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## Microfluidic platforms for DNA methylation analysis

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In the field of genetics, epigenetics is the study of changes in gene expression without any change in DNA sequences. Chemical base modification in DNA by DNA methyltransferase, and specifically methylation, has been well studied as the main mechanism of epigenetics. Therefore, the determination of DNA methylation of, for example, 5'-methylcytosine in the CpG sequence in mammals has attracted attention because it should prove valuable in a wide range of research fields including diagnosis, drug discovery, and therapy. Methylated DNA bases and DNA methyltransferase activity are analyzed using conventional methods; however, these methods are time-consuming and require complex multiple operations. Therefore, new methods and devices for DNA methylation analysis are now being actively developed. Furthermore, microfluidic technology has also been applied to DNA methylation analysis because the microfluidic platform offers the promising advantage of making it possible to perform thousands of DNA methylation reactions in small reaction volumes, resulting in a high-throughput analysis with high sensitivity. This review discusses epigenetics and the microfluidic platforms developed for DNA methylation analysis.

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## 1. Introduction

### 1.1 Epigenetics and DNA methylation

Epigenetics is the genetic study of cellular and physiological phenotypic trait variations and a mechanism for controlling gene expression that does not depend on DNA sequence

changes.<sup>1,2</sup> Namely, daughter cells inherit genetic characteristics through cell division, but epigenetics is an independent mechanism of change in DNA bases. Epigenetics is known to be a chemically stable modification in DNA; however, DNA is also known to be dynamically changed by environmental factors such as exposure to oxidative stress.<sup>3–5</sup> DNA methylation and histone modification have received particular attention as the main mechanisms of epigenetics. In this review, we mainly focus on DNA methylation as indicated by our title.

DNA methylation, especially the addition of a methyl group at the fifth position of the cytosine base (5'-methylcytosine) in mammalian cells, was first discovered<sup>6</sup> in

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1948 in thymus-derived bovine DNA. It became clear that the methylation of genomic DNA is related to various life phenomena<sup>7–9</sup> that can be seen in a wide range of creatures, *Escherichia coli*, plants and vertebrates. In particular, cytosine methylation at CpG islands in mammals is becoming a crucially important study in ontogeny and cytodifferentiation. This is because the methylation of the CpG sequence has been revealed to relate to the genetic silence mechanism. The methylation of DNA is also known to be accompanied by a change in the chromatin structure. The methylation of DNA controls gene expression and functions as a storage system for tissue-specific expressed genes.

The determination of the DNA methylation information for various gene regions is important not only for basic biology areas such as cytogenesis and reproduction but also for nuclear cell transfer technology, tissue engineering and a range of diagnostic techniques. Furthermore, epigenetic drug discovery has been receiving a lot more attention lately. It is clear that epigenetics research is essential in the life sciences field. Epigenetics research is positioned between work on stable genome sequences and work on variable mRNA expression, and it represents a new life science paradigm.

### 1.2 Determination of 5'-methylcytosine

The methylation of the 5' carbon of cytosine in DNA (5'-methylcytosine) is an epigenetic modification that regulates gene expression and plays crucial roles in embryonic development.<sup>10</sup> 5'-Methylcytosine at CpG islands has received particular attention as mentioned above because it is thought to be involved in controlling genetic expression, including that in cancer,<sup>9</sup> genomic imprinting,<sup>11</sup> cellular differentiation and Alzheimer's disease.<sup>12</sup> 5'-Methylcytosine is now recognized as the fifth DNA base containing heritable information. Therefore, highly sensitive, accurate and quantitative information concerning cytosine methylation in DNA would be valuable with respect to genetic disease diagnosis.

Now, two major 5'-methylcytosine detection methods have been developed; bisulfite treatment followed by PCR and sequencing, and DNA restriction digests. A bisulfite-based determination method is widely used to distinguish between cytosine and 5'-methylcytosine.<sup>13–15</sup> Treatment with bisulfite converts cytosine to uracil, while 5'-methylcytosine remains unaffected. Therefore, information about 5'-methylcytosine in DNA can be obtained at the single base level by determining the differences between the sequences of bisulfite-treated and untreated samples. For example, bisulfite-sequencing,<sup>16</sup> combined bisulfite restriction analysis (COBRA),<sup>17</sup> methylation-specific PCR<sup>15</sup> and pyrosequencing<sup>18</sup> provide the methylation status of a specific sequence with a single CpG level.

Methylation-sensitive restriction enzyme-based methods have also been used for the site-specific detection of DNA methylation.<sup>17,19</sup> When nucleotides in the DNA recognition sequence are subjected to methylation, certain kinds of restriction enzymes are no longer able to cleave the DNA

sequence. By combining the cleavage provided by a methylation-sensitive restriction enzyme and genetic engineering techniques such as real-time PCR, it is possible to perform a cytosine methylation analysis of the target DNA sequence.

### 1.3 Determination of DNA methyltransferase activity

DNA methylation is carried out by the catalysis of DNA methyltransferase. DNA methyltransferase can be divided into three different groups on the basis of the chemical reactions. These DNA methyltransferase groups generate *N*<sup>6</sup>-methyladenine, *N*<sup>4</sup>-methyladenine, and *C*<sup>5</sup>-methylcytosine (5'-methylcytosine). Riggs and Holliday first proposed the idea that heritable DNA methylation provides a mechanism for the developmental regulation of gene expression.<sup>20,21</sup> They revealed the existence of a maintenance methyltransferase that does not add a methyl group to unmethylated bases; however, it promptly methylates hemi-methylated base pairs in a DNA duplex. Some research groups subsequently demonstrated the existence of such a maintenance methyltransferase activity by performing experiments showing the clonal inheritance of methylation patterns in mammalian cells.<sup>22,23</sup> The first cloned mammalian DNA methyltransferase was DNA methyltransferase-1 (Dnmt1).<sup>24,25</sup> Purified Dnmt1 protein was confirmed to methylate a DNA duplex that contains hemi-methylated CpG sites more efficiently than unmethylated DNA *in vitro*.<sup>26</sup> In the process of DNA methylation, a methyl group is transferred from a donor molecule to the target base in the unmethylated site. *S*-Adenosyl-*l*-methionine (SAM) is a well-known donor molecule that is used for various DNA methylation assays. Furthermore, new methyltransferases, namely the Dnmt2 and Dnmt3 families, were discovered and they exhibit *de novo* DNA methyltransferase activity. Specifically, the murine Dnmt3 family consists of two genes, Dnmt3a and Dnmt3b, which are highly expressed in undifferentiated ES cells but downregulated after differentiation and expressed at low levels in adult somatic tissues.<sup>25,27</sup>

The traditional method for detecting DNA methyltransferase activity is radioactive labeling with [methyl-<sup>3</sup>H]-SAM or the separation of methylated fragments using high-performance liquid chromatography and gel electrophoresis.<sup>28</sup> However, most of these methods have unavoidable disadvantages related to measurement time, complicated procedures and exclusive-use facilities for the radioactive materials. To avoid these disadvantages, alternative measurement techniques have recently been proposed, for example, fluorescence,<sup>29</sup> colorimetry<sup>30</sup> and electrochemical<sup>31</sup> methods. Furthermore, microfluidic technology has been used to reduce the measurement time and sample volume as we will discuss later.

### 1.4 Microfluidics for epigenetics

Many researchers have reported integrated analysis systems called lab-on-a-chip or micro total analysis systems (micro-





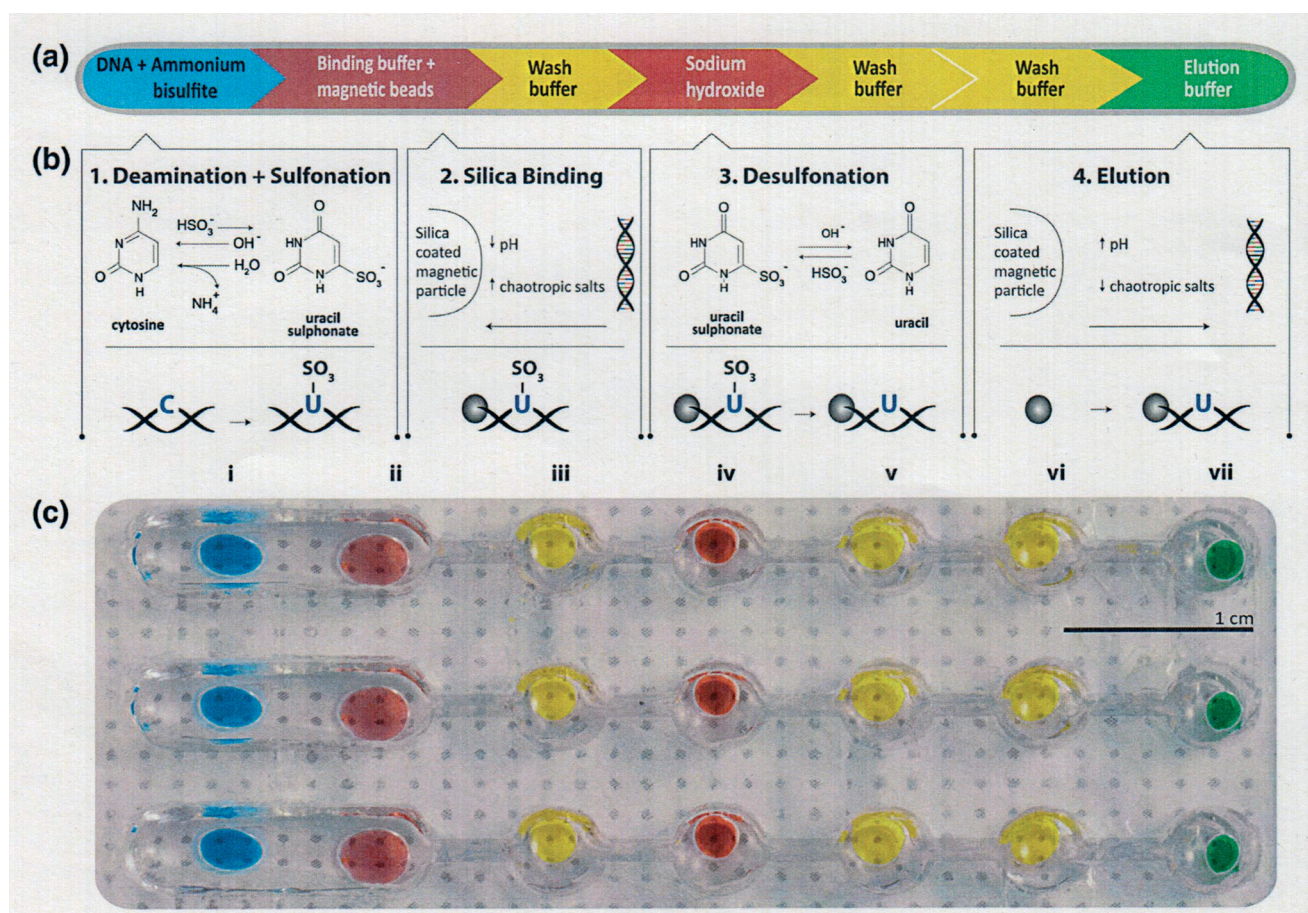
TAS) that are small, light, and capable of integrating all sample-handling steps in microfluidic channels on a chip. These techniques have made it possible to undertake various biochemical and clinical measurements simply and rapidly. These microfluidic devices for biochemical analysis have been reviewed by many researchers in relation to such applications as drug discovery,<sup>32,33</sup> drug delivery,<sup>34–36</sup> microbiology,<sup>37</sup> immunosensors,<sup>38,39</sup> PCR,<sup>40</sup> single-cell analysis,<sup>41–43</sup> point-of-care testing,<sup>44–47</sup> cell separation<sup>48,49</sup> proteomics,<sup>50</sup> nucleic acids,<sup>51–53</sup> and diagnostics.<sup>54,55</sup> There is good chemistry between microfluidic technology and life science research because microfluidic technology enables us to deal with valuable small-volume samples for analysis with high sensitivity and a high throughput. Recently, microfluidic technology has also been applied to epigenome analysis. A microfluidic platform offers the advantage of making it possible to perform thousands of methylation reactions in nanoliter reaction volumes on a single device within isolated reaction units. A microfluidics-based methylation assay technique has been applied to the high-throughput screening of large-scale chemical/biological libraries for novel DNA methyltransferase

