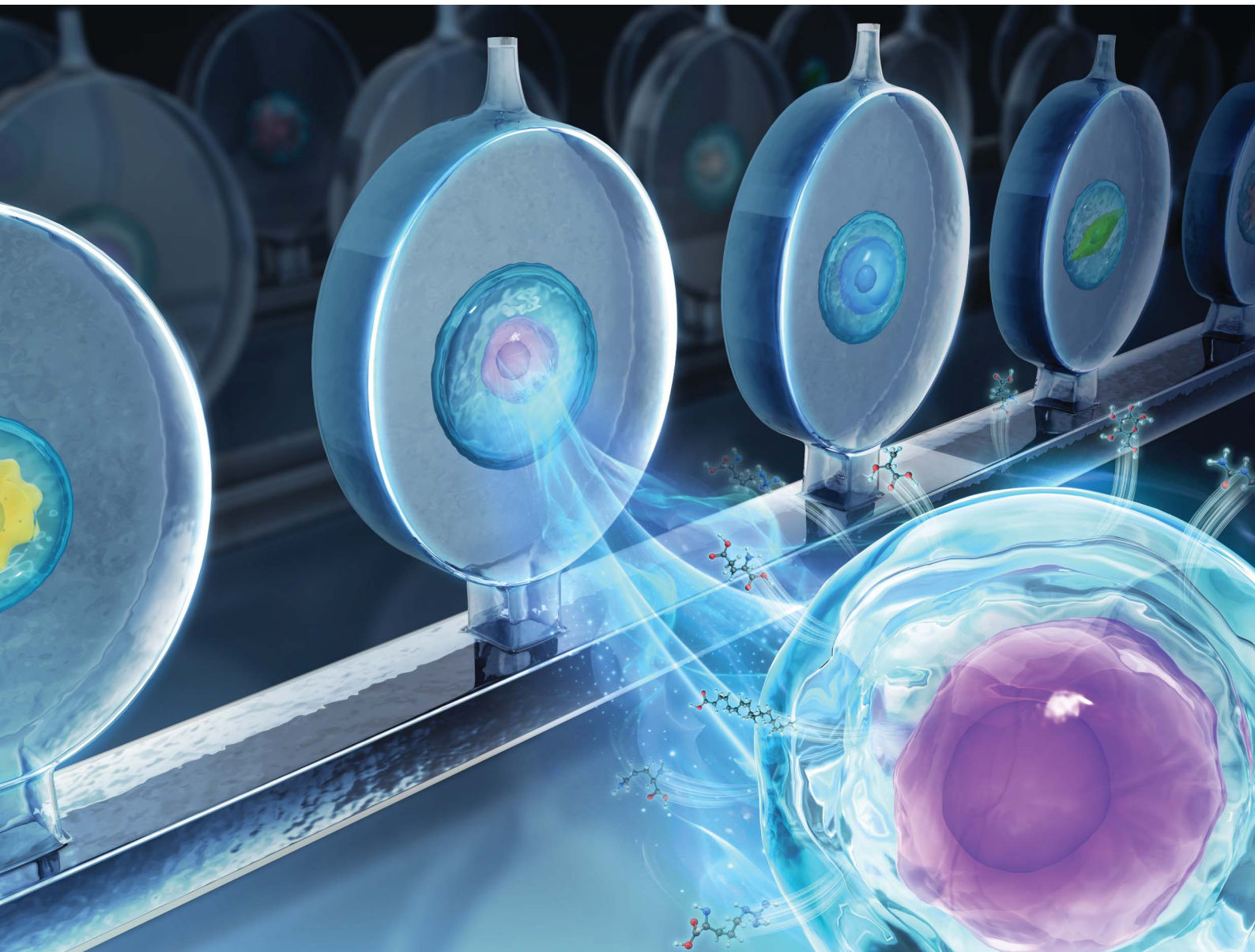


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Single-cell metabolic accumulation analysis by microfluidic hydrogel microspheres combined with mass spectrometry

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Metabolic analysis of tumor cells is crucial for understanding tumor metabolic reprogramming, and single-cell metabolic accumulation studies provide precise insights into tumor biology. In this work, we established a microfluidic assay for single-cell metabolic accumulation analysis by combining droplet-generated hydrogel microspheres for single-cell encapsulation with a microchamber culture chip for microsphere isolation and 3D cultivation. This system enables efficient accumulation of secreted metabolites from individual cells for downstream analysis. Coupled with mass spectrometry, this system revealed metabolic accumulation heterogeneity among individual cells of the same tumor type. Moreover, metabolic profiling of different tumor types, including A549, HepG2, and HCT116, demonstrated distinct metabolic patterns, enabling cell classification based on accumulation differences. The method supports high-throughput, multiplexed, and dynamic metabolic analysis in a 3D single-cell context, offering a scalable strategy for decoding tumor heterogeneity with potential application in cell-state characterization and advancing oncology research.

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Introduction

Cancer is a complex genetic disorder characterized by the uncontrolled growth of abnormal cells, primarily driven by intricate genomic alterations involving mutations in oncogenes and tumor suppressor genes.¹ These genetic mutations instigate metabolic reprogramming in cancer cells, leading to distinct metabolic pathways compared to normal cells.² A well-known phenomenon in this context is the “Warburg effect”,³ wherein tumor cells, even in the presence of sufficient oxygen, prominently convert a substantial amount of glucose into lactate. Metabolic reprogramming is a pivotal process that governs the survival, metastasis, and resistance activities of cancer cells.^{4–6} Understanding these intricate processes not only contributes to a comprehensive comprehension of cancer cells but also provides a crucial avenue for therapeutic interventions.

