

MINIREVIEW

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FLASH radiotherapy: mechanisms, nanotherapeutic strategy and future development

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Ultra-high dose-rate (FLASH) radiotherapy serves as an ideal procedure to treat tumors efficiently without harming normal tissues and has demonstrated satisfactory antitumor effects in multiple animal tumor models. However, the biological mechanisms of FLASH radiotherapy have not yet been fully elucidated, and the small number of devices delivering FLASH dose rate has limited its wide application. This review summarizes the possible biological mechanisms and antitumor effects of FLASH radiotherapy, its application in nanotherapeutic strategy, as well as its challenges and future development. Furthermore, some valuable guidance for promoting the progress of FLASH radiotherapy in nanotherapeutic strategies are provided.

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1 Introduction

As one of the foremost clinical treatments for cancer, radiotherapy, either alone or in combination, is necessary for 60–70% of cancer patients during the treatment process.¹ Although radiotherapy has been a cornerstone of cancer treatment used across many types of tumors for both curative and palliative purposes, the negative impact on care and quality of life of patients due to the unnecessary acute and late damage to normal tissues while administering high dose of radiotherapy as needed still restricts the further utilization of radiotherapy.² To overcome this problem, radiation oncology is targeting the application of more precise and safer radiotherapy techniques to simultaneously increase the radiation dose used for irradiating tumor tissues while protecting normal tissues from dose toxicity.³ The two main ways to achieve this goal are as follows: (1) precise deposition of ionizing radiation energy to the tumor sites, thereby limiting its exposure to the surrounding normal tissues, and (2) different biological radiation responses between tumor and normal tissues.⁴ Researchers have been actively exploring specific solutions *via* these techniques. With the continuous advancements of modern radiotherapy technology, new radiotherapy methods, such as intensity-modulated radiotherapy,⁵ stereotactic body radiotherapy,⁶ and proton- and carbon-particle radiotherapy,^{7,8} have gradually emerged in the past few decades. Although these emerging radiation modalities could achieve the delivery of radiation with some degree of conformity to the target sites, reducing the radiation-

induced toxicity to normal tissues to a certain extent, the therapeutic effect remains relatively limited.⁹ In particular, when the treatment area overlaps with organs at risk, a significant number of patients still experience severe toxicity during radiation treatment.¹⁰ Recently, an unexpected differential effect called the FLASH effect was discovered, which uses high-dose and high-precision radiotherapy to reduce the complications of radiotherapy, increase the tolerance of normal tissues, and ensure the antitumor effects without limited.¹¹

FLASH radiotherapy, an emerging radiotherapy technology, was referred to as the FLASH effect before 2014, which was first reported by Dewey *et al.*¹² In contrast to conventional radiotherapy techniques, which employ a dose rate of $\sim 0.03 \text{ Gy s}^{-1}$ with a dose of $\sim 2 \text{ Gy}$ and deliver radiation in 10–30 fractions over several weeks, FLASH radiotherapy has a single ultra-high dose rate $\geq 40 \text{ Gy s}^{-1}$ with a shorter radiation time $< 200 \text{ ms}$ and administers the entire treatment dose in a single FLASH, which is achieved using a linear electron accelerator (LINAC).^{11,13–16} A 75 year-old individual with multiresistant CD30⁺ T-cell cutaneous lymphoma, which had disseminated throughout the skin surface, was the first patient treated with FLASH radiotherapy. The prescribed dose for the planned target volume was 15 Gy delivered in 90 milliseconds, and the results have shown promise for both normal skin and tumors, which prompted further clinical evaluation of FLASH radiotherapy.^{17,18} Recent studies have shown that FLASH radiotherapy could shorten the duration of radiotherapy treatment, deliver a high curative dose, improve the therapeutic potential, and reduce radiation-induced damage in normal tissues.^{19,20} Considering that FLASH radiotherapy has a unique set of advantages such as instantaneous, ultra-high dose and one-time irradiation, and demonstrates superior antitumor activity in various animal models, it is reasonable to predict that FLASH radiotherapy may become one of the major radiotherapy techniques for future

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clinical applications.²¹ However, the biological mechanisms of FLASH radiotherapy are incomplete and inconclusive, making it an immature technology; moreover, the availability of a small number of devices for delivering FLASH dose rates limits its clinical translation.²² It requires more effort to realize the future development of FLASH radiotherapy.

In this review, we summarize the potential biological mechanisms and antitumor effects of FLASH radiotherapy and discuss the application of FLASH radiotherapy in the nanotherapeutic strategy, challenges, and future development. In a word, this review provides some valuable guidance for promoting the progress of FLASH radiotherapy in the nanotherapeutic strategy for cancer treatment.

