Shape-memory and self-healing functions of DNA-based carboxymethyl cellulose hydrogels driven by chemical or light triggers†

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Photoresponsive nucleic acid-based carboxymethyl cellulose (CMC) hydrogels are synthesized, and their application as shape-memory and self-healing functional matrices are discussed. One system involves the preparation of a carboxymethyl cellulose hydrogel crosslinked by self-complementary nucleic acid duplexes and by photoresponsive trans-azobenzene/β-cyclodextrin (β-CD) supramolecular complexes. Photoisomerization of the trans-azobenzene to the cis-azobenzene results in a hydrogel exhibiting lower stiffness due to the separation of the azobenzene/β-CD bridging units. The hydrogel is switched between high and low stiffness states by the cyclic and reversible light-induced isomerization of the azobenzene units between the trans and cis states. The light-controlled stiffness properties of the hydrogel are used to develop a shape-memory hydrogel, where the duplex bridging units act as permanent memory in the quasi-liquid shapeless state of the hydrogel. A second system in the study is a carboxymethyl cellulose hydrogel crosslinked by the K⁺-stabilized G-quadruplex bridging units and by trans-azobenzene/β-CD complexes. The resulting hydrogel includes dual-trigger functionalities, where the trans-azobenzene/β-CD complexes can be reversibly formed and dissociated through the trans and cis photoisomerization of the azobenzene units, and the K⁺-stabilized G-quadruplexes can be reversibly dissociated and reformed in the presence of 18-crown-6-ether/K⁺-ions. The signal-responsive crosslinked hydrogel reveals controlled stiffness properties, where the hydrogel crosslinked by the trans-azobenzene/β-CD and K⁺-ion-stabilized G-quadruplex reveals high stiffness and the hydrogel crosslinked only by the K⁺-ion-stabilized G-quadruplexes or only by the trans-azobenzene/β-CD complexes reveals low stiffness properties. The controlled stiffness properties of the hydrogel are used to develop shape-memory hydrogels, where the trans-azobenzene/β-CD complexes or the K⁺-ion-stabilized G-quadruplexes act as permanent memories in the shapeless and quasi-liquid states of the hydrogels. In addition, the hydrogel that includes two types of stimuli-responsive crosslinking units is used as a self-healing matrix, where each of the triggers guides the self-healing processes.

Introduction

Hydrogels attract growing interest as functional materials for sensing, biomedical applications and tissue engineering. One broad class of hydrogels consists of hydrophilic polymers crosslinked by supramolecular complexes. Different crosslinking motifs were reported, and these include receptor/ligand complexes (receptor = cyclodextrin, cucurbituril), donor-acceptor complexes, ionic interactions, and bimolecular recognition complexes and metal–organic complexes. One class of hydrogels is the stimuli-responsive hydrogel matrices that undergo gel-to-liquid or gel-to-solid phase transitions in response to external triggers. Such systems are particularly interesting, as these phase transitions might occur upon the interaction with disease biomarkers or under specific cellular conditions (e.g., pH or redox conditions). As a result, these stimuli-responsive hydrogels might act as functional sensing matrices, targeted drug-delivery systems or tissue repair. Different external triggers, such as pH, heat, light, chemical agents or magnetic fields, were used to induce phase transitions of hydrogels or to control their stiffness. For example, photoresponsive polyacrylamide hydrogels were prepared by mixing polyacrylamide polymer chains modified with trans-azobenzene units and with β-cyclodextrin receptor units. The supramolecular binding of the trans-azobenzene units to the receptor units resulted in the...
crosslinking of the polymer chains and the formation of the hydrogel. Photoisomerization of the trans-azo-benzene to the cis-azo-benzene state lacks binding affinity to the β-cyclodextrin receptor, led to the separation of the supramolecular bridging units and to the hydrogel-to-liquid transition. In addition, polyacrylamide chains modified with terpyridine ligands were crosslinked by metal ions, e.g. Ru²⁺, via the formation of Ru²⁺–terpyridine complexes, to yield redox-responsive polyacrylamide hydrogels.³⁸ A further class of supramolecular hydrogels and, particularly, stimuli-responsive supramolecular hydrogels includes nucleic acid (DNA)-bridged hydrogels.³³–³⁵ The crosslinking of the polymer chains (e.g., polyacrylamide chains) by duplex nucleic acids provides a versatile means to generate hydrogels. Furthermore, the signal-triggered reversible reconfiguration of nucleic acid structures provides a rich arsenal of motifs to induce hydrogel-to-solution phase transitions or to control the stiffness of the hydrogel matrices. For example, polyacrylamide hydrogels crosslinked by stimuli-responsive K′-ions-stabilized G-quadruplex units were separated in the presence of 18-crown-6-ether (CE),³⁶ and hydrogels crosslinked by i-motif units at acidic pH values (pH = 5.5) were separated at neutral pH as a resulted of the dissociation of the supramolecular i-motif bridges.³⁷,³⁸ Of particular interest are the hybrid DNA hydrogels bridged by two different bridging motifs, such as duplex/G-quadruplex, duplex/triplex DNA or duplex/i-motif crosslinkers.³⁹ The signal-triggered reversible and switchable control over the stiffness of these hydrogels was demonstrated.

