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Electrocatalytic oxidation and determination of dexamethasone at an Fe₃O₄/PANI–Cu^{II} microsphere modified carbon ionic liquid electrode

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A novel, simple, sensitive and selective electrochemical sensor based on an Fe₃O₄/PANI–Cu^{II} microsphere modified carbon ionic liquid electrode is constructed and utilized for the determination of dexamethasone. The synthesized Fe₃O₄/PANI–Cu^{II} microspheres are characterized by routine methods such as X-ray photoelectron spectroscopy (XPS), X-ray diffraction (XRD), transmission electron microscopy (TEM), scanning electron microscopy (SEM), Fourier transform infrared spectroscopy (FT-IR), thermo gravimetric analysis (TGA), and inductively coupled plasma atomic emission spectroscopy (ICP-AES). The Fe₃O₄/PANI–Cu^{II} microspheres can significantly accelerate the electron transfer rate and represent excellent synergistic electrochemical activity for the oxidation of dexamethasone. Differential pulse voltammetry (DPV) was used for the quantitative determination of dexamethasone. As shown, the oxidation peak current is linear with the concentration of dexamethasone in the range of 0.05 to 30 μM with a detection limit of 3.0 nM which is more sensitive than most of the previously reported methods. The proposed method is successfully applied to the sensitive determination of dexamethasone in real samples with satisfactory recoveries.

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1. Introduction

Dexamethasone-11 β ,16 α -9-fluoro-11,17,21-trihydroxy-16-methylpregna-1,4-diene-3,20-dione, abbreviated here as DXM, is a potent synthetic derivative of the glucocorticoid hydrocortisone. It is regularly employed as an anti-inflammatory and immunosuppressive agent for the treatment of conditions such as inflammation, allergy, and autoimmune conditions.^{1,2} This medication has been added to the list of banned medications because of its misuse as a doping agent in sports such as cycling and horse racing to improve performance.³ Therefore, development of new, sensitive, selective and simple analytical approaches and techniques for determining dexamethasone in biological fluids such as plasma and urine is essential after administration for efficient and safe use. Different reports have been published in the literature for determining dexamethasone which include LC-MS,^{4–6} LC-MS-MS,⁷ GC-MS detection,⁸ HPLC chemiluminescence^{9,10} thin-layer chromatography,¹¹ and electrochemical detection.¹² Although these approaches show some merits, they are disadvantageous due to the complicated instruments required and the associated time-consuming

sample pretreatment. Electrochemical techniques make a good candidate for the analysis of dexamethasone due to their practicality, simplicity, low-cost, and ease of miniaturization for small-volume samples.^{3,13,14} In recent years, carbon ionic liquid electrode (CILE), which is prepared by incorporating an ionic liquid as both binder and modifier in carbon paste electrode (CPE) have been widely used in the field of electrochemical sensing.^{15–17} These types of sensors have different advantages such as low cost, easy preparation, high sensitivity, high conductivity, wide electrochemical windows, antifouling effect and renewable surface. Composites of conducting polymers (CPs) and metal nanoparticles have received much attention in the last decades because of their various applications such as catalysts, biosensors and capacitors.^{18,19} Incorporation of metal nanoparticles would preserve the properties of low dimensional conductors, enhance the conductivity of polymers, and obtain high surface areas. The incorporation of Fe₃O₄ nanoparticles into polyaniline (PANI) matrix has been extensively studied because Fe₃O₄–PANI composite reveals characteristics through the combination of both components including good biocompatibility, large surface areas, good electrochemical stability and enhanced electrocatalytic activity.²⁰ Recently, Fe₃O₄ composites or hybrids doped with noble or other transition metals have attracted great attention, because of their doping or synergetic effect. These effects have meaningfully broadened the property and potential application value of Fe₃O₄ nanomaterials.^{21–23} Among them, Cu loaded onto Fe₃O₄ improve the catalytic activity due to the synergetic effect.²⁴ In this research study,

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a novel electrochemical sensor was generated for determining of DXM based on $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ modified CILE. The results of voltammetric studies showed that the fabricated sensor has excellent advantages such as higher sensitivity and selectivity, wider linear ranges, simpler electrode fabrication process and stability. In addition, it can be applied to the sensitive detection of DXM in real samples as it has been shown.

2. Experimental

All experiments were carried out in accordance with the World Medical Association's "Ethical principles for medical research involving human subjects", and approved by the medical ethics committee at Kermanshah University of Medical Sciences. There is no experimentation with human subjects in this study.

2.1. Apparatus and chemicals

Electrochemical measurements were carried out with a potentiostat-galvanostat Autolab equipped with a three-electrode cell containing a saturated Ag/AgCl as a reference electrode and a platinum electrode as an auxiliary electrode. CILE modified with $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres was applied as working electrode. The system was run on a PC by NOVA and FRA 1.11 software. A Metrohm 710 pH meter was used for pH adjustment. The synthesized $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres was characterized by power X-ray diffraction (XRD) was performed on a Bruker D8-advance X-ray diffractometer with $\text{Cu K}\alpha$ ($k = 0.154 \text{ nm}$) radiation and thermo gravimetric analysis (TGA) was performed using a Shimadzu thermo gravimetric analyzer (TG-50). TEM analysis was carried out using TEM microscope (Philips CM30). FT-IR spectra were recorded on a Shimadzu Fourier Transform Infrared Spectrophotometer (FT-IR-8300). The morphology of the products was determined by using Hitachi Japan, model s4160 Scanning Electron Microscopy (SEM) at accelerating voltage of 15 kV. This system was equipped with a concentric hemispherical (CHA) electron energy analyzer (Specs model EA10 plus) suitable for X-ray photoelectron spectroscopy (XPS). The Cu loading amount was determined by OPTIMA 7300 DV ICP analyzer.

Chemicals were purchased from Merck and Fluka Chemical Company. DXM powder (pure) was provided from Aldrich chemicals (Milwaukee, USA). All the reagents used were of analytical grade and double distilled water was used throughout the experiments. Daily-based fresh frozen blood serum samples were prepared from the venous blood of random healthy male and female blood donors, obtained from Imam Reza Hospital (Kermanshah, Iran). Urine sample obtained from healthy individuals were stored frozen until assay.

2.2. Synthesis of Fe_3O_4 microspheres

Magnetite particles were synthesized by using a solvothermal method.²⁵ $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$ (1.4 g, 5 mmol) was dissolved in ethylene glycol (EG) (40 mL) to form a clear solution, followed by the addition of sodium acetate (NaAc) (3.6 g). The mixture was stirred vigorously for 15 min, and then was sealed in a Teflon-lined stainless-steel autoclave. The autoclave was heated to

200 °C and maintained at this temperature for 5 h, and then was cooled to room temperature (RT). The resulting black product was washed with ethanol and deionized water several times, and was finally dried.

