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## Introduction

Stimuli-responsive polymer vesicles, regarded as a kind of smart nanovehicle, have sparked great attention in recent years since they are a promising prospective candidate for drug delivery systems and nanomedicine.<sup>1</sup> In general, these nanovehicles can respond to external stimuli and then undergo drastic chemical structural changes,<sup>2</sup> thus inducing controlled dissociation so as to release cargos for target therapy. To date, a variety of external signals including temperature,<sup>3</sup> light,<sup>4</sup> and electric field,<sup>5</sup> as well as physiological factors, such as redox,<sup>6</sup> pH,<sup>7</sup> and enzyme<sup>8</sup> have been exploited for building responsive polymersomes. Recently, more and more intracellular applications have required us to directly utilize bioactive molecules as triggers to manipulate payload release. This new strategy has two particular advantages: endogenous stimuli are conducive to enhancing specific drug biodistribution in diseased cells<sup>1a</sup> and prevent cell damage from chemical agent accumulation. In this respect, despite an imperative to simulate bioresponsive modes, building macromolecular assemblies that can sense a particular bioactivator remains elusive.<sup>9</sup>

Hydrogen sulfide ( $H_2S$ ), known as a toxic gas in the atmosphere, is also an important neuromodulator and cell signaling molecule. In the cell,  $H_2S$  can be generated from L-cysteine via cystathionine  $\gamma$ -lyase (CSE) mediated decomposition.<sup>10</sup> The latest reports have demonstrated that it plays a pivotal role in tuning blood vessel dilation, resisting inflammation and inducing cell apoptosis.<sup>11</sup> Metabolic disturbance of  $H_2S$  is

directly related to numerous diseases including angioedipathy and neurodegeneration. Taking into account the importance of the effect of  $H_2S$  on cells, exploring how to use this bioactivator as a stimulation mode to activate polymer self-assembly behaviors for targeted drug delivery is quite challenging.

At present, some nascent studies have been devoted to embedding biosignals into polymer systems. A successful example is the proposed  $CO_2$ -sensitive polymer assemblies of Yuan and Zhao *et al.*<sup>12</sup> The Davis group designed a nitric oxide (NO)-tuning copolymer.<sup>13</sup> In spite of the progress at this frontier, polymers that can feedback  $H_2S$  gasotransmitter have not been synthesized so far. Here we developed the new idea of using a class of peculiar *o*-azidomethylbenzoate-containing block copolymers to fabricate  $H_2S$ -responsive polymer vesicles. Their disassembly process is dependent on the stimulus concentration. Actually, *o*-azido-methylbenzoate (AzMB) is a sensitive self-cleavable precursor, which can be converted into benzylamine by  $H_2S$ , and the latter is able to cause a series of intramolecular cascade reactions that finally sever the benzoyl bond (Fig. 1a). Based on this, we speculated that the AzMB pendants covalently linked to the copolymer could be cleaved by a low concentration of  $H_2S$ . This will thereby drive a change in amphiphilicity of the block copolymer, further triggering a desirable disassembly of the polymer aggregates, as shown in Fig. 1b.

## Results and discussion

### Designing a $H_2S$ -responsive block copolymer

To fulfil the goal, we designed and synthesized a kind of diblock copolymer, consisting of a biocompatible poly(ethylene oxide) (PEO) chain as the hydrophilic block and a poly(*o*-azidomethyl benzoyl glycerol methacrylate) chain (termed as PAGMA) as the

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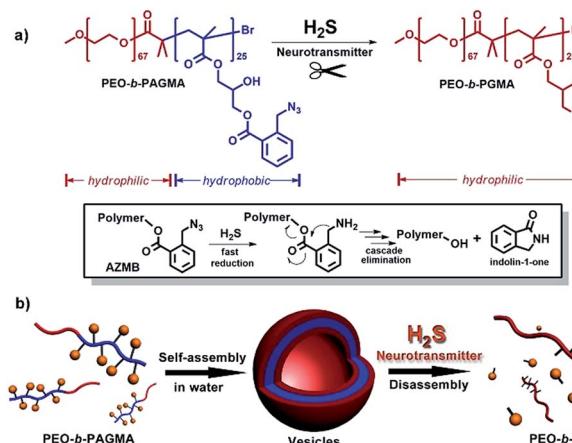


Fig. 1 (a)  $\text{H}_2\text{S}$ -responsive cleavage of *o*-azidomethylbenzoate (AzMB)-containing diblock copolymer (PEO-*b*-PAGMA) and  $\text{H}_2\text{S}$ -induced cascade reaction mechanism. (b) Schematic illustration of their polymer self-assembly into vesicles and  $\text{H}_2\text{S}$ -responsive controlled disassembly process.

