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# Straightforward access to biocompatible poly(2-oxazoline)-coated nanomaterials by polymerization-induced self-assembly†

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**We report the synthesis of poly(2-ethyl-2-oxazoline)-based (PEtOx) nanoobjects by polymerization-induced self-assembly (PISA). First, well-defined PEtOx macromolecular chain transfer agents were synthesized by cationic ring-opening polymerization and click chemistry. The photoinitiated PISA of 2-hydroxypropyl methacrylate mediated by these PEtOx produced nanoobjects spanning the full range of core-shell morphologies. The nanoparticles exhibited high biocompatibility and stealth properties *in vitro* or *in vivo*, as well as thermoresponsive behavior.**

Poly(2-alkyl/aryl-2-oxazoline)s (PAOx), synthesized by cationic ring-opening polymerization (CROP), are valuable polymers in the biomedical field, thanks to their biocompatibility, stealth behavior, and chemical and physical versatility.<sup>1–4</sup> Coinciding with the recently renewed interest in PAOx, the first poly(2-ethyl-2-oxazoline) (PEtOx) conjugate has already entered phase II clinical trials for the treatment of Parkinson's disease.<sup>5</sup> Several studies have focused on the synthesis of functional PAOx to achieve functional hydrogels,<sup>6–8</sup> surface coatings,<sup>9</sup> and polymer-peptide/protein/drug conjugates.<sup>10,11</sup> Besides, the interest in PAOx-based complex structures is also increasing.<sup>12</sup> PEtOx brush-arm star and comb-shaped polymers incorporating nitroxide radicals and perfluorinated segments, respectively, have been reported for magnetic resonance imaging.<sup>13,14</sup> Patterned PEtOx bottlebrush copolymer brushes on diamond were reported for biosensor design.<sup>15</sup> Notably, PAOx-based core-shell nanoparticles (NPs) are promising nanocarriers for biomedicine.<sup>16</sup> Until now, these have been exclusively prepared by classic self-assembly of pre-synthesized amphiphilic block copolymer (ABCP).

Polymerization-induced self-assembly (PISA), developed in the last decade, has become an important approach for the fabrication of ABCP NPs with elaborate and precise macromolecular architecture, colloidal morphology, and functionality.<sup>17–23</sup> In a nutshell, PISA rests upon two events: (i) chain extension of a solvophilic macromolecular precursor with a monomer forming a solvophobic block and (ii) synchronous self-assembly of the so-formed amphiphilic block copolymer leading to core-shell NPs. As opposed to the classic nanoprecipitation-solvent exchange/evaporation method, PISA can be performed at a high polymer concentration (up to 50 vs. 1–2 wt%) and gives *in situ* access to morphologies as diverse as plain spheres, rods/fibers, and hollow vesicles. Reversible-deactivation radical polymerization, mostly reversible addition-fragmentation transfer (RAFT) polymerization, is the major underlying polymerization mechanism for PISA, occurring under either dispersion or emulsion polymerization conditions with styrene, (meth)acrylate, or (meth)acrylamide monomers. Other polymerization mechanisms are slowly making an appearance in the PISA realm, such as ring-opening metathesis polymerization,<sup>24–27</sup> in order to expand the chemistry and functionality of NPs.<sup>28</sup> However, because of the interest in greener solvents and the general requirement for polar solvents to produce biocompatible nanoparticles (*i.e.*, alcohols and water), employment of ionic polymerization is still limited.<sup>29</sup> Therefore, many interesting biocompatible polymers such as PAOx have not yet been included in PISA nanoobjects.

In this study, we describe the first combination of CROP and RAFT/PISA to obtain PAOx-based nanoobjects spanning a wide range of morphologies. First, dithiobenzoate-functionalized PAOx were prepared by CROP of a 2-oxazoline monomer in an aprotic solvent, followed by capping to introduce the chain transfer agent (CTA) moiety necessary for the RAFT polymerization. The functional PAOx were then used as a macromolecular CTA (macroCTA) in photoinitiated aqueous RAFT/PISA (photoRAFT/PISA). The influence of several parameters on the morphology was investigated, *i.e.*, mode of synthesis of the macroCTAs, chain length ratio between the solvophilic and solvophobic blocks, and concentration. Besides, we demonstrate that the obtained NPs are biocompatible *in vitro* and *in vivo*, and hence are suitable for potential bioapplications.

