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Measuring the size and density of nanoparticles by centrifugal sedimentation and flotation†

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The successful translation of nanoparticle-based systems into commercial products depends upon the ability to reliably measure important physical and chemical properties of these particles. The density of nanoparticles is one such property, because it provides important information about the composition of the material. In this work, an analytical centrifugation approach based on line-start centrifugal sedimentation and flotation measurements is described. The two independent measurements permit both the size and the density of these nanoparticles to be determined with excellent precision. A set of monodisperse polystyrene nanoparticles of different sizes is used to demonstrate this method. The density and size measurements are validated by comparison to accurate Small Angle X-ray Scattering (SAXS) analysis for particles within the size range of SAXS, *i.e.* less than ~300 nm in diameter. Both sedimentation and flotation measurements produce consistent high resolution size distributions of the particles and the measured size and density values are identical, within experimental uncertainty, to the SAXS results. This approach has the potential to provide useful characterisation of a range of particles of interest, for example, for medical application, such as liposomes and polymeric drug carriers.

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Introduction

The majority of nanoparticles (NPs) used in technological applications contain internal structures with, for example, engineered coatings or compartments loaded with functional molecules. Some of the particles used in medicine have coatings that prevent protein fouling to avoid their agglomeration or elimination *via* the reticuloendothelial system.¹ Liposomal and polymeric carriers which package drug molecules in their core have been successfully commercialised, as in the case of liposomal doxorubicin (Doxil®)² and protein-bound paclitaxel (Abraxane®)³ for cancer treatment. A similar situation is true in other areas, for example in catalysis the NanoSelect™ technology has enabled the commercialisation of Pd catalysts as lead-free Lindlar catalyst replacements in alkyne-to-*cis*-alkene hydrogenations.⁴ Their organic coatings are essential in ensuring chemoselectivity and efficiency.

The successful translation of particle-based systems into commercial products requires the ability to reliably measure the physical and chemical properties of these particles, to ensure that: the synthesis is reproducible and efficient, batch to batch variability is reduced, and the stability of the final product can be monitored. Ideally, the measurement methods should be cost effective and rapid, sufficiently precise to reliably measure differences and changes in the products, and provide statistically relevant information. For example, dynamic light scattering (DLS) is extensively used in this setting for the measurement of particle size and an expanding selection of other benchtop techniques are available.⁵

Size is only one characteristic of a particle system and further insight into particle properties is required. For example, combining the knowledge of particle size with that of their density can provide access to a range of additional information, such as molecular coating thickness and pack density,^{6–10} core porosity,⁵ chemical composition,¹¹ particle deformation,¹² particle encapsulation into vesicles,¹³ and drug loading.¹⁴ The knowledge of particle density is also useful during sample preparation for formulation and analysis. For example centrifugal sedimentation of NPs is commonly used in science and technology to separate particles of different size and density.

Differential centrifugal sedimentation (DCS), also known as centrifugal photo-sedimentation, is a benchtop technique which is commonly used to measure high resolution size distributions of NPs. DCS measures the time it takes to NPs to sediment through a fluid when exposed to a centrifugal field.

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† Electronic supplementary information (ESI) available: Synthesis details of PS particles, size and density measurements by DCS in sedimentation, flotation and combined mode and widths of the size distributions as measured by DCS in sedimentation and flotation modes, SEM and SAXS. See DOI: 10.1039/c8ay00237a



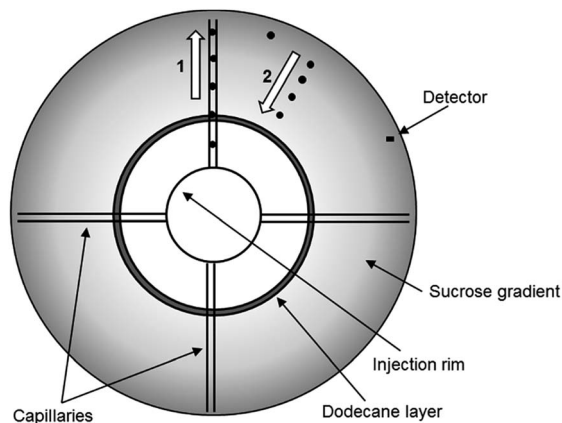


Fig. 1 Schematic representation of the principles of the functioning of the DCS disc for low density particles. The particles are injected in a rim and travel to the edge of the disc through four capillaries (1). From the edge, the particles float towards the centre of the disc through a sucrose gradient of higher density (2). The particles are detected when travelling in front of the detector.