$\text{H}_2\text{S}$ -sensitive hydrophobic segment. This target copolymer, PEO-*b*-PAGMA, was prepared by atom transfer radical polymerization with a well-defined molecular weight ( $M_w = 11.2$  kDa) and near-monodispersity ( $M_w/M_n = 1.09$ , the details of the synthesis and characterization are in the ESI†).

We investigated the  $\text{H}_2\text{S}$ -responsiveness of this copolymer using UV-vis spectroscopy. While increasing  $\text{H}_2\text{S}$  concentration, the absorption changes of PEO-*b*-PAGMA can be monitored. We found that in the absence of an external stimulus, the polymer solution ( $9 \times 10^{-3} \text{ g L}^{-1}$ , containing  $20 \mu\text{M}$  concentration of AzMB groups) exhibited a characteristic absorption at 290 nm ascribed to the AzMB species (Fig. 2a, pink curve). Upon gradual addition of  $\text{H}_2\text{S}$  from 0 to  $20 \mu\text{M}$ , interestingly, the intensity of the AzMB absorption band declined by 94%, whereas a group of new double peaks at 248 nm and 259 nm appeared and slowly strengthened (Fig. 2a, green curve), suggesting that  $\text{H}_2\text{S}$  can react with the AzMB functionality. To further elucidate this chemical process, before and after gas treatment, all the reactive components in solution were separated by liquid chromatography and analysed by  $^1\text{H}$  NMR spectroscopy (Fig. 2b). Before the stimulus, it is clear that the  $^1\text{H}$  NMR spectrum of PEO-*b*-PAGMA showed a group of typical aromatic region proton shifts ( $\text{H}_a\text{--H}_d, \delta = 7.30\text{--}7.76 \text{ ppm}$ ) and a benzyl peak ( $\text{H}_h, \delta = 3.95 \text{ ppm}$ ) ascribed to AzMB species. After the copolymer solution was exposed to  $\text{H}_2\text{S}$ , however, all the above peaks in the final products totally vanished, indicating the cleavage of the benzoyl bond. In addition, the three groups of methylene peaks ( $\text{H}_e, \text{H}_f$  and  $\text{H}_g$ ) belonging to the glycerol motif are relatively shifted upfield ( $\text{H}_e \rightarrow \text{H}_{e'}: \delta = 4.63 \rightarrow 3.81, \text{H}_f \rightarrow \text{H}_{f'}: \delta = 4.43 \rightarrow 4.36, \text{H}_g \rightarrow \text{H}_{g'}: \delta = 4.31 \rightarrow 4.19$ ), which is in line with the spectrum of poly(glycerol methacrylate) (PGMA, Fig. S3 in ESI†). These results provided key evidence of the detachment of AzMB pendants from the copolymer main chain. Furthermore, we attempted to reveal the reaction mechanism of  $\text{H}_2\text{S}$  cutting off the AzMB group. To this end, we separated and purified the other byproducts from the reactive solution. A cyclic

