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## Novel dual-function near-infrared II fluorescence and PET probe for tumor delineation and image-guided surgery†

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Accurate tumor identification is essential in cancer management. Incomplete excision of tumor tissue, however, negatively affects the prognosis of the patient. To accomplish radical excision of tumor tissue, radiotracers can be used that target tumor tissue and can be detected using a gamma probe during surgery. Intraoperative fluorescence imaging could allow accurate real-time tumor delineation. Herein, a novel dual-modal imaging platform using base-catalyzed double addition of thiols into a propiolamide scaffold has been developed, allowing for the highly efficient and selective assembly of various thiol units in a protecting-group-free manner. The first small-molecule based  $\alpha v\beta_3$ -targeted NIR-II/PET probe <sup>68</sup>Ga-SCH2 was concisely generated *via* this strategy and subsequently evaluated in mice bearing the U87MG xenograft. Excellent imaging properties such as good tumor uptake, high tumor contrast and specificity, tumor delineation and image-guided surgery were achieved in the small animal models. These attractive results of <sup>68</sup>Ga-SCH2 allow it to be a promising  $\alpha v\beta_3$ -targeted NIR-II/PET probe for clinical translation.

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## Introduction

Maximizing tumor excision and minimizing collateral damage are the primary goals of cancer surgery. Incomplete excision of tumor tissue, however, negatively affects the prognosis of the patient. Evidence from numerous experimental and clinical studies has demonstrated the significant benefits of molecular imaging in targeted surgery with preoperative molecular diagnostic screening, fluorescence image-guided surgery and post-operative imaging.<sup>1–5</sup> So far only two small molecules, methylene blue and indocyanine green (ICG), have been

approved by the FDA, emitting within the traditional NIR-I region (750–900 nm) and with the desirable features of rapid renal excretion and low toxicity.<sup>6,7</sup> Despite their imaging qualities being superior to those of visible wavelengths in accurate real-time tumor delineation, photostability and the penetration depth of emitted light in biological tissues remain challenging. To address this limitation, fluorophores emitting within the second near-infrared region (NIR-II, 1000–1700 nm) show great promise. NIR-II probes possess high spatial resolution and deep-tissue penetration due to reduced photon scattering and diminished auto-fluorescence.<sup>8–13</sup> At present, several classes of fluorescent NIR-II probes including small molecules,<sup>14–17</sup> carbon nanotubes,<sup>18,19</sup> Ag<sub>2</sub>S dots<sup>20,21</sup> and polymers<sup>22</sup> have been actively employed for NIR-II fluorescence for superior vascular imaging, cerebral imaging, lymphatic imaging and imaging-guided surgery.<sup>23,24</sup>

A surge in dual-modal instrumentation development for image-guided surgery and other clinical applications has sparked the discovery of more dual-modal contrast agents to clearly delineate the localization and expression of biochemical markers, and effectively track the tumor with high-resolution and high-sensitivity.<sup>2,4–6,25–37</sup> Using dual-modality probes for sentinel lymph node mapping and image-guided surgery shows promising results in prostate cancer,<sup>28,35</sup> breast cancer<sup>36</sup> and head and neck cancer.<sup>37</sup> Although radio-guided surgery and intraoperative fluorescence imaging are powerful techniques to improve accurate tumor detection and resection, they have their

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Table 1 Base-catalyzed thiol-addition chemistry

Entry <sup>a</sup>	Catalyst	<i>t</i> [min]	Thiol (equiv.)	Solvent	Yield <sup>b</sup> (%)	Product
1	Spontaneous	30	1.0 eq.	DMF	52	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 90 : 10)
2	TEMPO (10 equiv.)	30	1.0 eq.	DMF	49	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 90 : 10)
3	NEt <sub>3</sub> (0.1 equiv.)	30	1.0 eq.	DMF	70	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 83 : 17)
4	DIPEA (0.1 equiv.)	30	1.0 eq.	DMF	80	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 90 : 10)
5	DBU (0.1 equiv.)	30	1.0 eq.	DMF	83	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 80 : 20)
6	DIPEA (0.1 equiv.)	30	1.0 eq.	DCM	82	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 87 : 13)
7	DIPEA (0.1 equiv.)	30	1.0 eq.	MeOH	85	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 85 : 15)
8	DIPEA (0.1 equiv.)	30	1.0 eq.	THF	80	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 85 : 15)
9	DIPEA (0.1 equiv.)	30	1.0 eq.	PBS/DMF (8.2)	80	<b>1a</b> ( <i>cis</i> : <i>trans</i> = 87 : 13)
10	TBD (0.2 equiv.)	60	4.0 eq.	DMF	67	<b>1b</b>

<sup>a</sup> Reaction conditions: [alkyne] = 0.25 M in solvents, catalyst = 0.1 or 0.2 equiv. <sup>b</sup> Isolated yield calculated on the basis of the starting alkyne and referred to the major products.

