



Cite this: RSC Adv., 2015, 5, 55561

Received 24th April 2015  
 Accepted 17th June 2015

DOI: 10.1039/c5ra11431d  
[www.rsc.org/advances](http://www.rsc.org/advances)

## Low-cost optical manipulation using hanging droplets of PDMS†

Craig McDonald\* and David McGloin

We propose and demonstrate a low-cost optical micromanipulation system that makes use of simple microfabricated components coupled to a smartphone camera for imaging. Layering hanging droplets of polydimethylsiloxane (PDMS) on microscope coverslips, and curing with a 100 W bulb, creates lenses capable of optical trapping. Optically trapped 3.93  $\mu\text{m}$  silica beads were imaged with a second hanging droplet lens, doped with 1400  $\mu\text{g mL}^{-1}$  Sudan II dye. Through doping, a lens with an integrated long-pass filter that effectively blocks the 532 nm trapping light was produced. Illumination was provided by shining a lamp into polystyrene foam packaging, perpendicular to the imaging path, producing a diffuse light source. We observed two dimensional trapping and report a  $Q$  value of  $\sim 8.9 \times 10^{-3}$ . The techniques here are an addition to the growing body of work on low cost and adaptable microfluidics.

### Introduction

Light microscopes have become ubiquitous in modern research laboratories. Through their combination with optical tweezers, high-end systems which provide insight into the physical, biological and chemical processes occurring in single molecules,<sup>1</sup> aerosols<sup>2</sup> and liquids<sup>3</sup> have been created. However, these sophisticated systems come with an associated high cost, thus limiting their use both in research labs throughout the world (especially the developing world) but also in pedagogical settings.

The development of elastomeric optics using polydimethylsiloxane (PDMS)<sup>4</sup> has provided a high quality, low-cost, alternative to many optical components. PDMS has a high transparency (>95%) within the visible wavelength range and a high refractive index ( $n = 1.47\text{--}1.55$ ), making it an ideal material to fashion lenses from. The low moulding temperature (<100 °C) of PDMS negates the need for specialised high temperature equipment, making it easy to work with in the lab.<sup>4</sup> Elastomeric optics have found use in an increasing number of novel applications such as a rubber microscope,<sup>5</sup> biologically inspired wide field lenses<sup>6</sup> and a low-cost digital dermascope, which makes use of a mobile phone with added lenses fabricated from hanging droplets of PDMS.<sup>7</sup>

With the unprecedented growth of the mobile phone market, low-cost miniature microscopes that exploit the high quality digital camera of many mobile phones have been developed.<sup>8–11</sup>

Much recent work in the lab on a chip field makes use of smartphone sensing capabilities.<sup>12</sup>

Liquid droplets can be used to magnify small objects.<sup>13,14</sup> A hanging droplet is formed when the interfacial energies (liquid, air and solid surface) and gravity reach equilibrium.<sup>14,15</sup> By repeatedly adding and curing a hanging PDMS droplet, Lee *et al.* formed low-cost elastomer lenses which were able to resolve structures as small as 4  $\mu\text{m}$ .<sup>7</sup>

In this paper, we present a low-cost and low-tech method of creating PDMS droplet lenses and use these droplet lenses as the basis of a basic optical trap. We use a second droplet lens, doped with Sudan II dye, and a commercial smartphone to image optically trapped 3.93  $\mu\text{m}$  silica beads. Doping of PDMS with Sudan II dye, prior to moulding, produces a long pass filter with negligible autofluorescence.<sup>16</sup> Integration of the imaging lens and long pass filter allowed for a more compact system, while still effectively blocking the 532 nm trapping light, preventing saturation of the phone camera. Illumination was provided by shining a lamp into polystyrene foam packaging, perpendicular to the imaging path, producing a diffuse light source that was sufficient for resolving the silica beads. At all stages of fabrication of the system we present methods which make use of materials that are often discarded or overlooked in the lab, or are easily attainable for a low cost. Neglecting the cost of a laser, which could be replaced by a laser pointer or other low cost alternative, our system can be constructed for approximately £23.23, a full cost breakdown of all components required is available in the ESI.† We also present measurements of the trapping ability and efficiency of a droplet lens based optical manipulation system.