This time depends on both the NP size and density. Where the size of the particles is known from an independent technique, DCS has been used with success to measure their density.^{5,11,12} DCS has also been used to measure both the size and density of particles by performing two independent DCS experiments using different fluid densities.^{5,15–17}

Recently, the DCS method has been developed to permit the analysis of particles which have a density close to, or below that of water. These low density particles “float” through a gradient of higher density rather than sedimenting through a gradient of lower density (Fig. 1). In a sedimentation experiment the sample is injected at the centre of a rotating disc and sediments towards the edge, where it is detected by a photodetector placed near the edge. To allow experiments by flotation, the disc has been modified so that the sample injected at the centre of the disc is delivered to the disc edge through four capillaries. From the disc edge the sample is released into the gradient and floats towards the detector. This technical innovation has opened up the possibility to measure high resolution size distributions and densities of particles such as liposomes, low density polymer particles and oil droplets. However, the literature on DCS operated in flotation mode is extremely scarce and, to our knowledge, this approach has only been briefly described in one of our previous publications.¹⁵

In this work we show the utility of the DCS technique to analyse particles with density below 1.2 g cm^{-3} . We describe in detail the set-up which is required for this type of analysis. Furthermore, we provide examples of application to the measurement of both the diameter and density of a set of polystyrene particles ranging in size from about 120 nm to 600 nm, and to the analysis of liposomes with diameters of about 100 nm.

Experimental

Materials

The polystyrene NPs were synthesized by emulsion polymerization of styrene using sodium dodecyl sulphate (SDS) as

surfactant. The amount of monomer and surfactant in the reaction mixture was properly adjusted to obtain particles with different size (Table S1 of the ESI†). The polymerization reactions were carried out in a 1 L five-neck reactor equipped with a condenser, a mechanical stirrer, a thermometer and inlets for nitrogen and styrene. 500 mL of ultrapure water containing the appropriate amount of SDS (see Table S1† for details) was introduced into the reactor at room temperature with a stirring rate of 300 rpm, then the appropriate amount of styrene (Table S1†) was added dropwise. The mixture was purged with nitrogen, and nitrogen was fluxed during the entire polymerization procedure. The reactor was heated to 80°C , then a potassium persulfate aqueous solution (5.0 mL, 0.74 mmol) was added, and the mixture was reacted for 24 h. The obtained latex was purified from surfactant and unreacted monomer by repeated dialyses against ultrapure water (cellulose membrane, molecular weight cut-off 12 kDa). Table S1† collects the details of the various preparations, including the latex yield.

Differential centrifugal sedimentation (DCS)

DCS measurements were performed with CPS Disk Centrifuge instruments, Model DC24000 (CPS Instruments, Prairieville, LA, USA), in both sedimentation and flotation configurations. Prior to the measurements a sucrose (Amresco LLC, OH, USA) gradient was built within the disc, according to manufacturer instructions. The density gradient is necessary to counteract the destabilizing effect of higher apparent density in the sample and avoid so called “streaming” *i.e.* the behaviour of the particle sample like a fluid of higher density, rather than like individual particles suspended in a fluid of lower density.¹⁸ The gradient was allowed to thermally equilibrate for 30 minutes before starting the measurements. The resulting average densities of the gradients were 1.011 g cm^{-3} (sucrose/water) for sedimentation and 1.14 g cm^{-3} (sucrose/ D_2O) for flotation experiments respectively. Turbidity measurements at the detector were performed using a diode laser at a wavelength of 405 nm. All experiments used a rotational frequency of 24 000 rpm and injection volume of 100 μL . Each sedimentation measurement was calibrated using polystyrene particles of nominal size 522 nm and density 1.05 g cm^{-3} . Each flotation measurement was calibrated using polybutadiene particles of nominal size 510 nm and density 0.91 g cm^{-3} . The PS NP samples were diluted 20 000 times from the original solution using ultrapure water for sedimentation experiments and 16% (w/w) sucrose solution in D_2O for flotation experiments. The liposomes (Excytex, Zeist, The Netherlands) were also diluted 100 times in a 30% (w/w) sucrose solution in water. Each sample injection in flotation mode was followed by three 100 μL injections of 16% (w/w) sucrose in D_2O to remove any sample particles retained in the disc injection rim and capillaries. Results are expressed as the arithmetic mean of the number weighted modal particle diameter from 3 repeat experiments. The uncertainty is the combined repeatability and propagated standard uncertainty.

