

Solid phase synthesis of functionalised SAM-forming alkanethiol–oligoethyleneglycols†

Cite this: *J. Mater. Chem. B*, 2014, 2, 3741Received 10th April 2014
Accepted 22nd April 2014

DOI: 10.1039/c4tb00573b

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We present an efficient solid phase synthesis methodology that provides easy access to a range of functionalised long-chain alkanethiol–oligoethyleneglycols that form well-defined self-assembled monolayers on gold and are compatible with pre- or post-assembly conjugation of (bio)molecules. We demonstrate the versatility of our synthetic route by synthesising LCAT–OEGs with a range of functional moieties, including peptides, electro-active redox groups, chemical handles for post-assembly conjugation of (bio)molecules, and demonstrate the application of our LCAT–OEG monolayers in immunosensing, where they show good biocompatibility with minimal biofouling.

Self-assembled monolayers (SAMs) of functionalised long-chain alkanethiolates (LCATs) on metals¹ provide an excellent and versatile platform for the chemoselective immobilisation of (bio)molecules on planar and nanoparticle surfaces. Their well-defined thickness, structure, and dielectric properties² make them ideally suited for applications where a high degree of control of the physical and chemical properties of surfaces is required. Functionalised LCATs also enable the creation of patterned surfaces³ critical for protein and DNA microarrays. SAMs used for protein biosensing applications usually require LCATs incorporating oligoethylene glycol (OEG) linkers to help reduce non-specific protein adsorption⁴ and functional groups that allow the further tuning of surface chemistry providing control over the immobilisation, density and orientation of capture molecules. Thus, easy access to a variety of functionalised LCAT–OEGs is essential for optimisation of, for example, immobilisation chemistry and OEG and alkanethiolate length.

†School of Chemistry, University of Leeds, LS2 9JT, UK. E-mail: r.bon@leeds.ac.uk

‡Astbury Centre for Structural Molecular Biology, University of Leeds, UK

§School of Electronic and Electrical Engineering, University of Leeds, UK

¶School of Physics and Astronomy, University of Leeds, UK

**Department of Electronics, University of York, Heslington York, YO10 5DD, UK

† Electronic supplementary information (ESI) available: Synthesis and characterisation of compounds, XPS, EIS, AFM, contact angle measurements, CV, colorimetry and SPR. See DOI: 10.1039/c4tb00573b

James Murray,^{ab} Dominika Nowak,^{bc} Laurynas Pukenas,^{bd} Rizuan Azhar,^e Mathieu Guillorit,^a Christoph Wälti,^c Kevin Critchley,^{bd} Steven Johnson^e and Robin S. Bon^{*ab}

However, commercial availability of functionalised LCAT–OEGs is severely limited and synthetic routes often laborious. In this study, we present a versatile solid phase synthesis route that provides easy access to a range of functionalised LCAT–OEGs. Using a range of surface characterisation techniques including surface plasmon resonance (SPR) and electrochemical spectroscopy, we demonstrate that the resulting LCAT–OEGs form dense, well-defined mixed SAMs of high quality, which are compatible with on-surface bioorthogonal ligation reactions.

Customised SAMs presenting ligands and/or biomolecules can be prepared according to two general strategies (Fig. 1): (i) conjugation of (bio)molecules to LCAT–OEGs after SAM formation (*post-assembly conjugation*); (ii) total synthesis of functionalised LCAT–OEGs followed by SAM formation (*pre-assembly conjugation*). Post-assembly conjugation requires robust, chemoselective, and mild chemistry to ensure complete surface functionalisation without side reactions.^{2,5} For pre-assembly conjugation approaches, total synthesis of LCAT–OEGs terminated with, amongst others, biotin,⁶ peptides,^{6,7} ferrocene,⁸ azides,⁹ aminoxy groups,⁹ and sugars¹⁰ has been demonstrated. Such functionalised LCAT–OEGs are usually synthesised in solution, which requires multiple chromatographic steps and suffers from poor overall yields. Solid phase chemistry presents an attractive alternative for synthesising

