RSC Advances



PAPER

View Article Online
View Journal | View Issue



Cite this: RSC Adv., 2017, 7, 1418

One-step immobilization of antibodies on ZIF-8/ Fe_3O_4 hybrid nanoparticles for the immunoassay of Staphylococcus aureus

Changyong Yim,† Hyeonjeong Lee,† Sanghee Lee and Sangmin Jeon*

Zeolitic imidazolate framework-8 (ZIF-8)-coated Fe_3O_4 magnetic nanoparticle clusters (MNCs) were synthesized and used to detect pathogenic bacteria in milk. Hydrothermally synthesized MNCs were encapsulated with ZIF-8 *via* sonochemical reactions. Half fragments of monoclonal *Staphylococcus* antibodies were conjugated to the low-coordinated Zn sites located on the outer layer of ZIF-8 *via* Zn-S bonding, which allows one-step immobilization of antibodies with favorable orientations on ZIF-8. Furthermore, ZIF-8 encapsulation improved the stability of MNCs in water by suppressing the Fe_3O_4 oxidation. After the capture and magnetic separation of *Staphylococcus* in milk using hybrid nanoparticles, bacteria concentration was determined with a portable ATP luminometer and the detection limit was found to be 300 cfu mL⁻¹.

Received 20th October 2016 Accepted 23rd November 2016

DOI: 10.1039/c6ra25527b

www.rsc.org/advances

Introduction

 ${\rm Fe_3O_4}$ magnetic nanoparticles have recently attracted considerable attention in bio-applications owing to their inherent superparamagnetic properties and biocompatibility. The functionalization of antibodies on the ${\rm Fe_3O_4}$ nanoparticles enables the selective capture and magnetic separation of target molecules such as DNA, biomarker proteins, for and pathogens from complex sample solutions. The efficiency of magnetic separation increases with the size of the ${\rm Fe_3O_4}$ particles. However, clusters of small ${\rm Fe_3O_4}$ nanoparticles are preferred to large individual nanoparticles for immunomagnetic assays because ${\rm Fe_3O_4}$ assumes ferromagnetic properties at sizes larger than 30 nm.

Despite the several advantages of Fe₃O₄ magnetic nanoparticles for bioapplications, their use is hindered by the fact that Fe₃O₄ undergoes oxidation in water, which affects the magnetic properties and appearance of the nanoparticles. To prevent the oxidation of Fe₃O₄, iron oxide particles are encapsulated with protective layers such as silicon dioxide (SiO₂).⁹⁻¹¹ However, encapsulation with silica requires the careful control of reaction conditions for avoiding particle aggregation and decreases the saturation magnetization value of the encapsulated magnetic particles due to the high density of SiO₂ (2.195 g cm⁻³).¹² Furthermore, the antibodies immobilized on silicacoated magnetic nanoparticles *via* silane chemistry generally

Department of Chemical Engineering, Pohang University of Science and Technology (POSTECH), Pohang, Gyeongbuk 37673, Republic of Korea. E-mail: jeons@postech. ac.kr

possesses random orientations, which degrades the binding efficiency of the antibodies to target molecules.¹³

To overcome these drawbacks of silica encapsulation, we coated magnetic nanoparticle clusters (MNCs) with metalorganic frameworks (MOFs). Owing to their large surface areas, exceptional chemical and thermal stabilities, and negligible cytotoxicity, MOFs have been widely applied in drug delivery, ¹⁴ biomineralization, ¹⁵ and biomolecule purification. ⁵ Among the various MOFs, zeolitic imidazolate framework-8 (ZIF-8) was used in this study because it can be synthesized within 10 min without inducing nanoparticle aggregation and is chemically and thermally stable. ¹⁶ In addition, the low density of ZIF-8 (0.35 g cm⁻³) does not significantly decrease the saturation magnetization value of the hybrid MNCs. Furthermore, the low-coordinated Zn sites located on the outer shell of ZIF-8 could form Zn–S bonds, ¹⁷⁻¹⁹ which allows conjugation with thiolated antibodies and offers an attractive functionalization route for ZIF