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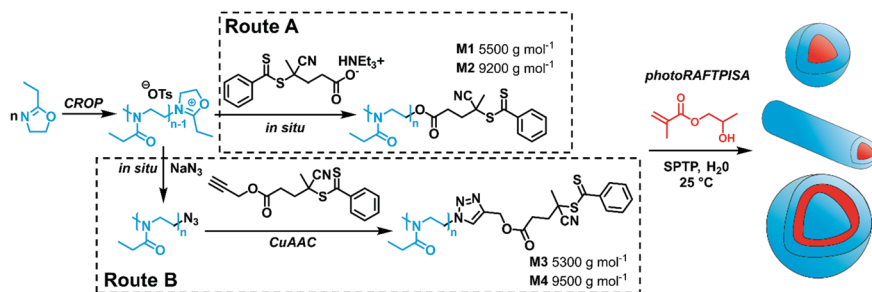
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**Scheme 1** Synthetic routes towards PETox-stabilized NPs by merging CROP and photoRAFTPISA. SPTP = sodium phenyl-2,4,6-trimethylbenzoylphosphine.

In particular, PETox was used in this study for its great hydrophilicity and its potential as an alternative to the established polyethylene glycol (PEG).<sup>30</sup> PETox was synthesized by CROP using methyl tosylate as an initiator. As shown in Scheme 1, the CTA end group could be incorporated either by direct capping with a deprotonated carboxylic acid-functionalized CTA (Route A)<sup>31,32</sup> or by a two-step sequence consisting of a nucleophilic substitution with sodium azide and a subsequent copper-catalyzed azide-alkyne cycloaddition (CuAAC) (Route B). Both routes showed similar kinetic features and fulfilled elementary criteria for a controlled/living polymerization, *i.e.*, linear increase of pseudo-first order plot, linear increase of number-average molar mass with conversion, and a clear shift of size-exclusion chromatography (SEC) traces (Fig. S2, ESI†). However, the nature of the capping reaction impacted the dispersity of the PETox (*D*); the *D* values were systematically slightly higher when capping with the carboxyl CTA, as compared with NaN<sub>3</sub>, concomitant with the presence of a significant shoulder at higher molar masses on the SEC traces (Fig. S2C, ESI†). In Route B, reaction conditions to introduce the CTA moiety by CuAAC (time, solvent) also influenced the shape of the molar mass distribution (MMD) and *D* (Fig. S7, ESI†). Performing CuAAC for 4 hours in dichloromethane (DCM) led to the smallest broadening of the MMD. This shouldering phenomenon may be – at least to some extent – due to partial decomposition of the CTA moiety to a thiol, which can be readily oxidized to disulfide and produce high molar mass coupled species (Fig. S5B and C, ESI†).<sup>33</sup> Indeed, CuAAC of PETox-N<sub>3</sub> with propargyl alcohol in similar conditions led to a significant reduction of MMD broadening (Fig. S8, ESI†). Overall, Route B required one more step but provided well-defined polymers with *D* ≤ 1.2 (Fig. S9, ESI†). For each route, two batches of PETox-CTAs were synthesized for the PISA experiments, with *M<sub>n</sub>* of approx. 5500 and 9500 g mol<sup>−1</sup>. The characteristics of these polymers are listed in Table S1 (ESI†). <sup>1</sup>H NMR and SEC coupled to electrospray ionization mass spectrometry (SEC-ESI-MS) data ascertained high RAFT functionality in all polymers (Fig. S3, S4, S10–S12, ESI†). The chain extension experiments with benzyl methacrylate in solution confirmed the previous trends: while macroCTAs from Route A underwent only partial chain extension (Fig. S13, ESI†), Route B led to clean block copolymers (Fig. S14 and S15, ESI†). Nevertheless, as a living character is not mandatory to obtain nanoparticles by PISA,<sup>34</sup> we further employed all four macroCTAs.

