



Cite this: *Soft Matter*, 2025, 21, 914

Received 29th August 2024,  
Accepted 7th January 2025

DOI: 10.1039/d4sm01036a

[rsc.li/soft-matter-journal](https://rsc.li/soft-matter-journal)

# $\alpha$ -Synuclein interaction with POPC/POPS vesicles†

Marija Dubackic,<sup>id</sup>\*<sup>a</sup> Veronica Lattanzi,<sup>id</sup><sup>ab</sup> Yun Liu,<sup>cd</sup> Michael Haertlein,<sup>e</sup>  
 Juliette M. Devos,<sup>id</sup><sup>e</sup> Emma Sparr,<sup>id</sup><sup>a</sup> Sara Linse,<sup>id</sup><sup>b</sup> and Ulf Olsson<sup>id</sup><sup>a</sup>

We have investigated the adsorption of the amyloid-forming protein  $\alpha$ -Synuclein ( $\alpha$ Syn) onto small unilamellar vesicles composed of a mixture of zwitterionic POPC and anionic POPS lipids.  $\alpha$ Syn monomers adsorb onto the anionic lipid vesicles where they adopt an  $\alpha$ -helical secondary structure. The degree of adsorption depends on the fraction of anionic lipid in the mixed lipid membrane, but one needs to consider the electrostatic shift of the serine  $pK_a$  with increasing fraction of POPS. The vesicles with adsorbed  $\alpha$ Syn monomers are kinetically stable. However, after fibrils have been formed, here triggered by the addition of a small concentration of pre-formed fibrils (seeds), we observed that the average vesicle size increased by approximately a factor of two. This increase in the vesicle size can be explained by vesicle fusion taking place during the fibril formation process.

## 1 Introduction

$\alpha$ -Synuclein ( $\alpha$ Syn) is a 140 amino acid residues long, intrinsically disordered protein, abundantly present in neurons. Monomeric  $\alpha$ Syn in solution has a random coil conformation. However, when associated with lipid membranes, a part of the protein molecule can adopt an  $\alpha$ -helical structure<sup>1,2</sup> and, under certain conditions, the protein can self-assemble into amyloid fibrils by arranging part of its sequence into  $\beta$ -strands.<sup>3,4</sup>  $\alpha$ Syn has been receiving significant attention since it has been associated with Parkinsons disease (PD), following the discovery that mutations in the SNCA gene are related to PD.<sup>5</sup> The protein is moreover the main component of neuronal inclusions that are a hallmark of PD, so-called Lewy bodies (LBs),<sup>6</sup> where  $\alpha$ Syn is present in fibrillar form ref. 7.

The  $\alpha$ Syn sequence can be divided into three domains. The N-terminal domain, composed of the first 60 residues, has a positive net charge around neutral pH and has been found to adopt an  $\alpha$ -helical structure upon association with negatively charged lipid membranes.<sup>8</sup> It is believed that it is the presence of a repetitive KTKGEV sequence in the N-terminus, which

allows  $\alpha$ Syn to adopt an  $\alpha$ -helical structure.<sup>9</sup> The middle part of the  $\alpha$ Syn sequence, the so-called non-amyloid- $\beta$  component (NAC), consists of 34 residues that are mostly hydrophobic. The NAC region is believed to play a critical role in amyloid formation<sup>10</sup> and is also implicated in the interaction with lipid moieties.<sup>1</sup> The C-terminus contains mainly negatively charged residues, and it is unstructured also when the protein is adsorbed at lipid membranes<sup>11</sup> as well as in amyloid fibrils.<sup>4</sup>

The physiological role of  $\alpha$ Syn is not fully understood. However, it is implied in the interaction with lipids and lipid membranes,<sup>12–16</sup> as well as in neurotransmission and the corresponding trafficking of synaptic vesicles.<sup>12,13</sup> While the protein has been reported to facilitate vesicle fusion,<sup>17,18</sup> a recent study highlights that fission or stable shape deformations are more likely scenarios.<sup>19</sup> Furthermore, the presence of various lipids has been detected in LBs.<sup>20,21</sup> Hence, as both the physiological function and possibly the role of  $\alpha$ Syn in PD are related to interactions of the protein with lipid membranes, such interactions have been extensively studied in the past decades.<sup>22</sup> It has been demonstrated that  $\alpha$ Syn monomers adsorb to anionic lipid membranes,<sup>23–28</sup> with its N-terminal domain forming an  $\alpha$ -helix at the membrane interface<sup>1,2,29,30</sup> which leads to increased acyl-chain ordering of the lipids in the bilayer and stabilization of the vesicles.<sup>31,32</sup> It has also been shown that the number of residues in the N-terminus which adopts  $\alpha$ -helical conformation depends on lipid-to-protein ratio.<sup>1,11,30,33,34</sup> Due to the net positive charge of the N-terminus, attractive electrostatic interactions are considered to be an important driving force for adsorption<sup>35</sup> in addition to a hydrophobic component.<sup>36</sup> However, the role of the negative membrane charge may alternatively be to modulate and dampen the electrostatic repulsion between the positively charged N-termini in the adsorbed state.

<sup>a</sup> Physical Chemistry, Chemistry Centre, Lund University, SE-22100 Lund, Sweden.  
E-mail: [majuskad@hotmail.com](mailto:majuskad@hotmail.com)

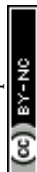
<sup>b</sup> Biochemistry and Structural Biology, Chemistry Centre, Lund University,  
SE-22100 Lund, Sweden

<sup>c</sup> Center for Neutron Research, National Institute of Standards and Technology,  
20878 Gaithersburg, Maryland, USA

<sup>d</sup> Chemical and Biomolecular Engineering Department, University of Delaware,  
19716, Newark, Delaware, USA

<sup>e</sup> Life Sciences Group, Institut Laue-Langevin, 38000 Grenoble, France

† Electronic supplementary information (ESI) available. See DOI: <https://doi.org/10.1039/d4sm01036a>



The electrostatic contribution is expected to depend on the pH of the solution, in particular around the effective  $pK_a$  of the anionic lipid and the isoelectric point (IP) of  $\alpha$ Syn, which are not necessarily that far apart for the serine lipid headgroup and  $\alpha$ Syn.

Fibril formation in the presence of various lipid membranes has been extensively studied,<sup>37–45</sup> and it was shown that under some conditions the presence of vesicles during fibril formation may act as an aggregation catalyser.<sup>37–40</sup> Protein-induced membrane remodeling has also been observed.<sup>22,46,47</sup>

In this work, we investigated how  $\alpha$ Syn interacts with small unilamellar vesicles (SUVs), composed of a mixture of zwitterionic phospholipids 1-palmitoyl-2-oleoyl-*glycero*-3-phosphocholine (POPC) and anionic 1-palmitoyl-2-oleoyl-*sn-glycero*-3-phosphoserine (POPS). The vesicle radii in this study were targeted to be similar to those of the synaptic vesicles,  $\approx 15$ –20 nm.<sup>48</sup> We investigated the adsorption of  $\alpha$ Syn onto lipid membranes by determining the amount of membrane-bound  $\alpha$ -helices using circular dichroism (CD), when the latter ones are composed of 10%, 15%, 20%, 30% and 50% charged lipids. We also calculated the number of lipid molecules per number of protein molecules, which are involved in binding at different fractions of anionic lipids ( $\beta$ ). Using small-angle X-ray scattering (SAXS), we looked into the effect of  $\alpha$ Syn on the vesicle scattering profile, and related the difference to the findings from CD experiments. We also investigated the end-state of the fibril formation in the presence of lipid vesicles by means of cryogenic transmission electron microscopy (cryo-TEM) and small-angle neutron scattering (SANS).

## 2 Materials and methods

### 2.1 $\alpha$ -Synuclein

Human  $\alpha$ Syn was expressed in *Escherichia coli* from a synthetic gene with *E. coli*-optimized codons cloned into a Pet3a plasmid (purchased from Genscript, Piscataway) and purified as described previously in ref. 49. Protein monomers were isolated by size exclusion chromatography (SEC) in 10 mM MES buffer at pH = 5.5 using a 24 mL Superdex75 column (GE healthcare). Protein samples corresponding to the central region of the peak were collected. Following this, buffer salts were removed by desalting on a 5 ml HiTrap desalting (GE Healthcare) column. The protein concentration was determined by absorbance at 280 nm using an extinction coefficient  $5800 \text{ M}^{-1} \text{ cm}^{-1}$ . To obtain the high concentration required for scattering experiments, samples were lyophilised after being desalted.

The matchout deuterated  $\alpha$ Syn was produced in *E. coli*. Cell pellet containing matchout deuterated  $\alpha$ Syn was prepared in the Deuteration Laboratory of the Institut Laue-Langevin in Grenoble, France using a modified protocol from the one described in ref. 2. A high cell density fed-batch culture using 85% deuterated Enfors minimal medium was grown at a temperature of 30 °C and  $pO_2$  at 30% saturation.<sup>50</sup> The degree of deuteration was 75% as confirmed by mass spectrometry. Deuterated  $\alpha$ Syn monomers were isolated by SEC as described above and lyophilised in order to obtain high concentration.

### 2.2 Lipid vesicles

The lipids used in this study were the zwitterionic POPC and anionic POPS. All lipids were obtained from Avanti Polar Lipids (Alabaster, AL, USA). In the preparation of mixed lipid vesicles, lipids were weighted and mixed at the desired proportion ( $\beta = 0.1$ ,  $\beta = 0.15$ ,  $\beta = 0.2$ ,  $\beta = 0.3$  and  $\beta = 0.5$ ). The powder was dissolved in a chloroform/methanol (3/1 volume ratio) mixture. The solvent was evaporated under a stream of  $N_2$  gas, and the created lipid film was dried in a overnight under vacuum. The lipids were finally dispersed in the desired buffer (20 mM phosphate buffer (PB) at pH 6.0, 6.5, 7.0 and 7.4) and vortexed for a few minutes.

SUVs were prepared *via* sonication. The sonication was performed for 15 min, 10 s on/off duty at 70% amplitude on ice. The lipid dispersions were then centrifuged for 10 min at 13 000 rpm in order to pellet any contaminating particles from the sonicator tip. The supernatant was collected and used as the vesicle dispersion.

### 2.3 Sample preparation

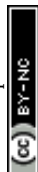
For circular dichroism (CD) spectroscopy, protein monomers were collected after SEC in 20 mM PB, pH = 7.0. Subsequently, the monomeric protein solution was mixed with different amounts of vesicle dispersion to obtained the desired lipid-to-protein (L/P) ratios.

For small-angle X-ray scattering (SAXS) and dynamic light scattering (DLS) samples were prepared using desalted and lyophilised  $\alpha$ Syn. The protein powder was first dissolved in 1 mM NaOH at pH = 11.4 for half an hour, which ensures that we are starting from monomeric solution. Following this, the same volume of 40 mM PB at pH = 7.0 was added. Finally, the correct amount of vesicle dispersion in 20 mM PB at pH = 7.0 was added.