Different applications of stimuli-responsive DNA-based hydrogels and, particularly, stimuli-responsive hybrid DNA crosslinked hydrogels were reported, including controlled drug release,⁴⁰ switchable catalysis and electrocatalysis,⁴¹ controlled ion-transport through nanopores⁴² and stress-induced shape transitions of hydrogel composites.³⁹ In addition, other applications of stimuli-responsive hybrid DNA-based hydrogels include the use of these soft materials as shape-memory matrices and self-healing materials. Shape-memory polymers represent a class of "smart" materials that are processed into a permanent shape, which can be transferred, by an external trigger, into a temporary metastable shape that includes a code ("memory") to recover the original shape in the presence of a counter-trigger.⁴³–⁴⁴ By using duplex DNA and stimuli-responsive DNA structures that cooperatively crosslink and stabilize shaped hydrogels, a variety of shape-memory hydrogels were reported.⁴⁵–⁴⁷ In the presence of the two crosslinking motifs, a stiff shaped hydrogel was generated. The dissociation of the stimuli-responsive bridging units by an appropriate trigger resulted in low-stiffness, quasi-liquid, shapeless hydrogels, which included the residual duplex bridges that retain the entanglement of the polymer chains in the quasi-liquid state as an internal "memory" to recover the shape upon applying the counter trigger that restores the cooperative crosslinking of the stiff hydrogel.

The self-healing phenomenon of hydrogels represents a related process, where the crosslinking of soft hydrogels stabilized by cooperative hybrid bridges may lead to healed, intact hydrogels.⁴⁷ In fact, self-healing matrices that use supramolecular ligand–receptor interactions,⁴⁸,⁴⁹ Diels–Alder adducts,⁵⁰ light⁵¹ or H-bonds⁵² as functional bridges to "heal" hydrogels were reported, and the applications of these processes for tissue engineering and tissue recovery were addressed.⁵³ The self-healing of DNA-based hydrogels and, particularly, the use of DNA-based hydrogels that reveal shape-memory and self-healing functionalities are unprecedented. Furthermore, to date all DNA-based shape-memory hydrogels include two types of DNA as crosslinkers of the hydrogels, where one motif acts as the permanent memory and the other acts as the stimuli-responsive crosslinker that controls the stiffness of the hydrogel. The availability of different non-DNA stimuli-responsive crosslinkers allows, however, combining these triggers with stimuli-responsive DNA bridges. This allows the design of hydrogels exhibiting two different codes for the recovery of shapes or self-healed matrices. Moreover, the incorporation of non-DNA stimuli-responsive triggers as functional units that control the shape-memory and stiffness of the hydrogels introduces new time-domains for the transitions between the hydrogel states.

