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PAPER

An examination of the calcium and strontium site distribution in bioactive glasses through isomorphous neutron diffraction, X-ray diffraction, EXAFS and multinuclear solid state NMR

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Strontium has been substituted for calcium in the glass series $(\text{SiO}_2)_{49.46}(\text{Na}_2\text{O})_{26.38}(\text{P}_2\text{O}_5)_{1.07}(\text{CaO})_{23.08-x}(\text{SrO})_x$ (where $x = 0, 11.54, 23.08$) to elucidate their underlying atomic-scale structural characteristics as a basis for understanding features related to the bioactivity. These bioactive glasses have been investigated using isomorphous neutron and X-ray diffraction, Sr K-edge EXAFS and solid state ^{17}O , ^{23}Na , ^{29}Si , ^{31}P and ^{43}Ca magic-angle-spinning (MAS) NMR. An effective *isomorphous substitution* first-order difference function has been applied to the neutron diffraction data, confirming that Ca and Sr behave in a similar manner within the glass network, with residual differences attributed to solely the variation in ionic radius between the two species. The diffraction data provides the first direct experimental evidence of split Ca–O nearest-neighbour correlations in these melt-quench bioactive glasses, together with an analogous splitting of the Sr–O correlations; the correlations are attributed to the metal ions correlated either to bridging or to non-bridging oxygen atoms. Triple quantum (3Q) ^{43}Ca MAS NMR corroborates the split Ca–O correlations. Successful simplification of the $2 < r(\text{\AA}) < 3$ region *via* the difference method has also revealed two distinct Na environments. These environments are attributed to sodium correlated either to bridging or to non-bridging oxygen atoms. Complementary multinuclear MAS NMR, Sr K-edge EXAFS and X-ray diffraction data supports the structural model presented. The structural sites present will be intimately related to their release properties in physiological fluids such as plasma and saliva, and hence the bioactivity of the material. Detailed structural knowledge is therefore a prerequisite for optimising material design.

1. Introduction

Bioactive $\text{SiO}_2\text{--Na}_2\text{O--CaO--P}_2\text{O}_5$ glasses, including the original Bioglass[®], have the ability to promote bone regeneration.^{1,2} Under physiological conditions these materials release essential elements such as Ca, P and Si, which promote the formation of hydroxyapatite (HA): the naturally occurring mineral present in

both teeth and bones. Following the discovery of Bioglass, advances in biomedical research have yielded many materials for various applications including bone and tissue regeneration, drug delivery systems and dental treatments.³ The importance of Sr in biomaterials has become of increasing interest due to its radio-opacity, antibacterial properties and effects on new bone growth.^{4–6} Thus, the incorporation of Sr into bioactive glasses could provide scope for a number of new applications in dental and other medical fields.

It is well established that cations with the same valence and a similar charge-to-size ratio can be substituted within a glass matrix. Sr and Ca have ionic radii of 1.18 and 1.00 Å, respectively,⁷ and this small difference allows Sr to be substituted for Ca in bioactive glasses and subsequently incorporated into HA. Indeed, Sr–Ca HA and pure Sr HA have both been reported to exist in mineral forms.^{8,9} Both Ca and Sr occur naturally in the body with >99% of the combined total localised in bone material.¹⁰ The concentration of Sr is typically between 0 and 3.5 mol% of the combined Ca + Sr content; however, Sr is preferentially sited in new bone structures where increases in Sr concentrations

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by factors of up to ~ 3 to 3.5 have been observed.¹⁰ Thus, the importance of Sr has attracted an increasing research interest in recent years due to its beneficial properties: it is known to stimulate the bone-forming osteoblast cells (and inhibit the bone-resorbing osteoclasts) as well as reduce bone desorption, which consequently increases bone formation and mass without demonstrating an adverse effect on the bone mineralization process.^{11,12} These are all key attributes that are influential in the treatment of osteoporosis and other degenerative bone diseases. Further research has led to the therapeutic use of Sr salts in the forms of strontium ranelate and strontium chloride as treatments for osteoporosis,^{13–15} where their usage has led to a reduced risk in the occurrence of vertebral and non-vertebral fractures in postmenopausal osteoporosis.^{16,17}

Strontium is also of interest in the field of dentistry. Some applications require the glasses and glass ceramics used to be relatively opaque to X-rays, in the context of post-treatment diagnostics, which can be achieved by incorporating Sr due to its greater radio-opacity compared to that of Ca.⁴ Strontium is also known to inhibit caries formation in teeth and promote apatite formation.^{18–22} In addition, Sr is used as an additive in toothpastes in the form of strontium chloride and strontium acetate to reduce tooth sensitivity. Hence, the incorporation of Sr into bioactive glasses that are currently used as remineralising additives in toothpaste is an attractive proposition. It is also worth noting that Sr has been shown to exhibit antibacterial properties⁶ which could be of benefit if a Sr-containing bioactive glass was to be used as an implant for bone or tissue regeneration, since it would reduce the risk of infection at the implant site and thus diminish the potential need for revision surgery.

Calcium, and in particular its release rate, is known to play a key role in the bioactivity of Bioglass, and the facile nature of Ca desorption is now reasonably well understood at the atomic scale following research on sol–gel synthesised analogues.^{23–25} However, the local environment that Ca adopts within melt-quench derived bioactive glasses is not as well understood. Calcium can adopt a wide range of environments in its crystalline phases; for example, the number of oxygen atoms surrounding calcium varies from 6.67 in wollastonite ($\text{CaO} \cdot \text{SiO}_2$) to 8 in pseudowollastonite (the high temperature phase of $\text{CaO} \cdot \text{SiO}_2$), whilst calcium oxide and HA have 6 and 8.4 oxygen atoms per Ca respectively.²⁶ The corresponding Ca–O bond lengths also vary over the range 2.28–2.72 Å.²⁶ It is anticipated therefore that Ca will have a complex local environment in amorphous bioactive glasses. In order to be able to model and predict the behaviour of such materials it is necessary to understand the local structure of the glass, particularly the local Ca environment, and secondly to monitor any differences that may arise with increasing Sr content. The dissolution of a bioresorbable glass will be determined partially by the connectivity of the glass-forming network^{27,28} and also in part by the local environment surrounding the active Ca^{2+} or Sr^{2+} ions.

We have therefore investigated the influence of substituting Sr for Ca in the glass series $(\text{SiO}_2)_{49.46}(\text{Na}_2\text{O})_{26.38}(\text{P}_2\text{O}_5)_{1.07}(\text{CaO})_{23.08-x}(\text{SrO})_x$ (where $x = 0, 11.54, 23.08$) in terms of the glass' atomic-scale structural characteristics using neutron and X-ray diffraction, EXAFS and solid state ^{17}O , ^{23}Na , ^{29}Si , ^{31}P and ^{43}Ca MAS NMR studies.

2. Experimental

2.1. Sample preparation

The melt-quenched glass samples were prepared using SiO_2 (Alfa Aesar, 99.5%), Na_2CO_3 (Sigma-Aldrich, 99.5+%), P_2O_5 (Sigma-Aldrich, 98.5%), and CaCO_3 (Alfa Aesar, 99.95–100.5%) and/or SrCO_3 (Sigma-Aldrich, 99.9%). The precursors were heated in a platinum crucible to 1400 °C at 10 °C min^{−1} and held at temperature for 1.5 h. The molten glass was then poured into a pre-heated graphite mould (350 °C) and annealed at this temperature overnight before being allowed to cool slowly to room temperature.²⁹ The composition of the three glasses prepared were $(\text{SiO}_2)_{49.46}(\text{Na}_2\text{O})_{26.38}(\text{P}_2\text{O}_5)_{1.07}(\text{CaO})_{23.08-x}(\text{SrO})_x$ (where $x = 0, 11.54$ and 23.08) and they are labelled $^{43}\text{CaBio}$, $^{43}\text{CaSrBio}$ and $^{43}\text{SrBio}$ respectively. Isotopically enriched glasses were similarly prepared for the ^{17}O and ^{43}Ca NMR experiments. The ^{17}O enriched samples were prepared using 40% enriched SiO_2 , the precursors were heated in an inert argon atmosphere to inhibit ^{17}O exchange in air. ^{43}Ca glasses were prepared using partially enriched ^{43}Ca calcium carbonate to give $\sim 8\%$ ^{43}Ca enrichment.

The macroscopic densities of the glass samples were determined by helium pycnometry using a Quantachrome Multi-pycnometer. Glass transition temperatures, T_g , were measured using a NETZSCH STA 409 PC differential scanning calorimeter.

2.2. Neutron diffraction

The neutron diffraction spectra were collected using the GEM diffractometer at the ISIS spallation neutron source at the Rutherford Appleton Laboratory, UK.³⁰ The samples were cast into 8 mm diameter rods, which eliminated the need for a container and therefore reduced the number of data corrections required. Interference patterns were collected for each of the samples, a vanadium rod of 8 mm diameter and the empty GEM instrument in order to perform the appropriate corrections. The data reduction and corrections were performed using the program GUDRUN.³⁰ The corrections involve the removal of background scattering, normalization, correction for absorption, inelastic and multiple scattering effects and subtraction of the self-scattering term.³⁰ Following these corrections, the resultant coherent scattering intensity, $i(Q)$, is defined by³¹

$$i(Q) = \sum_i \sum_j c_i c_j b_i b_j [p_{ij}(Q) - 1] \quad (1)$$

where c_i , c_j , b_i and b_j represent the atomic concentration and coherent scattering length of the chemical species i and j respectively, and $p_{ij}(Q)$ is the pair correlation function. Fourier transformation of $i(Q)$ generates the total correlation function, $T(r)$, given by

$$T(r) = T^0(r) + \frac{2}{\pi} \int_0^\infty Qi(Q)M(Q)\sin(Qr)dQ \quad (2)$$

where $M(Q)$ is a Lorch window function that takes into account the finite maximum experimentally attainable value of Q and $T^0(r)$ is the average density term, given by:³¹

$$T^0(r) = 4\pi r \rho^0 \left(\sum_i c_i b_i \right)^2 \quad (3)$$

where r is the distance from an arbitrary atom at the origin and ρ^0 is the number density.

