

## Block copolymer conjugates prepared by sequentially grafting from proteins *via* RAFT<sup>†</sup>

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Well-defined thermoresponsive block copolymer conjugates were prepared by two consecutive grafting-from polymerizations *via* reversible addition–fragmentation chain transfer (RAFT) polymerization. A RAFT agent containing an activated ester was conjugated to amines on lysozyme, and *N*-isopropylacrylamide was polymerized by grafting directly from the modified protein in aqueous buffer. Retention of the active thiocarbonylthio moieties on the  $\omega$  end of the conjugated chains allowed chain extension *via* polymerization of *N,N*-dimethylacrylamide to yield lysozyme–poly(*N*-isopropylacrylamide)-*b*-poly(*N,N*-dimethylacrylamide) (LYS–PNIPAM-*b*-PDMA) block copolymer conjugates. Analysis of the conjugates, as well as the cleaved homopolymers and block copolymers, indicated the grafting-from polymerizations were well controlled and that chain extension during block copolymerization was efficient. The temperature-responsive aqueous solution behavior of the resulting conjugates was investigated.

### Introduction

Conjugation to synthetic polymers is a viable means to modify the solubility, activity, and potential utility of proteins.<sup>1–5</sup> For applications *in vivo*, functionalization of a protein therapeutic with an appropriate high molecular weight polymer can substantially reduce immunogenicity and rates of renal clearance/proteolysis. Accordingly, many diverse routes of polymer–protein conjugation have been reported. Generally, these approaches can be classified as either *grafting-to*, which involves conjugation of a preformed polymer with a protein by reactive coupling, or *grafting-from*, which describes the polymerization of monomer from a protein capable of initiation.

Many previous reports of polymer–protein conjugation have involved immobilization of poly(ethylene glycol) (PEG) or its derivatives. Recent advances in controlled radical polymerization (CRP) have facilitated access to other polymers suitable for preparing well-defined polymer–protein conjugates.<sup>6,7</sup> For example, atom transfer radical polymerization (ATRP),<sup>8–14</sup> nitroxide-mediated polymerization (NMP),<sup>15,16</sup> and reversible addition–fragmentation chain transfer (RAFT) polymerization<sup>17–24</sup> have all been employed to prepare polymer conjugates of proteins or peptides.

In addition to allowing precise control of polymer molecular weight and end group functionality, one of the most valuable features of CRP is the ability to prepare block copolymers by

sequential polymerization of two or more monomers.<sup>25,26</sup> Block copolymer bioconjugates may have particular benefits over conventional homopolymer conjugates for a variety of applications. For instance, Stayton and coworkers suggested that addition of an outer hydrophilic block to the end of a enzyme-conjugated responsive polymer could prevent stimuli-induced collapse of the responsive segment from leading to intermolecular aggregation, while still allowing modulation of the protein's activity.<sup>27</sup> Low-to-moderate molecular weight block copolymer conjugates can be readily prepared by grafting-to biomolecules *via* reactive coupling.<sup>27,28</sup> However, given that the efficiency of the grafting-to approach is likely to decrease with increasing molecular weight of the polymer to be conjugated, an attractive alternative involves the synthesis of high molecular weight block copolymer conjugates by sequentially polymerizing two monomers from a biomolecule labeled with an initiating species. However, only a few examples of block copolymer bioconjugates prepared exclusively by grafting-from methods have been reported. For instance, Wooley *et al.* successfully employed NMP and ATRP to graft block copolymers from resin-supported peptides<sup>15</sup> and amino acids.<sup>29</sup> Proteins have also been modified by grafting-from *via* CRP, though the majority of examples have been limited to the synthesis of homopolymer–protein conjugates.<sup>6,7,30,31</sup> Methods that allow the synthesis of well-defined block copolymer–protein conjugates by two consecutive grafting-from polymerizations would be highly advantageous.

Herein, we describe the synthesis of block copolymer–protein conjugates by RAFT polymerization. By immobilizing the RAFT agent *via* its “R-group”,<sup>23</sup> the first monomer was polymerized under mild aqueous conditions<sup>32</sup> to yield

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homopolymer–protein conjugates with active thiocarbonylthio moieties on the distal end of the conjugated chains (Scheme 1). The resulting polymer–protein macro-chain transfer agent (macroCTA) was employed for a subsequent polymerization of a second monomer<sup>33</sup> to yield thermoresponsive block copolymer–protein conjugates. In addition to demonstrating end group retention, this report unambiguously demonstrates the molecular weight control possible while grafting-from a protein via CRP.