Results and discussion

In the present paper we report on the preparation of hybrid carboxymethyl cellulose (CMC) hydrogels consisting of nucleic acid bridges and trans-azo-benzene/β-cyclodextrin supramolecular crosslinking units as functional matrices for designing shape-memory hydrogels and self-healing materials. Specifically, we introduce hybrid CMC hydrogels crosslinked by duplex nucleic acids and supramolecular trans-azo-benzene/β-cyclodextrin photo-responsive units. In addition, we present CMC hydrogels crosslinked by two stimuli-responsive crosslinkers composed of K′-ion-stabilized G-quadruplexes/crown ether and trans/cis-azo-benzene/β-cyclodextrin units, respectively.

The CMC polymers P₃ and P₈ (Fig. 1A), were used to prepare the CMC hydrogel that is crosslinked by the light-active trans-azo-benzene/β-cyclodextrin units and the self-complementary nucleic acid-functionalized tethers (1)/(1) associated with the two polymer chains. The polymer P₃ was synthesized by the coupling of (N-aminoethyl p-carboxamide)-trans-azo-benzene (Scheme S1) via carbodiimide/N-hydroxysulfosuccinimide. In the next step, the aminohexyl-functionalized nucleic acid (1) was tethered to the carboxylic residues of CMC using carbodiimide/N-hydroxysulfosuccinimide coupling. The average loading of the azobenzene units on the CMC scaffold (Mₚ ≈ 250 kDa, degree of substitution = 0.9) was evaluated to be 1 : 10 by ¹H-NMR spectroscopy (Fig. S1 and S2†), and the loading of the nucleic acid tethers (1) on the CMC scaffold was determined spectroscopically to be 1 : 110, Fig. S3.† The polymer P₈ was prepared by the primary coupling of aminoethyl-β-cyclodextrin (β-CD) to the CMC scaffold, followed by the coupling of the aminoethoxy-modified nucleic acid (1) to the scaffold (for Experimental details see ESI†). The loading of β-CD units and the nucleic acid tethers (1) on the CMC backbone corresponded to 1 : 10 and 1 : 110, respectively (see ESI, Fig. S3–S5†). For further spectroscopic characterization of the polymers P₃ and P₈, see ESI Fig. S6 and S7.† The molecular weight of the
The photo-induced trans ↔ cis transitions proceed in the hydrogel, see ESI (Fig. S10).† Fig. S10A‡ depicts the absorption spectra of the trans-azobenzene/β-CD and (1)/(1)-crosslinked hydrogel (curve (a)), and of the (1)/(1)-crosslinked, free β-CD and cis-azobenzene-modified hydrogel (curve (b)). The spectra features are consistent with the light-induced formation of the trans-azobenzene and cis-azobenzene units. The photo-induced transitions between the trans-azobenzene and cis-azobenzene units are switchable and reversible, Fig. S10B.† The association constants of trans-azobenzene to β-CD ($K_a = 1100 \text{ M}^{-1}$) and of cis-azobenzene to β-CD ($K_a = 4.1 \text{ M}^{-1}$) were reported previously.29 This suggests that the photo-generated cis-azobenzene units indeed demonstrate low affinity towards the β-CD receptor units, leading to the hydrogel of low stiffness. The differences in the stiffness properties of the two hydrogel states are further supported by SEM images, Fig. 1D. The stiffer hydrogel crosslinked by the supramolecular trans-azobenzene/β-CD and the (1)/(1) duplexes demonstrates a high density of small pores, whereas the hydrogel of lower stiffness (quasi-liquid) only crosslinked by the (1)/(1) duplexes reveals substantially larger pores.

