent to a theoretical final dye concentration of 2.0  $\mu\text{M}$ ) and solutions of (2)<sub>MAN</sub> at increasing polymer concentrations, 0.0050–2.0  $\text{mg mL}^{-1}$  – corresponding to 0.084–34 for (2)<sub>MAN</sub>. Right: Emission ( $\lambda_{\text{em}} = 630 \text{ nm}$ ) vs. concentration profiles for these samples.

An analogous behaviour – that is,  $\gamma$  vs. concentration plots lacking the final plateau, has been previously described for polymers with topologies which structurally resembled the micellar structure. For example, Uhrich and co-workers utilised surface tension measurements to prove that the encapsulation of hydrophobic lidocaine molecules into mucic acid-fatty acids-PEG branched polymers was caused by individual unimolecular micelles.<sup>54</sup> McCormick's group showed that random copolymers with selected molar ratios of 2-acrylamido-2-methylpropane sulfonic acid (AMPS) and *n*-dodecyl acrylamide (DDAM) possessed unimolecular micellar features, and, similar to what was observed in our work, induced a continuous decrease of surface tension in the range of concentrations investigated (up to 10  $\text{mg mL}^{-1}$ ).<sup>27</sup>

In terms of structure–function relationships, 4-arm star (2)<sub>MAN</sub> induced a larger decrease in surface tension compared to its linear counterpart (1)<sub>MAN</sub>, 66.5 vs. 70.2  $\text{mN m}^{-1}$  at the highest concentration tested (5.0  $\text{mg mL}^{-1}$ ), respectively (Fig. 2A).

The observed effect of poly(triazolyl methacrylate)s (1)<sub>MAN</sub> and (2)<sub>MAN</sub> on surface tension suggested a partial orientation of their hydrophobic polymer backbone towards air, at the water–gas interphase.

To ascertain whether the balance between the hydrophilic sugar pendant units and the more hydrophobic polymer backbone affected the surface tension of the aqueous solution of these materials, these experiments were repeated using analogous linear and 4-arm star glycopolymers bearing larger sugar units, namely D-lactose and  $\alpha,\alpha$ -trehalose disaccharides, (1)<sub>LAC</sub> and (2)<sub>LAC</sub>, and (1)<sub>TRE</sub> and (2)<sub>TRE</sub>, respectively (Chart S1†). As these were prepared *via* post-polymerization modification of the same parent polymer precursor,<sup>35</sup> they possessed the same macromolecular features – average number of repeating units

(DP), dispersity ( $D$ ), and topology (linear and star) – as (1)<sub>MAN</sub> and (2)<sub>MAN</sub>, and thus allowed the dissection of the contribution of the nature of the carbohydrate pendant units on the ability of the corresponding glycopolymers to lower the surface tension of water.

The results (Fig. S4†) indicated that: (i) again, no CMC could be observed; (ii) glycopolymers with larger, more hydrophilic<sup>55</sup> sugar pendant units induced a lower overall decrease in surface tension, compared to (1)<sub>MAN</sub> and (2)<sub>MAN</sub>, showing that the hydrophobic/hydrophilic balance between the polymer backbone and the carbohydrate pendant units does affect the surfactant-like properties of these materials; (iii) 4-arm star polymers still induced a larger decrease in  $\gamma$ , which is in line with what was already observed for (1)<sub>MAN</sub> and (2)<sub>MAN</sub>; (iv) when used at the same concentrations utilised for the corresponding glycopolymers, individual D-mannose, D-lactose and  $\alpha,\alpha$ -trehalose mono- and disaccharides did not affect  $\gamma$ , showing that the physico-chemical nature of each glycopolymer as a whole, rather than the intrinsic properties of the pendant carbohydrates, is responsible for their effect on the surface tension.

Taken together, these experiments suggested that, in the range of concentrations and conditions investigated, these glycopolymers exist in water solution as individual polymer chains.

The propensity of poly(triazolyl methacrylates) (1)<sub>MAN</sub> and (2)<sub>MAN</sub> to aggregate was further probed by following the profile of the intensity of scattering of solutions with increasing glycopolymer concentration (Fig. 2B). The data showed a linear increase of scattering ( $K_{\text{cps}}$ ) for (1)<sub>MAN</sub> and (2)<sub>MAN</sub> in the 0.0010–2.0  $\text{mg mL}^{-1}$  range of concentrations, as previously observed for unimolecular micelles, *e.g.* by McCormick and co-





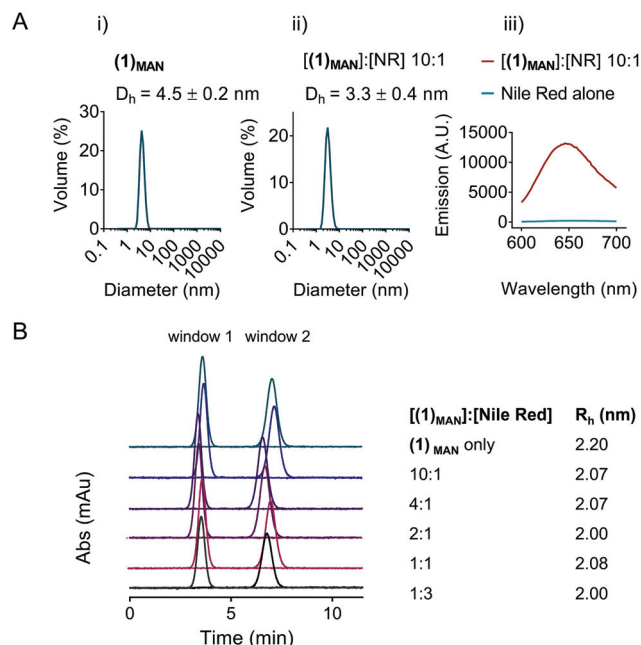
workers,<sup>27</sup> and in agreement with the results from the surface tension experiments.

Whilst surface tension and light scattering experiments suggested that glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> exist as individual chains in aqueous solution, in principle the presence of a hydrophobic probe may result in guest molecule-induced self-assembly, with the formation of larger aggregates containing multiple polymer chains and guest-molecules. For example, Mohr and co-workers showed that the hydrophobic probe Nile red promotes the formation of dye-loaded SDS, CTAB and Triton X micelles at sub-micellar surfactant concentrations.<sup>50</sup>

To address this point, here Nile red:glycopolymer interactions were investigated by fluorescence spectroscopy, under the hypothesis that if above a certain polymer concentration micelles or other large assemblies with a hydrophobic core were formed, a discontinuity in the emission intensity vs. polymer concentration plot would have been observed.<sup>56</sup> This would be suggestive of the formation of higher-order structures with a hydrophobic core able to enhance Nile red incorporation. Accordingly, a constant amount of Nile red, equivalent to a theoretical dye concentration of 2.0  $\mu\text{M}$ , was added to solutions of glycopolymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub> in deionised water at increasing polymer concentrations (Fig. 2C and D). Sample fluorescence increased almost linearly as the concentration of glycopolymers increased, with a tailing at higher concentrations for star polymer (**2**)<sub>MAN</sub> (Fig. 2D). The amount of the added dye was the same for all samples, thus the observed increase in fluorescence could be explained with the ability of increasing number of glycopolymer chains to complex a larger number of Nile red molecules. Additional contributing mechanisms may include the disruption of non-emissive dye H-dimers/aggregates which Nile red can form both in aqueous solution or within the hydrophobic domains of polymer carriers.<sup>50</sup>

Nile red is known to undergo a blue shift of the maximum of emission as the polarity of the surrounding (micro)environment decreases.<sup>48,57,58</sup> For example, Rimmer and co-workers utilised Nile red as a polarity-sensitive probe to show that specific highly-branched poly(*N*-isopropyl acrylamide)s possessed core-shell morphologies.<sup>59</sup> In our experiments we observed a shift from  $\sim 650$  nm, close to that of Nile red in water, at the lowest [polymer]:[dye] ratios (0.020 and 0.084 for linear (**1**)<sub>MAN</sub> and star (**2**)<sub>MAN</sub>, respectively), to 632–634 nm, starting from [polymer]:[dye]  $\sim 0.5$ –1 (Fig. S3†), indicative of Nile red existence in a more hydrophobic environment. This agrees with the studies of Alexiev and co-workers<sup>58</sup> and Mohr's group<sup>50</sup> where a blue shift of fluorescence emission was ascribed to the incorporation of the dye within the hydrophobic domains of their systems.