Structural information can be obtained by modelling the real-space correlation functions. Pair functions are generated in Q -space and Fourier transformed to allow comparison with the experimental data in real-space. The pair functions are given by:³¹

$$p_{ij}(Q)_{ij} = \frac{N_{ij} w_{ij}}{c_j} \frac{\sin Q r_{ij}}{Q r} \exp \left[\frac{-Q^2 \sigma_{ij}^2}{2} \right] \quad (4)$$

where N_{ij} , r_{ij} and σ_{ij} represent the coordination number, atomic separation and disorder parameters respectively. The weighting factor w_{ij} is given by:

$$w_{ij} = 2c_i c_j b_i b_j \text{ if } i \neq j \quad (5)$$

$$w_{ij} = c_i^2 b_i^2 \text{ if } i = j \quad (6)$$

The method of isomorphic substitution was applied to the neutron diffraction data.^{32,33} If three total structure factors $^{\text{Sr}}i(Q)$, $^{\text{CaSr}}i(Q)$ and $^{\text{Ca}}i(Q)$ are measured corresponding to scattering lengths $b_{\text{Sr}} > b_{\text{CaSr}} > b_{\text{Ca}}$ then those correlations not involving the calcium or strontium ion can be eliminated by subtracting two total structure factors to give a first order difference function such as $^{\text{Sr-Ca}}\Delta i(Q) = ^{\text{Sr}}i(Q) - ^{\text{Ca}}i(Q)$. The addition of the third total structure factor enables three separate first order difference functions to be determined, this can in turn be used to check the reliability/mutual consistency of these difference functions. Full details on the method of isomorphic substitution are given by Martin *et al.*³² The assumption of isomorphism is valid over the short and medium range order, however due to the size difference between the Ca^{2+} and Sr^{2+} ions the extended range order is not assumed to be isomorphic. The diffraction data is therefore only modelled up to 3 Å.

2.3. Solid state NMR

One-dimensional ^{43}Ca , ^{23}Na , ^{31}P , ^{29}Si and ^{17}O MAS NMR data were acquired using the set-up parameters given in Table 1. All data were collected under conditions to ensure

Table 1 Experimental parameters for the one-dimensional solid state NMR experiments

	Field (T)	Frequency (MHz)	MAS (kHz)	Probe	Reference
^{43}Ca	20	57.22	10	4 mm Bruker	0.1 M CaCl_2 (aq.)
^{43}Ca	14.1	40.34	10	4 mm Bruker	0.1 M CaCl_2 (aq.)
^{43}Ca	9.4	26.89	10	4 mm Bruker	0.1 M CaCl_2 (aq.)
^{23}Na	14.1	158.55	15	3.2 mm Bruker	0.1 M NaCl (aq.)
^{23}Na	9.4	105.65	15	3.2 mm Bruker	0.1 M NaCl (aq.)
^{31}P	9.4	161.92	10	4 mm Bruker	85% H_3PO_4
^{29}Si	7.05	59.58	5	7 mm Bruker	Kaolinite
^{17}O	14.1	81.25	20	3.2 mm Bruker	H_2O

quantitative reliability. Two-dimensional ^{43}Ca 3QMAS NMR data were also acquired at a Larmor frequency of 57.22 MHz. These 3QMAS measurements employed a conventional Z-filter experiment,³⁴ where initial (non-selective) 4.50 μs excitation and 1.25 μs conversion pulses were followed by two selective $\pi/2$ pulses each of ~ 25.00 μs duration which comprised the Z-filter. In each experiment 96 transients were acquired for each of the 128 F1 dimension slices, with a recycle delay of 5 seconds being used. Two-dimensional ^{17}O 3QMAS data were measured at a Larmor frequency of 81.25 MHz. The conventional Z-filter experiment used an excitation, conversion and Z-filter pulse durations of 4.2, 1.5 and 14.0 μs , respectively.

2.4. Extended X-ray absorption fine spectra (EXAFS)

The Sr K-edge EXAFS were collected using B18 at the Diamond Light Source.³⁵ The Sr-containing bioactive glasses were ground into a fine powder, mixed with cellulose and pressed into a pellet. The measurements were conducted at room temperature and in transmission mode. Ten scans were collected for each sample and the data averaged. The Sr K-edge is at 16 105 eV. Spectra were collected with 5 eV steps in the pre-absorption edge region (15 905–16 072 eV), 1 eV steps from 16 072 to 16 137 eV, and 0.05 \AA^{-1} steps up to a Q value of 16.95 \AA^{-1} . The Iffit software analysis suite was used for the background corrections and normalisation (Athena), and to model the local environment of Sr (Artemis).^{36,37}

2.5. X-ray diffraction

The X-ray diffraction data was measured using a Panalytical X'pert-Pro producing silver radiation ($\lambda = 0.5638$ Å) (ISIS, Rutherford Appleton Laboratory). The calcium-containing glasses were mounted in 1.0 mm diameter silica capillaries. Sr-containing glasses absorbed X-rays strongly, and there was a significant contribution from fluorescence in the measured data. To reduce the absorption corrections, the $^{\text{Sr}}\text{Bio}$ glass sample was mounted in a 0.5 mm thin-walled silica capillary.

The data was reduced and corrected using the program GudrunX.³⁸ The corrections applied follow the same procedure as Gudrun, detailed above, and also corrected for fluorescence and Bremsstrahlung effects. After the data corrections have been applied, the coherent scattering intensity, $i_x(Q)$, is obtained. As with neutron scattering, an X-ray total correlation function, $T_x(r)$, can be calculated from a Fourier transform of $i_x(Q)$. However, X-ray scattering arises from interactions with the electron cloud around each atom, and as such the $T_x(r)$ has relatively poor resolution due to the resultant form factor and to the limits imposed on the maximum attainable value of Q by the wavelength of the X-ray. To resolve this, GudrunX normalises the data by $\langle f(Q)^2 \rangle$, which has the effect of collapsing the scattering to that of an effective point scatterer. $i_x(Q)$ is calculated as:³⁹

$$i_x(Q) = \frac{I^{\text{coh}}(Q) - \left[\sum_{i=1}^n c_i f_i^2(Q) \right]}{\left[\sum_{i=1}^n c_i f_i(Q) \right]^2} \quad (7)$$

$T_x(r)$ is defined as:

$$T_x(r) = 2\pi^2 r \rho^0 + \int_0^\infty \frac{Q i(Q)}{\left(\sum_i c_i f_i(Q)\right)^2} M(Q) \sin(Qr) dQ \quad (8)$$

3. Results and discussion

The neutron diffraction interference functions ($i(Q)$) for the ${}^{\text{Ca}}\text{Bio}$, ${}^{\text{CaSr}}\text{Bio}$ and ${}^{\text{Sr}}\text{Bio}$ systems are shown in Fig. 1(a) and the first order difference functions ($\Delta i(Q)$) are shown in Fig. 1(b). Fig. 2(a) shows the corresponding real space total diffraction data, $T(r)$, obtained by Fourier transforming the $i(Q)$ functions given in Fig. 1(a) and 2(b) shows the real space pairwise correlation data $\Delta T(r)$ obtained by Fourier transforming the $\Delta i(Q)$ functions given in Fig. 1(b). The weighting factors for each of the total structure factors and difference functions are given in Table 2. The first feature in $T(r)$, Fig. 2(a), corresponds to P–O and Si–O correlations (~ 1.6 Å), the second feature (~ 2.1 to 2.9 Å) contains overlapping O–(P)–O, O–(Si)–O, Na–O and Ca–O and/or Sr–O correlations and it is therefore not usually possible to

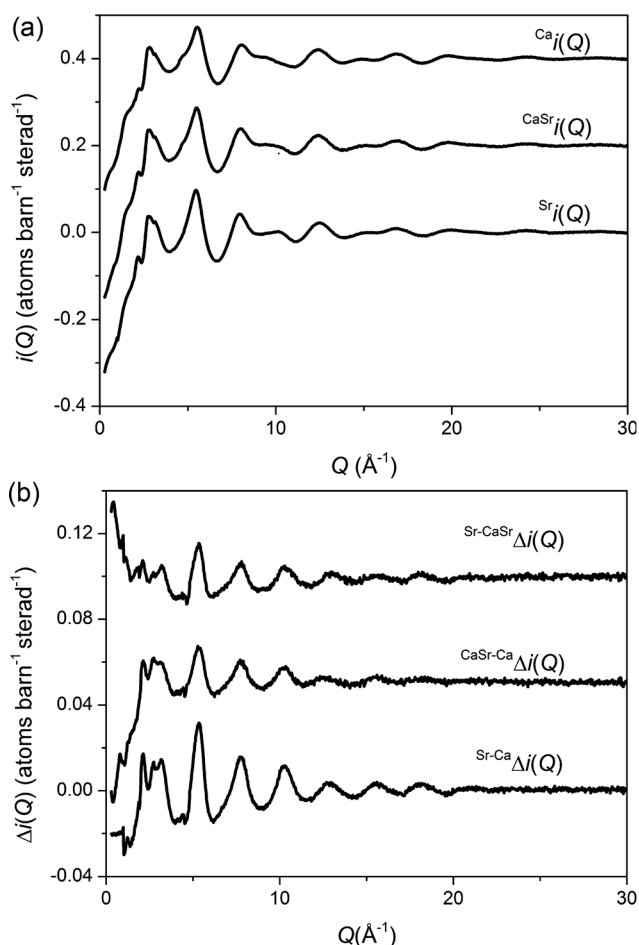


Fig. 1 (a) Q -space interference functions, $i(Q)$, for ${}^{\text{Ca}}\text{Bio}$, ${}^{\text{CaSr}}\text{Bio}$ and ${}^{\text{Sr}}\text{Bio}$, (b) Q -space interference difference functions, $\Delta i(Q)$, for ${}^{\text{Sr-CaSr}}\Delta i(Q)$, ${}^{\text{CaSr-Ca}}\Delta i(Q)$ and ${}^{\text{Sr-Ca}}\Delta i(Q)$. The datasets are offset for clarity. The Q -space data extends to 50 Å^{-1} but only $0 < Q (\text{Å}^{-1}) < 30$ is shown for clarity.

