

ChemComm

Chemical Communications

rsc.li/chemcomm



ISSN 1359-7345

COMMUNICATION

Lu Su, Patricia Y. W. Dankers *et al.*
Introducing carbohydrate patterning in mannose-decorated
supramolecular assemblies and hydrogels


 Cite this: *Chem. Commun.*, 2023, 59, 2090

 Received 14th November 2022,
Accepted 16th January 2023

DOI: 10.1039/d2cc06064g

rsc.li/chemcomm

Benzene-1,3,5-tricarboxamide (BTA) glyco-monomers containing one, two or three mannose units are synthesized and formulated into differently patterned supramolecular glycopolymers through homo-assembly or co-assembly with non-functionalized BTAs. Unfortunately, no cellular activity could be detected. Excitingly, these glyco-BTA monomers could be formulated into hydrogels, paving the way for (immune) cell culture.

Carbohydrate–protein interactions (CPIs) are abundant in many biological processes and involved in the immune response.¹ Importantly, many mammalian epithelial cells have a glycocalyx – a coating surrounding the cell surface containing glycoproteins, glycolipids and proteoglycans – which has a crucial role in cell–cell recognition and communication.² Synthetic glycopolymers as mimics of their natural counterparts that present carbohydrates in a multivalent manner are increasingly being designed and synthesized to gain better understanding of CPIs,^{3–9} of which the mannose – mannose receptor (CD206) is an important one.^{10,11}

Introducing carbohydrate patterning in mannose-decorated supramolecular assemblies and hydrogels†

 Laura Rijns,^{id abc} Lu Su,^{id *cd} Konrad Maxeiner,^e Giulia Morgese,^f
David Y. W. Ng,^{id e} Tanja Weil^e and Patricia Y. W. Dankers^{id *abc}

To illustrate, mannosylated nanoparticles and rods have been created by Besenius, Wurm, De Geest and others, which exhibit specific receptor–ligand interactions to both lectins and dendritic cells (DCs) as compared to poly(ethylene glycol) (PEG) or galactosylated controls,^{3,4,12} and are thus effective and selective in binding biological entities. Feng *et al.* investigated the morphological effects, *i.e.* elongated, rod-like *vs.* spherical, micellar morphology, of glucomannan-decorated particles.⁵ Especially the spherical, micellar morphology could trigger the release of cytokines in macrophages, highlighting the importance of morphology–function relationship of CPIs. Chen *et al.* fabricated glycoparticles bearing galactose and/or mannose, and explored the architectural effects, *i.e.* homogeneously mixed *vs.* blend mixed *vs.* homo-shells, on lectin-binding and macrophage endocytosis performance.¹³ They showed that the homogeneously mixed sugar shells outperform the blend-mixed shells, emphasizing the importance of carbohydrate patterning in CPIs.

Considering the importance of these morphological and architectural effects in effective receptor targeting, supramolecular glyco-assemblies based on non-covalent interactions that exhibit adaptivity in ligand presentation, morphology and dynamicity are emerging as a promising class of glycopolymers.^{14,15} In our lab, we have ample expertise with the benzene-1,3,5-tricarboxamide (BTA) monomer that assembles into different nanostructures, including micelles, sheets and micrometer long fibers, driven by triple amide hydrogen bonding and π – π interactions in the core together with the hydrophobic effect.^{16,17} Our ‘standard’, non-functionalized BTA (**nBTA**) has three C_{12} spacers connected to its core such that water cannot compete for amide hydrogen bonding, and three tetra(ethylene glycol) (EG_4) arms to provide water solubility (Fig. 1A), forming micrometer long double helical fibers.¹⁸ In these supramolecular fibers, the spatial rearrangement could easily be adopted through dynamic monomer exchange within the supramolecular polymers to promote binding events.¹⁹ Besides, control over morphology, supramolecular polymer length and dynamicity could be achieved by tuning the degree of hydrophobicity of the monomers and/or through copolymerization (*i.e.* mixing of different monomers within the same assembly).⁷