The potential self-assembly of (**1**)<sub>MAN</sub> was then further investigated by DLS (Fig. 3). The results showed a hydrodynamic diameter of 3–5 nm for linear (**1**)<sub>MAN</sub> at 2.0 mg mL<sup>-1</sup>, with and without added Nile red, at a 1 : 10 [Nile red] : [(**1**)<sub>MAN</sub>] molar ratio (Fig. 3A), consistent with the size expected for individual glycopolymer chains in this molecular weight range in



**Fig. 3** A. DLS size distributions of (i) linear mannose poly(triazolyl methacrylate) (**1**)<sub>MAN</sub> alone (top) and (ii) 10 : 1 mol : mol (**1**)<sub>MAN</sub>-Nile red (NR) complex at a [(**1**)<sub>MAN</sub>] = 10 mg mL<sup>-1</sup> in DI water. (iii) Fluorescence emission spectra of (**1**)<sub>MAN</sub>-Nile red complexes, and Nile red alone in water, at  $\lambda_{\text{ex}}$  = 550 nm. B. Taylor dispersion analysis (TDA) of (**1**)<sub>MAN</sub> alone and (**1**)<sub>MAN</sub>-Nile red complexes. Broadening of the concentration profile due to axial spreading of the solute pulse observed between two detection windows (windows 1 and 2 in the figure) is used to estimate the hydrodynamic radii. All samples in parts A and B were filtered through a 0.22  $\mu\text{m}$  membrane prior to analysis.

solution.<sup>60,61</sup> As the hydrodynamic diameters observed for (**1**)<sub>MAN</sub> with and without Nile red were close to the lower limit of detection for DLS, Taylor dispersion analysis (TDA) of (**1**)<sub>MAN</sub> was then carried out to obtain a more accurate estimation of its hydrodynamic size. TDA is an absolute method to determine the diffusion coefficients ( $D$ ), and thus the hydrodynamic radii ( $R_h$ ), of molecules in solution,<sup>62,63</sup> based on the dispersion of a solute plug through a uniform cylindrical tube under laminar Poiseuille flow.<sup>64</sup> Following injection, the UV absorbance ( $\lambda = 214$  nm) of the species in solution is recorded at two detection windows positioned along the capillary (windows 1 and 2, Fig. 3B). The diffusion coefficient of the injected solute(s) can be derived by fitting Taylor's solution to the concentration profile (taylorgram) of the solute(s).<sup>62</sup> In turn, this can be used to assess the size of molecules or particles with hydrodynamic diameter ( $2R_h$ ) from angstroms to submicron size,<sup>65,66</sup> typically in the 0.4–100 nm range. Hawe *et al.* showed that for peptide hormones and neuro-peptide oxytocin, with a hydrodynamic radius  $R_h = 0.9$ –1.1 nm, not too dissimilar from that expected for our polymers (**1**)<sub>MAN</sub> and (**2**)<sub>MAN</sub>, TDA was superior to DLS to estimate the peptide size.<sup>64</sup>

Importantly for our study, the deconvolution of taylorgrams from mixtures of species in solution allows the estimation of



the hydrodynamic radii of their individual components and their relative proportions,<sup>62,67</sup> and has been used to investigate the aggregation of macromolecules in solution.<sup>63,64</sup> For example, Latunde-Dada *et al.* estimated accurately size and relative proportion of the bovine serum albumin (BSA) monomer and thermally-induced aggregates in BSA:(BSA aggregates) in the 3–100% aggregation range.<sup>63</sup> Here, experiments were carried out at a concentration of linear (1)<sub>MAN</sub> of 2.0 mg mL<sup>-1</sup> and at variable [glycopolymer]:[Nile red] molar ratios (Fig. 3B). In all samples only one species in solution could be detected, with hydrodynamic radii ( $R_h$ ) in the 2.0–2.2 nm range, corresponding to diameters of 4.0–4.4 nm, which again was indicative of the presence of unimolecular polymer chains in solution.

### Effect of the nature of polymer backbone on guest molecule incorporation: loading and molecular dynamics (MD) simulations

The surface tension experiments showed that for glycopolymers with the same poly(triazolyl methacrylate) backbone, the nature and size of the pendant carbohydrate units have a direct effect on the surfactant properties of these materials. Here, we aimed at investigating the effect of the nature of the polymer backbone on the ability of these glycopolymers to incorporate hydrophobic fluorescent guest molecules.

To achieve this aim, linear poly(*N*-ethylacrylamido- $\alpha$ -D-mannopyranoside) (3)<sub>MAN</sub> (Fig. 4), analogous to (1)<sub>MAN</sub> but with a more hydrophilic polymer backbone, was synthesised by SET LRP (DP 67,  $\bar{D}$  1.22) and tested. In the first set of experiments, a fixed amount of Nile red was added to solutions at increasing concentration of polymers (1)<sub>MAN</sub> and (3)<sub>MAN</sub> (0.050–1.0 mg mL<sup>-1</sup>), and the fluorescence of the resulting mixtures was recorded (Fig. 4). The results clearly showed that whilst poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> was able to

interact with Nile red and incorporate it already at the lowest concentration tested (50  $\mu$ g mL<sup>-1</sup>), linear mannose acrylamide (3)<sub>MAN</sub> showed no detectable polymer–dye interaction. It should be noted that the increase of fluorescence is used here only for a qualitative assessment of relative amounts of Nile red, as a proportion of molecules of fluorophore incorporated within polymeric chains could still interact with each other and form non-fluorescent dimers and H-type aggregates through  $\pi$ – $\pi$  stacking interactions.<sup>50</sup>

9-(2,2-Dicyanovinyl)julolidine (DCVJ, Fig. 1A) was then tested as the hydrophobic probe. DCVJ belongs to a class of fluorophores known as molecular rotors, whose fluorescence depends on the velocity of rotation of a specific bond, presenting maximal fluorescence when the molecule is in a fully planar conformation. Upon irradiation, fluorescent molecular rotors undergo twisted intramolecular charge transfer (TICT), and relax *via* the nonradiative torsional relaxation pathway.<sup>68</sup> The fluorescence of molecular rotors is therefore more sensitive to changes in microenvironments which restrict rotation around key bonds – *e.g.* the increase of local viscosity or inclusion within the tightly packed microenvironment – than to the polarity of the medium the fluorophore is dissolved in.<sup>69</sup> Thus, DCVJ here served two purposes: (i) expanding the range of hydrophobic molecules which can be complexed by glycopolymers based on poly(triazolyl methacrylates), and (ii) gathering information on the molecular mobility of the entrapped guest molecule within dye:polymer complexes. As for the previous tests with Nile red, with DCVJ only poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> showed an increase in fluorescence (Fig. 4), suggesting a certain degree of steric rotational restriction of DCVJ guest molecules within the hydrophobic domain of the polymer.