According to Stokes’ law, the time of sedimentation t of a perfect rigid sphere as measured by DCS is:



$$t = \frac{\alpha}{(\rho_p - \rho_f) D_p^2} \quad (1)$$

with:

$$\alpha = \frac{18\eta \ln\left(\frac{R_f}{R_0}\right)}{\omega^2} \quad (2)$$

where D_p is the total particle diameter, ρ_p is the total particle density, ρ_f is the fluid density and t is the sedimentation time between radii R_0 and R_f at angular frequency ω and fluid viscosity η .

The parameter α is computed by means of a particle calibrant of known size and density which is run under the same experimental conditions as the sample. The time of sedimentation t_c of the calibrant particles with diameter D_c and density ρ_c is:

$$t_c = \frac{\alpha}{(\rho_c - \rho_f) D_c^2} \quad (3)$$

The ratio of eqn (1) and (3) provides the expression for the diameter of the particle D_p :

$$D_p = D_c \sqrt{\frac{(\rho_c - \rho_f)t}{(\rho_p - \rho_f)t_c}} \quad (4)$$

If the size of the particle D_p is known, for example from independent measurements, the density of the particle ρ_p can be measured according to:

$$\rho_p = \rho_f + \frac{t}{t_c} \left(\frac{D_c}{D_p}\right)^2 (\rho_c - \rho_f). \quad (5)$$

Dynamic light scattering (DLS)

DLS measurements were performed on a Zetasizer Nano ZS (Malvern Instruments Ltd., Malvern, UK) equipped with a max 4 mW He-Ne laser, emitting at 633 nm. Samples were diluted as appropriate and measurements performed in disposable capillary cuvettes (DTS1070, Malvern Instruments Ltd., UK). Each measurement was performed at the non-invasive back-scatter angle (NIBS) of 173° at a temperature of 25 °C and preceded by a 3 min equilibration time. Particle size is expressed as the Z-ave value calculated with the cumulant method. Each value is the mean of four measurements.

Scanning electron microscopy (SEM)

Particle diameter and size distribution were measured by scanning electron microscopy (SEM). The microscope was an Inspect F SEM-FEG (Field Emission Gun) from FEI Company (Hillsboro, USA), with a beam diameter of 3 nm, equipped with EDAX microanalysis. The samples were sputter coated under vacuum with a thin layer (20–30 Å) of gold. The SEM micrographs were elaborated by the ImageJ32 image processing program. From 300 to 350 individual NP diameters were measured for each sample. The results are expressed as

the mean value of the distribution and the uncertainty as the standard error of the mean.

Small angle X-ray scattering (SAXS)

The PS NPs in suspension were filled into vacuum-proof borosilicate glass capillaries (Hilgenberg, Malsfeld, Germany), where a solvent density gradient was achieved by bringing together two mixtures of the sample with different densities. For the bottom of the capillary, a high density mixture was prepared with a fructose (Sigma-Aldrich, Missouri, USA) mass fraction of 67% and a corresponding solvent electron density of 433 nm⁻³, while on the top side of the capillary a low density preparation with the same volume fraction of sample (17%) was introduced, using an ethanol mass fraction of 78.5% with a solvent electron density of 280 nm⁻³. The scattering experiments were performed with the SAXS setup of Helmholtz-Zentrum Berlin²⁵ at the four-crystal monochromator beamline of PTB¹⁹ at the synchrotron radiation facility BESSY II (Helmholtz-Zentrum Berlin, Germany) with a photon energy of $E = (8000.0 \pm 0.8)$ eV. By means of the continuous contrast variation technique described elsewhere²⁰ scattering patterns at different suspending medium electron densities were collected during 60 s at a distance $L = (4539 \pm 1)$ mm from the capillaries using a vacuum-compatible Pilatus 1 M hybrid pixel detector (Dectris Ltd, Baden, Switzerland) with a pixel size of $d = (172.1 \pm 0.2)$ μm.²¹ The recorded scattering patterns were circularly integrated and converted to momentum transfer q using

$$q = \frac{4\pi E}{hc} \sin(\theta) \quad (6)$$

where h is the Planck constant, c is the speed of light and θ is half of the scattering angle. The obtained scattering curves were normalized to the exposure time, the solid angle, the sample transmittance and the incident photon flux, the last two measured by means of calibrated semiconductor photodiodes.