3351.3, found: *m/z* 3350.2 (Fig. S10<sup>†</sup>). The UV-vis-NIR absorption band of the **CHS2** probe was at 600–900 nm (Fig. S11<sup>†</sup>). Meanwhile, the fluorescence emission spectrum of the **CHS2** probe indicated a maximum wavelength at 1055 nm in PBS buffer (Fig. 2a and S12<sup>†</sup>). The fluorescence quantum yield of the **CHS2** probe was ~0.20% in water, measured against an IR-26 reference with a nominal quantum yield of 0.5% under 785 nm excitation. **CHS2** also exhibited high photostability in PBS, water and mouse serum with negligible decay under continuous excitation for 1 h (Fig. 2b). However, NIR-I probes such as ICG decayed ~50% under the same conditions (Fig. 2c). Furthermore, the high viability of U87MG cell lines after 24 h incubation with different concentrations of **CHS2** and <sup>nat</sup>Ga-**CHS2** demonstrated the high biocompatibility of **CHS2** *in vitro* (Fig. 2d and S13<sup>†</sup>). Briefly, **CHS2** was then incubated with <sup>68</sup>Ga [2 mCi] under mild conditions for 15 min according to

a previously reported method,<sup>41</sup> and purified by RP-HPLC resulting in over 95% purity (Fig. S14<sup>†</sup>). The specific activity of <sup>68</sup>Ga-**CHS2** was determined to be ~25 GBq μmol<sup>-1</sup> and it demonstrated excellent stability in mouse serum (no release of <sup>68</sup>Ga for 2 h). U87MG cells were chosen to investigate the specificity of <sup>68</sup>Ga-**CHS2** toward integrin αvβ<sub>3</sub>.<sup>42,43</sup> As shown in Fig. S15,<sup>†</sup> <sup>68</sup>Ga-**CHS2** exhibited good uptake in U87MG cells. In the blocking group, the cells were incubated with <sup>68</sup>Ga-**CHS2** (1 μCi per well) and unlabeled RGD (2 μg per well) as a blocking agent, and the uptakes were significantly reduced, indicating that <sup>68</sup>Ga-**CHS2** can specifically bind to integrin αvβ<sub>3</sub> receptors on U87MG cells. Thus, the properties of <sup>68</sup>Ga-**CHS2** warrant further *in vivo* applications.

The nude mice bearing U87MG xenografts (*n* = 3) were injected with ~85 μCi (1 nmol) of <sup>68</sup>Ga-**CHS2** and were imaged with micro-PET/CT and NIR-II separately. As shown in Fig. 3a

Table 2 Base-catalyzed addition of various functional molecules into propiolamide-based scaffolds

Entry <sup>a</sup>	PA scaffolds <sup>b</sup>	Thiol <sup>c</sup>	<i>t</i> [h]	Product	Yield (%)
1	R <sub>1</sub> = c(RGDfK) ( <b>2a</b> )	2-AET-NOTA ( <b>Y1</b> )	1.5	R <sub>2</sub> = 2-AET-NOTA ( <b>3a</b> )	58
2	R <sub>1</sub> = c(RGDfK) ( <b>2a</b> )	2-AET-Cy5.5 ( <b>Y2</b> )	1.5	R <sub>2</sub> = 2-AET-Cy5.5 ( <b>3b</b> )	60
3	R <sub>1</sub> = c(RGDfK) ( <b>2a</b> )	2-AET-CH1055 ( <b>Y3</b> )	1.5	R <sub>2</sub> = 2-AET-CH1055 ( <b>3c</b> )	60
4	R <sub>1</sub> = AE105 ( <b>2b</b> )	2-AET-CH1055 ( <b>Y3</b> )	1.5	R <sub>2</sub> = 2-AET-CH1055 ( <b>3d</b> )	61
5	R <sub>1</sub> = JMV594 ( <b>2c</b> )	2-AET-CH1055 ( <b>Y3</b> )	1.5	R <sub>2</sub> = 2-AET-CH1055 ( <b>3e</b> )	60
6	R <sub>1</sub> = AE105 ( <b>2b</b> )	2-AET	2	R <sub>2</sub> = R <sub>3</sub> = 2-AET ( <b>4a</b> )	58
7	R <sub>1</sub> = c(RGDfK) ( <b>2a</b> )	2-AET-NOTA ( <b>Y1</b> ), 2-AET-Cy5.5 ( <b>Y2</b> )	2	R <sub>2</sub> = 2-AET-NOTA, R <sub>3</sub> = 2AET-Cy5.5 ( <b>4b</b> )	47