2 Biological mechanisms

At present, exploring the biological mechanisms of FLASH radiotherapy is an ongoing effort, and has some important findings. For example, preclinical evidence has shown that FLASH radiotherapy and conventional radiotherapy have similar levels of cytotoxicity, DNA damage, and activation of pathways, leading to cell death in tumor tissues,²³ while different from conventional radiotherapy, FLASH radiotherapy reduces apoptosis, fibrosis, DNA damage and secretion of inflammatory molecules significantly in various normal tissues.^{24–26} However, the biological mechanisms are intricate, remain unclear, and are far from conclusive.^{2,4} The internal causes of these intriguing differential responses are important and challenging questions in the study of biological mechanisms. In the process of exploration, researchers have put forward several hypotheses to explain the FLASH effect, and several most probable hypotheses are under investigation, such as oxygen depletion and reactive oxygen species (ROS), DNA damage, and immune response (Fig. 1).²⁷

2.1 Oxygen depletion and ROS

Oxygen depletion is a popular hypothesis that posits that the difference in oxygen tension between normal and tumor tissues is one of the key factors to understanding FLASH radiation

better, clarifying that normal tissues can be protected during FLASH radiotherapy while tumor tissues cannot escape.²⁸ Ultra-high dose rates contribute to oxygen depletion in normal tissues, which induces radio-resistance, meaning that normal tissues around the target are better able to tolerate radiation.^{29–31} Recent studies have indicated that many normal tissues could maintain cell populations for renewal and regeneration under low physiological oxygen conditions. Ultra-high dose rates of FLASH radiation led to rapid oxygen depletion, mimicking hypoxia and increasing normal cell radiation resistance.^{32,33} For tumors, due to the presence of a low-oxygen environment, the absorbed dose that triggers the FLASH effect has a negligible effect on the oxygen tension of the cancer cells, and the ultra-high dose rate preserves the tumor-killing ability of the radiation.³⁴

In addition, there are intrinsic differences in the response of normal and tumor tissues to ROS, which lead to FLASH radiotherapy, effectively killing tumors without harming normal tissues in their vicinity.³⁵ Compared with normal cells, tumor cells exhibit altered metabolism including increased rates of glycolysis and pentose phosphate cycle activity. Increased steady-state ROS levels in tumor cells may contribute to differential susceptibility to glucose deprivation-induced cytotoxicity and oxidative stress, and it also probably contributes to differential susceptibility to ionizing radiation.³⁶ Furthermore, Spitz *et al.* indicated that tumors have higher levels of redox-active iron than that of normal tissues, which results in a difference between their oxidative metabolisms.^{34,37} This differential recovery of ROS damage hypothesis describes the different abilities of normal and tumor cells to “detoxify” from ROS.³⁰ Compared to conventional radiotherapy, FLASH radiotherapy implanted much more hydroperoxides into tissues, and compared to tumors, normal cells have a higher catalase reduction reserve capacity and a lower oxidant load, thus obtaining a stronger capacity to scavenge peroxides.^{30,34,37}

2.2 DNA damage

The classical target theory suggests that DNA is the primary target of radiation, and as a lethal effect of radiation,

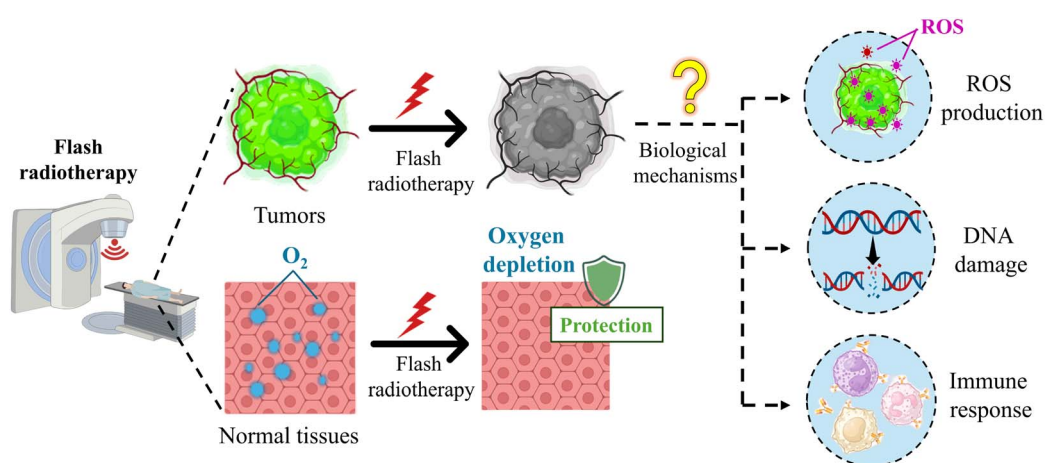


Fig. 1 Schematic of the biological mechanisms of FLASH radiotherapy.