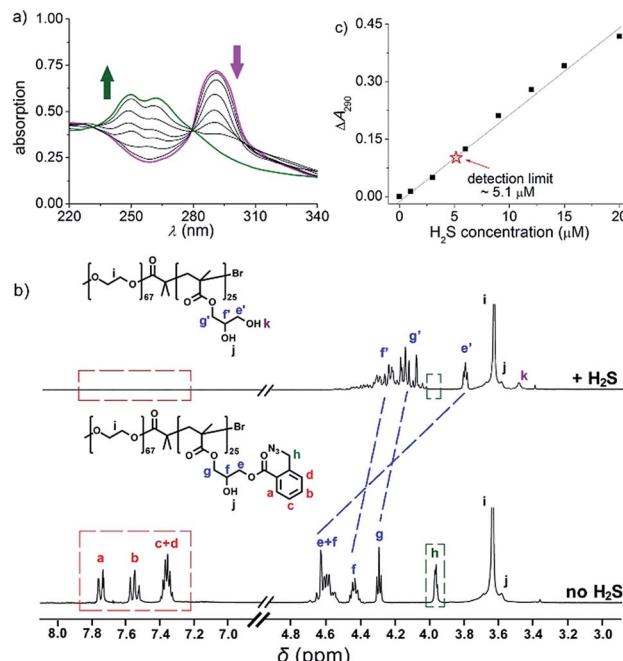


Fig. 2 (a) UV-vis absorption changes of PEO-*b*-PAGMA under different  $\text{H}_2\text{S}$  concentrations (from pink to green curve): 0, 2, 4, 6, 10, 12, 16, and  $20 \mu\text{M}$ . (b)  $^1\text{H}$  NMR spectra comparison of PEO-*b*-PAGMA before and after  $\text{H}_2\text{S}$  treatment ( $d_6$ -DMSO). (c) The UV-vis absorbed intensity changes of PEO-*b*-PAGMA for different  $\text{H}_2\text{S}$  levels ( $\lambda_{\text{max}} = 290 \text{ nm}$ ). All the experiments were carried out at the polymer concentration of  $9 \times 10^{-3} \text{ g L}^{-1}$ , containing  $20 \mu\text{M}$  AzMB groups.

benzolactam compound was detected in the filtrate residue. Its  $^1\text{H}$  NMR spectrum perfectly matched with commercial indolin-1-one (Fig. S4 in the ESI†) and its UV-vis absorbance was in accord with the double-peak curve (Fig. S5 in ESI†), indicating that  $\text{H}_2\text{S}$  can facilitate an intramolecular cyclization of the benzoyl bond to yield an indolin-1-one byproduct.

Infrared spectra (IR, Fig. S6 in ESI†) corroborated this reactive mechanism: the initial PEO-*b*-PAGMA solution displayed a strong azido group stretching vibration ( $2102 \text{ cm}^{-1}$ ); at 6 min of the  $\text{H}_2\text{S}$  gas stimulus, the benzylazide peak was greatly depressed but a shoulder peak at  $3465 \text{ cm}^{-1}$  ascribed to benzylamine was reinforced. However, this new vibration band vanished after 30 min of  $\text{H}_2\text{S}$  treatment and the final PEO-*b*-PAGMA was generated, as indicated by the disappearance of the phenyl group ( $1614 \text{ cm}^{-1}$ ) and the appearance of the broad hydroxyl band ( $3240\text{--}3640 \text{ cm}^{-1}$ ). All these findings demonstrate that  $\text{H}_2\text{S}$  quickly transforms benzylazide into a highly reactive nucleophilic benzylamine intermediate, and the latter is capable of attacking intramolecularly on the adjacent benzoyl to induce a cascade self-elimination reaction, leading to a site-specific chemical scission (Fig. 1a).

Since the designed PEO-*b*-PAGMA can respond to  $\text{H}_2\text{S}$ , we next aimed to quantitatively test its sensitivity. If the detection limit of  $\text{H}_2\text{S}$  is defined as a 10% change in UV-vis absorbance,<sup>13</sup> it is worth noting that PEO-*b*-PAGMA is determined to be extremely sensitive to the  $\text{H}_2\text{S}$  stimulus (detection limit is  $5.1 \mu\text{M}$ , Fig. 2c). Recent studies have indicated that the  $\text{H}_2\text{S}$



concentration in the brain is likely less than  $9.2 \mu\text{M}$ ,<sup>14</sup> but is nonetheless capable of activating the cleavage reaction. Additionally, we discovered that this polymer system showed a linear  $\text{H}_2\text{S}$  concentration-dependent responsiveness, which means that the cleavage ratio of the polymer is adjustable.