<sup>a</sup> The catalyst DIPEA for entries 1–5; TBD for entries 6–7. <sup>b</sup> c(RGDfK) = cyclo (Arg-Gly-Asp-d-Phe-Lys); AE105 = Ac-Lys-Gly-Asp-Cha-Phe-(D)Ser-(D)Arg-Tyr-Leu-Trp-Ser-NH<sub>2</sub>; JMV594 = (D)Phe-Gln-Trp-Ala-Val-Gly-His-Sta-Leu-NH<sub>2</sub>. <sup>c</sup> 2-AET is 2-aminoethanethiol; NOTA is 2-S-(4-isothiocyanatobenzyl)-1,4,7-triazacyclononane-1,4,7-triacetic acid; Cy5.5 is cyanine 5.5.





Fig. 2 (a) Fluorescence emission of CHS2 under 808 nm excitation; (b) photostability of CHS2 in water, PBS and serum under 808 nm laser illumination ( $105 \text{ mW cm}^{-2}$ ) for 1 h; (c) photostability of ICG vs. CHS2 under 808 nm laser illumination ( $82 \text{ mW cm}^{-2}$ ) for 1 h; (d) cellular toxicity of different concentrations of CHS2 in U87MG cell lines.

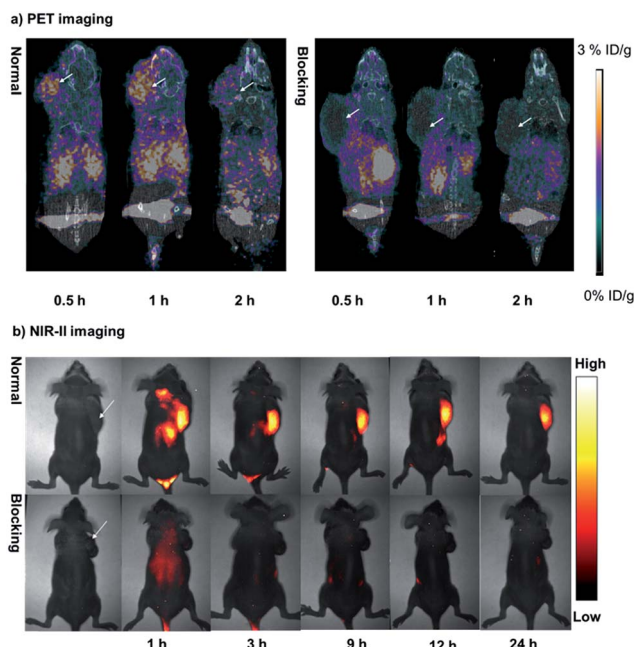


Fig. 3 (a) The PET/CT images of U87MG-tumor-bearing mice (white arrows indicate the location of the tumor,  $n = 3$  per group) acquired at 0.5, 1, and 2 h after tail vein injection of  $^{68}\text{Ga-CHS2}$  with and without the blocking agent RGD. (b) NIR-II images of the U87MG tumor at 1, 3, 9, 12, and 24 h after tail vein injection of CHS2 with and without the blocking agent RGD under 808 nm excitation ( $82 \text{ mW cm}^{-2}$ ), 1000 LP and 40 ms.

and b, at different time points during the scan, the tumor could be clearly visualized on both PET and NIR-II images with a high signal to background ratio (T/N). The *in vivo* specificity of the dual-modal imaging probe was confirmed by the blocking experiment and the intensity of the tumor signals was

significantly reduced after co-injection of unlabeled RGD ( $750 \mu\text{g}$  per mouse) for both PET and NIR-II imaging. The quantitative analysis of the PET images further revealed that the tumor uptake values of  $^{68}\text{Ga-CHS2}$  were gradually increased from 0.5 to 1 h, and then reduced at 2 h after injection, with  $0.77 \pm 0.13$ ,  $2.48 \pm 0.32$  and  $2.14 \pm 0.27\%$  ID  $\text{g}^{-1}$  at 0.5, 1 and 2 h, respectively (Fig. S16<sup>†</sup>). In contrast, significantly lower tumor uptake values were observed for the blocking group with values of  $0.32 \pm 0.07$ ,  $0.28 \pm 0.05$  and  $0.18 \pm 0.04\%$  ID  $\text{g}^{-1}$  at 0.5, 1 and 2 h, respectively. From the NIR-II imaging data, the U87MG tumor fluorescence signals were successfully reduced at later time points in the blocking group. The T/N ratios obtained by NIR-II imaging for CHS2 are shown in Fig. S17,<sup>†</sup> and are proven to be much higher than those of the blocking group at all time points. Moreover, the highest tumor contrast was obtained at the 12 h time point with a T/N value of  $4.77 \pm 0.26$ , which is 2-fold more than previously reported NIR-I/RGD based probes.<sup>27</sup> Bio-distribution studies were evaluated for this dual-modal probe in major organs (Fig. S18 and S19<sup>†</sup>). Pharmacokinetics of  $^{68}\text{Ga-CHS2}$  demonstrated renal and hepatobiliary excretion, with a trace amount of CHS2 remaining in the kidney and liver for 60 h post-injection (PI) (Fig. S19 and S20<sup>†</sup>). These results also matched well with PET and NIR-II imaging data. Thus, a powerful synergy can be achieved by combining radiotracers for the detection of tumor tissue, and NIR-II optical tracers for subsequent accurate delineation of tumor lesions and resection margins.