For small-angle neutron scattering (SANS) samples were prepared using the lyophilized protein powder containing buffer salts. The powder was resuspended in filtered  $D_2O$ . Seeds, *i.e.* preformed  $\alpha$ Syn fibrils, were added to a concentration corresponding to 5% of the total  $\alpha$ Syn concentration in monomer units. Finally, a lipid vesicle dispersion was added. At the end, the final concentration of  $\alpha$ Syn monomers was equal to 280  $\mu\text{M}$ . The samples were prepared with a lipid concentration of 2.1 mM, which corresponds to a lipid to protein ratio of 7.5. All samples were incubated in Axygen low-binding tubes at 37 °C for 14 days under quiescent conditions.

### 2.4 Circular dichroism

CD spectra were recorded using a JASCO J-715 CD spectrometer in 1 mm path length quartz cuvette (Hellma 110-QS). The measurement settings were 1 nm bandwidth, 2 s response time and 20 nm  $\text{min}^{-1}$  scan rate. The measurements were performed at 25 °C and an average of 5 scans was used for each measurement. The protein concentration was 5  $\mu\text{M}$  and the lipid concentration was varied. The data are presented as the mean residue ellipticity,  $[\theta]$ , which is calculated as  $[\theta] = \frac{\theta}{nlc}$ ,



where  $\theta$  is the ellipticity in deg,  $l$  is the path length in cm,  $c$  is the protein concentration in dmol per cm<sup>3</sup> and  $n$  is the number of residues.

## 2.5 Dynamic light scattering and electrophoretic mobility

The hydrodynamic radius of vesicles with adsorbed  $\alpha$ Syn was monitored over time using 3D LS Spectrometer, LS Instruments, AG, equipped with  $\lambda = 660$  nm Cobolt laser with maximum power of 100 mW. The correlation functions were recorded from 60° to 145° with 5° steps. The measurements were performed at 37 °C in 5 mm radius glass capillaries, emerged in a refractive index-matching liquid, decalin. A z-averaged decay rates,  $\langle \Gamma_z \rangle$  were obtained by applying cumulant analysis on correlation functions measured at different angles, as described in ref. 51.  $\langle \Gamma_z \rangle$  is further related to a collective diffusion coefficient,  $\langle D_c \rangle_z$  through the relation  $\langle \Gamma_z \rangle = \langle D_c \rangle_z q^2$ , where  $q = 4\pi/n\lambda \sin(\theta/2)$  is the scattering vector magnitude, with  $n$  being the refractive index of solvent. Hence, extrapolating  $\langle \Gamma_z \rangle$  to zero  $q$  we obtain the diffusion coefficient. Assuming non-interacting particles (infinite dilution)  $D_c = D_0$ , where  $D_0$  is the self-diffusion coefficient which is related to the hydrodynamic radius,  $\langle R_H \rangle_z$ , via the Stokes–Einstein relation  $\langle D_0 \rangle_z = k_B T / (6\pi\eta \langle R_H \rangle_z)$ , where  $K_B = 1.3810 \times 10^{-23}$  J K<sup>-1</sup> is the Boltzmann constant,  $T$  is temperature and  $\eta$  is the solvent viscosity.

Other DLS experiments and electrophoretic mobility measurements were performed on a Zetasizer Nano ZS instrument (Malvern Instruments, Ltd, Worcestershire, UK) at  $\theta = 173^\circ$  using laser light of  $\lambda = 632.8$  nm wavelength. The electrophoretic mobility,  $U_E$  provides information about the  $\zeta$ -potential, which tells us about the surface charge of the colloidal particles, via Henry's equation:  $U_E = \frac{2\varepsilon\varepsilon_0\zeta}{3\eta} f(kR_H)$ , where  $\varepsilon$  and  $\varepsilon_0$  are dielectric constant of the solvent and vacuum permittivity, respectively, and  $\eta$  is the solvent viscosity. The  $\zeta$ -potential was calculated assuming the Smoluchowski approximation, which gives  $f(kR_H) = 1.5$ .

## 2.6 Small-angle X-ray scattering

SAXS experiments were performed on a SAXS-lab Ganesha pinhole instrument JJ X-ray System APS (JJ X-ray, Hoersholm, Denmark) with an X-ray microsource (Xenocs, Sassenage, France) and a two-dimensional 300k Pilatus detector (Dectris Ltd, Baden-Daettwil, Switzerland). Two sample-to-detector distances were used and the X-ray wavelength,  $\lambda$ , was 1.54 Å. The two-dimensional scattering pattern was always isotropic (circularly symmetric) and was therefore radially averaged to obtain the one-dimensional scattering function,  $I(q)$ , where  $q = 4\pi/\lambda \sin(\theta/2)$  is the magnitude of the scattering vector,  $\theta$  being the scattering angle. Absolute scaling of the scattered intensity was performed by using water as a calibration standard. Scattering from the buffer measured in the same capillary as the sample was subtracted.

## 2.7 Small-angle neutron scattering

SANS experiments were performed at NIST Center for Neutron Research in Maryland, USA. The instrument used was NG7 SANS. Four sample to-detector distances (1 m, 4 m, 13 m and

15.3 m with lenses), and a neutron wavelength of 6.0 Å (sample-to-detector distances of 1 m, 4 m and 13 m) and 8.1 Å (15.3 m with lenses) were used to obtain a  $q$  range spanning from 0.001 Å<sup>-1</sup> to 0.5 Å<sup>-1</sup>. The wavelength spread is approximately 12%.<sup>52</sup> The data were reduced to the absolute scale using the Igor Pro software by following the standard protocol at NCNR to correct the effect of the background, empty cell, detector efficiency, and the transmission of each sample.<sup>53</sup> Samples were measured in 1 mm path length cylindrical quartz cells. Measurements were performed at  $T = 20$  °C, 30 °C, 37 °C, 50 °C and 80 °C.

## 2.8 Cryogenic transmission electron microscopy

Cryo-TEM experiments were performed using JEM-2200FS transmission electron microscope (JEOL) at the National Center for High Resolution Electron Microscopy (nCHREM) at Lund University. The Schottky field-emission electron source is operated at an acceleration voltage of 200 kV. The filters and slits used were an in-column energy (omega) filter and a 25 eV slits. The images were recorded via SerialEM software under low-dose conditions onto a bottom-mounted TemCam-F416 camera (TVIPS).

Samples were prepared by depositing 4  $\mu$ L droplets on carbon-coated Ted Pella grids, which were then blotted with filter papers. The grids were then plunged into liquid ethane at ca. -184 °C. The plunging was performed in an automatic plunge-freezer system (Leica EM GP) with the environmental chamber operated at 20.0 °C and 90% relative humidity. The grids were stored in liquid nitrogen at -196 °C before imaging.

# 3 Results and discussion

## 3.1 Adsorption of monomeric $\alpha$ Syn onto small unilamellar vesicles (SUVs)

As  $\alpha$ Syn undergoes a transition from a random coil to a large fraction of  $\alpha$ -helical structure when it adsorbs to anionic lipid membranes,<sup>1,2</sup> it is possible to follow the adsorption using CD spectroscopy.<sup>38</sup> Here we have focused on the adsorption of  $\alpha$ Syn to SUVs composed of a mixture of the zwitterionic lipid POPC and the anionic lipid POPS, at different fractions of the anionic lipid,  $\beta$ . The radii of vesicles at different  $\beta$  values varies between 25 nm and 27 nm. CD experiments were performed on solutions containing 5  $\mu$ M  $\alpha$ Syn and varying concentrations of lipids in 20 mM PB, pH = 7.0, at 25 °C. Results are shown in Fig. 1 where the lipid concentrations are presented as the lipid-to-protein molar ratio, L/P. In Fig. 1a we present CD spectra at different L/P for  $\beta = 0.3$ . For L/P = 0, we see the typical CD spectrum from proteins with a random coil conformation.<sup>54</sup> With addition of lipid vesicles we observe the emergence of two minima at  $\lambda \approx 208$  nm and  $\lambda \approx 222$  nm, which are signatures of an  $\alpha$ -helical conformation.<sup>54</sup> At high L/P values, the CD spectrum no longer changes, indicating that adsorption is saturated and essentially all protein molecules have adsorbed onto vesicles with the maximum amount of  $\alpha$ -helix of almost



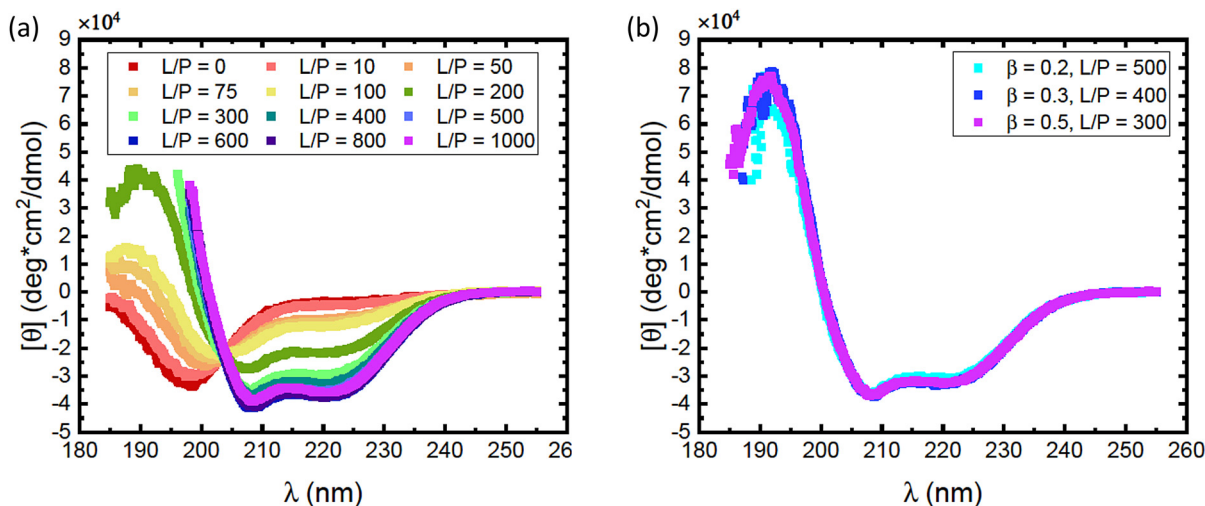


Fig. 1 (a) CD spectra obtained for different  $L/P$ , for the case of vesicles with composition  $\beta = 0.3$  at pH = 7.0. The protein concentration was  $c_p = 5 \mu\text{M}$  and the lipid concentration was varied. (b) Spectra obtained for lowest  $L/P$  above saturation for lipid systems with  $\beta = 0.2$  (cyan squares),  $\beta = 0.3$  (blue squares) and  $\beta = 0.5$  (purple squares). The saturation was found at  $L/P = 500$  for  $\beta = 0.2$ ,  $L/P = 400$  for  $\beta = 0.3$  and  $L/P = 300$  for  $\beta = 0.5$ .

100 residues. The  $L/P$  value above which saturation is observed we refer to as  $(L/P)_{\text{sat}}$ . At  $\beta = 0.3$ , we estimate  $(L/P)_{\text{sat}} = 400$ .