2.3. Synthesis of $\text{Fe}_3\text{O}_4/\text{PANI}$ composite microspheres

The $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres was prepared by *in situ* chemical oxidative polymerization of aniline in the presence of Fe_3O_4 microspheres. In this method, 0.3 mL HCl (0.1 M) was dissolved in 10 mL of deionized water. Then, the Fe_3O_4 (0.25 g) microspheres and 0.2 mL aniline monomer were added to the above reaction mixture and stirred at room temperature. Five milliliters of aqueous APS (2.2 mmol) was added dropwise to the solution of PANI/HCl complex containing Fe_3O_4 microspheres under ultrasonic irradiation and the reaction was allowed to proceed for 3 h at RT. The resultant product was washed with deionized water, methanol and ether three times, respectively, and then dried in vacuum for 12 h to obtain green-black powder of $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres.²⁶

2.4. Loading of Cu on $\text{Fe}_3\text{O}_4/\text{PANI}$ ($\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$)

The as-synthesised $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres (100 mg) were first dispersed in ethanol solution (50 mL) under ultrasonication for 0.5 h. The formed black suspension was ultrasonically mixed with (30 mL, 0.1 M) of CuCl_2 for 1 h. After this, the microspheres were harvested with the aid of a magnet and washed with deionized water three times and dried under vacuum.

2.5. Preparation of modified electrode

The traditional carbon paste electrode (CPE) was fabricated by mixing 30.0 w/w% of paraffin oil and 70.0 w/w% of graphite powder. The CILE was fabricated by mixing 20.0 w/w% of paraffin oil, 10.0 w/w% of solid I(EMIMPF₆) and 70.0 w/w% of graphite powder. The $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ was fabricated by hand mixing the optimal amounts of graphite powder, paraffin oil solid I(EMIMPF₆) and $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ (60 : 10 : 15 : 15% w/w). Other modified electrodes were prepared using a similar procedure for comparison. Each paste was packed firmly into pipette tube in which electrical contact was made with a copper wire that runs through the center of the electrode body. Prior to experiment, the surface of each the prepared electrodes polished using a butter paper to produce reproducible working surface and then was used for electrochemical studying of DXM by voltammetric techniques.

2.6. Real sample preparation

Human urine and serum samples were taken from healthy donors and used shortly after collection. The urine sample was centrifuged and diluted 10 times without any further pretreatment. The serum sample was treated with 2 mL methanol (as protein precipitating agent). The precipitated proteins were separated out by centrifugation for 3 min at 6000 rpm. The clear supernatant layer was filtered and diluted to a definite volume.



3. Results and discussion

3.1. Characterization of the $\text{Fe}_3\text{O}_4/\text{Cu}(\text{II})$ microspheres

Scanning electron microscope (SEM) images of the resulting Fe_3O_4 microspheres are shown in (Fig. 1a). As it can be seen, the generated Fe_3O_4 microspheres have a spherical shape with a rough surface and an average diameter of 145 nm. The $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres consisted of aggregates of small magnetite particles with sizes from 15 to 20 nm as calculated using transmission electron microscopy (TEM) (Fig. 1b). A continuous layer of PANI could be observed on the outer shell of the Fe_3O_4 microsphere cores. The average thickness of the PANI shell was 25 nm. From the TEM image of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ (Fig. 1c), it could be seen that the morphology of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ almost remained the same after loading CuCl_2 on $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres.

The structures of the (a) Fe_3O_4 microspheres, (b) $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres, and (c) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres were analyzed using FT-IR spectroscopy, as shown in Fig. 2. In curve (a), the strong absorption peak at 576 cm^{-1} corresponds to the Fe–O vibrations, the adsorption peaks located at 3384 , 1622 and 1406 cm^{-1} can be attributed to the stretching vibration of –OH, C=O and C–O of carboxyl groups, respectively. As for $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres displayed in Fig. 2b the characteristic peaks at 1585 and 1498 cm^{-1} ($\text{C}=\text{N}$ and $\text{C}=\text{C}$ stretching vibration of the quinoid and benzenoid ring, respectively), 1304 and 1143 cm^{-1} (C–N stretching of the secondary aromatic amine), 1247 cm^{-1} (C–N stretching vibration in protonic acid doped PANI), and 829 cm^{-1} (out of plane deformation of C–H in the 1,4-disubstituted benzene ring) showed that aniline was successfully polymerized onto the Fe_3O_4 core. In curve (c), the FT-IR spectrum of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ was similar to that of $\text{Fe}_3\text{O}_4/\text{PANI}$, but it can be seen the C=C, C–N, C–H stretching vibrations take place blue shift, which exhibited CuCl_2 was fastened on the supporter.²⁷

Fig. 3 shows the XRD patterns of the samples. The diffraction peaks marked in Fig. 3a can be indexed to (111), (220), (311), (400), (422), (511), (440), and (533) planes of face-centered cubic Fe_3O_4 . For the XRD spectrum of the $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres (Fig. 3b), the main peaks are similar to the pristine Fe_3O_4 microspheres (Fig. 3a), which reveals that the crystalline phase of Fe_3O_4 is well-maintained after the coating process under acidic conditions. Compared with that for bare Fe_3O_4 (Fig. 3a), the slight decrease in peak intensity for the $\text{Fe}_3\text{O}_4/\text{PANI}$ is due to

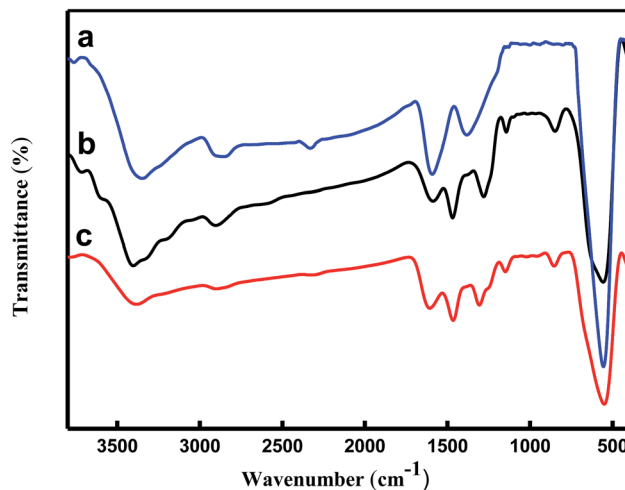


Fig. 2 FT-IR spectra of (a) Fe_3O_4 (b) $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres and, (c) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres.

the amorphous polymer coating. The main peaks of the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres were similar to $\text{Fe}_3\text{O}_4/\text{PANI}$, which revealed that immobilizing CuCl_2 on the surface of $\text{Fe}_3\text{O}_4/\text{PANI}$ did not affect the structure of $\text{Fe}_3\text{O}_4/\text{PANI}$.