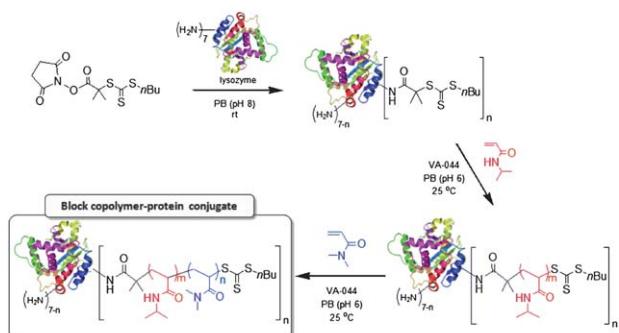
## Experimental

### Materials

The *N*-hydroxysuccinimide functionalized trithiocarbonate chain transfer agent (NHS–CTA) was prepared as previously reported.<sup>34</sup> 2,2-Azobis[2-(2-imidazolin-2-yl)propane]dihydrochloride (VA-044) was purchased from Wako Pure Chemical Industries, Ltd. and was recrystallized ( $\times 3$ ) from methanol. *N*-Isopropylacrylamide (NIPAM, TCI America) was recrystallized from hexanes. *N,N*-Dimethylacrylamide (DMA, Fluka, 98%) was passed through basic alumina prior to use. Lysozyme (LYS, MP Biochemicals), methanol (EMD Chemicals), and deuterium oxide ( $D_2O$ , Acros, 99.8% D) were used as received. Dialysis membranes were purchased from Pierce. Protein markers were purchased from Fisher Science. The Quick Start Bradford<sup>TM</sup> Protein Assay kit was purchased from Bio-Rad. All other chemicals were purchased from VWR and used without further purification, unless otherwise noted.

### Analyses

UV-Vis spectroscopy for trithiocarbonate quantification and turbidity measurements for characterization of responsive solution behavior were carried out on a Beckman Coulter DU Series 800 UV-Vis spectrophotometer equipped with a Peltier temperature controller. Lysozyme concentration was determined by comparison with a quantified lysozyme solution based on a relative protein standard curve made with a protein assay kit. <sup>1</sup>H NMR spectroscopy was conducted with a JEOL Delta 500 spectrometer operating at 500 MHz. Conversion of NIPAM and DMA during polymerization was determined by <sup>1</sup>H NMR spectroscopy. Sodium dodecyl sulfate-polyacrylamide gel electrophoresis (SDS-PAGE) was performed with a Bio-Rad



**Scheme 1** Synthesis of LYS-PNIPAM-*b*-PDMA conjugates by sequential RAFT polymerizations from CTA-modified LYS.

electrophoresis system using 12% polyacrylamide gels at 160 V constant voltage for 60 min. Samples were dissolved in deionized (DI) water (18  $\mu$ L,  $[LYS] = 2 \text{ mg mL}^{-1}$ ), mixed with 6  $\mu$ L sample buffers (containing 3% of  $\beta$ -mercaptoethanol), and heated at 95 °C for 5 min before loading. Staining was accomplished with Coomassie blue. Size exclusion chromatography (SEC) of the cleaved poly(*N*-isopropylacrylamide) PNIPAM or PNIPAM-*b*-poly(*N,N*-dimethylacrylamide) (PDMA) was conducted in DMF with 50 mM LiBr at 55 °C at a flow rate of 1.0  $\text{mL min}^{-1}$  (Viscotek VE 2001 GPCmax; columns: guard + two Polymer Laboratories PolarGel-M mixed bed columns). The detector setup included a Viscotek VE 3580 refractive index detector operating at 660 nm and a Viscotek Model 270 Series Platform, consisting of a laser light scattering detector (operating at 3 mW,  $\lambda = 670 \text{ nm}$  with detection angles of 7° and 90°) and a four capillary viscometer. Molecular weights were determined by the triple detection method.

