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Development of tungsten bronze nanorods for redox-enhanced photoacoustic imaging-guided photothermal therapy of tumors†

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Although various kinds of nanomaterials have been used as anticancer theranostics by exploiting the tumor microenvironment, relatively few nanomaterials can be efficiently activated by the tumor redox status for imaging and therapy. Oxygen-deficient tungsten-based oxides or bronzes are appearing as new classes of near-infrared (NIR)-responsive nanomaterials due to their unique properties such as tunable and broad NIR absorption. Herein, we synthesized PEG- Na_xWO_3 nanorods (NRs) by a simple thermal decomposition method and investigated their redox-activated performance for enhanced photoacoustic (PA) imaging and photothermal therapy (PTT) of cancers. Both *in vitro* and *in vivo* studies revealed that such a novel class of tungsten bronzes with low toxicity could be used as efficient photothermal agents for PA imaging-guided PTT of cancers.

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1. Introduction

The tumor microenvironment (*e.g.*, hypoxia, redox state, acidic pH, and so forth) has enabled tumor cells to evade or defend against the damage caused by traditional therapeutics such as radiotherapy, photodynamic therapy, chemotherapy, *etc.*^{1–3} Fast development of nano-therapy has provided promising perspectives, approaches, and strategies for anticancer therapy by exploiting the tumor microenvironment.^{4–7} Amongst all the physiological parameters, redox status plays an important role in the tumor to counteract tumor aggressive oxidative stresses by upregulating the redox species (*e.g.*, glutathione, superoxide dismutase, catalase, and glutathione peroxidase).^{8,9} Among

them, glutathione (GSH) is widely used as an indicator to assist cancer imaging or therapy since the levels of GSH in cancer tissues range from $0.5\text{--}10 \times 10^{-3} \text{ M}$,^{10,11} which is four-fold higher than that of normal tissues.

Development of novel strategies to detect and utilize the redox status for imaging or enhanced nano-therapy *in vivo* is highly desirable, as these could improve therapeutic efficacy and simultaneously reduce the damage of anticancer agents to normal tissues.^{12–15} By employing redox-activated molecules or nanomaterials, various approaches for monitoring the redox status have been reported,^{16,17} while relatively few cancer nano-therapies by exploiting tumor redox status have been reported so far. It is well known that photothermal therapy (PTT) can transform near-infrared (NIR) energy to heat for killing the tumor cells *via* hyperthermia or thermal ablation.^{18–22} Meanwhile, PTT can also be combined with photoacoustic (PA) imaging for imaging-guided cancer treatment since both use NIR-responsive nanomaterials.^{23–25} The design and synthesis of redox-responsive nanomaterials which can be reduced in the tumor redox microenvironment to increase NIR absorption for enhanced PA imaging-guided PTT are of great significance to eliminate the side effects of traditional PTT.

The oxygen-deficient tungsten oxides (WO_x) and tungsten bronzes (M_xWO_3) are promising photothermal agents because of their strong NIR photothermal conversion.^{26–38} Recently, Shi and co-workers reported that tunable oxygen vacancy concentrations could be regulated to enhance nanomaterials' magnetic resonance imaging performance due to the high affinity between the oxygen vacancies and water molecules.³⁸ Such critical features of tunable oxygen vacancies of tungsten

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bronzes under oxidized/redox status could be further applied to the GSH-enhanced photothermal conversion. Herein, oxygen-deficient PEGylated Na_xWO_3 nanorods (NRs) were synthesized to explore their properties and applications as theranostics for enhanced PTT in the tumor redox microenvironment. We found that the photothermal properties of Na_xWO_3 NRs were strengthened after GSH incubation, which was demonstrated by various *in vitro* experiments including PA imaging of NR-containing aqueous and GSH-responsive PTT therapy on 4T1 tumor cells. Furthermore, PA imaging-guided PTT of tumors was successfully achieved on 4T1 tumor-bearing mice after intravenous injection of Na_xWO_3 NRs.

2. Experimental

2.1 Materials

Sodium tungstate dihydrate ($\text{Na}_2\text{WO}_4 \cdot 2\text{H}_2\text{O}$) and ammonia solution ($\text{NH}_3 \cdot \text{H}_2\text{O}$) were purchased from Sinopharm Chemical Reagent Co., Ltd. 1-Octadecene (90%), oleic acid (OA), and cyclohexane (C_6H_{12}) were obtained from Sigma-Aldrich. SH-PEG_{5k} was acquired from Jenkem Co., Ltd. All reagents were of analytical grade and used without any purification.