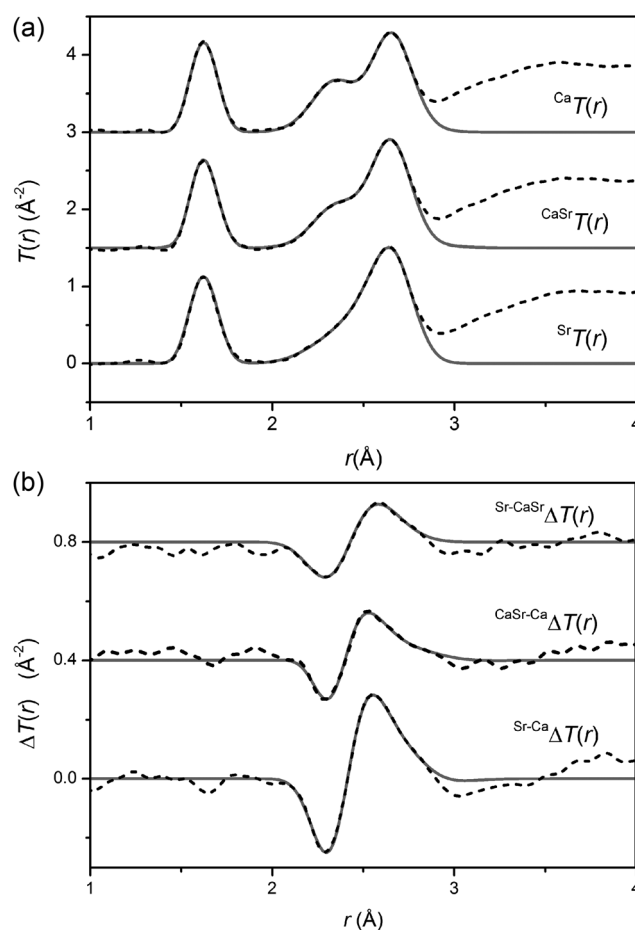


Fig. 2 The real-space diffraction data for (a) the total diffraction patterns, $T(r)$, and (b) the difference functions, $\Delta T(r)$. The broken curves represent the experimental data and the solid curves are the resultant fits. The datasets are offset for clarity.

deconvolve these correlations from the real space total diffraction data. However, those correlations that do not contain Ca or Sr cancel during the formation of the first order difference functions (Table 2). This is confirmed by the notable absence of the P–O and Si–O peaks at ~ 1.5 to 1.6 Å in the $\Delta T(r)$ functions, illustrated in Fig. 2(b). Similarly, the O–(P)–O, O–(Si)–O and Na–O correlations have been eliminated during the formation of the difference functions. Of the remaining correlations present, the first (shortest separation in r -space) correlations will correspond to nearest neighbours Ca–O and Sr–O. The second nearest neighbours such as Ca–(O)–Ca, Ca–(O)–Na, Ca–(O)–P and Ca–(O)–Si are not expected to occur until beyond 3 Å. The first order difference functions were therefore modelled exclusively using Ca–O and Sr–O correlations. The data was fitted using the NXFit program developed by Moss.⁴⁰ Initially, the first order difference data was modelled over the region $2.1 < r (\text{Å}) < 2.9$ using a single Ca–O correlation and a single Sr–O correlation. The single Ca–O/Sr–O fit was in reasonable agreement with the experimental data and the output parameters are given in Table 3. However, a small residual peak was present at high- r and the asymmetry in the $\Delta T(r)$ peaks suggested the data would be better modelled using two peaks for the Ca–O correlation and two peaks for the Sr–O correlation. The fit parameters for the

Table 2 Neutron weighting factors (mbarn)

	Ca $i(Q)$	CaSr $i(Q)$	Sr $i(Q)$	Sr–Ca $\Delta i(Q)$	Sr–CaSr $\Delta i(Q)$	CaSr–Ca $\Delta i(Q)$
$p_{\text{Ca–O}}(Q)$	24.48	12.24	—	–24.48	–12.24	–12.24
$p_{\text{Ca–Si}}(Q)$	5.63	2.82	—	–5.63	–2.82	–2.82
$p_{\text{Ca–Na}}(Q)$	5.26	2.63	—	–5.26	–2.63	–2.63
$p_{\text{Ca–P}}(Q)$	0.30	0.15	—	–0.30	–0.15	–0.15
$p_{\text{Ca–Ca}}(Q)$	1.49	0.37	—	–1.49	–0.37	–1.12
$p_{\text{Ca–Sr}}(Q)$	—	1.11	—	—	–1.11	1.11
$p_{\text{Sr–O}}(Q)$	—	18.28	36.57	36.57	18.28	18.28
$p_{\text{Sr–Si}}(Q)$	—	4.21	8.41	8.41	4.21	4.21
$p_{\text{Sr–Na}}(Q)$	—	3.93	7.85	7.85	3.93	3.93
$p_{\text{Sr–P}}(Q)$	—	0.22	0.45	0.45	0.22	0.22
$p_{\text{Sr–Sr}}(Q)$	—	0.83	3.32	3.32	2.49	0.83
$p_{\text{Si–O}}(Q)$	46.31	46.31	46.31	—	—	—
$p_{\text{P–O}}(Q)$	2.48	2.48	2.48	—	—	—
$p_{\text{O–O}}(Q)$	100.67	100.67	100.67	—	—	—
$p_{\text{Na–O}}(Q)$	43.22	43.22	43.22	—	—	—
$p_{\text{Si–Na}}(Q)$	9.94	9.94	9.94	—	—	—
$p_{\text{Si–P}}(Q)$	0.57	0.57	0.57	—	—	—
$p_{\text{Si–Si}}(Q)$	5.33	5.33	5.33	—	—	—
$p_{\text{Na–P}}(Q)$	0.53	0.53	0.53	—	—	—
$p_{\text{Na–Na}}(Q)$	4.64	4.64	4.64	—	—	—
$p_{\text{P–P}}(Q)$	0.02	0.02	0.02	—	—	—

three first order difference functions, modelled both with a single and with double peaks, and the goodness-of-fit parameter ($F(X)$) are given in Table 3. The NXFit program requires a nominal input for each correlation and a separate value to determine the range over which each individual correlation may vary. During the fitting the individual values were free to vary and none of these values were constrained. In particular, the coordination numbers for the second set of Ca–O/Sr–O correlations were allowed to vary to include zero values, thus effectively allowing a single peak fit if this resulted in a better goodness-of-fit. However, as shown, the $F(X)$ values are significantly lower when fitting the data with two Ca–O and two Sr–O correlations. It is also apparent that the parameters for the first Ca–O and Sr–O parameter are largely unchanged whether fitting with a single or double peak model suggesting there is relatively little effective overlap between the first and second peaks, especially in the case of the Ca–O correlations. The negative peak in the 3–3.3 Å range consists of Ca–(O)–Ca, Ca–(O)–Na, Ca–(O)–P and Ca–(O)–Si correlations (the negative term arises solely due to the subtraction of Ca species from Sr as defined in Table 2), whilst the positive peak at ~3.6 to 4 Å corresponds to next nearest neighbour Sr correlations. These second-neighbour correlations are not modelled due to the complexity of the overlapping pairwise correlations present at these larger separations. The $\text{Sr–Ca}\Delta T(r)$ has the highest signal : noise ratio, being approximately twice that of the other first order difference functions. The average fit parameters given in Table 3 are therefore weighted 2 : 1 : 1 for the $\text{Sr–Ca}\Delta T(r)$: $\text{Sr–CaSr}\Delta T(r)$: $\text{CaSr–Ca}\Delta T(r)$ respectively.

The Ca–O values of ~2.33 and ~2.73 Å presented in Table 3 are consistent with crystalline $\text{Na}_2\text{CaSi}_2\text{O}_6$ for which Ca–O values in the range 2.32–2.72 Å are reported.⁴¹ This compares with similar distances measured from sol–gel derived bioactive glasses where three distinct Ca–O correlations at ~2.3, 2.5 and 2.75 Å have been assigned to Ca–non-bridging oxygen (Ca–O_{NB}), Ca–OH and Ca–bridging oxygen (Ca–O_B) bonds, respectively.^{23,42} Thus, the present results are in agreement with regard to the Ca bridging and Ca non-bridging oxygen species, whilst hydroxyl groups (and

Table 3 Structural parameters obtained by fitting the $\Delta T(r)$ difference functions

		Single peak			Split peak		
		r (Å)	N	σ (Å)	r (Å)	N	σ (Å)
$\text{Sr–Ca}\Delta T(r)$	Ca–O	2.33	5.21	0.10	2.33	5.42	0.09
	Sr–O	2.52	4.85	0.14	2.49	4.70	0.14
	Ca–O				2.73	1.39	0.19
	Sr–O				2.75	1.23	0.12
		$F(X) = 0.006$			$F(X) = 0.001$		
		r (Å)	N	σ (Å)	r (Å)	N	σ (Å)
$\text{CaSr–Ca}\Delta T(r)$	Ca–O	2.33	5.67	0.11	2.33	5.34	0.08
	Sr–O	2.52	4.64	0.15	2.46	4.73	0.14
	Ca–O				2.74	1.20	0.25
	Sr–O				2.75	1.85	0.18
		$F(X) = 0.0008$			$F(X) = 0.0004$		
		r (Å)	N	σ (Å)	r (Å)	N	σ (Å)
$\text{Sr–CaSr}\Delta T(r)$	Ca–O	2.32	5.14	0.08	2.33	5.56	0.11
	Sr–O	2.53	5.29	0.15	2.53	4.64	0.15
	Ca–O				2.72	1.27	0.17
	Sr–O				2.74	0.83	0.15
		$F(X) = 0.003$			$F(X) = 0.0011$		
		r (Å)	N	σ (Å)	r (Å)	N	σ (Å)
Average	Ca–O	2.33	5.3	0.10	2.33	5.4	0.10
	Sr–O	2.52	4.9	0.14	2.49	4.7	0.14
	Ca–O				2.73	1.3	0.20
	Sr–O				2.75	1.3	0.14

hence Ca–OH correlations) are absent, as reasonably expected for the melt-quench systems under study here. Furthermore, these results indicate that the addition of a second network modifier such as Na into the glass does not significantly change the Ca–O_{NB} and Ca–O_B correlations. This is an important observation since previous results have suggested that Na–Ca silicate glasses show a non-random distribution of cations, with a preference for Ca–O–Na bonds at the expense of Ca–O–Ca and Na–O–Na bonds.⁴³ The Sr–O distances in strontium metasilicate, SrSiO_3 , range from 2.46 to 2.74 Å (ref. 44 and 45) whilst in sodium perovskite, $\text{Na}_2\text{SrSi}_2\text{O}_6$, a shorter Sr–O distance of 2.46 Å dominates.⁴⁶ Thus, the Sr–O distances measured in this study (see Table 3) of ~2.50 and ~2.75 Å are in good agreement with previously reported range of values from these crystalline systems.