In this study, we synthesized ZIF-8-coated hybrid magnetic nanoparticle clusters (ZIF-8/MNCs) and functionalized them with half fragments of monoclonal *Staphylococcus aureus* (*S. aureus*) antibodies *via* Zn–S bonding, which enabled onestep immobilization of antibodies with favorable orientations. *S. aureus* is enterotoxigenic bacteria found in various foods such as milk and cheese. Milk was selected as a real food matrix to confirm that ZIF-8/MNCs can detect *S. aureus* in the presence of various interferents. After the capture and magnetic separation of *S. aureus* in milk using the hybrid nanoparticles, the concentration of bacteria was determined with a portable ATP luminometer. The detection limit of the assay was found to be 300 cfu mL⁻¹. In addition, it was found that the ZIF coating improved the stability of MNCs in water by

[†] These authors contributed equally.

suppressing $\mathrm{Fe_3O_4}$ oxidation. To the best of our knowledge, this study reports the first approach for the direct functionalization of antibodies on ZIF-8/MNCs and their applications in immunomagnetic assays.

Experimental

Materials

Iron(III) chloride hexahydrate (FeCl₃·6H₂O), sodium citrate, urea, polyacrylamide (PAM; $M_{\rm w}=5\,000\,000$ –6 000 000 g mol⁻¹), zinc nitrate hexahydrate (Zn(NO₃)₂·6H₂O), 2-methylimidazole (2-MIM), potassium dihydrogen phosphate (H₂KPO₄), potassium phosphate dibasic (HK₂PO₄), tris(2-carboxyethyl)-phosphine (TCEP), Tween 20, lysogeny broth (LB) and methanol were purchased from Sigma-Aldrich (St. Louis, MO) and used without further purification. A monoclonal *S. aureus* antibody was purchased from Abcam (Cambridge, UK), and casein hydrolysate was purchased from MP Biomedicals (Santa Ana, CA, USA). Deionized (DI) water (18.3 MΩ cm) was obtained from a reverse osmosis water system (Human Science, Korea). H₂KPO₄ (0.272 g) and HK₂PO₄ (1.714 g) were dissolved in 1 L of DI water to prepare a phosphate buffer (PB) with pH = 7.4.

Synthesis of Fe₃O₄ magnetic nanoparticle clusters (MNCs)

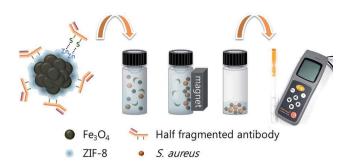
 ${
m Fe_3O_4}$ was synthesized using a one-pot hydrothermal method described elsewhere. Priefly, 2.16 g of ${
m FeCl_3\cdot 6H_2O}$, 4.7 g of sodium citrate, and 1.44 g of urea were dissolved in 30 mL of DI water and 30 mL of 0.02 g mL $^{-1}$ PAM solution in DI water was then added to the solution. The mixture was transferred to a 100 mL Teflon-lined stainless-steel autoclave and maintained at 200 °C in an oven for 12 h. After the autoclave was cooled to room temperature (RT), the black precipitate was collected using a permanent magnet and washed several times with DI water and ethanol. The resulting MNCs were dried in an oven at 90 °C for 12 h under reduced pressure.

Synthesis and oxidation stability test of ZIF-8-coated hybrid MNCs (ZIF-8/MNCs)

The ZIF encapsulation reaction was conducted under sonication at 60 °C for 10 min by adding 0.1 g of Fe $_3$ O $_4$ MNCs to a 30 mL methanol solution containing 0.238 g of Zn(NO $_3$) $_2 \cdot 6H_2$ O, 0.657 g of 2-MIM, and 10 μ L of HCl. The hybrid ZIF-8/MNCs were then collected using a permanent magnet and washed several times with methanol. The hybrid nanoparticles were dried in a vacuum oven at 90 °C for 12 h. For the oxidation stability test of ZIF-8/MNCs, they were kept in DI water at 200 °C for 1 h and variations in light absorption were measured using a UV-Vis spectrometer (UV-1800, SHIMADZU).

Direct immobilization of half-fragmented antibody on ZIF-8/MNCs

 $10~\mu L$ of $1.4~mg~mL^{-1}$ TCEP in PB was added to $400~\mu L$ of PB containing $10~\mu g$ of monoclonal *S. aureus* antibody and incubated for 1~h at RT to reduce the disulfide bonds between the heavy and light chains of the antibody. After purification



Scheme 1 Detection of *Staphylococcus aureus* using antibodyconjugated ZIF-8/MNCs and a portable ATP luminometer.

using Amicon centrifugal 10k filters (Millipore, Ireland), the half-fragmented antibodies were added to 1.5 mg of ZIF-8/MNC in PB for 1 h at RT to immobilize *via* Zn–S bonding. This one-step antibody conjugation using the half-fragmented antibodies eliminates the use of linker molecules and results in the immobilization of the antibodies with favorable orientations. The antibody-conjugated MNCs were sequentially incubated with 0.7 wt% casein and 0.1 wt% Tween 20 to prevent nonspecific binding and rinsed several times with PB.

