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Hyperspectral-enhanced dark field analysis of individual and collective photo-responsive gold–copper sulfide nanoparticles†

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We used hyperspectral-enhanced dark field microscopy for studying physicochemical changes in biomaterials by tracking their unique spectral signatures along their pathway through different biological environments typically found in any biomedical application. We correlate these spectral signatures with discrete environmental features causing changes in nanoparticles' physicochemical properties. We use this correlation to track the nanoparticles intracellularly and to assess the impact of these changes on their functionality. We focus on one example of a photothermal nanocomposite, *i.e.*, polymer-coated gold/copper sulfide nanoparticles, because their performance depends on their localized surface plasmon peak, which is highly sensitive to environmental changes. We found spectral differences both in the dependence of time and discrete environmental factors, affecting the range of illumination wavelengths that can be used to activate the functionality of these types of nanoparticles. The presence of proteins (protein corona) and the increase in ionic strength induce a spectral broadening towards the NIR region which we associated with nanoparticles' agglomeration. In acidic environments, such as that of the lysosome, a red shift was also observed in addition to a decrease in the scattering intensity probably associated with a destabilization of the proteins and/or the change in the net charge of the polymer around the nanoparticles. We observed a loss of the photo-excitation potential of those nanoparticles exposed to acidic conditions in the <600 nm spectral range. In a similar manner, ageing induces a transitioning from a broad multipeak spectrum to a distinct shoulder with time (up to 8 months) with the loss of spectral contribution in the 450–600 nm range. Hence, a fresh preparation of nanoparticles before their application would be recommended for an optimal performance. We highlight the impact of ageing and the acidic environment on the responsiveness of this type of plasmonic nanoparticle. Regardless of the spectral differences found, polymer-coated gold/copper sulfide nanoparticles retained their photothermal response as demonstrated *in vitro* upon two-photon irradiation. This could be ascribed to their robust geometry provided by the polymer coating. These results should be useful to rationally design plasmonic photothermal probes.

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Introduction

Bio-nanotechnology aims at designing, engineering, and applying nanomaterials and nanotools for the diagnosis and therapy of diseases among other applications. Examples of such nanomaterials are those with unique photo-physical or magnetic properties for sensing, imaging, and photodynamic or radiation therapy,^{1–3} and those with thermo/magnetic-responsive properties that allow their remote manipulation (such as on demand opening or targeting),^{4–6} or their use for hyperthermia treatment of tumors.^{7–9} There are many materials with outstanding nanoscale control over the composition, size, and shape and they have potential biomedical applications.¹⁰ However, an extremely small portion of the



huge variety of nanostructures assembled in research laboratories are translocated to clinics. The reasons for the relatively poor translation from development to clinics are not only fundamental problems such as targeted delivery or biocompatibility, but also failed interaction between fabrication and application. Often there is a deficient biological (and toxicological) characterization of the materials, mostly due to a lack of full control over the nanomaterial physicochemical properties.^{11–15} Even for relatively simple questions, such as labelling of cells with nanoparticles (NPs), the relationship between the biological effect, *e.g.*, uptake efficiency of NPs, and physicochemical parameters such as the size of the NPs is not trivial to understand.^{12,16–19} Biomedical nanomaterials are dynamic systems changing their physicochemical properties upon their interaction with the physiological milieu. Changes in these properties can induce a performance loss. Therefore, it is strictly necessary to better elucidate the behavioral patterns of nanostructured materials in the physiological milieu and to correlate this with the physicochemical parameters of the materials such as their geometry, size, composition, and charge.^{12,13,20–22} Only in this way, the cellular response can be anticipated and the interactions of the materials with the cells and the cellular environments can be controlled.^{11,13,14} The final aim is to maintain the NP physicochemical properties in complex media (like the biological milieu) that are responsible for their functionality because they are likely to change, thus decreasing NP performance.

An example of the profitability of such a correlation is the use of plasmonic NPs for photothermal therapy (PTT).^{9,23} In recent years, photothermal therapy assisted with nanoprobe for cancer treatment has been extensively studied to improve the low selectivity, aggressiveness, and systemic/regional side effects of chemotherapy.⁵² One of the main advantages is the

sensitization of tumor cells to regular treatments such as radiation and chemotherapy.^{53–58} Heat also causes other positive effects such as alterations in the tumor blood flow and environment, and immune response activation.^{59,60} NP-based photothermal probes are designed to be excited at a specific plasmon resonance maximum to induce heat and damage of tumor cells. The plasmon resonance wavelength is highly sensitive to the NPs' geometry and the environment.^{24–26} Exposure of the NPs to the tumour cells induces uptake and clustering into vesicles of different compositions and pH values.^{27,28} This results in changes in the surface plasmon resonance wavelength, affecting absorption and heat production, and therefore has a clear impact on performance. This highlights the importance of performing appropriate characterization of nanomaterial interactions with physiological fluids, and biological barriers such as the plasma membrane or endocytic vesicles. This enables better designing and engineering of applicable NPs, which are robust to changes of environmental conditions, thus ensuring performance maintenance. Such performance is ultimately the major metrics to establish the clinical relevance of nanostructured materials.

