







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To chelate thallium(i) – synthesis and evaluation of Kryptofix-based chelators for $^{201}\text{Tl}^{\dagger}$

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While best known for its toxic properties, thallium has also been explored for applications in nuclear diagnostics and medicine. Indeed, [^{201}Tl]TlCl has been used extensively for nuclear imaging in the past before it was superseded by other radionuclides such as $^{99\text{m}}\text{Tc}$. One reason for this loss of interest is the severe lack of suitable organic chelators able to effectively coordinate ionic forms of Tl and deliver it to specific diseased tissue by means of attached biological vectors. Herein, we describe the synthesis and characterisation of a series of Kryptofix 222-based chelators that can be radiolabelled with $^{201}\text{Tl}(\text{i})$ in high radiochemical yields at ambient temperature. We demonstrate that from these simple chelators, targeted derivatives are readily accessible and describe the synthesis and preliminary biological evaluation of a PSMA-targeted ^{201}Tl -labelled Kryptofix 222-peptide conjugate. While the Kryptofix system is demonstrably capable of binding the thallium cation, no PSMA-mediated cell-uptake could be detected with the PSMA conjugate, suggesting that this targeting moiety may not be ideal for use in conjunction with ^{201}Tl .

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Introduction

Thallium is most commonly known for its detrimental properties such as its former use in rat poison or as a popular means to murder in both fiction and non-fiction.¹ However in academic and medical settings, thallium, and in particular its radioactive isotopes have been recognised for their potential utility in healthcare. In 1975 Lebowitz *et al.* discussed the possible application of thallium-201 for myocardial imaging due to the similarities in size between Tl(i) and K(i).² Thallium-201 (^{201}Tl) has a half-life of 73 hours and emits γ -photons at 72 keV (X-ray, 94% abundance), 135 keV (3% abundance) and 167 keV (10% abundance) making it suitable for application in single photo emission computed tomography (SPECT). As predicted, ^{201}Tl initially found widespread use as a myocardial imaging agent until it was replaced by emerging technetium-99 m tracers.³ In a few instances [^{201}Tl]TlCl has also been employed for tumour detection and monitoring.⁴ Additionally, ^{201}Tl decays through electron capture (EC) to ^{201}Hg , emitting an average of 36.9 Meitner-Auger electrons per decay event. Meitner-Auger electron-emitting agents have

shown significant potential for application in systemic, targeted radionuclide therapy of cancer.⁵ With its high decay yield of Meitner-Auger electrons, ^{201}Tl has promise as a radiotherapeutic isotope and possibly for theranostic applications.⁶

The clinical application of ^{201}Tl is currently limited to its use as the “free” or “unchelated” metal ion. Many other radioactive metallic isotopes have demonstrated clinical utility but are largely used in a complexed or chelated form. For example, [^{68}Ga]Ga³⁺ and [^{177}Lu]Lu³⁺ can be complexed to chelators which are appended to peptides that target receptors expressed in cancer tissue. The ensuing ^{68}Ga and ^{177}Lu radiopharmaceuticals are used for PET imaging and systemic radiotherapy respectively, and have had clinical impact in management and treatment of neuroendocrine cancer and prostate cancer.⁷ Advancements in the development of new ^{201}Tl -based radiopharmaceuticals are currently prevented by an almost complete lack of studies into the formation of stable compounds between thallium and organic chelators that could feature biological targeting functions. Thus far, only two studies have investigated the coordination of thallium to popular radioimaging chelators. In 2011, Hijnen *et al.* described the evaluation of [^{201}Tl]Tl(III)-DOTA (1,4,7,10-tetraazacyclododecane-*N,N',N'',N'''* tetraacetic acid) complexes. The authors oxidized the readily available $^{201}\text{Tl}(\text{i})$ by treatment with hydrochloric acid and ozone and found good radiochemical yields and purity for the formation of DOTA and DTPA (diethylenetriaminepentaacetic acid) [^{201}Tl]Tl(III)-labelled complexes. Unfortunately, the DTPA compound was found to rapidly decay in human blood serum. Although the DOTA complex

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was found to be stable in serum, the biodistribution of the compound mirrored that of non-chelated or “free” $[^{201}\text{Tl}]\text{Tl}(\text{i})$, suggesting limited stability of $[^{201}\text{Tl}]\text{Tl}(\text{iii})\text{-DOTA}$ *in vivo*.⁸ Interestingly, Fodor *et al.* described the same complex as an “extraordinarily robust macrocyclic complex” in a 2015 report.⁹ However no *in vivo* experiments were reported, suggesting that while $[^{\text{nat}}\text{Tl}]\text{Tl}(\text{iii})\text{-DOTA}$ may possess favorable stability *in vitro*, the $\text{Tl}(\text{iii})$ core is readily reduced *in vivo*, leading to rapid decomplexation.

We recently described a more robust protocol for the oxidation of commercially available $[^{201}\text{Tl}]\text{Tl}(\text{i})\text{Cl}$ to $[^{201}\text{Tl}]\text{Tl}(\text{iii})\text{Cl}_3$. In this work the ability of the readily available chelators, DTPA, DOTA and EDTA, for binding $[^{201}\text{Tl}]\text{Tl}(\text{iii})$ was investigated. Radiolabelling was possible with all three chelators as evidenced by iTLC, however only $[^{201}\text{Tl}]\text{Tl}(\text{iii})\text{-DOTA}$ showed sufficient stability in human serum, ruling out the other two chelates for *in vivo* applications.¹⁰

While the ability to chelate $[^{201}\text{Tl}]\text{Tl}(\text{iii})$ with sufficient stability required for *in vivo* applications is promising (though yet to be fully realized), this approach will always be susceptible to *in vivo* reduction of $[^{201}\text{Tl}]\text{Tl}(\text{iii})$ to $[^{201}\text{Tl}]\text{Tl}(\text{i})$, and likely subsequent metal dissociation, as has been indicated by the work of Hijnen. We therefore started to explore the possible chelation of “native” $[^{201}\text{Tl}]\text{Tl}(\text{i})$. This presents some challenges as the monovalent thallium is a very large ion with an ionic radius of 150 pm and, like the alkali metals, its solution chemistry is dominated by aquation.¹¹

We initially looked at two classes of compounds for which there was some evidence in the literature that suggested potential for radiolabelling $[^{201}\text{Tl}]\text{Tl}(\text{i})$, crown ethers and cryptophanes. Crown-ethers are well-documented to bind a wide range of cations.¹² However in our hands, we could not detect any binding of $[^{201}\text{Tl}]\text{Tl}(\text{i})$ by 18-crown-6, dibenzo-18-crown-6 and dicyclohexyl-18-crown-6 under radiolabelling conditions. The group of Brotin has reported an impressive series of different cryptophane derivatives over the last years, including extensive characterization of their ability to bind different cations, including non-radioactive thallium.¹³ As the synthesis of these compounds represents a significant challenge, their group kindly provided us with two samples of cryptophanes with which to conduct preliminary studies. While we did observe the appearance of a new peak in the radio-HPLC upon reaction of **Crypt1** with $[^{201}\text{Tl}]\text{Tl}(\text{i})\text{Cl}$, this could only be achieved under strongly basic conditions (Fig. 1). Adjusting the pH to ~ 7 or exposure to human serum resulted in the release of the thallium cation, hence we did not pursue these chelators any further.