2-Hydroxypropyl methacrylate (HPMA) was used as a core-forming monomer in water. Since PETox exhibits a lower critical solution temperature in water at approx. 60 °C,<sup>35</sup> photopolymerization at 25 °C

was applied to maintain good solubility and the ability for steric stabilization. Firstly, PISA experiments with the short PETox-CTA **M1** were performed with varying targeted degrees of polymerization of HPMA (DP<sub>HPMA</sub>) and total solids content (Table S3, ESI†). All PISA experiments were conducted for 3 h and led to complete conversion of HPMA, as verified by <sup>1</sup>H NMR spectroscopy (Fig. S16, ESI†). As observed by TEM, only pure spherical NPs were obtained in the DP<sub>HPMA</sub> = 30–100 range at 5 wt% solids (Fig. S18, left, ESI†). At 10 wt%, a mixture of spheres and nanofibers was obtained for DP<sub>HPMA</sub> = 50 (Fig. S18, right, ESI†). Higher DP<sub>HPMA</sub> or solids concentration led to precipitation. Similar results were achieved for the CuAAC-based PETox-CTA **M3** with mainly plain spherical morphology but also large, possibly multicompartmented particles (Table S5 and Fig. S22, ESI†). While both short PETox-CTAs seemed to provide insufficient stabilization and led to aggregation at high DP<sub>HPMA</sub> and high concentration, PISA with longer analogs allowed the formation of nanoobjects spanning the full range of morphologies. Pure spheres, worm-like nanofibers, vesicles as well as morphology mixtures were obtained with **M2** (Table S4 and Fig. S20, ESI†). Higher-order morphologies evolved with increasing DP<sub>HPMA</sub> and solid contents. However, a significant rise in dispersity was also observed, which is most probably due to non-reinitiating PETox-CTA rather than to a loss of control. Indeed, SEC traces of PISA samples showed important amounts of low-molecular-mass species consistent with non-functionalized PETox and unreacted POx-CTA (Fig. S19, ESI†). By using the better-defined PETox-CTA **M4**, strongly improved MMDs were obtained with a total consumption of POx-CTA (Fig. S23, ESI†). Concomitantly, the PISA NPs displayed well-defined morphologies, as well as further more intricate shapes such as donut- and jellyfish-like (Fig. 1). At low solids content (5 wt%) and with DP<sub>HPMA</sub> up to 200, only spheres or donuts were observed, as for higher solids content with DP<sub>HPMA</sub> ≤ 100. However, a range of nanoobjects from spheres to vesicles was achieved when targeting higher DP<sub>HPMA</sub> above 5 wt%. In particular, conditions for the preparation of pure phases were established, even for jellyfish-like objects, an intermediate stage of the nanofiber-to-vesicle morphological transformation. PISA with higher-molar-mass PETox-CTAs, therefore, gave better results in terms of colloidal stability and morphology control. There is, however, no clear influence of the degree of livingness of the macromolecular CTAs on the morphological control.

In analogy to systems reported by Armes and co-workers,<sup>36</sup> phase transition of the final dispersions could be triggered by changing temperature. At high concentration, the vesicle-to-nanofiber-to-sphere



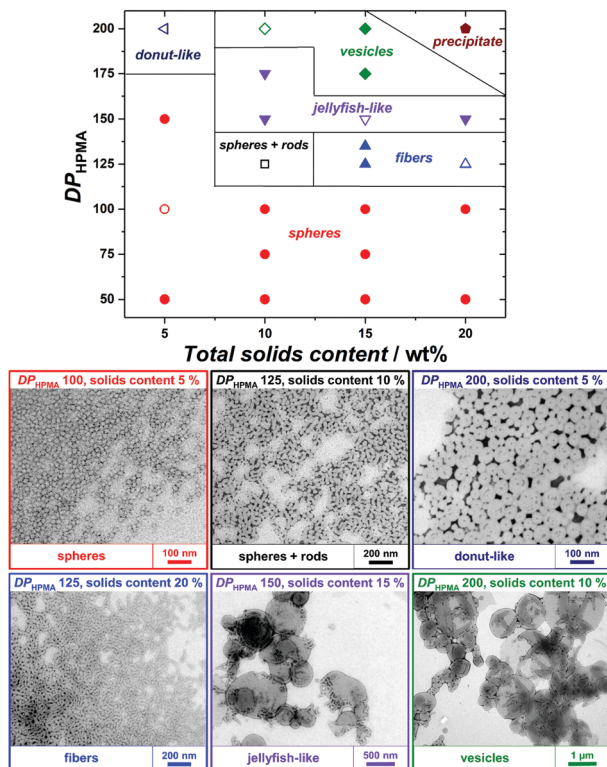


Fig. 1 (top) Phase diagram for RAFTPISA of HPMA using PETox-CTA **M4** as macroRAFT agent and (bottom) TEM images of representative samples (empty symbols from above). Larger TEM images are provided as Fig. S25 (ESI<sup>†</sup>).