Detection of *Staphylococcus aureus* in milk using antibodyconjugated ZIF-8/MNC

Scheme 1 shows the experimental procedure for detecting pathogenic bacteria. Half fragments of monoclonal *S. aureus* antibody were immobilized onto ZIF-8/MNCs. A pure culture of *S. aureus* was grown in LB at 37 °C overnight, and the concentration of *S. aureus* was determined by cell counting on an agar plate. Subsequently, the culture solution was serially diluted into milk to obtain 10^2 to 10^5 cfu mL $^{-1}$. Diluted solutions (10 mL) were incubated with 0.1 mg of antibody-conjugated ZIF-8/MNCs for 1 h at RT. The bacteria were magnetically separated and dispersed in 100 μ L PB and mixed with benzalkonium chloride solutions for the lysis and ATP extraction of bacteria. Lysate solutions were sequentially added to lyophilized luciferase and luciferin powder, and the luminescence intensity from oxidized luciferin was measured by a portable luminometer (Kikkoman PD-20). 22,23

Results and discussion

Fig. 1(a) and (b) show a scanning electron microscopy (SEM) image and transmission electron microscopy (TEM) image of the MNCs, respectively. The average diameter of the MNCs was measured to be \sim 300 nm. The SEM and TEM images of the ZIF-8/MNCs are shown in Fig. 1(c) and (d), respectively. The thickness of the ZIF-8 shell was \sim 80 nm. The crystal structures of the MNCs and ZIF-8/MNCs were investigated using X-ray diffraction (XRD; Fig. 1(e)). The magnetite phase was observed in the MNCs at 18.1°, 29.7°, 35.0°, 42.5°, 52.7°, and 56.3°, which correspond to the (111), (220), (311), (400), (422), and (511) planes, respectively (indexed by JCPDC 890951). The

RSC Advances

Fig. 1 Characterization of MNCs and ZIF-8/MNCs: (a) SEM and (b) TEM images of MNCs; (c) SEM and (d) TEM images of ZIF-8/MNCs; (e) XRD patterns of MNCs (black) and ZIF-8/MNCs (red); and (f) magnetization curves of MNCs (black) and ZIF-8/MNCs (red). (g) Optical images of ZIF-8/MNCs in DI water before (left) and after (right) magnetic separation for 30 s.

5000

Applied Magnetic Field (Oe)

XRD pattern of ZIF-8 on MNCs showed peaks at 7.31° and 12.71° , which correspond to the (110) and (211) planes of ZIF-8, according to CCDC 602542. Both the TEM and XRD results of the ZIF-8/MNCs indicated that the ZIF-8 shell was successfully coated onto the MNCs. Fig. 1(f) shows that both the MNCs and ZIF-8/MNCs exhibited superparamagnetic properties with saturation magnetizations of 70 and 49 emu g⁻¹, respectively.

Because of the low density of ZIF-8, the encapsulation of the MNCs with an $\sim\!80$ nm-thick layer of ZIF-8 decreased the saturation magnetization value only by 30%. If the MNCs were covered by a layer of SiO_2 with the same thickness, the saturation magnetization would decrease by 70%. Fig. 1(g) shows that nearly complete magnetic separation was achieved within 30 s using a permanent magnet. Both the nanoparticles were well re-dispersed after the permanent magnet was removed.

To assess the degree of oxidation of Fe₃O₄ in water, MNCs and ZIF-8/MNCs were kept in DI water at 200 °C for 1 h. Fe₃O₄ is known to be oxidized to maghemite (γ-Fe₂O₃) at this moderate temperature and to hematite (α-Fe₂O₃) at higher temperatures (>500 °C).24,25 Although the saturation magnetization value of maghemite is not considerably different from that of Fe₃O₄, ^{24,25} their different appearances often mislead people to conclude that the properties have been changed. Fig. 2(a) and (b) show optical images of MNCs and ZIF-8/MNCs, respectively, before and after heat treatment. The MNC solution changed from dark brown to pale yellow brown after heat treatment, whereas negligible changes in color were observed for the ZIF-8/MNC solution. Fig. 2(c) shows variations in the light absorption spectra of MNCs and ZIF-8 MNCs after heat treatment. Whereas a substantial change in the absorption peak wavelength was observed for MNCs, a negligible change was observed for ZIF-8/MNCs. This indicates that the ZIF-8 layers prevented the oxidation of Fe₃O₄ due to their hydrophobic pore structures.26