Due to the similarities in ionic radii between $\text{K}(\text{i})$ and $\text{Tl}(\text{i})$ we turned our attention to 4,7,13,16,21,24-hexaoxa-1,10-diazabicyclo[8.8.8]hexacosane, more commonly known as Kryptofix 222. This compound was first reported by Sauvage *et al.* in 1969. In this first report the authors described the remarkable propensity of these compounds to form complexes with “metallic cations”.¹⁴ Since then, this compound class has found applications in many different fields ranging from crystallography to chemical sensing.¹⁵ Interestingly, its ability to

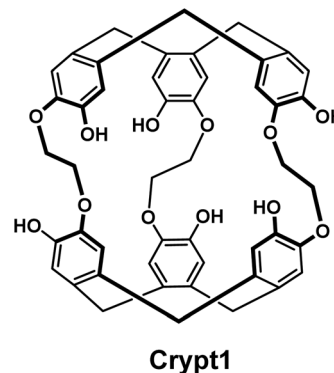


Fig. 1 Chemical structure of the cryptophane **Crypt1**.

encapsulate potassium ions led to its use as a phase-transfer catalyst for the radiosynthesis of $[^{18}\text{F}]\text{-fluoro-2-deoxy-2-D-glucose}$ ($[^{18}\text{F}]\text{FDG}$).¹⁶ Based on these findings we have developed a series of Kryptofix 222 derivatives that can be conjugated to a biological targeting function of choice. Herein we report the synthesis and characterization of these derivatives as well as the preparation of a prostate-cancer targeted analogue. Furthermore, the ability of the Kryptofix compound class to coordinate both non-radioactive and radioactive $[^{201}\text{Tl}]\text{Tl}(\text{i})$ has been investigated.

Results and discussion

Before embarking on the synthesis of functionalized derivatives, the ability of commercially available Kryptofix 222 (**K222**) and Kryptofix 22 (**K22**, Fig. 2) to complex $[^{\text{nat}}\text{Tl}]\text{Tl}(\text{i})$ was investigated by NMR spectroscopy. Addition of TlPF_6 in D_2O to a solution of the cryptand in D_2O resulted in a clear shift in resonances for **K222** but only a very small shift for **K22** (ESI Fig. S1 and S2†). A proof-of-concept radiolabelling study was conducted with **K222**. Incubation of the cryptand with $[^{201}\text{Tl}]\text{TlCl}$ in saline led to almost quantitative formation of a new peak with a significantly higher retention time compared to free $[^{201}\text{Tl}]\text{Tl}(\text{i})$ on reverse-phase radioHPLC (ESI Fig. S3†). Encouraged by these preliminary data we pursued the synthesis of bifunctional **K222** chelators. We focused on **K222-NH₂** as this compound could be conjugated to carboxylic acids *via* amide-coupling, whilst also offering the possibility to convert it to other synthons for “click”-type coupling reactions *i.e.* **K222-N₃** and **K222-DBCO** (Fig. 2).

The synthetic strategy towards **K222-NH₂** was based on works by Gansow,¹⁷ Pettit,¹⁸ and Allen¹⁹ adjusted with our own optimisations (Scheme 1). Compound **1** was obtained by reacting 4-nitrocatechol with ethyl bromoacetate in acetone in the presence of sodium carbonate. The reaction could be shortened to 60 min if conducted in a microwave reactor at 180 °C. Hydrolysis to **2** with excess LiOH was straightforward and the chlorination to **3** with thionyl chloride could be achieved after optimization *i.e.* it was important to keep the reaction refluxing overnight and to directly use the crude product after evap-



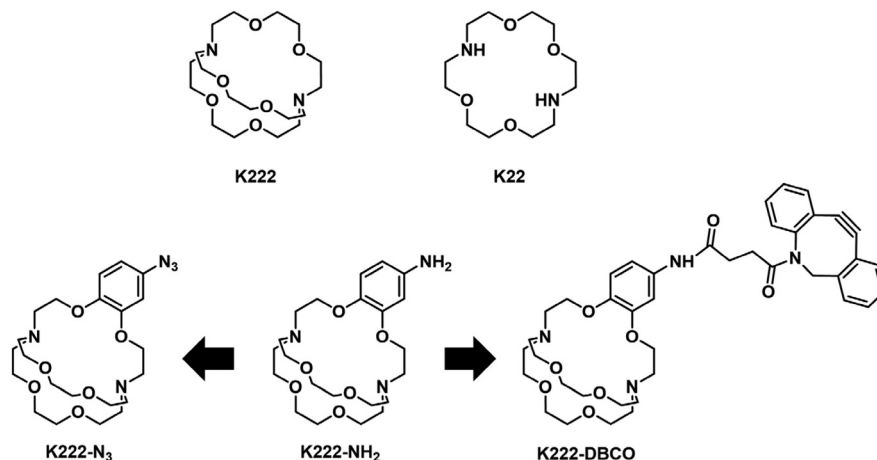
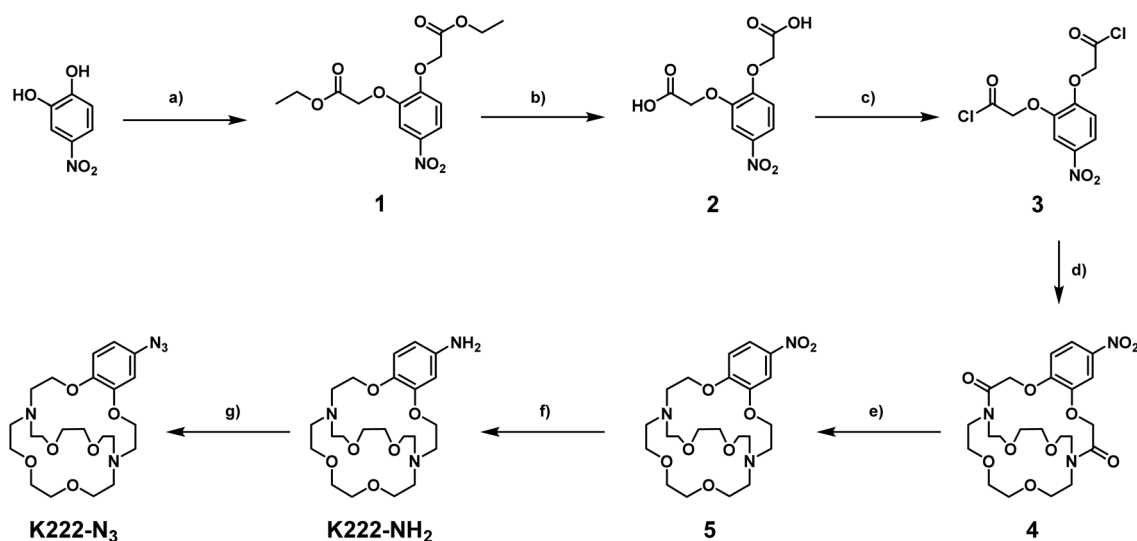


Fig. 2 Chemical structures of Kryptofix 222-based compounds reported in this work.