activity or cellular proteins involved in DNA methylation regulation.<sup>56,57</sup>

## 2. Microfluidic DNA methylation analysis

### 2.1 Pretreatment devices (bisulfite conversion, DNA enrichment)

Bisulfite-based detection is the gold standard for DNA methylation analysis because it provides information about the methylation status across the entire PCR-amplified region with a single base level.<sup>15,58</sup> However a significant limitation of all bisulfite-based approaches is the duration of the bisulfite treatment, which usually requires an overnight reaction and rigorous control for complete deamination.<sup>59,60</sup> Microfluidic technology is known to be useful for reducing the total measurement time of various biomolecules because it allows manipulation with fast response times. Moreover, it can handle small fluid volumes, sense and control flows, and pattern substrates on small length scales.<sup>61</sup> Furthermore, an arrayed microfluidic platform is a powerful tool for the high-



**Fig. 1** (a) Bisulfite conversion process composed of four main chemical reactions with three intermediate washing steps to prevent reagent carryover. (b) Chemical reactions detailed for each step. (c) Photograph of aqueous reagents loaded onto a single lane of a droplet chip. Each reagent is contained in a round well that holds the droplet within it. The wells are connected either by a single open channel to merge the droplets or a narrow sieve to separate the beads from the droplet by surface tension. Reproduced with permission from Springer.



throughput treatment and measurement of multiple samples. Stark and Wang *et al.*<sup>62</sup> reported a parallelized microfluidic DNA bisulfite conversion module. Their module has three parallelized microchannels made of polydimethylsiloxane (PDMS), and each channel consists of one wide and five circular reservoir chambers, each containing aqueous reagent droplets methylated on beads that are isolated within topographic walls (Fig. 1). They used their module to successfully perform a simultaneous bisulfite conversion for all three channels with high reproducibility.

A new pretreatment technique for biofluid samples such as blood or cell suspension is also critical in terms of reducing the total assay time of DNA methylation and not simply for bisulfite conversion. If it requires a lot of time to extract and purify DNA from a biological sample, the total epigenomic assay time will be extremely long. Phenol/chloroform extraction has generally been used for genomic DNA purification. Otherwise, anti-methylcytosine antibody and methyl-CpG binding domain (MBD) proteins are used to purify and preconcentrate genomic DNA in biofluids. There have been some reports of pretreatment with microfluidics before epigenomic measurement with a view to obtaining genomic DNA that can withstand the bisulfite reaction. Two research groups have reported unique solid-phase extraction techniques in a microchannel for epigenomic analysis. Shin and Park *et al.*<sup>63</sup> reported a silicon microfluidic device that employs dimethyl adipimidate-based solid-phase extraction for the purification and extraction of nucleic acids from human body fluid samples for epigenetic analysis (Fig. 2). The silicon microfluidic chip has three components, including a pre-filtration part for cell separation, a micromixer consisting

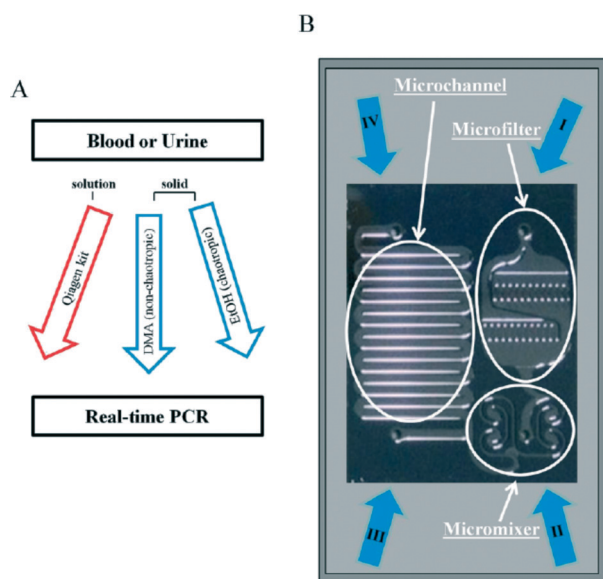


Fig. 2 (A) Work-flow for DNA extraction with dimethyl adipimidate-based solid-phase method. (B) Photograph of a microfluidic chip. The microfluidic device consists of a microfilter, micromixer, and microchannel. (I–III) Inlets for addition of samples, lysis buffer, washing and elution buffer. (IV) Outlet for collection of extracted DNA. Reproduced from ref. 63 with permission from The Royal Society of Chemistry.

of a two-stage spiral mixer for cell lysis, and a meander-shaped microchannel for dimethyl adipimidate-based solid-phase extraction to maximize the SiO<sub>2</sub> surface area. They confirmed that the device can be used to extract genomic DNA with higher purity from human blood and urine samples than other chaotropic methods. Furthermore, they showed that the device effectively captured and purified DNA, including methylated DNA, and improved the DNA amplification for the epigenetic analysis of disease-related DNA biomarkers.

On the other hand, De and Carlen *et al.*<sup>64</sup> reported a rapid microfluidic solid-phase extraction system for the capture and elution of low concentrations of hyper-methylated DNA, based on a methyl-binding domain protein modified surface, in small volumes using a passive microfluidic lab-on-a-chip platform (Fig. 3). They observed each assay step in Fig. 3 using a real-time surface plasmon resonance biosensor and undertook a quantitative characterization using fluorescence spectroscopy. The hyper-methylated DNA capture/elution process was completed in less than 5 min with efficiencies of 71% and 92% using elution volumes of 25 and 100  $\mu$ L, respectively.

## 2.2 Bisulfite-based methylcytosine assay

A total system for measuring DNA methylation has been developed and not simply for the bisulfite reaction mentioned above. It is very difficult to integrate all required chemical and biological reactions into one chip, and at present a few pretreatment and detection chips are needed. For example, a two-module system for DNA methylation analysis was

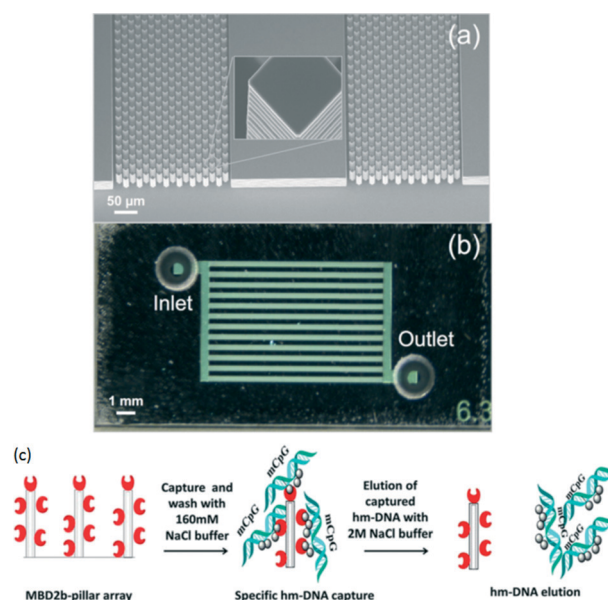


Fig. 3 (a) SEM image of pillar array etched in silicon substrate. (b) Optical image of glass-silicon bonded chips with inlet and outlet holes. (c) Hyper-methylated DNA capture and elution protocol using an MBD capture surface. Reproduced with permission from American Institute of Physics.