Recently, the non-covalent synthesis (*i.e.* assembly of monomers into larger supramolecular structures, connected through dynamic,

^a Institute for Complex Molecular Systems (ICMS), Eindhoven University of Technology, PO Box 513, Eindhoven 5600 MB, The Netherlands.
E-mail: p.y.w.dankers@tue.nl

^b Department of Biomedical Engineering, Laboratory of Chemical Biology, Eindhoven University of Technology, PO Box 513, Eindhoven 5600 MB, The Netherlands

^c Department of Biomedical Engineering, Laboratory for Cell and Tissue Engineering, Eindhoven University of Technology, PO Box 513, Eindhoven 5600 MB, The Netherlands

^d Leiden Academic Centre for Drug Research (LACDR), Leiden University, Einsteinweg 55, Leiden 2333 CC, The Netherlands.
E-mail: l.su@lacdr.leidenuniv.nl

^e Max Planck Institute for Polymer Research, Ackermannweg 10, Mainz 55128, Germany

^f ZHAW Zurich University of Applied Sciences, School of Engineering, Forschungsbereich Polymere Beschichtungen, Technikumstrasse 9, Winterthur 8400, Switzerland

† Electronic supplementary information (ESI) available: Synthetic procedures and characterization, methods, supporting data of cryoTEM, CD, microDSC, variable temperature UV-Vis, rheology, toxicity, metabolic flux and ELISA assays, flow cytometry and internalization data. See DOI: <https://doi.org/10.1039/d2cc06064g>





Fig. 1 Molecular design and cartoon showing the summary of this study. (A) Molecular design and synthetic route of M_x BTA ($x = 1$ or 2 or 3) through statistical glycosylation towards **nBTA**, followed by deprotection with sodium methoxide in MeOH. (B) Illustration showing the copolymerization approach of fully mannosylated **M3 BTA** with non-functionalized **nBTA** to afford co-assemblies with similar mannose density, but distinct mannose patterns as compared to their homopolymer analogues.

reversible interactions) of a series of saccharide-substituted BTA monomers, including glucose, galactose and mannose, was investigated in detail on the structural and dynamic properties.^{7,20,21} Interestingly, a triple mannose-decorated BTA that forms micelles (**M3 BTA**) was successfully incorporated into **nBTA** polymers, resulting in long fibers with increased overall stability, realizing control over the dynamic behavior and morphology.⁷ Surprisingly, the patterning effect of mannose (*i.e.* similar mannose density but different spatial distribution in the fiber) as well as the formation of mannosylated hydrogels and their effect towards (immune) cells remains yet unknown.

Therefore, we here introduce mannose patterning in BTA-based supramolecular assemblies – *via* similar mannose densities but distinct spatial distribution throughout the fiber – and explore their effect on macrophages (Fig. 1B). To achieve this, asymmetric, mono-mannosylated BTA (**M1 BTA**) and double-mannosylated BTA (**M2 BTA**) homo-assemblies were compared to their corresponding copolymers consisting of fully mannosylated BTA (**M3 BTA**) and **nBTA** (**Copolymer_1** with **nBTA**:**M3 BTA** = 2:1 (mol) and **Copolymer_2** with **nBTA**:**M3 BTA** = 1:2) (Fig. 1A). The non-covalent synthesis of the homo-assemblies and their corresponding co-assemblies are investigated in MQ-H₂O. Furthermore, mannosylated supramolecular gels are fabricated by increasing the concentration above their critical gelation concentration (CGC).