### $\text{H}_2\text{S}$ -triggered controlled disassembly of the polymersomes

To further explore whether this polymer system is adaptable for use as a drug nanovehicle, we studied its self-assembly behavior. Owing to the amphiphilicity, PEO-*b*-PAGMA can spontaneously form aggregates in aqueous solution. The critical aggregate concentration (CAC) is determined to be  $0.02 \text{ g L}^{-1}$ , as measured by a fluorescent probe method (Fig. S7 in ESI†).<sup>15</sup> A transmission electron microscope (TEM) was employed to visualize the size and morphology of these polymeric aggregates. It is clear that PEO-*b*-PAGMA can self-assemble into a sphere-like nanostructure (Fig. 3a). The legible contrast between the dark periphery and hollow center indicates that these globular aggregates have a typical vesicular architecture and their membrane thickness is evaluated to be  $8 \text{ nm}$  by TEM statistics (Fig. 3a, inset). Normally, in the vesicles, PEO block chains serve as the hydrophilic outer and inner layers while the PAGMA portion is the hydrophobic core layer. The TEM images showed that the average diameter of these aggregates is  $62 \text{ nm}$ , corresponding to a hydrodynamic radius ( $R_h$ ) of  $34.6 \text{ nm}$  determined by dynamic light scattering (DLS, Fig. S8 in ESI†). The small deviation ( $7.2 \text{ nm}$ ) between the TEM and DLS results is representative of the fact that DLS measures the hydrated state while TEM, using dried samples, does not. In the absence of any stimuli, these aggregates are stable in water, and neither their size nor shape changes over two months.

Since the PAGMA block chain can react with  $\text{H}_2\text{S}$  and further remove the AzMB moieties to yield PGMA block, we speculated that their polymer assemblies could disassemble in a  $\text{H}_2\text{S}$  atmosphere. As expected, when  $\text{H}_2\text{S}$  was passed through the polymer solution ( $0.02 \text{ g L}^{-1}$ , containing  $45 \mu\text{M}$  of AzMB

groups), their assembling structures began to change. In the presence of a small amount of  $\text{H}_2\text{S}$  gas ( $15 \mu\text{M}$ ), these vesicles expanded remarkably. As shown in Fig. 3b, much larger vesicles were dominant in the solution. Their diameter rose on average  $160\%$  from  $62 \text{ nm}$  to  $98 \text{ nm}$  and their volume increased  $410\%$ . The reason is that one-third of the hydrophobic PAGMA block chains convert to hydrophilic PGMA block, which results in a strong hydration effect within the core layer; as a consequence, these vesicles swell quickly in order to lower the interaction free energy. A near double thickening of these vesicle walls from  $8 \text{ nm}$  to  $19 \text{ nm}$  supported this hydration-driven expansion mechanism. Similar results have been found in other responsive vesicles.<sup>12a,c</sup> When the  $\text{H}_2\text{S}$  level was increased to  $30 \mu\text{M}$ , a large amount of PAGMA block chains transformed. Because the sharp enhancement of the water solubility of the polymer chains resulted in an insupportable interfacial tension, these swollen vesicles started to crack and their membrane presented many random fractured points (Fig. 3c). With injecting  $\text{H}_2\text{S}$  to a concentration of  $45 \mu\text{M}$ , the majority of AzMB groups were disconnected and the amphiphilic PEO-*b*-PAGMA changed to water-soluble PEO-*b*-PGMA, finally leading to complete vesicle dissociation. Only a few nanofragments remained in solution, whose size ( $<10 \text{ nm}$ ) was in line with that of dried PEO-*b*-PGMA unimers (Fig. 3d). DLS monitoring confirmed this disassembly process. By changing the  $\text{H}_2\text{S}$  aeration time, we could tune the  $\text{H}_2\text{S}$  stimulus level. Under a lower  $\text{H}_2\text{S}$  level ( $15 \mu\text{M}$ ), the  $R_h$  of these aggregates climbed up to  $54.3 \text{ nm}$ , consistent with the early vesicle expansion. Then their  $R_h$  underwent an abrupt decrease from a maximum value to  $4.3 \text{ nm}$  with a  $\text{H}_2\text{S}$  increase to  $45 \mu\text{M}$ , corresponding to the later vesicular burst process (Fig. 4a).