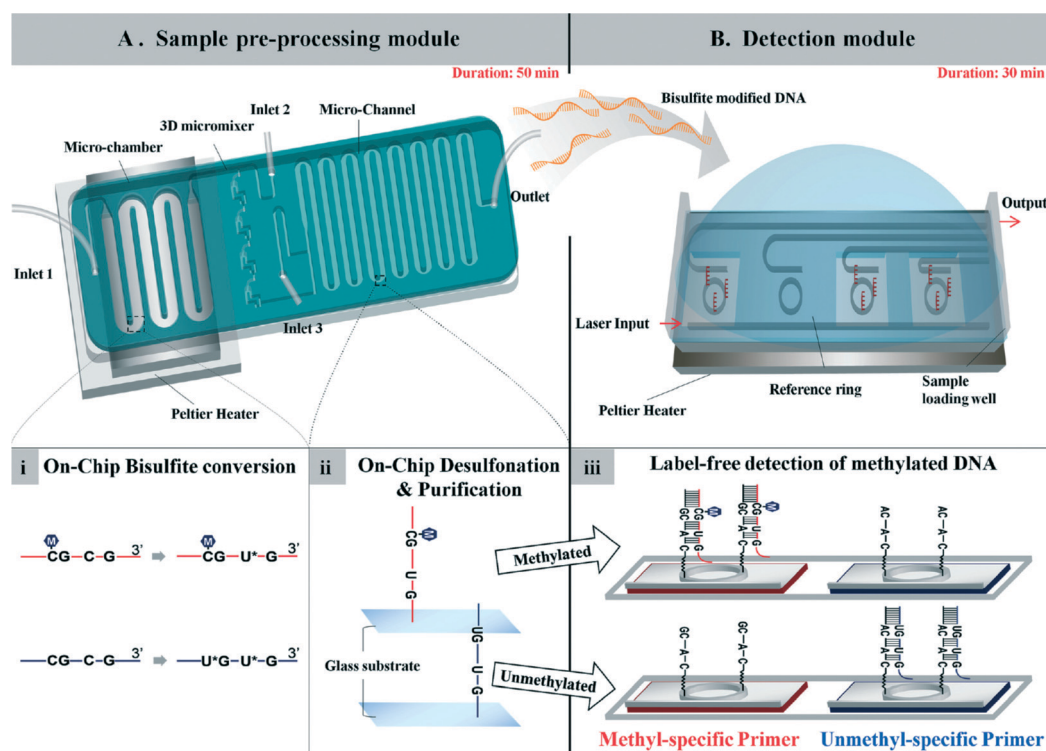




developed by Yoon and Shin *et al.*<sup>65</sup> The system is based on bisulfite conversion, which couples a sample pretreatment module for on-chip bisulfite conversion and a label-free, real-time detection module for the rapid analysis of the DNA methylation status using an isothermal DNA amplification/detection technique. The system consists of two modules, one is a sample pretreatment module, and the other is a detection module (Fig. 4). The pretreatment module for on-chip DNA bisulfite conversion consists of a microchamber, a 3D micromixer, and a microchannel. A Peltier heater is also incorporated with a microfluidic device to maintain the temperature for the on-chip bisulfite reaction. The detection module employs an isothermal solid-phase amplification/detection technique after immobilization with either methyl- or non-methyl-specific primer to analyze the DNA methylation status. The methylation status of the RAR $\beta$  gene in human genomic DNA extracted from MCF-7 cells was analyzed by the system within 80 min (excluding the 16 h needed for preparation). This is fast compared with a conventional methylation-specific PCR technique which takes 24 h. The authors also stated that the system is highly sensitive and can detect as little as 1% methylated DNA in a methylated/unmethylated cell mixture.

Combined bisulfite restriction analysis (COBRA), which is a bisulfite-based technique, involves the PCR amplification of bisulfite converted DNA followed by the digestion of a restriction enzyme.<sup>17</sup> COBRA is technically simple, and depending on the region being investigated, information on the DNA methylation status of several CpG sites can be explored in a single reaction. For these reasons, various research laboratories employ COBRA to screen large sample sets for DNA methylation.<sup>66</sup> Microfluidic electrophoresis was employed by Brena and Plass *et al.* to confirm enzymatic digestion.<sup>66–68</sup> They called their method Bio-COBRA, which is a modified COBRA protocol that incorporates an electrophoresis step in microfluidic chips. They used an Agilent 2100 Bioanalyzer, which provides quantitative results for DNA fragments by electrophoresis in microfluidic chips. A DNA methylation assay of 12 samples was completed within 1 h by using Bio-COBRA.

A unique COBRA-based method utilizing an electrophoretic feature has also been reported for analyzing electrophoretic separation differences in an ssDNA conformation with a self-complementary strand. Chen and Chang *et al.*<sup>69</sup> reported the combination of COBRA and electrophoresis with laser-induced fluorescence for determining the heterogeneity of DNA methylation. Chang's group further reported<sup>70</sup> a



**Fig. 4** (A) Sample pre-processing module for on-chip DNA bisulfite conversion consisting of a microchamber, 3D micromixer, and microchannel. (i) Human gDNA with bisulfite solution was loaded into the module using inlet 1 and incubated at 70 °C for 20 min in a continuous flow passing through the microchamber region. (ii) Then, the bisulfite-converted DNA was mixed with chaotropic buffer through the 3D micromixer and bound to the surface of the microchannel for the desulfonation and purification steps. (B) Detection module employing the isothermal solid-phase amplification/detection technique after immobilization with either methyl- or non-methyl-specific primer for analysis of the DNA methylation status. The modified DNA was loaded onto the sensing window, and resonant wavelength shifts were observed during the reaction. (iii) Amplification of methylated DNA occurs on the sensor functionalized with the methyl-specific primer, while no amplification occurs on the chip with the non-methyl-specific primer. Reproduced from ref. 65 with permission from The Royal Society of Chemistry.



screening method for DNA methylation based on single-strand conformation polymorphisms and electrophoresis with laser-induced fluorescence. PCR products that were amplified from bisulfite-treated genomic DNA were denatured, followed by immediate chilling in ice water to form ssDNA. The ssDNA was separated with poly(ethylene oxide) in the presence of an electroosmotic flow according to the different conformations represented by their methylation states. The method does not require a restriction endonuclease or specific saturating dye; thus it would be suitable for the large-scale screening of DNA methylation.

The analysis of bisulfite-based methylation by comparing differences between the target sequences of bisulfite-converted and unconverted samples is one of the most frequently used methods in conventional epigenomic research. An important point is to find a simple way of distinguishing the sequence differences in microfluidics on a chip because it is very hard to integrate all the functions of a DNA sequencer onto a single chip with the current technology. COBRA-based methods are considered to be suitable for microfluidics. This is because assay results obtained by digestion with a restriction enzyme can be quickly observed by employing electrophoretic separation or a hybridization assay with microfluidic technology. The conventional COBRA technique is unsuitable for making multiple simultaneous measurements of DNA methylation. Microfluidic technology will provide a high-throughput

assay by employing parallel processing for multiple measurements. In fact, a DNA methylation assay of 12 samples has been completed within 1 h on a microchip,<sup>66–68</sup> which is much faster than the conventional polyacrylamide gel electrophoresis (PAGE) technique.

### 2.3 Bisulfite-free methylcytosine assay

The main drawbacks of the bisulfite-based determination methods are the degradation of the sample DNA and the treatment time. More than 99% of the original DNA is reportedly destroyed after a 16 h standard bisulfite treatment.<sup>71</sup> This is mainly caused by depurination under the required acidic and thermal conditions. Therefore, to avoid misleading results, the quality of the bisulfite-treated DNA must be assessed before a detection assay is undertaken. Moreover, the bisulfite treatment makes the analyte DNA thymine-rich since unmethylated cytosine is converted to thymine, and this complicates the design of specific probes for PCR amplification.<sup>72</sup> Therefore, bisulfite-free techniques have been proposed such as chemical or protein modification. These techniques are simple because assay results can be obtained by measuring the interaction between the target DNA and the methylcytosine recognition molecules. This allows us to design the microfluidics very simply. New recently reported methods and devices for DNA methylation analysis are listed in Table 1.

Table 1 New methods and devices for determining epigenetic base modifications

Discrimination molecule	Target	Response range	Detection limit	Biological application	Detection principle	Ref.
Antibody	5-mC	0.5–10 nM	0.5 nM	—	Electrochemical	73
	5-mC	$1 \times 10^{-14}$ – $5 \times 10^{-9}$ M	$2 \times 10^{-15}$ M	Spiked test in serum	Electrochemical	74
	m6A	0.01–10 nM	2.57 pM	Rice seeding	Electrochemical	75
	5-mC	50–3200 fM	50 fM	Spiked test in serum	SPR	76
	5-mC	0.1–10 pM	6 amol	Human cancer cell	SPR	77
	5-mC	0.5–3 nM	0.5 nM	$\lambda$ DNA	Absorbance	78
	5-mC, 5-hmC	$3 \times 10^{-13}$ – $5 \times 10^{-11}$ M	$4.2 \times 10^{-13}$ M	—	Optical microcavity	79
Chromatographic or electrophoretic separation	5-mC, m6A	—	Single cell	Circulating tumor cells	MS	80
	m6A	0.00005–0.002% in DNA	0.42 fmol	Human cell lines and plants	MS	81
	5-mC, 5-hmC, 5-fC, and 5-caC	—	0.10, 0.06, 0.11, and 0.23 fmol, respectively	Human cancer cell	MS	82
	Various RNA modifications	0.21–4.0 fmol	63 amol–1.2 fmol	Human ES cells	MS	83
	5-mC, 5-hmC	2–64 nM	50 pM, 100 pM	Mouse stem cell	MS	84
$\beta$ -Glucosyltransferase	5-mC	1–50 $\mu$ M	0.02 pmol	Blood	Fluorescence	85
	5-hmC	0–0.1087% in DNA	0.0012% (0.489 pg)	Mouse tissues and cancer cell lines	Electrochemical	86
	5-hmC	0.01–50 nM	1.43 pM	—	Electrochemical	87
MBD	5-mC	—	200 pg (input DNA)	Cancer cell lines	SERS	88
Oxidation potential	5-mC	0.6–400 $\mu$ M	0.23 $\mu$ M	—	Electrochemical	89
Silver nanocluster	5-mC	$2.0 \times 10^{-9}$ – $6.3 \times 10^{-7}$ M	$9.4 \times 10^{-10}$ M	Spiked test in serum	Fluorescence	90

5-mC, 5'-methylcytosine; 5-hmC, 5'-hydroxymethylcytosine; 5-fC, 5'-formylcytosine; 5-caC, 5-carboxylcytosine; SRP, surface plasmon resonance; MBD, methyl-CpG binding domain; m6A, N<sup>6</sup>-methyladenosine.