transitions were reversible, irrespective of the initial state, *e.g.*, nanofibers and vesicles for **M4-*b*-PHPMA<sub>125</sub>** and **M4-*b*-PHPMA<sub>175</sub>** at 25 °C, respectively (Fig. 2A). Such order–order transitions in a narrow temperature range are due to not only the weakly hydrophobic nature of the core-forming PHPMA block<sup>37</sup> but also the temperature-dependent solubility of PETox. However, at low concentration, *e.g.*, 0.1 wt%, the transitions became irreversible (Fig. 2B) because the fusion of spheres or fibers is less likely under these conditions. For instance, vesicles of **M4-*b*-PHPMA<sub>125</sub>** obtained by heating a concentrated solution at 40 °C and carefully diluted at the same temperature irreversibly led to nanofibers, then spheres by gradual cooling.

Since PETox is considered as an attractive alternative to PEG for *in vivo* applications, we sought to preliminarily assess the biocompatibility and blood circulation behavior of the present PETox-coated NPs. For imaging purposes, fluorescent NPs were thus produced by simply adding a small amount of fluorescein methacrylate (FMA) or rhodamine 4-vinylbenzyl ester (RVB) comonomer to a PISA recipe (Scheme S2, ESI<sup>†</sup>). Spherical NPs with intensity-average hydrodynamic diameters of 40 and 60 nm were obtained (Table S7 and Fig. S27, ESI<sup>†</sup>) and expected maxima absorption and emission for fluorescein and rhodamine B (Fig. S28, ESI<sup>†</sup>).

To assess the biocompatibility and ability of the FMA-labeled PETox NPs to evade clearance by the reticuloendothelial system (RES), murine macrophages (RAW 264.7), human umbilical vein endothelial cells (HUVEC), and human epithelial lung cancer cells (A549) were incubated for 24 h, using fluorescein-labeled