Our work fits in very well with the burgeoning field of microfluidics for developing world, real world, applications<sup>17</sup>

SUPA, Division of Physics, University of Dundee, Nethergate, Dundee, Scotland. E-mail: [cymcdonald@dundee.ac.uk](mailto:cymcdonald@dundee.ac.uk)

† Electronic supplementary information (ESI) available. See DOI: [10.1039/c5ra11431d](https://doi.org/10.1039/c5ra11431d)



and should integrate straightforwardly with existing optofluidic devices and urban sensing systems.

## Materials and methods

### Fabricating the trapping lens with a hanging droplet

The trapping lens of our optical manipulation system was formed from hanging droplets of PDMS, which had been prepared using the typical soft lithography PDMS procedure, and followed similar steps as those outlined by Lee *et al.*,<sup>7</sup> and shown in Fig. 1(a)–(c). That is to say, PDMS monomer and hardener were mixed at a ratio of 10 : 1 v/v (Sylgard 184 Silicone Elastomer kit, Dow Corning, Coventry, UK) and then placed in a vacuum desiccator until all bubbles were removed. A 1 mL syringe (BD Plastipak, Ref: 300013) was carefully filled with PDMS and pressure applied until a single drop (<100  $\mu$ L) fell from the syringe on to a microscope coverslip, thickness no. 1. The microscope slide was immediately inverted and suspended (~20 mm) above a sheet of tin foil on the lab bench. Any excess PDMS falls from the slide until single drips are formed.

An anglepoise lamp was used to lower a 100 W incandescent light bulb to ~20 mm above the microscope slide, to provide heat for the curing step, while the tin foil reflected the heat back towards the droplet lens. Temperatures in excess of 100 °C could be reached, with temperature crudely controlled by raising and lowering the light bulb. Droplet lenses were left in the “oven” until set, which took up to 15 minutes, at temperatures ranging from 70–80 °C. In order to shorten the focal length and increase the numerical aperture (NA) of the lens, up to four droplets were layered one on top of each other, with each droplet cured before the next was applied. Due to the maximum surface tension that the droplet can hold before falling, the eventual droplet shape at the apex of the lens resembles that of a parabola, with a curvature that increases with layer number. The fabricated trapping lens is shown in Fig. 1(d) and cost

approximately £0.06 per lens, including the microscope cover glass used as the support layer.<sup>‡</sup>

The length of the droplet lens ( $L$ ) was found to vary, with typical measured values of  $8.48 \pm 0.19$  mm and  $7.38 \pm 0.15$  mm. However, the diameter of the entrance pupil ( $D$ ) and back aperture (BA) was found to remain roughly constant, with average values of, respectively,  $2.62 \pm 0.27$  mm and  $6.1 \pm 0.2$  mm. This led to a variation in measured focal lengths of different lenses, with used trapping lenses having a focal length  $0.9 \pm 0.21$  mm and  $1.0 \pm 0.26$  mm. The effective NA of these lenses was estimated as  $0.70 \pm 0.17$  and  $0.68 \pm 0.18$ .

### Combined long-pass filter and imaging lens fabrication

To image the optically trapped beads with a droplet lens and a mobile phone camera, it was necessary to filter the trapping light in order to prevent saturation of the camera. This was achieved by doping the PDMS mixture with  $1400 \mu\text{g mL}^{-1}$  Sudan II dye prior to moulding. 14 mg of Sudan II dye (Sigma-Aldrich, Gillingham, UK) was first dissolved in ~1 mL of toluene and then added to premixed PDMS monomer and hardener, ratio of 10 : 1 v/v, to give a dye-loading of  $1400 \mu\text{g mL}^{-1}$ .<sup>16</sup> Manual mixing was continued until a uniform PDMS colour was observed. A hanging droplet lens was then fabricated, using the coloured PDMS, at an increased cost of £0.08 per lens, by following the steps outlined above, the result of which is shown in Fig. 1(e).

### Illumination and optical manipulation setup assembly

Our experimental set-up is shown in Fig. 2 and makes use of a 1.5 W (maximum output) 532 nm solid-state laser (Model: Ventus, Laser Quantum) as the trapping source. No expansion optics were used before the droplet lens in order to keep the system as simple as possible. A 50 : 50 beam splitter (EBS1, Thorlabs, £23.08) was used to reflect the trapping light up to the clear PDMS droplet lens and transmit the white light illumination. Transmission microscopy, where the sample is illuminated from below and imaged from above, was chosen as it was necessary to place the mobile phone camera in direct contact with the imaging lens.