Investigating the metabolism of tumor cells provides a direct avenue for understanding tumor reprogramming. However, the predominant approach in studying human tumor metabolism

involves collective measurements obtained from bulk tumors. Nevertheless, heterogeneity arises within the same tumor mass due to diverse external microenvironments at different locations and hierarchical levels. As a result, each tumor cell may exhibit unique metabolic states.^{7,8} Thus, it is crucial to examine tumor cell metabolism at the single-cell level.

Methods for studying single-cell metabolism typically involve the initial isolation of individual cells. Researchers have developed various techniques for single-cell isolation, including laser capture microdissection,^{9,10} flow cytometry,^{11,12} microfluidic chips,^{13–15} and others.^{16,17} Among these, microfluidics-based single-cell analysis for various applications, including single-cell proteomics,¹⁸ transcriptomics,¹⁹ metabolomics,²⁰ lipidomics,²¹ multiomics²² and post-translational modifications.²³ And droplet microfluidic methods, due to their integration of the high operability and the throughput advantages of flow cytometry, have found widespread applications in single-cell genomics,^{24,25} transcriptomics,^{26,27} proteomics,^{28,29} and other fields. They also hold significant potential for single-cell metabolomics research.³⁰ In particular, the recent development of microfluidic hydrogel microspheres has emerged as a valuable tool for constructing three-dimensional (3D) culture systems. Compared with traditional 2D culture systems, hydrogel microspheres with 3D porous structure can maintain cell morphology and activity for a long time and can conduct bidirectional interactions with the extracellular microenvironment. This advancement allows for better simulation of the 3D extracellular matrix environment surrounding cells.^{31–34}

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Approaches for single-cell metabolism analysis encompass Raman spectroscopy,³⁵ fluorescence spectroscopy,³⁶ mass spectrometry,^{37,38} and other detection methods. However, these techniques commonly provide information on the metabolic state of cells at particular time points rather than offering insights into metabolic accumulation.³⁹ The substances measured often constitute intracellular components rather than metabolites released by the cells. The cumulative measurement of metabolites from single cells over time could facilitate the quantification of single-cell metabolism, providing more comprehensive information than that obtained from analysis at specific time points.

Here, we present a microfluidic method for analyzing single-cell metabolic accumulation by integrating a droplet microfluidic device with a hydrogel microsphere manipulation chip (Fig. 1a). Single-cell encapsulated hydrogel microspheres were generated using droplet microfluidics and subsequently isolated on a dedicated single-microsphere culture chip. This system enables downstream mass spectrometry analysis of metabolites, allowing in-depth investigation of metabolic accumulation at the single-cell level. The duration of each operational step for single-cell analysis is illustrated in Fig. 1b. This microfluidic hydrogel assisted mass spectrometry method was applied to analyze the tumor cell metabolism in 3D culture, revealing heterogeneity in single-cell metabolic accumulation. Expanding upon previous studies,^{40–42} we applied our method to various tumor cell types, including A549, HepG2 and HCT116 (from National Infrastructure of Cell Line Resource, Beijing, China), and classified the cells based on distinct metabolic profiles. Our device supports multiplexed analysis of metabolites in individual cells, offering new insights into the dynamic metabolic states of single cells. This method holds significant promise for tumor analysis and stem cell research, highlighting the importance and versatility of our approach.

Results and discussion

Single-cell hydrogel microspheres generation by droplet microfluidics

It is crucial to examine tumor cell metabolism at the single-cell level because each tumor cell may exhibit unique metabolic states. The microfluidic hydrogel microspheres can maintain cell morphology and activity for a long time, realizing 3D cell culture.^{31,32} In addition, the 3D porous network structure of the hydrogel microspheres allows for the free diffusion of water molecules, ions, oxygen, and small molecule nutrients, without hindering the transport of cellular metabolites into the culture media.^{33,34} Therefore, we use microfluidic hydrogel microspheres to encapsulate single cells and investigate the metabolism of single cells. The hydrogel microspheres containing individual cells were generated using a droplet microfluidic chip (Fig. S1a and b), which was fabricated according to our previous work.^{43,44} To optimize encapsulation rates and achieve uniform cell distribution, we employed a pinched flow setup in a co-flow arrangement (left structure in Fig. 2a). Here, a cell-containing hydrogel (Inlet 1, 5, 10, 20 and 40 $\mu\text{L h}^{-1}$) was introduced, flanked by sheath flows of cell-free hydrogel solution (Inlet 2, 55, 50, 40 and 20 $\mu\text{L h}^{-1}$), creating a laminar flow that aligned single cells into a single column. At these relatively low flow rates, the shear stress exerted on cells is negligible.⁴⁵ The hydrogel in Inlet 1 and Inlet 2 was the mixture of sodium alginate and EDTA-Ca solution, acting as the dispersed phase for droplet generation. The sodium alginate, with the advantage of acid-triggered crosslinking properties, encapsulates cells into sodium alginate microcapsules that allow for free diffusion of metabolites and nutrients, simulating the extracellular matrix.^{46,47} The continuous phase, consisting of a fluorinated oil with surfactant (Inlet 3) and acetic acid (Inlet 4), enabled droplet detachment. The acetic acid can release calcium ions to complete alginate cross-linking. The hydrogel microspheres, whose size can be adjusted over a wide range, are suitable for