### Preparation of lysozyme macroCTA (LYS–macroCTA)

LYS (0.20 g, 14  $\mu$ mol) was dissolved in phosphate buffer (PB) solution (pH 8.0, 69.2 mL) in a 150 mL flask and stirred gently with a magnetic bar while purging with nitrogen for 20 min. A solution of NHS–CTA (48.0 mg, 137  $\mu$ mol) dissolved in methanol (10.8 mL) was added drop wise. The resulting solution was stirred at 25 °C for 51 h. The reaction mixture was filtered with a 0.22  $\mu$ m hydrophilic nylon membrane filter and subsequently dialyzed against DI water (3  $\times$  20 L) for 15 h (molecular weight cut-off (MWCO) = 10 kDa). The resulting solution was lyophilized to yield the LYS–macroCTA.

### Determination of trithiocarbonate content in LYS–macroCTA and LYS–PNIPAM macroCTA

S-Butyl-*S'*-( $\alpha,\alpha'$ -dimethyl- $\alpha''$ -acetic acid)-trithiocarbonate<sup>34</sup> was dissolved in methanol to make a 1.76  $\text{mg mL}^{-1}$  ( $6.97 \times 10^{-3} \text{ M}$ ) concentrated solution, which was then diluted to 0.0176  $\text{mg mL}^{-1}$  ( $6.97 \times 10^{-5} \text{ M}$ ) with DI water to obtain a stock solution. The above prepared CTA solution was again diluted with DI water in six plastic cuvettes (1 mL, 1 cm path length) to contain 0, 20, 40, 60, 80, and 100% of the stock solution, respectively. The absorbance of each solution was measured at 310 nm to obtain a linear plot of CTA concentration *versus* absorbance. The CTA extinction coefficient was determined to be  $\varepsilon = 9686 \text{ M}^{-1} \text{ cm}^{-1}$ , and this value was used to calculate the concentration of trithiocarbonate groups within the LYS–macroCTA and LYS–polymer conjugates.

### RAFT polymerization of NIPAM with LYS–macroCTA

A typical grafting-from RAFT polymerization of NIPAM from the LYS–macroCTA was conducted as follows. NIPAM (121 mg, 1.07 mmol), LYS–macroCTA (53.7 mg, 3.65  $\mu$ mol protein, which contained 4.89  $\mu$ mol of CTA functionality, as determined by UV-Vis), and PB (pH 6.0, 3.8 mL) were sealed in a 4 mL glass vial equipped with a magnetic stir bar. The solution was cooled in an ice bath and purged with nitrogen for 30 min. A nitrogen-purged solution of VA-044 (6.46  $\mu$ mol) in PB (pH 6.0, 0.2 mL) was added by syringe, and the reaction vial was placed in a preheated reaction block at 25 °C. Samples were removed

periodically by nitrogen-purged syringe to monitor monomer conversion by  $^1\text{H}$  NMR spectroscopy. The polymerization was quenched after 6.9 h (83% conversion) by opening the vial to air and cooling the reaction in an ice bath. The reaction mixture was dialyzed against DI water ( $3 \times 20$  L) for 15 h using a membrane of MWCO = 10 kDa. The resulting LYS–PNIPAM was isolated by lyophilization. For the block copolymerization study, CTA content per protein (2.1 trithiocarbonates per LYS) was determined by dividing the concentration of trithiocarbonates determined from the absorbance of the conjugate at 310 nm by the protein concentration determined by protein assay.

### LYS–PNIPAM purification by thermoprecipitation

While dialysis proved effective, thermoprecipitation was an alternative method for the removal of unreacted LYS from the LYS–PNIPAM product that resulted from the polymerization of NIPAM with the LYS–PNIPAM macroCTA. The crude LYS–PNIPAM solution ( $\sim 10 \text{ mg mL}^{-1}$ ) was heated at  $40^\circ\text{C}$  for 5 min, followed by centrifugation at 13 200 rpm at  $40^\circ\text{C}$  for 3 min. The supernatant containing unreacted LYS was decanted, and the precipitate was dissolved in DI water and lyophilized to isolate LYS–PNIPAM. While one round of thermoprecipitation successfully removed most of the unreacted LYS, the bioactivity of the purified conjugates was negatively affected. Control experiments with native LYS being exposed to the same heating procedure also resulted in significant loss of activity, suggesting the denaturation was due to the thermal treatment instead of the presence of the polymer.