On the other hand, one may doubt that other factors such as mechanical effects could bring about this vesicle disruption. In a control experiment, we prepared a copolymer counterpart, PEO-*b*-poly(benzoyl glycerol methacrylate) (PEO-*b*-PBGMA) lacking the azido group. It can form an analogous nano-object in aqueous solution as well but is unable to disaggregate even at a higher  $\text{H}_2\text{S}$  level ( $100 \mu\text{M}$ ), thus eliminating this possibility and proving that the vesicular disassembly mechanism arises

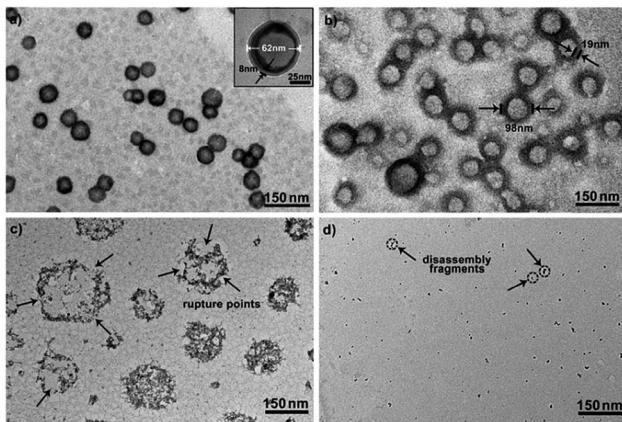


Fig. 3 TEM images of PEO-*b*-PAGMA aggregates for various levels of  $\text{H}_2\text{S}$  stimulus: (a)  $0 \mu\text{M}$ , (b)  $15 \mu\text{M}$ , (c)  $30 \mu\text{M}$  and (d)  $45 \mu\text{M}$  (the polymer concentration is  $0.02 \text{ g L}^{-1}$ , which contains an AzMB group concentration of  $45 \mu\text{M}$ ).

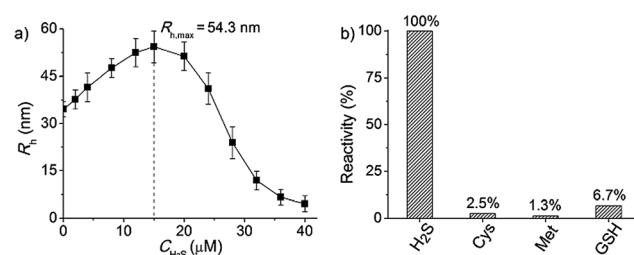


Fig. 4 (a) The polymersome radius changing as a function of  $\text{H}_2\text{S}$  concentration monitored by DLS counting (after gas treatment for  $30 \text{ min}$ , the polymer solution was incubated for  $30 \text{ min}$  and then tested by DLS). (b) The responsive specificity comparison among other sulphur-containing bioactivators ( $\text{H}_2\text{S}$ :  $20 \mu\text{M}$ ; Cys, Met and GSH:  $45 \mu\text{M}$ ;  $\text{H}_2\text{S}$  is the reference of  $100\%$  activity and the treatment time of all stimulants was kept at  $60 \text{ min}$ ).



from  $\text{H}_2\text{S}$ -sensitive macromolecular structural alteration (Fig. S9 in ESI†).

### The specificity of $\text{H}_2\text{S}$ -triggered polymersome disassembly

To better adapt to the cell environment, it is desirable that this disassembly is  $\text{H}_2\text{S}$  specific and selective. In biological cells, besides the  $\text{H}_2\text{S}$  gasotransmitter, there are other sulphur-containing bioactivators to guide cell activities such as cysteine (Cys), methionine (Met), and glutathione (GSH).<sup>16</sup> According to the above experiments, we know that the cleavage of the polymer leads to an absorption change. Based on this characteristic, we surveyed the effects of these sulphur-containing chemicals by UV-vis spectroscopy. A higher level of bioactivators ( $45 \mu\text{M}$ ) was injected into the polymer solution and the system was incubated for 60 min. Regarding the  $\text{H}_2\text{S}$ -induced spectral change as a 100% active reference, other bioactivators (Cys, Met and GSH) showed negligible activities (<7%, Fig. 4b and S10 in ESI†). This shows that these polymersomes entering the cells can selectively respond to the  $\text{H}_2\text{S}$  gasotransmitter but prevent the influence of other sulphur interferences.