To investigate the nature of triazolyl methacrylate glycopolymer–Nile red interactions at an atomistic level, Molecular Dynamics (MD) simulations<sup>70</sup> were employed. Our initial MD experiments focussed on the self-assembly of Nile red alone, in the absence of added glycopolymers. Accordingly, five Nile red molecules were randomly placed in an aqueous environment and were allowed to interact freely over a 100 ns time-scale. In agreement with their known aggregation mechanism,<sup>49,50</sup> the dye molecules rapidly aggregated through  $\pi$ – $\pi$  stacking (Fig. S10†). Next, we explored the average conformation in the water of poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> and poly(*N*-ethylacrylamido- $\alpha$ -D-mannopyranoside) (3)<sub>MAN</sub>, through 80 ns simulations. The polymers were built using tleap of AMBERtools, with the number of sugar repeating units matching exactly their DP calculated by <sup>1</sup>H NMR. Three replica simulations were performed for each polymer, and the evolution over time of the static properties of a single polymer chain, namely the end-to-end distance and the radius of gyration, was monitored. In all replicas, within 40 ns poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> adopted a globular conformation with a radius of gyration ( $R_g$ ) of 1.7 nm with the  $\alpha$ -D-mannopyranoside sugar moieties of the repeating units pointing towards the surrounding water-filled space. Combined with the hydrodynamic radius ( $R_h$ ) measured by TDA (Fig. 3),

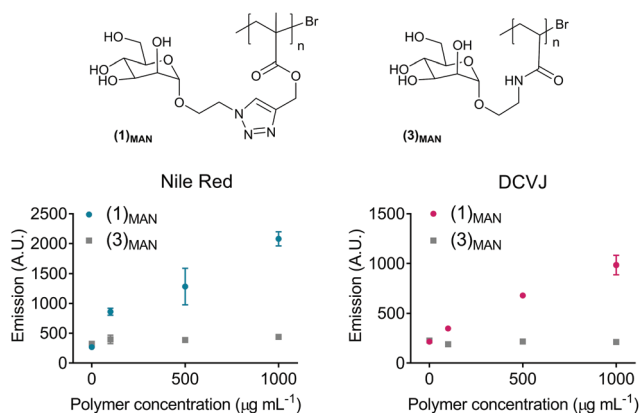


Fig. 4 Fluorescence of Nile red- and DCVJ (20  $\mu$ g mL<sup>-1</sup>, 63  $\mu$ M and 80  $\mu$ M, respectively) in the presence of increasing concentrations of mannose poly(triazolyl methacrylate) (1)<sub>MAN</sub> and poly(*N*-ethylacrylamido- $\alpha$ -D-mannopyranoside) (3)<sub>MAN</sub>. Nile red:  $\lambda_{ex}$  550 nm, max emission recorded in the  $\lambda_{em}$  = 520–700 nm region; DCVJ:  $\lambda_{ex}$  430 nm, max emission recorded in the  $\lambda_{em}$  = 400–600 nm region. For some points error bars are smaller than data symbols.



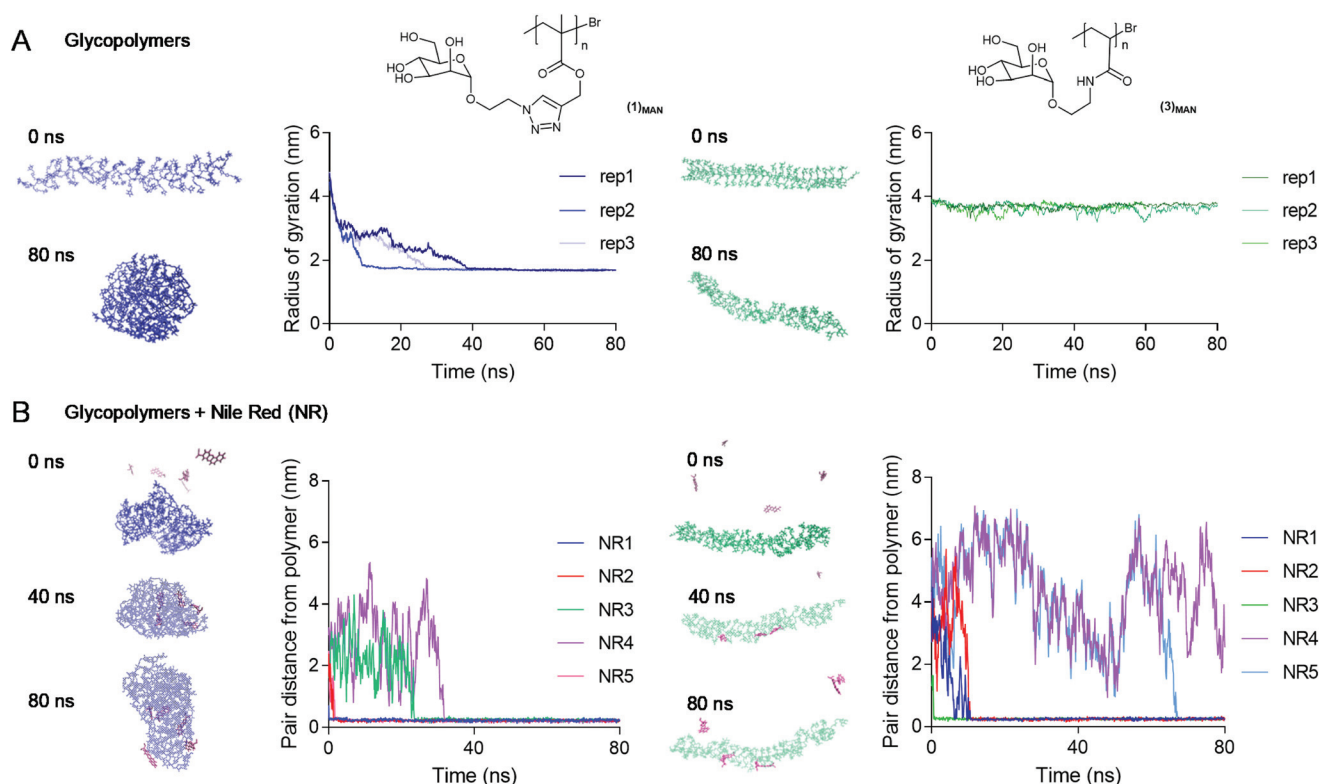
this gave a shape factor  $\rho = R_g/R_h$  of 0.77, which is characteristic of spherical conformations.<sup>71</sup> In contrast, most likely due to its more hydrophilic poly(*N*-ethylacrylamidoyl) backbone, within the timescale of the simulation experiments glycopolymer (3)<sub>MAN</sub> remained in a more solvated, chain-extended conformation, with radius of gyration of ~3.5–4.0 nm (Fig. 5B).