### Block copolymerization of DMA from the LYS–PNIPAM macroCTA

LYS–PNIPAM with  $M_{n,\text{PNIPAM}} = 11.2 \text{ kg mol}^{-1}$  (LYS–PNIPAM) was used as macroCTA for the RAFT polymerization of DMA. DMA (88  $\mu\text{L}$ , 0.85 mmol), LYS–PNIPAM (1.67  $\mu\text{mol}$  in LYS, which contained 3.55  $\mu\text{mol}$  of CTA functionality, as determined by UV-Vis), and PB (pH 6.0, 3.6 mL) were sealed in a 4 mL glass vial equipped with a magnetic stir bar. The resulting solution was purged with nitrogen for 30 min in an ice bath. A nitrogen-purged solution of VA-044 (2.23 mg, 6.89  $\mu\text{mol}$ ) in PB (pH 6.0, 0.2 mL) was added by syringe, and the reaction vial was placed in a preheated reaction block at  $25^\circ\text{C}$ . Samples were removed periodically by nitrogen-purged syringe to monitor monomer conversion by  $^1\text{H}$  NMR spectroscopy. The polymerization was quenched after 6.5 h (79% conversion) by opening the vial to air and cooling the reaction in an ice bath. The reaction mixture was dialyzed against DI water ( $3 \times 20$  L) for 15 h using a membrane of MWCO = 10 kDa. The resulting LYS–PNIPAM-*b*-PDMA was isolated by lyophilization.

### Cleavage of grafted polymer by protein decomposition

PNIPAM and PNIPAM-*b*-PDMA were cleaved from their respective LYS conjugates by protein decomposition in the presence of Tergazyme. A typical procedure was as follows. LYS–PNIPAM ( $\sim 0.17 \mu\text{mol}$ ) was dissolved in 360  $\mu\text{L}$  of PB buffer (0.1 M, pH 7.5). An aliquot of a Tergazyme stock solution (40  $\mu\text{L}$ , 1 mg  $\text{mL}^{-1}$  in PB buffer) was added, and the solutions were stirred at room temperature for 2 days. For the reactions

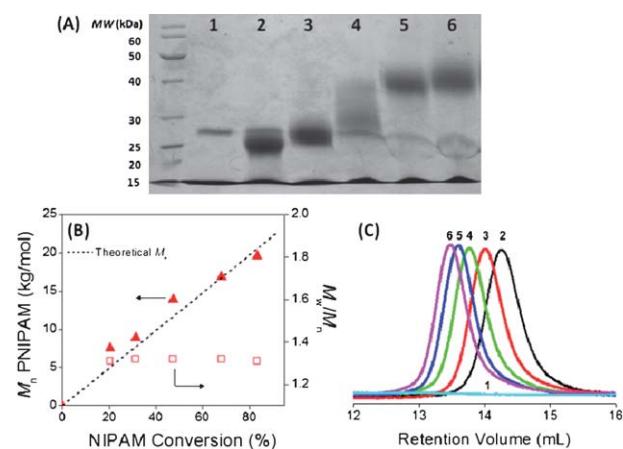
involving the cleavage of PNIPAM from the LYS–PNIPAM conjugates, the reaction solution was then saturated with NaCl, and PNIPAM was extracted with an equal volume of ethyl acetate. The resulting organic phase was divided equally into two scintillation vials and the solvent was evaporated. During the cleavage of PNIPAM-*b*-PDMA from LYS–PNIPAM-*b*-PDMA, the conjugate/Tergazyme solution was dialyzed (MWCO = 10 kDa) for 24 h, separated into two scintillation vials, and lyophilized. For both of the methods described above, DMF was added to one of the vials for SEC analysis and DI water was added to the other vial for SDS-PAGE analysis. The SEC results are shown in the main text. No protein band was observed during SDS-PAGE, indicating the successful decomposition of LYS (Fig. S3†). As a control experiment, a PNIPAM homopolymer and PNIPAM-*b*-PDMA block copolymer were treated with Tergazyme under the identical conditions as described above. No noticeable difference was observed in the SEC traces and NMR spectra of the polymer before and after incubation with Tergazyme (ESI†).