Scheme 1 Synthetic route towards **K222-NH₂** and **K222-N₃**. Reaction conditions: (a) ethyl bromoacetate, Na₂CO₃, acetone, reflux, 16 h, 45%; (b) LiOH, THF/H₂O, r.t., 16 h, 70%; (c) thionyl chloride, reflux, 16 h; (d) Kryptofix 22, NEt₃, dry toluene, 0–30 °C, 1 h, 25%; (e) BH₃·THF, reflux, 16 h, 55%; (f) Zn dust, AcOH/DCM, r.t., overnight, 43%; (g) FSO₂N₃, 3 M KHCO₃, MTBE/DMF/H₂O, r.t. 5 min, 37%.

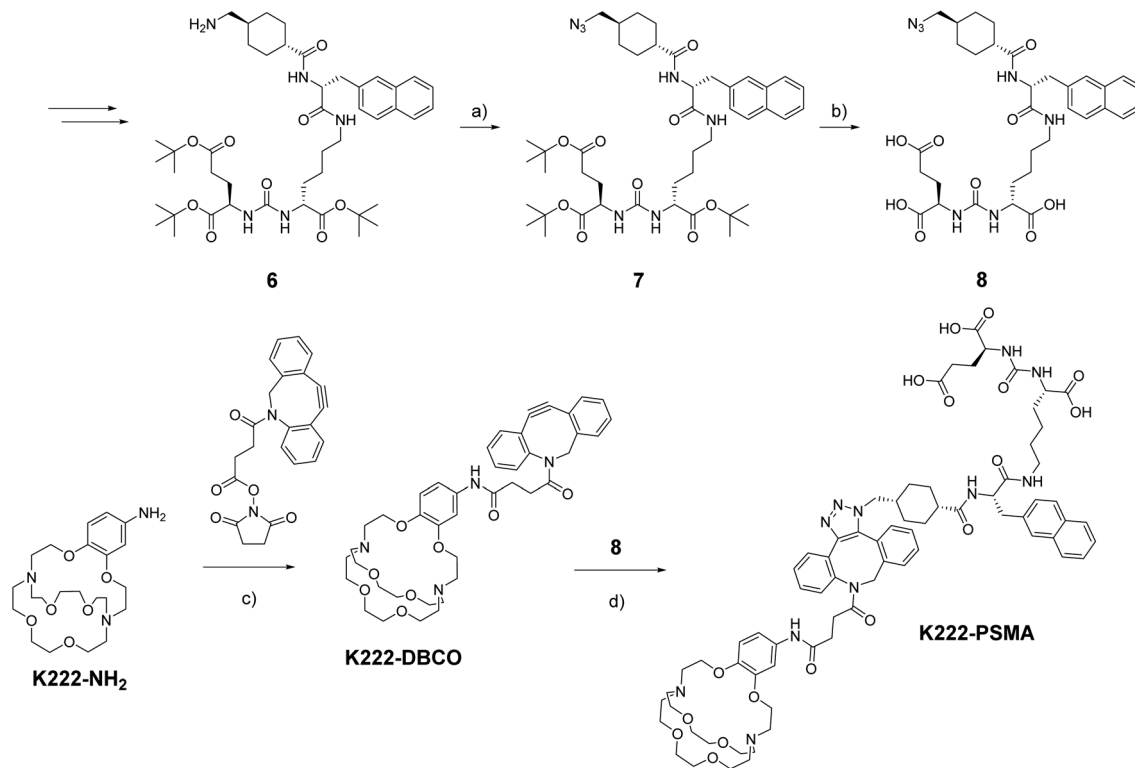
oration of thionyl chloride. For the preparation of **4** both reagents (**3** and Kryptofix 22) were dissolved in fresh anhydrous toluene in separate round-bottom flasks and sonicated until dissolved. Both were added *via* syringe to a third round-bottom flask filled with more anhydrous toluene cooled by means of an ice bath. The speed of addition was not important for this reaction as both slow addition over 1 h by means of a syringe pump and fast addition over 1 minute gave roughly equivalent yields. The reaction was complete after 1 h at room temperature and did not require overnight stirring as described in some literature reports.¹⁹ Compound **5** was obtained by refluxing **4** in BH₃·THF overnight and was used without further purification. Reduction of the nitro group of **5** was achieved by using fine zinc dust instead of powder, giving **K222-NH₂** after purification on a C18 cartridge. FSO₂N₃ was

prepared as described in the literature²⁰ and reacted with **K222-NH₂** to form **K222-N₃** after purification by column chromatography on silica. NHS-ester activated dibenzocyclooctyne (DBCO-NHS) was reacted with **K222-NH₂**, forming **K222-DBCO** as evidenced by LC-MS. This compound was then utilised further without purification.

As a model targeting function, we chose peptidomimetic **6** which has a high affinity for the prostate specific membrane antigen (PSMA), a receptor that is highly overexpressed in prostate cancer cells and for which many cell assays and murine models have been developed over the last decades.²¹

The PSMA-targeting precursor **6** was prepared as described elsewhere.²² Utilizing FSO₂N₃, the terminal amine on **6** was transformed into the azide **7** (Scheme 2). Deprotection with TFA cleaved off all *tert*-butyl protecting groups yielding **8**





Scheme 2 Synthetic route towards **K222-DBCO** and **K222-PSMA** Reaction conditions: (a) FSO_2N_3 , 3 M KHCO_3 , MTBE/DMF/ H_2O , r.t., 5 min; (b) TFA, DCM (1 : 2), r.t., 3 h; (c) DBCO-NHS, DMF, r.t., overnight; (d) **8**, DMF/MeOH (1 : 1), r.t., overnight.

which could be reacted with **K222-DBCO** under copper-free click-conditions forming the final conjugate **K222-PSMA** which was purified by preparative HPLC. The quantity of **K222-PSMA** obtained was not sufficient for NMR assignment. The compound was characterized by ^1H NMR, LC-MS and HR-MS (ESI †).