The diameter of the particles was determined by fitting the scattering curve measured at a solvent electron density of 290 nm⁻³ using a model equation describing polydisperse spherical particles with a Gaussian diameter distribution. An additive two-component background comprising a constant intensity and a term proportional to q^{-4} was assumed. The combined standard uncertainty associated to the particle diameter is dominated by the contribution arising from the fitting procedure, which is calculated with a confidence level of one standard deviation ($k = 1$) by examining the change in χ^2 when varying the diameter. The average electron density of the NPs was determined by analyzing the behaviour of the scattering intensity at zero-angle as a function of the solvent electron density¹⁵ whereas the associated measurement uncertainty is related to the size of the photon beam.

Tunable resistive pulse sensing (TRPS)

TRPS measurements were performed with a qNano instrument (Izon Science Ltd, Christchurch, NZ). Based on the Coulter principle, TRPS measures the reduction in ionic current across a pore on a stretchable membrane (NP100, supplied by Izon)



due to the temporary occlusion of the pore as a particle traverses it. As the exact geometry of the pore is not known, calibration particles (CPC100, nominal mean size of 118 nm, supplied by Izon) with known properties are measured at the same pore stretch as the sample and the relative values from the two measurements are compared.²² The blockade event signal is recorded by the instrument each time a particle traverses the pore. The magnitude of the measured blockade signal is directly proportional to the volume of the particle, allowing the determination of the particle diameter assuming spherical geometry. A minimum of 500 and 1000 events were recorded for each measurement of the calibrant and the sample respectively. Liposomes from Excytex (Zeist, The Netherlands) were diluted 4000 times in phosphate buffer (PBS, Sigma, St Louis, MO). The measurements were performed in duplicate for each of three different pressures. The current pulse signals were collected and exported for analysis using the Izon Control Suite software v2.2. The results were averaged and the uncertainty is expressed as the standard deviation of the values.

Results and discussion

A set of 5 monodisperse PS NPs with average diameters ranging from about 120 nm to 600 nm were successfully synthesized. Fig. 2 shows some representative SEM images of the particles. The particles appear spherical and highly monodisperse in diameter.

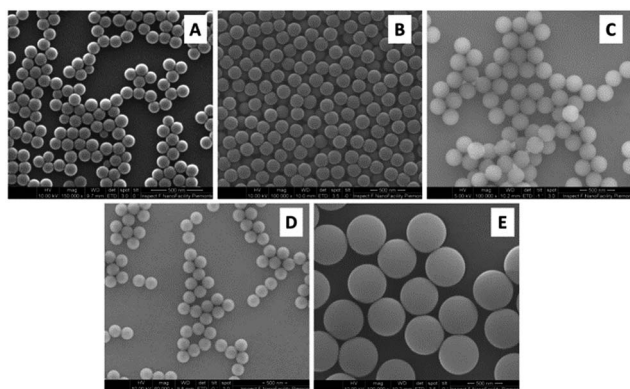


Fig. 2 Representative SEM images of PS NPs of samples (A) PS120, (B) PS200, (C) PS250, (D) PS300 and (E) PS600.

The average diameter of the particles as measured by SEM is summarised in Table 1. These are in close agreement with the particle diameters measured in water by SAXS using a spherical model, which are also summarised in Table 1. It is important to note that SAXS is a traceable technique, thus the obtained NP diameter can be related to the definition of the unit 'meter' in the International System of Units.²³ The traceability of SAXS arises from the precise determination of the oscillation period on the q -axis, which is calibrated using SI traceable values of the X-ray wavelength and the scattering angle.²⁴ The polydispersity of a particle sample affects SAXS accuracy, but typically, SAXS can measure particles with a polydispersity (defined as FWHM/mean) of up to 30% with high accuracy. In this work we take into account the polydispersity of the particles when computing the fit uncertainty, which is the major contribution to the measurement uncertainty. The agreement between SAXS and SEM results indicates that the SEM sample preparation and measurement conditions did not significantly affect the geometry of the particles or introduce artefacts. In fact, the sphericity values (derived from a model equation describing polydisperse spherical particles) used in the SAXS data evaluation were in good agreement with the micrograph observations. Unfortunately, SAXS could only be employed in a traceable way to determine the diameter of NPs with sizes up to 250 nm due to the limited q -range available in the experiment.