### Extending the bioresponsive scope of the polymersomes

In view of the excellent  $\text{H}_2\text{S}$ -responsiveness of our vesicles, we expected that we could extend their responsive range to a variety of biomolecules or biological metabolites. In the cell,  $\text{H}_2\text{S}$  can be endogenously produced by many kinds of proteases. For example, CSE enzyme is capable of converting intracellular Cys into  $\text{H}_2\text{S}$ .<sup>10</sup> Therefore, introducing CSE into the vesicle system can broaden the responsiveness from  $\text{H}_2\text{S}$  to a specific amino acid, Cys. Based on this principle, a trace amount of CSE protein ( $20 \text{ nM}$ ) was co-assembled with PEO-*b*-PAGMA. After the vesicle forms, there should be a part of CSE dispersed in the solution. To remove these residues, the aggregate solution was centrifuged for 5 min at 11 000 rpm at certain intervals (2 h), and 2 mL of the supernatant was withdrawn and replaced by fresh medium. Measuring the UV-vis spectra of the supernatant until there was no obvious CSE absorption indicated that unassembled CSE was removed and only 35% of proteins were non-covalently anchored on the vesicular membrane (Fig. S11 in ESI†). Adding Cys ( $45 \mu\text{M}$ ) in place of  $\text{H}_2\text{S}$ , this amino acid can penetrate across the membrane and further be decomposed into  $\text{H}_2\text{S}$  by CSE. Afterwards the generated  $\text{H}_2\text{S}$  can *in situ* react with PAGMA block chains to provoke a similar vesicular disruption (Fig. 5a and b). In comparison to the  $\text{H}_2\text{S}$  stimulus, the Cys-triggered disassembly rate is 45% slower than that of  $\text{H}_2\text{S}$  treatment, as indicated by DLS counting experiments (Fig. 5c). It is understandable since the CSE-mediated enzymatic reaction needs an induction period for Cys transmembrane penetration and  $\text{H}_2\text{S}$  production. In a similar way, if one can introduce other  $\text{H}_2\text{S}$ -producing proteins into the polymer vesicle, the responsive scope will be expanded to the corresponding biomolecules.

### $\text{H}_2\text{S}$ -responsive controlled drug release

Finally, to assess the feasibility of these polymersomes as drug delivery vectors, we performed payload release tests. It is known

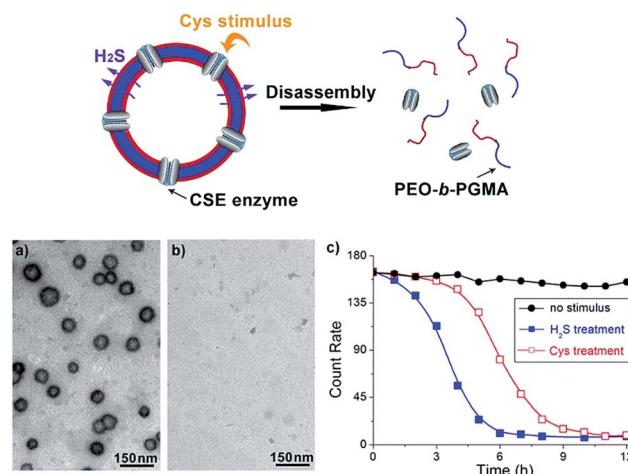


Fig. 5 Schematic illustration of Cys-responsive polymer vesicle disruption (top). (a) and (b) TEM images showing Cys-triggered disassembly of CSE/PEO-*b*-PAGMA hybrid polymersomes: (a) no stimulus, (b) injecting  $45 \mu\text{M}$  Cys into the aggregate solution (the polymer concentration is  $0.02 \text{ g L}^{-1}$ , containing an AzMB group concentration of  $45 \mu\text{M}$ ). (c) The disassembly rate of the polymersomes upon various conditions: no stimulus (●),  $\text{H}_2\text{S}$  treatment (■) and Cys treatment (□). The test was conducted using the DLS counting rate.

that the overproduction of  $\text{H}_2\text{S}$  gasotransmitter can result in blood vessel overexpansion and hypotension.<sup>11a</sup> Epinephrine (EP), as a water-soluble vasoconstrictor, is used for resisting vessel dilation. By encapsulating EP into our vesicles, it is anticipated that when these drug-loaded nanocarriers enter  $\text{H}_2\text{S}$ -overproducing cells, they can rapidly rupture to liberate internal cargos for *in situ* inhibition of vessel dilation.