To assess the propensity of the glycopolymers to complex Nile Red (NR), five Nile red molecules were randomly placed around a single pre-equilibrated polymer chain, and the evolution of the pair-distances between the centre of mass of the glycopolymers and each Nile red molecule was monitored over an 80 ns period. Poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> was found to bind all five Nile red molecules within the first 60 ns, as shown by the distances between the centre of mass of the glycopolymers and Nile red molecules decreasing to values close to zero (Fig. 5B, left). In contrast, with glycopolymer (3)<sub>MAN</sub> at the end of some of the replica simulations, a few NR molecules were found to be still unbound (Fig. 5B, right and S12†). Rapid dye incorporation in poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> appeared to prevent Nile red self-aggregation, which was instead observed in the presence of glycopolymer (3)<sub>MAN</sub> (NR4 and NR5 in Fig. 5, showing identical distance from the polymer centre of mass for a proportion of the simulation experiment).

Interestingly, in these simulations all five Nile red molecules were rapidly incorporated within (1)<sub>MAN</sub> single-chain nanocarriers, while in our initial complexation studies a maximum of fluorescence at [Nile red]:[polymer] ratios in the 0.5–1 range was observed. While it may be difficult to rationalise this partial discrepancy at this stage, possible explanations may include an overestimation in the simulations of the ability of the glycopolymers to disrupt dye-dye aggregates and incorporate individual Nile red molecules, or the formation of non-emissive H-type  $\pi$ - $\pi$  stacked Nile red aggregates within each complex, favoured at higher Nile red concentrations.

In a final experiment, we found that two water-equilibrated (1)<sub>MAN</sub> polymer chains existed as individual coiled chains for the duration of the experiment (80 ns), showing that, under these simulation conditions, glycopolymer (1)<sub>MAN</sub> did not form larger aggregates (Fig. S14†).

Taken together, these simulations provided an atomistic insight on the Nile red-glycopolymer interactions, and supported the structure-function observations derived from our Nile red-glycopolymer complexation experiments and the literature, that is: (i) under aqueous conditions poly(mannose triazolyl methacrylate) (1)<sub>MAN</sub> appears to adopt a coiled conformation able to rapidly incorporate Nile red molecules, (ii) more hydrophilic poly(*N*-ethylacrylamidoyl- $\alpha$ -D-mannopyranoside) (3)<sub>MAN</sub> appeared to remain in a more extended conformation.



**Fig. 5** A: Metrics obtained from the 80 ns simulations with poly(mannose triazolyl methacrylates) (1)<sub>MAN</sub> and poly(*N*-ethylacrylamidoyl- $\alpha$ -D-mannopyranoside) (3)<sub>MAN</sub> alone, in the absence of Nile red: evolution of radius of gyration of the glycopolymers in water during the 0–80 ns simulations (3 replicas – rep1, rep2, and rep3 – per polymer). B: Five Nile red (NR1 to NR5) molecules were randomly placed in the space surrounding glycopolymers (1)<sub>MAN</sub> (left) and (3)<sub>MAN</sub> (right) ( $t = 0$  ns). The graphs show the evolution of the pair-distances between the centre of mass of the polymer chains and each Nile red molecule for one of the replica simulations.





side) (3)<sub>MAN</sub> is comparatively less prone to incorporate Nile red and exists in solution in a more chain extended conformation; (iii) in the absence of glycopolymers, Nile red rapidly associated into aggregates through  $\pi$ - $\pi$  stacking interactions; (iv) under the conditions investigated, (1)<sub>MAN</sub> was not prone to self-assemble into larger aggregates, in agreement with what was observed in our light scattering and TDA experiments.

### Delivery of guest molecules to lectin targets

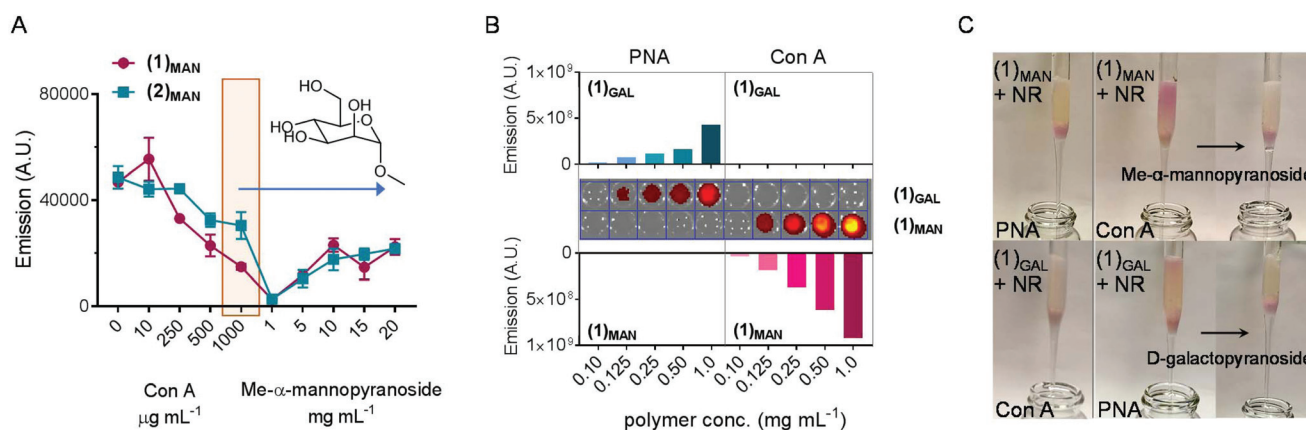
This part of our study assessed the potential of the synthesized glycopolymers to target carbohydrate-binding proteins (lectins). In nature carbohydrates are involved in the regulation of a plethora of biological processes such as cell differentiation, proliferation and adhesion, inflammation, and immunological response,<sup>72</sup> thus targeted drug delivery through sugar-binding receptors to modulate these key processes is particularly attractive.<sup>73</sup> Initially, an agglutination assay using mannose-binding concanavalin A model lectin<sup>74,75</sup> was developed, based on a protocol described by Haddleton and co-workers.<sup>76</sup>

In the first part of the assay, increasing amounts of Con A were added to solutions of glycopolymer–Nile red complexes (obtained from 1.00 mg mL<sup>-1</sup> of (1)<sub>MAN</sub> or (2)<sub>MAN</sub> and 20  $\mu$ g mL<sup>-1</sup> (63  $\mu$ M) of Nile red), resulting in the formation of insoluble Con A-complex clusters. The highest Con A concentration, 1.00  $\mu$ g mL<sup>-1</sup>, corresponds to one molecule of the Con A monomer per two polymer chains. The fluorescence of (1)<sub>MAN</sub>-Nile red samples was found to decrease steadily as the concentration of added Con A was increased from 0 to 1.00 mg mL<sup>-1</sup> (Fig. 6A). This can be explained in terms of (i)

Con A-induced aggregation and precipitation of fluorescent glycopolymer–Nile red complexes, (ii) sequestration of glycopolymers by the added Con A, followed by precipitation of Nile red due to the lack of polymer chains able to solubilise it, or (iii) a combination of these two effects.

In the second part of the assay, the reversibility of this process was evaluated. The release of glycopolymers from the clusters formed at 1.00 mg mL<sup>-1</sup> Con A concentration was tested by adding increasing concentrations of methyl- $\alpha$ -mannopyranoside (1–20 mg mL<sup>-1</sup>), which acts as a competitive monovalent ligand for Con A. An increase in fluorescence, proportional to the amount of the monovalent mannose ligand added, was observed, indicating that Nile red was retained within the mannose glycopolymers, or re-complexed, according to the mechanism (ii) above, following decomplexation from Con A lectin.