The size and density of the PS particles, modelled as perfect rigid spheres, were both measured by DCS. To measure the two parameters, two experiments were performed for each particle sample. One experiment involved the sedimentation of the particles through a sucrose gradient of average density 1.011 g cm^{-3} , while a second experiment involved the flotation of the particles through a gradient of average density 1.14 g cm^{-3} . The results of these experiments are summarised in Table S2 of the ESI.[†] The results of the two experiments were combined to produce a unique solution for the mode of the size distribution and the density of the particles. The number based size distributions as measured by DCS in the two modes are shown in Fig. 3 and the resulting diameter and density values are summarised in Table 1.

The size distributions measured in flotation mode appear noisier and broader than those measured in sedimentation (see Table S3 of the ESI.[†]), but did not exhibit the artefactual tail at smaller sizes that was observed in previous works.¹⁵ One reason for peak broadening is particle diffusion due to Brownian

Table 1 Diameter of the PS particles as measured by SEM, SAXS, DCS and DLS and density measured by SAXS and DCS

Name	SEM diameter ^a (nm)	SAXS		DCS		DLS diameter ^a (nm)
		Diameter (nm)	Density (g cm^{-3})	Diameter (nm)	Density (g cm^{-3})	
PS120	121	119.6 ± 1.6	1.049 ± 0.009	115.2 ± 4.1	1.050 ± 0.002	139
PS200	197	199.3 ± 3.0		188.4 ± 5.8	1.050 ± 0.002	215
PS250	250	249.2 ± 3.5		235.9 ± 6.9	1.051 ± 0.002	260
PS300	305	not measured	not measured	298.6 ± 8.5	1.051 ± 0.002	331
PS600	591	not measured	not measured	576 ± 16	1.047 ± 0.002	650

^a The estimation of the uncertainty for DLS and SEM is beyond the scope of the work. Precision was found to be $\sim 0.3 \text{ nm}$ for SEM and 1% for DLS.



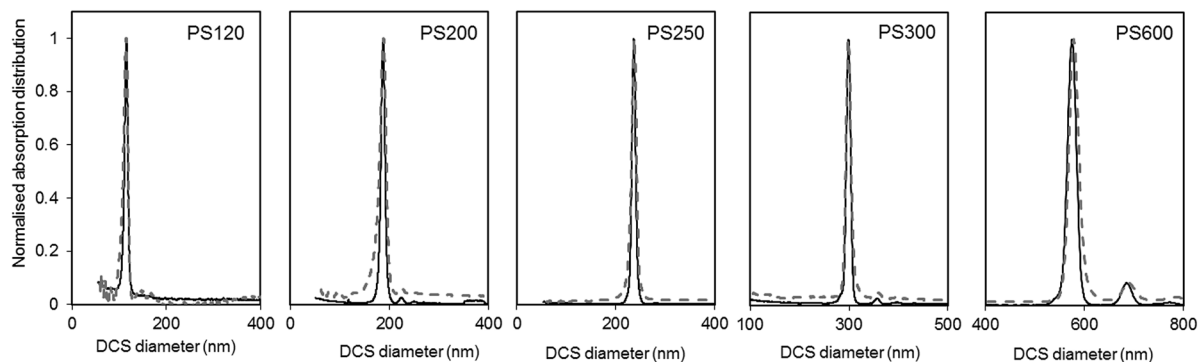


Fig. 3 Normalised light extinction weighted size distributions of the PS NPs as measured by DCS in sedimentation (continuous black line) and flotation (dash grey line) modes. The NPs are assumed perfect spheres of density as in Table 1.

motion, which is more significant for smaller particles and for longer sedimentation or flotation times. This effect is typically neglected for particles larger than 200 nm. In our experiments, sedimentation times were longer than flotation times (typically 10 minutes against 8 minutes for PS120), but the size distributions measured in sedimentation had lower polydispersity index (PDI) than those measured in flotation. For this reason, it is more likely that other experimental factors contribute more significantly to peak broadening. The different width of the size distribution could be the result of a lower resolution achieved with the set up for measurements in flotation. This may relate to the typically shorter flotation times with respect to sedimentation times, which is in part due to the distance between the edge of the disc and the position of the detector through which the samples float being shorter than the equivalent distance for sedimentation. The removal of the artefactual tail in the size distribution is the result of an optimised measuring protocol aimed at removing this artefact. The rim and capillaries of the flotation disc can retain part of the sample that is released with a delay or during later injections. This causes artefactual peaks in subsequently measured size distributions or a characteristic tail at lower sizes (longer sedimentation time). In this work every sample injection was followed by an injection of the particle dispersant (*i.e.* 16% sucrose in D_2O) to remove particles retained in the rim or capillaries. Although this procedure has the benefit of reducing artefacts in the size distributions, the injected volume should be minimised to limit changes to the density gradient. Because the dispersant has higher density than the rest of the sucrose gradient it accumulates at the edge of the disc. This causes the gradient to physically shift towards the centre of the disc. Thus, every injection of samples, calibrant particles or dispersant alters the gradient between the edge of the disc and the detector. This effect is, in part, compensated for by running a calibrant before each measurement and is considered negligible in this analysis.