### Cloud point measurements of LYS–PNIPAM and LYS–PNIPAM-*b*-PDMA

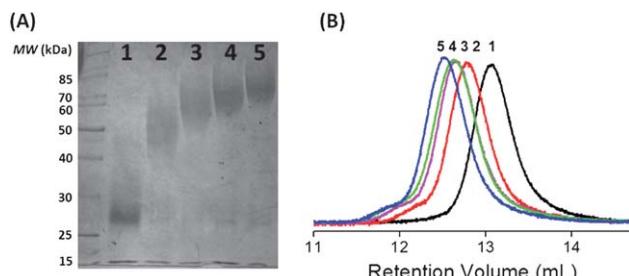
After incubating aqueous solutions (0.11 mM) of the conjugates at  $15^\circ\text{C}$  to ensure complete dissolution, turbidity measurements were monitored by recording solution absorbance at 600 nm. The temperature was gradually raised from 24 to  $48^\circ\text{C}$  by increments of  $1^\circ\text{C}$  with 5 min equilibration time at each increment. The cloud point was defined as the temperature at 10% of the maximum absorbance.

## Results and discussion

A RAFT chain transfer agent containing an *N*-hydroxysuccinimide activated ester was reacted at room temperature with LYS in phosphate buffer at pH 8.0 (Scheme 1). After removal of the unreacted CTA by filtration and extensive dialysis, the trithiocarbonate content of the resulting LYS–macroCTA was determined by UV-Vis spectroscopy using the



**Fig. 1** Results from the aqueous homopolymerization of NIPAM with a LYS-macroCTA. (A) SDS-PAGE results as a function of time (Lanes 1–6:  $t = 0, 1.9, 2.6, 3.5, 4.5$ , and  $6.9 \text{ h}$ , respectively). (B)  $M_n$  and  $M_w/M_n$  vs. monomer conversion for cleaved PNIPAM. (C) SEC traces of cleaved PNIPAM [numbers correspond to lane labels in (A)].



**Fig. 2** (A) SDS-PAGE from the polymerization of DMA with a LYS-PNIPAM macroCTA (Lanes 1–5:  $t = 0, 1.7, 2.6, 3.8$ , and  $6.5$  h, respectively). (B) SEC traces of cleaved PNIPAM-*b*-PDMA as a function of time [numbers correspond to lane labels in (A)]

thiocarbonylthio extinction coefficient at  $310\text{ nm}$  (Fig. S1, ESI†). NIPAM was polymerized in PB (pH 6.0) at  $25\text{ }^\circ\text{C}$  in the presence of the LYS-macroCTA ([NIPAM]/[LYS-macroCTA]/[initiator] = 219/1/1.3). A relatively high concentration of initiator was required because of the long half-life of VA-044 at  $25\text{ }^\circ\text{C}$ .<sup>7</sup> SDS-PAGE indicated the molecular weight of the LYS-PNIPAM conjugates increased with conversion (Fig. 1A). A small amount of unreacted LYS and LYS dimer ( $\sim 28\text{ kDa}$ ) was present throughout the polymerization but was significantly reduced by subsequent dialysis (Fig. 2A, lane 1). Alternatively, the temperature-responsive nature of PNIPAM allowed purification by selective precipitation of the LYS-PNIPAM from aqueous solution (conc. =  $10\text{ mg mL}^{-1}$ ) upon heating to  $40\text{ }^\circ\text{C}$  for 5 min.<sup>7,16</sup> While LYS contains seven primary amines, careful control of pH during reactions with activated esters leads to amine protonation and reduced nucleophilicity, allowing the degree of functionalization to be limited.<sup>35–37</sup> UV-Vis analysis of the isolated homopolymer conjugates indicated that an average of 2.1 polymer chains were conjugated to each LYS.

To gain further insight into the controlled nature of the polymerization, conjugate samples taken at various points during the polymerization were treated with Tergazyme, which led to protein decomposition and retention of the PNIPAM chains, as determined by SDS-PAGE and NMR spectroscopy, respectively. After dialysis to remove low molecular weight (poly)peptide fragments, SEC analysis verified that the number

average molecular weight ( $M_n$ ) of the “cleaved” polymer increased linearly with conversion and was in good agreement with theoretical values, as expected for the RAFT process (Fig. 1B). Additionally, the molecular weight distributions of the cleaved chains were narrow and unimodal, with polydispersity indices ( $M_w/M_n$ ) remaining less than 1.32 over the conversion range considered (Table 1).