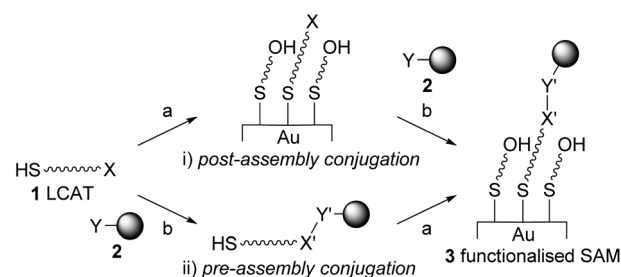


Fig. 1 SAM functionalisation strategies. (a) SAM formation (in the example: a mixed SAM, with a hydroxy-terminated diluent, on a gold surface); (b) conjugation of LCAT 1 with reagent 2 (in which functional groups X and Y react to form linker X'Y').



cleaved from the solid support at any point using trifluoroacetic acid and triethylsilane (at least one equivalent to scavenge resin-bound trityl cations). After purification by chromatography (either SiO₂ or C18), the pure LCAT-OEGs **11a**, **11b**, **13**, **15**, **17** and **18** were obtained in good total yields, based on the loading of 2-chlorotrityl chloride resin **8**.[‡]

Next, we analysed the quality of SAMs assembled from our functionalised LCAT-OEGs on sputtered gold surfaces. Using X-ray photoelectron spectroscopy (XPS), we found S 2p peaks of SAMs of **11a**, **11b**, and **13** to have binding energies consistent with the formation of thiolate bonds (Fig. S2.1[†]). The C 1s region consisted of three peaks for all SAMs, corresponding to the alkyl chain, the OEG chain, and carbonyls (Fig. 2A). The analysis of the N 1s region for SAMs of **13** was complicated due to rapid degradation of the azide group under XPS conditions (see the ESI[†]). The azide-terminated SAM **13** resulted in a surface that was of slightly lower surface energy than SAMs of **11a** or **11b**. This enabled the degree of mixing in the SAMs between diluents **11a** or **11b** and azide **13** to be estimated by contact angle analysis by applying the Cassie equation¹⁸ (Fig. 2B). The insulating properties of SAMs containing different ratios of **11a** : **15** or **11a** : **17a** were assessed by electrochemical impedance spectroscopy (Fig. S3.1 and S3.2[†]). The minimum phase angles of -88° to -83° for SAMs of **11a** : **15** and -88° to -87° for SAMs of **11a** : **17a**, measured at 0.1 Hz, correspond to the formation of well-packed, insulating monolayers that are almost free of pinholes and collapsed sites effects. Furthermore, atomic force microscopy

(AFM) of a SAM of **11a** : **17a** (1 : 1) revealed uniform surfaces absent of macroscopic islands resulting from phase separation (Fig. S5.1[†]). Cyclic voltammetry (CV) measurements of mixed SAMs formed from different ratios of **11b** : **15** (Fig. S6.1–S6.3[†]) revealed SAM capacitance values of $4.4 \times 10^{-6} \text{ F cm}^{-2}$, which corresponds well with the capacitance of simple LCAT monolayers.¹⁹ Furthermore, the absence of redox peaks due to electron transfer to solution phase redox probe confirms the absence of pin holes within the LCAT-OEG monolayers.