Illumination of the sample was achieved by shining a lamp into polystyrene foam packaging<sup>§</sup> perpendicular to the imaging path, Fig. 2. This produced diffuse light, which was sufficient to illuminate the sample without saturating the camera. Images presented in this paper were achieved through illumination with a Thorlabs OSL1-EC fibre illuminator as it was convenient. We found that stray laser light was reflecting from the foam packaging and illuminating the sample with scattered laser light and reducing the image contrast. To counteract this effect we made a PDMS filter, consisting of a single droplet of doped PDMS on a microscope coverslip and cured in a non-inverted

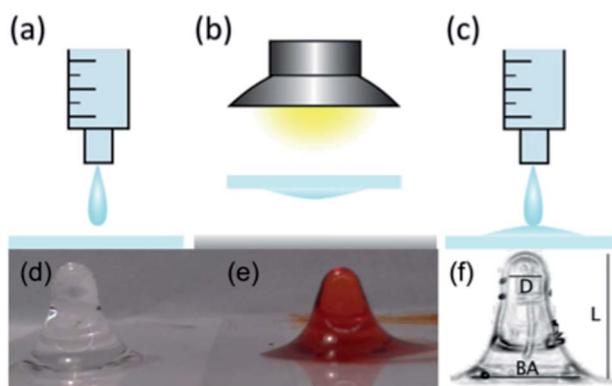


Fig. 1 Steps used to fabricate a droplet lens: (a) droplet of PDMS from syringe, deposited on microscope coverslip; (b) coverslip inverted and suspended above tin foil, 100 W incandescent light bulb used to cure PDMS; (c) additional droplet of PDMS deposited on top of the cured drop. Steps (b) and (c) are repeated to increase droplet curvature. In our system, four invert and cure steps were performed. Fabricated lenses used for (d) trapping and (e) imaging are shown, along with (f) a schematic of how lenses were measured.

<sup>‡</sup> It is assumed that the end user is able to supply tin foil and a lightbulb.

<sup>§</sup> Illumination can be provided from any sufficiently bright lamp – bike lamps, torches and camera flash from mobile phone were all successfully tested. If discarded polystyrene foam packaging cannot be found, it can be purchased for approximately £0.02 per use.



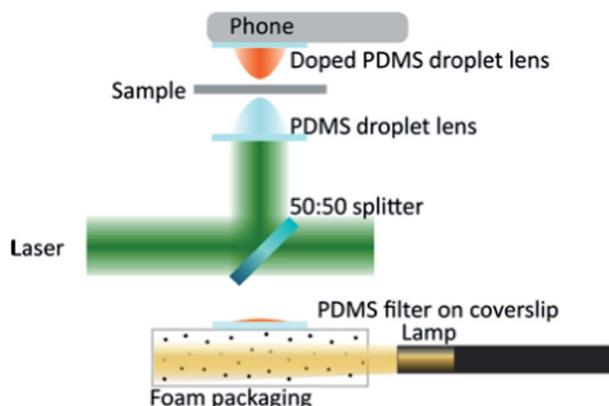


Fig. 2 Experimental system for optical trap based on PDMS droplet lenses.

geometry. This droplet filter was placed in the illumination pathway, preventing the scatter from degrading the image quality.

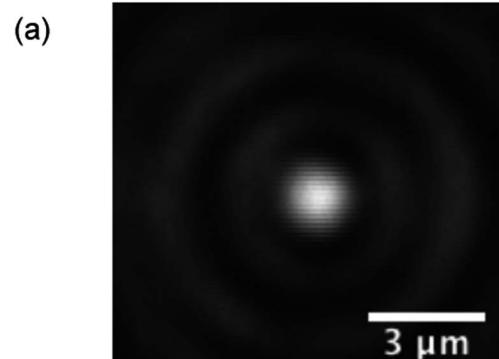
## Results and discussion

### Optical manipulation using a drip lens

Initially, the focal spot produced by the drip lens was investigated to ensure a spot of sufficient quality to trap was produced. A Mitutoyo 0.55 NA 100 $\times$  long working distance objective was used to image the focal spot on to a CCD camera. Fig. 3 shows the experimental airy disk obtained from a droplet lens, the focal length of which was measured as  $0.9 \pm 0.2$  mm, giving an estimated effective NA of  $0.70 \pm 0.17$ .