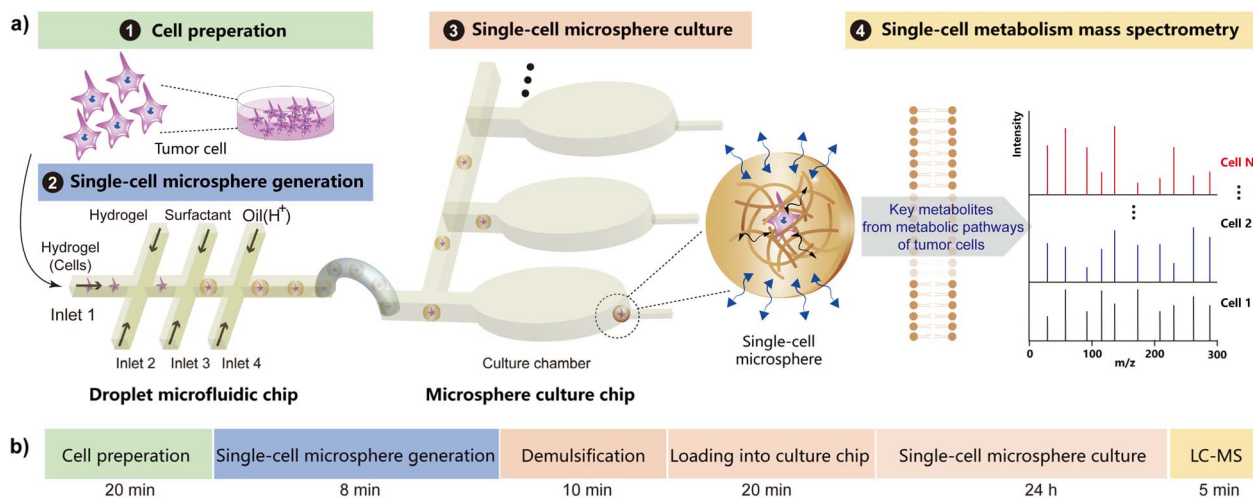


Fig. 1 Overview of single-cell metabolic accumulation analysis of microfluidic hydrogel microspheres. (a) Illustration of single-cell metabolic accumulation analysis of microfluidic hydrogel microspheres, including cell preparation, single-cell microsphere generation and culture, and single-cell metabolism spectrometry. (b) Timeline for each handling step.



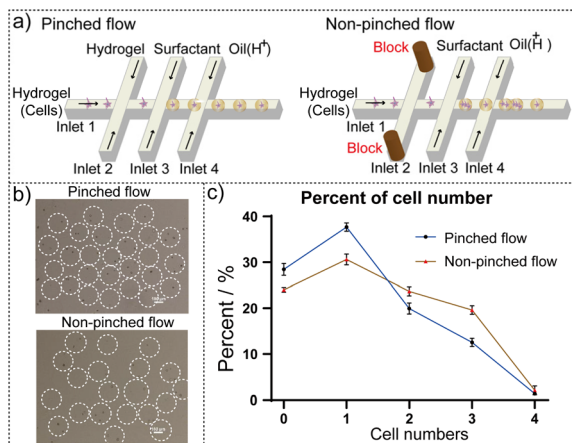


Fig. 2 Generation of single-cell hydrogel microspheres. (a) Illustration of the different types of pinched and non-pinched flow. (b) Micrograph of hydrogel microspheres generated by pinched and non-pinched flow (scale bar = 100 μm). (c) Proportion of the number of cells in hydrogel microspheres generated by pinched and non-pinched flow ($n = 3$, the number of microspheres was 100 for each experiment).

cell cultivation and facilitate the manipulation of cells for metabolic analysis using mass spectrometry methods,^{48,49} and their size can be adjusted over a wide range. The size of the hydrogel microspheres can be adjusted by modulating the continuous-to-dispersed phase flow rate ratio. By increasing the flow rate of the continuous phase from 200 to 400 $\mu\text{L h}^{-1}$ while maintaining a constant dispersed phase flow rate (from Fig. S1c–g). The smallest size (approximately 140 μm) was achieved at a flow rate of 350 $\mu\text{L h}^{-1}$. Beyond this flow rate, the uniformity of hydrogel microspheres began to decline (Fig. S1h). Therefore, we set the optimal continuous phase flow rate at 350 $\mu\text{L h}^{-1}$ to ensure consistent microsphere size and quality.

The pinched flow method of droplet generating, compared with direct cutting (right structure in Fig. 2a), minimized cell number dispersion and enhanced the rate of single-cell encapsulation in the microfluidic hydrogel microspheres. As shown in Fig. 2b, there are more single-cell microspheres generated by the pinched flow method when the flow rate ratio between the inner and outer phases was 1:2 at the same cell concentration (1×10^6). Lower cell concentrations made it easier to obtain single-cell microspheres (Fig. S2). The percentages of single-cell microspheres were calculated under a microscope at a cell concentration of 1×10^6 according to the two droplet generation methods. As shown in Fig. 2c, the pinched flow was better for single-cell encapsulation with higher single-cell encapsulation efficiency (approaching 40%). Furthermore, this structure allowed for precise control over cell encapsulation and the production of hydrogel microspheres containing different numbers of cells.

Single-cell microsphere cultivation in the culture chip

The single-microsphere culture chip was designed to isolate and culture single-cell microspheres (Fig. S3). Here, we

designed 7 chambers on the chip for representative cell analysis (Fig. 3a). Furthermore, the number of chambers can be expanded on a single chip or connecting multiple chips in series to increase the throughput (Fig. S4). When the culture medium containing the single-cell microspheres was injected into the culture chip channel, microspheres (approximately 140 μm in diameter) flowed smoothly through side channels (Fig. 3b) into the chambers. Notably, due to their size, these microspheres could not pass through the 50 μm high extraction channels, leading to their retention at the end of the chambers (Fig. 3c). This retention also sealed the channel to prevent the medium containing the single-cell microspheres from flowing into the current and subsequent chambers, achieving isolation of individual microspheres. Reducing microsphere concentration, decreasing the injection flow rate, and gently shaking the culture chip can prevent multiple microspheres from entering a single chamber. After all chambers were loaded, paraffin oil was introduced into the inlet channels to partition them. The entire process can be observed under the microscope (Fig. S5).