Hyperspectral-Enhanced Dark Field Microscopy (HEDFM) is currently being implemented in nanomedicine as a promising method for the study of NP–environment interactions (see the scheme in Fig. 1).^{24,29–33} It provides *in situ*, real time, long-term, fast-reaction, and label-free optical observation of a wide range of nanomaterials while they interact with biological-based matrices. The interaction of the nanomaterial with light generates characteristic scattering profiles that act as spectral signatures for their *in vitro* tracking^{30,31,34–36} and also act as scatterers for advanced cardiovascular *in vivo* imaging.³⁷ In this way, changes in the physicochemical properties of the nanomaterials upon interaction with the environment can be

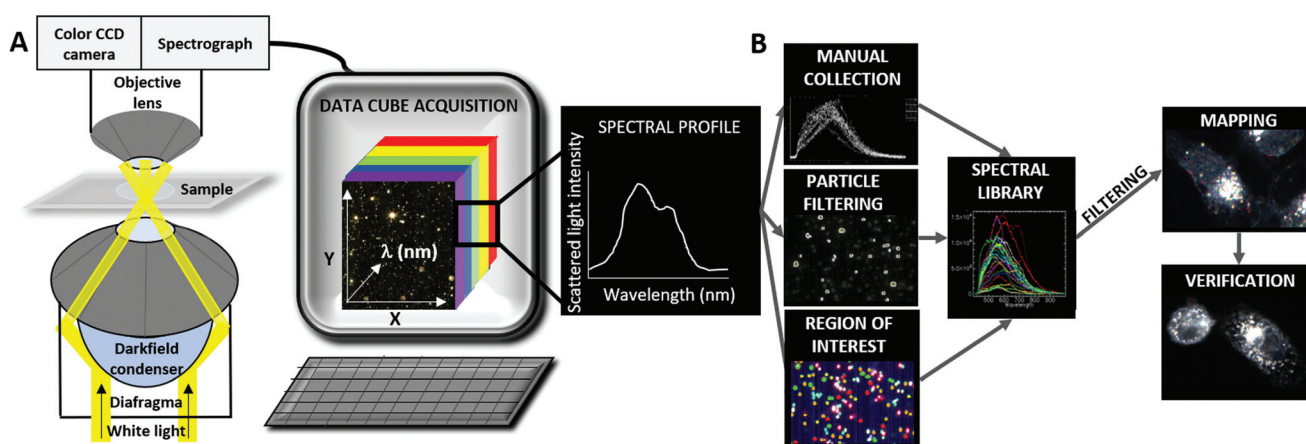


Fig. 1 Schematic representation of the HEDFM set-up and the data analysis process. (A) Imaging system that allows spatio-spectral data cube acquisition for the characterization of nanomaterials in the visible–NIR spectral range (400–1000 nm); (B) mapping workflow description: (i) first, the spectral library (SL) is created by collecting the spectra of interest from the HDC of NPs. The spectral profiles can be compiled manually by using software tools for NP filtering or analysis of regions of interest (ROIs); (ii) then, the SL of the NPs is filtered against the spectral data of cells to remove spectral coincidences; (iii) after that, the resultant SL is mapped in the HDC of the cells exposed to NPs using the Small Angle Mapper (SAM) algorithm; and (iv) finally, the SL of the NPs is mapped into the HDC of unexposed control cells using the same parameters to confirm no identification of NPs with the algorithm.³³



tracked over time.^{30,33,36,38–40} HEDFM allows for high resolution and long-term studies in live cells/tissues and optionally also under flow conditions if required. Live and real-time monitoring of cell-induced individual and collective changes in NPs is achieved due to negligible phototoxicity produced by the low power light source. HEDFM provides imaging of low contrast objects in a label-free manner with nanometer resolution, together with spectral and spatial information, engaging non-contact and remote sensing. Other advantages over other techniques such as electron microscopy include its non-invasive operability with simple sample manipulation under standard environmental conditions.²⁹ HEDFM best permitted the direct dynamic analysis of individual and collective particle evolution by tracking the scattering profiles of the nanomaterial in different media,³⁰ and particle–particle and particle–environment interaction patterns under different conditions such as pH values, polarity, cellular milieu, and over time.³³

Our aim is to study the effectiveness of HEDFM for sensing (probing) and tracking changes in the NPs' physicochemical properties potentially affecting cellular responses (*i.e.*, toxicity) or NPs' functionality. We selected polymer-coated gold/copper sulfide (Au/CuS) NPs as a candidate for HEDFM evaluation owing to their unique plasmonic properties^{41–43} and potential for two-photon excitation (2PE) photothermal therapy (PTT)^{44–47} in triple-negative breast cancer (TNBC) cells.^{48–50} The dynamic characterization of NP evolution in different biological media is especially relevant for plasmonic NPs. Their performance as photothermal probes or for sensing^{2,51} is attributed to the presence of light-induced localized surface plasmons which are highly sensitive to the environment, NP geometry, or NP aggregation state. These factors change during NP interactions with cells, and therefore, their optical properties and consequently also their performance can be affected.

Our results confirm the use of polymer-coated Au/CuS NPs as biocompatible, two-photon-assisted photothermal probes regardless of the changes in the NP geometry (composition and shape) induced by the cellular environment. We further demonstrate the effectiveness of HEDFM for the dynamic analysis of the evolution of individual and collective NPs based on their scattering signature generated upon particle–environment interactions. The analysis is performed by creating a spectral library of NPs based on their behavior when key environmental parameters are individually changed. Those key parameters are the ionic strength, pH, protein corona, solvent polarity, and time. These conditions are known to change the physicochemical properties of the NPs and are therefore potentially connected to toxicity or dysfunctionality.