2.2 Synthesis of PEG- Na_xWO_3 nanorods

Typically, 2 mmol $\text{Na}_2\text{WO}_4 \cdot 2\text{H}_2\text{O}$ was dissolved in 5 mL ammonia solution and placed into a flask, and 10 mL oleic acid and 30 mL 1-octadecene were added to the flask. The mixture was then stirred at room temperature for 3 h. After evaporation of ammonia at 80 °C under an argon atmosphere for 2 h, followed by 120 °C under an argon atmosphere for 2 h, the solution was heated to 280 °C and maintained for 2 h, then cooled down to room temperature. The product was centrifuged and dispersed in 20 mL cyclohexane. After washing with 10 mL ethanol, the mixed solution was centrifuged and the Na_xWO_3 nanorods (NRs) were finally dispersed in 15 mL DMSO. The PEG- Na_xWO_3 NRs were prepared by strong thiol-metal interactions. Briefly, the as-synthesized Na_xWO_3 NRs were re-dispersed in 15 mL deionized water, followed by addition of 5 mL deionized water containing 500 mg SH-PEG_{5k}, and stirred for 48 h at room temperature. Excess free PEG was removed by centrifugation (20 000 rpm, 15 min). The PEG- Na_xWO_3 NRs were dispersed in water or PBS for future experiments.

2.3 Photothermal evaluation of PEG- Na_xWO_3 NRs

An aqueous solution containing PEG- Na_xWO_3 NRs before and after incubation with different concentrations of 5 mM and 10 mM GSH was poured into a quartz cuvette. The cuvette was illuminated by a 980 nm laser with power density 1.5 W cm^{-2} for 5 min. The increase curves of temperature were monitored by FLIR™ A320 camera.

2.4 Cytotoxicity assessment

Murine breast carcinoma tumor 4T1 cells and murine macrophage cells (RAW 264.3) cells were cultured in Roswell Park Memorial Institute medium 1640 supplemented with 10% fetal bovine serum and 1% penicillin/streptomycin at 37 °C under

5% CO_2 . Human embryonic kidney 293 (HEK293) cells were cultured under 5% CO_2 at 37 °C in Dulbecco's Modified Eagle Medium supplemented with 1% penicillin/streptomycin and 10% fetal bovine serum. The cells were seeded into a 96-well cell culture plate at 10^5 per well and after 24 h incubation, PEG- Na_xWO_3 NRs with different concentrations (0.025, 0.05, 0.1, 0.2 and 0.4 mg mL^{-1}) were put into the wells and then incubated for another 24 h or 48 h at 37 °C under 5% CO_2 . Cell viability was determined by an MTT assay.

For photothermal ablation of 4T1 cells *in vitro*, the 4T1 cells were seeded into the 96-well plate at a density of 10^5 per well and then incubated at 37 °C under 5% CO_2 for 24 h. The PEG- Na_xWO_3 NRs reduced by GSH (5 and 10 mM) were dispersed in cell culture media with different concentrations (0.08, and 0.16 mg mL^{-1}). After 4 h incubation, the cells were exposed to the 980 nm laser (1.5 W cm^{-2}) for 5 min and then incubated for 20 h. The cell viability was calculated by the MTT assay.

2.5 Trypan blue stain

PBS containing PEG- Na_xWO_3 NRs (0.16 mg mL^{-1}) was added to a cell culture plate containing 4T1 cells and incubated for 24 h. Then cells were irradiated with the 980 nm laser (1.5 W cm^{-2}) for 5 min, followed by staining with 0.4% trypan blue solution for 15 min. Then, the cells were washed with PBS three times, and cell morphology of the cells was monitored by an inverted optical microscope (Olympus, IX71, Japan). Cells stained with blue were dead cells.