The loaded culture chip was then placed in a culture dish with PBS, creating a saturated vapor environment to prevent the evaporation of the aqueous phase inside the chambers, and incubated in a CO_2 incubator. After 24 h incubation, the cell viability was evaluated after live/dead staining of cells. The staining reagents (Calcein AM/PI) were injected into the culture chip and then permeated in the chamber within 20 min (Fig. S6). The cell viability was confirmed for both single-cell and multiple cells without cell division (Fig. 3d), demonstrating robust biological compatibility of our approach. In addition, the single-cell viability rate was statistically calculated to be over 95% (Fig. S7). By combining droplet microfluidics with microscopes, the single cells were accurately encapsulated and cultured in the culture chip, suitable for further studies on single-cell metabolic activity.

Mass spectrometry detection of single-cell metabolism

The proposed single-microsphere culture chip enables the accumulation of metabolites from individual cells in a controlled 1.5 μL chamber volume over 24 h, allowing these metabolites to concentrate for mass spectrometry analysis, which is more suitable compared with oil–water droplets for cell analysis with high cell activity. After 24 h of cultivation, the culture medium from each chamber was extracted and adjusted to 10 μL for subsequent mass spectrometry testing. All tests were conducted under the same conditions, ensuring that any potential metabolite adsorption or degradation would be consistent across samples. For metabolic profiling, all metabolites of cells can be determined by our method through establishing separate mass spectrometry detection methods for each metabolite. As a proof of concept, we selected 10 key metabolites from common tumor cell metabolic pathways, including glucose from glycolysis, glutamate and glutamine from amino acid metabolism, arginine, ornithine, and citrulline from guanidino metabolism, arachidonic acid from arachidonic acid metabolism, and stearic acid and palmitic acid from fatty acid metabolism.^{50,51} These key metabolites were



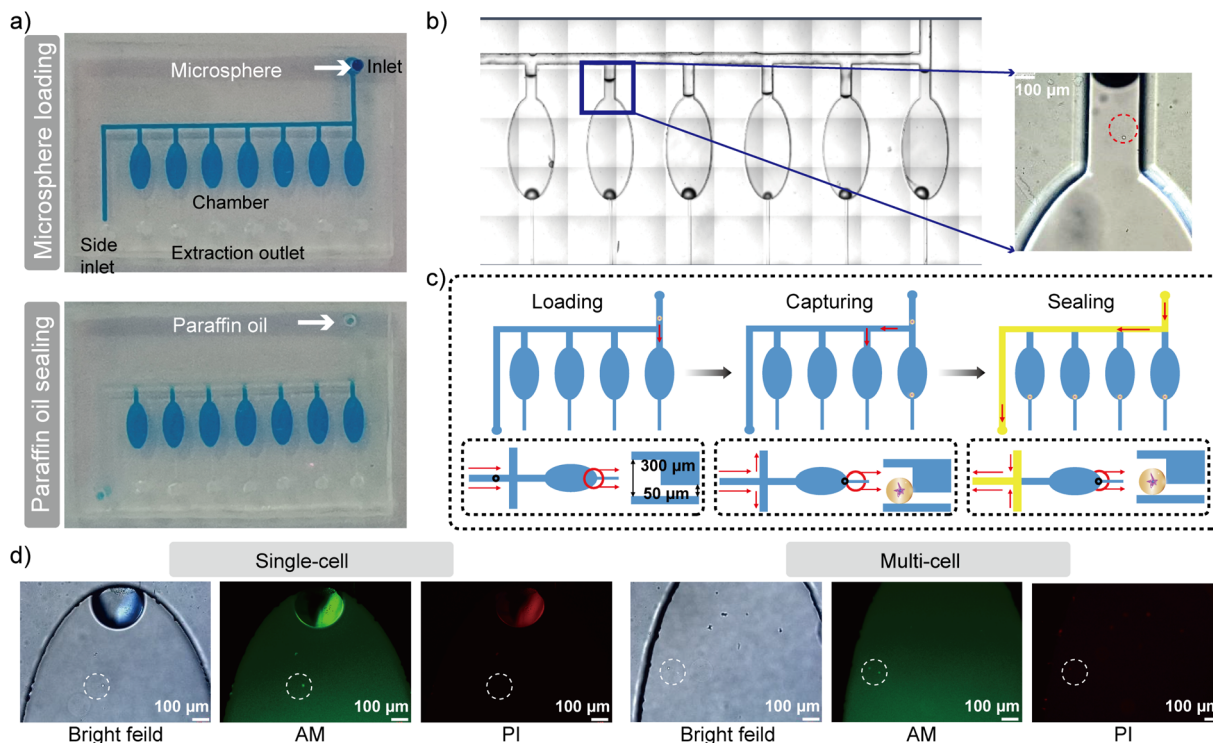


Fig. 3 Structure of single-microsphere culture chip and the activity of single and multiple cells therein. (a) Loading and culturing of single microspheres on the culture chip. (b) Micrograph of loading single microsphere into the culture chip. (c) Process of microspheres loading into the single-microsphere culture chip. (d) Activity of single and multiple cells in hydrogel microspheres after cultivation on the culture chip. (Scale bar = 100 μm).

selected, based on previous reports, from representative metabolic pathways of common tumor cells to validate our single-cell analysis method.^{50,51} Mass spectrometry methods for each metabolite were validated with pre-experimental checks confirming the feasibility of the assays (Fig. S8, S9 and Table S1). To this end, hydrogel microsphere concentrations in the Petri dish were controlled to match those within the chip chambers (one microsphere per 1.5 μL), and culture medium samples were collected at 0 h and 24 h (Fig. S10). Also, the arachidonic acid metabolism from single A549 cells cultured on the chip was analyzed (Fig. S11). Furthermore, the glutamic acid metabolism of microspheres encapsulating one or two A549 cells cultured on the chip was analyzed (Fig. S12). The 24 h variations in metabolite levels revealed detectable heterogeneity in single-cell metabolic activity.