The DCS modes of the particle size distributions were consistently smaller than the average diameters measured by SEM and SAXS, with differences of 5.6% or less (see Fig. 4). However, the agreement increases with increasing size of the particles. Discrepancies in the measured values, however, are expected as the two techniques do not measure the same type of

size.⁵ Besides, the expanded uncertainty on the measurement of the DCS diameter is between 5% and 6%. When the size distributions are compared with those measured by SAXS, we observe that the width of the distributions are very close in value, with PDIs measured by DCS in sedimentation and flotation mode being lower and higher those measured by SAXS respectively (Table S3 of the ESI†). This is an indication that both SAXS and DCS have similar resolution.

The high resolution of the DCS technique permits the discrimination of non-agglomerated particles from those that are agglomerated. Some samples show the presence of a minor population of doublets whose mode appears about 1.2 times larger than the main population mode.^{25–27} It should be noted, in fact, that the instrument interprets every agglomerate as a sphere with equivalent sedimentation time. This time depends on the forces due to gravity, buoyancy and drag in a centrifugal field, which will depend on the volume, shape and orientation of the particles or particle agglomerates. Furthermore, particle agglomerates can have different shapes and orientations, which means that the forces need to be averaged

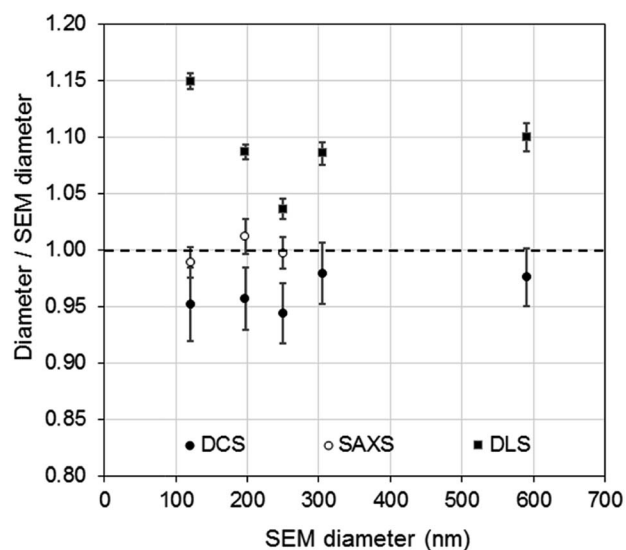


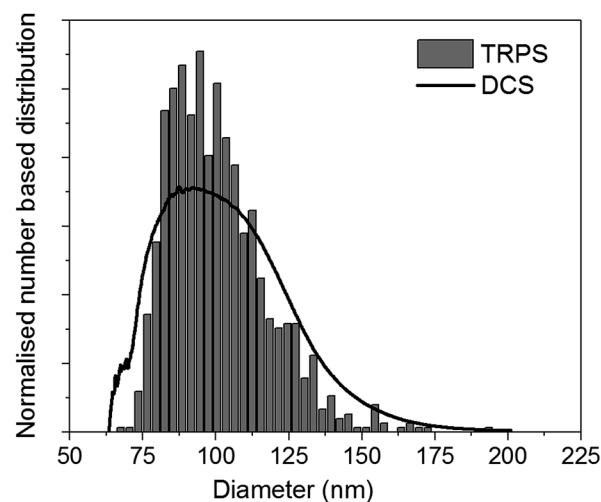
Fig. 4 Comparison of PS NP diameters as measured by DCS (●) SAXS (○) and DLS (■) with respect to the diameters measured by SEM.