unrepaired DNA double-strand breaks are thought to determine the fate of cells.³⁸ The differential response between normal and tumor tissues in FLASH radiotherapy is probably because of the intrinsic factors “yield of DNA damage” and “clustered DNA damage”.² Compared to tumors, normal tissues recover faster and more precisely from radiation-induced DNA damage, which is the basis of routine hyperfractionation radiotherapy. Ohsawa *et al.* studied the effect of proton FLASH radiotherapy and conventional radiotherapy on DNA damage. They found that compared with conventional radiotherapy, the single-strand DNA breakage in the FLASH radiotherapy group was reduced significantly, but the double-strand DNA breakage was similar.^{39,40} In addition, a recent study has showed that the number of DNA damage sites to normal tissues in conventional radiotherapy is more than that of FLASH radiotherapy, whereas tumors are unaffected by the mode of irradiation.^{24,41} Another study has shown that lower levels of DNA damage were induced after FLASH irradiation, which was modulated by the oxygen tension and increased with the total dose and dose rate of irradiation, indicating that an oxygen related mechanism, such as transient radiation-induced oxygen depletion, may contribute to the tissue sparing effect of FLASH irradiation.⁴² Several other studies further proved that FLASH radiotherapy leads to fewer dicentric chromosome formations compared to conventional dose rate irradiation and that there is a difference in the G2 cell cycle block after FLASH radiotherapy and conventional radiotherapy.^{43–45} In fact, the difference between normal and tumor tissues in response to clustered DNA damage remains unclear.

2.3 Immune response

Another popular hypothesis for explaining the FLASH effect involves the role of the immune response and the tumor microenvironment.⁴⁶ The antitumor effect of radiation therapy can be exerted by immune modulation, but radiation-induced lymphocyte reduction promotes tumor progression, and the patient survival rates were reduced.⁴⁷ Studies have found that immune responses can be induced by FLASH radiotherapy, followed by the recruitment of T lymphocytes increasing in the tumor microenvironment, improvement of the suppressive tumor immune microenvironment, and reduction of the damage to circulating immune cells under irradiation.^{48–50} Specifically, inflammatory and immune responses may further promote FLASH effects.^{51,52} Intrinsic factors may alter the expression and activation of immune factors and immune cells or indirectly influence the immune response in inducing DNA damage or interfering with the microenvironment surrounding exposed tissues.² Among them, transforming growth factor- β (TGF- β), an important intrinsic factor contributing to radiotherapy resistance and the inflammatory response induced by radiation therapy,⁵³ mediates radiation-induced antitumor responses and regulates ROS production and DNA repair.⁵¹ Fouillade *et al.* investigated the role of immune inflammatory changes in lung injury after FLASH radiotherapy. The results indicated that the expression of the pro-inflammatory factor gene (EGR1) in FLASH radiotherapy and the up-regulation of

inflammatory factors (TGF- β 1, NF-KB) were lower than conventional radiotherapy.⁵⁴ Activation of the TGF- β pathway was observed in conventional radiotherapy, and FLASH radiotherapy may have avoided the induction of this pathway, leading to a reduction of ROS and DNA damage. Other studies have also found that FLASH radiotherapy leads to a reduced level of TGF- β ,^{26,55} however, this mechanism remains yet to be evaluated.^{2,56}