Two proteins have mainly been used to label the methylated regions of a genome; one is an anti-methylcytosine antibody and the other is a methyl-CpG binding domain (MBD) protein.<sup>59,91</sup> The anti-methylcytosine antibody recognizes single-stranded molecules containing one or more methylated CpG sites. In contrast, the MBD protein recognizes double-stranded methylated CpG sites in DNA fragments. MBD has a unique characteristic whereby different methylation densities can be analyzed depending on the salt fractionation employed;<sup>92</sup> lower salt fractions contain hypomethylated DNA fragments, while higher salt fractions contain hypermethylated DNA fragments.<sup>93</sup>

Small artificial molecules such as osmium complexes<sup>71,94</sup> and vanadium complexes<sup>95</sup> were also designed for labeling methylcytosine. Unfortunately, thymine in DNA as well as methylcytosine is labeled *via* OsO<sub>4</sub>. Therefore, it is difficult to distinguish methylcytosine from thymine in a methylcytosine determination of natural DNA sequences. Mixtures of V<sub>2</sub>O<sub>5</sub> or NaIO<sub>4</sub> and LiBr were used in an anaerobic condition to differentiate methylcytosine from both cytosine and thymine followed by a hot piperidine treatment and electrophoretic analysis.<sup>95</sup> A sequence-selective cleavage assay technique with a metal complex at a DNA bulge has been reported;<sup>96</sup> however, this approach requires a hot piperidine treatment and electrophoresis. The main drawbacks of the chemical modification methods as regards methylcytosine assay are the relatively long detection time and the need for a high concentration (around  $\mu\text{M}$ ) DNA sample, and in many cases this is insufficient to detect DNA methylation in genomic DNA without PCR amplification.

Recently, several bisulfite-free methylcytosine assays were further integrated with microfluidics. Heimer and Sikes *et al.*<sup>97</sup> reported a microfluidic device for detecting methylated DNA fragments from the MGMT gene promoter. Target oligonucleotides from the test sample hybridize directly to capture probes printed in 300  $\mu\text{m}$  diameter spots on a chip without the bisulfite conversion. They detected methylated DNA duplexes using an MBD protein by interaction between the MBD protein and the methylated DNA using either fluorescence or photo-polymerization-based signal amplification (Fig. 5). They also fabricated a reusable PDMS-based microfluidic device so that they could use a recirculating mixing method to improve DNA hybridization efficiency and provide an assay format suitable for automation. They stated that signals in the microfluidic device were enhanced by about one-third compared with those obtained with static DNA hybridization.

A microfluidic system integrating the entire experimental process for a DNA methylation assay was reported by Wang and Lee *et al.*<sup>98</sup> The system includes target DNA isolation, *HpaII/MspI* endonuclease digestion, and nucleic acid amplification (Fig. 6). Instead of employing a bisulfite reaction, they attempt to shorten the entire process using endonuclease digestion. In their system, all the genomic DNA from the cultured cell lines was directly extracted and purified with a specific nucleotide probe conjugated on the surface of magnetic

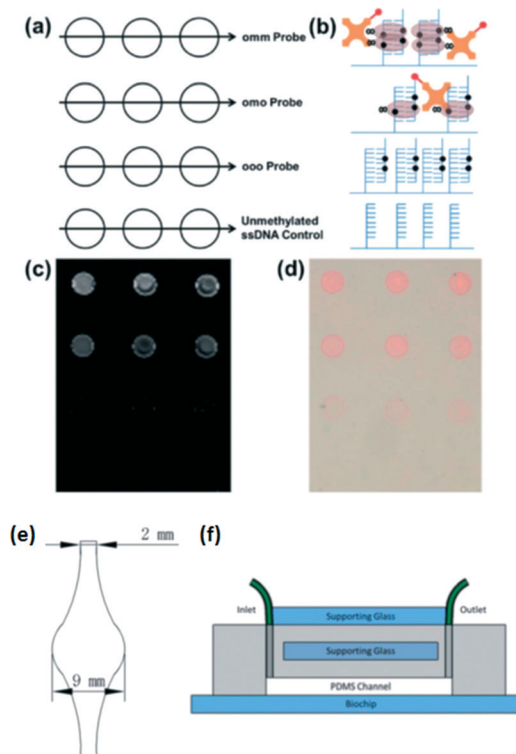


Fig. 5 (a) Biochips were spotted with capture probe ssDNA having two, one or no methylated CpG in order to epigenotype the target DNA. Unmethylated ssDNA served as the negative control. (b) Schematic representation of the area within each group of spots following hybridization with 100 nM doubly methylated target ssDNA and detection. Fluorescence (c) and colorimetric (d) readout of MBD binding to methylated DNA. (e) Diagram of the microfluidic channel etched in PDMS. (f) Supporting glass was added to the unetched side of the microfluidic device, and it was clamped to the biochip. Inlet and outlet tubing was connected to each end of the channel, fed into a microcentrifuge tube reservoir, and passed through a peristaltic pump for recirculation. Reproduced from ref. 97 with permission from The Royal Society of Chemistry.

beads. Methylated DNAs of tumor suppressor genes, HAAO, HOXA9 and SFRP5, were chosen as candidates for the detection of ovarian cancer cells. The detection limit of their microfluidic system was found to be  $10^2$  cells per reaction. Three hours were required to complete the entire process from sample loading to analysis, which is much faster than the conventional protocols. They concluded that different sources of biosamples, for example, other cell lines, ascites and serum, would be applicable to the detection of DNA methylation, indicating that the developed microfluidic system will be useful for clinical use.

An anti-methylcytosine antibody has been used for epigenetics analysis; however, its use has been limited to the immunoprecipitation or pre-concentration of methyl-CpG regions in a DNA sample.<sup>99–101</sup> Recently, immunochemical methods for detecting methylcytosine with an anti-methylcytosine antibody have been reported for analyzing the methylation level. The reported methods employ a microtiter plate,<sup>102</sup> capillary electrophoresis,<sup>103</sup> magnetic particles,<sup>104</sup>





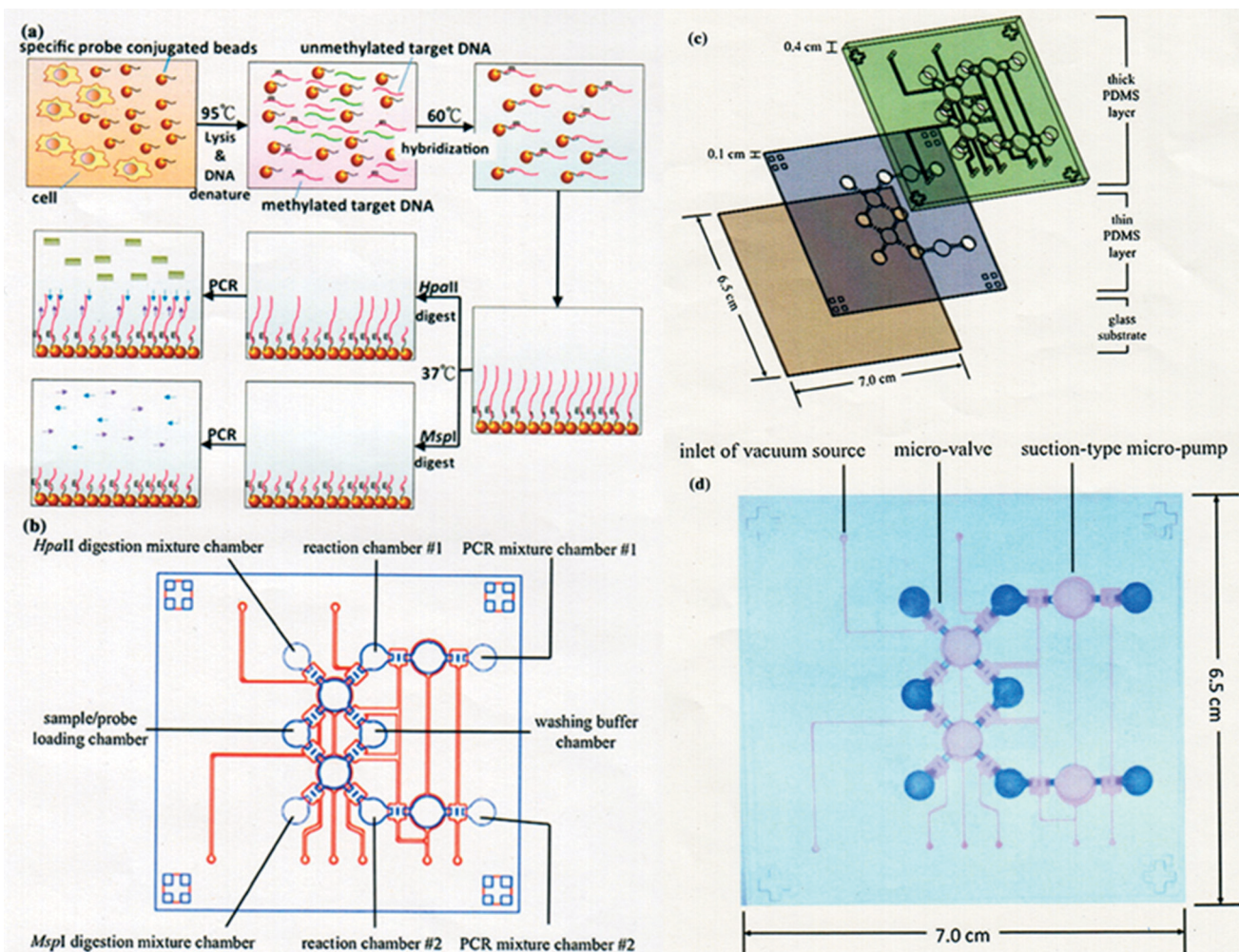


Fig. 6 (a) Illustration of working principle for detection of DNA methylation. (b) Schematic diagram of integrated microfluidic chip. (c) Exploded view of integrated microfluidic chip consisting of two PDMS layers and one glass substrate. A thick PDMS structure with air chambers and a thin PDMS membrane as a fluidic channel layer are used for flow control. (d) Photograph of integrated microfluidic chip. The measured dimensions of the chip were 6.5 cm (length) × 7.0 cm (width) × 0.5 cm (height). Reproduced with permission from Springer.

microspheres,<sup>105</sup> a nitrocellulose membrane<sup>106</sup> and a DNA microarray.<sup>107</sup> However, previously reported immunochemical methods for detecting methylcytosine have no sequence specificity and so only the total amount of methylcytosine in the analyte DNA was quantified. One of the authors found that an anti-methylcytosine antibody can recognize mismatched methylcytosine especially in a bulge region but cannot recognize methylcytosine in a pair.<sup>78,108</sup> This is because methylcytosine at a single-base bulge is predominantly in a looped-out state due to the  $\pi$ - $\pi$  stacking formation between the flanking bases of bulged methylcytosine. In contrast, methylcytosine paired with guanine is in a stacked state in a duplex. This makes it possible to perform a site-specific methylation analysis of genome DNA on a conventional microtiter plate with a biotinylated probe DNA that has a sequence to form a single base bulge at the target cytosine. We further reported<sup>77</sup> a sequence-specific microfluidic chip for DNA methylation assessment by surface plasmon resonance detection (Fig. 7a). This was achieved by utilizing an

affinity measurement involving the target, (methyl-) cytosine, in a single-base bulge region and an anti-methylcytosine antibody in a microchannel, following hybridization with a biotinylated bulge-inducing DNA probe. The probe alters the target cytosine in a looped-out state because of the  $\pi$ - $\pi$  stacking between flanking bases of the target. The probe design is simple and consists of the elimination of guanine paired with the target cytosine from a fragmented full-match sequence. The single methylation status in 6 attomoles (48 femtograms) of DNA was obtained within 45 min, which is the fastest DNA methylation assessment yet reported (Fig. 7b). The discrimination of the methylation status of single cytosine in genomic HCT116 human colon cancer cells was also carried out with the microfluidic device.