The copper content in $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres was determined by means of ICP-AES and amounted to 4.2 wt%. The X-ray photoelectron spectroscopy (XPS) elemental survey scans of the surface of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres are shown in Fig. 4. Peaks corresponding to oxygen, carbon, nitrogen, copper and iron were clearly observed (Fig. 4a). To determine the oxidation state of Cu, the XPS experiments were carried out and results are reported in Fig. 4b. As it can be observed, in Fig. 3b the Cu binding energy of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ exhibited two strong peaks located at 932.8 and 952.5 eV , which were assigned to $\text{Cu } 3d_{3/2}$ and $\text{Cu } 3d_{5/2}$, respectively. These values suggests that the oxidation state of copper in the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres is +2.²⁸

Fig. 5 illustrates the results of the thermogravimetric analysis of the $\text{Fe}_3\text{O}_4/\text{PANI}$ composite, for which the thermal degradation of the PANI occurs at 450°C .²⁹ The initial mass loss at lower temperatures is mainly due to the release of water and solvent molecules in the polymer matrix. The major weight loss is observed at 290°C and continues to 630°C , possibly due to a large scale thermal degradation of the PANI chains. From the

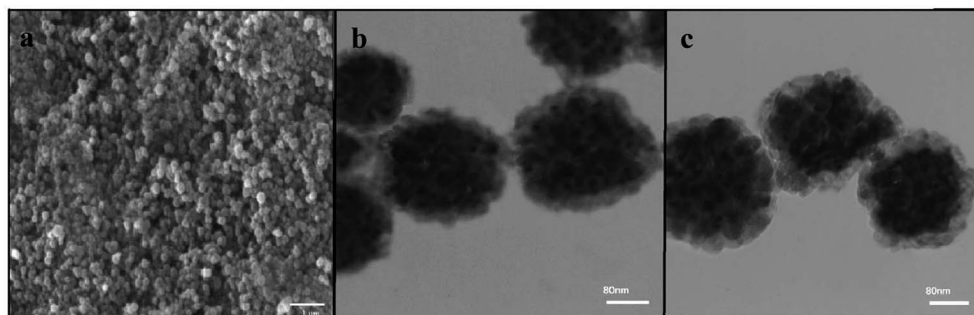


Fig. 1 (a) SEM images of Fe_3O_4 microspheres; (b) TEM images of $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres; (c) TEM images of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres.



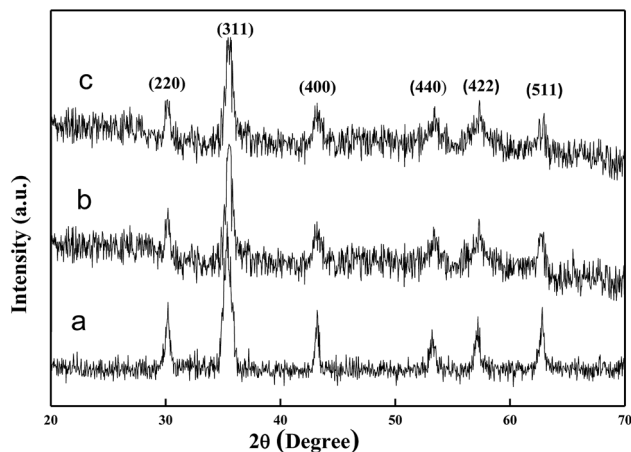


Fig. 3 XRD patterns of (a) Fe_3O_4 microspheres; (b) $\text{Fe}_3\text{O}_4/\text{PANI}$ microspheres and (c) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$.

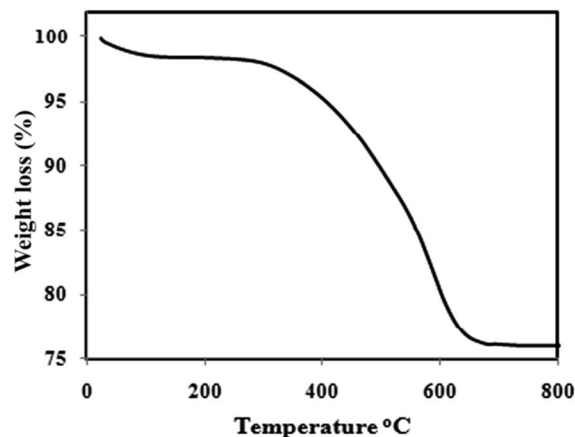


Fig. 5 Thermogravimetric analysis curve of the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres.

TG analysis, the mass ratio of the PANI in the magnetic core/shell composite is about 21%.

3.2. Characterization of the modified electrode

Surface morphologies of CPE, CILE and $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ were investigated by SEM, respectively (Fig. 6). The surface of the CPE (Fig. 6a) showed a homogeneous surface and the SEM image of CILE (Fig. 6b) shown an smooth surface appeared without separated carbon layer, which was due to the embedment of ionic liquids EMIMPF₆ between the layer of carbon and disperse the carbon powder homogeneously. When $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres were introduced into the paste (Fig. 6c), the uniformity of the surface was remained almost unchanged while the surface roughness seemed to be increased by appearing uniform layer of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres on the surface which fairly distributed in paste.

Electrochemical impedance spectroscopy (EIS) is an efficient analytical method to monitor the modification procedure of the electrode surface. The semicircle diameter of the Nyquist plots at high frequency is corresponding to the charge-transfer limited process and can be used to describe the interface properties of the electrode. The Nyquist plots of different electrodes including bare

CPE, CILE, $\text{Fe}_3\text{O}_4/\text{CILE}$, $\text{Fe}_3\text{O}_4/\text{PANI}/\text{CILE}$, and $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ in 1.0 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ solution containing 0.1 M KCl are given in Fig. 7. The smaller semicircle portion at higher frequencies of CILE than the bare CPE indicates that ionic liquids can improve the electron transfer rate. The reason might be attributed to the excellent electrical conductivity of ionic liquids EMIMPF₆. $\text{Fe}_3\text{O}_4/\text{CILE}$ shows a small semicircle at the high frequency region when compared with the CILE, this can be attributed to the presented Fe_3O_4 with good conductivity and large surface area in the modified electrode, which could effectively increase the rate electron transfer between electrode surface and $[\text{Fe}(\text{CN})_6]^{3-/4-}$ and decrease interface electron transfer resistance. After modifying of the Fe_3O_4 microsphere with PANI, the semicircle portion at higher frequencies decreased visibly. It is due to good electrical conductivity of the PANI polymer. Finally, the semicircle portion at higher frequencies of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ smaller than the $\text{Fe}_3\text{O}_4/\text{PANI}/\text{CILE}$ which may be due to presence of copper ions in $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$. It can facilitate the electron transfer.