Subsequently, metabolic accumulation analysis was conducted on individual A549 cells using our method, which revealed significant metabolic differences within the same cell line (Fig. 4). As shown in Fig. 4a, certain cells (cell 1 and cell 11) exhibited higher glutamate metabolism, while others showed increased fatty acid metabolism (cell 7 and cell 10). Additionally, some cells displayed substantial citrulline cycling (cell 15 and cell 22), while others demonstrated higher overall metabolic activity (cell 4) or generally lower activity (cell 14). These findings highlight the metabolic heterogeneity among single cells. Analysis of single-cell metabolic distribution revealed distinct patterns (Fig. 4b). Some metabolites, such as arginine,

ornithine, and citrulline, showed single-peaked distributions, indicating that most cells shared similar metabolic levels. Others, like arachidonic acid and lactate, displayed bimodal distributions, indicating heterogeneity across the cell population. These results illustrate the diversity in metabolic characteristics among individual cells, highlighting the significance of single-cell analysis in decoding the intricacies of cellular biology. This metabolic diversity forms a solid scientific foundation for forthcoming research on cellular states, functions, and potential applications in personalized medicine. Notably, the system enables repeated metabolite collections. Following an initial extraction, the chambers can be refilled with culture media or therapeutic compounds for subsequent treatment, thereby facilitating analysis of the real-time metabolic effects of treatments (Fig. S13).

Metabolic accumulation differences across different cell types

Single-cell variability in parameters like cell size, migration capacity, protein expression, and metabolic function is commonly used for cell sorting,⁵² including the isolating of circulating tumor cells.⁵³ While metabolic distinctions between normal and tumor cells have been well investigated,⁵⁴ research on metabolic differences among different tumor cell types often focuses on functional proteins and specific metabolites. Using our microfluidic hydrogel microspheres combined with mass spectrometry method, we analyzed single-cell metabolic



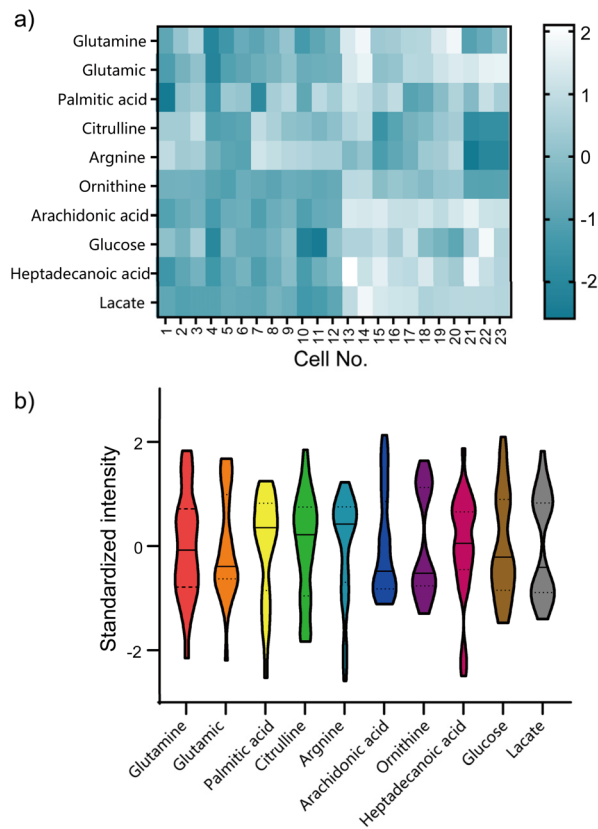


Fig. 4 Single-cell metabolic accumulation analysis of A549 in single-microsphere culture chip ($n = 23$). (a) Heatmap of metabolic accumulation differences between different A549 cells. (b) Heterogeneity of metabolic accumulation of A549 cells for different metabolites (dashed lines: quartiles; solid lines: the median) (the intensity of all MS peaks was processed by standardization by logarithmic transformation and normalization).

accumulation across several cancer cell types to probe the cellular heterogeneity in the following experiment.

The single-microsphere culture chip enabled single-cell metabolic accumulation studies across human lung cancer A549 cells, human colon cancer HCT116 cells, and human hepatocellular carcinoma HepG2 cells. Ten compounds were analyzed after logarithmic transformation and normalization, followed by Partial Least Squares-Discriminant Analysis (PLS-DA). The results showed that component I accounted for 37.5% and component II for 24.1%, suggesting distinct metabolic accumulation among the three tumor cell types (Fig. 5a). However, partial overlap of plots indicated that metabolic accumulation alone may not fully discriminate the cell types. The heatmap (Fig. S14) indicated that the metabolic accumulation alone partially discriminated the cell types. Importantly, further analysis of individual metabolites revealed distinct distributional features. For example, heptadecanoic acid accumulation in HepG2 cells displayed a unimodal profile, while A549 cells showed a bimodal distribution (Fig. 5b). Arginine accumulation showed cell type-dependent variation, with HepG2 cells exhibiting a wider distribution range (6.3–7.0) compared with the narrower range observed in HCT116 cells