While this project was ongoing, another group reported on the synthesis and application of **K222** derivatives as chelators for ^{203}Pb , an emerging radiometal for SPECT applications.²³ While the synthetic derivatives reported by McDonagh *et al.* are slightly different to the ones reported here, their general findings that successful radiolabelling is possible with this class of compounds and that the resulting $\text{Pb}(\text{II})$ complexes possess suitable stability in human blood serum, encouraged us to proceed with the investigation of the thallium-binding ability of our compounds.

With all target compounds in hand we proceeded to investigate the ability of these derivatives to bind $\text{Tl}(\text{I})$. First, we repeated the NMR experiments conducted with **K222** and **K22** with the new derivative **5**. Compound **5** was dissolved in CD_3OD and an initial ^1H NMR was recorded. TlPF_6 (1.5 equivalents) was pre-dissolved in CD_3OD , added to the solution of **5** and a second proton spectrum was recorded immediately after (Fig. 3). A clear change in the chemical shifts pertaining to the alkyl-protons of the **K222** scaffold can be observed in the ^1H NMR spectra. On the other hand, the three aromatic protons show little to no change. These experimental findings were

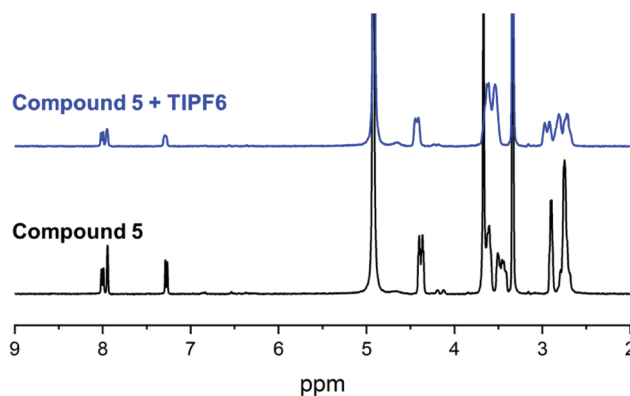


Fig. 3 ^1H NMR binding experiment with compound **5** and TlPF_6 in MeOD.

supplemented with density functional theory (DFT) calculations performed on both the $\text{Tl}(\text{I})$ as well as the $\text{K}(\text{I})$ complexes with ligand **5**. For reference, DFT calculations were also performed for the already reported complex of **K222** with potassium (ESI Fig. S19 †). Comparison of the oxygen- and nitrogen-metal bonds showed good agreement between the calculated and experimentally determined structures. The structures for $\text{Tl}(\text{I})$ (Fig. 4) and $\text{K}(\text{I})$ are similar, with all 6 oxygens and 2 nitrogen atoms of the macrocycle involved in interactions with the metal centre (ESI Fig. S20 †).



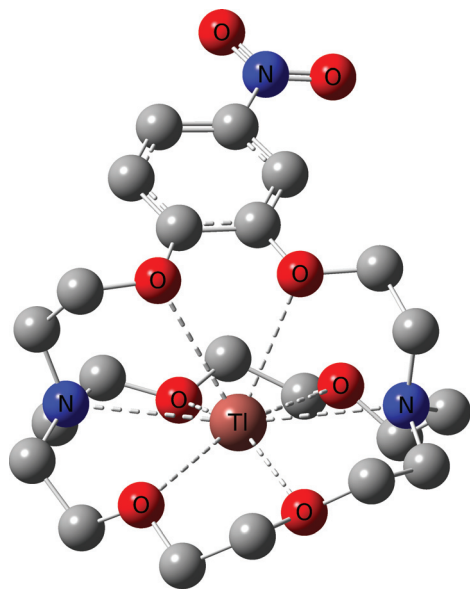


Fig. 4 DFT optimized structure for $\text{Tl}(5)^+$. Hydrogen atoms are omitted for clarity.

Slightly longer distances between putative coordinating atoms and metal centre were detected for the calculated $\text{Tl}(i)$ complex structure compared to the $\text{K}(i)$ analogue (ESI Table S2†). Comparison of the $\text{Tl}(i)$ with the $\text{K}(i)$ coordination environments revealed that the $\text{K}(i)$ ion sits more centrally in the cryptand scaffold whereas in the case of $\text{Tl}(i)$, the ion is located near the plane formed by the four non-aromatic oxygen and nitrogen atoms. These calculations suggest that the binding mode of $\text{K}(i)$ and $\text{Tl}(i)$ are similar with regards to **5** but that in the case of $\text{Tl}(i)$, the metal ion is less encapsulated by the cryptand which could indicate lower stability. Altogether, these experimental and computational studies strongly suggest that an interaction between the chelator and $\text{Tl}(i)$ is occurring and that it is, as expected, between the oxygen and nitrogen atoms of the **K222** cryptand and the thallium cation. As additional confirmation, the NMR solution was analysed by ESI-MS and the mass peak for a thallium ion bound by **5** was detected (ESI Fig. S18†).

All initial radiolabelling studies were conducted with compound **5** as it was available in larger amounts than the other derivatives. Initial attempts at radiolabelling **5** with $^{201}\text{Tl}(i)$ in water were unsuccessful. Reactions were monitored by analytical radioHPLC utilizing a C18 column and a 0–100% water/acetonitrile gradient with 0.1% TFA. During the synthesis of the **K222** derivatives, the last step involves purification on reverse phase columns and through trial and error it was found that neutralisation of the collected fractions *via* addition of 1 M NaOH was necessary, otherwise no chelation of TlPF_6 could be observed by NMR. We hypothesised that this is due to protonation of the nitrogen atom in the macrocycle ring, as supported by DFT calculations. Visualisation of the HOMO for $\text{5}(\text{Tl})$ revealed overlap of nitrogen and Tl-based orbitals, originating from the p and d orbitals, respectively (ESI Fig. S19,†

left image). This interaction was no longer observed in the HOMO upon protonation of the nitrogen (ESI Fig. S19,† right image), and is reflected in the N–Tl distances where an elongation from 3.04 Å to 3.83 Å was observed upon protonation. In the absence of this stabilisation from N–Tl interactions, $\text{Tl}(i)$ was found to reside further away from the aromatic oxygen donors, resulting in a noticeably less enveloped structure. Based on these findings we assume that concentration of collected fractions in the presence of small amounts of HPLC mobile phase acid additives (TFA or formic acid) resulted in the formation of a protonated cryptand which is unable to coordinate $^{201}\text{Tl}(i)$.