Methods

Synthesis and polymer coating of Au/CuS nanoparticles

The NPs have been kindly provided by Huan Wang, Wenhua Li and Zhishan Bo, Department of Chemistry, Beijing Normal

University, Beijing, 100875, P. R. China. The synthesis procedures have been published previously.⁶¹ Afterwards, Au/CuS NPs were transferred to water using an amphiphilic polymer (poly(isobutylene-*alt*-maleic anhydride)-*graft*-dodecylamine, PMA). This methodology has been previously reported.^{62–64} Here, the number of polymer monomers per NP's surface area was experimentally optimized to the value of $R_{p/area} = 1000 \text{ nm}^{-2}$. The concentration of the NPs was determined by inductively coupled plasma mass spectrometry (ICP-MS) combined with transmission electron microscopy (TEM) to elucidate the NP size and morphology.⁶³ After the completion of the polymer coating process, the NPs were cleaned from the excess of empty polymer micelles using centrifugation. The samples were cleaned 3 times with Milli Q water after their centrifugation at 12 500 rpm for 20 min. The centrifugation conditions were also optimized to warrant the integrity of the NPs. The NPs were characterized by TEM, ICP-MS, dynamic light scattering (DLS), photon correlation laser Doppler anemometry (LDA), gel electrophoresis, and HEDFM. The NPs were filtered under sterile conditions using a sterile 0.2 μm syringe filter before their use *in vitro*. The final stock solution had a NP concentration of 1.08 μM . We refer the reader to the first section of the ESI (*cf.* Section 1†) for more exhaustive information on surface coating, concentration determination, and the physicochemical characterization of the NPs.

Cell culture

MDA-MB-231 human TNBC cells (ATCC® HTB-26)⁶⁵ were cultured and maintained in Dulbecco's modified Eagle's medium/Nutrient Mixture F-12, DMEM/F-12 (Gibco, 11330-057) supplemented with 10% fetal bovine serum (complete cell growth medium, GM), FBS (Sigma-Aldrich, F0804), and 1% penicillin/streptomycin (GE Healthcare Hyclone, SV30010). For cell passaging, the cells were washed with 1× phosphate buffered saline (PBS) (GE Healthcare Hyclone, SH30028.02) and exposed to trypsin phenol red (Gibco, 25300062) for 5–10 minutes. After that, trypsin was inactivated with GM and the cells were cultured at 1:10 dilution for subsequent cell maintenance. The cells were cultured at 37 °C under a 5% CO₂ modified atmosphere.

Cellular uptake of polymer-coated Au/CuS nanoparticles by confocal laser scanning microscopy

MDA-MB-231 TNBC human cells were seeded on glass coverslips and incubated for 24 hours in GM for proper cell attachment. Then, polymer-coated Au/CuS NPs at 5 nM in GM were added to the cells and incubated for 3 hours. After NP exposure, the supernatant was removed, and the cells were washed twice with PBS 1× to remove the non-internalized NPs. Moreover, 1 μM LysoTracker Red DND-99 (Life Technologies, L7528) solution in PBS 1× was added to the cells and incubated for 20 minutes at 37 °C, 5% CO₂. Finally, the cells were washed with PBS 1× and placed in GM for imaging. Images were acquired with a 543 nm He/Ne laser, using a Leica TCS SP2 laser scanning confocal microscope (Leica Microsystems, IL, USA). Image processing was performed with Fiji.⁶⁶



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selected for the final mapping. The subsets were tested using a parameter of 0.1 radians for the mapping procedure. Recognized spectra were converted into false-color images. The non-identified spectra were not classified. The mapping process is shown in Fig. 1B and further explained in *cf.* ESI Section 6.† The same procedure was followed for the HDCs of polymer-coated Au/CuS NPs under acidic conditions (pH 4) simulating the lysosomal intracellular fluid, obtaining the SLs (*cf.* ESI Section 3†). The two SLs of NPs in the simulated cellular fluids (neutral and acidic) were mapped against the MDA-MB-231 human TNBC cells exposed to 15 nm polymer-coated Au/CuS NP solution for 3 hours. The relative abundance of the pixels mapped per cell for the two SLs was calculated using the ROI tool, analyzing a total of 14 cells. For the verification of the spectra mapped, the two SLs were mapped in the HDC of the cells unexposed to NPs, confirming that no spectrum was matched (*cf.* ESI Section 6†) and that all the spectra belonged to the NPs.

Statistical analysis

All data are expressed as the mean $\pm$ standard error of the mean (SEM). Significance between data sets was determined by a one-way ANOVA test followed by Dunnett's post-test, with an asterisk for p -values ≤ 0.05 . Three independent sample sets were run for each experiment ($n = 3$). "One-way ANOVA with Bonferroni's post-test was performed using GraphPad Prism version 5.01 for Windows, GraphPad Software, San Diego California USA, <http://www.graphpad.com>".