A suspension of 3.93  $\mu\text{m}$  diameter silica beads in deionised water, between two microscope coverslips separated by a vinyl spacer, was used as the trapping sample. The particle size was chosen as previous studies<sup>7</sup> have shown the smallest resolvable structure with droplet lenses to be 4  $\mu\text{m}$ . Fig. 4 shows a 3.93  $\mu\text{m}$  silica bead which has been trapped using a PDMS droplet lens. We found that the minimum power to trap these beads was  $34.0 \pm 0.4$  mW, in the focal spot. Particle height was observed to change as a function of power, indicating two dimensional trapping.

In order to examine the ability of the droplet based trap to function as a more robust research grade instrument, a simple measure of the transverse  $Q$  value<sup>18</sup> of the trapping spot was made. The simplest method to find the transverse  $Q$  value is to laterally displace the trapped sphere at increasing velocity until it falls from the trap, which is equivalent to the sphere remaining stationary while the surrounding fluid is moved. The applied drag force at the point of escape is equal to the trapping force of the optical manipulation system. Moving the sample with increasing velocity increases the drag force acting on the acting on the sphere, given by Stokes' law. Making use of the Stokes' drag technique, and the expression  $F = Q(n_m P/c)$ , where  $F$  and  $P$  are, respectively, the trapping force and power,  $n_m$  is the suspending medium's refractive index and  $c$  being the speed of light, the trapping efficiency of the system was determined.



(a) Intensity of Airy disk

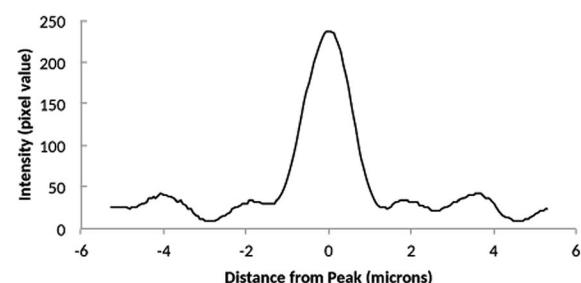


Fig. 3 (a) Airy disk produced by PDMS droplet lens, imaged with Mitutoyo 0.55 NA 100 $\times$  long working distance objective. (b) Line profile through centre of Airy disk.

3.93  $\mu\text{m}$  beads were trapped with  $58.48 \pm 0.08$  mW of laser power and a  $Q$  value of  $0.0089 \pm 0.0001$  was measured.

The low  $Q$  value indicates that quantitative measurements, or experiments which require high optical forces, would not be suited to our low cost, droplet lens based optical manipulation system. However, qualitative measurements and trial experiments could be easily performed.

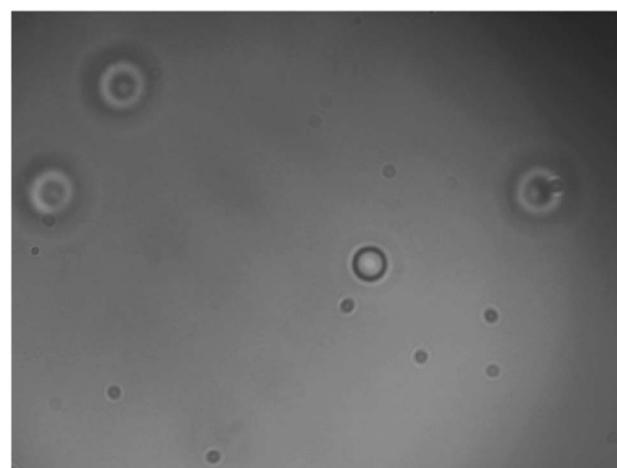


Fig. 4 3.93  $\mu\text{m}$  silica bead (in focus), optically trapped in two dimensions with a clear PDMS droplet lens, among untrapped, and therefore out of focus, beads. Imaged with Mitutoyo 0.55 NA 100 $\times$  long working distance objective. A video of the trapped bead is available in the ESI.†