With this knowledge in mind, further $^{201}\text{Tl}(i)$ radiolabelling reactions were conducted in water with the addition of small amounts of 1 M Na_2CO_3 (final pH = 11). As no new peaks could be detected by radioHPLC, we hypothesized that the acidic mobile phase resulted in decomplexation of **5** from $^{201}\text{Tl}(i)$. Monitoring of a reaction mixture of **5** and $^{201}\text{Tl}(i)$ under neutral solvent conditions, without inclusion of an ionic solvent modifier, resulted in the observation of a new peak, putatively assigned as $^{201}\text{Tl}(\text{5})^+$, with a retention time that is clearly distinct from that of unchelated ^{201}Tl . Unfortunately, under these conditions, we could not obtain reproducible radio-HPLC traces. We attribute this to adsorption of hydrophilic $^{201}\text{Tl}(\text{5})^+$ to silica as in some repeated experiments, radioactive species were retained on the C18 column and did not elute. Such behaviour is sometimes observed in HPLC experiments using mobile phases without inclusion of a buffering or ion pairing reagent or acid.²⁴ Through further extensive experimentation it was found that addition of 0.01% formic acid to the HPLC mobile phase (pH ~ 4) enabled reproducible radio-HPLC chromatography. With the HPLC conditions optimised, radiosynthetic protocols for preparation of putative $^{201}\text{Tl}(\text{5})^+$ were found to be robust: exclusive formation of $^{201}\text{Tl}(\text{5})^+$ in >95% radiochemical yield was observed upon reaction of **5** with $^{201}\text{Tl}(i)\text{Cl}$ at pH = 11, in aqueous solution at room temperature after 15 minutes reaction time (Fig. 5 left).

Comparison of the UV-trace of **5** with the γ -trace of $^{201}\text{Tl}(\text{5})^+$ shows a large difference between the retention times of the free ligand (8.0 min) and radioactive complex (4.2 min). The $\text{Tl}(i)$ complex of **5** is significantly more hydrophilic than that of the free ligand, which we attribute in part to the single positive charge of $^{201}\text{Tl}(\text{5})^+$, as well as conformational differences between chelated **5** and non-chelated **5**.

With the optimized $^{201}\text{Tl}(i)$ radiolabelling conditions determined for compound **5** we proceeded to the reaction of bioconjugate **K222-PSMA** with $^{201}\text{Tl}(i)\text{Cl}$, which also led to the formation of a single new peak in the radioHPLC (Fig. 5 right). Reaction of **K222-PSMA** with $^{201}\text{Tl}(i)$ yielded putative $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ in >98% radiochemical yield, with a retention time of 5.8 min, distinct from that of **K222-PSMA**, which elutes later, with a retention time of 11.4 min.

So far, all evidence pointed to **K222**-based chelators complexing $\text{Tl}(i)$ under both non-radioactive (stoichiometric) and radioactive (non-stoichiometric tracer) conditions. A crucial



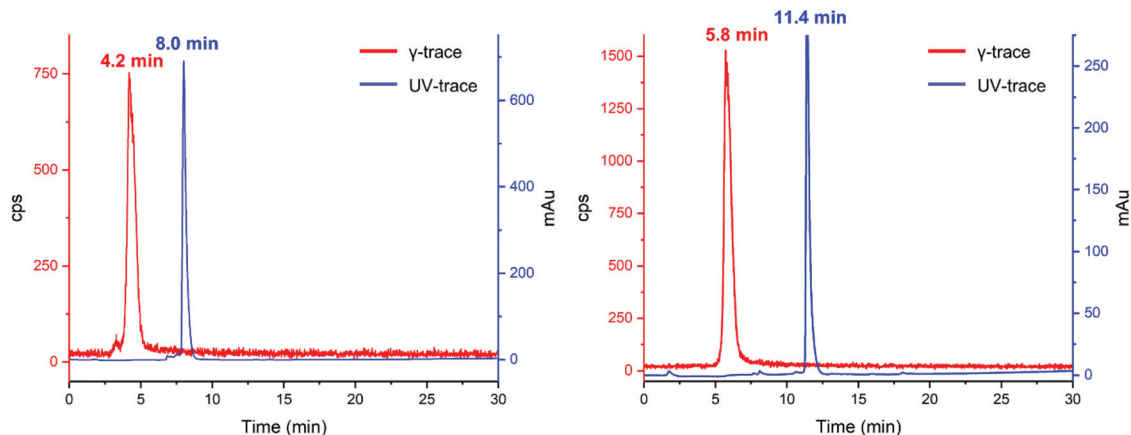


Fig. 5 UV (254 nm, blue) and γ -traces (red) of reaction of **5** (left) and **K222-PSMA** (right) with ^{201}Tl .

benchmark for any radiochelator is not only the ability to bind a given radiometal but stably retain it under physiologically relevant conditions. A common assay to evaluate the stability of radiolabelled bioconjugates is to incubate them with human blood serum over time. We incubated $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ in human blood serum at 37 °C, and monitored its stability. Radio-HPLC analysis of aliquots of serum, taken at 0 min, 30 min and 2 h incubation times, indicated that a fraction (around 10%) of $^{201}\text{Tl}(\text{i})$ was released from **K222-PSMA** immediately upon addition of the serum to $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ (ESI Fig. S17[†]). However, after that, no significant changes were observed, indicating that $^{201}\text{Tl}(\text{i})$ **K222** chelates are relatively stable in human serum over 2 h.

Having shown that $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ exhibits adequate stability under physiological conditions we investigated the ability of this conjugate to specifically bind PSMA *in vitro*. To this end, the PSMA-positive cell line, DU145-PSMA+, and the parental PSMA-negative DU145 cell line (~500 000 cells), were incubated with $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ for either 10 min or 1 h.²¹ Additionally, a control experiment was performed where both cell types were pre-incubated with the PSMA inhibitor, 2-PMPA (2-(phosphonomethyl) pentane-1,5-dioic acid),^{21a} to block PSMA receptors, prior to incubation with $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ for 1 h. After incubation, cells were washed and lysed, and cell lysates were collected and counted for radioactivity using a γ -counter (Fig. 6 and ESI, Table S1[†]).

Uptake of ^{201}Tl activity in DU145-PSMA+ cells measured $4.7 \pm 0.2\%$ AR (percentage added radioactivity to 500 000 cells), however uptake in the PSMA-negative DU145 cell line similarly measured $4.9 \pm 0.2\%$ AR, and uptake in DU145-PSMA+ cells blocked with 2-PMPA measured $5.0 \pm 0.1\%$ AR. This suggested that uptake of ^{201}Tl radioactivity was not mediated by PSMA receptors. To further probe this, both DU145-PSMA+ and DU145 cells were treated with solutions of “free”/“unchelated” $^{201}\text{Tl}[\text{Tl}(\text{i})\text{Cl}]$ for 1 h. ^{201}Tl activity measured $6.1 \pm 0.9\%$ AR in DU145-PSMA+ and $6.3 \pm 0.1\%$ AR in DU145 cells.