It has been shown that  $\alpha\text{Syn}$  adsorbs to negatively charged membranes with its net positively charged N-terminus which adopts an  $\alpha$ -helical conformation, while the net negatively charged C-terminus remains disordered and protrudes into the bulk solution.<sup>1,30</sup> The fraction of the molecule that adopts an  $\alpha$ -helical conformation can vary.<sup>1,11,30,33,34</sup> Typically this fraction is smaller at low  $L/P$  and involves a maximum of  $\approx 100$  residues at saturation.<sup>1,30</sup> Thus, the CD spectrum at saturation is expected to represent a mixture of approximately 2/3  $\alpha$ -helix and 1/3 random coil. These saturation spectra were essentially identical for  $\beta = 0.2, 0.3$  and  $0.5$ , as shown in Fig. 1b. The noisy data at low wavelengths are caused by significant scattering from vesicles which are present in high concentrations at these  $L/P$  ratios.

Consistent with an earlier study,<sup>26</sup> we note that the variation with  $L/P$  shows an isodichroic point at  $\lambda \approx 203 \text{ nm}$ , indicating the coexistence of two states that are populated to varying degree. In fact, the CD spectra at different  $L/P$ , here presented as the mean residue ellipticity,  $[\theta]$ , are well described by a linear combination of the random coil spectrum at  $L/P = 0$ ,  $[\theta]_{L/P=0}$ , and the spectrum obtained at saturation,  $[\theta]_{\text{sat}}$ .<sup>55</sup> This can be seen in Fig. 2a, where we compare data with linear combinations for a few selected  $L/P$  in the lipid system with  $\beta = 0.3$ . The linear combination was calculated as

$$[\theta] = (1 - f)[\theta]_{L/P=0} + f[\theta]_{\text{sat}} \quad (1)$$

where  $f$  is the fraction of  $[\theta]_{\text{sat}}$  spectrum in the linear combination. In Fig. 2b, we have plotted how  $f$  varies with  $L/P$  for different fractions,  $\beta$ , of POPS in the lipid mixture. As can be seen,  $f$  increases approximately linearly with  $L/P$  until

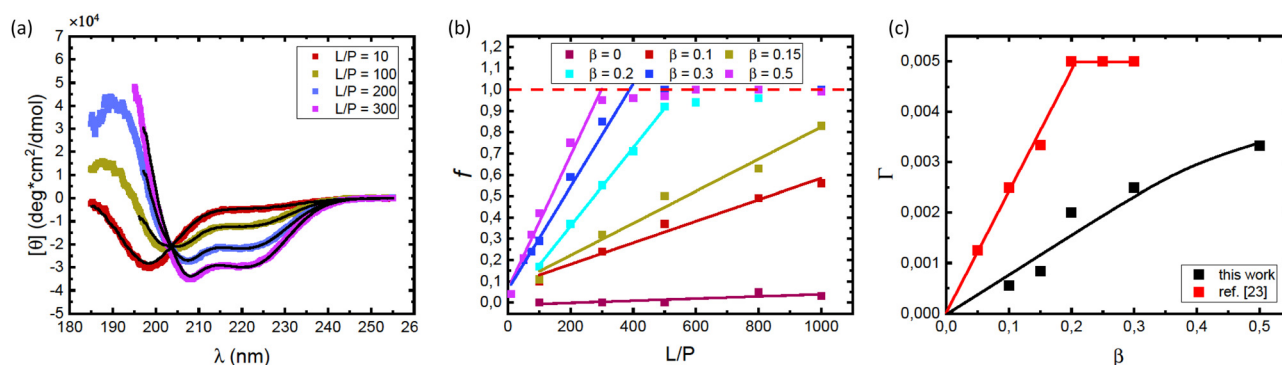
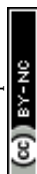


Fig. 2 (a) CD spectra obtained for different  $L/P$ , for the case of vesicles with composition  $\beta = 0.3$  at pH = 7.0. The protein concentration was  $c_p = 5 \mu\text{M}$ . Solid black lines are best fits of linear combinations as described by eqn (1), from which values of the fraction  $f$  were obtained. (b) The fraction  $f$  plotted versus  $L/P$  for different lipids compositions  $\beta$  as indicated in the figure. The protein concentration was  $c_p = 5 \mu\text{M}$ . The saturation points, i.e. the minimum  $L/P$  values for which  $f = 1$  were evaluated. The saturation points estimated were  $(L/P)_{\text{sat}} = 500$  for  $\beta = 0.2$ ,  $(L/P)_{\text{sat}} = 400$  for  $\beta = 0.3$ , and  $(L/P)_{\text{sat}} = 300$  for  $\beta = 0.5$ . (c) Estimated adsorbed amount  $\Gamma = 1/(L/P)_{\text{sat}}$  plotted versus the fraction of anionic lipid,  $\beta$ . Data from the present work (pH = 7.0) are shown with black square symbols. For comparison we also plot similar data from ref. 23, obtained at pH = 5.5. Solid lines are merely guides to the eye.



saturation is reached. We note that  $f$  may not be a direct measure of the adsorbed amount of protein, but rather reports on the relative amounts of  $\alpha$ -helix and random coil conformations in total.

Saturation with respect to  $\alpha$ -helical signal ( $f = 1$ ) is concluded by no further changes in the CD spectra with increasing L/P ratio. Here we can identify an adsorbed amount as  $\Gamma = 1/(L/P)_{\text{sat}}$ , where  $(L/P)_{\text{sat}}$  is estimated from Fig. 2b as the L/P value where  $f$  reaches 1. For  $\beta = 0.2$ , we estimate  $\Gamma = 1/500$ , for  $\beta = 0.3$  we estimate  $\Gamma = 1/400$  and for  $\beta = 0.5$  we estimate  $\Gamma = 1/300$ . By linear extrapolation we also estimate  $\Gamma = 1/1200$  for  $\beta = 0.15$ , with reasonable accuracy. For  $\beta = 0.1$  extrapolation becomes more uncertain, but if we assume a linear dependence, we obtain  $\Gamma = 1/1800$ . These  $\Gamma$ -values are plotted against  $\beta$  in Fig. 2c. The fact that an increased amount of POPS leads to an increase in  $\Gamma$  implies that the adsorption is, to a large extent, governed by an electrostatic attraction between the net positively charged N-terminal part of  $\alpha$ Syn and the negatively charged membrane.<sup>24,25</sup> Additionally, the observed increase in  $\Gamma$  with  $\beta$  appears to level off at higher  $\beta$  values.

With the goal of gaining further insight into how electrostatic interactions govern the adsorption process, it is useful to compare our findings with the recent work of Andersson *et al.*,<sup>23</sup> who also investigated  $\alpha$ Syn adsorption onto a lipid membrane system while varying the fraction of anionic lipids, but at a lower pH of 5.5. The lipid systems used in both studies are nearly identical, with a slight difference reflected in the fact that Andersson *et al.* used 1,2-dioleoyl-*sn*-glycero-3-phospho-L-serine (DOPS) as the anionic lipid. However, the difference between DOPS and POPS, used in the current study, is considered negligible. Furthermore, it has been shown that changes in headgroup chemistry do not affect  $\alpha$ Syn binding to vesicles, provided that the charge of the headgroups remains unchanged.<sup>56</sup> As a result, the response to changes in pH is expected to be similar in the two studies compared.

In Fig. 2c we have included how  $\Gamma = 1/(L/P)_{\text{sat}}$  varies with  $\beta$  taken from the data presented in Fig. 2b of ref. 23. As can be seen,  $\alpha$ Syn has a significantly stronger affinity for the PC/PS membrane at pH = 5.5 compared to at pH = 7.0. Furthermore, at pH = 5.5,  $\Gamma$  appears to level off to a plateau at  $\Gamma = \Gamma_{\text{max}} = 0.005$  for  $\beta \geq 0.2$ .

A similar strong difference in adsorption between pH = 7.0 and pH = 5.5 has been reported for the case of POPC/POPS vesicles.<sup>26</sup> Furthermore, Middleton and Rhoades studied the adsorption of  $\alpha$ Syn onto POPC/POPS ( $\beta = 0.5$ ) vesicles at pH = 5.0 and found saturation at an L/P as low as  $\approx 40$ .<sup>27</sup> We note also that our observed  $L/P_{\text{sat}}$  at pH = 7.0 for  $\beta = 0.5$  is very similar to that observed by Lokappa and Ulmer at pH = 7.4.<sup>28</sup>

The leveling off of  $\Gamma$  at higher values of L/P could be due to a state of saturation being reached, where the vesicles are completely covered with protein and there is no room for more. Another possibility is that the net surface charge density,  $\sigma$ , varies linearly with  $\beta$  for low POPS fractions, but approaches a saturation at higher  $\beta$ -values. This is indeed indicated by the data in Fig. 3a where we have plotted the  $\zeta$  potential as a function of  $\beta$ . The  $\zeta$ -potential decreases to negative values when  $\beta$  increases. However, the slope decreases with increasing  $\beta$ . At pH = 7 we are well above the intrinsic  $pK_a$  of the carboxylate group of the POPS headgroup.<sup>57</sup> However, with increasing  $\beta$  the interface is becoming increasingly negatively charged, leading to an increase of the  $pK_a$ , which is expected to significantly shift the acid-base equilibrium towards the acid state as also observed in highly charged proteins and protein aggregates.<sup>58,59</sup> We illustrate this effect below by estimating how the surface charge density,  $\sigma$ , depends on  $\beta$ .

The  $pK_a$  depends on the surface potential,  $\psi_s$ , according to ref. 60.

$$pK_a = pK_a^0 - \frac{e\psi_s}{\log_{10} k_B T}. \quad (2)$$

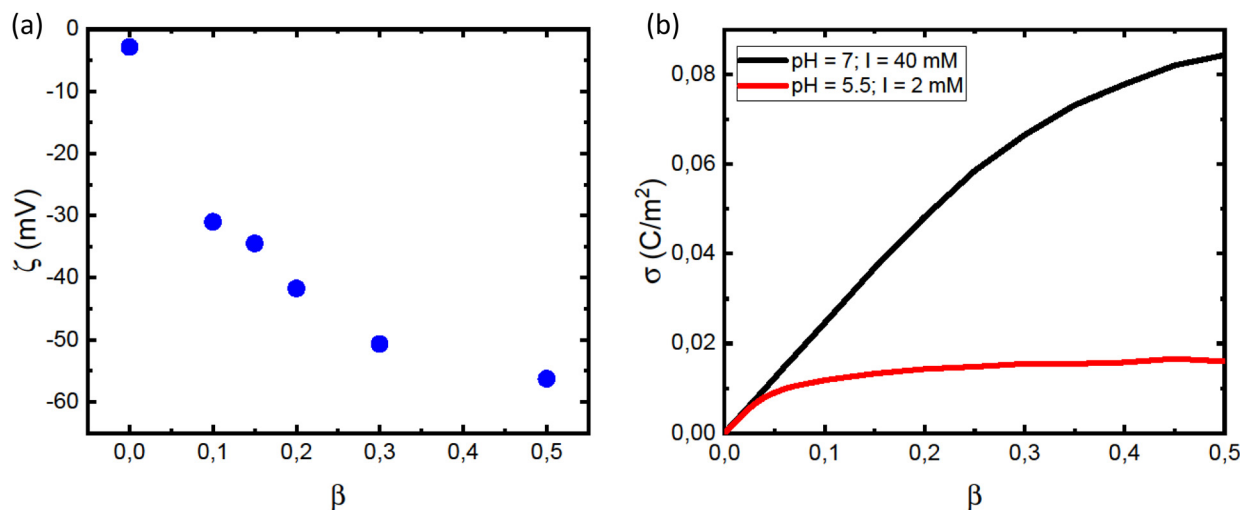


Fig. 3 (a) Dependence of the vesicle  $\zeta$  potential on the fraction of charged lipids,  $\beta$ . (b) Calculated dependence of the surface charge,  $\sigma$ , on  $\beta$ , for pH = 7.0 and  $I = 40$  mM (black line) and pH = 5.5 and  $I = 2$  mM (red line).