The asymmetric **M1** and **M2 BTA** molecules were synthesized by direct glycosylation towards the **nBTA** with active mannose

imidate as the donor and trimethylsilyl trifluoromethanesulfonate as the promoter, followed by deprotection with sodium methoxide, to obtain pure (purity > 99%) **M1** and **M2 BTA** with an overall yield of 14% (305 mg) and 26% (629 mg), respectively (Fig. 1A). The successful synthesis of **M1** and **M2 BTA** was confirmed by a combination of nuclear magnetic resonance (NMR) measurements (¹H, ¹³C and 2D NMR), Fourier-transform infrared (FT-IR) spectroscopy and with matrix assisted laser absorption/ionization-time of flight (MALDI-TOF) mass spectrometry (Fig. S1–S6, ESI†).

nBTA¹⁷ and **M3 BTA**⁷ have shown to form micrometer-long fibers and micelles, respectively. Both homo-assembled **M1** and **M2 BTA** show maximum absorptions in UV at 211 and 227 nm, which is also observed for their counterparts **Copolymer_1** and **_2** (Fig. 2A). This almost completely overlaps with the absorption spectrum of **nBTA**, indicative for fibers (Fig. 2A). However, the absorption peaks for **M2 BTA** and its **Copolymer_2** are less pronounced than that of **nBTA**, which might indicate different fibrous structures. Nile red assays indicated a significant blue shift for the homo-assembled BTAs as well as for the co-assemblies (610 nm), when compared with the micelle-forming **M3 BTA** (630 nm), demonstrating the presence of a hydrophobic pocket (Fig. 2B). Static light scattering (SLS) showed a dependence of the Rayleigh ratio on the scattering angle for all homo- and co-assembled BTAs, except for the micelle-forming **M3 BTA**, indicating elongated structures (Fig. 2C). Cryo-TEM further confirmed the morphology of micrometer long nanofibers with a

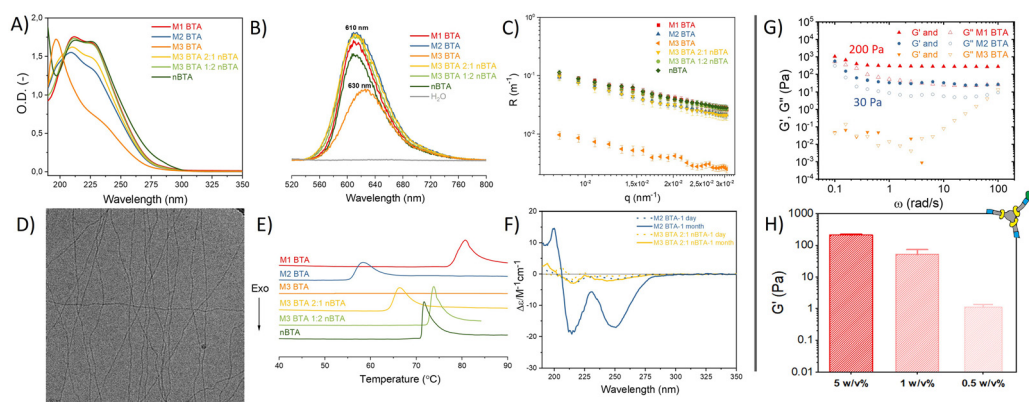


Fig. 2 Characterization of the supramolecular mannose BTA homo-assemblies and their corresponding co-assemblies as well as mechanical characterization of mannosylated supramolecular hydrogels. (A) UV spectra (50 μ M), (B) Nile red assay (50 μ M), (C) SLS profile (500 μ M), (D) representative Cryo-TEM image of **M1** and **M2 BTA** (500 μ M). Scale bar = 50 nm. (E) microDSC profiles (500 μ M), and (F) CD spectra (50 μ M) of BTAs in MQ-H₂O. (G, H) Mechanical characterization of supramolecular mannosylated BTA hydrogels using rheology, with in (G) angular frequency sweep plot at 1% strain showing the storage (G') and loss modulus (G'') at 5 w/v% and in (H) G' quantified at different concentrations of **M1 BTA** to determine its CGC.