The similar values of ^{201}Tl radioactivity in cells treated with either $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ or $^{201}\text{Tl}[\text{Tl}(\text{i})\text{Cl}]$, suggests that in

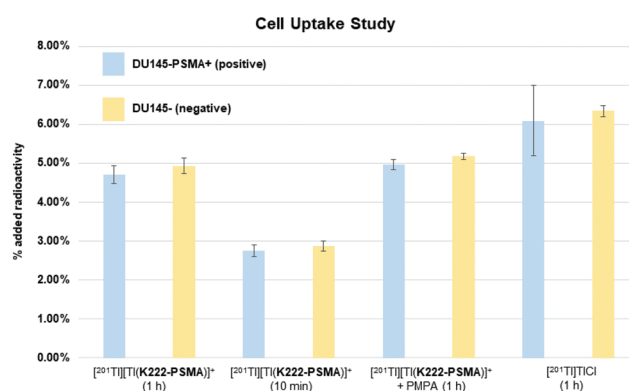


Fig. 6 Cell uptake study results for bioconjugate $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$ in PSMA-positive cell line, DU145-PSMA+ (positive) and the parental PSMA-negative DU145 cell line (negative) after 1 hour and 10 min incubation time (columns 1–4), in the presence of the PSMA inhibitor, 2-PMPA (2-(phosphonomethyl) pentane-1,5-dioic acid, columns 5 and 6). Columns 7 and 8 show the control experiment where positive and negative cells were incubated with “unchelated” $^{201}\text{Tl}[\text{Tl}(\text{i})\text{Cl}]$ for 1 h. Each experiment was conducted twice, values shown are the mean \pm standard deviation.

these *in vitro* experiments, $^{201}\text{Tl}(\text{i})$ dissociates from **K222-PSMA**. With the same charge and a similar ionic radius compared to K(i), biologically, Tl(i) can behave as a K(i) “mimic”.⁶ We hypothesize that after dissociating from **K222-PSMA**, $^{201}\text{Tl}(\text{i})$ is taken up by both DU145-PSMA+ and DU145 cells through potassium ion transporters. This accounts for the similar levels of cellular ^{201}Tl radioactivity, regardless of whether ^{201}Tl is administered as “free” $^{201}\text{Tl}[\text{Tl}(\text{i})\text{Cl}]$ or $^{201}\text{Tl}[\text{Tl}(\text{K222-PSMA})]^+$.

There are many endogenous biomolecules that are likely to compete with ligands such as **K222** derivatives for binding to K(i)-mimics such as Tl(i). For example, potassium ion channels transport K(i) across cell membranes. These channels possess high affinity for K(i) to compensate for the energetic cost of dehydration/desolvation of K(i), which is required to enable



transport.²⁵ It is entirely plausible that in addition to transporting [²⁰¹Tl]Tl(i) into prostate cancer cells, such transporters (alongside other biomolecules either present in cell media, excreted by cells or on the surface of cells) compete for [²⁰¹Tl]Tl(i) complexation. The abundance of high affinity K(i)-binding sites, and thus Tl(i)-binding sites in the biological environment, is likely a formidable hurdle to stable chelation of Tl(i), and such factors require due consideration for future Tl(i) ligand design.

In conclusion, we have demonstrated the synthesis and characterisation of a series of new Kryptofix-222 derivatives with the ability to be conjugated to targeting functionalities through a variety of chemical modification strategies. We further demonstrated that these conjugates interact strongly with free [^{nat}Tl]Tl(i) in solution through NMR experiments. Radiolabelling of these conjugates with [²⁰¹Tl]Tl(i) showed promise with both **K222** derivatives, **5** and **K222-PSMA**, successfully radiolabelled with [²⁰¹Tl]Tl(i) in greater than 98% radiochemical yield. The PSMA-targeting conjugate, [²⁰¹Tl][Tl(**K222-PSMA**)]⁺ exhibited encouraging stability in human serum which prompted us to explore its ability to specifically accumulate in PSMA-expressing cell lines. Unfortunately, these assays indicated no PSMA-receptor mediated uptake of ²⁰¹Tl activity, and the observed cellular uptake of [²⁰¹Tl]Tl(i) activity was attributed to non-specific uptake, likely *via* K(i) transporters.

While these data with [²⁰¹Tl]Tl(i) are encouraging, we believe that other radiometals might be better suited to complexation with **K222**-based bioconjugates and therefore, we are exploring the application of **K222**-based compounds to ²²³Ra, ²¹³Bi and ¹¹¹In.

Experimental

Materials and methods

Commercially available reagent grade solvents and chemicals were used without further purification. Anhydrous solvents were acquired from solvent towers within the department and stored over 3 Å molecular sieves. ¹H, ¹³C, COSY, TOCSY, HSQC, HMBC NMR spectra were recorded on a Bruker AVIII 400 or 700 spectrometer. Chemical shifts are reported in ppm and referenced to residual protonated impurities in the solvent for NMR spectra. High Resolution Electrospray Mass Spectrometry was carried out by Dr Lisa Haigh of the mass spectrometry service at Imperial College, or independently on an Agilent 6200 TOF LC-MS instrument. LC-MS for **K222-PSMA** was measured on a Waters 3100 Mass Detector equipped with a Waters 2998 Photodiode Array Detector, Waters 515 HPLC Pump, Waters 2545 Quarternary Gradient Module, and a Waters 2767 Sample Manager. LC-MS solvents were Millipore water and acetonitrile (with 0.1% formic acid). A 18 min gradient was run from 5% to 100% Acetonitrile on a XBridge BEH C18 Column, 130 Å, 5 μm, 4.6 mm × 100 mm. Flash chromatography used silica gel (60 Å pore size). Where specified, automated flash chromatography was performed using a Biotage

Isolera Four unit and 10 g or 25 g SNAP KP-Sil/Sfar duo cartridge. HPLC was performed on an Agilent 1200 Series Liquid Chromatograph with UV and LabLogic Flow-Count detector with a sodium-iodide probe (B-FC-3200). Unless otherwise mentioned the mobile phase A contained H₂O with 0.1% FA, and mobile phase B contained MeCN with 0.1% FA. Preparative reverse-phase HPLC was conducted using a Pursuit XRs C18 column (250 × 10 mm, 5 μm) and UV spectroscopic detection at 250 nm. ²⁰¹TlCl in saline was purchased from Curium Pharma, UK and used without further processing. Fresh human serum was obtained from a healthy volunteer.

Synthesis of **K222** derivatives

Compound 1. Nitrocatechol (1.00 g, 6.45 mmol) was dissolved in acetone (30 mL). Ethyl bromoacetate (1.5 mL, 13.56 mmol) and K₂CO₃ (4 g, 29 mmol) were added to the yellow solution. The reaction mixture was refluxed overnight (72 °C, 16 h). The solution was then filtered and the filtrate was dried *in vacuo*. Automated column chromatography on silica (dry loading after dissolution in DCM; gradient 0–100% EtOAc:hexane) yielded **1** as a brown oil (0.96 g, 2.93 mmol, 45%). Instead of thermal heating the reaction can also be conducted *via* microwave reactor (400 mg scale in a 2–5 mL vial) at 120 °C for 1 h. The NMR data matched that reported previously.²⁶

¹H NMR (400 MHz, CDCl₃) δ 7.91 (dd, ³J_{H-H} = 2.5, 8.9 Hz, 1H), 7.73 (d, ³J_{H-H} = 2.6 Hz, 1H), 6.87 (d, ³J_{H-H} = 9.0 Hz, 1H), 4.80 (d, ³J_{H-H} = 11.4 Hz, 2H), 4.27 (m, 4H), 1.30 (q, J = 7.0 Hz, 6H).