Here  $pK_a^0$  is the intrinsic  $pK_a$  value at  $\psi_s = 0$ ,  $e$  is the elemental charge,  $k_B$  is Boltzmann's constant and  $T$  is the absolute temperature. Within the Debye-Hückel approximation, the surface potential depends linearly on  $\sigma$ ,

$$\psi_s = \frac{\sigma}{\epsilon_0 \epsilon_r \kappa} \quad (3)$$

where  $\epsilon_0$  is the permittivity of vacuum,  $\epsilon_r$  is the dielectric constant of the solvent, and  $\kappa$  is the inverse of the Debye screening length. Denoting the fraction of dissociated acid molecules  $\alpha$ , and assuming a constant area per lipid molecule,  $a_L$ , we have

$$\sigma = \frac{\alpha \beta e}{a_L} \quad (4)$$

We also have

$$pK_a = pH - \log_{10} \frac{\alpha}{1 - \alpha}, \quad (5)$$

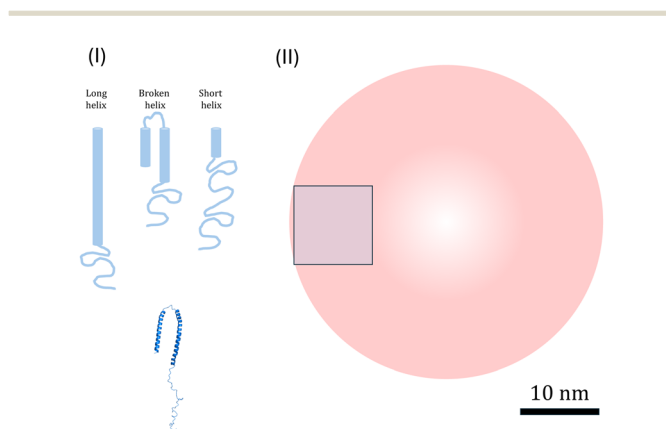
and from eqn (2) and (5) is possible to solve how  $\alpha$ ,  $\psi_s$  and  $\sigma$  depend on  $\beta$ . In Fig. 3b, we have plotted  $\sigma$  versus  $\beta$  using reasonable values for the different parameters:  $pK_a^0 = 3.6$ ,<sup>57</sup>  $a_L \approx 0.65 \text{ nm}^2$ ,<sup>61</sup>  $\epsilon_r = 80$ ,  $T = 298 \text{ K}$ , and calculating  $\kappa$  from the buffer ionic strength,  $I \approx 40 \text{ mM}$ . As can be seen, the calculated  $\sigma$  increases linearly at lower  $\beta$ -values, whereas the nonlinear dependence at higher  $\beta$  values is at least in qualitative agreement with the  $\zeta$ -potential data. In Fig. 3b we also include the corresponding calculated values of  $\sigma$  at  $pH = 5.5$ . At these experiments  $10 \text{ mM}$  MES buffer was used giving an ionic strength  $I = 2 \text{ mM}$ . At this lower  $pH$  we are closer to  $pK_a^0$ , and the  $\sigma$  is therefore lower compared to  $pH = 7.0$ .

We conclude that  $\alpha\text{Syn}$  adsorbs with higher surface coverage to the anionic vesicles at  $pH = 5.5$  compared to  $pH = 7.0$ , even though the estimated membrane charge density appears to be significantly lower. There is clearly an attractive electrostatic component to the adsorption as this is promoted by anionic lipids, and there is likely also an attractive hydrophobic interaction.<sup>36</sup> However, in addition, there is the unfavorable electrostatic repulsion between the disordered negatively charged C-termini that lowers the coverage. One should also keep in mind that there is a repulsive electrostatic component to the coverage as a result of the overall protein net charge, which is  $pH$  dependent. For  $\alpha\text{Syn}$ ,  $IP \approx 4.7$ . The net charge of monomeric  $\alpha\text{Syn}$  at  $pH 5.5$  is  $\approx -5$  as calculated based on the reported  $pK_a$  values of His50 and all acidic groups,<sup>62</sup> while at  $pH = 7.0$ , the protein charge is close to  $-9$ .<sup>63,64</sup> The higher surface coverage at  $pH = 5.5$  we therefore ascribe to the lower negative charge of the protein that lowers the repulsive protein-protein interactions at the lipid membrane interface, as well as the repulsive electrostatic component of the protein-membrane interaction. Moreover, the net charge of the protein is reduced in fibrils due to a  $pK_a$  value upshift of ca one unit upon assembly, an effect also expected upon surface adsorption of the protein on vesicles. We note that for  $pH = 5.5$ ,  $\sigma$  essentially levels off to a plateau for  $\beta > 0.2$  (Fig. 3b). This correlates well with the observed plateau in the adsorption,  $\Gamma$ , for  $\beta > 0.2$  (Fig. 2c), and is consistent with the view that it is

mainly the negative charges on the membrane that attract  $\alpha\text{Syn}$  molecules.

It is also useful to consider the density of  $\alpha\text{Syn}$  helices on the vesicle surfaces, and their possible packing. Several  $\alpha\text{Syn}$ -binding modes have been reported.<sup>11,30,33,34</sup> On lipid vesicle membranes,  $\alpha\text{Syn}$  can adsorb with a short helix, involving approximately the first 25 residues, an intermediate helix, involving approximately 50 first residues<sup>34</sup> or a long helix involving residues 1–97.<sup>11</sup> On the other hand, upon binding to small SDS micelles,  $\alpha\text{Syn}$  adopts a broken helical form with 2 almost equally long anti-parallel helical segments, involving residues 3–37 and 45–92, respectively, connected by a short linker.<sup>33</sup> These different modes are schematically illustrated in Fig. 4. More recently it has been reported that  $\alpha\text{Syn}$  for low L/P can also form long helix with only a part docking to the lipid membrane and the remaining part extending into the bulk.<sup>65</sup> This can be seen as an alternative to the short  $\alpha$ -helix, while at the same time the structure resembles the broken helix with only the N-terminal part in contact with the membrane.

CD spectra obtained at saturation are expected to represent the state of  $\alpha\text{Syn}$  adsorbed *via* a long helix. The CD spectra at saturation for  $\beta = 0.2$ ,  $0.3$  and  $0.5$ , respectively, presented in Fig. 1b are strikingly similar. As can be seen, they are essentially identical and show a significant contribution from  $\alpha$ -helical signal. A typical  $\alpha$ -helix far UV CD spectrum shows a positive band at  $\lambda = 193 \text{ nm}$  and two negative bands of similar amplitude at  $208 \text{ nm}$  and  $222 \text{ nm}$ , respectively, where the positive amplitude of the  $193 \text{ nm}$  band is approximately twice the negative amplitudes of the  $208 \text{ nm}$  and  $222 \text{ nm}$  bands.<sup>66,67</sup> In terms of mean residue ellipticity,  $[\theta]_\lambda$ , the typical values for  $\alpha$ -helix are  $[\theta]_{\text{helix}}(193 \text{ nm}) \approx 8 \times 10^4 \text{ deg cm}^2 \text{ dmol}^{-1}$  and  $[\theta]_{\text{helix}}(208 \text{ nm}) \approx [\theta]_{\text{helix}}(222 \text{ nm}) \approx -4 \times 10^4 \text{ deg cm}^2 \text{ dmol}^{-1}$ . This is in fact close to what we actually observe in Fig. 1b, and we conclude from this that, at saturation, a major part of the adsorbed  $\alpha\text{Syn}$  molecules must have adopted an  $\alpha$ -helix conformation.



**Fig. 4** (I) Illustration of three possible modes of  $\alpha$ -helices (light blue): long, broken and short, and the PDB structure of broken helix taken from ref. 33 (darker blue). (II) Illustration of  $R = 20 \text{ nm}$  vesicles (red) and  $100 \text{ nm}^2$  square (blue) corresponding to an average membrane area occupied by one  $\alpha\text{Syn}$  molecule at saturation for  $\beta = 0.5$ . The scale bar (10 nm) refer to all illustrations.



We can also consider the density of the  $\alpha$ Syn molecules on the vesicle surface at the saturation. For the highest fraction of POPS investigated here,  $\beta = 0.5$ , we find  $\Gamma = 1/300$  (see Fig. 2b). Since there are approximately the same number of lipids in the two monolayers, this means that there is one  $\alpha$ Syn molecule adsorbed per 150 lipid molecules in the outer monolayer. With an area per lipid of  $a_L = 0.65 \text{ nm}^2$ , this corresponds to one  $\alpha$ Syn molecule per *circa*  $100 \text{ nm}^2$ . To visualize this we show a  $10 \text{ nm} \times 10 \text{ nm}$  square in Fig. 4. A vesicle with  $R = 20 \text{ nm}$  has a bilayer area of *ca.*  $1300 \text{ nm}^2$ , hence we expect *circa* 13 adsorbed  $\alpha$ Syn molecules per vesicle for  $\beta = 0.5$  at saturation.

A typical  $\alpha$ -helix has 3.6 residues per turn, with  $0.54 \text{ nm}$  rise per turn, and has a diameter of approximately  $1.2 \text{ nm}$ . The long 97 residue extended  $\alpha$ -helix of  $\alpha$ Syn is thus *circa*  $15 \text{ nm}$  long. We note first that this length is similar to the vesicle radius of  $\approx 20 \text{ nm}$ . In Fig. 4 we have also drawn a  $20 \text{ nm}$  radius vesicle on scale together with the different forms of  $\alpha$ -helix-containing  $\alpha$ Syn. The Figure also illustrates the average area occupied by a single  $\alpha$ Syn molecule at saturation for  $\beta = 0.5$ . From these simple geometrical considerations, we can conclude that  $\alpha$ Syn can adopt either of the possible helical states under the conditions investigated. In fact, Lokappa and Ulmer has suggested that  $\alpha$ Syn populates both elongated and broken helix states on small unilamellar vesicles.<sup>28</sup>

In order to gain further insight in the  $\alpha$ Syn adsorption, we investigated how the presence of protein influences the vesicle structure utilizing SAXS.<sup>68</sup> Due to the overall low lipid-water X-ray contrast, which results in relatively low scattered intensity at lower  $q$ -values, we used higher lipid concentrations compared to the CD experiments. In Fig. 5a, we compare SAXS data from vesicle samples in the presence and absence of  $\alpha$ Syn. The lipid concentration was  $c_L = 42 \text{ mM}$ , with  $\beta = 0.3$ , and the protein concentration was  $c_P = 0.14 \text{ mM}$ , corresponding to  $L/P = 300$ . As the signature of the bilayer scattering, a broad peak at

$q \approx 0.1 \text{ \AA}^{-1}$ , is essentially the same in both cases, we can conclude that the protein adsorption does not affect the bilayer structure. However, there is an increase in forward scattering when the vesicles are coated with protein.