Next, the ability of these glycopolymers to mediate selective targeting to lectin-functionalised surfaces was investigated. To achieve this aim, commercially available 45–165  $\mu$ m agarose beads functionalised with mannose-binding Con A and galactose-binding peanut agglutinin (PNA) were utilised, along with a linear galactose glycopolymer (1)<sub>GAL</sub> analogous to mannosylated (1)<sub>MAN</sub>. Lectin-decorated beads were treated with (1)<sub>MAN</sub>- and (1)<sub>GAL</sub>-Nile red complexes (1 : 1 glycopolymer : dye ratio) in the 0.10–1.0 mg mL<sup>-1</sup> range of polymer concentrations. Upon centrifugation and removal of the supernatant, followed by several washing cycles, the beads were suspended in HEPES buffer and analysed by fluorescence microscopy (Fig. 6B). Selective recognition of (1)<sub>MAN</sub>- and (1)<sub>GAL</sub>-Nile red complexes to Con A and PNA, respectively, was observed. No



**Fig. 6** Binding of (1)<sub>MAN</sub>-Nile red non-covalent conjugates to mannose-specific model lectins. **A:** Con A agglutination assay. To a polymer solution (1.0 mg mL<sup>-1</sup> in 20 mM HEPES buffer (pH 7.4 with 50 mM NaCl, 5 mM CaCl<sub>2</sub> and 5 mM MnCl<sub>2</sub>), Nile red was added (1 : 1 mol : mol glycopolymer : dye), and the fluorescence at  $\lambda_{\text{ex}}$  = 630 nm ( $\lambda_{\text{em}}$  = 550 nm) was recorded. Upon addition of Con A, the decrease of fluorescence due to the formation of insoluble Con A-(1)<sub>MAN</sub>-Nile red was recorded. Reversible agglutination: the solid precipitate obtained from the 1000  $\mu$ g mL<sup>-1</sup> Con A experiment (highlighted) was treated with different concentrations of Me- $\alpha$ -mannopyranoside competitive ligand, and recovery of fluorescence due to re-dissolution (or re-formation) of (1)<sub>MAN</sub>-Nile red complexes was measured. **B:** Agarose-bound lectin beads were treated with different amounts of (1)<sub>MAN</sub>- and (1)<sub>GAL</sub>-Nile red complexes (1 : 1 polymer : dye molar ratio). After extensive rinsing with 20 mM HEPES buffer, the samples were seeded on a 96-well plate and the fluorescence was recorded. **C:** Affinity chromatography assay. Con A- and PNA-immobilised beads were utilised as stationary phases for affinity chromatography on (1)<sub>MAN</sub>- and (1)<sub>GAL</sub>-Nile red complexes (1 : 1 polymer : dye molar ratio), eluting with HEPES buffer. (1)<sub>MAN</sub>-Nile red was found to selectively bind to Con A, and (1)<sub>GAL</sub>-Nile red to PNA. These complexes could be eluted from the lectin stationary phase by the addition of a mobile phase containing an excess of monovalent competitive ligands, Me- $\alpha$ -mannopyranoside, and D-galactopyranoside, respectively.





binding to 'mismatched' lectins – that is,  $(1)_{\text{MAN}}$  to PNA and  $(1)_{\text{GAL}}$  to Con A – was detected, thus ruling out any significant binding to the lectin surfaces due to non-specific adsorption or other non-specific binding mechanisms.

Utilising Con A and PNA agarose beads as stationary phases for affinity chromatography (Fig. 6C, S7 and S8†) showed a retention by Con A of  $(1)_{\text{MAN}}$ -Nile red samples, while these were readily eluted from the PNA column. This demonstrated that poly(mannose triazolyl methacrylate)  $(1)_{\text{MAN}}$  was able to efficiently transport Nile red through the PNA stationary phase. Treatment with a  $10 \text{ mg mL}^{-1}$  aqueous solution of methyl- $\alpha$ -mannopyranoside monovalent competitive ligand resulted in the complete elution of  $(1)_{\text{MAN}}$ -Nile red samples from the Con A column, confirming that  $(1)_{\text{MAN}}$  here acted as a targeted nanocarrier for Nile red. On repeating this experiment using  $(1)_{\text{GAL}}$ , a linear glycopolymer identical to  $(1)_{\text{MAN}}$  except for the presence of galactose instead of mannose binding units yielded analogous results, with selective binding of  $(1)_{\text{GAL}}$ -Nile red complexes to PNA and not to Con A.

Guest probe (Nile red) release profiles were then assessed using Nile red- $(1)_{\text{MAN}}$  complexes in deionised water ( $[(1)_{\text{MAN}}]: 1.00 \text{ mg mL}^{-1}$ , [Nile red]:  $20 \text{ } \mu\text{g mL}^{-1}$  ( $63 \text{ } \mu\text{M}$ )) through a 5 kDa MWCO membrane under sink conditions. To evaluate the effect of polymer topology on Nile red release, 4-arm star  $(2)_{\text{MAN}}$  was also tested. Consistent with a reversible polymer-probe interaction, near complete Nile red release was observed already after 4 hours for both linear and star glycopolymers (Fig. S6†).

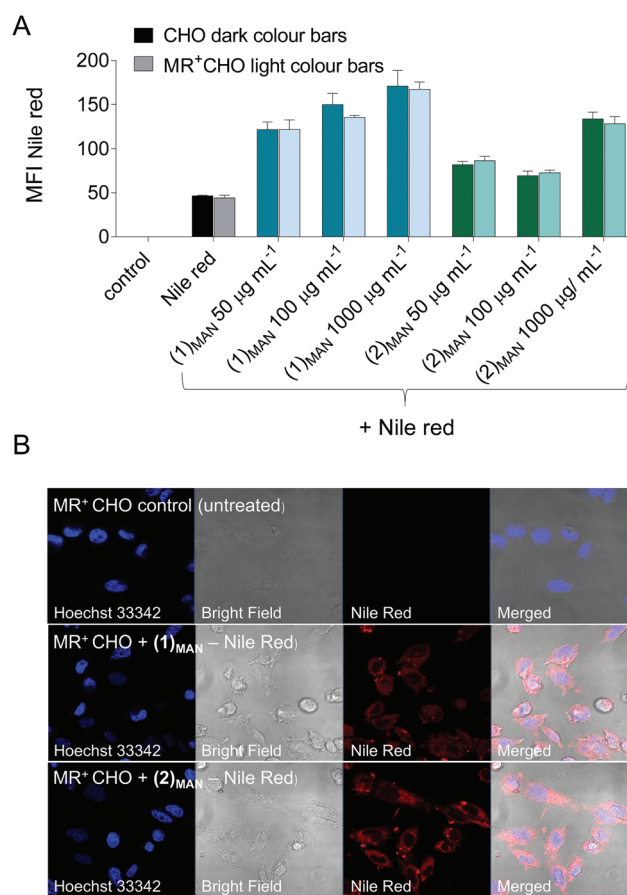
Attempts to quantify the amount of Nile red retained in the polymers following filtration through a  $0.22 \text{ } \mu\text{m}$  membrane resulted in a significant amount of Nile red being retained in the filter membrane (see the ESI†), possibly suggesting a relatively low stability of the dye:polymer complexes under shear stress and/or the presence of relatively large free Nile red aggregates in equilibrium with complexed dye. Importantly, no loss of glycopolymers following filtration could be detected by  $^1\text{NMR}$  analysis (Fig. S5†), again confirming that under the conditions utilised to form the glycopolymer-Nile red complexes, only a very small or no appreciable amount of glycopolymers were involved in the formation of large aggregates with Nile red. The stability of the complexes under specific stress conditions will be the focus of future studies. Taken together, this part of our work showed that upon complexation of Nile red, glycopolymers conserved their ability to bind model lectins Con A and PNA, whilst at the same time retained their Nile red payload.