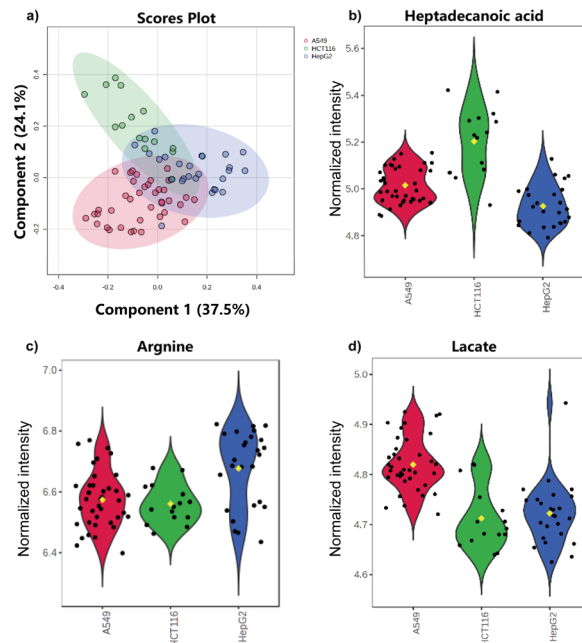


Fig. 5 Tryptophan metabolism results analyzed by LC-MS. (a) PLS-DA plot of metabolic accumulation differences between different cells in single microsphere culture microarrays. Differential metabolic accumulation plots of different cells in single microsphere culture microfluidic chips corresponding to (b) heptadecanoic acid, (c) arginine and (d) lactate (red: A549 ($n = 47$), green: HCT116 ($n = 41$), blue: HepG2 ($n = 35$)). The intensity of all MS peaks was processed by logarithmic transformation and normalization.

(6.4–6.8) (Fig. 5c). Lactate accumulation also differed in distributional shape, with HepG2 cells exhibiting a broader, multimodal distribution (Fig. 5d). Overall, while metabolic differences among various tumor cell types were observed, they were less pronounced than those between normal and tumor cells. These results emphasize that classifying tumor cells by common metabolite accumulation alone may require additional data for a more comprehensive analysis.

Conclusions

In conclusion, we developed an integrated system that combines droplet microfluidics with a cell culture chip to enable the generation, isolation, and subsequent collection of metabolic products, facilitating detailed metabolic accumulation analysis at the single-cell level. By using the proposed method, we reveal metabolic heterogeneity, providing insights into cellular metabolic processes and regulatory mechanisms. Through the analysis of multiple tumor cell types, our system not only uncovered metabolic diversity among individual tumor cells but also established a versatile experimental framework for studying metabolic distinctions across different tumor types. With the increasing more types of cellular metabolites analysis, this system is poised for advanced 3D single-cell metabolomic analysis across diverse cell types and may be extended to other single-cell omics applications, including those related to therapeutic research. Furthermore, this system can be used for



probing the interfering factors of cellular heterogeneity. When combined with microscopic imaging, it establishes the correlation between heterogeneity and key factors such as cell cycle or size. In future iterations, a cell screening module can be integrated into the droplet generation chip to improve the efficiency of single-cell encapsulation. Analytical throughput can also be expanded by increasing the number of culture chambers on a single chip or linking multiple chips in series. Moreover, incorporating microfluidic structures for real-time metabolite collection and continuous flow culture will enable dynamic monitoring of single-cell metabolic accumulation, providing a robust foundation for studying cellular dynamics and developing personalized medical strategies.

Author contributions

J.-M. L. obtained the funds, provided conceptualization and supervised the project. G. X. obtained the funds, designed, fabricated and characterized the microchip. Y. H. performed all cell experiments. G. X. and H. Y. wrote the original manuscript. Z. W. edited the manuscript and supervised the project. H. Y. performed the HPLC-MS/MS experiments and analyzed the data. All authors reviewed the manuscript.

Conflicts of interest

There are no conflicts to declare.

Data availability

The data supporting this article have been included as part of the supplementary information (SI). Supplementary information: materials and methods; the droplet microfluidic device and the statistics of microsphere sizes; cell numbers in hydrogel microspheres at different cell densities; mask design of the single-microsphere culture chip; schematic diagram of increasing throughput; photomicrograph of loading microsphere into the culture chip; diffusion of sodium fluorescein over time in the culture chips; viability of single cells cultured on the culture chip ($n = 100$); mass spectrometry condition optimization process; chromatograms of single-cell metabolites samples; pre-experimental procedure of cellular metabolites; metabolic accumulation of arachidonic acid from A549 cultured on the chip ($*P < 0.05$); metabolic accumulation of glutamic acid from A549 cultured on the chip ($**P < 0.01$, $*P < 0.05$); schematic diagram of repeating metabolite collections; heatmap of metabolic accumulation differences among HCT116 cells ($n = 41$), A549 cells ($n = 47$) and HepG2 cells ($n = 35$); MRM conditions of single-cell metabolite. See DOI: <https://doi.org/10.1039/d5sc05261k>.