3.3. Determination of surface area

The active surface area of the modified electrode was estimated, using the $[\text{Fe}(\text{CN})_6]^{3-/4-}$ redox system and applying the

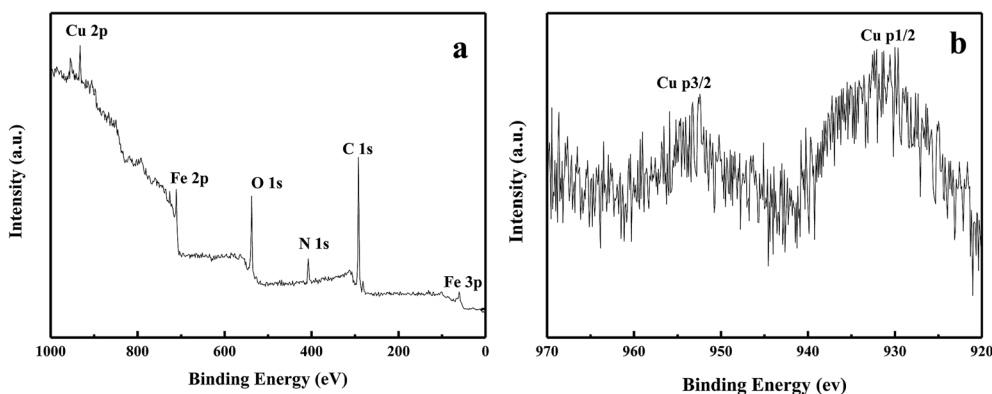


Fig. 4 XPS spectra of (a) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres; (b) Cu 2p of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ microspheres.



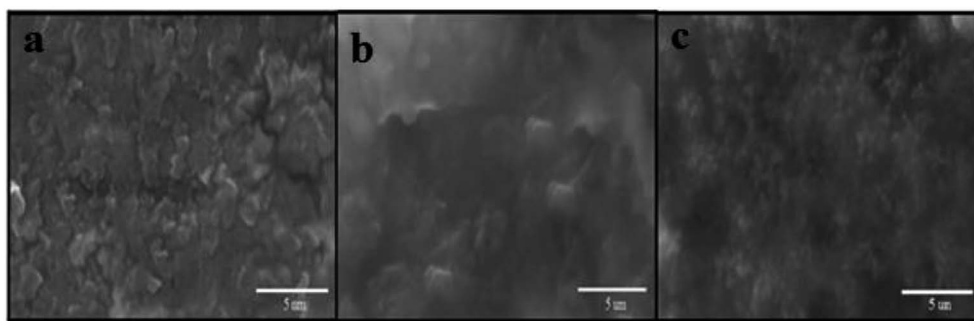


Fig. 6 SEM images of: (a) CPE, (b), CILE and (c) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$.

Randles–Sevcik equation for a reversible process.³⁰ For a typical reversible process, the following formula can be employed:

$$I_p = (2.69 \times 10^5) A n^{3/2} D^{1/2} C_0 \nu^{1/2}$$

where I_p is the peak current, D is diffusion coefficient ($7.6 \times 10^{-6} \text{ cm}^2 \text{ s}^{-1}$), ν is scan rate (V s^{-1}) and C_0 is the concentration of $\text{K}_4[\text{Fe}(\text{CN})_6]$ in mol L^{-1} . n is the number of electron transferred ($n = 1$), ν is the scan rate and A is the effective surface area. Cyclic voltammetry experiments at different scan rates were carried out with the bare and modified sensors immersed in a solution of 1 mM $\text{K}_4[\text{Fe}(\text{CN})_6]$ in 0.1 M KCl. The surface area could be calculated from the slope of I_p versus $\nu^{1/2}$ plot, which were found as 0.08 cm^2 , and 0.4045 cm^2 for bare CILE and $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$, respectively. The results show that the presence of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ makes the active surface of the electrode increases.

3.4. Electrochemical behavior of DXM at $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$

The electrochemical study of different modified electrodes was performed in 0.1 M KH_2PO_4 electrolyte containing a 100 μM DXM solution with a cyclic voltammetry technique, and the results are shown in Fig. 8. Due to slow electron transfer, DXM

did not show any significant peaks at bare CPE (curve a), while the responses at the CILE were stronger (curves b), compared with the CPE and CILE, the enhancement in peaks current at the surface of CILE/ Fe_3O_4 (curves c), this is confirms the synergetic effect of the Fe_3O_4 microspheres on the electro-oxidation of DXM. The significant increase in peaks current and shift in peaks potential at the surface of $\text{Fe}_3\text{O}_4/\text{PANI}/\text{CILE}$ in comparison with those obtained CILE/ Fe_3O_4 , CILE and CPE is due to the presence of PANI which possesses good electrical conductivity. It also must be noted that the enhancement in the peak currents at the surface of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ in comparison with other electrodes is due to the presence of copper ions in the composition of the modified electrode. The complex formation between electrode surface copper ions and DXM increases the accumulated drug and an enhancement in the peak current and sensitivity of the proposed electrode towards DXM is resulted.

3.5. Optimization of the amount of modifier in the electrode

The effect of the amount of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ on the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ performance toward electrooxidation of DXM was examined by DPV. It was observed that the sensitivity of the sensor first rapidly increases with increasing the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}$ nanoparticles content in the paste up to about 15% and

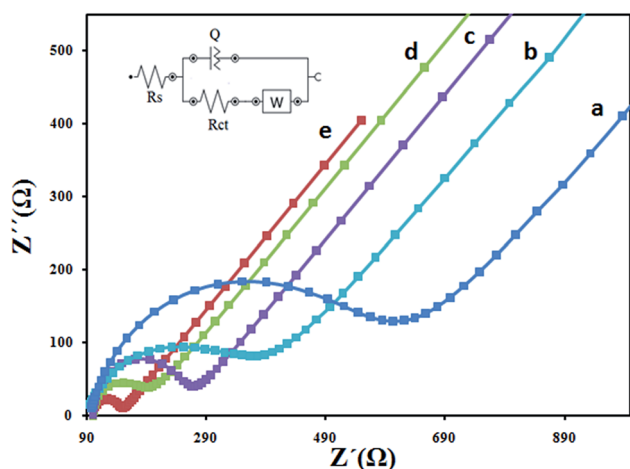


Fig. 7 EIS for (a) CPE, (b) CILE (c) $\text{Fe}_3\text{O}_4/\text{CILE}$ (d) $\text{Fe}_3\text{O}_4/\text{PANI}/\text{CILE}$ and (e) $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ in 1 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ with 0.1 M KCl.