In our experiments, the EP-loaded polymersomes were packed in a semipermeable bag (MWCO = 3.0 kDa), which was dialyzed against a phosphate buffer (pH = 7.2). The quantity of release was recorded through the intensity of EP diagnostic excitation<sup>17</sup> ( $\lambda_{\text{ex}} = 317 \text{ nm}$ ) by fluorescence spectra. The release amount plotted against release time for various stimulation cases is depicted in Fig. 6. Without any trigger the nanocapsules showed a low-level free release process (less than 10% over 16 h). When applying a low concentration of  $\text{H}_2\text{S}$  stimulus ( $15 \mu\text{M}$ ), these vesicles expand but do not crack, thus leading to an increase of the number of membrane nanoporous defects in the vesicles. Such a result further enhances leaking of the internal EP payloads, so the release rate had a modest ascent (nearly 32% within 16 h). In contrast, when adding a high concentration of  $\text{H}_2\text{S}$  stimulus ( $45 \mu\text{M}$ ), the complete disruption of these polymer vesicles caused a rapid cargo release. The maximum release amount reached 94% in a shorter time (6 h).

In another case, we utilized Cys as an alternative stimulant to trigger the CSE-anchored hybrid polymersomes. In comparison to those corresponding entities without enzymes, their release speeds were decelerated ( $15 \mu\text{M}$  Cys caused a 25% release within 16 h and  $45 \mu\text{M}$  Cys caused an 86% release within 10 h: blue dash line and blue solid line, respectively). The result that can

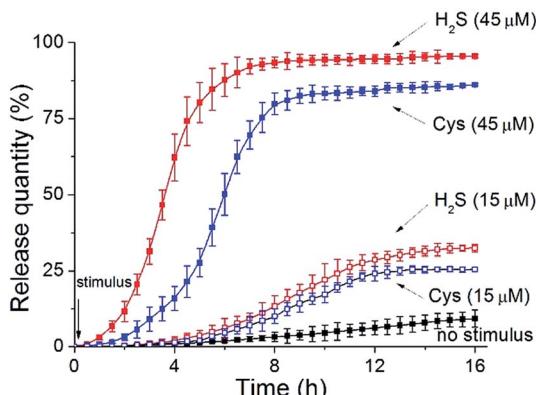


Fig. 6 Controlled drug release of EP from PEO-*b*-PAGMA vesicles or CSE/PEO-*b*-PAGMA hybrid vesicles under different conditions: no stimulus (■), non-hybrid vesicles upon a 45  $\mu\text{M}$   $\text{H}_2\text{S}$  stimulus (■), non-hybrid vesicles upon a 15  $\mu\text{M}$   $\text{H}_2\text{S}$  stimulus (□), hybrid vesicles upon a 45  $\mu\text{M}$  Cys stimulus (■) and hybrid vesicles upon a 15  $\mu\text{M}$  Cys stimulus (□). The polymer aggregate concentration is 0.02  $\text{g L}^{-1}$ , containing an AzMB group concentration of 45  $\mu\text{M}$ .

be drawn is that our vesicles can serve as intelligent nano-vehicles for realizing controllable drug delivery by modulating biosignal strength.

## Conclusions

In summary, we have designed and developed a new class of *o*-azidomethylbenzoate (AzMB)-containing block copolymers. They can spontaneously form a vesicular architecture in aqueous media on the basis of their amphiphilicity. The particular functionality in the polymer endows these vesicles with unique sensitivity to a gaseous signaling molecule,  $\text{H}_2\text{S}$ .  $\text{H}_2\text{S}$  can motivate a controlled disassembly of the polymersomes by site-specific cleavage of the AzMB groups. Moreover, we propose a concept, by means of installing various  $\text{H}_2\text{S}$ -producing proteins onto the vesicle membrane, to reasonably extend the polymer responsive scope from simple  $\text{H}_2\text{S}$  to complex biomolecules. With respect to drug delivery, due to this endogenous stimulus mode, the nanovectors are promising for intracellular targeted release and therapy. We envisage that this kind of polymer model will open up a new avenue to construct bioresponsive nanocapsules for more biological applications.

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