Results and discussion

Bio-physicochemical characterization of polymer-coated Au/CuS nanoparticles

The NPs selected for this work comprise a spherical gold (Au) nanoparticle anchored to a semiconductor domain, copper sulfide (CuS). The final size of the hybrid structure is 25 nm. CuS nanostructures are easy to synthesize at low costs and the NPs show good conductivity, small particle size, and particular optical properties.^{42,67–70} CuS absorbs in the near infrared (NIR) region and is well-suited for photo-responsive applications. The plasmonic properties of Au strongly enhance the local electromagnetic field and therefore the absorption capacity of CuS.^{42,69,71} The combination of both nanomaterials results in the improvement of the optical properties compared to their individual counterparts. The improvement in the absorption ability of the resultant nanomaterials is interesting for photo-responsive applications such as PTT where the energy absorbed is transformed into heat.^{7,8} The absorption enhancement of the NPs is translated into a lower energy required from the laser irradiation for PTT.^{62,70,72,73}

Initially hydrophobic Au/CuS NPs (Fig. 2A "Chloroform" and *cf.* ESI Section 1.1†) were coated with an amphiphilic polymer, PMA (*cf.* ESI Section 1.2†), to render the NPs hydrophilic and thus providing them colloidal stability in aqueous solution.⁷⁴ The water transfer process reshaped the morphology of the NPs (Fig. 2A "Water" and Fig. S1-Section 1.3†). Despite this structural change, the NPs maintained their

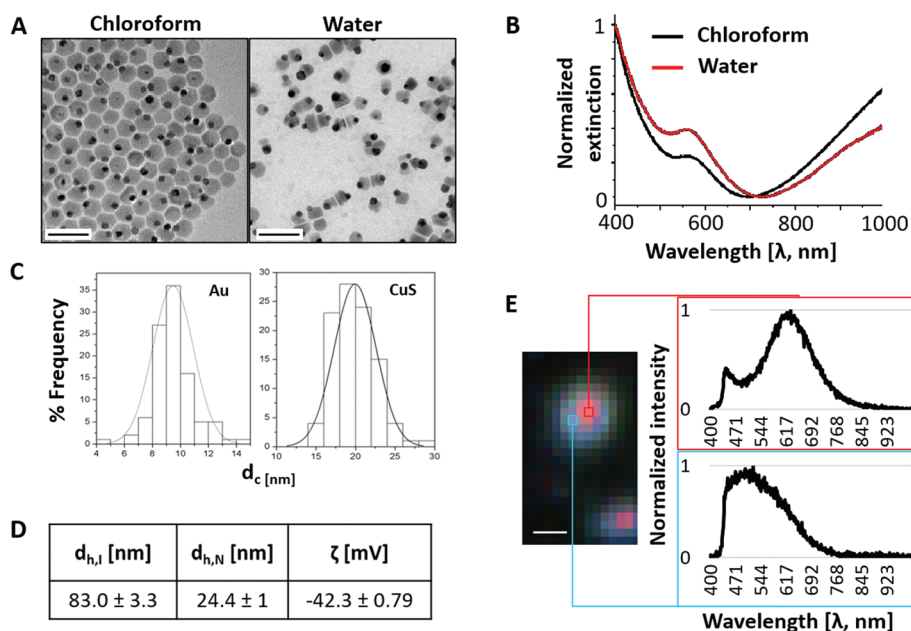


Fig. 2 Characterization of polymer-coated Au/CuS nanoparticles. (A) TEM images of Au/CuS NPs before (left) and after (right) their overcoating with an amphiphilic polymer and subsequent transfer to the aqueous phase. Scale bar: 50 μ m. (B) Normalized extinction spectra of the particles before (red) and after (black) polymer coating and water transfer; (C) histograms showing the size distribution (diameter) of Au and CuS parts as determined from TEM images; (D) determination of the hydrodynamic diameter of NPs in water by the intensity ($d_{h,I}$) and number ($d_{h,N}$) using DLS; and (E) dark field image showing the scattering properties of the NPs and the relevant spectral profiles of a single particle. The maximum intensity for each pixel has been set up to 1.



optical behavior and their NIR absorption (Fig. 2B) even after days in PBS 1× solution (Fig. S3-Section 1.4†). To measure the size, two different histograms were produced considering that once in water, the Au NPs were normally localized as satellites of the CuS domains. The resulting inorganic core diameters as determined by TEM were 9.4 ± 1.4 nm and 19.9 ± 2.6 nm for the Au and CuS nanostructures, respectively (Fig. 2C). Fig. 2D shows the NPs' hydrodynamic diameter and zeta potential values (plots shown in *cf.* ESI Section 1.5, Fig. S4†). Fig. 2E shows the improved optical response of Au/CuS required for two-photon PTT when comparing the extinction spectra of Au, CuS, and Au/CuS NPs, respectively. The electrophoretic mobility of the NPs was also tested in comparison with control Au NPs of 10 nm modified with phosphine (*cf.* ESI Section 1.5, Fig. S5†).⁷⁵ All the results confirm that the narrow size distribution of the NPs after their water transfer is maintained, despite the structural changes. The resulting NP concentration in solution was determined by combining the results obtained from TEM and ICP-MS (*cf.* ESI Section 1.3†).⁶³

Additionally, we characterized the scattering properties of polymer-coated Au/CuS NPs through HEDFM (Fig. 2F and *cf.* ESI Section 1.6, Fig. S6†) showing two characteristic spectral profiles in the 600 nm (612–646 nm, red arrows, Fig. S6B-Section 1.6†) and 500 nm (461–582 nm, blue arrows, Fig. S6B-Section 1.6†) regions in individual NPs. The peak in the red region may correspond to the Au domain responsible for the electromagnetic field enhancement, whereas the peak in the blue region shows a multipoint band with lower intensity. This may correlate with the thin edges of the CuS nanoplate that might be more efficient at absorbing light than at scattering it. Remarkably, HEDFM can image single NPs smaller than 50 nm.^{76,77} To elucidate whether this was a single-particle or a collective effect, we mapped the two characteristic spectra found in the HDC of polymer-coated Au/CuS NPs in water (the original dispersion medium) (see Fig. S7-Section 1.6†). The pattern found in most of the light spots indicates a similar spectral behavior in water. We refer to the ESI, Section 1,† for further information related to the characterization of the nanomaterials.