While we previously demonstrated grafting-from a protein by RAFT is a viable means to prepare homopolymer–protein conjugates,<sup>23</sup> the possibility of CTA degradation by hydrolysis, aminolysis, *etc.* suggests retention of the end group should be unambiguously confirmed. In this case, end group retention after the polymerization of NIPAM with the LYS-macroCTA was demonstrated by chain extension with DMA. LYS-PNIPAM with a molecular weight of  $25.5\text{ kg mol}^{-1}$  ( $14.3\text{ kg mol}^{-1}$  LYS +  $11.2\text{ kg mol}^{-1}$  PNIPAM) was employed as a macroCTA for the RAFT polymerization of DMA in PB (pH 6.0) at  $25\text{ }^\circ\text{C}$  ([DMA]/[LYS-PNIPAM macroCTA]/[VA-044] = 240/1/1.9). SDS-PAGE analysis indicated an increase in the apparent molecular weight of the conjugate over the course of the block copolymerization (Fig. 2A). SEC analysis of residual PNIPAM-*b*-PDMA obtained by LYS decomposition demonstrated a clear increase in molecular weight of the cleaved chains over the course of the block copolymerization (Fig. 2B). A small high molecular weight shoulder was detected, potentially arising from bimolecular coupling during polymerization or incomplete protein decomposition, though the results indicate  $M_w/M_n$  remained less than 1.35 throughout the polymerization (Table 1).

Preliminary thermoresponsive solution behavior of the homopolymer and block copolymer conjugates was also investigated. Turbidity measurements indicated the cloud point of the conjugates increased from  $34\text{--}36\text{ }^\circ\text{C}$  for LYS-PNIPAM to  $38\text{--}40\text{ }^\circ\text{C}$  for LYS-PNIPAM-*b*-PDMA (Fig. 3). Therefore, while the increased hydrophilicity of the PDMA block increased the cloud point of the conjugates, it did not prevent intermolecular aggregation directed by the internal thermoresponsive PNIPAM segment. In fact at a concentration of  $0.11\text{ mM}$ , precipitation and sedimentation of the block copolymer conjugates were observed at high temperatures, as evidenced by the apparent decrease in turbidity at high temperatures ( $>43\text{ }^\circ\text{C}$ ) (Fig. 3B).

**Table 1** Molecular weight data of the free PNIPAM homopolymers and PNIPAM-*b*-PDMA block copolymers after cleavage

| Entry <sup>a</sup>         | Time <sup>b/h</sup> | Conv. <sup>c</sup> (%) | Cleaved polymer                                  |  |                        |
|----------------------------|---------------------|------------------------|--|--|------------------------|
|                            |                     |                        | $M_n$ ,theory <sup>d</sup> /kg mol <sup>-1</sup> | $M_n$ <sup>e</sup> /kg mol <sup>-1</sup> | $M_w/M_n$ <sup>e</sup> |
| LYS-macroCTA               | 0                   | 0                      | —  | —  | —                      |
| LYS-PNIPAM                 | 1.9                 | 20                     | 5.0  | 7.5                                      | 1.31                   |
| LYS-PNIPAM                 | 2.6                 | 31                     | 7.7  | 8.9                                      | 1.32                   |
| LYS-PNIPAM                 | 3.5                 | 47                     | 11.6   | 13.9                                     | 1.32                   |
| LYS-PNIPAM                 | 4.5                 | 68                     | 16.8   | 16.9                                     | 1.32                   |
| LYS-PNIPAM                 | 6.9                 | 83                     | 20.5   | 19.6                                     | 1.31                   |
| LYS-PNIPAM macroCTA        | 0                   | 0                      | 11.2   | 11.2                                     | 1.30                   |
| LYS-PNIPAM- <i>b</i> -PDMA | 1.7                 | 26                     | 17.4   | 18.6                                     | 1.33                   |
| LYS-PNIPAM- <i>b</i> -PDMA | 2.6                 | 46                     | 22.1   | 23.8                                     | 1.35                   |
| LYS-PNIPAM- <i>b</i> -PDMA | 3.8                 | 59                     | 25.2   | 29.2                                     | 1.21                   |
| LYS-PNIPAM- <i>b</i> -PDMA | 6.5                 | 79                     | 30.0   | 35.7                                     | 1.31                   |

<sup>a</sup> Conjugate from which each polymer was cleaved. <sup>b</sup> Polymerization time. <sup>c</sup> Determined by NMR spectroscopy. <sup>d</sup> Theoretical  $M_n$ . <sup>e</sup> Determined by SEC.