2.6 Tumor models

All animal procedures were under the guidelines of the Institutional Animal Care and Use Committee of Fudan University. All Balb/c or Kunming mice with an average weight of 20 g were purchased from the Laboratory Animal Centre, Shanghai Medical College of Fudan University, China. The 4T1 tumor-bearing models were generated by subcutaneously injecting 4T1 cells (10^6 in 100 μL PBS) on the right front leg region of the Balb/c mice. The mice were used when their tumor volumes reached about 80 mm^3 .

2.7 PA imaging *in vitro* and *in vivo*

To investigate the redox-activated PA imaging, PEG- Na_xWO_3 NRs were incubated with different concentrations of GSH (0, 10, and 15 mM) for 12 h and then were used for *in vitro* PA imaging.

Since the levels of GSH in cancer tissues range from $0.5\text{--}10 \times 10^{-3} \text{ M}$,^{10,11} for *in vivo* PA imaging, the 4T1 tumor-bearing mice were put on a Vevo LAZR instrument, and the tumor was covered with ultrasonic coupling gel. PA imaging was performed before intravenous injection of PEG- Na_xWO_3 NRs (150 μL , 3 mg mL^{-1}) and at different time (1, 2, 24 h) points post-injection (p.i.).

2.8 *In vivo* photothermal imaging and therapy

For *in vivo* photothermal therapy, 4T1 tumor-bearing mice were randomly divided into four treatment groups: (1) PBS alone; (2) PEG- Na_xWO_3 NRs alone; (3) NIR alone; (4) PEG- Na_xWO_3 NRs +



NIR. A dosage of PEG- Na_xWO_3 NRs ($150\ \mu\text{L}$, $3\ \text{mg mL}^{-1}$ in saline) was intravenously injected into the mice in groups 2 and 4. The mice in group 4 were then exposed to a $980\ \text{nm}$ laser with an output power density of $1.5\ \text{W cm}^{-2}$ (duration time: $5\ \text{min}$) at $2\ \text{h p.i.}$ The same power density and duration time of the laser were applied on the mice in group 3 as a control. Photothermal imaging was recorded using the FLIRTM A320 camera. The tumor volume of mice in the different groups were recorded every two days for two weeks. Relative tumor volume (V/V_0 , where V_0 represents the initial tumor volume), body weight, and tumor appearance were monitored. Hematoxylin-eosin (H&E) staining was performed at two days after the corresponding treatment.

2.9 Histological assessment

The standard H&E staining was conducted to monitor *in vivo* biocompatibility of PEG- Na_xWO_3 nanorods. Tissues (heart, liver, spleen, lung and kidney) of the Kunming mice were dissected for H&E staining after intravenous injection of NRs ($300\ \mu\text{L}$, $3\ \text{mg mL}^{-1}$ in saline) at two weeks and one month p.i. The histological sections were observed under an optical microscope.

3. Results and discussions

Tungsten bronzes (Na_xWO_3) were achieved using a modified thermal decomposition approach,⁴⁰ along with poly(ethylene glycol)-thiol modification through the strong coordination interactions between metal cations and thiol groups to further improve their biocompatibility.^{41–43} Transmission electron microscopy (TEM) images of the PEG- Na_xWO_3 NRs revealed an average size of around $30\ \text{nm}$ in width and $130\ \text{nm}$ in length (Fig. 1a and S1†). The HRTEM image indicated the NRs' crystalline nature (Fig. 1b), and the energy-dispersive X-ray (EDX)

spectrum (Fig. 1c) demonstrated the presence of all expected essential chemical elements (Na, W, and O). As shown in Fig. 1d, the X-ray diffraction pattern showed that the as-made NRs contained a Na_xWO_3 phase structure. All the above results demonstrated that the tungsten bronzes were successfully synthesized. The obtained PEG- Na_xWO_3 NRs exhibited excellent stability in aqueous solution (insert in Fig. 1a and S2†) and their hydrated size was $\sim 219.9\ \text{nm}$ with a low PDI of 0.140 (Fig. S3†), as measured by dynamic light scattering (DLS).