The density of the particles measured by DCS was close to the density expected for bulk polystyrene material and showed high consistency around 1.050 g cm^{-3} . A more significant deviation, yet still smaller than 2%, is observed for sample PS600, which is also the sample with the largest diameter of the set of particles and with the broadest size distribution. Interestingly, the experiment using flotation mode produces a measurement of the size of the particles within 0.5% of the size measured by SEM when a density of 1.050 g cm^{-3} is used. The measurement

The complementary use of the SAXS and DCS techniques opens the possibility to analyse the size distribution and density of a broad range of particles with high certainty. For example,

The size distribution of the liposomes was also measured by DCS in flotation mode. In order to measure their density, this parameter was adjusted so that the mean of the number-based size distribution would result the same as that measured by TRPS. A representative number-based size distribution measured by DCS is plotted in Fig. 5 as a continuous line and shows very good agreement with the TRPS measurements. The resulting average density of the liposomes is 1.046 g cm^{-3} , with uncertainty of $\sim 16\%$, which is dominated by that on the density of the calibrant particles. Recent studies have shown that the density of these calibrants may be known with better accuracy than the nominal values declared by the instrument manufacturers.²⁹ This is an example of how well characterised and well described reference and calibrant materials can substantially reduce measurement uncertainty and allow more accurate measurements.



The DCS measurements presented in Fig. 5 were performed using a density gradient made of sucrose in water. It is also possible to perform the measurements using a gradient made of sucrose in D_2O to increase the difference in density between the particles and the sucrose solution. With this set up, the average density of the gradient increases from 1.096 g cm^{-3} to 1.14 g cm^{-3} , which leads to a reduction in flotation time of the liposomes from about 11 minutes to about 8 minutes. The sample was prepared by diluting the liposomes, initially in water, 100 times in 16% (w/w) sucrose in D_2O . The measurements resulted in a density of the liposomes of 1.096 g cm^{-3} . This value is higher than previously measured and reflects the fact that the molecules of D_2O may penetrate and adsorb onto the liposomes. If it is the relative changes in density of these materials that is measured, the choice of the set up used for the measurements is irrelevant. However, if the absolute value of the density is measured to optimise, for example, sample preparation procedures, then it is important to consider the medium where the experiments will be carried out. This is the case, for instance, in common procedures such as liposome separation by a sucrose density centrifugation approach.

We have shown that the DCS technique can be used to measure both the size and density of NPs by performing two measurements. We demonstrate this by using a set of polystyrene particles with different sizes and performing the measurements by first sedimenting, and second floating the particles through fluids of different densities. This approach provides results which are identical, within the uncertainties of the methods, to SAXS measurements of the same particles. While the particle size range accessible by SAXS is limited due to instability of the samples, *e.g.* due to sedimentation phenomena, the DCS technique could be applied with success to a broader range of particle sizes. We use polystyrene NPs as model particles, but

this approach can be easily applied to any particle with density between 1.2 g cm^{-3} and 1.03 g cm^{-3} . This includes a variety of particles of interest for medical applications, such as liposomes, polymersomes²⁴ and more generally polymer-based drug delivery systems.

We also show that DCS in flotation mode can be used to measure the density of NPs when the diameter is measured by a complementary technique and provide an example of application to liposomes.

Conflicts of interest

There are no conflicts to declare.