3 Antitumor effects of FLASH radiotherapy

Several studies have been published on the effects of FLASH radiotherapy compared with conventional radiotherapy over the past few years. The results have indicated that FLASH radiotherapy exhibits similar or even better therapeutic effects compared to conventional radiotherapy on ovarian cancer, glioblastoma, melanoma, osteosarcoma, Lewis lung carcinoma, *etc.*, and in various species, including mice, cats, dogs, and mini-pigs,^{23,57–62} which suggest the possible clinical application of FLASH radiotherapy in cancer treatment (Table 1).^{11,63} For example, Rama *et al.* found that FLASH radiotherapy recruited more CD3⁺ T lymphocytes in mouse lung tumor tissues, resulting in significantly smaller tumor volumes in the lungs, and induced more efficient lung-tumor eradication than in the conventional dose rate group.⁶³ FLASH radiotherapy protected the proliferation of intestinal crypt cells and inhibited their fibrosis formation while preserving tumor-killing effects in a mouse pancreatic cancer model.⁶⁴ Moreover, FLASH radiotherapy has shown similar antitumor effects to conventional radiotherapy in murine models of ID8 ovarian cancer peritoneal metastasis and may be an effective strategy for enhancing the therapeutic index of abdominal radiotherapy, with potential application to metastatic ovarian cancer.²³ Furthermore, Vozenin *et al.* found that single-dose FLASH radiotherapy has shown promise as a novel treatment option for cat patients with locally advanced squamous cell carcinoma of the nasal planum, and the results in cats and pigs provided a strong rationale for further evaluating FLASH radiotherapy in human patients.⁵⁷ In addition to being clinically tested with good tumor control in animals such as mice, cats, and dogs,^{57,62,65} the first clinical trial of FLASH radiotherapy for treating patients with cutaneous lymphoma was conducted at the Lausanne University Hospital in Switzerland in 2019, where similar antitumor effects were observed in different treatment groups using FLASH radiotherapy and conventional radiotherapy.⁶⁶ Although FLASH radiotherapy has shown similar or even better tumor-killing ability as conventional radiotherapy, studies on the killing role and biological mechanism of FLASH effect are limited.

4 FLASH radiotherapy-based nanotherapeutic strategy

FLASH radiotherapy has shown great potential for tumor treatment, while it also necessitates technological improvement. Recently, nanotechnology has proposed some valuable



Table 1 Summary of antitumor effects of FLASH radiotherapy

Cancer type	Model	Antitumor efficacy of FLASH radiotherapy	References
Lung tumor (LLC cells)	Mice	More efficient lung-tumor eradication compared to the conventional dose rate group	63
Lung tumor	Mice	Eradicated lung tumors and reduce the occurrence of early and late complications affecting normal tissues	67
Pancreatic cancer	Mice	Preserve tumor growth inhibition and decrease acute cell loss and late fibrosis	64
Ovarian cancer (ID8 cells)	Mice	Similar antitumor effects to conventional radiotherapy	23
Osteosarcoma (LM8 cells)	Mice	In addition to normal tissue sparing, tumor control and a substantial reduction of lung metastasis were observed	58
Acute lymphoblastic leukemia	Mice	Compared with conventional radiotherapy, reduced functional damage to human blood stem cells with the same therapeutic effect	59
Melanomas	Mice	Ablated 50% of mouse melanomas, preventing organ metastases and local tumor recurrence for 18 months	60
Sarcoma	Mice	Decrease radiation damage and favor mechanisms of tissue repair	61
Squamous cell carcinoma	Cats	Complete tumor remission and all but one cat in each group remained tumor-free throughout the follow-up period	65
Squamous cell carcinoma	Mini-pigs, cats	Tumor growth was under control after a single dose of FLASH radiotherapy	57
Oral cancer	Canines	Generally effective but with an elevated risk of high-grade adverse effects	68
Superficial solid cancers	Canines	Treatments were found to be feasible	62
Cutaneous lymphoma	Humans	Similar or even better tumor-killing ability as conventional radiotherapy	66

applications for the widespread use of FLASH radiotherapy. Several studies have applied nanomaterials to FLASH radiotherapy, which has a good therapeutic effect in tumor treatment (Table 2). For example, because tumor self-protection mechanisms limit the therapeutic effect of FLASH radiotherapy, Lyu

et al. reported a novel strategy to enhance FLASH radiotherapy through the synergistic effects of Pd-C SAzyme-induced CO gas and GSH depletion therapy (Fig. 2a), involving ferroptosis induced by multipathway and immunotherapy induced by ferroptosis and radiotherapy (Fig. 2b).⁶⁹ Besides, a critical problem

Table 2 Summary of FLASH radiotherapy-based nanotherapeutic strategies

Name	Component	Cancer type	Treatment	References
CSM	MnCO, Pd-C SAzyme, cell membrane	Breast cancer	FLASH radiotherapy + ferroptosis + immunotherapy	69
TPT NPs	TBP-2, TaO _x , platelet cell membrane	Residual cancer stem cells	FLASH radiotherapy + photodynamic therapy	70
TCH	TPE-BBT dots, CB-839 liposomes	Colorectal cancer	FLASH radiotherapy + photothermal therapy	71
TAFL	TPE-BBT, aspirin, fused membrane liposomes	Cancer stem cells	FLASH radiotherapy + photothermal therapy	72
AuNP-IMQ hydrogel	PCPP, selenocystamine, Sub-5 nm AuNP, IMQ	Melanoma	FLASH radiotherapy + immunotherapy	73