The UV-vis-NIR spectra of the PEG- Na_xWO_3 NRs showed a broad NIR absorption band from $700\ \text{nm}$ to $1200\ \text{nm}$ (Fig. 2a), which was very similar to the behavior of previously reported tungsten oxides and tungsten bronzes.^{33,39} Importantly, after incubation with GSH, the absorption of NRs enhanced gradually as the GSH concentration increased. The morphology of PEG- Na_xWO_3 NRs remained unchanged after GSH reduction (Fig. S4†). GSH reduction was supposed to occur on the surface of nanorods, which would not alter the nanorod's shape. The spectral difference indicated that the oxygen vacancy concentration on the surface of the NRs was increased after reduction by GSH, which is caused by the partial valence decrease of W^{6+} to W^{5+} . PA images of PEG- Na_xWO_3 NRs with and without GSH incubation further demonstrated the NRs' redox-activated performance, where the samples with higher levels of reduction exhibited higher PA signal intensities (Fig. 2b). Then, the PEG- Na_xWO_3 NRs were exposed to a $980\ \text{nm}$ laser ($1.5\ \text{W cm}^{-2}$) to evaluate their photothermal conversion. As shown in Fig. 2c, the temperature of the PEG- Na_xWO_3 NR dispersed aqueous solution increased rapidly over $5\ \text{min}$, while pure water showed a limited temperature change under irradiation. Furthermore, we found that the solutions with higher GSH concentrations exhibited higher temperature change, which was consistent with the above results, demonstrating that the PEG- Na_xWO_3 NRs after redox-activation were more efficient at transforming light-energy to heat.

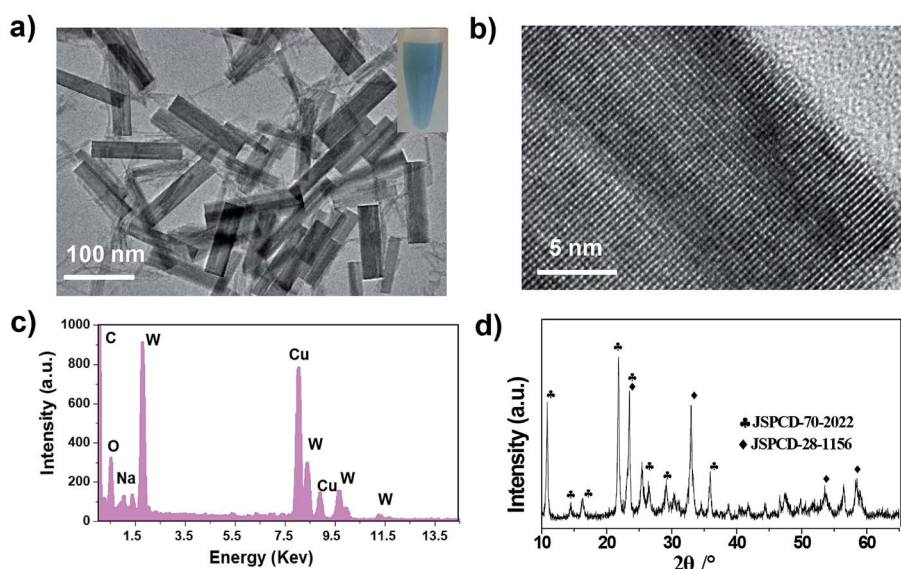


Fig. 1 (a) TEM image of PEG- Na_xWO_3 NRs dispersed in water. (b) High-resolution TEM image of one nanorod. (c) EDX spectrum and (d) XRD of Na_xWO_3 NRs.