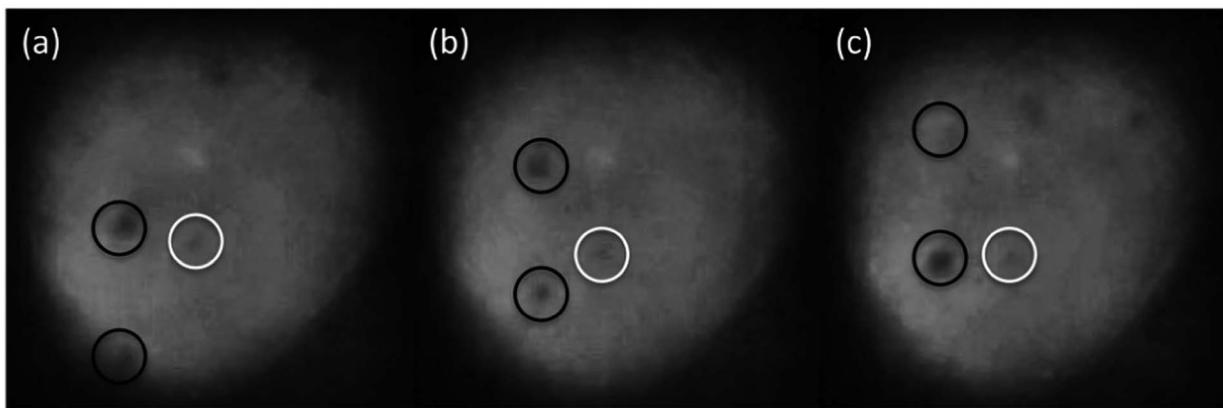


Fig. 5 (a)–(c) show an optically trapped, in two dimensions,  $3.93\text{ }\mu\text{m}$  silica bead (circled in white) moving between two untrapped, reference, beads (circled in black). Beads have been trapped with a clear PDMS droplet lens and imaged with a Sudan II doped PDMS droplet lens attached to a smartphone camera.

### Drip lens imaging

The Mitutoyo objective and CCD camera were removed and replaced with the doped PDMS droplet lens and the camera from a Samsung Galaxy S3 Mini smartphone.<sup>¶</sup> At first, the trapping laser was turned off to ensure that the addition of Sudan II dye did not negatively impact the imaging ability of the lens. Using the macro photography autofocus and digital zoom features on the smartphone camera, the  $3.93\text{ }\mu\text{m}$  beads were resolvable. When exploiting the camera's  $4\times$  digital zoom, each pixel was found to correspond to  $0.22 \pm 0.1\text{ }\mu\text{m}$ .

The laser was turned on and power slowly increased, while the smartphone camera was monitored for any sign of laser light transmitted through the filter lens. Trap power was increased until optical trapping was observed, Fig. 5. Trap power was further increased to  $112.2 \pm 0.2\text{ mW}$ , more than 3 times the minimum trapping power required, in order to test the filtering ability of the doped droplet lens. At this power, the trapping light started to be visible through the doped PDMS droplet lens.

## Conclusions

The optical manipulation system presented here can be fabricated with very little optical experience and at a very low cost. Although our system may not be suitable for high precision work, qualitative, low precision quantitative measurements and trial experiments could be easily performed. By making use of easy to handle materials that are readily found in many labs (including non-optics labs), we have developed a system that keeps the cost of optical components to a minimum. This would allow optical trapping systems based on hanging droplets to be quickly constructed in any lab with access to a laser. Although there was some variation in the length of the lenses, the other dimensions of the lenses were found to be roughly constant, owing to the material properties of PDMS leading to the

droplets naturally taking this shape. Due to the low trapping power that is required, a laser pointer with sufficient output beam quality could be used as the trapping source, thus significantly lowering the cost of the overall optical manipulation system and allowing for their use in schools or university research labs without access to significant resources. This would also make an excellent undergraduate laboratory project in which almost all the components of the optical system can be made from scratch.

Through the addition of Sudan II dye, an imaging lens with an integrated long pass filter suitable for fluorescence detection was created. Integration with other microfluidic systems to create simple optofluidic<sup>19</sup> devices should be straightforward due to much of the system being made from PDMS. This work, therefore, contributes to the burgeoning field of disposable, point-of-care diagnostic devices by allowing for the simple incorporation of optical trapping, fluorescence microscopy techniques and microfluidics.