Interaction of polymer-coated Au/CuS nanoparticles with cells

To characterize the impact of the NPs' biological environment on their functionality as photo-responsive probes, their interaction with MDA-MB-231 TNBC human cancer cells was probed. We selected this cell model as it originates from a type of breast cancer that is resistant to conventional treatments and presents poor patient prognosis due to the lack of three surface receptors: progesterone, estrogen and HER2.⁴⁸ TNBC represents an aggressive cancer type with a high recurrence rate and invasiveness.^{48–50} Thus, there is a clinical need of finding novel therapeutic strategies. In recent years, NP-assisted PTT has been studied as an alternative^{7,8} or complementary therapy to conventional cancer treatments characterized by a limited efficacy due to low-specificity systemic side effects.^{57,78}

The polymer-coated Au/CuS NPs were exposed to the cells after which we studied the internalization, and the intracellular fate, toxicity and therapeutic value of the NPs. The NPs were taken up and were found colocalizing with the lysosomes after 3 hours cellular exposure (Fig. 3A and *cf.* ESI Section 2.1†). In general, NPs' uptake can follow diverse mechanisms depending on the NP size, shape, and charge.^{21,79–81} Most pathways involved vesicles maturing along their pathway. This maturation is specially characterized by a progressive decrease in the pH. Lysosomes present the highest acidic conditions (pH 5–4).^{28,82,83} They are a common destination for internalized NPs.^{82–85} To probe the potential cytotoxicity of the NPs, a fluorometric metabolic assay was employed. Viable cells metabolize the non-fluorescent product into a fluorescent metabolite; therefore, cell viability is correlated with an increase in fluorescence. The results (Fig. 3B and *cf.* ESI Section 2.2†) indicate that the polymer-coated Au/CuS NPs do not induce acute cytotoxicity for MDA-MB-231 cells at NP concentrations up to 30 nM. Even though the cellular viability at 60 nM of NPs is close to reaching the LC50 threshold (concentration of the NPs responsible for killing half of the cell population), the concentration range of ≤ 15 nM used in this work correlates with 90% cell viability. Our results indicate that polymer-coated Au/CuS NPs are as biocompatible as other reported CuS NPs.^{42,70,73,86,87} Copper-based NPs suffer from fast oxidation, regardless of their superior synthesis yielding control over the atomic structure and photothermal properties. As a result, toxic copper ions are leaked to the environment and contribute to killing cells in an uncontrolled manner.^{62,88,89} This effect has also been reported for other photothermal NPs.^{90–93} Copper plays a key role in human physiology, controlling different enzymatic processes.^{94,95} *In vivo* metabolism of CuS NPs has been reported.^{94,96} The results showed a size-dependent hepatic and/or renal excretion.^{94,96} The slow dissociation rates of Cu ions from the NPs, combined with a metabolic elimination of Cu ions, is responsible for maintaining Cu homeostasis and preventing toxicity.^{94,96} Considering these results, we would expect similar degradation behavior for our NPs.

To validate the two-photon assisted photothermal activity of polymer-coated Au/CuS NPs, the cells were treated with the NPs and were irradiated with 2PE (830 nm). 2PE has several advantages over conventional one-photon excitation: (i) pinhole-free sectioning for the analysis of thick samples and 3D imaging reconstruction and (ii) deeper tissue penetration that empowers this technique for surgical applications.^{97–99} The increased photothermal effect is correlated with an increase in membrane permeability and cellular damage. We used DAPI as a positive indicator for hyperthermia-driven toxicity because it only penetrates cells upon membrane disruption. Because laser irradiation of NP treated cells caused a significant increase in the fluorescence signal (Fig. 3C (*cf.* ESI Section 2.3†)), we can confirm the photothermal activity of the NPs. In Fig. 3C, we show the nucleus of treated cells (indicated by a red circle) progressively labelled with DAPI (blue fluorescence signal) at 1 and 5 minutes after 2PE. However, in *cf.*