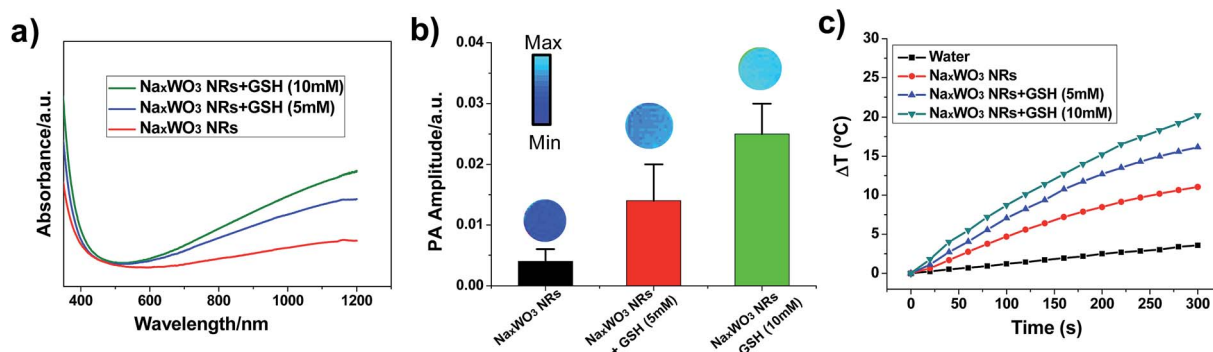


Fig. 2 (a) UV-vis-NIR absorption spectra of an aqueous dispersion containing PEG-Na_xWO₃ NRs before and after reduction by GSH with different concentrations. (b) PA imaging and PA signal of PEG-Na_xWO₃ NRs before and after incubation with different concentrations of GSH (control, 5, and 10 mM). (c) The temperature increase curves of pure water and aqueous dispersions of PEG-Na_xWO₃ NRs without or with GSH incubation when exposed to 980 nm laser irradiation for 5 min.

Before conducting imaging and therapy experiments *in vivo*, a standard MTT assay was conducted to evaluate the cytotoxicity of PEG-Na_xWO₃ NRs at various concentrations (0.025, 0.05, 0.1, 0.2, and 0.4 mg mL⁻¹), which exhibited negligible toxicity to 4T1 cells and normal cell lines (*i.e.*, RAW264.3 and HEK293 cells) at both 24 h and 48 h incubation (Fig. 3a and S5[†]), demonstrating that PEGylation of nanomaterials can significantly enhance the biocompatibility. Subsequently, the PEG-Na_xWO₃ NRs reduced by different concentrations of GSH (5 and 10 mM) were incubated with 4T1 cells, followed by exposure to the 980 nm laser for 5 min at the power of 1.5 W cm⁻². As shown in Fig. 3b, more cells were killed upon NIR laser irradiation with stronger reducing levels or higher concentrations of PEG-Na_xWO₃ NRs. Furthermore, trypan blue staining was performed to confirm the MTT results, which could differentiate dead cells from live

cells (Fig. 3c). Most of the tumor cells treated with nanorods and NIR exposure were killed, while only negligible dead cells were observed for the groups without any treatment, or treatment with nanorods or NIR laser irradiation only.

Encouraged by these *in vitro* findings, we then performed the *in vivo* PA along with ultrasound images on 4T1 tumor-bearing mice prior to, and at different time points after, intravenous injection of PEG-Na_xWO₃ NRs. As shown in Fig. 4a and S6[†], the ultrasound images could visualize the tumor anatomy (*e.g.*, skin and inclusion edge), while the PA images were utilized to reveal the accumulation of NIR-responsive PEG-Na_xWO₃ NRs. The PA imaging signal was clearly detected in the tumors after injection, which reached the highest at 2 h p.i., demonstrating that PEG-Na_xWO₃ NRs could act as PA imaging agents after accumulation in the tumor by the well-known enhanced