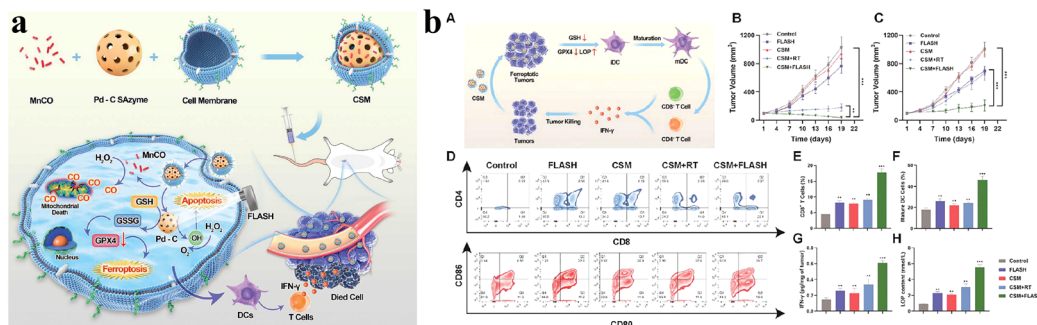


Fig. 2 FLASH radiotherapy-based nanotherapeutic strategy: (a) illustration of the synthesis of CSM radiosensitizers and the mechanism of CSM-mediated tumor therapy. (b) Immunotherapy induced by ferroptosis and radiotherapy *in vivo*: (A) illustration of immunotherapy induced by CSM, change of (B) primary and (C) distant tumor volume in mice, (D) representative flow cytometry analysis of CD4⁺ and CD8⁺ T lymphocyte and dendritic cell (DC) maturation in the lymph nodes, flow cytometric examination of (E) mature DC and (F) CD8⁺ T cells, ELISA measurements of (G) IFN- γ and (H) lactoperoxidase. Reproduced with permission from ref. 69. Copyright 2023, Wiley-VCH Verlag.

after radiotherapy is that residual cancer stem cells (CSCs) may generate tumor cells, leading to tumor recurrence. The research team further developed TPT NPs, aggregation-induced emission luminogen (AIEgen)-based hollow TaO_x nanospheres with platelet cell membrane camouflaged, which specifically target tumor regions and enhance FLASH radiotherapy *via* promoting the photoelectric effect (Fig. 3a). TPT NPs exhibited a remarkable cancer stem cell-killing effect under FLASH radiotherapy and inhibited tumor recurrence significantly. Furthermore, compared with conventional radiotherapy, TPT NPs combined with FLASH radiotherapy efficiently eliminated tumors while preventing reoccurrence and reducing the severity of complications affecting normal tissues (Fig. 3b).⁷⁰ To overcome tumor recurrence, an agarose-based thermo-sensitive hydrogel containing a glutaminase inhibitor (CB-839) and a mild photothermal agent (TPE-BBT) was prepared by Shen *et al.* (Fig. 4a). In the tumor site, CB-839 and TPE-BBT were released from the hydrogel upon 660 nm irradiation for concurrent mild photothermal therapy and chemotherapy, and jointly inhibiting homologous recombination repair of DNA. This work

deciphered the unrestricted molecular motions in bright organic fluorophores as a source of phototherapy and enhanced FLASH radiotherapy by efficiently killing tumor tissues without recurrence and significant systematic toxicity (Fig. 4b).⁷¹

Furthermore, as shown in Fig. 5a and b, Suo *et al.* developed a biomimetic nanoplatform (TAFL) consisting of fused membrane liposomes loaded with aspirin and aggregation-induced emission photothermal agents (TPE-BBT) for scavenging the existence of intractable CSCs after FLASH radiotherapy. TAFL ruptured under laser irradiation and released aspirin that targeted and eliminated CSCs specifically, and TAFL-mediated mild PTT could improve hypoxic transmission electron microscopy (TEM) and promote DNA damage, thereby further exerting a killing effect on CSCs. The results indicated that the combination therapy inhibited self-renewal and growth of breast CSCs effectively, accomplishing substantial inhibition of tumor recurrence and metastasis after FLASH radiotherapy.⁷² The effects of combining FLASH radiotherapy and immunotherapy have not been extensively studied in melanoma. Dong *et al.* reported an integrative therapy combining FLASH