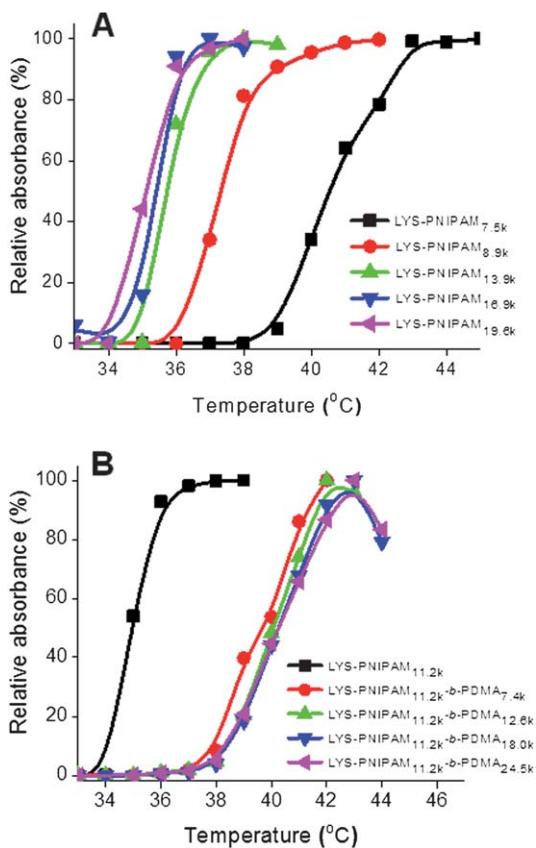


Fig. 3 Turbidity measurements for the cloud point determination of (A) LYS-PNIPAM and (B) LYS-PNIPAM-*b*-PDMA conjugates.

## Conclusions

Grafting-*from* RAFT polymerization is possible when the initial CTA is conjugated to the protein *via* its R-group. Conveniently, this method leads to the retained thiocarbonylthio end group being readily available for subsequent chain extension during block copolymerization. However, given that a high degree of end group retention is a fundamental criterion of living polymerization and that there are many unfavorable fates the end groups may meet in an aqueous polymerization with a highly functional protein (e.g., hydrolysis, aminolysis), the significance of these results goes beyond demonstrating that this method is a viable means to prepare block copolymer–protein conjugates. Indeed, these findings indicate that grafting-*from* by aqueous RAFT polymerization proceeds with considerable control that rivals that observed during more typical RAFT polymerizations conducted with low molecular weight CTAs. Moreover, as compared to the alternative grafting-*to* approach, the reduced steric limitations of this method may substantially facilitate access to a wide variety of block copolymer bioconjugates with high molecular weight synthetic components.