Encouraged by these promising results obtained *in vivo* PET/NIR-II images, CHS2 was further evaluated for subsequent precise and accurate delineation of tumor lesions, resection margins and image-guided surgery. U87MG tumor-bearing mice ( $n = 3$ ) were injected with  $100 \mu\text{g}$  of CHS2 and the tumor delineation could be notably identified from the surrounding background tissue at 4 h (Fig. S21<sup>†</sup>). The T/N ratio reached  $4.75 \pm 0.22$  at 12 h post-injection, and when the tumor was dissected and removed from the soft tissue in the leg region, the T/N ratio dropped to  $1.16 \pm 0.27$ , indicating that the tumor was thoroughly dissected (Fig. 4a–e). As NIR-II fluorescence image-guided surgery was carried out, all fluorescent surgical specimens including the whole tumor and para-cancerous tissues (marked as 1–4, right adjacent to the tumor tissue) were stained with hematoxylin and eosin assessed (Fig. 4f–l). Histological analysis of excised para-cancerous tissues at different magnifications has shown that the histological characteristics of cancer were not detected. The data further verified tumor delineation and resection margins, as well as fluorescence signals by NIR-II imaging (Fig. 4f–l). This way, tumor nodules that were missed by conventional surgery but were successfully detected by our fluorescent probe CHS2 can be analyzed to assess the sensitivity and specificity of the dual-modality intraoperative imaging approach at the histological level (Fig. 4). Our gamma probe activity measurements and NIR-II fluorescence imaging data obtained during surgery along with these hematoxylin-eosin staining results could lead to a reduced time of examination, which may aid the surgeon in making better decisions during the surgery.





Fig. 4 (a–e) U87MG tumor delineation and image-guided surgery at 12 h after the tail vein injection of CHS2 under 808 nm excitation ( $82 \text{ mW cm}^{-2}$ ), 1000 LP and 23 ms. (f) The tumor cells in this resected specimen were confirmed by high-power magnification ( $400\times$ ) of histological sections; (g) H&E-staining of the whole tumor. (h) The little muscle fibers marked as 1 were adjacent to the tumor tissue; (i) the brown band marked as 2 is the normal epithelium of the margin of the resected specimen; (j and k) the pink erythrocyte marked as 3 and 4 indicates the vessels in the margin of the tumor; (l) histological analysis of the excised para-cancerous tissue at  $400\times$  magnification. Cancer histologic characteristics were not detected in this para-cancerous tissue.

## Conclusions

In summary, we have successfully developed a base-catalyzed strategy for the concise construction of an integrin  $\alpha v \beta_3$ -targeted dual-modality imaging probe,  $^{68}\text{Ga}$ -CHS2, for tumor delineation and image-guided surgery. This probe has demonstrated excellent imaging characteristics *in vivo* and has high clinical and translational potential. Our highly innovative approach to obtain tumor-free resection margins or maximal cytoreduction using specific tumor targeting dual-label tracers that can be detected with a  $^{68}\text{Ga}$  probe and a fluorescence NIR-II camera during surgery will affect patient survival. Thus, our first targeted dual-modality NIR-II/PET image-guided surgery results show the potential to take oncological surgery one step further and may ultimately contribute to the improved survival of cancer patients.

All animal studies were performed in accordance with the Guidelines for the Care and Use of Laboratory Animals of the Chinese Animal Welfare Committee and approved by the Institutional Animal Care and Use Committee (IACUC), Wuhan University Center for Animal Experiment, Wuhan, China.

## Author contributions

X. C. Hong and Z. Cheng conceived and designed the experiments. Y. Sun, X. D. Zeng, Y. L. Xiao, C. H. Liu, H. Zhu and H.

Zhou performed the experiments. Z. Y. Chen, F. C. Xu, J. L. Wang, M. Y. Zhu, J. Z. Wu, M. Tian, H. Zhang, Z. X. Deng, Z. Cheng and X. C. Hong analyzed the data and wrote the manuscript. All authors discussed the results and commented on the manuscript.

## Conflicts of interest

There are no conflicts to declare.

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