The light-induced control over the stiffness properties of the hydrogel was then applied to develop a shape-memory hydrogel, Fig. 2. In this system, the stiff hydrogel crosslinked by the trans-azobenzene/β-CD and the (1)/(1) duplex crosslinkers was prepared in the mold and extruded from it as the triangle shape, Fig. 2A. Subjecting the hydrogel to UV irradiation ($\lambda = 365 \text{ nm}$) resulted in the dissociation of the supramolecular crosslinking units due to the isomerization of the trans-azobenzene to cis-azobenzene that lacks affinity toward β-CD. The separation of the trans-azobenzene/β-CD bridges leads to a shapeless, quasi-liquid hydrogel. The resulting hydrogel includes, however, the (1)/(1) duplex units that provide an internal memory code for the reshaping of the hydrogel. The entangled polymer chain network provides the code to retain the spatial positions of the azobenzene and β-CD functionalities and the configuration of these polymer network to recover the original shape. That is, upon the reverse photoisomerization of the cis-state to the trans-

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**Fig. 1** (A) Schematic composition of a photo-responsive CMC hydrogel crosslinked by self-complementary duplexes (1)/(1) and trans-azobenzene/β-CD complexes. (B) Rheometry analysis corresponding to: (a and a’) the $G'$ and $G''$ of the CMC hydrogel crosslinked by the (1)/(1) and trans-azobenzene/β-CD complexes; (b and b’) the $G'$ and $G''$ of the (1)/(1)-crosslinked hydrogel in the presence of the cis-azobenzene tethers. (C) The reversible and switchable changes of the $G'$ and $G''$ upon the photoisomerization of the (1)/(1)-crosslinked hydrogel in the presence of the trans-azobenzene/β-CD complex (state I) and in the presence of the cis-azobenzene and β-CD units (state II). (D) SEM images of: (I) the stiff hydrogel in state I; (II) the hydrogel of low stiffness in state II.

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**Fig. 2** (A) Schematic preparation of a triangle-shaped CMC hydrogel crosslinked by the (1)/(1) duplexes and trans-azobenzene/β-CD complexes, and light-induced reversible transitions between the stiff shaped hydrogel I and the shapeless quasi-liquid hydrogel II that is only crosslinked by the (1)/(1) bridges. (B) Macroscopic images of the reversible light-induced transitions of the hydrogel between the triangle-shaped hydrogel I and the quasi-liquid shapeless hydrogel II, respectively.
state ($\lambda > 420 \text{ nm}$), the network-dictated formation of the trans-azobenzene/$\beta$-CD complexes recovers the triangle-shaped stiff hydrogel. Fig. 2B shows the cyclic shape-memory properties of the hydrogel. Irradiation of the stiff triangle-shaped hydrogel in state I ($\lambda = 365 \text{ nm}$) leads to the separation of the azobenzene/$\beta$-CD bridges and to the formation of the quasi-liquid, shapeless hydrogel in state II. Further visible-light illumination of the quasi-liquid hydrogel ($\lambda > 420 \text{ nm}$) restores the triangle shape of the stiff hydrogel crosslinked by the trans-azobenzene/$\beta$-CD and (1)/(1) tethers (state I). Using the Image-Pro Plus software, we estimate that the transition between the shaped (stiff) state and the quasi-liquid state involves a volume increase of ca. 25%.

In the next step, we designed a hybrid hydrogel that includes two stimuli-triggered crosslinking units, where each of these bridges may act as a shape-memory code. Two CMC polymer chain $P_c$ and $P_d$ were synthesized, Fig. 3A. The CMC polymer chain $P_c$ was modified with the photoisomerizable trans-azo-benzene units and the guanosine-rich tethers (2) that represent the sequences of G-quadruplex subunits. The CMC polymer scaffold $P_d$ includes $\beta$-cyclodextrin receptor units and guanosine-rich tethers (2). The average loading of the trans-azobenzene units and the guanosine-rich tethers (2) on the polymer chains $P_c$ was evaluated to be 1:10 and 1:87 by $^1$H-NMR and absorption spectroscopy, respectively (see Fig. S1, S11 and S13†). Similarly, the average loading of the $\beta$-cyclodextrin receptors and of the guanosine-rich tethers (2) on the polymer chains $P_d$, was evaluated to be 1:10 and 1:87 by $^1$H-NMR and absorption spectroscopy, respectively (Fig. S3, S12 and S13†).