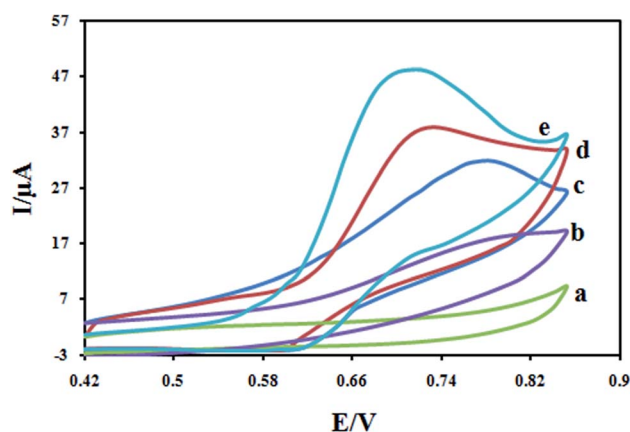


Fig. 8 Cyclic voltammograms for 100 μM DXM at scan rate 100 mV s^{-1} at CPE (a); CILE (b); $\text{Fe}_3\text{O}_4/\text{CILE}$ (c); $\text{Fe}_3\text{O}_4/\text{PANI}/\text{CILE}$ (d) and $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ (e) in 0.1 M KH_2PO_4 electrolyte.



then started to level off and even slowly decreases with the higher loadings. Initially, the maximum peak current was obtained when the amounts of the graphite powder, paraffin oil, ion liquid EMIMPF₆ and Fe₃O₄/PANI–Cu^{II} in the paste were 60 : 10 : 15 : 15% (w/w).

3.6. Investigation of the scan rate

Effect of the scan rate on the cyclic voltammograms of 100 μ M DXM at different scan rates were shown in Fig. 9a. The results showed that the peak currents vary linearly with the square root of the scan rate ($\nu^{1/2}$) (Fig. 9b), which indicates a diffusion-controlled process for DXM oxidation on the surface of the modified electrode in the studied range of potential sweep rates, with following equations: $I_{pa} = 144.51\nu^{1/2} + 3.7233$ ($R^2 = 0.9947$). The dependence of the peak potential and the logarithmic scan rate ($\ln \nu$) showed a linear relationship with a regression equation of $E_{pa}(\text{V}) = 0.0238 \ln \nu (\text{V s}^{-1}) + 0.7443$ ($R^2 = 0.9941$) (Fig. 9c). For an irreversible electrode process, according to Laviron equation,³¹ E_{pa} is defined by the following equation:

$$E_p = E_0 + RT/(1 - \alpha)nF \ln((1 - \alpha)nF/RTk_s) + (RT/(1 - \alpha)nF) \ln \nu$$

where α is the transfer coefficient, k_0 is the standard rate constant of the reaction; n is the electron transfer number; ν is the scanning rate; E_0 is the formal potential. Other symbols have their usual meanings. According to above equation, the value of $(1 - \alpha)n$ can be easily calculated from the slope. In our system, the slope is 0.0238, taking $T = 298.15 \text{ K}$, $F = 96485 \text{ C mol}^{-1}$ and $R = 8.314 \text{ J mol}^{-1} \text{ K}^{-1}$, the $(1 - \alpha)n$ was calculated to be 1.07. According to Bard and Faulkner,³² α can be calculated using the following equation: α can be given as: $\alpha = 47.7/(E_p - E_{p/2}) \text{ mV}$ where $E_{p/2}$ is the potential where the current is at half the peak value. Thus,

from this, the transfer coefficient (α) and the electron transfer number (n) are calculated to be 0.54 and $1.92 \approx 2$, respectively. Also, if the value of E_0 is known, the k_s value can be determined from the intercept of the straight line of E_p vs. $\ln \nu$. The E_0 value can be deduced from the intercept of E_p vs. ν plot by extrapolating the line to the vertical axis at $\nu = 0$, when ν was approached to zero, then E_p was approached to E_0 .³³ Thus, using this information and Laviron equation the k_s values obtained was 2.90 s^{-1} .

3.7. Effect of pH

The effect of pH of the buffer solution on the electrochemical behavior of DXM was studied by cyclic voltammetry using 0.1 M KH₂PO₄ electrolyte in the pH range of 1.0–9.0 (Fig. 10a). The pH of the KH₂PO₄ electrolyte solution was regulated by small amounts of NaOH and HCl solutions. As it can be seen, no voltammetric peak of DXM was observed at pH 5 and higher. On the other hand, the anodic peak current in the range of 1.0 to 5.0 increased with the decrease of pH, when the pH was less than 2.0, the oxidation current did not increase. Therefore, pH 2.0 was selected in the assay. In addition, the oxidation peak potential shifts negatively with increase in pH, suggesting that protons participate in the electrode reaction process. The relationship between the peak potential (E_{pa}) and pH is expressed as: $E_{pa}(\text{V}) = 0.0521\text{pH} + 0.7953$ ($R^2 = 0.9963$) (Fig. 10b). The absolute value of the slope (0.0521 V pH^{-1}) is close to the theoretical Nernstian value of 0.0586 V pH^{-1} , indicating that electron transfer was accompanied by an equal number of protons in electrode reaction of DXM.³⁴

3.8. Calibration curve and detection limit

The differential pulse voltammetry was used for the determination of DXM because of its higher sensitivity and selectivity than CV. Under the optimal experimental conditions, the oxidation