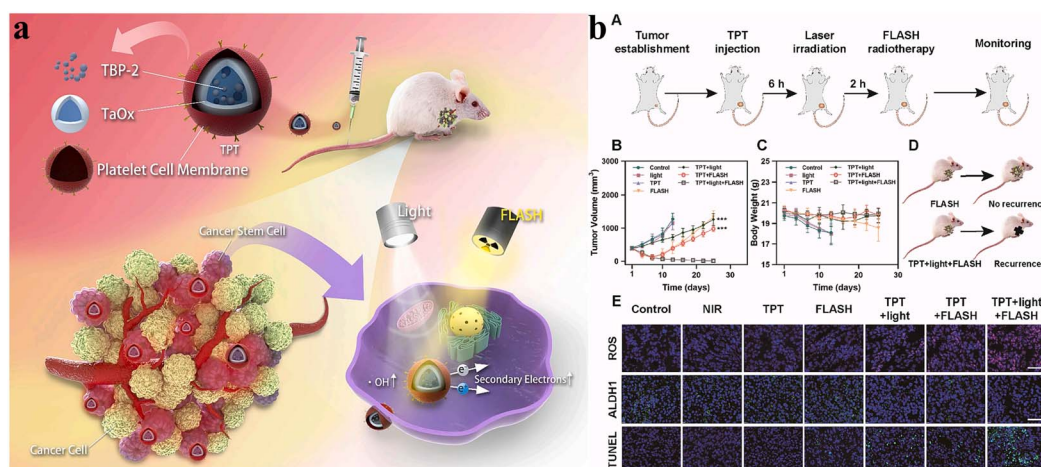


Fig. 3 (a) Synthesis of TPT NPs and application to FLASH radiotherapy enhancement to inhibit tumor recurrence. (b) TPT NP-mediated photodynamic therapy to overcome radioresistance *in vivo*: (A) schematic illustration of the treatment procedure, (B) tumor volumes, (C) body weights, (D) TPT NP-mediated photodynamic therapy for FLASH irradiation enhancement to avoid tumor recurrence, and (E) TUNEL, ROS, and ALDH1 analyses. Reproduced with permission from ref. 70. Copyright 2023, Elsevier BV.

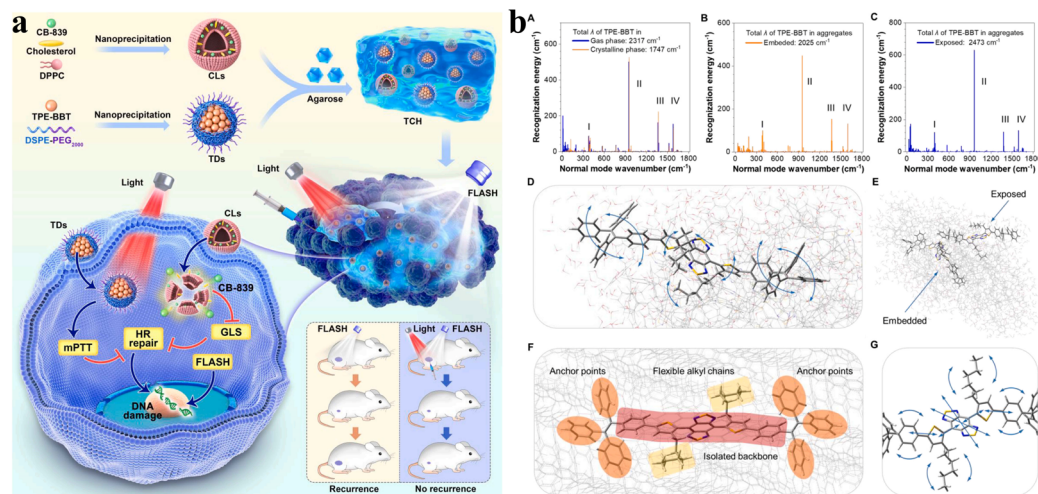


Fig. 4 (a) Schematic of the preparation and application of TPE-BBT dot (TD) and CB-839 liposome (CL) co-loaded agarose thermosensitive hydrogels for recurrence-resistant tumor therapy. (b) Reorganization analysis and molecular motion modes of TPE-BBT in different environments: (A) gas and crystalline phases, (B) surface part of the simulated aggregate (exposed TPE-BBT) and (C) core part of the simulated aggregate (embedded TPE-BBT), (D) identified low-frequency molecular motion modes of exposed TPE-BBT in simulated aggregates, (E) schematic of two different types of TPE-BBT in the aggregate phase, (F) spatial conformation characteristics of embedded TPE-BBT using the crystalline phase as the model, and (G) identified high-frequency molecular motion modes of embedded TPE-BBT using the crystalline phase as the model. Reproduced with permission from ref. 71. Copyright 2024, Elsevier BV.