For further characterization of the polymers $P_c$ and $P_d$, see ESI (Fig. S9, S14, S15 and Table S2).† The mixture of the polymers $P_c$ and $P_d$ yields the stimuli-responsive hydrogel in the presence of K$^+$-ions. The hydrogel is crosslinked by the supramolecular trans-azobenzene/$\beta$-CD bridges and by the K$^+$-ion-stabilized G-quadruplex units (that are composed by the two half G-rich subunits (2)). Rheometry experiments show that the storage modulus $G'$ and loss modulus $G''$ of the hydrogel in state I correspond to 83 Pa and 12 Pa, respectively (Fig. 3B). Photoisomerization of the trans-azobenzene to cis-azobenzene ($\lambda = 365 \text{ nm}$) separates the supramolecular azobenzene/$\beta$-CD bridges, leading to the hydrogel of low stiffness in state II that is crosslinked by the K$^+$-ion-stabilized G-quadruplex units ($G' = 51 \text{ Pa}, G'' = 7 \text{ Pa}$). Further illumination of the hydrogel in state II with visible light ($\lambda > 420 \text{ nm}$) restores the hydrogel in state I ($G' = 82 \text{ Pa}; G'' = 11 \text{ Pa}$). Subjecting the stiff hydrogel in state I to 18-crown-6-ether dissociates the G-quadruplex bridges by the elimination of K$^+$-ions that stabilize the G-quadruplex. This results in the hydrogel of low stiffness in state III, that is only crosslinked by the trans-azobenzene/$\beta$-CD supramolecular bridges ($G' = 56 \text{ Pa}, G'' = 8 \text{ Pa}$). By the reversible treatment of the hydrogel in state III with K$^+$-ions, the stiff hydrogel in state I is regenerated. The hydrogel can be cycled between high stiffness and low stiffness states by subjecting the stiff hydrogel in state I to reversible photoisomerization steps between the trans-azobenzene/cis-azobenzene states ($\lambda > 420 \text{ nm}/\lambda = 365 \text{ nm}$) or G-quadruplex/random strands (in the presence of K$^+$-ions/crown ether), Fig. 3C. Additional SEM images of the hydrogels in their different states support the stiffness properties of the hydrogels, Fig. 3D. The hydrogel in state I shows highly crosslinked structures of small pores (I), whereas the triggered transition of the hydrogel in state I to the hydrogel in state II or III generates hydrogels with lower crosslinking and large pores (images II and III, respectively).

The bimodal control over the stiffness properties of the G-quadruplex and trans-azobenzene/$\beta$-CD-crosslinked hydrogel by means of two alternative trigger, i.e., 18-crown-6-ether or light, were then applied to induce the controlled release of a load from the hydrogel, Fig. 4. Tetramethylrhodamine (TMR)-modified dextran was incorporated in the stiff hydrogel crosslinked by the G-quadruplex and trans-azobenzene/$\beta$-CD complex. No release of the TMR-dextran load from the hydrogel was observed after a time-interval of 4 h, Fig. 4, curve (a). The triggered photoisomerization of the trans-azobenzene to cis-azobenzene ($\lambda = 365 \text{ nm}$, irradiation time 10 min) resulted in the hydrogel of lower stiffness, due to the separation of the azobenzene/$\beta$-CD crosslinking units. The resulted hydrogel that exhibits lower stiffness allowed the release of the TMR-dextran.
The bifunctional stimuli-responsive hydrogel crosslinked by the \( \text{trans-azobenzene/}\beta\text{-CD + } K^+ \)-ion-stabilized G-quadruplex bridging units, was then applied to develop a shape-memory hydrogel, where each of the crosslinking elements is alternately applied as a shape-memory code, Fig. 5. The stiff hydrogel crosslinked by the \( \text{trans-azobenzene/}\beta\text{-CD + } K^+ \)-ion-stabilized G-quadruplex was prepared in a triangle-shaped mold. The extruded triangle-shaped hydrogel was subjected to UV light irradiation (\( \lambda = 365 \text{ nm} \)) that dissociated the \( \text{trans-azobenzene/}\beta\text{-CD + } K^+ \)-ion-stabilized G-quadruplex bridges. The low stiffness of the resulting hydrogel yielded a quasi-liquid shapeless hydrogel. The \( K^+ \)-ion-stabilized G-quadruplex-briding units provide, however, an internal memory for restoring the triangle-shaped hydrogel. The \( \beta\text{-CD} \)-quadruplex units provide the instructive memory of chain entanglement in the hydrogel to restore the shaped hydrogel upon the reverse photoisomerization of the cis-azobenzene units associated with the quasi-liquid hydrogel (\( \lambda > 420 \text{ nm} \)). The light-induced reversible shape-memory functions of the hydrogel are presented in Fig. 5A. Alternatively, the treatment of the triangle-shaped hydrogel in state I with \( \text{18-crown-6-ether} \) dissociates the G-quadruplex bridges, leading to the shapeless, quasi-liquid hydrogel in state III. The \( \text{trans-azobenzene/}\beta\text{-CD + } K^+ \)-ion-stabilized G-quadruplexes involve a volume transition of the shaped hydrogel in state I and the quasi-liquid hydrogel in state III, respectively. (B) Macroscopic images corresponding to shape-memory hydrogel transitions. (top) reversible and switchable light-induced transitions between a triangle-shaped hydrogel in state I and the shapeless quasi-liquid hydrogel in state II; (bottom) reversible and switchable transitions between the triangle-shaped hydrogel in state I and the quasi-liquid shapeless hydrogel in state III, using \( K^+ \) ions and \( \text{18-crown-6-ether} \) as triggers.