Some quick bisulfite-conversion kits are commercially available; however, the degradation of the input DNA remains an unavoidable problem. Ultimately, bisulfite-free assay is considered to be ideal; therefore the development of a new bisulfite-free methylation assay technique is being actively





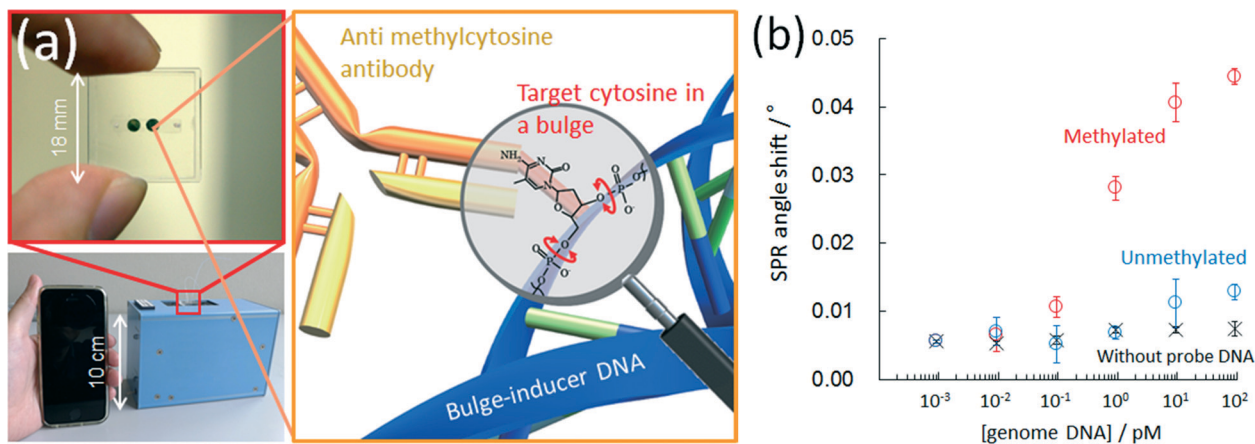


Fig. 7 (a) Photographs of microchip for assessing DNA methylation (top left) and hand-held surface plasmon resonance equipment (bottom left). Schematic of antibody binding with target methylcytosine in a DNA bulge region (right). (b) Calibration curves for methylated and unmethylated lambda DNAs with a microfluidic chip. Reproduced with permission from American Chemical Society Publications.

studied as mentioned in this section. Affinity measurements with an antibody to methylated bases or MDB proteins are a valid approach to a bisulfite-free assay; however, these affinity measurements cannot be combined with PCR amplification, *i.e.* in many cases the sensitivity is insufficient to detect DNA methylation in genomic DNA. Microfluidic technology is known to be useful for improving sensitivity with small samples and should prove to be a powerful tool for DNA methylation analysis. In fact, we showed that the methylation status of less than a pM of genomic DNA could be evaluated within 1 h by utilizing microfluidic technology.

#### 2.4 DNA methyltransferase activity

The determination of DNA methyltransferase activity has been attracting attention. One reason for this is that DNA methyltransferase and its inhibitors are reported to be a novel family of pharmacological targets for the treatment of tumors.<sup>141</sup> Therefore, there is a strong need for sensitive, selective and high-throughput methods for performing DNA methyltransferase activity assays.<sup>142</sup> However, traditional methods for DNA methyltransferase activity assay rely on radioisotope materials.<sup>109</sup> Therefore, radioisotope-free approaches have been developed, including electrochemical,<sup>109–119</sup> electrochemiluminescence,<sup>120–122</sup> photo-electrochemical,<sup>123</sup> fluorometric,<sup>124–135</sup> surface-enhanced Raman scattering (SERS),<sup>136–138</sup> and circular dichroism (CD) spectroscopy,<sup>139</sup> and surface plasmon resonance<sup>140</sup> based DNA methyltransferase measurement techniques have recently been proposed as summarized in Table 2 to realize simple, quick and easy monitoring.

By combining these DNA methyltransferase biosensors with microfluidic technology, they have the potential to reduce both the assay time and the required sample volume. Microfluidic DNA methyltransferase activity measurement is a challenge for the future. However, Ronen and Gerber *et al.*<sup>56</sup> have published a preliminary report on a microfluidic-based fluorometric assay technique for studying

DNA methylation *in vitro*. The microfluidic device consists of a  $64 \times 16$  reaction unit array in a flow channel, which is accessed through several input holes and drained into a single output (Fig. 8). The microfluidic device was compartmentalized with micromechanical valves into 16 separate reaction conditions on a single device within isolated columns. For the methylation reaction, a mixture solution containing DNA methyltransferase and SAM was injected into the microfluidic device, and the immobilized DNA substrate was incubated in the mixture solution. After washing, the endonuclease containing reaction buffer was injected and incubated. Finally, the cleaved DNA fragments were washed away and the fluorescence intensity of Cy5-modified DNA was measured. The same platform was then used to demonstrate a two-step approach for the high-throughput *in vitro* identification and characterization of small-molecule inhibitors of DNA methylation. The microfluidic device enabled the authors to perform thousands of simultaneous DNA methylation reactions on a one-chip device.

Various enzymatic activities have been measured with microfluidic technology to obtain quick and highly sensitive results by utilizing a large surface-to-volume ratio. Microfluidic technology is also considered a promising approach for measuring DNA methyltransferase activity. Moreover, in epigenetic research, huge numbers of samples must be evaluated during, for example, epigenetic drug screening. This is a challenge; however, it will be realized in the near future because the simultaneous monitoring of  $64 \times 16$  reactions has already been achieved on a chip.<sup>56</sup>

#### 2.5 Single cell epigenetics

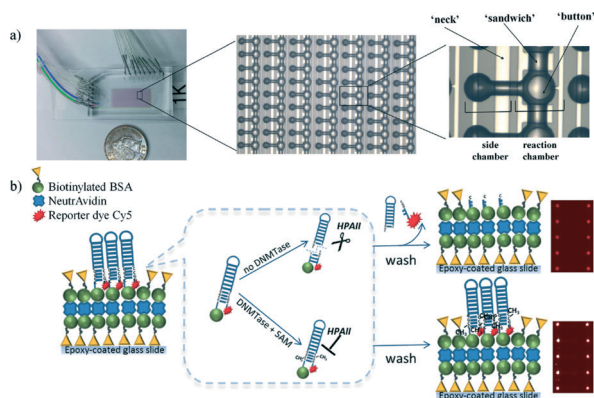
The goal of single cell epigenetics is to analyze information from a single cell to obtain a holistic understanding of the cell population. This reductionist approach allows researchers to unravel the way in which molecular events within a single cell link to the behaviour of tissues, organs,



**Table 2** New methods and devices for determining DNA methyltransferase activity

Detection principle	Target	Response range (U mL <sup>-1</sup> )	Detection limit (U mL <sup>-1</sup> )	Biological application	Signal generator	Ref.	
Electrochemical	Dam	0.1–20	0.04	—	1-Naphthyl phosphate	109	
	Dam	0.075–30	0.02	Human serum	Methylene blue	110	
	Dam	0.27–60	0.27	Human serum	Methylene blue	111	
	Dam	0.05–40	0.031	—	Ferricyanide	112	
	Dam	1–40	0.96	—	Hydroquinone	113	
	M.SssI	0.5–0.6	0.12	Human serum	Aniline	114	
	Dam	1–60	0.31	—	Hydroquinone	115	
	M.SssI	0.28–50	0.28	—	Methylene blue	116	
	Dam	0.04–4	0.004	—	Methylene blue	117	
	M.SssI	0.05–200	0.025	—	Ascorbic acid	118	
	Dam	0.12–20	0.04	—	Methylene blue	119	
	Electrochemiluminescence	M.SssI	1–120	0.05	Cancer human serum	CdS quantum dot	120
		Dam	0.1–100	0.03	—	Tris (2,2'-bipyridine) ruthenium	121
Dam		0.1–50	0.03	—	Luminol	122	
Photo-electrochemical	M.SssI	0.01–150	0.0042	—	CdSe quantum dot	123	
	Dam	0.1–8	0.1	—	Thioflavin	124	
Fluorometric	M.SssI	0.02–40	0.0082	Human serum	Molecular beacon/FAM	125	
	M.SssI	0.01–50	0.0024	HeLa cells	Sybr green I	126	
	Dam	1.2–10	0.57	LB medium	Molecular beacon/FAM	127	
	Dam	0.0005–50	$2 \times 10^{-4}$	<i>E. coli</i> cells	Molecular beacon	128	
	Dam	0–50	0.0025	<i>E. coli</i> cells	FAM	129	
	Dam	0.05–10	0.015	LB medium	FAM	130	
	Dam	0.0005–0.01	$1.5 \times 10^{-4}$	<i>E. coli</i> cells	Molecular beacon/FAM	131	
	Dam	0–15	0.1	—	FAM	132	
	Dam	1–100	1	—	Fluorescent silver nanocluster	133	
	Dam	0.2–20	0.14	—	FAM	134	
	Dam	0.0002–20	$8.6 \times 10^{-5}$	Human serum	Zinc protoporphyrin	135	
	SERS	Dam	0.001–10	$2.57 \times 10^{-4}$	Human serum	Au nanoparticles	136
		M.SssI	0.1–10	0.067	—	Silver nanoparticles	137
		Dam	0.1–10	0.02	—	Mesoporous silica nanoparticles	138
CD spectroscopy	M.SssI	0.5–150	0.27	Human serum	Gold nanoparticles dimer	139	
Surface plasmon resonance	Dam	0.5–120	0.2	HeLa cells	Gold nanorod	140	

Dam, deoxyadenosine methylase; M.SssI, CpG methyltransferase.