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Notes and references

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- ## Notes and references
- 1 C. Minelli, S. B. Lowe and M. M. Stevens, *Small*, 2010, **6**, 2336–2357.
 - 2 S. E. Krown, D. W. Northfelt, D. Osoba and J. S. Stewart, *Semin. Oncol.*, 2004, **31**, 36–52.
 - 3 W. J. Gradishar, *Expert Opin. Pharmacother.*, 2006, **7**, 1041–1053.
 - 4 P. T. Witte, P. H. Berben, S. Boland, E. H. Boymans, D. Vogt, J. W. Geus and J. G. Donkervoort, *Top. Catal.*, 2012, **55**, 505–511.
 - 5 N. C. Bell, C. Minelli, J. Tompkins, M. M. Stevens and A. G. Shard, *Langmuir*, 2012, **28**, 10860–10872.
 - 6 N. C. Bell, C. Minelli and A. G. Shard, *Anal. Methods*, 2013, **5**, 4591–4601.
 - 7 C. Minelli and A. G. Shard, *Biointerphases*, 2016, **11**, 04B306.
 - 8 R. Capomaccio, I. Ojea Jimenez, P. Colpo, D. Gilliland, G. Ceccone, F. Rossi and L. Calzolari, *Nanoscale*, 2015, **7**, 17653–17657.
 - 9 Ž. Krpetić, A. M. Davidson, M. Volk, R. Lévy, M. Brust and D. L. Cooper, *ACS Nano*, 2013, **7**, 8881–8890.
 - 10 A. M. Davidson, M. Brust, D. L. Cooper and M. Volk, *Anal. Chem.*, 2017, **89**, 6807–6814.
 - 11 C. Minelli, R. Garcia-Diez, A. E. Sikora, C. Gollwitzer, M. Krumrey and A. G. Shard, *Surf. Interface Anal.*, 2014, **10–11**, 663–667.
 - 12 S. M. North, E. R. Jones, G. N. Smith, O. O. Mykhaylyk, T. Annable and S. P. Armes, *Langmuir*, 2017, **33**, 1275–1284.
 - 13 C. J. Mable, R. R. Gibson, S. Prevost, B. E. McKenzie, O. O. Mykhaylyk and S. P. Armes, *J. Am. Chem. Soc.*, 2015, **137**, 16098–16108.
 - 14 D. Mehn, P. Iavicoli, N. Cabaleiro, S. E. Borgos, F. Caputo, O. Geiss, L. Calzolari, F. Rossi and D. Gilliland, *Int. J. Pharm.*, 2017, **523**, 320–326.
 - 15 R. Garcia-Diez, A. Sikora, C. Gollwitzer, C. Minelli and M. Krumrey, *Eur. Polym. J.*, 2016, **81**, 641–649.
 - 16 N. Kanokwan, R. Vinayak, A. F. Jeffrey and R. Vytas, *Nanotechnology*, 2013, **24**, 155701.
 - 17 M. Kamiti, D. Boldridge, L. M. Ndoping and E. E. Remsen, *Anal. Chem.*, 2012, **84**, 10526–10530.
 - 18 M. K. Brakke, *Arch. Biochem. Biophys.*, 1953, **45**, 275–290.
 - 19 M. Krumrey and G. Ulm, *Nucl. Instrum. Methods Phys. Res., Sect. A*, 2001, **467**, 1175–1178.
 - 20 R. Garcia-Diez, C. Gollwitzer and M. Krumrey, *J. Appl. Crystallogr.*, 2015, **48**, 20–28.
 - 21 J. Wernecke, C. Gollwitzer, P. Muller and M. Krumrey, *J. Synchrotron Radiat.*, 2014, **21**, 529–536.
 - 22 R. Vogel, G. Willmott, D. Kozak, G. S. Roberts, W. Anderson, L. Groenewegen, B. Glossop, A. Barnett, A. Turner and M. Trau, *Anal. Chem.*, 2011, **83**, 3499–3506.
 - 23 F. Meli, T. Klein, E. Buhr, C. G. Frase, G. Gleber, M. Krumrey, A. Duta, S. Duta, V. Korpelainen, R. Bellotti, G. B. Picotto, R. D. Boyd and A. Cuenat, *Meas. Sci. Technol.*, 2012, **23**, 125005.
 - 24 M. Krumrey, G. Gleber, F. Scholze and J. Wernecke, *Meas. Sci. Technol.*, 2011, **22**, 094032.
 - 25 C. Gollwitzer, D. Bartczak, H. Goenaga-Infante, V. Kestens, M. Krumrey, C. Minelli, M. Palmi, Y. Ramaye, G. Roebben, A. Sikora and Z. Varga, *Anal. Methods*, 2016, **8**, 5272–5282.
 - 26 D. Mehn, F. Caputo, M. Rosslein, L. Calzolari, F. Saint-Antonin, T. Courant, P. Wick and D. Gilliland, *RSC Adv.*, 2017, **7**, 27747–27754.
 - 27 L. Bondoc and S. Fitzpatrick, *J. Ind. Microbiol. Biotechnol.*, 1998, **20**, 317–322.
 - 28 N. Dingenouts, J. Bolze, D. Potschke and M. Ballauff, in *Polymer Latexes - Epoxide Resins - Polyampholytes*, ed. M. Ballauff, Springer-Verlag Berlin, Berlin, 1999, vol. 144, pp. 1–47.
 - 29 V. Kestens, V. A. Coleman, P.-J. De Temmerman, C. Minelli, H. Woehlecke and G. Roebben, *Langmuir*, 2017, **33**(33), 8213–8224.