For further experimental support on the reversible reconfiguration of the \( K^+ \)-stabilized G-quadruplex-crosslinked hydrogel and its separation, in the presence of \( \text{18-crown-6-ether} \), into random-coil nucleic acid-modified hydrogel matrices, see Fig. S16† and the accompanying discussion. Fig. S16† shows the method and experimental results to follow the reversible reconfiguration of the G-quadruplex and its separation in the hydrogel matrix in the presence of \( K^+ \)-ions and \( \text{18-crown-6-ether} \), respectively. We make use of the fact that the \( K^+ \)-stabilized G-quadruplex binds hemin, and the resulting hemin/G-quadruplex exhibits horseradish peroxidase DNAzyme activities, where the catalyzed oxidation of Amplex Red by \( H_2O_2 \) generates the fluorescent resorufin product (Fig. S16A†). The hydrogel crosslinked by the \( K^+ \)-stabilized G-quadruplexes and the \( \text{trans-azobenzene/}\beta\text{-CD + } K^+ \)-ion-stabilized G-quadruplex units reveals, in the presence of hemin and \( H_2O_2 \), catalytic functions reflected by the formation of resorufin, Fig. S16B† curve (a). In contrast, treatment of the \( K^+ \)-stabilized G-quadruplex-crosslinked hydrogel with \( \text{18-crown-6-ether} \) leads to the separation of the G-quadruplex units, and to the loss of the catalytic activity towards the oxidation of Amplex.
Red to resorufin by H$_2$O$_2$, Fig. S16B† curve (b). These results confirm that the G-quadruplexes are presented as crosslinkers in the hydrogel matrix, in the presence of K$^+$-ions. Furthermore, the results imply that in the presence of 18-crown-6-ether, the G-quadruplex crosslinking units are separated. It should be noted that the transition of the shaped hydrogel to the quasi-liquid state, in the presence of 18-crown-6-ether, and the reverse re-assembly of the quasi-liquid state into the shaped state are quite slow, and each of the transitions proceeds for a time-interval of ca. 4 h after the application of the respective trigger. However, the photo-induced shape-memory transitions are faster. The irradiation (λ = 365 nm) of the shaped stiff hydrogel for a time-interval of 10 min, resulted in the quasi-liquid state. Similarly, illumination (λ > 420 nm) of the quasi-liquid state for 10 min recovered the original triangle-shaped hydrogel.