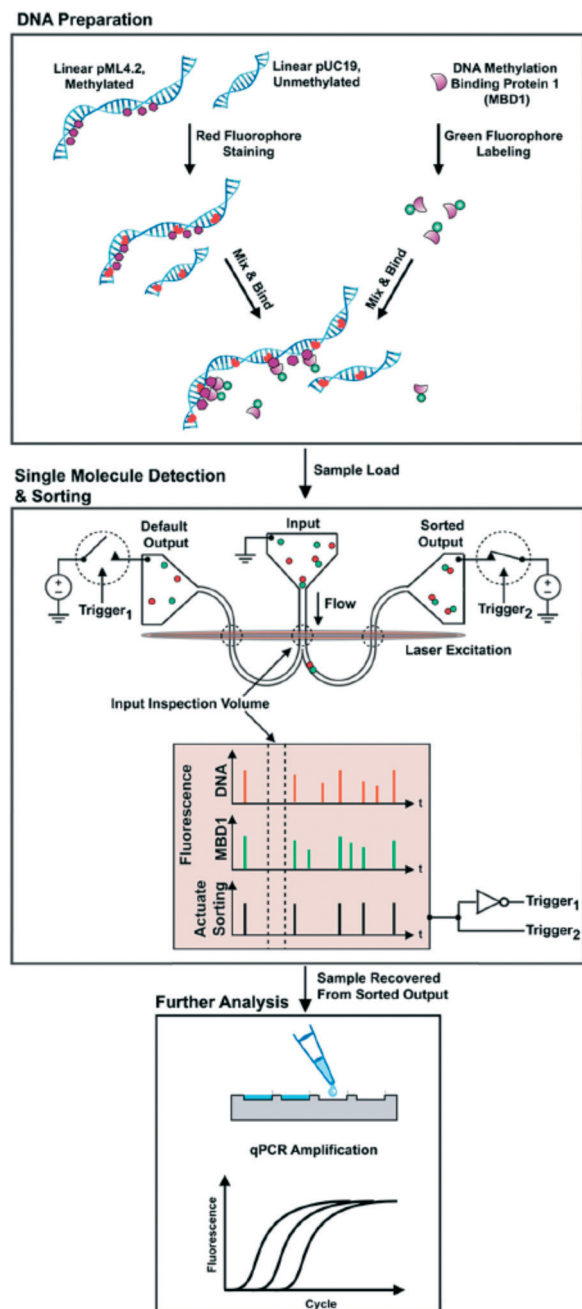
**Fig. 8** a) Photograph and schematic representation of a microfluidic device consisting of flow and control layers. b) Schematic representation of microfluidic-based methylation assay using biotinylated hairpin-shaped DNA probe substrate. The DNA probe is immobilized to the surface through biotin-avidin interactions. The recognition site becomes resistant to *HpaII* activity only when there is a methylation event. Otherwise, the unprotected DNA probe is digested and the unbound Cy5-containing DNA piece is washed out leading to an overall reduction in fluorescence signal. Reproduced from ref. 56 with permission from The Royal Society of Chemistry.

and eventually entire organisms.<sup>143</sup> The small dimensions of microfluidic systems offer a great advantage as regards single cell epigenomics because minimal dilution is required, resulting in a highly sensitive epigenomic analysis. Furthermore, microfluidic systems offer several potential advantages for the study of single cells including facile automation, parallelization and reagent reduction.<sup>144</sup>

As mentioned above, the damage to DNA that occurs during bisulfite conversion is serious. Therefore, direct DNA methylation analysis in a single cell with a bisulfite-based assay requires great skill. ChIP-on-chip, which is a technology that combines chromatin immunoprecipitation with a DNA microarray, is currently used for single cell epigenetics. The results of epigenetic modifications of chromatin by traditional methods usually include blended responses from many cells in a tissue; however, such bulk measures miss the spatial and temporal differences that occur from cell to cell and cannot uncover novel or rare populations of cells.<sup>145</sup> As regards combining micro- and nanofluidic technology, Cipriany and Craighead *et al.*<sup>146</sup> reported a method using nanofluidics and multicolor fluorescence microscopy to detect DNA and histones in individual chromatin fragments at about 10 Mbp min<sup>-1</sup>. They demonstrated its utility for







**Fig. 9** (Top) Schematic of DNA preparation. (Middle) Samples were loaded into the input of a bifurcated nanofluidic device. An applied voltage flowed molecules through the device. As each fluorescently labeled molecule passed through the input inspection volume its fluorescence signature was detected and then evaluated in real time. In this panel, an MBD bound to methylated DNA was identified by its two-color fluorescence signature. This signature actuated a sorting trigger and a pair of opposing switches to direct the molecules toward the sorted output. After a molecule was delivered to the sorted output, the flow was redirected to the default output. (Bottom) At the conclusion of a sorting experiment, material in the sorted output was recovered with a pipette and the amounts of pUC19 and pML4.2 were measured by qPCR analysis.

epigenetic analysis by identifying DNA methylation on individual molecules. They further reported<sup>147</sup> a nanofluidic de-

vice that combines real-time detection and the automated sorting of individual molecules based on their epigenetic state. Fluorescently labeled antibodies or proteins were bound to epigenetic modifications located on histone proteins or DNA, and then the mixture solutions were injected into the nanofluidic device (Fig. 9) to identify these molecules and their corresponding modifications by their fluorescence color signature. Each molecule with a color signature that matches the criteria for collection is then sorted during a brief actuation, or pulse, that redirects the flow to the sorted output. Sorted molecules are collected downstream, and then the collected samples are analyzed by quantitative PCR. They stated that up to 98% accuracy was achieved in sorting molecules from femtogram quantities of genetic material.

### 3. Conclusions and future prospects

In this review article, we have presented and discussed epigenomic research undertaken with microfluidic devices. Epigenetics is a biological application that can take advantage of the features included in microfluidic technology, and it continues to be a fascinating research area. Many examples of application to bio-sensing devices have been reported for measuring DNA methyltransferase activity. This is because DNA methyltransferase activity can be detected by using relatively simple chemical and biological reactions with a methylation-sensitive restriction enzyme. The cleavage with the methylation sensitive restriction enzyme was monitored with electrochemical and optical measurements and involved a relatively minor change in existing biosensors. By employing nanomaterials such as carbon nanotubes, graphene, quantum dots and metal nanoparticles, sensitivity was improved and these results have been reported. Quick and highly sensitive measurements with small sample volumes can be expected by integrating the methods and materials with microfluidics. In the future, microfluidic devices will be reported that employ the above materials, and their device performance is promising. Because most of them are being developed to obtain high sensitivity with a similar approach to conventional affinity biosensors, there have been some problems as regards non-specific adsorption and selectivity when measuring real samples. Unless these problems are overcome, industrial application will be difficult; therefore it might also be useful to integrate pretreatment systems utilizing microfluidic technology.

When measuring base methylation in DNA, the detection principle is somewhat more complicated than that used for methyltransferase activity; therefore coming up with a bio-sensing device for DNA methylation analysis remains a challenging proposition. There have been several reports on PCR-free measurement of DNA methylation. However, the sensitivity and selectivity are insufficient for genomic DNA measurement; therefore results with genomic DNA are limited. It is difficult to integrate all the complicated chemical and biological reactions into a single chip. Therefore, each elemental



technology, for example, genomic extraction, pretreatment, and detection, is currently being developed. Epigenomic analysis in a single cell, which is difficult the conventional analytical technique, may be realized by integrating these devices. This work does not relate solely to biomolecular researchers; it is certain that the need to detect DNA methylation is high in the fields of diagnosis and drug development. The microfluidic approach will provide a promising way to realize a DNA methylation sensor which can obtain epigenomic information quickly and with a high throughput.