An obvious extension for our system is to build it with something like lego, or to 3d print the microscope structure. There are printers that will print/cure polymers, and our thinking is that our methodology is a precursor for the full 3d printing of an optical trapping system, this would be much better engineered than our device, and therefore would be much higher precision, all incorporated onto the camera of a mobile phone. This seems perfectly plausible, with the growing interest in 3d printing of lab equipment, with particular reference to the developing world, as indicated in the recent PLoS Biology paper by Baden *et al.*<sup>20</sup> We also suggest that the device, once developed into a compact form would open up field studies of aerosols, part of the development of compact, mobile, urban sensors for airborne aerosols.<sup>21</sup> Our initial development appears to have a number of future developmental options.

## Acknowledgements

We acknowledge EPSRC for support through grant EP/J500392/1. We also thank Paul O'Mahoney from the University of

<sup>¶</sup> It is assumed that a system developer would have access to a smartphone, with the vast majority of models suitable for use with our system.



Dundee, Dundee, UK for his knowledge of the colour wheel, which put the authors on the path to constructing filters.

## References

- 1 K. Svoboda, C. Schmidt, B. Schnapp and S. Block, *Nature*, 1993, **365**, 721–727.
- 2 D. R. Burnham and D. McGloin, *Opt. Express*, 2006, **14**, 4176–4182.
- 3 A. Pralle, E. Florin, E. H. K. Stelzer and J. K. H. Hörber, *Appl. Phys. A: Mater. Sci. Process.*, 1998, **73**, 71–73.
- 4 J. L. Wilbur, R. J. Jackman and G. M. Whitesides, *Chem. Mater.*, 1996, **8**, 1380–1385.
- 5 Y. Gambin, O. Legrand and S. R. Quake, *Appl. Phys. Lett.*, 2006, **88**, 174102.
- 6 K.-H. Jeong, J. Kim and L. P. Lee, *Science*, 2006, **312**, 557–561.
- 7 W. M. Lee, A. Upadhyay, P. J. Reece and T. G. Phan, *Biomed. Opt. Express*, 2014, **5**, 1626–1635.
- 8 D. N. Breslauer, R. N. Maamari, N. A. Switz, W. A. Lam and D. A. Fletcher, *PLoS One*, 2009, **4**, e6320.
- 9 L. Bellina and E. Missoni, *Diagn. Pathol.*, 2009, **4**, 4.
- 10 Z. J. Smith, K. Chu, A. R. Espenson, M. Rahimzadeh, A. Gryshuk, M. Molinaro, D. M. Dwyre, S. Lane, D. Matthews and S. Wachsmann-Hogiu, *PLoS One*, 2011, **6**, e17150.
- 11 A. Skandarajah, C. D. Reber, N. A. Switz and D. A. Fletcher, *PLoS One*, 2014, **9**, e96906.
- 12 D. Erickson, D. O'Dell, L. Jiang, V. Oncescu, A. Gumus, S. Lee, M. Mancuso and S. Mehta, *Lab Chip*, 2014, 3159–3164.
- 13 F. A. Chowdhury and K. J. Chau, *J. Opt.*, 2012, **14**, 055501.
- 14 H. Ren, S. Xu and S.-T. Wu, *Opt. Commun.*, 2010, **283**, 3255–3258.
- 15 R. Tadmor, P. Bahadur, A. Leh, H. E. N'guessan, R. Jaini and L. Dang, *Phys. Rev. Lett.*, 2009, **103**, 266101.
- 16 O. Hofmann, X. Wang, A. Cornwell, S. Beecher, A. Raja, D. D. C. Bradley, A. J. Demello and J. C. Demello, *Lab Chip*, 2006, **6**, 981–987.
- 17 X. Mao and T. J. Huang, *Lab Chip*, 2012, **12**, 1412.
- 18 A. Ashkin, *Biophys. J.*, 1992, **61**, 569–582.
- 19 P. Fei, Z. Chen, Y. Men, A. Li, Y. Shen and Y. Huang, *Lab Chip*, 2012, **12**, 3700.
- 20 T. Baden, A. M. Chagas, G. Gage and T. Marzullo, *PLoS Biol.*, 2015, **13**, e1002086.
- 21 M. Budde, M. Busse and M. Beigl, Networked Sensing Systems (INSS), 2012 Ninth International Conference on Networked Sensing, 2012, pp. 1–4.