In Fig. 5a, we are also showing the scattering curve from a sample containing only protein monomers. A protein concentration of  $0.14 \text{ mM}$  is sufficiently low for protein-protein interactions to be neglected, and the scattered intensity,  $I(q)$ , of protein monomers can be written as

$$I(q) = I(0)P_m(q). \quad (6)$$

Here  $P_m(q)$  is the normalized protein monomer form factor, given by the Debye equation<sup>69</sup>

$$P_m(q) = 2 \frac{e^{-q^2 R_g^2} + q^2 R_g^2 - 1}{q^2 R_g^2}, \quad (7)$$

where  $R_g$  is radius of gyration, and  $I(0)$  is the forward scattering, given by

$$I(0) = \frac{\Delta\rho^2 M_w}{d_p^2 N_A} c_p. \quad (8)$$

Here,  $\Delta\rho = 3.6 \times 10^{10} \text{ cm}^{-2}$  is the scattering length density (SLD) difference between protein ( $\rho_p = 12.6 \times 10^{10} \text{ cm}^{-2}$ ) and solvent ( $\rho_s = 9.47 \times 10^{10} \text{ cm}^{-2}$ ),  $M_w = 14.4 \times 10^3 \text{ g mol}^{-1}$  is the protein molar mass,  $d_p = 1.4 \text{ g cm}^{-3}$  is the protein mass density,  $N_A = 6.022 \times 10^{23} \text{ mol}^{-1}$  is Avogadro's number and  $c_p = 2 \times 10^{-3} \text{ g cm}^{-3}$  is the protein mass concentration. In Fig. 5a we are also showing the Debye model that best describes the data. The best agreement between the model and the data is obtained for  $I_0 = 0.02 \text{ cm}^{-1}$  and  $R_g = 4 \text{ nm}$ .

The bilayer contribution to the scattering profile of vesicles, both in the presence and absence of protein, was modeled using an approach proposed by Pabst *et al.*<sup>70</sup> The model takes

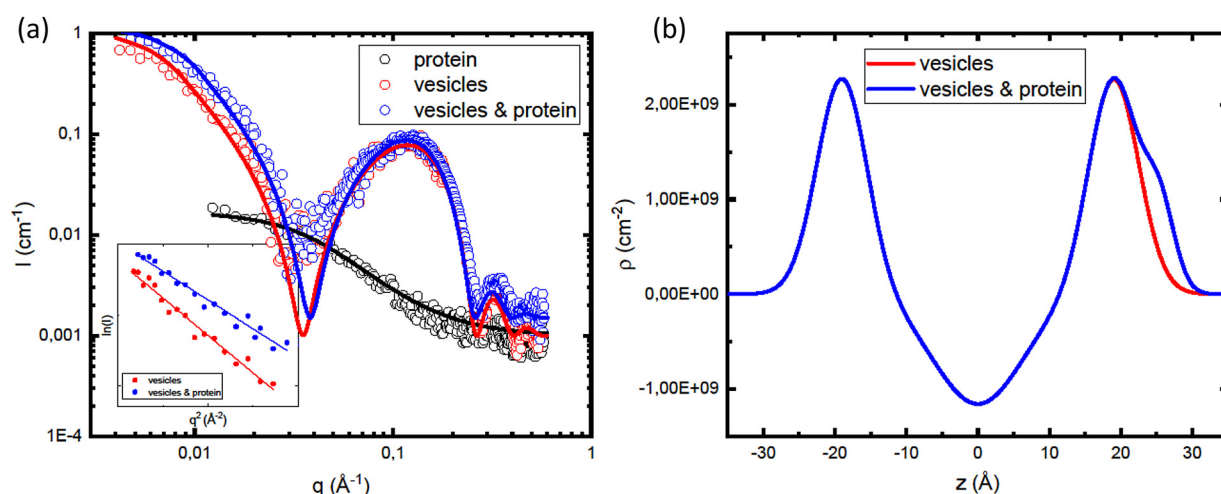


Fig. 5 (a) SAXS profiles of  $\alpha$ Syn monomers (black open circles), at  $c_P = 0.14 \text{ mM}$ , pure vesicle dispersion with  $\beta = 0.3$  (red open circles) at  $c_L = 42 \text{ mM}$  and sample containing vesicles and  $\alpha$ Syn monomers (blue open circles) at  $L/P = 300$ . The full lines are representing models fitted to the data: Debye model (black line) with  $I(0) = 0.02 \text{ cm}^{-1}$  and  $R_g = 4 \text{ nm}$ , and Pabst–Guinier–Porod model (red and blue lines). The inset shows Guinier fit yielding  $I(0) = 0.8 \text{ cm}^{-1}$  and  $R_g = 17.8 \text{ nm}$  in the case of vesicles (red), and for  $I(0) = 1.0 \text{ cm}^{-1}$  and  $R_g = 15.6 \text{ nm}$  in the case of sample containing protein and vesicles (blue line). (b) Electron density profile as a function of distance from the bilayer center,  $z$ .



into account strong electron density variation across the  $z$  direction of the bilayer (Fig. 5b), which is responsible for the appearance of the broad peak in the scattering profiles at  $q \approx 0.1 \text{ \AA}^{-1}$ . The advantage of this model is that the electron density profiles are described with Gaussian distributions, taking into account the diffuse scattering of bilayer. Separating the contribution of all three lipid regions (inner and outer head group and hydrocarbon regions), the bilayer form factor can be written as

$$F(q) = 2F_{\text{HG}} + F_{\text{T}} \quad (9)$$

where  $F_{\text{HG}}$  and  $F_{\text{T}}$  are form factors of the head group and hydrocarbon tail regions, respectively. Fixing the middle of the hydrocarbon region at  $z = 0$ , form factors are given by the following analytical expressions

$$F_{\text{HG}} = \sqrt{2\pi}\sigma_{\text{HG}}\Delta\rho_{\text{HG}}e^{-\frac{\sigma_{\text{HG}}^2q^2}{2}}\cos(qz_{\text{HG}}); \quad (10)$$

$$F_{\text{T}} = \sqrt{2\pi}\sigma_{\text{T}}\Delta\rho_{\text{T}}e^{-\frac{\sigma_{\text{T}}^2q^2}{2}} \quad (11)$$

Here  $z$  and  $\sigma$  denote the position and the standard deviation of the electron density distributions, respectively, and  $\Delta\rho$  the contrast between the lipid and the solvent. An additional profile, described by  $z_{\text{P}}$ ,  $\sigma_{\text{P}}$  and  $\Delta\rho_{\text{P}}$ , was included when modeling scattering from sample containing both vesicles and protein in order to account for the contribution of the adsorbed layer of  $\alpha\text{Syn}$  to the scattering profile.

To include contribution of the scattering of vesicles as whole, we combined the bilayer form factor (eqn (9)) with the Guinier–Porod model.<sup>71</sup> The Guinier–Porod model assumes that scattering profiles are composed of two regions: Guinier

region where  $q \leq \sqrt{\frac{3d}{2}}/R_{\text{g}}$  and Porod region where  $q \geq \sqrt{\frac{3d}{2}}/R_{\text{g}}$ ,  $d$  being the Porod exponent. The Porod exponent describes the roughness of the surface of the scattering particles, and  $d = 2$  for the 2-dimensional surface of the lipid vesicles. The scattering intensity in the Guinier ( $I_{\text{G}}$ ) and the Porod ( $I_{\text{P}}$ ) regions are given with the following expressions

$$I_{\text{G}} = Ge^{-\frac{q^2R_{\text{g}}^2}{3}}, \quad (12)$$

$$I_{\text{P}} = Dq^{-d} \quad (13)$$

where  $G$  is the Guinier scaling factor, or the forward intensity ( $I(q \rightarrow 0)$ ), and the  $D = Ge^{-\frac{d}{2}}\left(\frac{3d}{2}\right)^{\frac{d}{2}}R_{\text{g}}^{-d} = Ge^{-3}R_{\text{g}}^{-2}$  is the Porod scaling factor.

In Fig. 5b, we are showing the obtained electron density distribution. As expected, the head group region and  $\alpha\text{Syn}$  have higher electron density compared to water, unlike the hydrocarbon region with electron density lower than that of water. The fitting parameters used in the models shown in the Fig. 5a are summarized in Table 1.

Table 1 Parameters used to model SAXS data for  $\beta = 0.3$

| Fitting parameters                  | Values                                |
|-------------------------------------|---------------------------------------|
| $z_{\text{HG}}$                     | 19.0 $\text{\AA}$                     |
| $z_{\text{P}}$                      | 25.5 $\text{\AA}$                     |
| $\sigma_{\text{HG}}$                | 3.5 $\text{\AA}$                      |
| $\sigma_{\text{T}}$                 | 6.2 $\text{\AA}$                      |
| $\sigma_{\text{P}}$                 | 2.1 $\text{\AA}$                      |
| $\Delta\rho_{\text{HG}}$            | $2.0 \times 10^{10} \text{ cm}^{-2}$  |
| $\Delta\rho_{\text{T}}$             | $-1.8 \times 10^{10} \text{ cm}^{-2}$ |
| $\Delta\rho_{\text{P}}$             | $0.4 \times 10^{10} \text{ cm}^{-2}$  |
| $R_{\text{g}}$ vesicles alone       | 20.0 nm                               |
| $R_{\text{g}}$ vesicles and protein | 16.0 nm                               |

In the inset in Fig. 5a we are showing the Guinier plots, *id est*  $\ln I(q)$  vs.  $q^2$ , from which we are able to estimate  $R_{\text{g}}$  and  $I(0)$  directly. As was obtained from the model fitting,  $\alpha\text{Syn}$  adsorption leads to a decreases in  $R_{\text{g}}$  from 18 nm to 16. On the other hand, there is an increase of the forward scattering from  $0.8 \text{ cm}^{-1}$  to  $1.0 \text{ cm}^{-1}$  upon the addition of the protein.

For a particle system, the forward scattering intensity can be written as

$$I(0) = \frac{N}{V}\Delta\rho^2V_{\text{part}}^2, \quad (14)$$

where  $N/V$  is the number density of particles with volume  $V_{\text{part}}$ . For the pure lipid vesicles  $V_{\text{part}} = n_{\text{L}}v_{\text{L}}$ , where  $n_{\text{L}}$  is the number of lipid molecules,  $v_{\text{L}}$  is the average volume of the lipid molecules. We denote the vesicle scattered intensity as  $I_{\text{L}}(q)$ . We note in passing that  $V_{\text{part}}$  here is an average volume because of the vesicle size polydispersity.