Finally, whilst not within the scope of this present work, initial experiments aiming at using these single-chain nanocarriers for targeted delivery to cells presenting endocytic lectin receptors were carried out. Chinese Hamster Ovary (CHO) cells were selected due to the availability of a mutant cell line expressing Mannose Receptor (MR, CD206),<sup>77,78</sup> an endocytic receptor expressed in subpopulations of dendritic cells (DCs), macrophages, and selected endothelial cells, and which plays a role in both innate and adaptive immunity.<sup>79,80</sup> Here, MR<sup>+</sup>-CHO cells were incubated for 30 minutes with

glycopolymer:Nile red-containing solutions at constant Nile red theoretical concentration ( $10 \text{ } \mu\text{M}$  if all of it were solubilised) and increasing polymer concentrations ( $50\text{--}1000 \text{ } \mu\text{g mL}^{-1}$ ). Nile red cell uptake was monitored by flow cytometry (FACS), and was found to be significantly increased in the presence of  $(1)_{\text{MAN}}$  and  $(2)_{\text{MAN}}$ , relative to free dye control and to be dependent on the concentration of the added glycopolymers (Fig. 7).

Interestingly, the uptake was found to be not significantly different in mannose receptor positive and negative CHO cells (Fig. 7A). This was observed even for systems where dye uptake was only marginally higher than that of Nile red alone ( $(2)_{\text{MAN}}$ -Nile red at 50 and  $100 \text{ } \mu\text{g mL}^{-1}$ , Fig. 7A), suggesting that this effect may not be due to receptor saturation.

Several studies have described Nile red transfer from nanoparticle systems to hydrophobic acceptors, such as cell membranes,<sup>81,82</sup> lipid nanocapsules and triglyceride oil,<sup>83</sup> and



**Fig. 7** A: Flow cytometry quantification of the uptake of Nile red by CHO (MR<sup>−</sup>), and MR<sup>+</sup>CHO cells incubated with  $(1)_{\text{MAN}}$ - and  $(2)_{\text{MAN}}$ -Nile red complexes at a constant concentration of Nile red ( $10 \text{ } \mu\text{M}$  if all of it were solubilised), and increasing concentrations of glycopolymers. 'Nile red' columns are relative to cells incubated with Nile red at the same theoretical concentration, in the absence of glycopolymers. 'Control' refers to untreated cells. B: Confocal microscopy analysis of these samples: Top. MR<sup>+</sup>CHO untreated cells (negative control). Middle: MR<sup>+</sup>CHO cells incubated with  $1.00 \text{ mg mL}^{-1}$   $(1)_{\text{MAN}}$  +  $10 \text{ } \mu\text{M}$  Nile red, and Bottom: MR<sup>+</sup>CHO cells treated with  $1.00 \text{ mg mL}^{-1}$   $(2)_{\text{MAN}}$  +  $10 \text{ } \mu\text{M}$  Nile red, for 30 min.



emulsion droplets.<sup>84</sup> Thus, our results could be explained in terms of an equilibrium between Nile red reversibly complexed to the glycopolymers, and the unbound fraction being able to enter CHO cells by diffusion through the plasma membrane, or other mechanisms. Confocal analysis of the cells following treatment with Nile red and (1)<sub>MAN</sub> or (2)<sub>MAN</sub> showed diffuse intracellular cytosolic fluorescence, with a few punctuated spots (Fig. 6). This is in line with the analogous fluorophore distribution patterns described by Snipstad *et al.* who showed that on using Nile red-loaded poly(butylcyanoacrylate) nanoparticles, dye uptake by human prostate adenocarcinoma cells (PC3) did not occur by endocytosis, but rather by nanoparticle–cell contact-mediated transfer directly to the cytosol and, to a lesser extent, release of payload into the medium, followed by diffusion into the cells.<sup>82</sup>

Taken together our *in vitro* experiments showed that the targeted delivery of host molecules to soluble and surface-immobilised lectins can be successfully achieved, and preliminary cell experiments revealed that, whilst not directly suitable to probe MR-mediated targeted cell delivery at this stage, poly(triazolyl methacrylate)s (1)<sub>MAN</sub> and (2)<sub>MAN</sub> can act as carriers for Nile red and enhance its cellular uptake.

## Conclusions

Poly(triazolyl methacrylate) glycopolymers are a class of synthetic carbohydrate-based materials investigated for a range of applications as diverse as inhibition of human lectin interactions with HIV viral envelope, modulation of antibody aggregation and as ligands for specific cancer cells. The work presented here suggests that, intriguingly, in addition to their known modalities of action, under specific conditions they can also function as unimolecular targeted carriers for hydrophobic guest molecules.

In this study, these guest molecule–glycopolymer complexes were characterised through a range of techniques – DLS, TDA, fluorescence spectroscopy, surface tension analysis – and an initial structure–function relationship, *i.e.* how the nature of both the sugar repeating units and polymer backbone affects probe complexation was identified. Molecular dynamics (MD) simulations supported the experimental results and provided an insight into the mechanism of formation of these nano-complexes. While at this stage the structure of the glycopolymers was not optimised to enhance guest molecule incorporation and delivery, this work provides an *ab initio* investigation on the factors that control non-covalent complexation of small hydrophobic probes with poly(triazolyl methacrylate) glycopolymers.

Glycopolymers are often utilised as tools for selective targeting of carbohydrate-binding proteins (lectins). While a limited number of studies have looked at the effect of different spacers linking carbohydrate pendant units to the polymer backbone on lectin binding affinity and specificity,<sup>85–87</sup> from a synthetic design standpoint focus is typically placed on the nature, number, and orientation of the sugar repeating units. A

broader implication of our study is that it suggests that the physico-chemical nature of both spacers and macromolecular backbone can affect the conformation of glycopolymers in solution – thus potentially affecting their ability to span over multiple lectin receptors and the orientation of their sugar binding units – and their ability to reversibly interact with small molecules in solution. The latter phenomenon may need to be considered when glycopolymers are utilised within multi-component systems such as those encountered in complex biological systems, and could be exploited for the reversible binding and delivery of specific guest molecules within biomedical settings.

## Conflicts of interest

CvdW is an employee of AstraZeneca Ltd and PJSK is an employee of Malvern Panalytical Ltd.

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## Notes and references

- 1 J.-F. Lutz, M. Ouchi, D. R. Liu and M. Sawamoto, *Science*, 2013, **341**, 1238149.
- 2 M. Gonzalez-Burgos, A. Latorre-Sanchez and J. A. Pomposo, *Chem. Soc. Rev.*, 2015, **44**, 6122–6142.
- 3 A. M. Hanlon, C. K. Lyon and E. B. Berda, *Macromolecules*, 2016, **49**, 2–14.
- 4 O. Altintas and C. Barner-Kowollik, *Macromol. Rapid Commun.*, 2012, **33**, 958–971.
- 5 O. Altintas and C. Barner-Kowollik, *Macromol. Rapid Commun.*, 2016, **37**, 29–46.
- 6 C. K. Lyon, A. Prasher, A. M. Hanlon, B. T. Tuten, C. A. Tooley, P. G. Frank and E. B. Berda, *Polym. Chem.*, 2015, **6**, 181–197.
- 7 I. Berkovich, S. Mavila, O. Iliashevsky, S. Kozuch and N. G. Lemcoff, *Chem. Sci.*, 2016, **7**, 1773–1778.
- 8 S. Mavila, C. E. Diesendruck, S. Linde, L. Amir, R. Shikler and N. G. Lemcoff, *Angew. Chem., Int. Ed.*, 2013, **52**, 5767–5770.
- 9 S. Mavila, I. Rozenberg and N. G. Lemcoff, *Chem. Sci.*, 2014, **5**, 4196–4203.