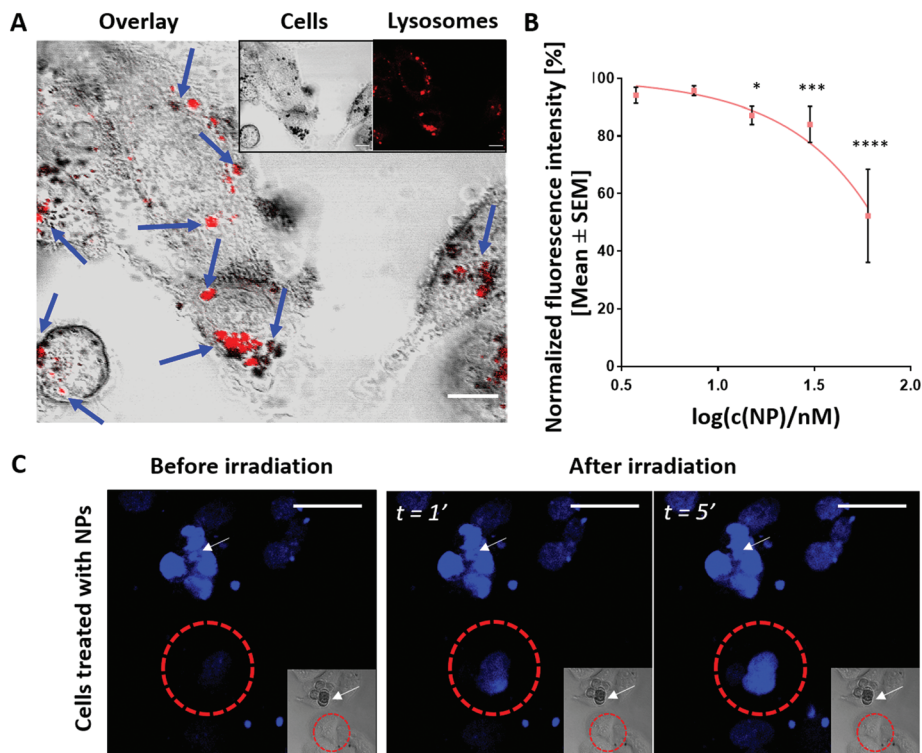


Fig. 3 Interaction of polymer-coated Au/CuS nanoparticles with MDA-MB-231 TNBC human cells. (A) CLSM images presenting internalized NPs intracellularly confined in the lysosomes (red fluorescence signal) after 3 hours of incubation (see blue arrows). Bright field (cells) and fluorescence (lysosomes) single images are provided (insets); (B) viability assay of cells exposed to different concentrations of NPs; (C) CLSM images of cells taken before and after PTT with two photon emission at 830 nm (red circle). White arrows highlight the presence of dead cells with a blue fluorescence signal (DAPI). The insets show the bright field image of the cells. Scale bar: 10 μ m.

ESI Section 2, Fig. S9B and S9C,[†] we observed that the fluorescence signal appears in the nucleus just 15 seconds after NP irradiation. The photothermal effect appears to be highly localized because only cells carrying the irradiated NPs were affected by the heat (see the ESI, *cf.* Section 2, Fig. S9B and S9C[†]). Cells non-treated with the NPs and irradiated with the laser maintained their viability (see the ESI, *cf.* Section 2, Fig. S9A[†]). These preliminary results indicate that polymer-coated Au/CuS NPs may possess improved photothermal properties as compared to CuTe NPs.⁶²

Dark field imaging and hyperspectral analysis of polymer-coated Au/CuS nanoparticles interacting with dynamic biological environments

As mentioned in the Introduction, it is crucial to correlate the physicochemical properties of NPs with their biological behavior to maintain their functionality and to predict the responses of both systems (NPs and cells). In this work, we hypothesize the use of HEDFM to track changes in the physicochemical properties of the NPs caused by the environment which are susceptible to interfere with their performance. We selected plasmonic NPs because their therapeutic performance as photo-responsive probes depends on their spectral characteristics. We used HEDFM to track the NP physicochemical changes caused by cellular/biological environments.

The spectral information of the polymer-coated Au/CuS NPs was first characterized in physiologically relevant environments known to affect the NPs' morphology and with different refractive indexes (RI) ranging from 1.35 to 1.6.¹⁰⁰ Changes in the refractive index are known to alter the plasmon peak, and as a result, the scattering profile recorded by HEDFM. We selected the following media: (i) water (*ca.* pH 7, RI 1.33);¹⁰¹ (ii) PBS solution characterized by a high ionic strength (*ca.* pH 7, 140 mM NaCl, RI 1.33¹⁰¹) known to affect colloidal stability because of NPs' charge screening;^{102–104} (iii) a simulated extracellular and early endosome fluid (GM pH 7, RI 1.35¹⁰¹) with high ionic strength and content on macromolecules responsible for the formation of a dynamic protein corona around the NPs' surface affecting cellular interactions;^{105–108} and (iv) a simulated intracellular lysosomal fluid (GM pH 4, RI 1.6¹⁰⁰) where NPs frequently locate and which also affects the colloidal stability and the structure's integrity.^{79–81,109} We also tracked the optical changes in the NPs over time. NPs' post-processing in the biological environment is a fact affecting colloidal stability and causing NPs' reshaping.¹¹⁰

Fig. 4 shows the DFIs (insets) and the spectral signature acquired for polymer-coated Au/CuS NPs in the different dispersion media, *i.e.* water, PBS, GM pH 7, and GM pH 4. NPs in water (original NP dispersion medium, *ca.* pH 7, RI 1.3), shows a spectral profile with a maximum scattering peak at 556 nm.