In the presence of protein, a fraction,  $P_{\text{b}}$ , of  $\alpha\text{Syn}$  molecules adsorbs onto the vesicles. If this occurs at a constant number of vesicles,  $N/V$ , it changes the vesicle contribution to  $I(0)$  by a change in the average contrast, and by a small increase in  $V_{\text{part}}$ . When the protein is in excess,  $P_{\text{b}} < 1$ , every vesicle is covered by the maximum adsorbed amount of  $\alpha\text{Syn}$  molecules. Denoting the forward scattering  $I_{\text{LP}}(0)$  we write

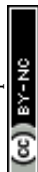
$$I_{\text{LP}}(0) = \frac{N}{V}\Delta\rho_{\text{av}}^2(n_{\text{L}}v_{\text{L}} + n_{\text{P}}v_{\text{P}})^2 + (1 - P_{\text{b}})\frac{\Delta\rho_{\text{P}}^2M_{\text{w}}}{d_{\text{p}}^2N_{\text{A}}}c_{\text{P}}. \quad (15)$$

Here  $n_{\text{P}}$  is the number of adsorbed protein molecules per vesicle, and  $v_{\text{P}}$  is the molecular volume of  $\alpha\text{Syn}$ . The average SLD,  $\rho_{\text{av}}$ , is the weighted average of lipid,  $\rho_{\text{L}}$ , and protein,  $\rho_{\text{P}}$ , SLDs. The averaged SLD difference we write as

$$\Delta\rho_{\text{av}} = (\phi_{\text{L}}\rho_{\text{L}} + P_{\text{b}}\phi_{\text{P}}\rho_{\text{P}})/(\phi_{\text{L}} + P_{\text{b}}\phi_{\text{P}}) - \rho_{\text{s}}. \quad (16)$$

Here,  $\phi_{\text{L}}$  and  $\phi_{\text{P}}$  are the volume fraction of lipid and protein, respectively.

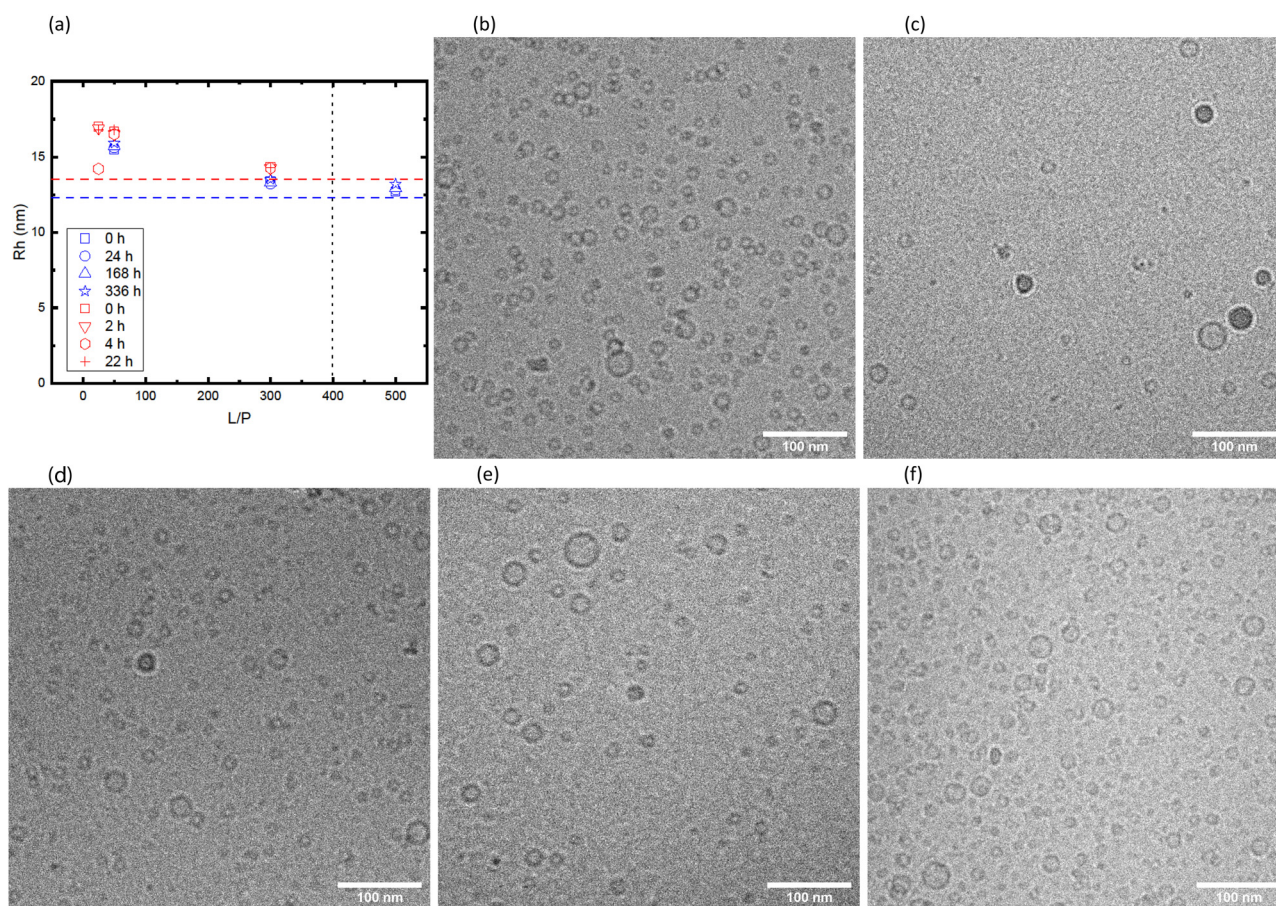
Assuming that for the corresponding solvent conditions and for  $\beta = 0.3$  all protein molecules are adsorbed with a long helical segment at  $L/P_{\text{sat}} = 400$  (Fig. 2b), we obtain the fraction of residues in helical conformation in the current case ( $L/P = 300$ ) to be  $P_{\text{b}} = 0.75$ . By simple geometrical analysis, we can estimate the maximum amount of the protein molecules that can be adsorbed onto vesicle. DLS measurements of vesicle suspensions yield the average vesicle radius of 24.6 nm, which allows for estimation of the average vesicle surface area of



$A_V = 7.6 \times 10^3 \text{ nm}^2$ . From the literature values for area per lipid HG of  $a_L = 0.65 \text{ nm}^2$ , we can estimate the amount of lipid molecules per vesicle to be  $2A_V/a_L = 2.3 \times 10^4$  ( $1.17 \times 10^4$  lipid molecules per outer layer). Knowing that 400 lipid molecules bind 1  $\alpha$ Syn molecule, we can estimate the maximum amount of  $\alpha$ Syn molecules per vesicle adsorbed with a maximal helical segment to be  $n_p = 58$ . Furthermore, considering the length of a lipid molecule to be  $l_L = 2 \text{ nm}$ ,<sup>72</sup> we can calculate the volume of a lipid molecule  $v_L = a_L \times l_L = 1.3 \text{ nm}^3$  and the volume of a protein molecule can be calculated as  $v_p = M_w/(d_p \times N_A) = 17 \text{ nm}^3$ . The volume fractions can be calculated from molecular weight, mass concentration and mass density as  $\phi = (M_w c)/d$ . Finally, assuming lipid mass density of  $1 \text{ mg ml}^{-1}$  gives SLD equal to  $\rho_L = 9.42 \times 10^{10} \text{ cm}^{-2}$ . Inserting these values in eqn (14)–(16), we obtain the following values for the forward intensities:  $I_L = 0.26$  and  $I_{LP} = 0.46$ . The ratio of these intensities of 1.5 is in a good agreement with the experimental ratio of 1.8 obtained for low- $q$  data, as is the difference of  $\Delta I = 0.2 \text{ cm}^{-1}$ .

The vesicles with adsorbed  $\alpha$ Syn are kinetically stable. This is seen from Fig. 6 where we have plotted the hydrodynamic radii obtained from DLS as function of time, for samples with

different L/P and  $\beta = 0.3$ . The data shown in the figure are coming from two different sample preparation and were measured with two different instruments. The horizontal dashed lines are illustrating the size of vesicles without adsorbed  $\alpha$ Syn for each of the cases, and the vertical line illustrates the saturation point for the given  $\beta$ . We can see from the Fig. 6a that there is essentially no variation with time during the 14 days timescale. It can also be observed that the apparent size of vesicles is biggest at intermediate L/P. As has been proposed earlier,<sup>1,30</sup> at L/P lower than  $L/P_{\text{sat}}$ ,  $\alpha$ Syn adsorbs only with a small segment (*ca.* 20 amino acids) and the rest of the protein is extending from the vesicle surface as a random coil, leading to increase in the vesicles' hydrodynamic radius. The increase of  $\approx 3 \text{ nm}$  at intermediate L/P is in good agreement with what is expected for *ca.* 120-amino-acid-long protein (the radius of gyration for the whole protein is estimated to be  $4 \text{ nm}$  as shown in Fig. 5a), and the increase of  $1 \text{ nm}$  around the saturation point can be explained by 40 amino acid residues at the C-terminus that extend as the random coil. It is also important to note that fibril formation did not occur under these conditions, as demonstrated in Fig. S1 (ESI†), where we are showing CD spectra obtained at different time points.



**Fig. 6** (a) Hydrodynamic radii from two different sample preparations, measured with 3D LS Spectrometer (blue) and Zetasizer Nano ZS (red) vs. L/P for different time points and  $\beta = 0.3$ . The dashed lines represent hydrodynamic radius of pure vesicle solutions, and the vertical dashed line illustrates the saturation point. (b)–(f) Cryo-TEM images of pure  $\beta = 0.3$  vesicle dispersion (b) and vesicles in the presence of  $\alpha$ Syn at L/P 2.5 (c), 25 (d), 50 (e), 300 (f). The images are cropped areas of  $500 \text{ nm} \times 500 \text{ nm}$  from selected cryo-TEM micrographs.



The samples shown in red in Fig. 6a were also imaged with cryo-TEM (rest of Fig. 6). The samples were vitrified  $\approx 15$  min after sample preparation. The observed size distributions are consistent with the DLS results. We also note that the vesicle shapes remain spherical after adsorption of  $\alpha$ Syn. Significant deformations in the shape of vesicles after adsorption of  $\alpha$ Syn have recently been observed with small unilamellar vesicles composed of DOPC/DOPS.<sup>19</sup> The vesicles in the present system are in fact very small which might explain their stronger resistance to deformation.

## 4 Fibril formation induces vesicle fusion

Having established that vesicles are kinetically stable also with adsorbed  $\alpha$ Syn monomers, we now turn to the fate of the lipid vesicles after the formation of  $\alpha$ Syn fibrils has occurred in their presence. We have recently shown, using small angle X-ray scattering (SAXS), that POPC/POPS vesicles in the presence of  $\alpha$ Syn retained locally their bilayer membrane structure also after the protein has formed fibrils.<sup>3</sup> However the SAXS pattern was at lower  $q$ -values dominated by fibril scattering and it was not possible to investigate any potential membrane remodeling. Here, we have therefore turned to neutron scattering and contrast variation, SANS. SANS experiments were performed using deuterated  $\alpha$ Syn and protonated lipids in  $D_2O$  buffer. The deuterated  $\alpha$ Syn is almost completely contrast matched to the solvent, with a negligible contribution to the scattering pattern.