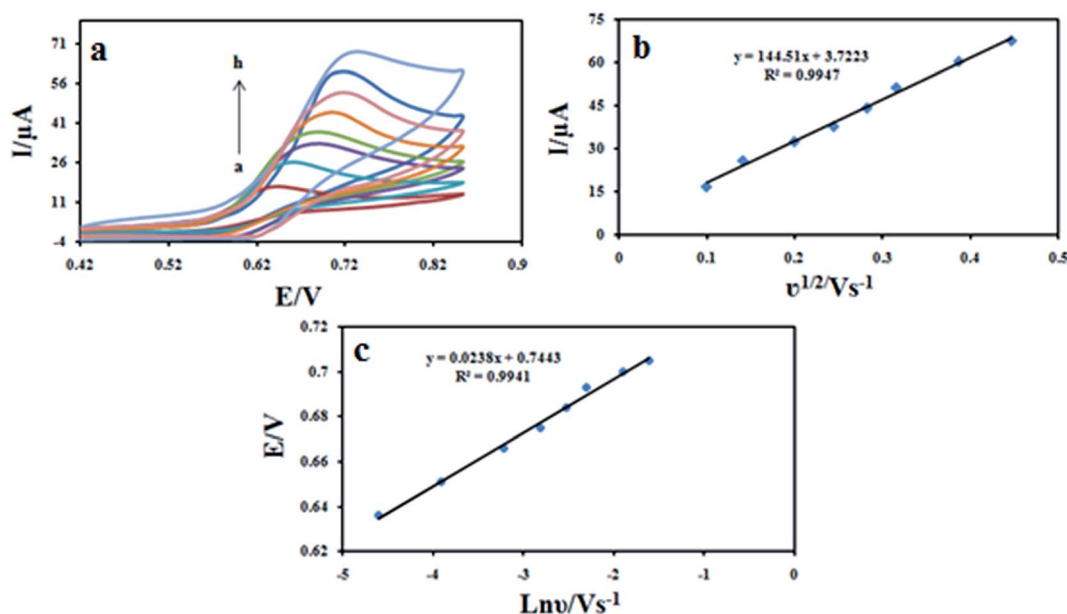


Fig. 9 (a) Cyclic voltammograms of 100 μ M DXM at Fe₃O₄/PANI–Cu^{II}/CILE in 0.1 M KH₂PO₄ electrolyte at different scan rates. The numbers of 1–8 correspond to 10, 20, 40, 60, 80, 100, 150 and 200 mV s⁻¹, respectively. (b) Variation of the peak current with square root of scan rate ($\nu^{1/2}$); (c) variation of the peak potential and the logarithmic scan rate.



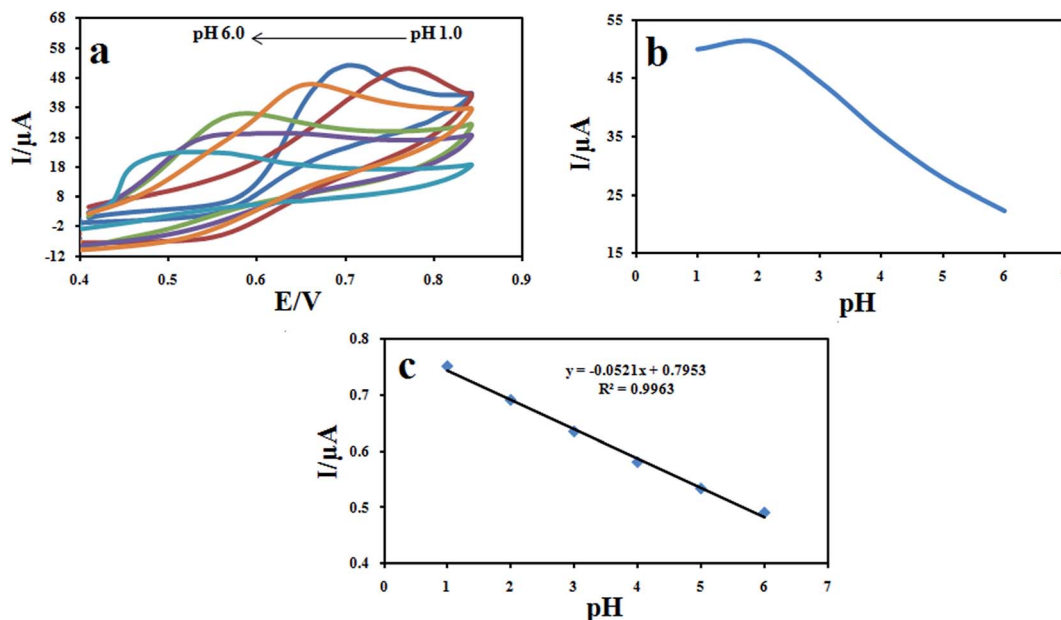


Fig. 10 Cyclic voltammograms of 100 μM DXM recorded (a) from pH 1.0 to 6.0 at a scan rate of 100 mV s^{-1} (b) effect of pH of DXM solutions on the peak current (b) and (c) peak potential.

peak current of DXM was proportional to its concentration in the range from 0.05 to $30.0 \mu\text{M}$ (Fig. 11). The linear regression equation can be expressed as $I_{\text{pa}} (\mu\text{A}) = 0.5377 + 1.5957 (\text{mA})$ ($R^2 = 0.9931$). Based on the relation 3 (S/N), the detection limit was 3.0 nM . Compared with other electrochemical sensors (Table 1), the proposed methods in our work gave higher sensitivities with wider linear ranges for DXM detection.

3.9. Chronoamperometric measurements

The chronoamperometry as well as other electrochemical methods was employed for the investigation of electrode

reaction at chemically modified electrodes. Chronoamperometric measurements of DXM at $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ were done (Fig. 12) for various concentrations of DXM. For an electroactive material (DXM in this case) with a diffusion coefficient of D , the current for the electrochemical reaction at a mass transport limited rate is described by the Cottrell equation:

$$I = nFAD^{1/2}C_b\pi^{-1/2}t^{-1/2}$$

Under diffusion control, a plot of I versus $t^{-1/2}$ will be linear, and from the slope the value of D can be obtained. The mean value of the D was found to be $5.15 \times 10^{-4} \text{ cm}^2 \text{ s}^{-1}$.

3.10. Interference, stability and reproducibility

In order to evaluate the ability of anti-interference, some ordinary compounds in biological media and drugs were selected. No significant interference was found for the detection of $50 \mu\text{M}$ DXM from the following compounds: NaCl, KCl, KNO_3 , tryptophan, cysteine, uric acid, ascorbic acid, hydrocortisone, and phenazopyridine. The stability of the sensor was also investigated by examining its response current after storage period of

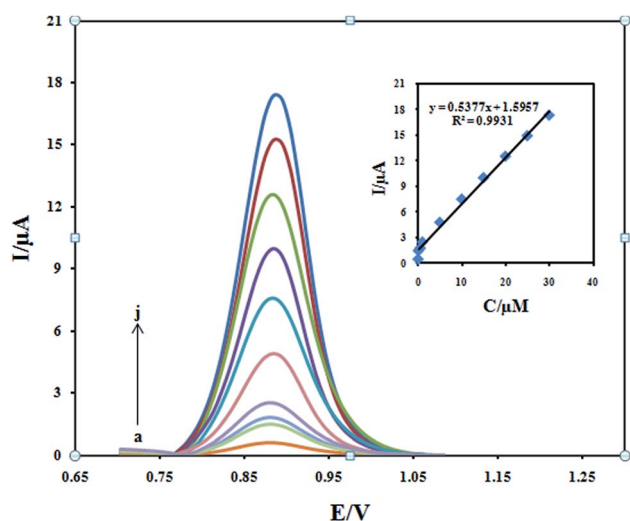


Fig. 11 Differential pulse voltammograms of $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ in $0.1 \text{ M KH}_2\text{PO}_4$ electrolyte containing different concentrations of DXM in the ranges $0.05\text{--}30 \mu\text{M}$. Inset: plot of the peak current against concentration of DXM.