In vitro studies of bioactive calcium silicate sol–gel glasses using isotopic substitution in neutron diffraction have shown that the gel preferentially loses the shortest length Ca–O correlation, which is attributed to Ca non-bridging oxygen species.^{23,42,47} It is anticipated that the Ca/Sr non-bridging oxygen species will be lost preferentially compared to bridging oxygen species in melt quench glasses. The presence of calcium associated with non-bridging oxygen correlations will therefore act as a driver for bioactivity being the first to leach under physiological conditions thereby releasing soluble Ca into the media. The calcium then precipitates to form a calcium phosphate layer which in turn crystallises into hydroxyapatite. The solid state ⁴³Ca, ²³Na, ³¹P and ²⁹Si MAS NMR data acquired

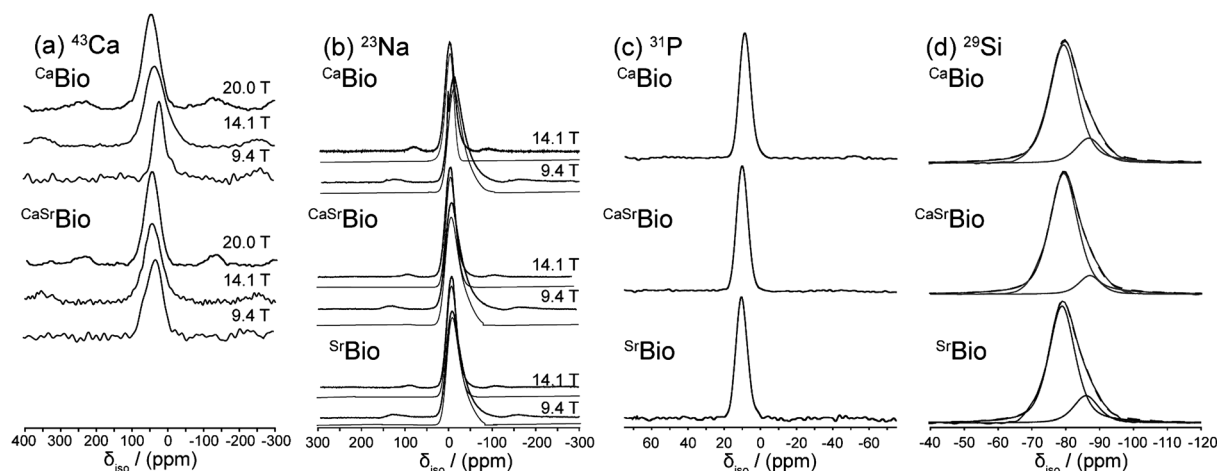


Fig. 3 Solid state MAS NMR data for, (a) variable B_0 ^{43}Ca study, (b) variable B_0 ^{23}Na study (spectral simulations in grey), (c) ^{31}P study and (d) ^{29}Si study demonstrating the deconvolution into Q^2 and Q^3 components (spectral simulations in grey).

from the $^{\text{CaBio}}$, $^{\text{CaSrBio}}$ and $^{\text{SrBio}}$ systems is shown in Fig. 3(a)–(d), respectively. All ^{43}Ca MAS NMR data were acquired using a rotor-synchronised echo experiment and exhibit a single disorder-broadened resonance which exhibits a pronounced downfield movement of the apparent shift (δ) with increasing B_0 field (see Fig. 3(a)). A graphical analysis of these data shown in Fig. 4(a) where the centre-of-gravity shift of the ^{43}Ca resonance measured at each field is plotted against $1/\nu_0^2$ (ν_0 = Larmor frequency), the slope of this behaviour yields the mean value of the quadrupole interaction parameter P_Q where:^{48,49}

$$P_Q = C_Q \sqrt{(1 + \eta_Q^2/3)} \quad (9)$$

and

$$C_Q = e^2 q Q / h \quad (10)$$

In P_Q the quadrupole coupling constant (C_Q) and asymmetry parameter (η_Q) are combined, however, the y intercept of this

plot yields the mean value of the isotropic chemical shift (δ_{iso}). Fig. 4(a) suggests that this phenomenon is more evident for the $^{\text{CaSrBio}}$ system than for its $^{\text{CaBio}}$ counterpart, thus indicating that the *average* field gradient (eq) and the δ_{iso} characterising the Ca positions in the $^{\text{CaBio}}$ glass are larger. From Table 4 the P_Q values for the $^{\text{CaBio}}$ and $^{\text{CaSrBio}}$ systems are 2.1 and 2.8 MHz, respectively; although η_Q values are not known explicitly, these P_Q values approximate the characteristic C_Q values for these systems to within a maximum error of $\sim 15\%$. Quadrupole coupling constants of this magnitude are typical of Ca in nearest-neighbour O–Ca–O environments,⁵⁰ with the trend to larger C_Q and δ_{iso} values upon Sr incorporation being attributed to next nearest neighbour effects whilst the nearest neighbour (Ca–O) effects are unperturbed, as shown in Table 3.

The ^{43}Ca 3QMAS and numerical inversion data from the $^{\text{CaBio}}$ and $^{\text{CaSrBio}}$ systems are shown in Fig. 4(c) and (d). Each dataset suggests that more than one Ca species is present in the Bioglass. The two distinct Ca environments described in Fig. 4(c) for the $^{\text{CaBio}}$ system corroborate the neutron diffraction

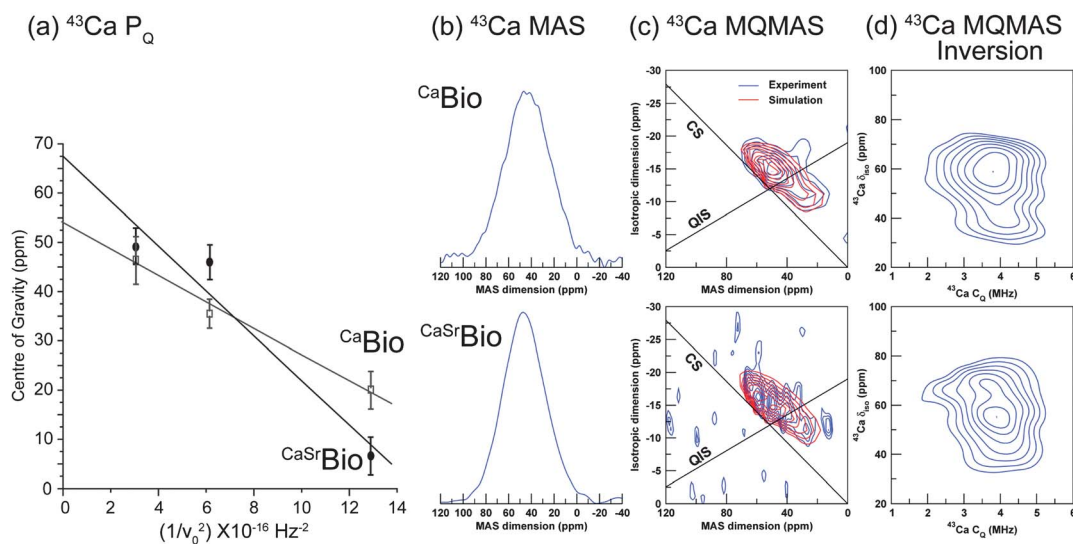


Fig. 4 ^{43}Ca solid state MAS NMR data showing, (a) a plot of the resonance centre of gravity against the inverse square of the Larmor frequency ν_0 , (b) the 1D MAS spectra, (c) the 3QMAS data and corresponding spectral simulation, and (d) the numerical inversion of the simulated 3QMAS data.