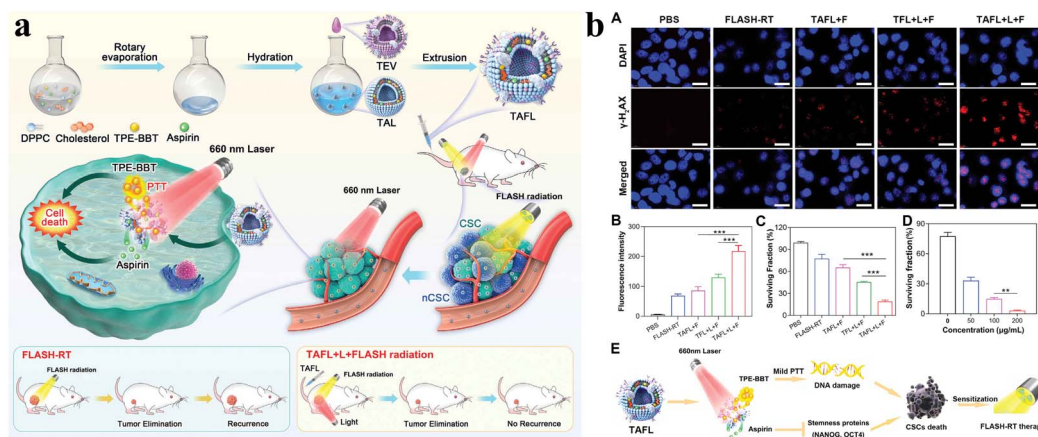


Fig. 5 (a) Schematic of the AIEgen-based biomimetic nano-cancer stem cell scavenger. (b) Surviving situation of 4T1 CSC cells treated with different formulations: (A) γ -H2AX-stained CSCs treated with different formulations, (B) corresponding γ -H2AX fluorescence intensity after different treatments, (C) surviving fraction of 4T1 CSC cells treated with different formulations, (D) surviving fraction of 4T1 CSC cells treated with different concentrations, and (E) proposed mechanism for combined mild PTT/aspirin based on the TAFL system. Reproduced with permission from ref. 72. Copyright 2024, Wiley-VCH Verlag.

radiotherapy with immunotherapy, which suppressed melanoma growth effectively (Fig. 6a). In detail, they developed a radiation response and radiopaque hydrogel loaded with gold nanoparticles (AuNPs) and imiquimod (IMQ), and the hydrogel was imageable with CT *via* the inclusion of AuNPs and IMQ which was released from the hydrogel for immunomodulatory and tumor cell killing under the effective stimulation of FLASH radiotherapy (Fig. 6b). The findings demonstrated that the combination therapy of AuNP-IMQ-gel and FLASH radiotherapy is a promising treatment method for melanoma and merits further study.⁷³

In a word, FLASH radiotherapy-based nanotherapeutic strategies have made progress to some degree, could be combined with other treatments, and have demonstrated therapeutic efficacy in various tumor models, including breast cancer⁷² and melanoma;⁷³ however, the overall number of studies in this area is too small, and more subsequent research is needed to further explore.

5 Challenges and future development

FLASH radiotherapy, as an innovative and transformative radiation modality, has great potential to achieve dose escalation