diameter of 6 ± 2 nm for **M1** and **M2 BTA** as well as for **Copolymer_1** and **_2** (Fig. 2D – representative image, Fig. S7–S10, ESI†). Micro Differential Scanning Calorimetry (microDSC) suggested a co-assembled state for **Copolymer_1** and **Copolymer_2** rather than self-sorting, as suggested by the absence of **nBTA** endothermic peaks in the curves (Fig. 2E and Fig. S13, ESI†). **M1 BTA** showed an endothermic peak in microDSC at higher temperature (80 °C) than **Copolymer_1** (75 °C), suggesting different microstructure and higher thermal stability for **M1 BTA** (Fig. 2E). On the contrary, **M2 BTA** showed an endothermic peak at 58 °C and **Copolymer_2** at 66 °C, suggesting less thermal stability for **M2 BTA** (Fig. 2E). Noteworthy, for **M1 BTA**, **M2 BTA** and both **Copolymer_1** and **_2**, the endothermic peaks in microDSC appear at higher temperatures in all cases than the transition in the variable temperature (vt) UV heating curves. To illustrate, the transition in microDSC is at 80 and 75 °C for **M1 BTA** and **Copolymer_1** (Fig. 2E), respectively, vs. at 65 °C for both in vt UV (Fig. S11, ESI†). Likewise for **M2 BTA** and **Copolymer_2**, the transition in microDSC occurs respectively at 58 and 66 °C (Fig. 2E) vs. at 45 and 60 °C for vt UV (Fig. S12, ESI†). These differences might arise from the different heating rate and concentrations used for the different techniques. Interestingly, the CD spectra of **M1 BTA** (Fig. S14, ESI†) and of **M2 BTA** (Fig. 2F) showed significant ageing effect. Although the exact molecular mechanism for the increased CD signal after ageing remains questionable, it is proposed that ageing is required for the polymer to reach its maximal preferred helical bias, accompanied by decreased dynamics.²² Besides, **M2 BTA** showed a more profound CD signal (Fig. 2F; peaks at 210 and 250 nm) as compared to its **Copolymer_2**. This indicates that the mannose pattern within the fibers should be different. This is of great interest for further cell experiments. In conclusion, micelle-forming **M3 BTA** was successfully co-assembled with **nBTA** to form supramolecular copolymers with similar mannose density but different mannose pattern as their corresponding homo-assemblies (**M1** and **M2 BTA**).

Next, hydrogels were fabricated with the mannosylated BTAs. The CGC of **M1 BTA** was found to be ~ 0.5 w/v%. **M1 BTA** could still withstand its own weight at 0.5 and 1 w/v% concentrations in vial-inversion tests (Fig. S16A, ESI†), but forms very soft gels with a G' of only a few Pa and of ~ 50 Pa for the 0.5 and 1 w/v% samples, respectively (Fig. 2H and Fig. S17, ESI†). On the contrary, **M2 BTA** could not pass the vial-inversion test at 0.5 and 1 w/v% concentrations (Fig. S16B, ESI†) and appeared as a liquid. This indicates that its CGC is higher than 1 w/v%, but lower than 5 w/v%. Rheology performed at 5 w/v% concentrations revealed that **M1** and **M2 BTA** form soft gels with a $G' \sim 200$ Pa and 30 Pa, respectively (Fig. 2G and Fig. S15, ESI†). However, **M3 BTA** remained a liquid with G'' exceeding G' and containing higher $\tan(\delta)$ values than **M1** and **M2 BTA**, indicating a higher viscous-like behavior for **M3 BTA** (Fig. 2G and Fig. S15, ESI†). The difference in bulk stiffness between **M1** and **M2 BTA** could be explained by the longer fibrous structures of **M1 BTA** in comparison with **M2 BTA**, resulting in a stronger gel. We hypothesize that the fibers of both **M1** and **M2 BTA** entangle at these concentrations also due to carbohydrate–carbohydrate interactions, resulting in the formation of a gel. Whereas the more hydrophilic **M3 BTA** that forms micelles in diluted state prevents the formation of a gel. It should also be realized that fewer molecules of **M3 BTA** ($c = 28.2$ mM) are present in the 5 w/v% samples as compared to **M1**

($c = 34.5$ mM) and **M2 BTA** ($c = 31$ mM), owing to its higher molecular weight. Therefore, a control sample of **M3 BTA** at 5 w/v% was created, containing a similar molar concentration ($c = 34.5$ mM) to that of **M1 BTA** at 5 w/v%. The control remained a liquid that could not hold its own weight during a vial-inversion test (Fig. S16C, ESI†). Importantly, the mannosylated gels exhibit self-healing behavior as demonstrated with the **M1 BTA** gel (Fig. S17B, ESI†).