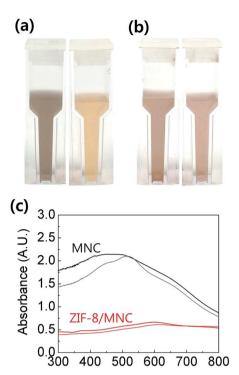


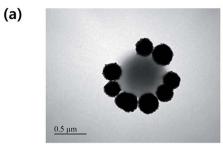
Fig. 2 (a) Optical images of as-synthesized MNCs before (left) and after (right) heat treatment at 200 $^{\circ}$ C for 1 h. (b) Optical images of assynthesized ZIF-8/MNCs before (left) and after (right) heat treatment at 200 $^{\circ}$ C for 1 h. (c) Variations in UV-VIS spectrum of as-synthesized MNCs (black: before heat treatment, gray: after heat treatment) and ZIF-8/MNCs (red: before heat treatment, orange: after heat treatment) in water.

Wavelength (nm)

The sensitivity of the assay was investigated using milk solutions spiked with various concentrations of *S. aureus*. Antibody-functionalized ZIF-8/MNCs were added to 10 mL of milk that had been spiked with 0–10⁵ cfu mL⁻¹ of *S. aureus*. After incubation at RT for 1 h, the bacteria were magnetically separated and rinsed several times with PB. Fig. 3(a) shows a TEM image of a ZIF-8/MNC-bound *S. aureus* bacterium. The bacterial surface was covered by ZIF-8/MNCs, indicating the effective capture of target bacteria using ZIF-8/MNCs. The ATP luminescence was measured using a portable ATP luminometer. The luminescence intensities were increased with increasing concentration of *S. aureus*. The detection limit for the *S. aureus*-spiked milk solution was found to be 300 cfu mL⁻¹ as shown in Fig. 3(b).

The selectivity of the assay was examined using control experiments with milk solutions spiked with 10⁵ cfu mL⁻¹ *Escherichia coli, Salmonella typhimurium, Vibrio parahaemolyticus*, and *Listeria monocytogenes. S. aureus*-antibodyconjugated ZIF-8/MNCs were used to capture the bacteria in each solution, and the ATP luminescence was measured. Fig. 4 shows that the intensity of the ATP luminescence measured in the control experiments was very weak, indicating that nonspecific binding was negligible.

RSC Advances Paper



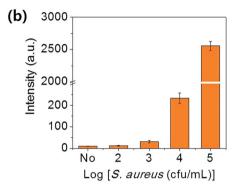


Fig. 3 (a) TEM image of a ZIF-8/MNC-bound S. aureus bacterium. (b) Intensities of ATP luminescence measured from a milk solution spiked with different concentrations of S. aureus

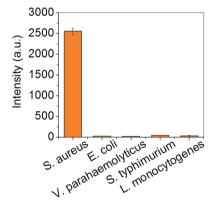


Fig. 4 Intensities of ATP luminescence measured from milk solutions spiked with different bacteria at concentrations of 10⁵ cfu mL⁻¹.

Conclusions

In summary, we synthesized ZIF-8-coated MNCs and used them to detect pathogenic bacteria in milk. The low-coordinated Zn sites located on the outer layer of ZIF-8 offer binding sites for thiolated antibodies; also, half-fragmented antibodies could be directly conjugated on the ZIF-8/MNCs without linker molecules. After the capture and magnetic separation of S. aureus in milk using the hybrid ZIF-8/MNCs, the concentration of bacteria was determined using a portable ATP luminometer. The detection limit was 300 cfu mL⁻¹. Furthermore, ZIF encapsulation was found to improve the stability of MNCs in water by suppressing the oxidation of Fe₃O₄, which facilitates the application of the hybrid particles for the on-site detection of pathogenic bacteria.

Acknowledgements

This research was supported by the National Research Foundation of Korea (NRF) funded by the Korea government (MEST) (NRF-2014R1A2A2A01007027).