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## References

- R. Jaenisch and A. Bird, *Nat. Genet.*, 2003, **33**, 245–254.
- P. A. Jones and S. B. Baylin, *Nat. Rev. Genet.*, 2002, **3**, 415–428.
- R. R. Kanherkar, N. Bhatia-Dey and A. B. Csoka, *Front. Cell Dev. Biol.*, 2014, **2**, 49.
- V. K. Cortessis, D. C. Thomas, A. J. Levine, C. V. Breton, T. M. Mack, K. D. Siegmund, R. W. Haile and P. W. Laird, *Hum. Genet.*, 2012, **131**, 1565–1589.
- L. Hou, X. Zhang, D. Wang and A. Baccarelli, *Int. J. Epidemiol.*, 2012, **41**, 79–105.
- R. D. Hotchkiss, *J. Biol. Chem.*, 1948, **175**, 315–332.
- M. Esteller, *Annu. Rev. Pharmacol. Toxicol.*, 2005, **45**, 629–656.
- K. D. Robertson and A. P. Wolffe, *Nat. Rev. Genet.*, 2000, **1**, 11–19.
- P. A. Jones, *Cancer Res.*, 1996, **56**, 2463–2467.
- J. A. Yoder, C. P. Walsh and T. H. Bestor, *Trends Genet.*, 1997, **13**, 335–340.
- M. Monk, *Dev. Genet.*, 1995, **17**, 188–197.
- S. Ledoux, J. Nalbantoglu and N. R. Cashman, *Mol. Brain Res.*, 1994, **24**, 140–144.
- S. J. Clark, J. Harrison, C. L. Paul and M. Frommer, *Nucleic Acids Res.*, 1994, **22**, 2990–2997.
- S. J. Docherty, O. S. P. Davis, C. M. A. Haworth, R. Plomin and J. Mill, *Methods*, 2010, **52**, 255–258.
- J. G. Herman, J. R. Graff, S. Myohanen, B. D. Nelkin and S. B. Baylin, *Proc. Natl. Acad. Sci. U. S. A.*, 1996, **93**, 9821–9826.
- C. Bock, S. Reither, T. Mikeska, M. Paulsen, J. Walter and T. Lengauer, *Bioinformatics*, 2005, **21**, 4067–4068.
- Z. G. Xiong and P. W. Laird, *Nucleic Acids Res.*, 1997, **25**, 2532–2534.
- A. S. Yang, M. R. H. Estecio, K. Doshi, Y. Kondo, E. H. Tajara and J. P. J. Issa, *Nucleic Acids Res.*, 2004, **32**, e38.
- L. J. Rush and C. Plass, *Anal. Biochem.*, 2002, **307**, 191–201.
- A. D. Riggs, *Cytogenet. Genome Res.*, 2002, **99**, 17–24.
- R. Holliday and J. E. Pugh, *Science*, 1975, **187**, 226–232.
- M. Wigler, D. Levy and M. Perucho, *Cell*, 1981, **24**, 33–40.
- R. Stein, Y. Gruenbaum, Y. Pollack, A. Razin and H. Cedar, *Proc. Natl. Acad. Sci. U. S. A.*, 1982, **79**, 61–65.
- T. Bestor, A. Laudano, R. Mattaliano and V. Ingram, *J. Mol. Biol.*, 1988, **203**, 971–983.
- M. Okano, D. W. Bell, D. A. Haber and E. Li, *Cell*, 1999, **99**, 247–257.
- T. H. Bestor, *EMBO J.*, 1992, **11**, 2611–2617.
- M. Okano, S. P. Xie and E. Li, *Nat. Genet.*, 1998, **19**, 219–220.
- Q. Q. Lai, M. D. Liu, C. C. Gu, H. G. Nie, X. J. Xu, Z. H. Li, Z. Yang and S. M. Huang, *Analyst*, 2016, **141**, 1383–1389.
- Y. Zhao, F. Chen, Y. Wu, Y. Dong and C. Fan, *Biosens. Bioelectron.*, 2013, **42**, 56–61.
- T. Liu, J. Zhao, D. Zhang and G. Li, *Anal. Chem.*, 2010, **82**, 229–233.
- N. B. Muren and J. K. Barton, *J. Am. Chem. Soc.*, 2013, **135**, 16632–16640.
- P. S. Dittrich and A. Manz, *Nat. Rev. Drug Discovery*, 2006, **5**, 210–218.
- B. H. Weigl, R. L. Bardell and C. R. Cabrera, *Adv. Drug Delivery Rev.*, 2003, **55**, 349–377.
- J. K. Oh, R. Drumright, D. J. Siegwart and K. Matyjaszewski, *Prog. Polym. Sci.*, 2008, **33**, 448–477.
- W. M. Saltzman and W. L. Olbricht, *Nat. Rev. Drug Discovery*, 2002, **1**, 177–186.
- A. Nisar, N. AftuIpurkar, B. Mahaisavariya and A. Tuantranont, *Sens. Actuators, B*, 2008, **130**, 917–942.
- D. B. Weibel, W. R. DiLuzio and G. M. Whitesides, *Nat. Rev. Microbiol.*, 2007, **5**, 209–218.
- A. Bange, H. B. Halsall and W. R. Heineman, *Biosens. Bioelectron.*, 2005, **20**, 2488–2503.
- M.-I. Mohammed and M. P. Y. Desmulliez, *Lab Chip*, 2011, **11**, 569–595.
- C. S. Zhang, J. L. Xu, W. L. Ma and W. L. Zheng, *Biotechnol. Adv.*, 2006, **24**, 243–284.
- C. E. Sims and N. L. Allbritton, *Lab Chip*, 2007, **7**, 423–440.
- D. Wang and S. Bodovitz, *Trends Biotechnol.*, 2010, **28**, 281–290.
- S. Lindstrom and H. Andersson-Svahn, *Lab Chip*, 2010, **10**, 3363–3372.
- A. J. Tudos, G. A. J. Besselink and R. B. M. Schasfoort, *Lab Chip*, 2001, **1**, 83–95.
- F. B. Myers and L. P. Lee, *Lab Chip*, 2008, **8**, 2015–2031.
- A. M. Foudeh, T. F. Didar, T. Veres and M. Tabrizian, *Lab Chip*, 2012, **12**, 3249–3266.
- T. Tian, J. Li, Y. Song, L. Zhou, Z. Zhu and C. J. Yang, *Lab Chip*, 2016, **16**, 1139–1151.
- D. R. Gossett, W. M. Weaver, A. J. Mach, S. C. Hur, H. T. K. Tse, W. Lee, H. Amini and D. Di Carlo, *Anal. Bioanal. Chem.*, 2010, **397**, 3249–3267.
- C. W. Shields, C. D. Reyes and G. P. Lopez, *Lab Chip*, 2015, **15**, 1230–1249.
- N. Lion, T. C. Rohner, L. Dayon, I. L. Arnaud, E. Damoc, N. Youhnovski, Z. Y. Wu, C. Roussel, J. Josserand, H. Jensen,





- J. S. Rossier, M. Przybylski and H. H. Girault, *Electrophoresis*, 2003, **24**, 3533–3562.
- 51 P. A. Auroux, Y. Koc, A. deMello, A. Manz and P. J. R. Day, *Lab Chip*, 2004, **4**, 534–546.
- 52 L. Chen, A. Manz and P. J. R. Day, *Lab Chip*, 2007, **7**, 1413–1423.
- 53 C. W. Price, D. C. Leslie and J. P. Landers, *Lab Chip*, 2009, **9**, 2484–2494.
- 54 B. Weigl, G. Domingo, P. LaBarre and J. Gerlach, *Lab Chip*, 2008, **8**, 1999–2014.
- 55 P. Y. Liu, L. K. Chin, W. Ser, H. F. Chen, C. M. Hsieh, C. H. Lee, K. B. Sung, T. C. Ayi, P. H. Yap, B. Liedberg, K. Wang, T. Bourouina and Y. Leprince-Wang, *Lab Chip*, 2016, **16**, 634–644.
- 56 M. Ronen, D. Avrahami and D. Gerber, *Lab Chip*, 2014, **14**, 2354–2362.
- 57 D. Gerber, S. J. Maerkl and S. R. Quake, *Nat. Methods*, 2009, **6**, 71–74.
- 58 X. Lu, C.-X. Song, K. Szulwach, Z. Wang, P. Weidenbacher, P. Jin and C. He, *J. Am. Chem. Soc.*, 2013, **135**, 9315–9317.
- 59 Y. Yu, S. Blair, D. Gillespie, R. Jensen, D. Myszyka, A. H. Badran, I. Ghosh and A. Chagovetz, *Anal. Chem.*, 2010, **82**, 5012–5019.
- 60 L. S. Kristensen and L. L. Hansen, *Clin. Chem.*, 2009, **55**, 1471–1483.
- 61 H. A. Stone and S. Kim, *AIChE J.*, 2001, **47**, 1250–1254.
- 62 A. Stark, D. J. Shin, T. Pisanic, II, K. Hsieh and T.-H. Wang, *Biomed. Microdevices*, 2016, **18**, 5.
- 63 Y. Shin, A. P. Perera, C. C. Wong and M. K. Park, *Lab Chip*, 2014, **14**, 359–368.
- 64 A. De, W. Sparreboom, A. van den Berg and E. T. Carlen, *Biomicrofluidics*, 2014, **8**, 054119.
- 65 J. Yoon, M. K. Park, T. Y. Lee, Y.-J. Yoon and Y. Shin, *Lab Chip*, 2015, **15**, 3530–3539.
- 66 R. M. Brena, H. Auer, K. Kornacker, B. Hackanson, A. Raval, J. C. Byrd and C. Plass, *Nucleic Acids Res.*, 2006, **34**, e17.
- 67 R. M. Brena, H. Auer, K. Kornacker and C. Plass, *Nat. Protoc.*, 2006, **1**, 52–58.
- 68 R. M. Brena and C. Plass, *Methods Mol. Biol.*, 2009, **507**, 257–269.
- 69 H.-C. Chen, Y.-S. Chang, S.-J. Chen and P.-L. Chang, *J. Chromatogr.*, 2012, **1230**, 123–129.
- 70 M.-H. Yu, Y.-C. Huang and P.-L. Chang, *Electrophoresis*, 2014, **35**, 2378–2385.
- 71 K. Tanaka, K. Tainaka, T. Umemoto, A. Nomura and A. Okamoto, *J. Am. Chem. Soc.*, 2007, **129**, 14511–14517.
- 72 *DNA Methylation - From Genomics to Technology*, ed. T. Tatarinova and O. Kerton, Rijeka, 2012.
- 73 H. Yanagisawa, R. Kurita, T. Yoshida, T. Kamata and O. Niwa, *Sens. Actuators, B*, 2015, **221**, 816–822.
- 74 M. Daneshpour, L. S. Moradi, P. Izadi and K. Omidfar, *Biosens. Bioelectron.*, 2016, **77**, 1095–1103.
- 75 H. Yin, Y. Zhou, Z. Yang, Y. Guo, X. Wang, S. Ai and X. Zhang, *Sens. Actuators, B*, 2015, **221**, 1–6.
- 76 A. H. Nguyen and S. J. Sim, *Biosens. Bioelectron.*, 2015, **67**, 443–449.
- 77 R. Kurita, H. Yanagisawa, K. Yoshioka and O. Niwa, *Anal. Chem.*, 2015, **87**, 11581–11586.
- 78 R. Kurita, H. Yanagisawa, K. Yoshioka and O. Niwa, *Biosens. Bioelectron.*, 2015, **70**, 366–371.
- 79 R. M. Hawk and A. M. Armani, *Biosens. Bioelectron.*, 2015, **65**, 198–203.
- 80 W. Huang, C.-B. Qi, S.-W. Lv, M. Xie, Y.-Q. Feng, W.-H. Huang and B.-F. Yuan, *Anal. Chem.*, 2016, **88**, 1378–1384.
- 81 W. Huang, J. Xiong, Y. Yang, S.-M. Liu, B.-F. Yuan and Y.-Q. Feng, *RSC Adv.*, 2015, **5**, 64046–64054.
- 82 Y. Tang, S.-J. Zheng, C.-B. Qi, Y.-Q. Feng and B.-F. Yuan, *Anal. Chem.*, 2015, **87**, 3445–3452.
- 83 M. Basanta-Sanchez, S. Temple, S. A. Ansari, A. D'Amico and P. F. Agris, *Nucleic Acids Res.*, 2016, **44**, e26.
- 84 F. Yuan, X.-H. Zhang, J. Nie, H.-X. Chen, Y.-L. Zhou and X.-X. Zhang, *Chem. Commun.*, 2016, **52**, 2698–2700.
- 85 M. Giel-Pietraszuk, M. Insinska-Rak, A. Golczak, M. Sikorski, M. Barciszewska and J. Barciszewski, *Acta Biochim. Pol.*, 2015, **62**, 281–286.
- 86 S. Chen, Y. Dou, Z. Zhao, F. Li, J. Su, C. Fan and S. Song, *Anal. Chem.*, 2016, **88**, 3476–3480.
- 87 Y. Zhou, Z. Yang, X. Li, Y. Wang, H. Yin and S. Ai, *Electrochim. Acta*, 2015, **174**, 647–652.
- 88 Y. Wang, E. J. H. Wee and M. Trau, *Chem. Commun.*, 2016, **52**, 3560–3563.
- 89 P. Wang, P. Han, L. Dong and X. Miao, *Electrochem. Commun.*, 2015, **61**, 36–39.
- 90 M. Dadmehr, M. Hosseini, S. Hosseinkhani, M. R. Ganjali and R. Sheikhejad, *Biosens. Bioelectron.*, 2015, **73**, 108–113.
- 91 L. G. Acevedo, A. Sanz and M. A. Jelinek, *Epigenomics*, 2011, **3**, 93–101.
- 92 D. Serre, B. H. Lee and A. H. Ting, *Nucleic Acids Res.*, 2010, **38**, 391–399.
- 93 S. S. Nair, M. W. Coolen, C. Stirzaker, J. Z. Song, A. L. Statham, D. Strbenac, M. D. Robinson and S. J. Clark, *Epigenetics*, 2011, **6**, 34–44.
- 94 K. Tanaka, K. Tainaka, T. Kamei and A. Okamoto, *J. Am. Chem. Soc.*, 2007, **129**, 5612–5620.
- 95 S. Bareyt and T. Carell, *Angew. Chem., Int. Ed.*, 2008, **47**, 181–184.
- 96 A. Okamoto, K. Tainaka and T. Kamei, *Org. Biomol. Chem.*, 2006, **4**, 1638–1640.
- 97 B. W. Heimer, T. A. Shatova, J. K. Lee, K. Kaastrup and H. D. Sikes, *Analyst*, 2014, **139**, 3695–3701.
- 98 C.-H. Wang, H.-C. Lai, T.-M. Liou, K.-F. Hsu, C.-Y. Chou and G.-B. Lee, *Microfluid. Nanofluid.*, 2013, **15**, 575–585.
- 99 C. Bock, E. M. Tomazou, A. B. Brinkman, F. Mueller, F. Simmer, H. Gu, N. Jaeger, A. Gnirke, H. G. Stunnenberg and A. Meissner, *Nat. Biotechnol.*, 2010, **28**, 1106–U1196.
- 100 J. Borgel, S. Guibert, Y. Li, H. Chiba, D. Schuebeler, H. Sasaki, T. Forne and M. Weber, *Nat. Genet.*, 2010, **42**, 1093–1100.
- 101 L. Zhang, K. E. Szulwach, G. C. Hon, C.-X. Song, B. Park, M. Yu, X. Lu, Q. Dai, X. Wang, C. R. Street, H. Tan, J.-H. Min, B. Ren, P. Jin and C. He, *Nat. Commun.*, 2013, **4**, 1517.