Next, the biological effect of the mannose-decorated homo- and co-assemblies on immune cells was tested. Therefore, the fiber stability in complex media is of great importance. In absence and presence of fetal bovine serum (FBS), an abundant component in cell medium, the presence of fibers, but also aggregated structures, was confirmed using total internal reflection microscopy (TIRF) (Fig. 3A). This indicates that serum does not affect the structural properties homo-assemblies nor the co-assemblies. None of the mannose BTAs affect the cell viability of RAW 264.7 macrophages, important cells of the immune system, up to 100 μ M concentrations (Fig. 3B and Fig. S18, ESI†). For efficient targeting of the immune cells using mannose as ligand, the expression of CD206 on the cell surface is crucial. Flow cytometry experiments confirmed the presence of the CD206 ($\sim 50\%$) on the macrophages (Fig. S19, ESI†). Subsequent internalization experiments showed endocytosis for all assemblies by the macrophages already after incubation of 2 h (Fig. 3C and Fig. S20, ESI†), agreeing with other studies that also reveal endocytosis of glycoparticles by immune cells.^{3,23} However, internalization was also observed for **nBTA**, suggesting that the endocytosis is not CD206-mediated, in contrast to other studies.^{3,13} The internalization could be caused by the origin of the cells, as macrophages are known for their phagocytic capabilities, but could also be Cy5-mediated, as Cy5 is known to facilitate cellular uptake caused by its tendency to bind the mitochondria.^{24,25} To study whether metabolic pathways, *i.e.* oxidative phosphorylation or glycolysis, are affected during and after endocytosis of the BTA assemblies, extracellular flux assays were executed to reveal how the integrity of intracellular structures are influenced, thereby affecting cell viability. Minimal increase in oxygen consumption rate (indicative for oxidate phosphorylation) or extracellular acidification rate (indicative for glycolysis) was detected with 10 h incubation (Fig. S21 and S22, ESI†), indicating limited energy consumption by the macrophages during the internalization and that associated binding events by the BTAs do not increase the metabolic load of the cells.

To explore if the mannosylated glycopolymers could activate CD206 in macrophages, their IL-10 cytokine release was quantified using Enzyme-linked Immuno Sorbent Assay (ELISA) assays. Unfortunately, no IL-10 release could be detected after 24 h incubation (Fig. 3D and Fig. S23, ESI†). Lipopolysaccharide (LPS) was used as positive control and showed extremely high IL-10 release of up to 6000 pg mL^{-1} IL-10 for the 10 $\mu\text{g mL}^{-1}$ condition, while mannan (*i.e.* poly mannose) could not induce any release (Fig. S24, ESI†). Although similar concentrations of BTA or LPS were used (100 μM BTA roughly equals 100 – 200 $\mu\text{g mL}^{-1}$ BTA, which is in the same order of magnitude as used for LPS; 0.01 – 100 $\mu\text{g mL}^{-1}$ and mannan; 100 $\mu\text{g mL}^{-1}$), it should be realized that LPS is a more complex mix of various carbohydrates. Also, our BTA assemblies could interact with bovine serum albumin (BSA)²⁰ that is present in FBS in complex media. A possible scenario might include the complete ‘blocking’ of the mannose residues on the BTA assemblies by BSA. Another