The vesicle dispersion was tip-sonicated to produce small unilamellar vesicles, yielding a  $z$ -averaged mean radius of  $\langle R \rangle_z = 24.8 \pm 0.3$  nm, as measured by DLS. The fibril formation of 280  $\mu$ M monomeric  $\alpha$ Syn in the presence of vesicles ( $c_L = 2.1$  mM,  $\beta = 0.3$ ) was initiated by adding 14  $\mu$ M fibril seeds. The samples were then incubated for 14 days at 37  $^{\circ}$ C in a pH 7.0 buffer.

Table 2 Parameters used to model SANS data for  $\beta = 0.3$

| Fitting parameters         | Values                                |
|----------------------------|---------------------------------------|
| $z_{HG}$                   | 19.0 $\text{\AA}$                     |
| $\sigma_{HG}$              | 3.5 $\text{\AA}$                      |
| $\sigma_T$                 | 6.2 $\text{\AA}$                      |
| $\Delta\rho_{HG}$          | $3.9 \times 10^{10} \text{ cm}^{-2}$  |
| $\Delta\rho_T$             | $-6.8 \times 10^{10} \text{ cm}^{-2}$ |
| $R_g$ vesicles alone       | 22.0 nm                               |
| $R_g$ vesicles and protein | 44.0 nm                               |

Fig. 7a compares the scattering profiles of the pure vesicle dispersion and vesicles in the presence of  $\alpha$ Syn fibrils. As can be seen, the two scattering patterns essentially overlap for  $q > 0.01 \text{ \AA}^{-1}$ . However, they deviate in the low  $q$  regime. Here, the scattering intensity is significantly higher in the sample with fibrils, demonstrating that the vesicles are larger after fibril formation had taken place in their presence. The data were fitted using the same model that was used to analyze the SAXS data (eqn (9)–(13)). The neutron scattering densities used in the model<sup>73</sup> are presented in Table 2. The best fits are shown as solid lines. For the vesicles alone, we obtain an average radius of 22 nm, while in the sample fibrils the average radius had increased to twice the size, approximately 44 nm.

The twofold increase in vesicle size was confirmed by cryo-TEM. A representative image is shown in Fig. 7b, where we observe that  $\alpha$ Syn fibrils coexist with lipid vesicles with radii in the range 20–40 nm. The representative image of a pure vesicle dispersion is shown in ESI† (Fig. S3g). From the histogram constructed by analysis of 388 vesicles in the presence of fibrils at pH = 7.0, shown in Fig. 7c, we find average size of vesicle radius to be  $\approx 23$  nm, while that of vesicles without adsorbed protein is  $\approx 11$  nm (see ESI†). Since we have shown that the initial small vesicles are kinetically stable over time (Fig. 6), the results indicate that a small finite number of fusion events have occurred during the process of fibril formation. The twofold increase observed by SANS and cryo-TEM in the radius

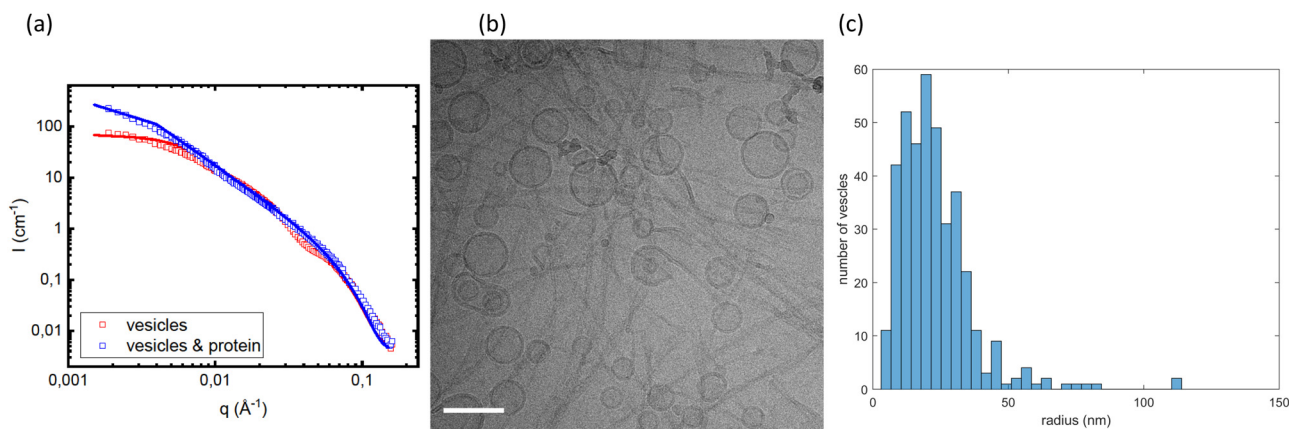


Fig. 7 (a) Comparison of SANS profiles of pure vesicle dispersion (open red squares) at  $c_L = 2.1$  mM and vesicles in the presence of fibrils (open blue squares) at  $c_p = 280 \mu$ M ( $L/P = 7.5$ ) and pH = 7.0 measured at 20  $^{\circ}$ C. The Pabst–Guinier–Porod model are represented with solid lines: red corresponding to  $R_g = 22$  nm and blue to  $R_g = 44$  nm. Cryo-TEM image of vesicles in the presence of fibrils at pH = 7.0 and (b) and size distribution of vesicles diameter obtained from cryo-TEM images by analyzing 388 vesicles (c). The scale bar corresponds to 100 nm.



corresponds to a four-fold increase of the bilayer area per vesicle, and hence three fusion events occurred during fibril formation.

The same SANS and cryo-TEM experiments were repeated at three different pH values, pH = 6.0, 6.5 and 7.4, respectively, with essentially identical results. The results from these experiments are presented in ESI†, Fig. S2 and S3. In Fig. S2 (ESI†), the SANS patterns are also compared with a calculated scattering pattern from deuterated  $\alpha$ Syn fibrils, confirming that the deuterated  $\alpha$ Syn fibrils do not contribute significantly to the SANS patterns.

## 5 Conclusions

We have investigated the interactions of  $\alpha$ Syn with POPC/POPS small unilamellar lipid vesicles at pH = 7.0. As has been reported frequently in the literature,<sup>23–28</sup>  $\alpha$ Syn monomers readily adsorb onto anionic lipid vesicles, and this was also observed here. The adsorbed amount increased with increasing fraction of the negatively charged POPS in the membrane, but with a tendency to level off at highest POPS fraction investigated.

A comparison with similar studies<sup>23,27</sup> conducted at lower pH values (5.5 and 5.0) offers new insights into the electrostatic interactions between  $\alpha$ Syn and lipid vesicles, clarifying the mechanisms that govern the adsorption process. This further extends our understanding of how factors such as vesicle charge, pH, and ionic strength influence protein adsorption. We show that the saturation point is pH dependent, as demonstrated in Fig. 3b, where we show that  $\sigma$  saturates for lower  $\beta$  values at pH = 5.5 compared to pH = 7.0. This correlates with the up-shift of the carboxyl group  $pK_a$  value with increasing charge density of the membrane, resulting in that the membrane charge density approaches a plateau at higher POPS fractions. Additionally, the adsorbed amount is shown to be strongly pH dependent, decreasing with increasing pH, even though the membrane charge density increases with increasing pH. We ascribe this to the increased protonation of the proteins acidic residues. Lowering the pH from 7.0 to 5.0 makes the N-terminus increasingly positively charged, thus increasing its electrostatic attraction to negatively charged surfaces. Furthermore, it makes the C-terminus less negatively charged decreasing the lateral protein–protein repulsion in the adsorbed state.

Moreover, we show that small POPC/POPS vesicles, with size similar to those of synaptic vesicles, are found to be kinetically stable over the course of 14 days, both with and without adsorbed monomeric  $\alpha$ Syn. However, when fibril formation, here induced by the addition of small amounts of preformed fibril seed, occurs in their presence, the vesicle size increases by approximately a factor of two. While it remains unclear exactly when this thermodynamic drive for fusion arises, it is certain that a small number of fusion events occurred during fibril formation.

## Author contributions

MD, ES, SL and UO designed research; MD performed SANS experiments with help of VL and YL; MH and JMD produced the

deuterated protein; MD analysed data; MD wrote the paper with input from all other co-authors.

## Data availability

Data for this article are now available at [https://docs.google.com/spreadsheets/d/19nbgLK\\_HnAgfCpWh-8iA49P1qGpIqj\\_N/edit?usp=drive\\_link&ouid=109662728783235682590rtopf=truesd=true](https://docs.google.com/spreadsheets/d/19nbgLK_HnAgfCpWh-8iA49P1qGpIqj_N/edit?usp=drive_link&ouid=109662728783235682590rtopf=truesd=true).

## Conflicts of interest

There are no conflicts to declare.

## Acknowledgements

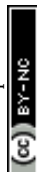
This work was supported by Swedish Foundation for Strategic Research through the national Graduate School SwedNessESS (GSn15-0008), the Swedish Research Council VR (SL 2015-00143) and the Knut and Alice Wallenberg Foundation grant (ES, SL, UO 2016.0074). We would like to acknowledge the work of Anna Carnerup and Crispin Hetherington who performed cryo-TEM experiments, and Katja Bernfur for the help with mass spectrometry. Certain commercial equipment, instruments, or software are identified in this paper to foster understanding. Such identification does not imply recommendation or endorsement by the National Institute of Standards and Technology, nor does it imply that the materials or equipment identified are necessarily the best available for the purpose.

## References

- 1 G. Fusco, A. D. Simone, T. Gopinath, V. Vostrikov, M. Vendruscolo, C. M. Dobson and G. Veglia, *Nat. Commun.*, 2014, **5**, 3827.
- 2 E. Hellstrand, M. Grey, M. L. Ainalem, J. Ankner, V. T. Forsyth, G. Fragneto, M. Haertlein, M. T. Dauvergne, H. Nilsson, P. Brundin, S. Linse, T. Nylander and E. Sparr, *ACS Chem. Neurosci.*, 2013, **4**, 1339–1351.
- 3 M. Dubackic, S. Linse, E. Sparr and U. Olsson, *Front. Soft. Matter*, 2022, **1**, 741996.
- 4 Y. Li, C. Zhao, F. Luo, Z. Liu, X. Gui, Z. Luo, X. Zhang, D. Li, C. Liu and X. Li, *Cell Res.*, 2018, **28**, 897–903.
- 5 M. H. Polymeropoulos, C. Lavedan, E. Leroy, S. E. Ide, A. Dehejia, A. Dutra, B. Pike, H. Root, J. Rubenstein, R. Boyer, E. S. Stenroos, S. Chandrasekharappa, A. Athanassiadou, T. Papapetropoulos, W. G. Johnson, A. M. Lazzarini, R. C. Duvoisin, G. D. Iorio, L. I. Golbe and R. L. Nussbaum, *Science*, 1997, **276**, 2045–2047.
- 6 M. G. Spillantini, M. L. Schmidt, V. M. Y. Lee, J. Q. Trojanowski, R. Jakes and M. Goedert, *Nature*, 1997, **388**, 839–840.
- 7 M. G. Spillantini, M. L. Schmidt, V. M. Y. Lee, J. Q. Trojanowski, R. Jakes and M. Goedert, *Proc. Natl. Acad. Sci. U. S. A.*, 1998, **95**, 6469–6473.