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Notes and references

- 1 S. Nong, X. Han, Y. Xiang, Y. Qian, Y. Wei, T. Zhang, K. Tian, K. Shen, J. Yang and X. Ma, *MedComm*, 2023, **4**, e218.
- 2 X. Xu, Q. Peng, X. Jiang, S. Tan, Y. Yang, W. Yang, Y. Han, Y. Chen, L. Oyang and J. Lin, *Exp. Mol. Med.*, 2023, **55**, 1357–1370.
- 3 Y. Wang and G. J. Patti, *Trends Cell Biol.*, 2023, **33**, 1014–1024.
- 4 M. Parlani, C. Jorgez and P. Friedl, *Trends Cell Biol.*, 2023, **33**, 388–402.
- 5 M. H.-R. Bao and C. C.-L. Wong, *Cells*, 2021, **10**, 1715.
- 6 X. Chen, S. Chen and D. Yu, *Metabolites*, 2020, **10**, 289.
- 7 C. A. Lyssiotis and A. C. Kimmelman, *Trends Cell Biol.*, 2017, **27**, 863–875.
- 8 E. Reznik, A. Luna, B. A. Aksoy, E. M. Liu, K. La, I. Ostrovskaya, C. J. Creighton, A. A. Hakim and C. A. Sander, *Cell Syst.*, 2018, **6**, 301–313.
- 9 G. Jia, J. Preussner, X. Chen, S. Guenther, X. Yuan, M. Yekelchik, C. Kuenne, M. Looso, Y. Zhou and S. Teichmann, *Nat. Commun.*, 2018, **9**, 4877.
- 10 P. Ellis, L. Moore, M. A. Sanders, T. M. Butler, S. F. Brunner, H. Lee-Six, R. Osborne, B. Farr, T. H. H. Coorens and A. R. J. Lawson, *Nat. Protoc.*, 2021, **16**, 841–871.
- 11 B. B. Tournier, S. Tsartsalis, K. Ceyzeriat, Z. Medina, B. H. Fraser, M.-C. Grégoire, E. Kövari and P. Millet, *J. Cereb. Blood Flow Metab.*, 2020, **40**, 1242–1255.
- 12 J. P. Robinson, R. Ostafe, S. N. Iyengar, B. Rajwa and R. Fischer, *Cells*, 2023, **12**, 1875.
- 13 X. Zeng, X. Guo, S. Jiang, X. Yang, Z. Zhong, S. Liu, Z. Zhu, L. Song and C. Yang, *Anal. Chem.*, 2023, **95**, 13313–13321.
- 14 L. Yang, J. George and J. Wang, *Proteomics*, 2020, **20**, 1900226.
- 15 A. M. Xu, Q. Liu, K. L. Takata, S. Jeoung, Y. Su, I. Antoshechkin, S. Chen, M. Thomson and J. R. Heath, *Lab Chip*, 2018, **18**, 3251–3262.
- 16 M. Stevens, P. Harder and L. W. M. M. Terstappen, *Lab Chip*, 2024, **24**, 460–466.
- 17 D. Zheng, J. Zhang, W. Jiang, Y. Xu, H. Meng, C. L. Poh and C.-H. Chen, *Lab Chip*, 2024, **24**, 137–147.
- 18 D. Feng, H. Li, T. Xu, F. Zheng, C. Hu, X. Shi and G. Xu, *Anal. Chim. Acta*, 2022, **1221**, 340116.
- 19 S. T. Gebreyesus, A. A. Siyal, R. B. Kitata, E. S.-W. Chen, B. Enkhbayar, T. Angata, K.-I. Lin, Y.-J. Chen and H.-L. Tu, *Nat. Commun.*, 2022, **13**, 37.
- 20 L. Zhang, T. Xu, J. Zhang, S. C. C. Wong, M. Ritchie, H. W. Hou and Y. Wang, *Anal. Chem.*, 2021, **93**, 10462–10468.
- 21 A. Kontiza, J. V. Gerichten, K. D. G. Saunders, M. Spick, A. D. Whetton, C. F. Newman and M. J. Bailey, *Anal. Chem.*, 2024, **96**, 17594–17601.
- 22 J. Lamanna, E. Y. Scott, H. S. Edwards, M. D. Chamberlain, M. D. M. Dryden, J. Peng, B. Mair, A. Lee, C. Chan, A. A. Sklavounos, A. Heffernan, F. Abbas, C. Lam,