Fig. 3 Fiber stability, toxicity and cell internalization experiments. (A) Representative TIRF images of the homo- and co-assemblies (BTA = 2.5 μM , with 5% of BTA-Cy3) with and without the presence of FBS at 20 $^{\circ}\text{C}$, showing that the fibrous morphology could be maintained in cell-like environments. Scale bar = 10 μm . (B) Cell viability assay of 100 μM BTA assemblies towards RAW264.7 macrophages as determined with a resazurin assay. The cell viability is normalized on cells that were maintained in untreated medium (*i.e.* medium control). (C) Internalization experiment in which RAW 264.7 macrophages were incubated with Cy5-labeled BTAs ($c = 25 \mu\text{M}$ total, with 5% BTA-Cy3) in presence and absence of FBS for 2 h, and stained thereafter. Scale bar = 10 μm . (D) ELISA assay to quantify the release of IL-10 in RAW 264.7 macrophages after treatment with 25 μM mannose BTAs for 24 h.

explanation could be the dynamicity of the supramolecular assemblies. In case the monomer exchange rate is faster than the time-frame in which CD206 could recognize and bind mannose, binding between the receptor and mannose-decorated fibers will be limited.

To conclude, mannose patterning was introduced in BTA-based, supramolecular assemblies through supramolecular copolymerization of fully mannosylated BTA (M3 BTA) and nonfunctionalized BTA (nBTA) to produce a series of BTA copolymers that were compared with their asymmetric, homo-assembled counterparts (M1 BTA and M2 BTA). Unfortunately, no biological effect could be detected. Interestingly, mannosylated hydrogels could be formed for M1 BTA (CMC $\sim 0.5 \text{ w/v}\%$) and M2 BTA ($1 \text{ w/v}\% < \text{CMC} < 5 \text{ w/v}\%$), whereas the more hydrophilic M3 BTA remained a liquid. We anticipate that these mannose-patterned supramolecular glycopolymers and hydrogels exhibiting inherent dynamicity and great tunability allow us to arrive at deeper understanding of multivalent CPIs, which are essential to many biological processes.

We thank Svenja Ehrmann and Sandra Schoenmakers for measuring the cryoTEM images. We thank prof. Bruno de Geest and prof. Bert Meijer for useful discussions. We acknowledge financial support from NWO (TOP-PUNT Grant 10018944), the Dutch Ministry of Education, Culture and Science (Gravitation programs 024.001.035 and 024.003.013), the European Commission (SYNMAT- 788618-1).

Conflicts of interest

There are no conflicts to declare.