- 102 B. Chowdhury, I.-H. Cho, N. Hahn and J. Irudayaraj, *Anal. Chim. Acta*, 2014, **852**, 212–217.
- 103 X. L. Wang, Y. L. Song, M. Y. Song, Z. X. Wang, T. Li and H. L. Wang, *Anal. Chem.*, 2009, **81**, 7885–7891.
- 104 Z. Wang, X. Wang, S. Liu, J. Yin and H. Wang, *Anal. Chem.*, 2010, **82**, 9901–9908.
- 105 C. Ge, Z. Fang, J. Chen, J. Liu, X. Lu and L. Zeng, *Analyst*, 2012, **137**, 2032–2035.
- 106 D. D. Deobagkar, C. Panikar, S. N. Rajpathak, N. S. Shaiwale and S. Mukherjee, *Methods*, 2012, **56**, 260–267.
- 107 A. Kelkar and D. Deobagkar, *Epigenetics*, 2009, **4**, 311–316.
- 108 R. Kurita and O. Niwa, *Anal. Chem.*, 2012, **84**, 7533–7538.
- 109 H. Wu, S. Liu, J. Jiang, G. Shen and R. Yu, *Chem. Commun.*, 2012, **48**, 6280–6282.
- 110 L. Hong, J. Wan, X. Zhang and G. Wang, *Talanta*, 2016, **152**, 228–235.
- 111 P. Liu, D. Wang, Y. Zhou, H. Wang, H. Yin and S. Ai, *Biosens. Bioelectron.*, 2016, **80**, 74–78.
- 112 X. Li, Z. Xie, W. Wang, Y. Zhou, H. Yin, Z. Yang and S. Ai, *Anal. Methods*, 2016, **8**, 2771–2777.
- 113 P. Liu, M. Liu, H. Yin, Y. Zhou and S. Ai, *Sens. Actuator, B*, 2015, **220**, 101–106.
- 114 L. Zhang, M. Wei, C. Gao, W. Wei, Y. Zhang and S. Liu, *Biosens. Bioelectron.*, 2015, **73**, 188–194.
- 115 Z. Yang, L. Xie, H. Yin, Y. Zhou and S. Ai, *Microchim. Acta*, 2015, **182**, 2607–2613.
- 116 P. Liu, J. Pang, H. Yin and S. Ai, *Anal. Chim. Acta*, 2015, **879**, 34–40.
- 117 W. Li, X. Liu, T. Hou, H. Li and F. Li, *Biosens. Bioelectron.*, 2015, **70**, 304–309.
- 118 J. Zhou, X. Zhang, E. Xiong, P. Yu and J. Chen, *Chem. Commun.*, 2015, **51**, 5081–5084.
- 119 X. Wang, X. Liu, T. Hou, W. Li and F. Li, *Sens. Actuators, B*, 2015, **208**, 575–580.
- 120 H. Zhou, T. Han, Q. Wei and S. Zhang, *Anal. Chem.*, 2016, **88**, 2976–2983.
- 121 X. Luo, Y. Li, J. Zheng, H. Qi, Z. Liang and X. Ning, *Chem. Commun.*, 2015, **51**, 9487–9490.
- 122 H.-F. Zhao, R.-P. Liang, J.-W. Wang and J.-D. Qiu, *Biosens. Bioelectron.*, 2015, **63**, 458–464.
- 123 Q. Shen, L. Han, G. Fan, E. S. Abdel-Halim, L. Jiang and J.-J. Zhu, *Biosens. Bioelectron.*, 2015, **64**, 449–455.
- 124 C. Ma, H. Liu, W. Li, H. Chen, S. Jin, J. Wang and J. Wang, *Mol. Cell. Probes*, 2016, **30**, 118–121.
- 125 W. Cui, L. Wang and W. Jiang, *Biosens. Bioelectron.*, 2016, **77**, 650–655.
- 126 H. Zhao, L. Wang and W. Jiang, *Chem. Commun.*, 2016, **52**, 2517–2520.
- 127 W. Zhang, X. Zu, Y. Song, Z. Zhu and C. J. Yang, *Analyst*, 2016, **141**, 579–584.
- 128 Q. Xue, Y. Zhang, S. Xu, H. Li, L. Wang, R. Li, Y. Zhang, Q. Yue, X. Gu, S. Zhang, J. Liu and H. Wang, *Analyst*, 2015, **140**, 7637–7644.
- 129 F. Tang, X.-W. Xing, J.-M. Chu, Q. Yuan, X. Zhou, Y.-Q. Feng and B.-F. Yuan, *Analyst*, 2015, **140**, 4636–4641.
- 130 Y. Zhang, W.-j. Xu, Y.-p. Zeng and C.-y. Zhang, *Chem. Commun.*, 2015, **51**, 13968–13971.
- 131 Q. Xue, L. Wang and W. Jiang, *Chem. Commun.*, 2015, **51**, 13538–13541.
- 132 Y. Ma, L. Chen, L. Zhang, S. Liao and J. Zhao, *Analyst*, 2015, **140**, 4076–4082.
- 133 W. Liu, H. Lai, R. Huang, C. Zhao, Y. Wang, X. Weng and X. Zhou, *Biosens. Bioelectron.*, 2015, **68**, 736–740.
- 134 H. Deng, X. Yang and Z. Gao, *Analyst*, 2015, **140**, 3210–3215.
- 135 Q. Xue, Y. Lv, S. Xu, Y. Zhang, L. Wang, R. Li, Q. Yue, H. Li, X. Gu, S. Zhang and J. Liu, *Biosens. Bioelectron.*, 2015, **66**, 547–553.
- 136 Y. Li, C. Yu, H. Han, C. Zhao and X. Zhang, *Biosens. Bioelectron.*, 2016, **81**, 111–116.
- 137 P. P. Hu, H. Liu, S. J. Zhen, C. M. Li and C. Z. Huang, *Biosens. Bioelectron.*, 2015, **73**, 228–233.
- 138 X. Wang, M. Cui, H. Zhou and S. Zhang, *Chem. Commun.*, 2015, **51**, 13983–13985.
- 139 Y. Liu, M. Wei, L. Zhang, W. Wei, Y. Zhang and S. Liu, *Chem. Commun.*, 2015, **51**, 14350–14353.
- 140 X. Li, T. Song and X. Guo, *Analyst*, 2015, **140**, 6230–6233.
- 141 M. Esteller, *Oncogene*, 2002, **21**, 5427–5440.
- 142 W. Li, P. Wu, H. Zhang and C. Cai, *Anal. Chem.*, 2012, **84**, 7583–7590.
- 143 S. J. Husic, S. K. Murthy and A. N. Koppes, *Anal. Chem.*, 2016, **88**, 354–380.
- 144 A. K. White, K. A. Heyries, C. Doolin, M. VanInsberghe and C. L. Hansen, *Anal. Chem.*, 2013, **85**, 7182–7190.
- 145 M. Dhar, R. Khojah, A. Tay and D. Di Carlo, *Lab Chip*, 2015, **15**, 4109–4113.
- 146 B. R. Cipriany, R. Zhao, P. J. Murphy, S. L. Levy, C. P. Tan, H. G. Craighead and P. D. Soloway, *Anal. Chem.*, 2010, **82**, 2480–2487.
- 147 B. R. Cipriany, P. J. Murphy, J. A. Hagarman, A. Cerf, D. Latulippe, S. L. Levy, J. J. Benitez, C. P. Tan, J. Topolancik, P. D. Soloway and H. G. Craighead, *Proc. Natl. Acad. Sci. U. S. A.*, 2012, **109**, 8477–8482.