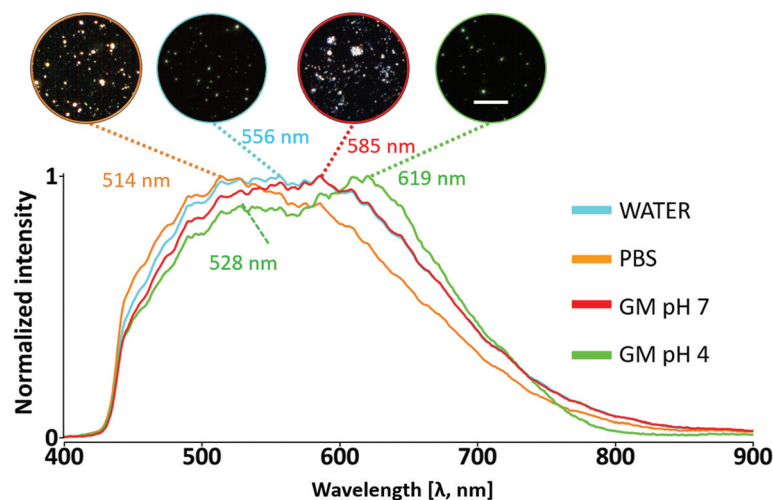


Fig. 4 Spectral characterization of polymer-coated Au/CuS nanoparticles exposed to different environments. The mean spectral profiles of NPs exposed to water (blue), PBS (orange), GM at pH 4 (green), and GM at pH 7 (red) are plotted. The mean spectra were calculated as an average from 9275, 6318, 9520 and 10 754 spectra. The numbers show the wavelength of the maximum intensity of scattered light. The insets show the dark field images of the NPs under analysis. Agglomerates were not included in this analysis. Scale bar: 10 μm .

NPs transferred to high ionic strength (PBS, same pH and RI value as water) exhibit less spectral broadening, resulting in a narrower band towards smaller wavelengths compared to water likely due to the presence of salts affecting the polymer at the interface. However, when they were transferred from water to the simulated extracellular/early endosome fluid with a neutral pH and containing biomolecules (GM pH 7 in Fig. 4), the shape of the curve was maintained as in water but with a band maximum at 585 nm. This can be ascribed to an increase in particle size due to the interfacial protein corona because the RI and pH values are maintained.¹¹¹ The adsorption of serum proteins (transport proteins and opsonins, among others) onto the surface of the NPs forms a complex corona, affecting the size, aggregation state, and interfacial composition of the nanomaterials, creating a distinct “biological identity”.¹¹² Agglomerates are also visible in the DFI (white areas in the red-labelled inset of Fig. 4 and ESI *cf.* Section 3, Fig. S10†). Nonetheless, they were not included in the analysis. NPs’ agglomeration induces plasmon coupling, altering the overall spectral responses and patterns.^{26,113,114} In the simulated lysosomal fluid (“GM pH 4” in Fig. 4), a pronounced shoulder appears at higher wavelengths upon acidification and increase of the medium’s RI. Moreover, its light scattering profile shows two maxima, one at 528 nm and a more pronounced one at 619 nm. The acidic pH may affect the protonation status at the interface and consequently the stability of NPs.¹¹⁵ These results confirm that we can accurately identify spectral changes with enough sensitivity using this methodology as reported elsewhere.^{30,32,36}

We also performed single particle spectral analysis of individual pixels randomly selected from the DFIs (ESI *cf.* Section 3, Fig. S10†) in the different environments. When comparing the spectra, the NPs in the original dispersant (water) and in neutral GM present a more consistent signature, while the NPs in PBS and acidic GM are more heterogeneous. Then we took

the same HDC from Fig. S10† and sorted the light spots by the number of pixels, establishing different size ranges grouped by colors (ESI *cf.* Section 3, Fig. S11 and S12†).

We observed a homogeneous pattern in the behavior of the NPs in the different environments. The increase in the light spot size is correlated with a red shift of the maximum scattering peak inter- and intra-medium (ESI, *cf.* Section 3, Fig. S13†). The formation of the protein corona is a common behavior for NPs interacting with a biological system. The proteins change the physicochemical properties of NPs; for example, the hydrodynamic diameter increases, and the composition and charge vary at the interface.¹¹⁶ Therefore, we performed a more detailed analysis. Fig. 5 summarizes the mean scattering profile of NPs because of exposure to protein-rich media. Clearly visible agglomerates of different sizes lead to a heterogeneous multi-peak spectral profile. The presence of proteins (“ROI 1, 2”) and increase in ionic strength (“ROI 4”) induce spectral broadening (ESI *cf.* Section 4.1, Fig. S14A†) compared to the response in the acidic environment (“ROI 3”). This broadening (“ROI 1”) in the NIR region (*ca.* 650–850 nm) occurs at the level of the whole agglomerate (Fig. 5) as well as at the level of individual pixels from the same agglomerate (ESI *cf.* Section 4.1 Fig. S14†). Similar spectral behavior has already been reported.^{32,36,117–119} Big agglomerates resulting from the presence of proteins in the media (“ROI 1”) exhibit a strong scattering variability that affects the signal intensity and spectral profile of each pixel (ESI *cf.* Section 4.1, Fig. S14†). Comparable results (ESI *cf.* Section 4.2, Fig. S15 and S16†) were found for other agglomerates (“GM pH 7”) which were excluded in previous analysis (Fig. 4, and ESI, *cf.* Section 4.1, Fig. S12 and S13†). The mean spectral profile for the NPs exposed to pH 4 (“ROI 3”) showed a different pattern including a red shift associated with agglomeration.^{32,36,120,121} A decrease in the scattering intensity in the range of *ca.* 450–600 nm was also observed, suggesting a prominent