Table 4 Solid state NMR parameters. Errors are given in parenthesis for the ^{43}Ca δ_{iso} and P_{Q} values

Bioglass	δ_{iso} (ppm)	P_{Q} (MHz)	δ_{iso} (ppm)	C_{Q} centre	Width (MHz)	η_{Q}	$\delta_{\text{iso(MAS)}}$ (ppm)	δ_{iso} (ppm)	Environment (%)	δ_{iso} (ppm)	Environment (%)
Nucleus	^{43}Ca	^{43}Ca	^{23}Na	^{23}Na	^{23}Na	^{23}Na	^{31}P	^{29}Si	^{29}Si	^{29}Si	^{29}Si
CaBio	53.3 (4.2)	2.1 (0.3)	8.3	6.1	5.4	0.1	8.82	-79.0	$Q^2/83$	-86.0	$Q^3/17$
CaSrBio	67.5 (10.2)	2.8 (0.5)	10.0	7.3	6.7	0.1	9.71	-79.0	$Q^2/89$	-86.0	$Q^3/11$
SrBio	—	—	10.5	7.0	6.1	0.1	10.34	-79.0	$Q^2/81$	-86.0	$Q^3/19$

structural parameters described in Table 3. It is well established that Ca–O bond lengths profoundly influence the isotropic chemical shift position of each Ca resonance.⁵¹ Inversion of the 3QMAS data (see Fig. 4(d)) clearly exhibits two Ca populations with approximately the same C_{Q} but with δ_{iso} values differing by ~ 20 ppm. Previous work by Angeli *et al.* has demonstrated through a series of Ca-aluminosilicate glasses that a shift of up to ~ 60 ppm has been observed as Ca changes from being solely coordinated by non-bridging oxygens (Ca–O_{NB}) to being solely coordinated by bridging oxygens (Ca–O_B).⁵² This change in shift correlates strongly with the average Ca–O bond distance. In the cases studied here, the downfield (or more shielded) resonance at $\delta_{\text{iso}} \sim 41$ ppm will be associated with Ca sites exhibiting (on average) longer Ca–O bonds, and hence corresponds to the

feature in the neutron diffraction data identified at ~ 2.73 Å (see Table 3), which represents an environment more influenced by Ca–O_B linkages. Hence, the second more deshielded shift at $\delta_{\text{iso}} \sim 60$ ppm will be associated with the shorter bond length feature ~ 2.33 Å (see Table 3), thus representing a Ca environment associated with more Ca–O_{NB} moieties. The average of these shifts at ~ 50 ppm agrees well with the average δ_{iso} determined from the graphical analysis of the variable B_0 1D ^{43}Ca MAS NMR data ($\delta_{\text{iso}} \sim 53$ ppm, see Table 4). Both ^{43}Ca isotropic shifts of $\delta_{\text{iso}} \sim 41$ and ~ 60 ppm are consistent with Ca occupying distorted octahedral positions, where mean Ca–O distances in the region of 2.35 to 2.41 Å have been reported, though this does not preclude the possibility of some seven fold Ca–O environments being present.⁵⁰ A shift of δ_{iso} 59 ppm has been observed in

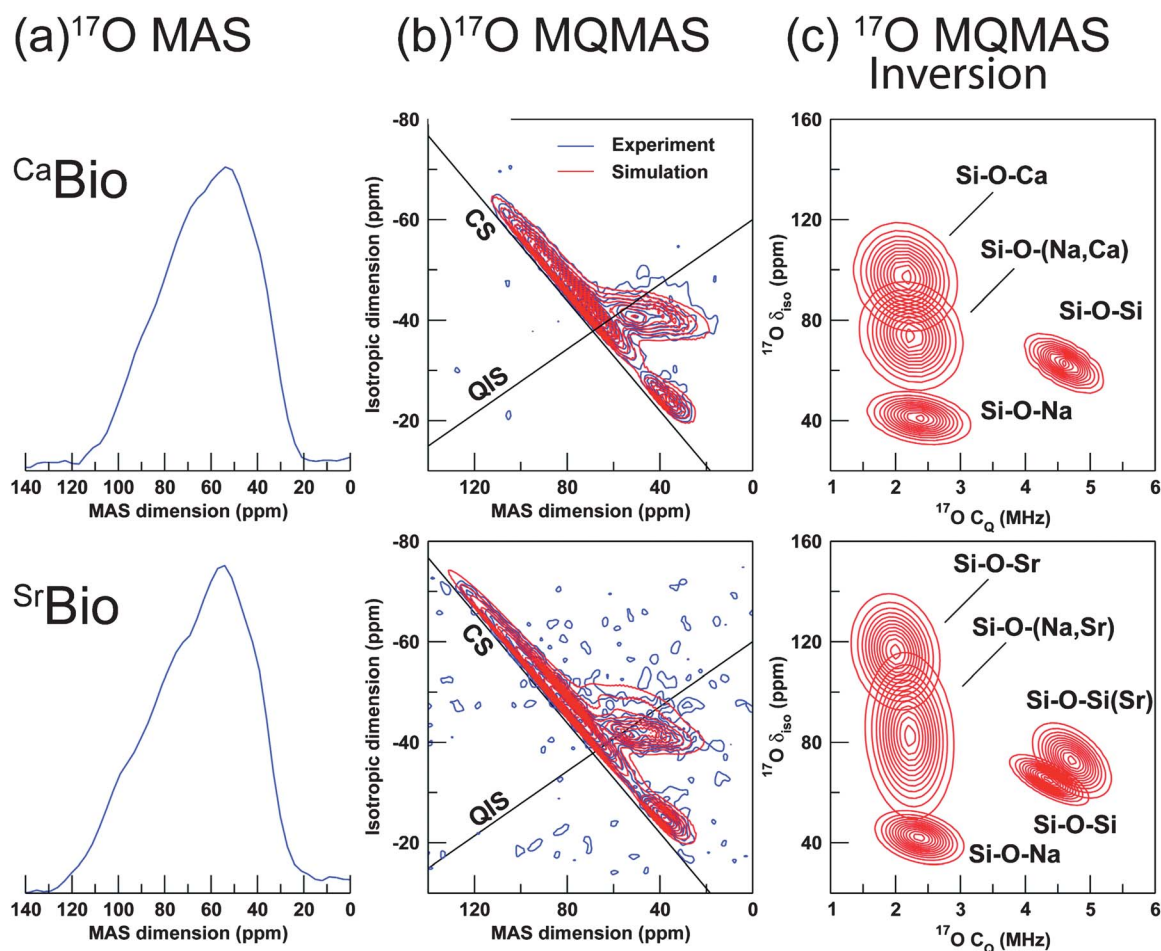


Fig. 5 ^{17}O solid state MAS NMR data ($\nu_0 = 20$ kHz) showing, (a) 1D MAS spectra, (b) the 3QMAS data and corresponding spectral simulations, and (c) the numerical inversion of the simulated 3QMAS data with assignments.

pectolite ($\text{Ca}_2\text{NaSi}_3\text{O}_8(\text{OH})$) which has a distorted octahedral environment with mean Ca–O distances of 2.36–2.37 Å.⁵⁰ However, a chemical shift of ~41 ppm can also be associated with longer Ca–O distances ~2.71 Å, as observed in perovskites.⁵⁰ This demonstrates, therefore, that the ^{43}Ca MAS NMR is in excellent agreement with the isomorphous neutron diffraction results. The introduction of Sr to this system shifts both resonances to lower field due to next nearest neighbour effects (Ca–O–Sr), however a minimal effect on the measured nearest neighbour (Ca–O) bond lengths is observed (see Table 3).

Fig. 5(a) presents the ^{17}O MAS NMR data for the $^{\text{Ca}}\text{Bio}$ and $^{\text{Sr}}\text{Bio}$ bioglasses. These are generally featureless resonances that preclude any insight into the O speciation that characterises these systems. In contrast, the ^{17}O 3QMAS and numerical inversion data of Fig. 5(b) and (c), respectively, evidently resolve this speciation and permit clear comparisons to be drawn. The left side of the 3QMAS numerically inverted data for both systems (see Fig. 5(c)) shows three distinct O environments in the ^{17}O C_Q region of ~2 to 2.5 MHz; as δ_{iso} increases these are assigned to Si–O–Na, Si–O–(Na, M) and Si–O–M environments (where M represents Ca or Sr),⁵³ providing strong evidence for the existence of a range of homo-bonds (Na–O–Na and M–O–M) and hetero-bonds (Na–O–M) within the glass structure. There is no significant variation in the Si–O–Na correlation at $\delta_{\text{iso}} \sim 40$ ppm observed for $^{\text{Ca}}\text{Bio}$ and $^{\text{Sr}}\text{Bio}$, verifying that the substitution of Sr for Ca does not influence the local Na environment. This similarity is also reflected in the ^{23}Na MAS NMR data shown in Fig. 3(b); the ^{23}Na NMR parameters elucidated from the variable B_0 simulation of these lineshapes which describe the structural disorder (using the QUADFIT simulation program)⁵⁴ are summarised in Table 4. These data indicate that the ^{23}Na isotropic shift values consistently reside in the $\delta_{\text{iso}} \sim 8.3$ to 10.5 ppm range, and the corresponding C_Q values are ~6.1 to 7.3 MHz. 2D inversion data for the $^{\text{Sr}}\text{Bio}$ Bioglass (Fig. 5(c)) shows that the δ_{iso} values of the Si–O–(Na, Sr) and Si–O–Sr moieties exhibit a marked downfield shift of ~10 and ~20 ppm, respectively, in comparison to its $^{\text{Ca}}\text{Bio}$ counterpart. This shift to increased deshielding is consistent with the longer Sr–O bond lengths, compared to Ca–O bond length, reported by the neutron diffraction measurements (see Table 3). Furthermore, the Si–O–(Na, Sr) and Si–O–Sr moieties for $^{\text{Sr}}\text{Bio}$ exhibit a greater distribution in their ^{17}O δ_{iso} values as evidenced by the projection upon the CS axis in Fig. 5(b), and the elongated Si–O–(Na, Sr) and Si–O–Sr correlations in Fig. 5(c), suggesting a greater variation in the Sr–O distribution compared to the Ca–O distribution. This is consistent with the neutron diffraction data, where the structural disorder parameter of Sr–O is 0.14 for the dominant peak at 2.49 Å compared to 0.10 for the Ca–O distribution at 2.33 Å.