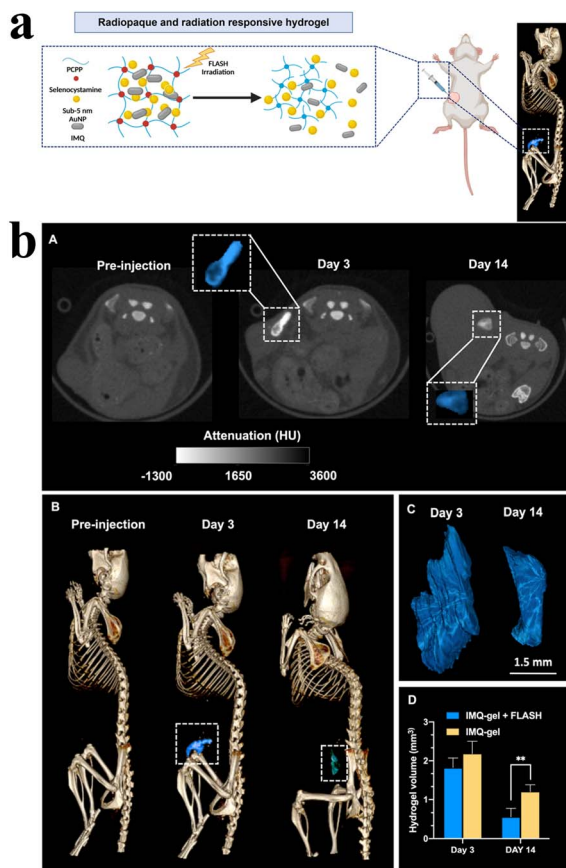


Fig. 6 (a) Illustration of FLASH radiotherapy and immunotherapy delivered by a radiopaque and radiation-responsive hydrogel. (b) *In vivo* images and hydrogel volume analysis: (A) representative CT images of the AuNP-IMQ hydrogel, insets are enlarged images of injected hydrogels highlighted in blue, (B) representative 3D CT images of a mouse with the hydrogel highlighted in blue, (C) 3D reconstructions of the hydrogels based on CT images in panel (B), and (D) quantification of the hydrogel degradation by comparing the hydrogel volumes. Reproduced with permission from ref. 73. Copyright 2023, the American Chemical Society.

for enhanced antitumor efficacy while significantly reducing normal tissue complications. However, there remain many obstacles to the clinical application of FLASH radiotherapy. At present, the radiobiological mechanisms remain unclear and far from conclusive, and there are plenty of biological studies requiring efforts of radiobiology and interdisciplinary studies, especially in understanding the underlying mechanisms of the intrinsic difference between the tumor tissues and the surrounding normal tissues in oxygen depletion, DNA damage response and immune response to FLASH radiotherapy or conventional radiotherapy. Besides, radiation therapy devices for performing FLASH radiotherapy are limited, expensive, and require highly specialized technical personnel to operate, which hampers its clinical application. In addition, most of the equipment can be applied only to animal experiments, and the radiotherapeutic field is limited. Therefore, more effort is required to modify the equipment to expand the irradiation range suitable for treating cancer patients.^{74,75} Another major

challenge in the clinical translation of FLASH radiotherapy is the specific physical parameter that can induce the FLASH effect. It has been shown that the magnitude of the average dose rate is not the only determinant of the FLASH effect, and the dose threshold for inducing the FLASH effect varies across different radiation sources and tissues.^{76,77} In addition to the average dose rate, the total treatment duration, pulse structure (pulse dose, pulse duration, and pulse number), and different energies also influence the FLASH effect.⁷⁸ Radiation sources capable of producing ultra-high dose rate beams, which are suitable for treating deep-seated and superficial tumors, need to be further explored. In addition, safety is particularly important when exposing such high dose rates. To ensure effective treatment, a comprehensive dose monitoring system, and highly accurate image-guidance equipment are needed to track the target area in real time.¹⁸ Finally, the biological diversity in most cancers needs to be considered, and tumors of different origins in different environments may have different responses to the dose rates used in FLASH radiotherapy; therefore, a lot of preliminary basic experiments need to be conducted.^{79,80}

The development of FLASH radiotherapy from ultra-high dose rates to the present evolved over a period of 60 years; from bacteria to cells *in vitro*, from mice to small animals, and finally to patients, opening up new ways for treating patients. The success of FLASH radiotherapy in treating the first patient in the world has greatly increased investigators' confidence in applying it to patients in clinical settings.¹⁸ Research on the biological mechanisms of FLASH radiotherapy and its translational clinical applications are facing many challenges, which are also important opportunities for development and innovation in the field of radiotherapy. We hope to see further research advances in FLASH radiotherapy in the near future.

6 Conclusions

FLASH radiotherapy has progressed from bench to bedside from 1959 to the present and shows great potential in clinical applications. The biological mechanism of FLASH radiotherapy remains unclear, which requires more basic experimental research before it becomes the main radiotherapy technology in cancer therapy. In addition, although limited relevant research literature has been published, nanotechnology needs to be further modified to fit larger fields of FLASH radiotherapy for better treatment benefits. In conclusion, the road of FLASH radiotherapy is tortuous, but the future is bright.

Data availability

No primary research results, software or code have been included and no new data were generated or analysed as part of this review.

Author contributions

Dr Yan Wang and Dr Jie Li have conceptualized the idea, following which Dr Yan Wang, Ms Jiawei Hu, and Ms Jingjing Chai reviewed the literature review and prepared the



manuscript. Dr Jiajie Luan, Dr Qingwen Xu, and Ms Huifang Wang supervised the writing process for the review article, and all 7 authors have finalized the manuscript.

Conflicts of interest

The authors declare no conflict of interest, financial or otherwise.

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