Notes and references

- R. A. Dwek, *Chem. Rev.*, 1996, **96**, 683–720.
- L. Möckl, *Front. Cell. Dev. Biol.*, 2020, **8**, 253.
- R. de Coen, N. Vanparijs, M. D. P. Risseeuw, L. Lybaert, B. Louage, S. de Koker, V. Kumar, J. Grooten, L. Taylor, N. Ayres, S. van Calenbergh, L. Nuhn and B. G. de Geest, *Biomacromolecules*, 2016, **17**, 2479–2488.
- B. Kang, P. Okwieka, S. Schöttler, S. Winzen, J. Langhanki, K. Mohr, T. Opatz, V. Mailänder, K. Landfester and F. R. Wurm, *Angew. Chem., Int. Ed.*, 2015, **54**, 7436–7440.
- Y. Feng, R. Mu, Z. Wang, P. Xing, J. Zhang, L. Dong and C. Wang, *Nat. Commun.*, 2019, **10**, 1–14.
- L. Wu, Y. Zhang, Z. Li, G. Yang, Z. Kochovski, G. Chen and M. Jiang, *J. Am. Chem. Soc.*, 2017, **139**, 14684–14692.
- S. I. S. Hendrikse, L. Su, T. P. Hogervorst, R. P. M. Lafleur, X. Lou, G. A. van der Marel, J. D. C. Codee and E. W. Meijer, *J. Am. Chem. Soc.*, 2019, **141**, 13877–13886.
- C. M. A. Leenders, G. Jansen, M. M. M. Frissen, R. P. M. Lafleur, I. K. Voets, A. R. A. Palmans and E. W. Meijer, *Chem. – Eur. J.*, 2016, **22**, 4608–4615.
- L. Su, W. Zhang, X. Wu, Y. Zhang, X. Chen, G. Liu, G. Chen and M. Jiang, *Small*, 2015, **11**, 4191–4200.
- P. D. Stahl and R. A. B. Ezekowitz, *Curr. Opin. Immunol.*, 1998, **10**, 50–55.
- I. D. Zlotnikov, A. A. Ezhov, R. A. Petrov, M. A. Vigovskiy, O. A. Grigorieva, N. G. Belogurova and E. V. Kudryashova, *Pharmaceuticals*, 2022, **15**, 1172.
- D. Straßburger, N. Stergiou, M. Urschbach, H. Yurugi, D. Spitzer, D. Schollmeyer, E. Schmitt and P. Besenius, *ChemBioChem*, 2018, **19**, 912–916.
- L. Wu, Y. Zhang, Z. Li, G. Yang, Z. Kochovski, G. Chen and M. Jiang, *J. Am. Chem. Soc.*, 2017, **139**, 14684–14692.
- J. F. Lutz, J. M. Lehn, E. W. Meijer and K. Matyjaszewski, *Nat. Rev. Mater.*, 2016, **1**.
- L. Su, S. I. S. Hendrikse and E. W. Meijer, *Curr. Opin. Chem. Biol.*, 2022, **69**, 102171.
- B. N. S. Thota, X. Lou, D. Bochicchio, T. F. E. Paffen, R. P. M. Lafleur, J. L. J. van Dongen, S. Ehrmann, R. Haag, G. M. Pavan, A. R. A. Palmans and E. W. Meijer, *Angew. Chem., Int. Ed.*, 2018, **57**, 6843–6847.
- C. M. A. Leenders, L. Albertazzi, T. Mes, M. M. E. Koenigs, A. R. A. Palmans and E. W. Meijer, *Chem. Commun.*, 2013, **49**, 1963–1965.
- R. P. M. Lafleur, S. Herziger, S. M. C. Schoenmakers, A. D. A. Keizer, J. Jahzerah, B. N. S. Thota, L. Su, P. H. H. Bomans, N. A. J. M. Sommerdijk, A. R. A. Palmans, R. Haag, H. Friedrich, C. Böttcher and E. W. Meijer, *J. Am. Chem. Soc.*, 2020, **142**, 17644–17652.
- D. Bochicchio, M. Salvalaglio and G. M. Pavan, *Nat. Commun.*, 2017, **8**, 1–11.
- S. Varela-Aramburu, G. Morgese, L. Su, S. M. C. Schoenmakers, M. Perrone, L. Leanza, C. Perego, G. M. Pavan, A. R. A. Palmans and E. W. Meijer, *Biomacromolecules*, 2020, **21**, 4105–4115.
- C. M. A. Leenders, G. Jansen, M. M. M. Frissen, R. P. M. Lafleur, I. K. Voets, A. R. A. Palmans and E. W. Meijer, *Chem. – Eur. J.*, 2016, **22**, 4608–4615.
- S. M. C. Schoenmakers, A. J. H. Spiering, S. Herziger, C. Böttcher, R. Haag, A. R. A. Palmans and E. W. Meijer, *ACS Macro Lett.*, 2022, **11**, 711–715.
- G. Gunay, M. Sardan Ekiz, X. Ferhati, B. Richichi, C. Nativi, A. B. Tekinay and M. O. Guler, *ACS Appl. Mater. Interfaces*, 2017, **9**, 16035–16042.
- A. R. Nödling, E. M. Mills, X. Li, D. Cardella, E. J. Sayers, S. H. Wu, A. T. Jones, L. Y. P. Luk and Y. H. Tsai, *Chem. Commun.*, 2020, **56**, 4672–4675.
- A. Lacroix, E. Vengut-Climent, D. de Rochambeau and H. F. Sleiman, *ACS Cent. Sci.*, 2019, **5**(5), 882–891.
- L. Albertazzi, D. van der Zwaag, C. M. A. Leenders, R. Fitzner, R. W. van der Hofstad and E. W. Meijer, *Science*, 2014, **344**, 491–495.