The Si–O–Si correlation at $\delta_{\text{iso}} \sim 65$ ppm, characterised by a larger C_Q value of ~4.5 MHz appears unperturbed by the substitution of Ca for Sr. However, a weak second correlation assigned to a Si–O_B–Si(Sr) moiety is observed in $^{\text{Sr}}\text{Bio}$ at $\delta_{\text{iso}} \sim 70$ ppm and exhibits a slightly larger C_Q value of ~4.75 MHz. Previously reported ^{17}O 3QMAS studies on Ca Bioglass have not resolved contributions from Si–O_B–Si(Ca) and Si–O_B–Si(Na).⁵³

Sr K-edge EXAFS for the $^{\text{Sr}}\text{Bio}$ and the $^{\text{CaSr}}\text{Bio}$ systems are shown in Fig. 6. The $^{\text{Sr}}\text{Bio}$ and $^{\text{CaSr}}\text{Bio}$ EXAFS, represented by the broken and solid grey curves respectively, are almost

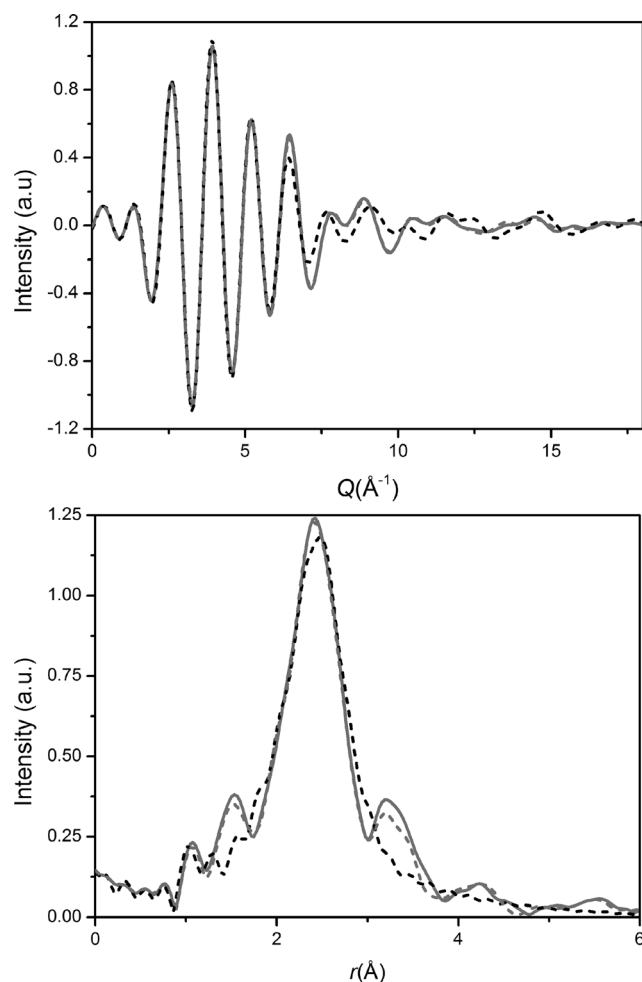


Fig. 6 Sr K-edge EXAFS spectra (a) reciprocal space data and (b) real space data. The $^{\text{CaSr}}\text{Bio}$ and $^{\text{Sr}}\text{Bio}$ data are represented by the grey dashed and solid curves respectively and the fit is given by the black dashed curve.

indistinguishable and confirm that the local nearest neighbour environment surrounding Sr is unaffected by substituting half of the Sr by Ca. A model system, representing the first shell of Sr in an octahedral environment with a mean Sr–O distance of 2.51 Å (broken dark curve), is in reasonable agreement with the measured $^{\text{Sr}}\text{Bio}$ and $^{\text{CaSr}}\text{Bio}$ datasets. The EXAFS data is therefore in good agreement with the neutron diffraction data (Table 3) where a distorted octahedral environment is reported where the main peak resides at 2.49(2) Å and a total Sr–O coordination number of 6.0 is reported.

As a result of the isomorphous substitution, and confirmation of the results through NMR and EXAFS, it is now possible to return to $T(r)$, Fig. 2(a), and fit the complex overlapping correlations. The short-range order comprises ~4 oxygens around Si at ~1.62 Å and ~4 oxygens around P at between 1.5–1.6 Å, depending on whether the P–O are bridging or non-bridging (also referred to as terminal).⁵⁵ As discussed the intermediate range order between 2.1–2.9 Å consists of overlapping Ca–O (and/or Sr–O), Na–O, O–(P)–O and O–(Si)–O correlations and cannot usually be unambiguously deconvolved. However, by accurately determining the Ca–O (and Sr–O) correlations using

the first order difference method, the remaining region is simplified and requires in addition only Na–O and O···O correlations to be fitted. Furthermore, it is possible to estimate *a priori* the most probable O···O correlations: the O–(P)–O and O–(Si)–O are both tetrahedrally coordinated, therefore the O–(X)–O separation is given by $\sqrt{8/3}r_{X-O}$, where X represents P or Si. The concentration of Si is more than 20 times greater than the concentration of P; the O···O correlation can therefore be modelled using a single O···O correlation that is largely determined by the O–(Si)–O term.

The O···O coordination number can be calculated using network connectivity models and confirmed using NMR data. For a silicate glass the network connectivity (NC) is given by

$$NC = 4 - 2Z, \quad (11)$$

where Z , the number of excess oxygens per SiO_2 , is given by

$$Z = \frac{c_O}{c_{\text{Si}}} - 2 \quad (12)$$

where c_O and c_{Si} represent the concentration of oxygen and silicon respectively.

The addition of P complicates the connectivity slightly since P does not behave in an identical manner to Si and eqn (12) cannot therefore be modified simply by substituting c_{Si} for $c_{\text{Si}} + c_{\text{P}}$. For a phosphate-based glass, $NC = 3 - y$, where y , the number of excess O per P_2O_5 , is given by $y = 2c_O/c_{\text{P}} - 5$.^{56,57}

^{31}P MAS NMR data (see Fig. 3(c)) shows a single resonance at $\delta_{\text{iso}} \sim 10$ ppm representing Q^0 species which are essentially isolated PO_4 moieties present throughout the structure.⁵³ There is no evidence of more covalent Si–O–P linkages as suggested by the absence of significant ^{31}P MAS sideband structure that would invoke a substantial chemical shift anisotropy (CSA) expected from such environments. The ^{17}O 3QMAS (Fig. 5(b) and (c)) also shows no signs of Si–O–P sites. This is consistent with results recently published by Pedone *et al.*⁵³

Since each phosphorus atom is surrounded by 4 non-bridging oxygen atoms, the number of excess oxygen atoms per SiO_2 is reduced accordingly and eqn (12) becomes

$$Z' = \frac{c_O - 4c_{\text{P}}}{c_{\text{Si}}} - 2 \quad (13)$$

In this case, c_O , c_{Si} and c_{P} are 0.603, 0.194 and 0.008 respectively. Therefore, $Z' = 0.935$ and the network connectivity of the glass is equal to 2.13. This corresponds to 13% of the Si occupying Q^3 connectivity and 87% occupying Q^2 connectivity. The ^{29}Si MAS NMR data (see Fig. 3(d)) show asymmetric resonances which can be deconvolved into two Gaussian components located at $\delta = -79$ and -86 ppm, which are assigned to be Q^2 and Q^3 units, respectively. The resultant fits give Q^3 abundances of 17%, 11% and 19% for the $^{\text{Ca}}\text{Bio}$, $^{\text{CaSr}}\text{Bio}$ and $^{\text{Sr}}\text{Bio}$ respectively, with the balance of the Si speciation occupying a Q^2 environment. The experimental data is therefore in good agreement with the calculated values (within experimental uncertainties). Knowledge of the Q speciation allows the average O···O coordination number to be calculated. A bridging O atom has six next nearest neighbour O atoms whilst a non-bridging O has only three next nearest neighbour O atoms. Thus, a Si atom having a Q speciation of Q^2 or Q^3 will have O···O coordination numbers

of 4 and 4.8 respectively. It can therefore be calculated that the average O–(Si)–O coordination number associated with the samples discussed herein is 4.10. Taking the small concentration of P into account, which is in an orthophosphate environment with a corresponding average O–(P)–O coordination number of 3, and allowing for the relative concentrations, the overall average O···O coordination number of these glasses is therefore estimated to be 4.06. The O···O peak position is expected to occur at ~ 2.66 Å, given that $r_{O-(\text{Si})-O} = \sqrt{8/3}r_{\text{Si}-O}$, where $r_{\text{Si}-O}$ is 1.63 Å. Thus, the complex region containing overlapping Ca–O, Na–O, O–(P)–O and O–(Si)–O correlations has effectively been further simplified and can now be modelled using the experimentally determined Ca–O input parameters and the O–(P)–O and O–(Si)–O parameters derived above, and confirmed using NMR. The only truly unknown feature remaining in this region of the total diffraction pattern (*i.e.* $r < 3$ Å) is the Na–O correlation.

The O···O coordination number calculated above is larger than the coordination determined by previous Reverse Monte Carlo simulation, which estimated an O···O coordination number of ~ 3.0 .⁵⁸ Given the significant weighting of the O···O term in the neutron diffraction studies modelled, this underestimation of coordination number has a significant effect upon modelling the remaining overlapping correlations in the intermediate range order.

The total structure factors were modelled using the above input factors. An initial attempt to fit the $T(r)$ functions using a single Na–O correlation resulted in a poor fit, and the data was thereafter modelled using two Na–O correlations. The fits are shown in Fig. 2(a) and the output parameters are given in Table 5.

A split Na–O peak has been predicted in molecular dynamics (MD) simulations for sodium silicates and for Bioglass.^{59,60} However, published MD results for Bioglass are dependent upon the type of simulation employed. For example, classical MD simulations using Shell Models, Rigid Ion Models and Car–Parrinello simulations predicted Na– O_{NB} distances of 2.33, 2.38 and 2.28 Å respectively with between 4.0 and 4.6 oxygen atoms surrounding each sodium atom, whilst Na– O_{B} distances ranging between 2.45 and 2.52 Å were reported with Na–O coordination numbers between 1.0 and 1.6.⁶⁰ In sodium silicates a lower Na– O_{NB} coordination of ~ 2.8 was reported.⁵⁹ In crystalline $\text{Na}_2\text{CaSi}_2\text{O}_6$ and $\text{Na}_2\text{SrSi}_2\text{O}_6$ a wide range of Na–O distances are reported: 2.30–2.90 Å,⁴¹ and 2.38–2.75 Å (ref. 46) respectively. Recently a split Na–O peak in Bioglass has been confirmed by employing an effective isomorphous difference study.⁶¹ Thus, the decision to fit the Na–O correlation with two separate peaks corresponding to Na– O_{NB} and Na– O_{B} may be justified, and the values reported here (see Table 5) are within the expected values based on existing simulations, recent experimental data and on experimental data from crystalline analogues.