Table 1 A comparison of analysis parameters of DXM with recently reported reference

Electrode	Linear range (μM)	LOD (μM)	Reference
HMDE	25.5–122.3	7.6	35
CDMCPCE	0.41–20	0.36	13
HMDE	0.61–4.98	0.002	14
PGE	0.05–100	0.055	3
MWNT	0.15–100	0.09	12
$\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$	0.05–30	0.003	This work



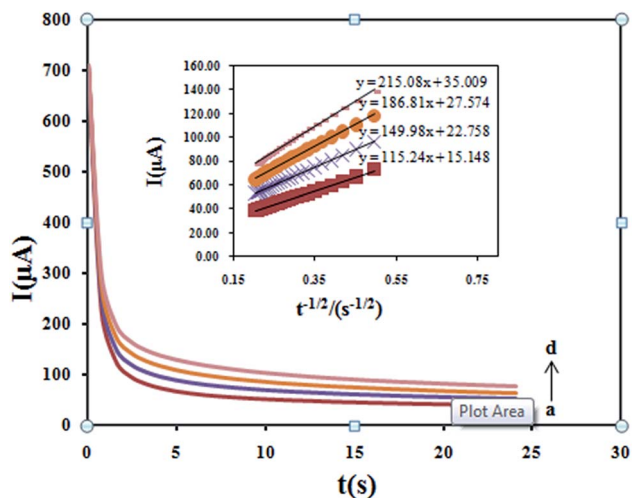


Fig. 12 Chronoamperograms obtained at the $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ in the presence of 100, 150, 200 and 250 μM DXM in the 0.1 M KH_2PO_4 electrolyte. (Inset) Cottrell's plot for the data from the chronoamperograms.

Table 2 Determination of DXM in body fluids using the proposed method

	Added (μM)	Found (μM)	Recovery (%)
Blood serum samples	0	Not detected	—
	1	1.05	105
	3	3.15	105
	5	4.9	99.8
Urine	0	Not detected	—
	1	0.96	0.96
	3	3.03	101
	5	5.25	105

30 days the current of DXM reduced 4.9%, indicating the excellent stability, after a storage period of 30 days. The reproducibility of the proposed sensor was tested using five different electrodes. The relative standard deviations (RSD) of the DPV response currents for these species were less than 6.8%. Thus, the modified electrode showed a high stability and excellent reproducibility and anti-interference ability.

3.11. Real sample analysis

The applicability of the proposed method was examined to determine DXM in the pharmaceutical samples using the calibration curve method. The sample treatment processes were described in the Experimental section. The obtained results are summarized in Table 2. As it is obvious, the recovery of DXM was found to be between 97.0–102.0% using DPV method, which confirm good sensitivity of the proposed procedure. This means that the proposed procedure should be applicable to the analysis of real samples with different matrices.

The R.S.D. value for determination was less than 3.7% for $n = 3$.

4. Conclusions

In the present study an efficient and sensitive catalytic system based on a $\text{Fe}_3\text{O}_4/\text{PANI}-\text{Cu}^{\text{II}}/\text{CILE}$ was introduced for nanomolar detection of DXM using DPV method. The results showed good stability as well as high electrocatalytic activity toward DXM. In comparison to other reported electrodes the proposed sensor has an acceptable limit of detection and linear range and can be used for monitoring of the drug in real samples with different matrices. In addition to its low detection limit, wide linear range, low cost, reasonable reproducibility and stability are the other advantages of this sensor.

References

- 1 R. B. Friedrich, A. Ravello, L. C. Cichota, C. M. B. Rolim and R. C. R. Beck, Validation of a simple and rapid UV spectrophotometric method for dexamethasone assay in tablets, *Quim. Nova*, 2009, **32**(4), 1052–1054.
- 2 M. M. Vdovenko, A. V. Gribas, A. V. Vylegzhanina and I. Y. Sakharov, Development of a chemiluminescent enzyme immunoassay for the determination of dexamethasone in milk, *Anal. Methods*, 2012, **4**(8), 2550–2554.
- 3 R. N. Goyal, V. K. Gupta and S. Chatterjee, Fullerene- C_{60} -modified edge plane pyrolytic graphite electrode for the determination of dexamethasone in pharmaceutical formulations and human biological fluids, *Biosens. Bioelectron.*, 2009, **24**(6), 1649–1654.
- 4 K. Wasch, H. Brabander, D. Courtheyn and C. V. Peteghem, Detection of corticosteroids in injection sites and cocktails by MSⁿ, *Analyst*, 1998, **123**, 2415–2422.
- 5 H. Shibasaki, T. Furuta and Y. Kasuya, Quantification of corticosteroids in human plasma by liquid chromatography-thermospray mass spectrometry using stable isotope dilution, *J. Chromatogr. B: Biomed. Sci. Appl.*, 1997, **692**(1), 7–14.
- 6 C. S. Creaser, S. J. Feely, E. Houghton and M. Seymour, Immunoaffinity chromatography combined on-line with high-performance liquid chromatography-mass spectrometry for the determination of corticosteroids, *J. Chromatogr. A*, 1998, **794**(1), 37–43.
- 7 M. Cherlet, S. De Baere and P. De Backer, Quantitative determination of dexamethasone in bovine milk by liquid chromatography-atmospheric pressure chemical ionization-tandem mass spectrometry, *J. Chromatogr. B: Anal. Technol. Biomed. Life Sci.*, 2004, **805**(1), 57–65.
- 8 O. H. Hidalgo, M. J. Lopez, E. A. Carazo, M. S. A. Larrea and T. B. Reuvers, Determination of dexamethasone in urine by gas chromatography with negative chemical ionization mass spectrometry, *J. Chromatogr. B: Anal. Technol. Biomed. Life Sci.*, 2003, **788**(1), 137–146.
- 9 Y. Iglesias, C. Fente, S. Mayo, B. Vazquez, C. Franco and A. Cepeda, Chemiluminescence detection of nine corticosteroids in liver, *Analyst*, 2000, **125**(11), 2071–2074.
- 10 Y. Iglesias, C. Fente, B. Vazquez, C. Franco, A. Cepeda and S. Mayo, Application of the luminol chemiluminescence