- M. E. Olson, J. Moffat and A. R. Wheeler, *Nat. Commun.*, 2020, **11**, 5632.
- 23 Y. Zhu, P. D. Piehowski, R. Zhao, J. Chen, Y. Shen, R. J. Moore, A. K. Shukla, V. A. Petyuk, M. Campbell-Thompson, C. E. Mathews, R. D. Smith, W.-J. Qian and R. T. Kelly, *Nat. Commun.*, 2018, **9**, 882.
- 24 H. K. Komori, S. A. LaMere, A. Torkamani, G. T. Hart, S. Kotsopoulos, J. Warner, M. L. Samuels, J. Olson, S. R. Head, P. Ordoukhanian, P. L. Lee, D. R. Link and D. R. Salomon, *Genome Res.*, 2011, **21**, 1738–1745.
- 25 A. Rotem, O. Ram, N. Shosh, R. A. Sperling, A. Goren, D. A. Weitz and B. E. Bernstein, *Nat. Biotechnol.*, 2015, **33**, 1165–1172.
- 26 E. Z. Macosko, A. Basu, R. Satija, J. Nemes, K. Shekhar, M. Goldman, I. Tirosh, A. R. Bialas, N. Kamitaki, E. M. Martersteck, J. J. Trombetta, D. A. Weitz, J. R. Sanes, A. K. Shalek, A. Regev and S. A. McCarroll, *Cell*, 2015, **161**, 1202–1214.
- 27 X. Zhang, T. Li, F. Liu, Y. Chen, J. Yao, Z. Li, Y. Huang and J. Wang, *Mol. Cell*, 2019, **73**, 130.
- 28 E. P. Mimitou, A. Cheng, A. Montalbano, S. Hao, M. Stoeckius, M. Legut, T. Roush, A. Herrera, E. Papalexi, Z. Ouyang, R. Satija, N. E. Sanjana, S. B. Koralov and P. Smibert, *Nat. Methods*, 2019, **16**, 409–412.
- 29 M. Stoeckius, C. Hafemeister, W. Stephenson, B. Houck-Loomis, P. K. Chattopadhyay, H. Swerdlow, R. Satija and P. Smibert, *Nat. Methods*, 2017, **14**, 865–868.
- 30 D. S. Wishart, Y. D. Feunang, A. Marcu, A. C. Guo, K. Liang, R. Vázquez-Fresno, T. Sajed, D. Johnson, C. Li, N. Karu, Z. Sayeeda, E. Lo, N. Assempour, M. Berjanskii, S. Singhal, D. Arndt, Y. Liang, H. Badran, J. Grant, A. Serra-Cayuela, Y. Liu, R. Mandal, V. Neveu, A. Pon, C. Knox, M. Wilson, C. Manach and A. Scalbert, *Nucleic Acids Res.*, 2018, **46**, D608–D617.
- 31 X. Liu, S. Yan, H. Wu, M. Chen, H. Dai, Z. Wang, M. Chai, Q. Hu, D. Li, L. Chen, R. Diao, S. Chen, L. Wang and X. Shi, *Adv. Funct. Mater.*, 2024, **34**, 2315907.
- 32 Y. Peng, X. Chen, Q. Zhang, S. Liu, W. Wu, K. Li, H. Lin, X. Qing, Y. Xiao, B. Wang, D. Quan, S. Feng, Z. Rao, Y. Bai and Z. Shao, *Adv. Sci.*, 2024, **11**, 2304761.
- 33 Z. Wu, Y. Zheng, L. Lin, Y. Lin, T. Xie, W. Liao, S. Chen, Y. Zhang and J.-M. Lin, *Matter*, 2024, **7**, 3645–3657.
- 34 Z. Wu, Y. Zheng, J.-M. Lin, Y. Li, Y. Lin, X. Wang and L. Lin, *Chem. Eng. J.*, 2024, **481**, 148403.
- 35 D. Sun, F. Cao, Y. Tian, A. Li, W. Xu, Q. Chen, W. Shi and S. Xu, *Anal. Chem.*, 2019, **91**, 15484–15490.
- 36 F. D. Ben, M. Turetta, G. Celetti, A. Piruska, M. Bulfoni, D. Cesselli, W. T. S. Huck and G. Scoles, *Angew. Chem.*, 2016, **128**, 8723–8726.
- 37 Q. Liu, W. Ge, T. Wang, J. Lan, S. Martínez-Jarquín, C. Wolfrum, M. Stoffel and R. Zenobi, *Angew. Chem.*, 2021, **133**, 24739–24747.
- 38 Q. Ruan, J. Yang, F. Zou, X. Chen, Q. Zhang, K. Zhao, X. Lin, X. Zeng, X. Yu, L. Wu, S. Lin, Z. Zhu and C. Yang, *Anal. Chem.*, 2022, **94**, 1108–1117.
- 39 M. Pelletier, L. K. Billingham, M. Ramaswamy and R. M. Siegel, *Methods Enzymol.*, 2014, **542**, 125–149.
- 40 C. Jin, Z. Cao, H.-L. Zhu and Z. Li, *Biosens. Bioelectron.*, 2024, **261**, 116484.
- 41 D. Sun, J. Lu, D. Chen, Y. Jiang, Z. Wang, W. Qin, Y. Yu, Z. Chen and Y. Zhang, *Sens. Actuators, B*, 2018, **268**, 359–367.
- 42 L. Kan, D. Cui, Y. Chai, L. Ma, X. Li and M. Zhao, *Int. J. Biol. Macromol.*, 2020, **165**, 1755–1764.
- 43 G. Xing, Y. Shang, X. Wang, Z. Wu, Q. Zhang, J. Ai, Q. Pu and L. Lin, *Chin. Chem. Lett.*, 2024, **35**, 109491.
- 44 G. Xing, Y. Shang, X. Wang, H. Lin, S. Chen, Q. Pu and L. Lin, *Biosens. Bioelectron.*, 2023, **220**, 114885.
- 45 Y. Zhao, Q. Li and X. Hu, *Anal. Methods*, 2018, **10**, 3489–3497.
- 46 B. Li, L. Zhang, Y. Yin, A. Chen, B. R. Seo, J. Lou, D. J. Mooney and D. A. Weitz, *Matter*, 2024, **7**, 3447–3468.
- 47 Q. Wei, J. Zhou, Y. An, M. Li, J. Zhang and S. Yang, *Int. J. Biol. Macromol.*, 2023, **232**, 123450.
- 48 S. Chen, Y. Li, Y. Zhang, H. Yao, T. Xu, Y. Zhang, J.-M. Lin and X.-L. Meng, *J. Pharm. Anal.*, 2024, **14**, 100967.
- 49 H. Yao, Y. Li, Y. Zheng and J.-M. Lin, *Anal. Chem.*, 2023, **95**, 10999–11006.
- 50 L. Wu, Y. Jin, X. Zhao, K. Tang, Y. Zhao, L. Tong, X. Yu, K. Xiong, C. Luo, J. Zhu, F. Wang, Z. Zeng and D. Pan, *Cell Metab.*, 2023, **35**, 1580–1596.
- 51 Z. N. Ling, Y. F. Jiang, J. N. Ru, J. H. Lu, B. Ding and J. Wu, *Targets Ther.*, 2023, **8**, 345.
- 52 M. Nian, B. Chen, M. He and B. Hu, *Anal. Chem.*, 2024, **96**, 766–774.
- 53 Y. Xu, B. Chen, M. He, Z. Cui and B. Hu, *Anal. Chem.*, 2023, **95**, 14061–14067.
- 54 S. Ansaryan, Y. C. Liu, X. Li, A. M. Economou, C. S. Eberhardt, C. Jandus and H. Altug, *Nat. Biomed. Eng.*, 2023, **7**, 943–958.