The dually triggered transitions of the trans-azobenzene/β-CD and G-quadruplex-crosslinked hydrogel between high and low stiffness were not only used as a hydrogel exhibiting shape-memory functions, but also as a functional matrix that reveals self-healing properties, Fig. 6. The hydrogel of low stiffness that was crosslinked by the trans-azobenzene/β-CD units was cut into two pieces that were physically interconnected, Fig. 6A. The inter-connected hydrogel was subjected to K$^+$-ions for a time-interval of 4 h. After this time-interval, the gel was self-healed into a non-separable, united hydrogel crosslinked by the K$^+$-ion-stabilized G-quadruplexes and the trans-azobenzene/β-CD supramolecular complexes. Then the resulting self-healed hydrogel could be cycled between low and high stiffness states. A control experiment of treating the two physically connected hydrogel pieces without K$^+$ ions did not lead to the healing of the hydrogel, and gentle shaking of the inter-connected hydrogel led to the separation of the hydrogel pieces, Fig. S17A†. In analogy, the light-induced self-healing of the hydrogel was demonstrated, Fig. 6B. The K$^+$-ion-stabilized G-quadruplex-bridged hydrogel including the non-bridged cis-azobenzene and β-cyclodextrin units was cut into two pieces. The pieces were physically inter-connected and subjected to visible irradiation (λ > 420 nm) for a time-interval of 15 min. The resulting hydrogel revealed self-healing properties, and the light-induced process led to the formation of a non-separable hydrogel matrix crosslinked by the two crosslinking motifs (the K$^+$-stabilized G-quadruplex and the trans-azobenzene/β-CD complex). Then, the resulting non-separable hydrogel could be cycled between lower and higher stiffness states by reversible photoisomerization of the azobenzene units between the cis and trans isomer states, respectively. In a control experiment, the physically connected two pieces were not irradiated, and gentle shaking of the pieces led to their separation (Fig. S17B†). Furthermore, UV irradiation of the two interconnected pieces did not yield a healed matrix, implying that possible healing of the matrix is not the source for the healing process. It should be noted that the initial inter-connection of the hydrogel pieces is not mandatory to reach the self-healing effect. Fig. S18† describes the self-healing of two separated pieces of low-stiffness hydrogel crosslinked by the trans-azobenzene/β-CD units upon shaking and addition of K$^+$-ions as the healing trigger.

**Conclusions**

The present study has introduced hybrid hydrogels that are cooperatively stabilized by photoisomerizable trans-azobenzene/β-cyclodextrin and nucleic acids as crosslinkers. In view of the G° and G° † values of the different hydrogels, we conclude that all hydrogel matrices are soft materials with moderate stiffness properties. In contrast to most previous stimuli-responsive DNA-based hydrogels that applied polyacrylamide as the polymeric backbone of the hydrogels, the present study introduced carboxymethyl cellulose (CMC) as the backbone matrix of the hydrogels. The availability of carboxylic acid residues on the CMC matrix provides effective anchoring sites for the conjugation of a variety of functional tethers. One system included the crosslinking of the hydrogel by trans-azobenzene/β-cyclodextrin supramolecular complexes and by duplex nucleic acid bridges. The stiffness of the hydrogel was shifted between high and low stiffness values by the cyclic switchable photoisomerization of the trans-azobenzene units to the cis-azobenzene units that lack binding affinity toward β-CD. These features were used to apply the photo-responsive hydrogel as a shape-memory. The second hydrogel system included a carboxymethyl cellulose backbone crosslinked by two stimuli-responsive units composed of trans-azobenzene/β-cyclodextrin and K$^+$-ion-stabilized G-quadruplex. The two types of crosslinkers were triggered individually to be separated by light (photoisomerization of the trans-azobenzene to cis-azobenzene) or by chemical means (separation of the G-quadruplexes by 18-crown-6-ether). These led to the development of a hydrogel that exhibited switchable and cyclic stiffness properties controlled either by light or chemical agents. The control over the stiffness
properties enables the development of shape-memory or self-healing hydrogels that use two different codes to stimulate these processes.

Conflicts of interest

There are no conflicts to declare.

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Notes and references