References

- 1 S. Laurent, D. Forge, M. Port, A. Roch, C. Robic, L. Vander Elst and R. N. Muller, Chem. Rev., 2008, 108, 2064-2110.
- 2 J. B. Mamani, A. J. Costa-Filho, D. R. Cornejo, E. D. Vieira and L. F. Gamarra, Mater. Charact., 2013, 81, 28-36.
- 3 S. Adarsh, H. Hiroshi and A. Masanori, Nanotechnology, 2010, 21, 442001.
- 4 D. Dressman, H. Yan, G. Traverso, K. W. Kinzler and B. Vogelstein, Proc. Natl. Acad. Sci. U. S. A., 2003, 100,
- 5 J. Zheng, Z. Lin, G. Lin, H. Yang and L. Zhang, J. Mater. Chem. B, 2015, 3, 2185-2191.
- 6 C. Chun, J. Joo, D. Kwon, C. S. Kim, H. J. Cha, M.-S. Chung and S. Jeon, Chem. Commun., 2011, 47, 11047-11049.
- 7 D. Kwon, S. Lee, M. M. Ahn, I. S. Kang, K.-H. Park and S. Jeon, Anal. Chim. Acta, 2015, 883, 61-66.
- 8 H. Deng, X. Li, Q. Peng, X. Wang, J. Chen and Y. Li, Angew. Chem., Int. Ed., 2005, 44, 2782-2785.
- 9 H. L. Ding, Y. X. Zhang, S. Wang, J. M. Xu, S. C. Xu and G. H. Li, Chem. Mater., 2012, 24, 4572-4580.
- 10 Y. Deng, D. Qi, C. Deng, X. Zhang and D. Zhao, J. Am. Chem. Soc., 2008, 130, 28-29.
- 11 P. Jung-Nam, Z. Peng, H. Yong-Sheng and W. M. Eric, Nanotechnology, 2010, 21, 225708.
- 12 C. Hui, C. Shen, J. Tian, L. Bao, H. Ding, C. Li, Y. Tian, X. Shi and H.-J. Gao, Nanoscale, 2011, 3, 701-705.
- 13 Q. Weiping, X. Bin, W. Lei, W. Chunxiao, S. Zengdong, Y. Danfeng, L. Zuhong and W. Yu, J. Inclusion Phenom. Macrocyclic Chem., 1999, 35, 419-429.
- 14 J. Zhuang, C.-H. Kuo, L.-Y. Chou, D.-Y. Liu, E. Weerapana and C.-K. Tsung, ACS Nano, 2014, 8, 2812-2819.
- 15 K. Liang, R. Ricco, C. M. Doherty, M. J. Styles, S. Bell, N. Kirby, S. Mudie, D. Haylock, A. J. Hill, C. J. Doonan and P. Falcaro, Nat. Commun., 2015, 6, 7240.
- 16 Y. Pan, Y. Liu, G. Zeng, L. Zhao and Z. Lai, Chem. Commun., 2011, 47, 2071-2073.
- 17 F. Ke, L.-G. Qiu, Y.-P. Yuan, F.-M. Peng, X. Jiang, A.-J. Xie, Y.-H. Shen and J.-F. Zhu, J. Hazard. Mater., 2011, 196, 36-43.
- 18 S. Wang, Y. Fan and X. Jia, Chem. Eng. J., 2014, 256, 14-22.
- 19 L. Chang-Moon, J. DooRye, C. Su-Jin, K. Eun-Mi, J. Min-Hee, K. Sun-Hee, K. Dong Wook, L. Seok Tae, S. Myung-Hee and J. Hwan-Jeong, Nanotechnology, 2010, 21, 285102.
- 20 W. Cheng, K. Tang, Y. Qi, J. Sheng and Z. Liu, J. Mater. Chem., 2010, 20, 1799-1805.
- 21 H. Sharma and R. Mutharasan, Anal. Chem., 2013, 85, 2472-
- 22 K. Ito, K. Nishimura, S. Murakami, H. Arakawa and M. Maeda, Anal. Chim. Acta, 2000, 421, 113-120.
- 23 W. Lee, D. Kwon, B. Chung, G. Y. Jung, A. Au, A. Folch and S. Jeon, Anal. Chem., 2014, 86, 6683-6688.

RSC Advances

25 M. I. Dar and S. A. Shivashankar, RSC Adv., 2014, 4, 4105-4113.

24 K. Haneda and A. H. Morrish, J. Phys. Colloques, 1977, 38, 26 K. Zhang, R. P. Lively, C. Zhang, W. J. Koros and R. R. Chance, J. Phys. Chem. C, 2013, 117, 7214-7225.