- 10 A. Sanchez-Sanchez, A. Arbe, J. Colmenero and J. A. Pomposo, *ACS Macro Lett.*, 2014, **3**, 439–443.
- 11 Y. Bai, X. Feng, H. Xing, Y. Xu, B. K. Kim, N. Baig, T. Zhou, A. A. Gewirth, Y. Lu, E. Oldfield and S. C. Zimmerman, *J. Am. Chem. Soc.*, 2016, **138**, 11077–11080.
- 12 A. P. P. Kröger and J. M. J. Paulusse, *J. Controlled Release*, 2018, **286**, 326–347.
- 13 S. Quader and K. Kataoka, *Mol. Ther.*, 2017, **25**, 1501–1513.
- 14 H. Cabral, Y. Matsumoto, K. Mizuno, Q. Chen, M. Murakami, M. Kimura, Y. Terada, M. R. Kano, K. Miyazono, M. Uesaka, N. Nishiyama and K. Kataoka, *Nat. Nanotechnol.*, 2011, **6**, 815.
- 15 S. Cheng, S.-J. Xie, J.-M. Y. Carrillo, B. Carroll, H. Martin, P.-F. Cao, M. D. Dadmun, B. G. Sumpter, V. N. Novikov, K. S. Schweizer and A. P. Sokolov, *ACS Nano*, 2017, **11**, 752–759.
- 16 H. Piwoński, T. Michinobu and S. Habuchi, *Nat. Commun.*, 2017, **8**, 15256.
- 17 X. Fan, Z. Li and X. J. Loh, *Polym. Chem.*, 2016, **7**, 5898–5919.
- 18 G. Chen, Y. Wang, R. Xie and S. Gong, *Adv. Drug Delivery Rev.*, 2018, **130**, 58–72.
- 19 Y. Wang, G. Qi and J. He, *ACS Macro Lett.*, 2016, **5**, 547–551.
- 20 G. Liu, H. Gao, Y. Zuo, X. Zeng, W. Tao, H.-i. Tsai and L. Mei, *ACS Appl. Mater. Interfaces*, 2017, **9**, 112–119.
- 21 X. Fan, Z. Hu and G. Wang, *RSC Adv.*, 2015, **5**, 100816–100823.
- 22 G. Chen, L. Wang, T. Cordie, C. Vokoun, K. W. Eliceiri and S. Gong, *Biomaterials*, 2015, 41–50.
- 23 Y. Xiao, H. Hong, A. Javadi, J. W. Engle, W. Xu, Y. Yang, Y. Zhang, T. E. Barnhart, W. Cai and S. Gong, *Biomaterials*, 2012, **33**, 3071–3082.
- 24 C. S. Popeney, M. C. Lukowiak, C. Böttcher, B. Schade, P. Welker, D. Mangoldt, G. Gunkel, Z. Guan and R. Haag, *ACS Macro Lett.*, 2012, **1**, 564–567.
- 25 C. Porsch, Y. Zhang, C. Ducani, F. Vilaplana, L. Nordstierna, A. M. Nyström and E. Malmström, *Biomacromolecules*, 2014, **15**, 2235–2245.
- 26 J. Xu, S. Luo, W. Shi and S. Liu, *Langmuir*, 2006, **22**, 989–997.
- 27 W.-M. Wan, P. D. Pickett, D. A. Savin and C. L. McCormick, *Polym. Chem.*, 2014, **5**, 819–827.
- 28 K. N. R. Wuest, H. Lu, D. S. Thomas, A. S. Goldmann, M. H. Stenzel and C. Barner-Kowollik, *ACS Macro Lett.*, 2017, **6**, 1168–1174.
- 29 A. P. P. Kröger, M. I. Komil, N. M. Hamelmann, A. Juan, M. H. Stenzel and J. M. J. Paulusse, *ACS Macro Lett.*, 2019, **8**, 95–101.
- 30 L. L. Kiessling and J. C. Grim, *Chem. Soc. Rev.*, 2013, **42**, 4476–4491.
- 31 Y. Miura, Y. Hoshino and H. Seto, *Chem. Rev.*, 2016, **116**, 1673–1692.
- 32 C. R. Becer, *Macromol. Rapid Commun.*, 2012, **33**, 742–752.
- 33 V. Ladmiral, G. Mantovani, G. J. Clarkson, S. Cauet, J. L. Irwin and D. M. Haddleton, *J. Am. Chem. Soc.*, 2006, **128**, 4823–4830.
- 34 J. Geng, G. Mantovani, L. Tao, J. Nicolas, G. Chen, R. Wallis, D. A. Mitchell, B. R. G. Johnson, S. D. Evans and D. M. Haddleton, *J. Am. Chem. Soc.*, 2007, **129**, 15156–15163.
- 35 J. Madeira do O, F. Mastrotto, N. Francini, S. Allen, C. F. van der Waalse, S. Stolnik and G. Mantovani, *J. Mater. Chem. B*, 2018, **6**, 1044–1054.
- 36 J. Jose and K. Burgess, *J. Org. Chem.*, 2006, **71**, 7835–7839.
- 37 T. Kroeger, B. Frieg, T. Zhang, F. K. Hansen, A. Marmann, P. Proksch, L. Nagel-Steger, G. Groth, S. H. J. Smits and H. Gohlke, *PLoS One*, 2017, **12**, e0177024.
- 38 C. R. Becer, M. I. Gibson, J. Geng, R. Ilyas, R. Wallis, D. A. Mitchell and D. M. Haddleton, *J. Am. Chem. Soc.*, 2010, **132**, 15130–15132.
- 39 J. Chen, C. Travelet, R. Borsali and S. Halila, *Biomacromolecules*, 2017, **18**, 3410–3417.
- 40 Y. Gou, J. Geng, S.-J. Richards, J. Burns, C. Remzi Becer and D. M. Haddleton, *J. Polym. Sci., Part A: Polym. Chem.*, 2013, **51**, 2588–2597.
- 41 Y. Gou, S. Slavin, J. Geng, L. Voorhaar, D. M. Haddleton and C. R. Becer, *ACS Macro Lett.*, 2012, **1**, 180–183.
- 42 K. Jono, M. Nagao, T. Oh, S. Sonoda, Y. Hoshino and Y. Miura, *Chem. Commun.*, 2018, **54**, 82–85.
- 43 J. Tanaka, A. S. Gleinich, Q. Zhang, R. Whitfield, K. Kempe, D. M. Haddleton, T. P. Davis, S. Perrier, D. A. Mitchell and P. Wilson, *Biomacromolecules*, 2017, **18**, 1624–1633.
- 44 Y. Zhao, Y. Zhang, C. Wang, G. Chen and M. Jiang, *Biomacromolecules*, 2017, **18**, 568–575.
- 45 K. Babiuch, A. Dag, J. Zhao, H. Lu and M. H. Stenzel, *Biomacromolecules*, 2015, **16**, 1948–1957.
- 46 J. Geng, J. Lindqvist, G. Mantovani, G. Chen, C. T. Sayers, G. J. Clarkson and D. M. Haddleton, *QSAR Comb. Sci.*, 2007, **26**, 1220–1228.
- 47 L. Nurmi, J. Lindqvist, R. Randev, J. Syrett and D. M. Haddleton, *Chem. Commun.*, 2009, 2727–2729.
- 48 P. Greenspan and S. D. Fowler, *J. Lipid Res.*, 1985, **26**, 781–789.
- 49 A. Eisfeld and J. S. Briggs, *Chem. Phys.*, 2006, **324**, 376–384.
- 50 I. N. Kurniasih, H. Liang, P. C. Mohr, G. Khot, J. P. Rabe and A. Mohr, *Langmuir*, 2015, **31**, 2639–2648.
- 51 I. Mukherjee, S. P. Moulik and A. K. Rakshit, *J. Colloid Interface Sci.*, 2013, **394**, 329–336.
- 52 A. Pan, A. K. Rakshit and S. P. Moulik, *Colloids Surf., A*, 2015, **464**, 8–16.
- 53 G. Kasza, G. Gyulai, A. Abraham, G. Szarka, B. Ivan and E. Kiss, *RSC Adv.*, 2017, **7**, 4348–4352.
- 54 H. Liu, A. Jiang, J. Guo and K. E. Uhrich, *J. Polym. Sci., Part A: Polym. Chem.*, 2000, **37**, 703–711.
- 55 M. F. Mazzobre, M. V. Román, A. F. Mourelle and H. R. Corti, *Carbohydr. Res.*, 2005, **340**, 1207–1211.
- 56 We were aware that dye H-dimerization/aggregation within these polymer assemblies could have potentially affected the final fluorescence readings.
- 57 A. Rei, M. I. C. Ferreira and G. Hungerford, *J. Fluoresc.*, 2008, **18**, 1083–1091.
- 58 A. Boreham, M. Pfaff, E. Fleige, R. Haag and U. Alexiev, *Langmuir*, 2014, **30**, 1686–1695.
- 59 R. Plenderleith, T. Swift and S. Rimmer, *RSC Adv.*, 2014, **4**, 50932–50937.