During the fitting process the nominal input values were allowed to vary in order to optimise the fit. Importantly, the parameters were not constrained during this fitting process, even the Ca–O/Sr–O parameters which had been previously measured. It is apparent from the fitting parameters returned that the model is fully self-consistent between the experimental values for the first order difference functions, the total diffraction data, the NMR data and theory.

Table 5 Structural parameters for the total diffraction patterns $T(r)$. Typical errors are $\pm 0.02 \text{ \AA}$ on the peak position (r), ± 0.2 on the coordination number (N) and $\pm 0.02 \text{ \AA}$ on the disorder parameter (σ)

	CaBio			CaSrBio			SrBio		
	$r(\text{\AA})$	N	$\sigma(\text{\AA})$	$r(\text{\AA})$	N	$\sigma(\text{\AA})$	$r(\text{\AA})$	N	$\sigma(\text{\AA})$
P–O	1.55	3.95	0.01	1.58	3.99	0.01	1.56	3.98	0.02
Si–O	1.63	3.93	0.06	1.63	3.82	0.06	1.63	3.92	0.06
Na–O	2.34	3.08	0.14	2.36	3.02	0.14	2.33	3.08	0.15
Na–O	2.64	1.49	0.09	2.64	1.47	0.10	2.66	1.47	0.09
Ca–O	2.34	5.34	0.10	2.32	5.28	0.10	—	—	—
Sr–O	—	—	—	2.51	4.67	0.14	2.51	4.77	0.12
O–O	2.66	4.17	0.10	2.66	4.01	0.10	2.65	4.01	0.10
Ca–O	2.72	1.24	0.17	2.71	1.35	0.17	—	—	—
Sr–O	—	—	—	2.75	1.24	0.23	2.74	1.28	0.09

The key assumption behind isomorphic substitution is that the pair correlations not containing the isomorphs, in this case Ca/Sr, are not significantly affected by the substitution and that these correlations therefore successfully cancel during the formation of the first order difference function. As shown in Table 5, the neutron diffraction correlations not containing Ca or Sr are consistent for each of the three total diffraction patterns. Further support is given by the ^{23}Na NMR spectra (Fig. 3(b)) which confirms there is no variation in the sodium environment upon substituting Sr for Ca within these bioactive glasses, and the Sr K-edge EXAFS (Fig. 6) which confirms there is no variation in the strontium environment upon substituting half the Sr for Ca within these bioactive glasses.

X-ray diffraction measurements were undertaken to verify the above results. The X-ray diffraction weighting factors are significantly different to neutron diffraction weightings, as shown in Fig. 7. The neutron diffraction spectra are dominated by the O–O correlations whereas the X-ray diffraction data is relatively more sensitive to the Ca–O (and/or Sr–O) correlations. The X-ray interference function data is shown in Fig. 8(a) and the corresponding real space data is given in Fig. 8(b). The X-ray data was modelled using the output values from the neutron diffraction as given in Table 5. No attempts were made to optimise the X-ray fitting since the isomorphic neutron diffraction data presented is intrinsically more reliable. For example, the X-ray data has a maximum Q value of 17 \AA^{-1} , compared to 50 \AA^{-1} for the neutron diffraction data, and is therefore relatively broadened in real-space. The neutron-derived fits are in

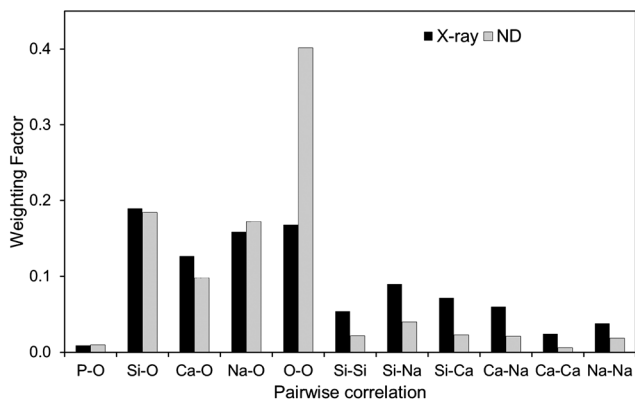


Fig. 7 X-ray and neutron diffraction weighting factors.

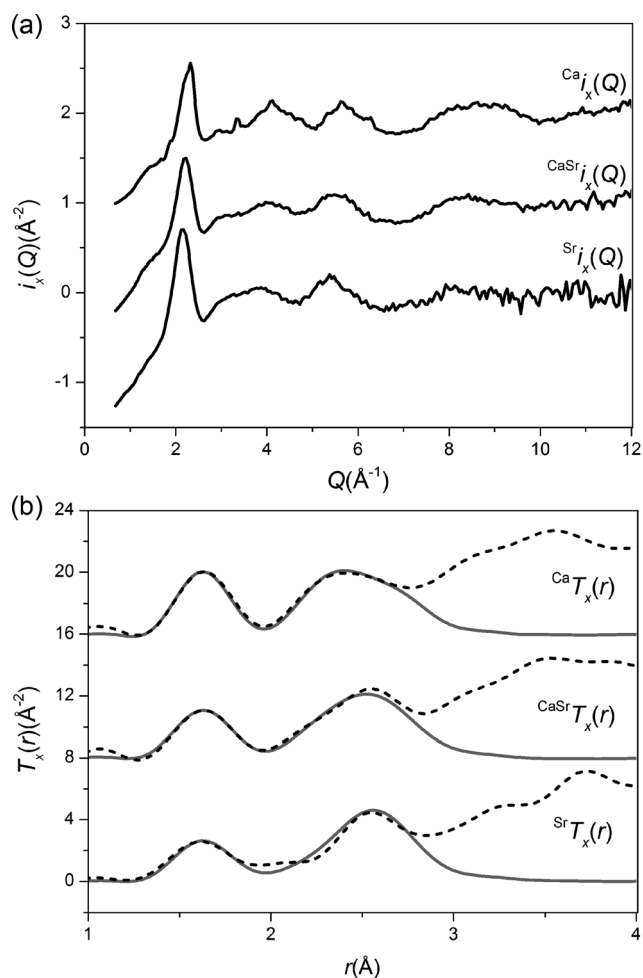


Fig. 8 (a). X-ray diffraction Q -space functions, $i_x(Q)$, measured for CaBio , CaSrBio and SrBio . (b) The real-space data X-ray diffraction patterns, $T_x(r)$, the dashed curve represents the experimental data and the solid curve represents the NXFIT data. The datasets are offset for clarity.

good overall agreement with the total X-ray diffraction patterns. The small variations between the X-ray experimental data and the fit for the SrBio and CaSrBio may be attributed to fluorescence effects. The X-ray diffraction data and the NMR spectra therefore both support the results determined from the neutron diffraction experiments.

Densities of 2.70 , 2.83 and 3.03 g cm^{-3} ($\pm 0.01 \text{ g cm}^{-3}$) were recorded for CaBio , CaSrBio and SrBio respectively via He pycnometry; the increase in density being directly attributed to the increased atomic weight of Sr compared to Ca. Glass transition temperatures, T_g , of 523 , 480 and $462 \text{ }^\circ\text{C}$ ($\pm 1 \text{ }^\circ\text{C}$) were recorded for CaBio , CaSrBio and SrBio respectively using DSC. The decrease in T_g is attributed to the expansion of the glass due to the increase in ionic radius of Sr compared to Ca.^{62,63} Based on the experimentally measured densities and the mean atomic weight, an expansion of the glass of the order 5.3% is calculated; using the nearest neighbour Ca–O and Sr–O distances an expansion of 5.1% is predicted for these glasses. This broad agreement provides assurance that the small differences in glass structure are due to the difference in ionic radius of Sr compared to Ca. The observed expansion of the glass network is thought to result in faster ion release and dissolution and increased bioactivity.⁶⁴

4. Conclusions

Neutron diffraction data affords a detailed structural model of the local and intermediate range order in an important class of bioactive glasses wherein the study of the Ca site is made more tractable by substituting Sr for Ca within these systems. The conclusions drawn from these neutron diffraction studies are strongly supported by the complementary multinuclear solid state MAS NMR and X-ray diffraction data. The diffraction and NMR studies both suggest that Ca adopts two distinct environments within these glasses. The assumption that isomorphic substitution could be employed to determine the short and intermediate range order of Ca and Sr bioactive glasses was verified. The Ca–O environment for the present melt-quench glass was found to be very similar to those present in sol–gel derived bioactive glasses with significantly different compositions, with the exception of the Ca–OH correlation present in the sol–gel derived glasses being absent here. This indicates that the presence of sodium (and Ca–OH) does not significantly affect the coexisting Ca–O_B and Ca–O_{NB} correlations. Bioglass is a complex glass system, containing 5 separate elements and 15 overlapping correlation functions: the present study therefore represents one of the most detailed studies undertaken on any glassy system and has resulted in the characterisation of the short and intermediate range order. Through the detailed identification and characterisation of the sites, especially those associated with calcium and strontium, understanding the structural features that drive important bioactive properties becomes possible.