Compound 2. To a solution of **1** (0.96 g, 2.93 mmol) in THF (20 mL) and H₂O (8 mL) was added LiOH (1.6 g). The yellow solution was stirred at room temperature overnight (4 hours are generally enough). The THF was then removed *via* rotary evaporator and concentrated HCl was added to the solution to initiate precipitation of the product. After cooling with ice for 1 h the precipitate was collected by filtration and washed with 3 M HCl (20 mL). Compound **2** was then collected by dissolution in MeOH and subsequent evaporation of the solvent, yielding the pure compound as an off-white powder (556 mg, 2.05 mmol, 70%). The NMR data matched that reported previously.²⁶

¹H NMR (400 MHz, MeOD) δ 7.95 (m, 1H), 7.85 (m, 1H), 7.12 (d, ³J_{H-H} = 9.1 Hz, 1H), 3.82 (d, J = 2.0 Hz, 4H).

Compound 3. Thionyl chloride (3 mL) was added to **2** and the mixture was heated to reflux (80 °C) under a nitrogen atmosphere overnight (~16 h). The thionyl chloride was removed *in vacuo* and the crude product used without further purification in the next step.

Compound 4. Compound **3** (107 mg, 0.4 mmol based on **2**) was dissolved in dry toluene (20 mL) in a round-bottom flask under a nitrogen atmosphere. Kryptofix 22 (103 mg, 0.39 mmol) and triethylamine (0.08 mL, 0.57 mmol) were dissolved in a separate round-bottom flask in dry toluene (20 mL). Both solutions were added simultaneously over 5 min to a third round-bottom flask containing dry toluene (40 mL) cooled to 0 °C by means of an ice bath. The reaction mixture



was allowed to warm to 25 °C under stirring for 16 h (however, reaction times as short as 1 h were found to be sufficient). The next day the solvent was removed *via* rotary evaporator and the crude was purified by automated silica column chromatography (dry loading after dissolution in DCM/MeOH; gradient 0–10% MeOH : DCM) yielding **4** as a yellowish oil (51.5 mg, 0.10 mmol, 25%). The NMR data matched that reported previously.¹⁹

¹H NMR (400 MHz, CDCl₃) δ 7.82 (dd, ³J_{H-H} = 2.6, 8.9 Hz, 1H), 7.77 (d, ³J_{H-H} = 2.6 Hz, 1H), 7.00 (d, ³J_{H-H} = 8.9 Hz, 1H), 5.63 (d, ³J_{H-H} = 15.0 Hz, 1H), 5.47 (d, ³J_{H-H} = 15.1 Hz, 1H), 4.83–4.75 (m, 2H), 4.38–4.26 (m, 2H), 3.92–3.47 (m, 20H), 3.28–3.17 (m, 2H), 2.84–2.75 (m, 2H).

Compound 5. Compound **4** (110 mg, 0.22 mmol) was dissolved in 1 M borane THF solution (2 mL) and refluxed under a nitrogen atmosphere overnight. The mixture was then allowed to cool to room temperature before 3 M HCl (10 mL) was added and the solution was refluxed for another 3 h. After cooling to room temperature, the solution was neutralised by addition of NH₄OH (15 mL). All solvent was removed *in vacuo*. The solid residue was re-dissolved in ACN/H₂O (1 : 1, 2 mL) and purified by automated column chromatography on a C18 cartridge (gradient 0–100% ACN : H₂O with 0.1% TFA). The fractions containing product were neutralised by addition of 1 M NaOH and dried, yielding **5** as a reddish oil (58.0 mg, 0.12 mmol, 55%). The NMR data matched that reported previously.¹⁹

¹H NMR (400 MHz, CDCl₃) δ 7.98 (dd, ³J_{H-H} = 2.6, 9.0 Hz, 1H), 7.92 (d, ³J_{H-H} = 2.6 Hz, 1H), 7.27 (d, ³J_{H-H} = 9.0 Hz, 1H), 4.39 (t, ³J_{H-H} = 4.8 Hz, 2H), 4.34 (t, ³J_{H-H} = 4.8 Hz, 2H), 3.69–3.57 (m, 12), 3.51–3.40 (m, 4H), 2.91–2.87 (m, 4H), 2.79–2.67 (m, 8H).

¹³C NMR (100.7 MHz, CD₃OD) δ 153.4, 148.0, 142.9, 119.0, 112.8, 108.4, 69.2, 68.7, 67.4, 67.0, 54.1, 53.8, 53.7.

ESI–HRMS (MeOH): found: 492.2340; calculated for [C₂₂H₃₅N₃O₈ + 1Na⁺]: 492.2322.

K222-NH₂. Compound **5** (98.7 mg, 0.21 mmol) was dissolved in a mixture of DCM (5 mL) and acetic acid (2 mL). Fine zinc dust (150 mg) was added to the solution and the mixture was stirred at room temperature for 3 h. The solution was diluted by addition of MeOH and water (1 : 1, 20 mL) and the DCM was evaporated. The zinc dust was filtered off and the filtrate was dried *in vacuo*. The crude product was purified by automated column chromatography on a C18 cartridge (gradient 0–100% ACN : H₂O with 0.1% TFA). The fractions containing product were neutralized by addition of 1 M NaOH and dried, yielding **K222-NH₂** as a brownish oil (41.5 mg, 0.094 mmol, 43%). The NMR data matched that reported previously.¹⁹

¹H NMR (400 MHz, CDCl₃) δ 6.77 (d, ³J_{H-H} = 8.7 Hz, 1H), 6.35 (d, ³J_{H-H} = 2.5 Hz, 1H), 6.18 (dd, ³J_{H-H} = 2.5, 8.7 Hz), 4.17 (t, ³J_{H-H} = 4.4 Hz, 2H), 4.06 (t, ³J_{H-H} = 4.7 Hz, 2H), 3.66–3.61 (m, 8H), 3.59–3.43 (m, 8H), 2.80–2.74 (m, 4H), 2.69–2.64 (m, 8H).

¹³C NMR (100.7 MHz, CD₃OD) δ 148.2, 141.8, 140.8, 115.0, 110.4, 104.5, 69.3, 68.8, 68.7, 66.8, 66.4, 54.4, 54.0.

ESI–HRMS (MeOH): found: 462.2570; calculated for [C₂₂H₃₇N₃O₆ + 1Na⁺]: 462.2580.