To demonstrate the potential suitability of MB-functionalised LCAT-OEGs for molecular electronics applications, we assessed the redox behaviour of surface-bound MB by CV. CV measurements on SAMs of **18** showed clear oxidation and reduction peaks associated with the MB moiety around $-130 \text{ mV vs. Ag/AgCl}$ (Fig. 2C). No redox peaks were observed in equivalent CV measurements performed on non-redox active LCAT-OEG SAMs (compounds **15** and **17a**, Fig. S6.1–S6.3[†]). The peaks are reasonably symmetric with only a small peak separation (9 mV at a scan rate of 200 mV s^{-1}), typical of the electrochemical behaviour of a fully reversible redox-active monolayer. Furthermore, the peak anodic and cathodic current was found to increase linearly with scan rate (see inset of Fig. 2C), again characteristic of a surface-tethered redox-active group. From the gradient of the straight line fit to peak current vs. scan rate we calculated a surface coverage, $\Gamma = 8.8 \times 10^{13}$ molecules per cm². This is slightly lower than the theoretical density predicted for a perfect SAM formed from LCATs only (4×10^{14} molecules per cm²) and is likely due to the steric hindrance of the bulky OEG and MB groups that inhibit denser monolayer assembly. Finally, the FWHM of the oxidation and reduction peaks was found to be 37 mV (at 200 mV s^{-1}). While this is lower than the theoretical ideal (45.3 mV for a 2 electron process) we note that deviations in the FWHM are not uncommon in densely packed redox-active monolayers due to electrostatic interactions between adjacent charged species.

Confident that our molecules formed well-defined SAMs, we demonstrated that they also allow (bio)molecule immobilisation by common post-assembly conjugation techniques: Copper-catalysed azide-alkyne cycloaddition (CuAAC) and bis-(sulfosuccinimidyl) suberate (BS3)-mediated amide coupling.

First, we 'clicked' propargyl biotin onto a SAM of **11a** : **13** (1 : 1; see ESI[†]) and tested for the presence of biotin attached covalently to the surface using a colorimetric assay (Fig. 3A). Briefly, we introduced streptavidin-alkaline phosphatase fusion protein to the surface and used western blue as a stain. Only spots where biotin had been successfully linked to the surface were stained purple (Fig. 3A, S7.1 and S7.2[†]). Finally, we tested the suitability of SAMs containing amine **15** for immobilisation of the clinically relevant human chorionic gonadotropin antibody (anti-hCG).²⁰ A SAM of **11a** : **15** (1 : 1) was formed and activated using the bis-succinimide crosslinker BS3 on a Biacore SPR chip (Scheme S8.1[†]). Injection of anti-hCG gave a much stronger signal in the channel pre-treated with BS3 than in the control channel (no BS3), indicating successful covalent immobilisation of anti-hCG (Fig. 3B). The lack of binding observed on the control channel suggests the LCAT-OEG monolayer is efficient at minimising non-specific adsorption.

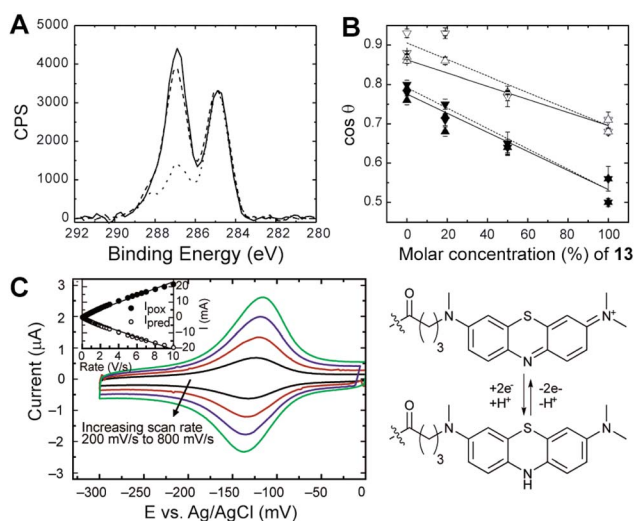


Fig. 2 Characterisation of LCAT-OEG SAMs. (A) XPS data of C 1s region for reference SAMs of **11a** (dotted), **11b** (dashed) and **13** (solid) normalised to the alkyl chain peak at 284.9 eV. Spectra reflect similar carbonyl (288.3 eV), but varying amount of OEG (286.9 eV) carbon. (B) A linear change in cosine of the contact angle with molar ratio of azide **13** in mixed SAMs was observed. Triangles facing down represent **11a** : **13**; facing up – **11b** : **13** SAMs; advancing and receding angles are filled and open symbols, respectively. Dotted and solid lines represent the line of best fit for the Cassie equation for contact angles for **11a** : **13** and **11b** : **13** SAMs, respectively. (C) Typical cyclic voltammograms (left) for the 2-electron oxidation/reduction of SAM-bound methylene blue (right) at scan rates of 200 (black), 400 (red), 600 (blue) and 800 mV s^{-1} (green). The inset shows the linear relationships between current and scan rate.