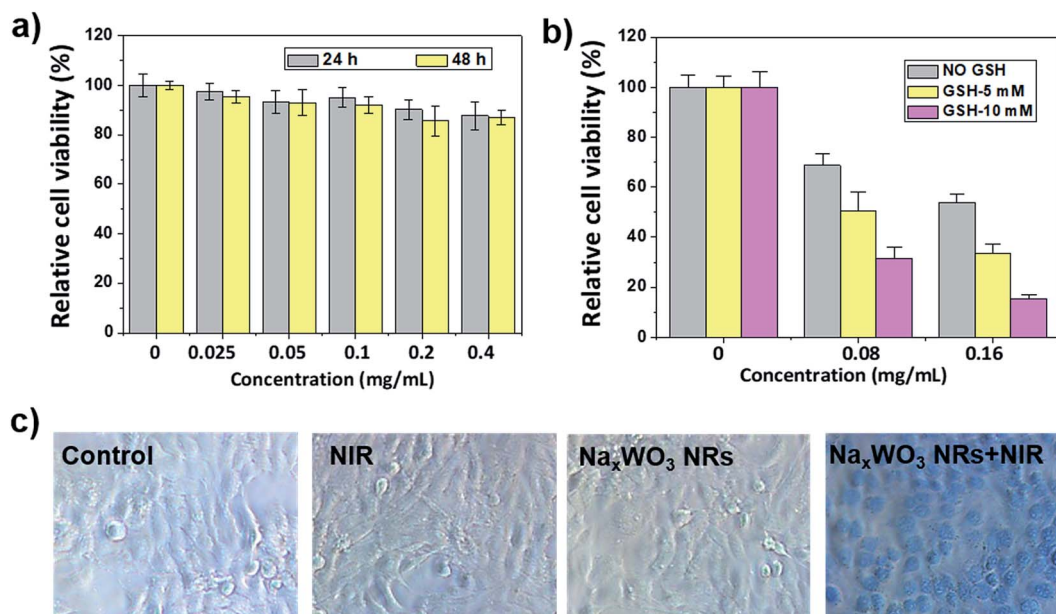


Fig. 3 (a) Relative viabilities of 4T1 cells after incubation with different concentrations of PEG-Na_xWO₃ NRs. (b) Relative viabilities of 4T1 cells after photothermal therapy at varied concentrations of PEG-Na_xWO₃ NRs reduced by different GSH concentrations under 980 nm NIR laser irradiation for 5 min. (c) Optical microscopy images of 4T1 cells stained with trypan blue after various treatments indicated.



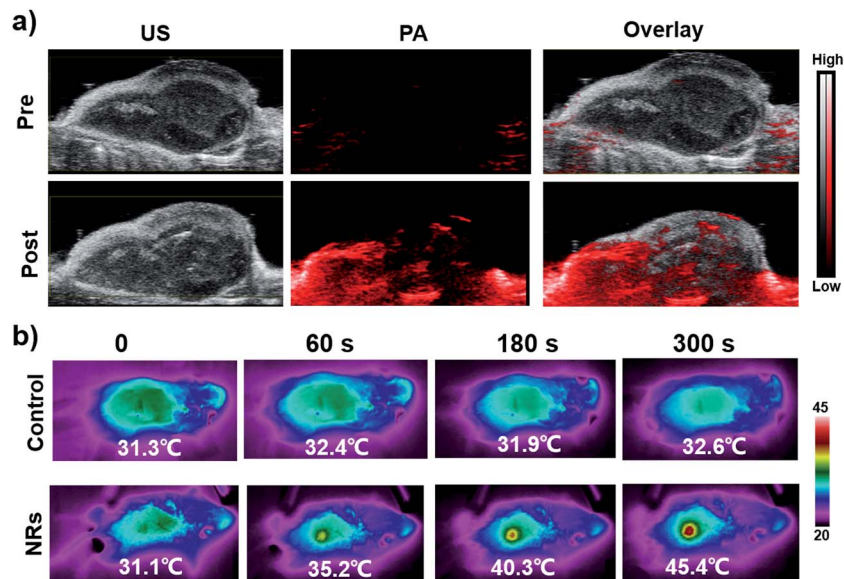


Fig. 4 (a) *In vivo* PA images of 4T1 tumor-bearing mice before and after intravenous injection with PEG- Na_xWO_3 NRs at 2 h p.i. (b) *In vivo* photothermal images of 4T1 tumor-bearing mice before and after intravenous injection with PEG- Na_xWO_3 NRs at 2 h p.i. under continuous 980 nm laser irradiation.

permeability and retention (EPR) effect. Since the GSH content in the tumor tissues is relatively high,^{10,11} partial PA imaging signals may be attributed to the redox-activated characteristics of PEG- Na_xWO_3 NRs. For photothermal imaging, the tumor temperatures without and with PEG- Na_xWO_3 NRs treatment

were increased by 1.3 °C and 14.3 °C, respectively, within 5 min of 980 nm laser irradiation (Fig. 4b). The highest temperature of a Na_xWO_3 NRs treated tumor reached about 45.4 °C, which could thereby kill cancer cells *via* hyperthermia (40–45 °C). These results confirm that the PEG- Na_xWO_3 NRs can serve as