K222-N₃. The fluorosulfonyl azide reagent was prepared as described in a literature report.²⁰ **K222-NH₂** (20 mg, 46 μmol) was dissolved in DMF and MTBE (1 : 1, 1 mL). Fluorosulfonyl azide (100 μL, 0.7 mM) and KHCO₃ (70 μL, 3 M) were added, and the solution was stirred overnight. LC-MS analysis revealed formation of the target compound. The solvent was evaporated and the crude product was purified by automated silica column chromatography (dry loading after dissolution in DCM/MeOH; gradient 0–10% MeOH : DCM) yielding **K222-N₃** as a reddish oil (8.1 mg, 17 μmol, 37%).

¹H NMR (400 MHz, CDCl₃) δ 6.89 (d, ³J_{H-H} = 8.7 Hz, 1H), 6.65 (dd, ³J_{H-H} = 6.1, 11.2 Hz), 6.52 (d, ³J_{H-H} = 2.5 Hz, 1H), 4.19–4.15 (m, 4H), 3.65–3.45 (m, 16H), 2.91–2.87 (m, 4H), 2.74–2.63 (m, 8H).

ESI–HRMS (MeOH): found: 466.2667 and 488.2484; calculated for [C₂₂H₃₅N₅O₆ + 1H⁺]: 466.2660 and [C₂₂H₃₅N₅O₆ + 1Na⁺]: 488.2480.

IR (Golden Gate ATR): = 2106 cm⁻¹.

K222-DBCO. **K222-NH₂** (21.5 mg, 0.049 mmol) was dissolved in DMF (1 mL). DBCO–NHS (18 mg, 0.045 mmol) and triethylamine (2 drops) were added, and the solution was stirred at room temperature for 2 days. LC-MS analysis confirmed formation of **K222-DBCO**. The solvent was evaporated *in vacuo* and the crude product was used in the next step without further purification.

Compound 7. The fluorosulfonyl azide reagent was prepared as described in a literature report.²⁰ The precursor **6**^{22b} (18.2 mg, 22.1 μmol) was dissolved in DMF and MTBE (1 : 1, 1 mL). Fluorosulfonyl azide (60 μL, 0.7 mM) and KHCO₃ (70 μL, 3 M) were added, and the solution was stirred overnight. LC-MS revealed formation of the target compound. The solvent was evaporated, and the crude was used without further purification.

Compound 8. Crude **7** was dissolved in DCM (2 mL), TFA (1 mL) added, and the solution was stirred at room temperature. The reaction was tracked by TLC (30 : 1 DCM/MeOH). After 2 h no more starting material could be detected and the target compound was identified by LC-MS. The solvent was evaporated and the crude product was then used without further purification.

K222-PSMA. Crude **8** was dissolved in DMF (0.5 mL) and crude **K222-DBCO** was dissolved in MeOH (1 mL). The two solutions were combined and stirred at room temperature for 3 h. After the target mass was detected by LC-MS, the solvents were evaporated, and the crude product was purified by preparative HPLC on a C18 column (10–100% H₂O/ACN with 0.1% formic acid over 30 min). Neutralisation of the collected product fractions with 1 M NaOH and subsequent evaporation of the solvents gave **K222-PSMA** as a white powder (3.5 mg, 2.5 μmol, 5% from **K222-NH₂**).

ESI–HRMS (MeOH): found: 1408.6879; calculated for [C₇₄H₉₃N₁₁O₁₇ + H⁺]: 1408.6829.

Radiolabelling experimental

²⁰¹Tl experiments. Caution! ²⁰¹Tl is a γ-emitter (t_{1/2} = 73 h) which should only be handled by trained personnel in a licensed and appropriately shielded facility.



In a typical experiment, [^{201}Tl]TlCl (~ 1 MBq, 50 μL) was added to an Eppendorf vial together with 50 μL of the organic chelator (0.5–2 mM). Na_2CO_3 (25 μL of 1 M) and water (75 μL) were added to the vial and the reaction was shaken at room temperature for 15 min.

Serum stability. A solution containing [^{201}Tl][Tl(K222-PSMA)] $^+$ (100 μL , ~ 1 MBq) was added to filtered human serum (Sigma-Aldrich, 300 μL) and incubated at 37 $^\circ\text{C}$ for either 0 min, 30 min or 120 min. After the indicated time the sample was treated with ice-cold acetonitrile (300 μL) to precipitate and remove serum proteins. Acetonitrile in the supernatant was then removed by evaporation under a stream of N_2 gas (30 min). The final solution was then analysed by reverse-phase analytical HPLC.

Cell assay experimental

DU145 (PSMA-negative) and DU145-PSMA (PSMA-positive) human prostate cancer cells were cultured in RPMI 1640 medium (R0883, Sigma) supplemented with 10% (v/v) foetal bovine serum (FBS), 2 mM L-glutamine, and penicillin/streptomycin (Sigma-Aldrich, UK) and maintained in a humidified atmosphere at 37 $^\circ\text{C}$ under 5% CO_2 .

To assess PSMA targeting, PSMA-expressing cells DU145-PSMA and non-PSMA-expressing cells DU145 cells were seeded in 6-well plates at a density of 0.5×10^6 cells per well 1 day prior to the experiment. Three technical replicates were performed for each condition. Cell medium was replaced with 1 mL complete medium 1 hour before the cells were treated. [^{201}Tl][Tl(K222-PSMA)] $^+$ (50 kBq, in 10 μL of phosphate buffered saline) was added to each well, and the cells incubated at 37 $^\circ\text{C}$ for 15 min and 1 h. Competition studies were also performed following co-incubation with the PSMA-inhibitor 2-(phosphonomethyl)pentane-1,5-dioic acid (PMPA; 30 μL of 750 mM PMPA solution per well). After incubation, plates were placed on ice, the supernatant was removed and the cells were washed with ice cold phosphate buffered saline solution (2×1 mL). The cells were lysed with ice cold radioimmunoprecipitation assay (RIPA) buffer (Thermo Fisher Scientific Inc., 500 μL), and radioactivity content was determined by gamma counter (1282 Compugamma; LKB, window set to channels 35–110 to measure ^{201}Tl gamma emissions). Cell uptake was also performed following [^{201}Tl]TlCl incubation (50 kBq, 10 μL) for 15 min and 1 h. Cells were harvested and radioactivity measured as described above.

DFT calculations

All calculations were performed using the Gaussian 16 package (Revision C.01). 27 Full geometry optimisations were performed using the $\omega\text{B97X-D}$ functional 28 in gaseous state with the LANL2DZ basis set and effective core potentials for Tl, and 6-311+G** for all other atoms. 29 Structures were optimised without using symmetry constraints. Frequency analysis of the optimised structures confirmed a true minimum energy structure by the absence of imaginary frequencies.

Conflicts of interest

There are no conflicts of interest to declare.

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