- 60 A. Muñoz-Bonilla, O. León, M. L. Cerrada, J. Rodríguez-Hernández, M. Sánchez-Chaves and M. Fernández-García, *Eur. Polym. J.*, 2015, **62**, 167–178.
- 61 A. Muñoz-Bonilla, O. León, V. Bordegé, M. Sánchez-Chaves and M. Fernández-García, *J. Polym. Sci., Part A: Polym. Chem.*, 2013, **51**, 1337–1347.
- 62 S. Latunde-Dada, R. Bott, K. Hampton, J. Patel and O. I. Leszczyszyn, *Anal. Methods*, 2015, **7**, 10312–10321.
- 63 S. Latunde-Dada, R. Bott, D. Barker and O. I. Leszczyszyn, *Anal. Methods*, 2016, **8**, 386–392.
- 64 A. Hawe, W. L. Hulse, W. Jiskoot and R. T. Forbes, *Pharm. Res.*, 2011, **28**, 2302–2310.
- 65 H. Cottet, J.-P. Biron and M. Martin, *Analyst*, 2014, **139**, 3552–3562.
- 66 L. Cipelletti, J.-P. Biron, M. Martin and H. Cottet, *Anal. Chem.*, 2015, **87**, 8489–8496.
- 67 H. Cottet, J.-P. Biron and M. Martin, *Anal. Chem.*, 2007, **79**, 9066–9073.
- 68 W. L. Goh, M. Y. Lee, T. L. Joseph, S. T. Quah, C. J. Brown, C. Verma, S. Brenner, F. J. Ghadessy and Y. N. Teo, *J. Am. Chem. Soc.*, 2014, **136**, 6159–6162.
- 69 A. Hawe, V. Filipe and W. Jiskoot, *Pharm. Res.*, 2010, **27**, 314–326.
- 70 R. O. Dror, R. M. Dirks, J. P. Grossman, H. Xu and D. E. Shaw, *Annu. Rev. Biophys.*, 2012, **41**, 429–452.
- 71 B. M. Tande, N. J. Wagner, M. E. Mackay, C. J. Hawker and M. Jeong, *Macromolecules*, 2001, **34**, 8580–8585.
- 72 M. Delbianco, P. Bharate, S. Varela-Aramburu and P. Seeberger, *Chem. Rev.*, 2016, **116**, 1693–1752.
- 73 K. Liu, X. Jiang and P. Hunziker, *Nanoscale*, 2016, **8**, 16091–16156.
- 74 A. Surolia, S. Bishayee, A. Ahmad, K. Balasubramanian, D. Thambi-Dorai, S. Podder and B. Bachhawat, *Adv. Exp. Med. Biol.*, 1975, **55**, 95–115.
- 75 I. Papp, J. Dervedde, S. Enders, S. Riese, T. Shiao, R. Roy and R. Haag, *ChemBioChem*, 2011, **12**, 1075–1083.
- 76 Y. Gou, J. Geng, S.-j. Richards, J. Burns, C. R. Becer and D. Haddleton, *J. Polym. Sci., Part A: Polym. Chem.*, 2013, **51**, 2588–2597.
- 77 L. Martinez-Pomares, D. M. Reid, G. D. Brown, P. R. Taylor, R. J. Stillion, S. A. Linehan, S. Zamze, S. Gordon and S. Y. C. Wong, *J. Leukocyte Biol.*, 2003, **73**, 604–613.
- 78 Y. Su, T. Bakker, J. Harris, C. Tsang, G. D. Brown, M. R. Wormald, S. Gordon, R. A. Dwek, P. M. Rudd and L. Martinez-Pomares, *J. Biol. Chem.*, 2005, **280**, 32811–32820.
- 79 P. R. Taylor, S. Gordon and L. Martinez-Pomares, *Trends Immunol.*, 2005, **26**, 104–110.
- 80 L. Martinez-Pomares, *J. Leukocyte Biol.*, 2012, **92**, 1177–1186.
- 81 S. Snipstad, S. Hak, H. Baghirov, E. Sulheim, Y. Mørch, S. Lélou, E. von Haartman, M. Bäck, K. P. R. Nilsson, S. Klymchenko Andrey, C. de Lange Davies and K. O. Åslund Andreas, *Cytometry, Part A*, 2016, **91**, 760–766.
- 82 S. Snipstad, S. Westrøm, Y. Mørch, M. Afadzi, A. K. O. Åslund and C. de Lange Davies, *Cancer Nanotechnol.*, 2014, **5**, 8.
- 83 G. Bastiat, C. O. Pritz, C. Roider, F. Fouchet, E. Lignières, A. Jesacher, R. Glueckert, M. Ritsch-Marte, A. Schrott-Fischer, P. Saulnier and J.-P. Benoit, *J. Controlled Release*, 2013, **170**, 334–342.
- 84 S. Petersen, A. Fahr and H. Bunjes, *Mol. Pharm.*, 2010, **7**, 350–363.
- 85 B. D. Polizzotti and K. L. Kiick, *Biomacromolecules*, 2006, **7**, 483–490.
- 86 S.-J. Richards, M. W. Jones, M. Hunaban, D. M. Haddleton and M. I. Gibson, *Angew. Chem., Int. Ed.*, 2012, **51**, 7812–7816.
- 87 M. W. Jones, L. Otten, S. J. Richards, R. Lowery, D. J. Phillips, D. M. Haddleton and M. I. Gibson, *Chem. Sci.*, 2014, **5**, 1611–1616.