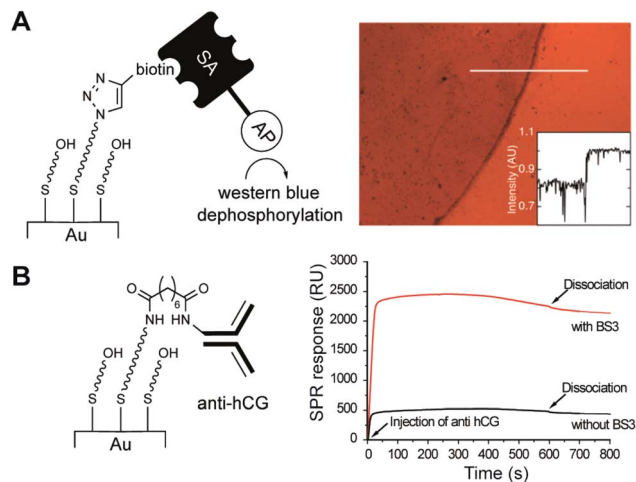


Fig. 3 Post-assembly conjugation: (A) biotin immobilised through CuAAC on SAMs of **11a** : **13** (1 : 1; left) was detected colorimetrically, as purple spots (right), upon incubation of the gold slide with streptavidin-alkaline phosphatase (SA-AP) and western blue. (B) Immobilisation of anti-hCG on a BS3-activated amine SAM (**11a** : **15**, 1 : 1; left) was detected by SPR (right).

In conclusion, we have established a robust and versatile solid phase synthesis of LCAT-OEGs functionalised with alcohols, azides, amines, peptides, and the redox probe methylene blue, thereby significantly expanding the range of LCAT-OEGs that are easily accessible through solid phase approaches such as those reported by Albericio.^{6b,7a} All LCAT-OEGs could be isolated in good yields as pure materials, and were used to form dense and well-defined, high quality mixed SAMs absent of macroscopic island formation (AFM data) and pinholes (EIS and CV data). In addition, the ratios of functionalised LCAT-OEGs and diluents on the surface were directly proportional to the ratios of these molecules in the applied solutions. Finally, we demonstrated that in addition to total synthesis of functional LCAT-OEGs for pre-assembly conjugations, our solid phase methodology also allows the use of bioorthogonal post-assembly conjugation techniques.

Acknowledgements

This research was funded by the Biomedical and Health Research Centre of the University of Leeds (RSB and SJ), a Henry Ellison PhD Studentship (JM), EPSRC Grants EP/J010731/1 (RSB, DN and SJ), EP/J01513X/1 (KC), and EP/I014039/1 (LP), the Centre for Chronic Diseases and Disorders (C2D2; RA), the University of York (SJ), and WELMEC, a Centre of Excellence in Medical Engineering funded by the Wellcome Trust and EPSRC, under grant number WT 088908/Z/09/Z (DN and CW). We thank Dr. Simon White for assistance with SPR measurements and Prof. Stephen Evans for assistance with interpretation of XPS data.

Notes and references

† We routinely perform the synthesis of **11a**, **11b**, **13**, **15**, and **18** on a 0.1–0.6 mmol scale per SPE tube, which provides plenty material for optimisation studies with SAMs. Instead of using chromatography, LCAT-OEGs incorporating basic

amines can also be purified by precipitation (as their TFA salts) into mixtures of diethyl ether and hexane.

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