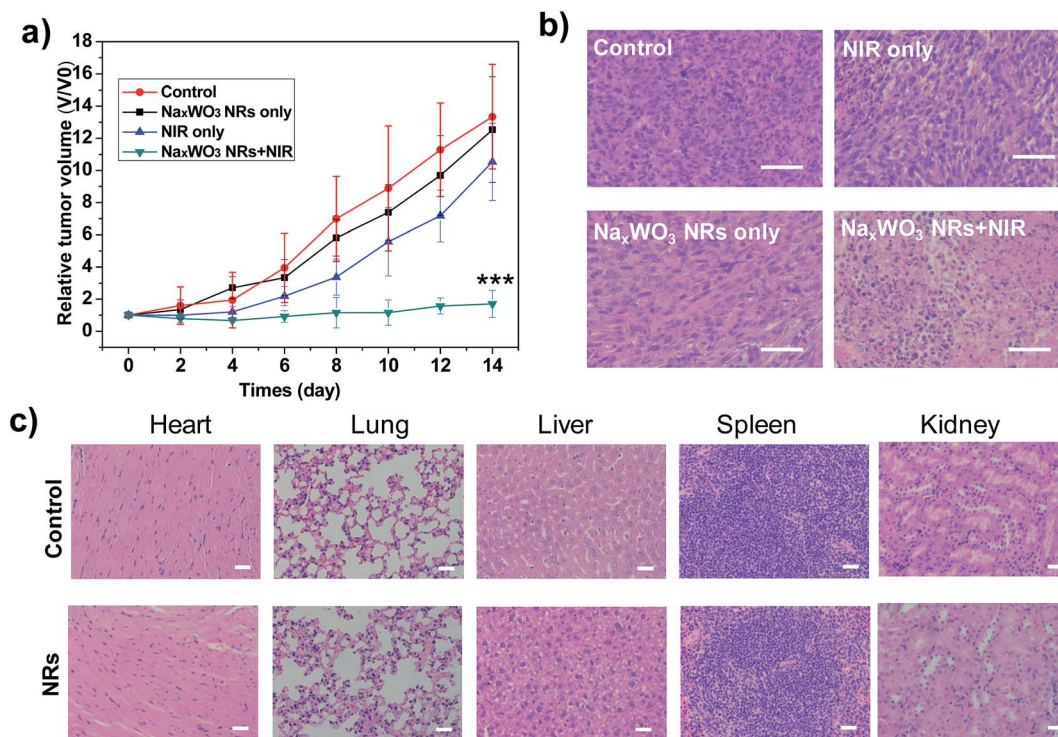


Fig. 5 (a) Relative tumor growth profiles of 4T1 tumor-bearing mice after various treatments indicated (for each group, $n = 4$, mean \pm s.d., *** $P < 0.001$, versus control). (b) The H&E staining of tumor tissues obtained from mice in different groups. Scale bar: 50 μm . (c) The H&E staining of major organs from mice after intravenous injection of PEG- Na_xWO_3 NRs at two weeks.



a sensitive PA imaging contrast agent for imaging-guided PTT of cancers.

As shown in Fig. 5a, the tumor growth is substantially inhibited by intravenous injection of PEG- Na_xWO_3 NRs under 980 nm laser irradiation, while the control, NRs, and NIR treated groups showed rapid tumor growth. Meanwhile, hematoxylin and eosin (H&E) staining of tumor tissues' histological changes further confirmed the above tumor growth results, where therapy groups showed the most tumor damage. In two weeks, neither significant weight loss nor any abnormal behavior were observed in any of the groups (Fig. S7†), indicating no noticeable side effects of the NRs. The H&E stained images of different organs (heart, liver, spleen, lung, and kidney) on normal mice revealed negligible organ damage or inflammatory lesions both in two weeks and one month (Fig. 5b and S8†), indicating the low toxicity of PEG- Na_xWO_3 NRs.

4. Conclusion

In summary, the novel oxygen-deficient PEG- Na_xWO_3 NRs were successfully synthesized and used for PA imaging-guided PTT. Upon application of 980 nm NIR light, the photothermal effect of PEG- Na_xWO_3 NRs led to a rapid increase of local temperature, which could be further enhanced under the tumor redox microenvironment, as demonstrated both in aqueous solutions and 4T1 cells *in vitro*. Moreover, PA imaging-guided photothermal therapy was also successfully achieved on 4T1 tumor-bearing mice *in vivo*. Our results not only provide the tunable oxygen vacancy properties of tungsten bronzes for PA imaging-guided cancer therapies but also encourage further exploration of the tumor redox microenvironment for biomedical applications.

Conflicts of interest

The authors declare no competing financial interest.

Acknowledgements

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