- 8 F. N. Emamzadeh, *J. Res. Med. Sci.*, 2016, **21**, 29.
- 9 Y. Zarbiv, D. Simhi-Haham, E. Israeli, S. A. Elhadi, J. Grigoletto and R. Sharon, *Neurobiol. Dis.*, 2015, **70**, 90–98.
- 10 K. Ueda, H. Fukushima, E. Masliah, Y. Xia, A. Iwai, M. Yoshimoto, D. A. Otero, J. Kondo, Y. Ihara and T. Saitoh, *Proc. Natl. Acad. Sci. U. S. A.*, 1993, **90**, 11282–11286.
- 11 C. R. Bodner, C. M. Dobson and A. Bax, *J. Mol. Biol.*, 2009, **390**, 775–790.
- 12 J. Burre, *J. Parkinson's Dis.*, 2015, **5**, 699–713.
- 13 M. Huang, B. Wang, X. Li, C. Fu, C. Wang and X. Kang, *Front. Neurosci.*, 2019, **13**, 28.
- 14 J. Varkey, J. M. Isas, N. Mizuno, M. B. Jensen, V. K. Bhatia, C. C. Jao, J. Petrova, J. C. Voss, D. G. Stamou, A. C. Steven and R. Langen, *J. Biol. Chem.*, 2010, **285**, 32486–32493.
- 15 A. Adamczyk, M. Kacprzak and A. Kazmierczak, *Folia Neuropathol.*, 2007, **45**, 230–235.
- 16 J. Madine, A. J. Doig and A. D. Middleton, *Biochemistry*, 2006, **45**, 5783–5792.
- 17 R. Khounlo, B. J. D. Hawk, T.-M. Khu, G. Yoo, N. K. Lee, J. Pierson and Y.-K. Shin, *Front. Cell Dev. Biol.*, 2021, **9**, 663431.
- 18 R. K. Nellikkaa, B. R. Bhaskara, K. Sanghrajkaa, S. S. Patila and D. Das, *Proc. Natl. Acad. Sci. U. S. A.*, 2021, **118**, e2021742118.
- 19 K. Makasewicz, S. Wennmalm, S. Linse and E. Sparr, *QRB Discovery*, 2022, **e10**, 1–9.
- 20 S. Fanning, D. Selkoe and U. Dettmer, *npj Parkinson's Dis.*, 2020, **6**, 3.
- 21 H. A. Lashuel, *Neurobiol. Dis.*, 2020, **141**, 104876.
- 22 K. Makasewicz, S. Wennmalm, B. Stenqvist, M. Fornasier, A. Andersson, P. Jönsson, S. Linse and E. Sparr, *ACS Chem. Neurosci.*, 2021, **12**, 2099–2109.
- 23 A. Andersson, S. Linse, E. Sparr, M. Fornasier and P. Jonsson, *Biophys. Chem.*, 2024, **305**, 107143.
- 24 M. Stockl, P. Fischer, E. Wanker and A. Herrmann, *J. Mol. Biol.*, 2008, **375**, 1394–1404.
- 25 V. V. Shvadchak, L. J. Falomir-Lockhart, D. A. Yushchenko and T. M. Jovin, *J. Biol. Chem.*, 2008, **286**, 13023–13032.
- 26 Z. Jiang, S. K. Hess, F. Heinrich and J. C. Lee, *J. Phys. Chem. B*, 2015, **119**, 4812–4823.
- 27 E. R. Middleton and E. Rhoades, *Biophys. J.*, 2010, **99**, 2279–2288.
- 28 S. B. Lokappa and T. S. Ulmer, *J. Biol. Chem.*, 2011, **286**, 21450–21457.
- 29 C. Pfefferkorn, F. Heinrich, A. J. Sodt, A. Maltsev, R. Pastor and J. Lee, *Biophys. J.*, 2012, **102**, 613–621.
- 30 C. C. Jao, A. Der-Sarkissian, J. Chen and R. Langen, *Proc. Natl. Acad. Sci. U. S. A.*, 2004, **101**, 8331–8336.
- 31 B. Nuscher, F. Kamp, T. Mehnert, S. Odoy, C. Haass, P. J. Kahle and K. Beyer, *JBC*, 2004, **279**, 21966–21975.
- 32 F. Kamp and K. Beyer, *JBC*, 2006, **281**, 9251–9259.
- 33 T. S. Ulmer, A. Bax, N. B. Cole and R. L. Nussbaum, *J. Biol. Chem.*, 2005, **280**, 9595–9603.
- 34 K. Makasewicz, G. Carlström, O. Stenström, K. Bernfur, S. Fridolf, M. Akke, S. Linse and E. Sparr, *Cell Rep. Phys. Sci.*, 2024, 102309.
- 35 E. Jo, J. McLaurin, C. M. Yip, P. S. George-Hyslop and P. E. Fraser, *J. Biol. Chem.*, 2000, **275**, 34328–34334.
- 36 E. Rhoades, T. F. Ramlall, W. W. Webb and D. Eliezer, *Biophys. J.*, 2006, **90**, 4692–4700.
- 37 C. Galvagnion, A. K. Buell, G. Meisl, T. C. T. Michaels, M. Vendruscolo, T. P. J. Knowles and C. M. Dobson, *Nat. Chem. Biol.*, 2015, **11**, 229–234.
- 38 C. Galvagnion, *J. Parkinson's Dis.*, 2017, **7**, 433–450.
- 39 M. Grey, C. J. Dunning, R. Gaspar, C. Grey, P. B. E. Sparr and S. Linse, *J. Biol. Chem.*, 2015, **11**, 2969–2982.
- 40 R. Gaspar, J. Pallbo, U. Weininger, S. Linse and E. Sparr, *Biochim. Biophys. Acta, Proteins Proteomics*, 2019, **1866**, 1062–1072.
- 41 E. Hellstrand, A. Nowacka, D. Topgaard, S. Linse and E. Sparr, *PLoS One*, 2013, **8**, e77235.
- 42 A. van Maarschalkerweerd, V. Vetri, A. E. Langkilde, V. Fodera and B. Vestergaard, *Biomacromolecules*, 2014, **15**, 3643–3654.
- 43 N. P. Reynolds, A. Soragni, M. Rabe, D. Verdes, E. Liverani, S. Handschin, R. Riek and S. Seeger, *J. Am. Chem. Soc.*, 2011, **133**, 19366–19375.
- 44 C. Galvagnion, D. Topgaard, K. Makasewicz, A. K. Buell, S. Linse, E. Sparr and C. M. Dobson, *J. Phys. Chem. Lett.*, 2019, **10**, 7872–7877.
- 45 R. Gaspar, I. Idini, G. Carlström, S. Linse and E. Sparr, *Front. Cell Dev. Biol.*, 2021, **9**, 266.
- 46 Z. Shi, J. N. Sachs, E. Rhoades and T. Baumgart, *Phys. Chem. Chem. Phys.*, 2015, **17**, 15561–15568.
- 47 A. West, B. E. Brummel, A. R. Braun, E. Rhoades and J. N. Sachs, *Biochim. Biophys. Acta, Biomembr.*, 2016, **1858**, 1594–1609.
- 48 T. Schikorski and C. F. Stevens, *J. Neurosci.*, 1997, **17**, 5858–5867.
- 49 M. Grey, S. Linse, H. Nilsson, P. Brundin and E. Sparr, *J. Parkinson's Dis.*, 2011, **1**, 359–371.
- 50 M. Haertlein, M. Moulin, J. Devos, V. Laux, O. Dunne and V. Forsyth, *Methods Enzymol.*, 2016, **566**, 113–157.
- 51 D. E. Koppel, *J. Chem. Phys.*, 1972, **57**, 4814–4820.
- 52 C. J. Glinka, J. G. Barker, B. Hammouda, S. Krueger, J. J. Moyert and W. J. Orts, *J. Appl. Crystallogr.*, 1998, **31**, 430–445.
- 53 S. R. Kline, *J. Appl. Crystallogr.*, 2006, **39**, 895–900.
- 54 T. Engel, G. Drobny and P. Reid, *Physical Chemistry for the Life Sciences*, Pearson Education, Upper Saddle River NJ, 2008.
- 55 M. Dubackic, PhD thesis, Lund University, Lund, Sweden, 2021.
- 56 R. Gaspar, J. Pallbo, U. Weininger, S. Linse and E. Sparr, *Biochim. Biophys. Acta, Proteins Proteomics*, 2018, **1866**, 1062–1072.
- 57 F. C. Tsui, D. M. Ojcius and W. L. Hubbell, *Biophys. J.*, 1986, **49**, 459–468.
- 58 T. Kesvatera, B. Jönsson, E. Thulin and S. Linse, *Proteins*, 2001, **45**, 129–135.
- 59 T. Pálmadóttir, A. Malmendal, T. Leiding, M. Lund and S. Linse, *J. Am. Chem. Soc.*, 2021, **143**, 7777–7791.
- 60 D. F. Evans and H. Wennerström, *The Colloidal Domain: Where Physics, Chemistry, Biology, and Technology Meet*, Wiley, 2nd edn, 1999.



- 61 N. Kucerka, M.-P. Nieh and J. Katsaras, *Biochim. Biophys. Acta, Biomembr.*, 2011, **1808**, 2761–2771.
- 62 R. L. Croke, S. M. Patil, J. Quevreaux, D. A. Kendall and A. T. Alexandrescu, *Protein Sci.*, 2011, **20**, 256–269.
- 63 B. Pogostin, S. Linse and U. Olsson, *Langmuir*, 2019, **35**, 16536–16544.
- 64 A. K. Buell, C. Galvagnion, R. Gaspar, E. Sparr, M. Vendruscolo, T. P. J. Knowles, S. Linse and C. M. Dobson, *Proc. Natl. Acad. Sci. U. S. A.*, 2014, **111**, 7671–7676.
- 65 S. J. Roeters, K. Strunge, K. B. Pedersen, T. W. Golbek, M. Bregnhøj, Y. Zhang, Y. Wang, M. Dong, J. Nielsen, D. E. Otzen, B. Schiøtt and T. Weidner, *Nat. Commun.*, 2023, **14**, 5731.
- 66 N. Sreerama and R. W. Woody, *Methods Enzymol.*, 2004, **383**, 318–351.
- 67 N. J. Greenfield and G. D. Fasman, *Biochemistry*, 1969, **8**, 4108–4116.
- 68 J. E. Nielsen, V. R. Koynarev and R. Lund, *COCIS*, 2023, **66**, 101709.
- 69 P. Debye, *J. Phys. Colloid Chem.*, 1947, **51**, 18–32.
- 70 G. Pabst, M. Rappolt, H. Amenitsch and P. Laggner, *Phys. Rev. E*, 2000, **62**, 4000–4009.
- 71 B. Hammouda, *J. Appl. Crystallogr.*, 2010, **43**, 716–719.
- 72 P. Jurkiewicz, L. Cwiklik, A. Vojtiskova, P. Jungwirth and M. Hof, *Biochim. Biophys. Acta*, 2012, **1818**, 609–616.
- 73 W. T. Heller, *Biomolecules*, 2022, **12**, 1591.