Acknowledgements

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References

- 1 L. L. Hench, *J. Mater. Sci.: Mater. Med.*, 2006, **17**, 967.
- 2 L. L. Hench, R. J. Splinter, W. C. Allen and T. K. Greenlee, *J. Biomed. Mater. Res. Symp.*, 1971, **5**, 25.
- 3 J. C. Knowles, *J. Mater. Chem.*, 2003, **13**, 2395.
- 4 R. G. Hill, A. Stamboulis, R. V. Law, A. Clifford, M. R. Towler and C. Crowley, *J. Non-Cryst. Solids*, 2004, **336**, 223.
- 5 E. Canalis, M. Hott, P. Deloffre, Y. Tsouderos and P. J. Marie, *Bone*, 1996, **18**, 517.
- 6 A. Guida, M. R. Towler, J. G. Wall, R. G. Hill and S. Eramo, *J. Mater. Sci. Lett.*, 2003, **22**, 1401.
- 7 R. Shannon, *Acta Crystallogr., Sect. A: Cryst. Phys., Diff., Theor. Gen. Crystallogr.*, 1976, **32**, 751.
- 8 J. Terra, E. R. Dourado, J. G. Eon, D. E. Ellis, G. Gonzalez and A. Malta Rossi, *Phys. Chem. Chem. Phys.*, 2009, **11**, 568.
- 9 S. Sugiyama, T. Moriga, M. Goda, H. Hayashi and J. B. Moffat, *J. Chem. Soc., Faraday Trans.*, 1996, **92**, 4305.
- 10 S. G. Dahl, P. Allain, P. J. Marie, Y. Mauras, G. Boivin, P. Ammann, Y. Tsouderos, P. D. Delmas and C. Christiansen, *Bone*, 2001, **28**, 446.
- 11 M. D. Grynpas and P. J. Marie, *Bone*, 1990, **11**, 313.
- 12 P. J. Marie, M. T. Garba, M. Hott and L. Miravet, *Miner. Electrolyte Metab.*, 1985, **11**, 5.
- 13 A. Barbara, P. Delannoy, B. G. Denis and P. J. Marie, *Metab., Clin. Exp.*, 2004, **53**, 532.
- 14 P. J. Marie, *Bone*, 2007, **40**, S5.
- 15 P. J. Marie, *Osteoporosis Int.*, 2005, **16**(suppl. 1), S7.
- 16 P. J. Meunier, C. Roux, E. Seeman, S. Ortolani, J. E. Badurski, T. D. Spector, J. Cannata, A. Balogh, E. M. Lemmel, S. Pors-Nielsen, R. Rizzoli, H. K. Genant and J. Y. Reginster, *N. Engl. J. Med.*, 2004, **350**, 459.
- 17 J. Y. Reginster, E. Seeman, M. C. De Vernejoul, S. Adami, J. Compston, C. Phenekos, J. P. Devogelaer, M. D. Curiel, A. Sawicki, S. Goemaere, O. H. Sorensen, D. Felsenberg and P. J. Meunier, *J. Clin. Endocrinol. Metab.*, 2005, **90**, 2816.
- 18 M. G. Dedhiya, F. Young and W. I. Higuchi, *J. Dent. Res.*, 1973, **52**, 1097.
- 19 M. E. J. Curzon, *J. Dent. Res.*, 1985, **64**, 1386.
- 20 T. M. Athanassouli, D. S. Papastathopoulos and A. X. Apostolopoulos, *J. Dent. Res.*, 1983, **62**, 989.
- 21 T. T. Thuy, H. Nakagaki, K. Kato, P. A. Hung, J. Inukai, S. Tsuboi, H. Nakagaki, M. N. Hirose, S. Igarashi and C. Robinson, *Arch. Oral Biol.*, 2008, **53**, 1017.
- 22 J. D. B. Featherstone, C. P. Shields, B. Khademazad and M. D. Oldershaw, *J. Dent. Res.*, 1983, **62**, 1049.
- 23 L. J. Skipper, F. E. Sowrey, D. M. Pickup, K. O. Drake, M. E. Smith, P. Saravanapavan, L. L. Hench and R. J. Newport, *J. Mater. Chem.*, 2005, **15**, 2369.
- 24 L. J. Skipper, F. E. Sowrey, R. Rashid, R. J. Newport, Z. Lin and M. E. Smith, *Phys. Chem. Glasses*, 2005, **46**, 372.
- 25 V. FitzGerald, R. A. Martin, J. R. Jones, D. Qiu, K. M. Wetherall, R. M. Moss and R. J. Newport, *J. Biomed. Mater. Res., Part A*, 2009, **91**, 76.
- 26 Z. J. Lin, M. E. Smith, F. E. Sowrey and R. J. Newport, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 2004, **69**, 224107.
- 27 R. Hill, *J. Mater. Sci. Lett.*, 1996, **15**, 1122.
- 28 I. Elgayar, A. E. Aliev, A. R. Boccaccini and R. G. Hill, *J. Non-Cryst. Solids*, 2005, **351**, 173.
- 29 R. A. Martin, H. Twyman, D. Qiu, J. C. Knowles and R. J. Newport, *J. Mater. Sci.: Mater. Med.*, 2009, **20**, 883.
- 30 A. C. Hannon, *Nucl. Instrum. Methods Phys. Res., Sect. A*, 2005, **551**, 88.
- 31 P. H. Gaskell, *Glasses and Amorphous Materials, Materials Science and Technology*, 9th edn, 1991, p. 175.
- 32 R. A. Martin, P. S. Salmon, H. E. Fischer and G. J. Cuello, *J. Phys.: Condens. Matter*, 2003, **15**, 8235.
- 33 R. A. Martin, P. S. Salmon, H. E. Fischer and G. J. Cuello, *Phys. Rev. Lett.*, 2003, **90**, 185501.
- 34 J.-P. Amoureux, C. Fernandez and S. Steuernagel, *J. Magn. Reson., Ser. A*, 1996, **123**, 116.
- 35 A. J. Dent, G. Cibin, S. Ramos, A. D. Smith, S. M. Scott, L. Varandas, M. R. Pearson, N. A. Krumpa, C. P. Jones and P. E. Robbins, *B18: A Core XAS Spectroscopy Beamline for Diamond*, 14th International Conference on X-Ray Absorption Fine Structure, ed. A. F. A. DiCicco, 2009, vol. 190.
- 36 B. Ravel and M. Newville, *J. Synchrotron Radiat.*, 2005, **12**, 537.
- 37 M. Newville, *J. Synchrotron Radiat.*, 2001, **8**, 322.
- 38 A. K. Soper and E. R. Barney, *J. Appl. Crystallogr.*, 2011, **44**, 714.
- 39 B. E. Warren, *X-ray Diffraction*, 1990.
- 40 R. M. Moss, PhD thesis, University of Kent, 2009.
- 41 H. Ohsato, I. Maki and Y. Takeuchi, *Acta Crystallogr., Sect. C: Cryst. Struct. Commun.*, 1985, **41**, 1575.
- 42 R. J. Newport, L. J. Skipper, V. FitzGerald, D. M. Pickup, M. E. Smith and J. R. Jones, *J. Non-Cryst. Solids*, 2007, **353**, 1854.
- 43 S. K. Lee and J. F. Stebbins, *J. Phys. Chem. B*, 2003, **107**, 3141.
- 44 F. Nishi, *Acta Crystallogr., Sect. C: Cryst. Struct. Commun.*, 1997, **53**, 534.
- 45 R. E. Marsh and F. H. Herbstein, *Acta Crystallogr., Sect. B: Struct. Sci.*, 1983, **39**, 280.

- 46 V. Kahlenberg, *J. Alloys Compd.*, 2004, **366**, 132.
- 47 R. A. Martin, S. Yue, J. V. Hanna, P. D. Lee, R. J. Newport, M. E. Smith and J. R. Jones, *Philos. Trans. R. Soc., A*, 2012, **370**, 1422.
- 48 A. Samoson, *J. Magn. Reson., Ser. A*, 1996, **121**, 209.
- 49 A. P. M. Kentgens, *Geoderma*, 1997, **80**, 271.
- 50 R. Dupree, A. P. Howes and S. C. Kohn, *Chem. Phys. Lett.*, 1997, **276**, 399.
- 51 C. Gervais, D. Laurencin, A. Wong, F. Pourpoint, J. Labram, B. Woodward, A. P. Howes, K. J. Pike, R. Dupree, F. Mauri, C. Bonhomme and M. E. Smith, *Chem. Phys. Lett.*, 2008, **464**, 42.
- 52 F. Angeli, M. Gaillard, P. Jollivet and T. Charpentier, *Chem. Phys. Lett.*, 2007, **440**, 324.
- 53 A. Pedone, T. Charpentier, G. Malavasi and M. C. Menziani, *Chem. Mater.*, 2010, **22**, 5644.
- 54 T. F. Kemp and M. E. Smith, *Solid State Nucl. Magn. Reson.*, 2009, **35**, 243.
- 55 U. Hoppe, G. Walter, A. Barz, D. Stachel and A. C. Hannon, *J. Phys.: Condens. Matter*, 1998, **10**, 261.
- 56 R. A. Martin, P. S. Salmon, C. J. Benmore, H. E. Fischer and G. J. Cuello, *Phys. Rev. B: Condens. Matter Mater. Phys.*, 2003, **68**, 054203.
- 57 R. A. Martin, P. S. Salmon, H. E. Fischer and G. J. Cuello, *J. Non-Cryst. Solids*, 2004, **345–346**, 208.
- 58 V. FitzGerald, D. M. Pickup, D. Greenspan, G. Sarkar, J. J. Fitzgerald, K. M. Wetherall, R. M. Moss, J. R. Jones and R. J. Newport, *Adv. Funct. Mater.*, 2007, **17**, 3746.
- 59 A. N. Cormack and J. C. Du, *J. Non-Cryst. Solids*, 2001, **293**, 283.
- 60 A. Tilocca, *J. Chem. Phys.*, 2008, **129**, 084504.
- 61 R. A. Martin, H. L. Twyman, G. J. Rees, J. M. Smith, E. R. Barney, M. E. Smith, J. V. Hanna and R. J. Newport, *Phys. Chem. Chem. Phys.*, 2012, **14**, 12105.
- 62 Y. Xiang and J. Du, *Chem. Mater.*, 2011, **23**, 2703.
- 63 Y. C. Fredholm, N. Karpukhina, R. V. Law and R. G. Hill, *J. Non-Cryst. Solids*, 2010, **356**, 2546.
- 64 Y. C. Fredholm, N. Karpukhina, D. S. Brauer, J. R. Jones, R. V. Law and R. G. Hill, *J. R. Soc., Interface*, 2011, 1742.