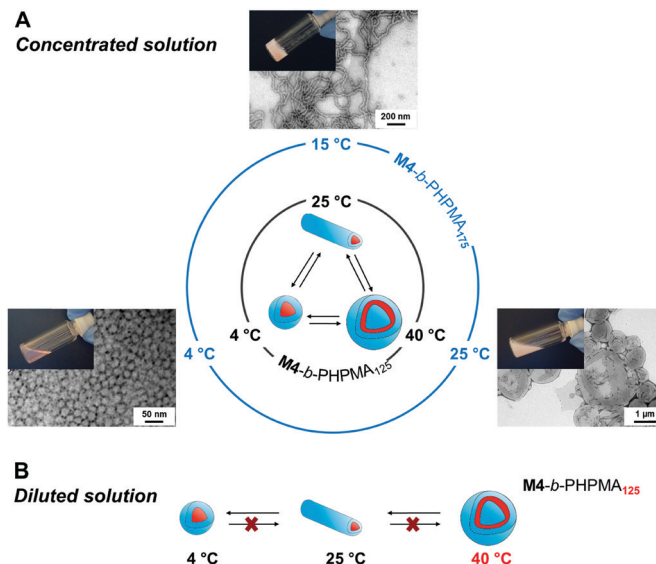


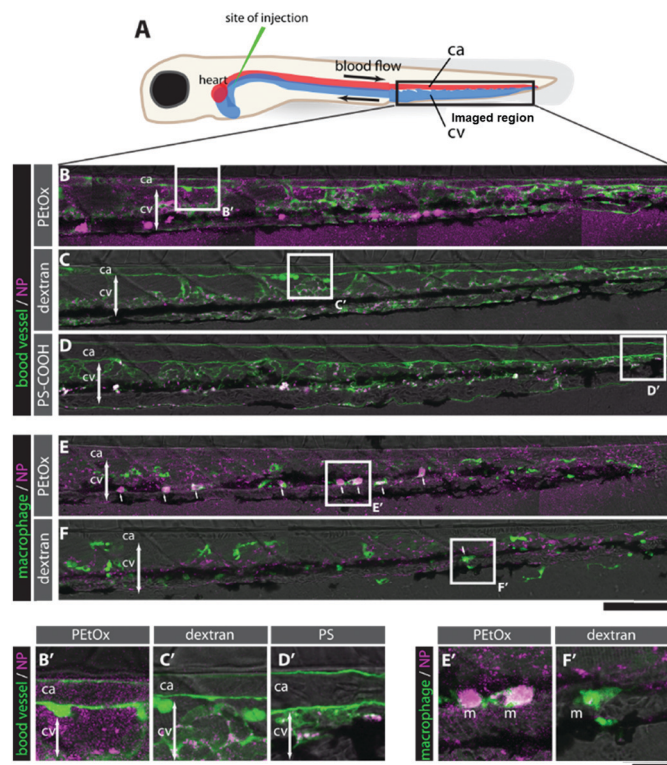
Fig. 2 Temperature-induced morphological transformation of (A) original nanofibers (**M4-*b*-PHPMA<sub>125</sub>**, 20 wt% at 25 °C) and vesicles (**M4-*b*-PHPMA<sub>175</sub>**, 15 wt% at 25 °C) in as-synthesized dispersions, and (B) vesicles (**M4-*b*-PHPMA<sub>125</sub>**, 0.1 wt% at 40 °C) at low concentration. Representative solutions and TEM images in (A) from the original nanofiber sample.

carboxylated polystyrene (PS-COOH) NPs as a reference material.<sup>38</sup> The RVB-labeled NPs were administered to zebrafish embryos and their biocompatibility, biodistribution, and clearance were examined for 24 h post-injection (hpi). As controls, PS-COOH NPs as well as rhodamine-labeled dextran were used in parallel. Both *in vitro* and *in vivo* studies are reported in more detail in the ESI<sup>†</sup>.

Briefly, as expected for the NPs covered with stealth polymers, the PETox NPs show none-to-very low uptake in all cell types and did not reduce cell viability up to 100  $\mu$ g mL<sup>-1</sup> (Fig. S31–S33, ESI<sup>†</sup>). In the zebrafish embryos, no noticeable morphological or behavioral changes were detected after intravenous injection of a 1 mg mL<sup>-1</sup> dispersion of the RVB-labeled NPs (Fig. 3). In contrast to dextran, which was rapidly cleared and only slightly accumulated in the endothelial cells in the caudal vein (CV) after 24 h (C, F, C', and F'), the RVB-PETox NPs mainly circulated in the bloodstream (B, E and B', E'). For comparison, the PS-COOH NPs were not detected in the circulation but were, as expected, entrapped in the RES (macrophages and endothelial cells) in the CV (D, and D'). However, contrary to the more simplistic *in vitro* experiments employing murine macrophages, a small fraction of RVB-PETox NPs could be detected in macrophages *in vivo* (E, and E'). In summary, our PETox NPs are biocompatible and display enhanced retention in the blood circulation. Furthermore, to accurately monitor clearance by the RES, the zebrafish model seems to be better suited than the conventional cell culture studies.

In the present communication, we described for the first time the synthesis of biocompatible PAOx-based diblock copolymer NPs by PISA. Control of morphology was achieved by varying the lengths of each block as well as the reaction mixture concentration. Dispersions based on pure phases of spheres, fibers, or vesicles were obtained. The nanoobjects display a thermosensitive behavior, enabling morphological transformation, which could be an asset





**Fig. 3** (A) Schematic of a 3 day-post-fertilization zebrafish embryo highlighting the artery (red), vein (blue), and site of NP injection, as well as the imaged region (rectangular region) shown in panels (B–F). The orientation of the embryos is dorsal up, anterior left. (B–D) Caudal region of zebrafish embryos at 24 hpi injected with either PETox NPs (magenta, B), rhodamine-conjugated 3 kDa dextran (magenta, C) or PS-COOH NPs (magenta, D). Blood vessels are demarcated with transgenic fluorescence (green). (E and F) The same region of the embryos highlighting the location of macrophages (green, arrows) injected either with PETox NPs (E) or dextran (F). ca: caudal artery; cv: caudal vein; m: macrophage; n: notochord. Scale bar: 100  $\mu$ m (B–F) and 20  $\mu$ m (B'–F').

for the preparation of bioactive materials. Importantly, the present PETox-based nanoparticles are non-toxic and exhibit prolonged circulation in the bloodstream. The versatility of PISA combined with the high potential of polyoxazolines in drug delivery and bioscaffolding promises rapid access to corresponding functional (nano)materials.

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## Conflicts of interest

There are no conflicts to declare.

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