- reaction for the determination of nine corticosteroids, *Anal. Chim. Acta*, 2002, **468**(1), 43–52.
- 11 O. Huetos, M. Ramos, M. M. de Pozuelo, T. B. Reuvers and M. San Andrés, Determination of dexamethasone in feed by TLC and HPLC, *Analyst*, 1999, **124**(11), 1583–1587.
 - 12 B. Rezaei, S. Zare and A. A. Ensafi, Square wave voltammetric determination of Dexamethasone on a multiwalled carbon nanotube modified pencil electrode, *J. Braz. Chem. Soc.*, 2011, **22**(5), 897–904.
 - 13 K. Balaji, G. R. Reddy, T. M. Reddy and S. J. Reddy, Determination of prednisolone, dexamethasone and hydrocortisone in pharmaceutical formulations and biological fluid samples by voltammetric techniques using b-cyclodextrin modified carbon paste electrode, *Afr. J. Pharm. Pharmacol.*, 2008, **2**(8), 157–166.
 - 14 T. M. B. Oliveira, F. W. P. Ribeiro, J. E. Soares, P. de Lima-Neto and A. N. Correia, Square-wave adsorptive voltammetry of dexamethasone: redox mechanism, kinetic properties, and electroanalytical determinations in multicomponent formulations, *Anal. Biochem.*, 2011, **413**(2), 148–156.
 - 15 A. Safavi, N. Maleki, O. Moradlou and F. Tajabadi, Simultaneous determination of dopamine, ascorbic acid, and uric acid using carbon ionic liquid electrode, *Anal. Biochem.*, 2006, **359**(2), 224–229.
 - 16 A. Safavi, N. Maleki, E. Farjami and F. A. Mahyari, Simultaneous electrochemical determination of glutathione and glutathione disulfide at a nanoscale copper hydroxide composite carbon ionic liquid electrode, *Anal. Chem.*, 2009, **81**(18), 7538–7543.
 - 17 M. Opallo and A. Lesniewski, A review on electrodes modified with ionic liquids, *J. Electroanal. Chem.*, 2011, **656**(1), 2–16.
 - 18 L. Ding and B. Su, A non-enzymatic hydrogen peroxide sensor based on platinum nanoparticle–polyaniline nanocomposites hosted in mesoporous silica film, *J. Electroanal. Chem.*, 2015, **736**, 83–87.
 - 19 A. K. Das, S. Maiti and B. Khatua, High performance electrode material prepared through *in situ* polymerization of aniline in the presence of zinc acetate and graphene nanoplatelets for supercapacitor application, *J. Electroanal. Chem.*, 2015, **739**, 10–19.
 - 20 B. H. Nguyen, L. Dai Tran, Q. P. Do, H. Le Nguyen, N. H. Tran and P. X. Nguyen, Label-free detection of aflatoxin M1 with electrochemical Fe₃O₄/polyaniline-based aptasensor, *Mater. Sci. Eng., C*, 2013, **33**(4), 2229–2234.
 - 21 J. Jiang, H. Gu, H. Shao, E. Devlin, G. C. Papaefthymiou and J. Y. Ying, Bifunctional Fe₃O₄–Ag Heterodimer Nanoparticles for Two-Photon Fluorescence Imaging and Magnetic Manipulation, *Adv. Mater.*, 2008, **20**(23), 4403–4407.
 - 22 F.-h. Lin, W. Chen, Y.-H. Liao, R.-a. Doong and Y. Li, Effective approach for the synthesis of monodisperse magnetic nanocrystals and M–Fe₃O₄ (M = Ag, Au, Pt, Pd) heterostructures, *Nano Res.*, 2011, **4**(12), 1223–1232.
 - 23 C.-M. Yu, J.-W. Guo and H.-Y. Gu, Direct electrochemical behavior of hemoglobin at surface of Au@Fe₃O₄ magnetic nanoparticles, *Microchim. Acta*, 2009, **166**(3–4), 215–220.
 - 24 L. Pan, Y. Chen and F. Wang, Synthesis of nanostructured M/Fe₃O₄ (M = Ag, Cu) composites using hexamethylenetetramine and their electrocatalytic properties, *Mater. Chem. Phys.*, 2012, **134**(1), 177–182.
 - 25 Q. Xiong, J. Tu, Y. Lu, J. Chen, Y. Yu, Y. Qiao, *et al.*, Synthesis of hierarchical hollow-structured single-crystalline magnetite (Fe₃O₄) microspheres: the highly powerful storage *versus* lithium as an anode for lithium ion batteries, *J. Phys. Chem. C*, 2012, **116**(10), 6495–6502.
 - 26 A. Mehdinia, F. Roohi and A. Jabbari, Rapid magnetic solid phase extraction with *in situ* derivatization of methylmercury in seawater by Fe₃O₄/polyaniline nanoparticle, *J. Chromatogr. A*, 2011, **1218**(28), 4269–4274.
 - 27 Y. Lu, Y. Yin, B. T. Mayers and Y. Xia, Modifying the surface properties of superparamagnetic iron oxide nanoparticles through a sol–gel approach, *Nano Lett.*, 2002, **2**(3), 183–186.
 - 28 U. G. Singh, R. T. Williams, K. R. Hallam and G. C. Allen, Exploring the distribution of copper–Schiff base complex covalently anchored onto the surface of mesoporous MCM 41 silica, *J. Solid State Chem.*, 2005, **178**(11), 3405–3413.
 - 29 S. Xuan, Y.-X. J. Wang, K. C.-F. Leung and K. Shu, Synthesis of Fe₃O₄@polyaniline core/shell microspheres with well-defined blackberry-like morphology, *J. Phys. Chem. C*, 2008, **112**(48), 18804–18809.
 - 30 N. Yang, Q. Wan and J. Yu, Adsorptive voltammetry of Hg(II) ions at a glassy carbon electrode coated with electropolymerized methyl-red film, *Sens. Actuators, B*, 2005, **110**(2), 246–251.
 - 31 J. Abbar and S. Nandibewoor, Voltammetric Behavior of Chlorzoxazone and Its Electroanalytical Determination in Pharmaceutical Dosage Form and Urine at Gold Electrode, *Crit. Rev. Anal. Chem.*, 2012, **42**(3), 272–281.
 - 32 A. J. Bard, L. R. Faulkner, J. Leddy and C. G. Zoski, *Electrochemical methods: fundamentals and applications*, Wiley, New York, 1980.
 - 33 Y. Wu, X. Ji and S. Hu, Studies on electrochemical oxidation of azithromycin and its interaction with bovine serum albumin, *Bioelectrochemistry*, 2004, **64**(1), 91–97.
 - 34 T. Łuczak, Preparation and characterization of the dopamine film electrochemically deposited on a gold template and its applications for dopamine sensing in aqueous solution, *Electrochim. Acta*, 2008, **53**(19), 5725–5731.
 - 35 C. Jeyaseelan and A. Joshi, Trace determination of dexamethasone sodium phosphate in pharmaceutical formulations by differential pulse polarography, *Anal. Bioanal. Chem.*, 2002, **373**, 772–776.