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## References

- 1 A. S. Hoffman and P. S. Stayton, *Prog. Polym. Sci.*, 2007, **32**, 922–932.
- 2 K. L. Heredia and H. D. Maynard, *Org. Biomol. Chem.*, 2007, **5**, 45–53.
- 3 J.-F. Lutz and H. G. Börner, *Prog. Polym. Sci.*, 2008, **33**, 1–39.
- 4 D. Roy, J. N. Cambre and B. S. Sumerlin, *Prog. Polym. Sci.*, 2010, **35**, 278–301.
- 5 P. J. Roth, F. D. Jochum, R. Zentel and P. Theato, *Biomacromolecules*, 2010, **11**, 238–244.
- 6 B. Le Droumaguet and J. Nicolas, *Polym. Chem.*, 2010, **1**, 563–598.
- 7 J. Nicolas, G. Mantovani and D. M. Haddleton, *Macromol. Rapid Commun.*, 2007, **28**, 1083–1111.
- 8 B. Le Droumaguet, G. Mantovani, D. M. Haddleton and K. Velonia, *J. Mater. Chem.*, 2007, **17**, 1916–1922.
- 9 K. L. Heredia, D. Bontempo, T. Ly, J. T. Byers, S. Halstenberg and H. D. Maynard, *J. Am. Chem. Soc.*, 2005, **127**, 16955–16960.
- 10 L. Tao, G. Mantovani, F. Lecolley and D. M. Haddleton, *J. Am. Chem. Soc.*, 2004, **126**, 13220–13221.
- 11 V. Vazquez-Dorbatt, Z. P. Tolstyka, C.-W. Chang and H. D. Maynard, *Biomacromolecules*, 2009, **10**, 2207–2212.
- 12 B. S. Lele, H. Murata, K. Matyjaszewski and A. J. Russell, *Biomacromolecules*, 2005, **6**, 3380–3387.
- 13 B. Le Droumaguet and K. Velonia, *Angew. Chem., Int. Ed.*, 2008, **47**, 6263–6266.
- 14 J. P. Magnusson, S. Bersani, S. Salmaso, C. Alexander and P. Caliceti, *Bioconjugate Chem.*, 2010, **21**, 671–678.
- 15 M. L. Becker, J. Liu and K. L. Wooley, *Chem. Commun.*, 2003, 180–181.
- 16 M. L. Becker, J. Liu and K. L. Wooley, *Biomacromolecules*, 2004, **6**, 220–228.
- 17 J. Liu, V. Bulmus, D. L. Herlambang, C. Barner-Kowollik, M. H. Stenzel and T. P. Davis, *Angew. Chem., Int. Ed.*, 2007, **46**, 3099–3103.
- 18 M. Li, P. De, S. R. Gondi and B. S. Sumerlin, *Macromol. Rapid Commun.*, 2008, **29**, 1172–1176.
- 19 M. Li, P. De, H. Li and B. S. Sumerlin, *Polym. Chem.*, 2010, **1**, 854–859.
- 20 V. Vazquez-Dorbatt, Z. P. Tolstyka and H. D. Maynard, *Macromolecules*, 2009, **42**, 7650–7656.
- 21 K. T. Wiss, O. D. Krishna, P. J. Roth, K. L. Kiick and P. Theato, *Macromolecules*, 2009, **42**, 3860–3863.
- 22 C. Boyer, V. Bulmus, J. Liu, T. P. Davis, M. H. Stenzel and C. Barner-Kowollik, *J. Am. Chem. Soc.*, 2007, **129**, 7145–7154.
- 23 P. De, M. Li, S. R. Gondi and B. S. Sumerlin, *J. Am. Chem. Soc.*, 2008, **130**, 11288–11289.
- 24 F. D. Jochum, P. J. Roth, D. Kessler and P. Theato, *Biomacromolecules*, 2010, **11**, 2432–2439.
- 25 D. Roy, J. N. Cambre and B. S. Sumerlin, *Chem. Commun.*, 2009, 2106–2108.
- 26 D. Roy, J. N. Cambre and B. S. Sumerlin, *Chem. Commun.*, 2008, 2477–2479.
- 27 S. Kulkarni, C. Schilli, B. Grin, A. H. E. Müller, A. S. Hoffman and P. S. Stayton, *Biomacromolecules*, 2006, **7**, 2736–2741.
- 28 C. L. Duvall, A. J. Convertine, D. S. W. Benoit, A. S. Hoffman and P. S. Stayton, *Mol. Pharmacol.*, 2010, **7**, 468–476.
- 29 S. Venkataraman and K. L. Wooley, *Macromolecules*, 2006, **39**, 9661–9664.
- 30 J. Nicolas, V. San Miguel, G. Mantovani and D. M. Haddleton, *Chem. Commun.*, 2006, 4697–4699.
- 31 D. Bontempo and H. D. Maynard, *J. Am. Chem. Soc.*, 2005, **127**, 6508–6509.
- 32 A. B. Lowe and C. L. McCormick, *Prog. Polym. Sci.*, 2007, **32**, 283–351.
- 33 M. Li, H. Li, P. De and B. S. Sumerlin, *Macromol. Rapid Commun.*, 2011, **32**, 354–359.
- 34 H. Li, A. P. Bapat, M. Li and B. S. Sumerlin, *Polym. Chem.*, 2011, **2**, 323–327.
- 35 K. T. Kim, J. J. L. M. Cornelissen, R. J. M. Nolte and J. C. M. van Hest, *Adv. Mater.*, 2009, **21**, 2787–2791.
- 36 K. T. Kim, J. J. L. M. Cornelissen, R. J. M. Nolte and J. C. M. van Hest, *J. Am. Chem. Soc.*, 2009, **131**, 13908–13909.
- 37 L. Tao, J. Liu, J. Xu and T. P. Davis, *Org. Biomol. Chem.*, 2009, **7**, 3481–3485.