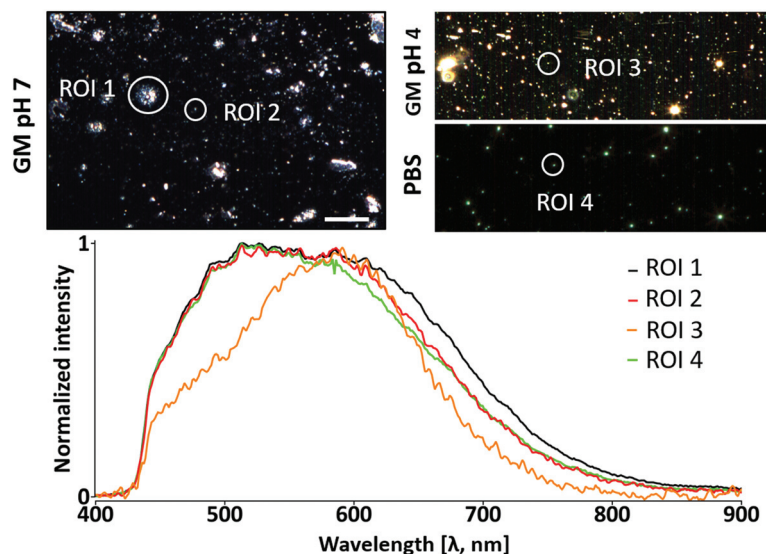


Fig. 5 Spectral changes of polymer-coated Au/CuS nanoparticle agglomerates upon protein corona formation. Mean spectral profiles of agglomerated (ROI 1) and individually dispersed NPs with protein corona at neutral (ROI 2) and acidic pH (ROI 3). NPs without protein corona are presented in ROI 4. DFI with the NPs under study are marked with white circles (top). The HDCs from Fig. 4 were analyzed in this plot. Scale bar: 10 μm .

change in their physicochemical properties. The destabilization of the proteins and/or the change in the net charge of the PMA polymer may be responsible for this different optical response in acidic media (lysosomal conditions).^{116,122} The spectral studies in biological media indicate a loss of photo-excitation potential of the NPs exposed to acidic conditions in the <600 nm spectral range. This effect is further analyzed in the following sections.

Spectral profile progression of polymer-coated Au/CuS nanoparticles in biological medium over time

We used a hyperspectral imaging system to characterize the NPs from HDCs (Fig. 6 and ESI *cf.* Section 5.1 Fig. S17†) obtained at $t = 0$ (HDC analyzed in Fig. 4 and 5) and after 2, 5, and 8 months of exposure in biological medium (GM pH 7, RI 1.35) to analyze the progression of the spectral profile over time. Fig. 6A shows the stabilization/homogenization of the mean spectral profiles of the false-colored yellow ROIs shown in Fig. 6B for the different time points. We observe the transitioning from a broad multipeak spectrum to a distinct shoulder with time. The spectral differences could be associated with a lowering in the size of the NPs as observed in the TEM images after 8 months (Fig. 6C). This is supported by the disappearance of the scattering signal at higher light spot sizes (ESI *cf.* Section 5.1 Fig. S17 and S18†). The same pattern of narrowing and loss of spectral contribution in the 450–600 nm range was observed under acidic conditions ($t = 0$ months) compared to the other environments (Fig. 5 and ESI *cf.* Section 3 Fig. S10 and S12†). These results prove that the time and pH dramatically alter NPs' geometry and that these changes happen in the dispersant but also in cellular environments. Spectra of cells exposed to NPs (Fig. 7 – “GM pH 4”) were similar for intralysosomal polymer-coated Au/CuS NPs.

The mean spectral profiles corresponding to different pixel ranges (ESI *cf.* Section 5.1 Fig. S17†) show the same profile pattern, indicating low variability in the spectral analysis at each time point. Within the same time point, the maximum scattering peak red shifts with increasing light spot size (ESI *cf.* Section 5.1 Fig. S17†). However, we could not elucidate if a red shift occurred because of the multipeak spectra. The range of the band maximum intensity goes from *ca.* 500 to 620 nm and corresponds to the range observed in the mean spectral profile of the NPs in this environment (Fig. 4 and 5).

The spectral losses of the polymer-coated Au/CuS NPs is associated with ageing, thus indicating NP transformation and/or degradation after 2 months that could affect their functionality. Hence, a fresh preparation of the NPs before PTT would be recommended for an optimal performance. Zhao *et al.* reported a similar spectral trend in silver NPs upon dissolution in hydrogen peroxide enriched medium monitored over time.³⁴ Hydrogen peroxide is found in cells because of homeostatic and pathological responses.¹²³

Tracking changes of the spectral profile of polymer-coated Au/CuS nanoparticles during intracellular processing

To predict the behavior of the polymer-coated Au/CuS NPs inside living cells, we created a SL of the object (*i.e.*, NPs in different environments), which is used to cross-reference the sample (*i.e.*, cells exposed to NPs) to search for matches. If matched, the HEDFM system sorts, labels the pixels, and provides a mapping image.³³ To start with the analysis, a reference SL for the NPs in the different environments (neutral, pH 7 and acidic, pH 4) was acquired (Fig. 7 and ESI *cf.* Section 6.2 Fig. S19†). Each SL was validated by mapping them on the corresponding NP sample (HDCs) and we overlaid the resulting false coloured NP image with the NP DFI to confirm colo-



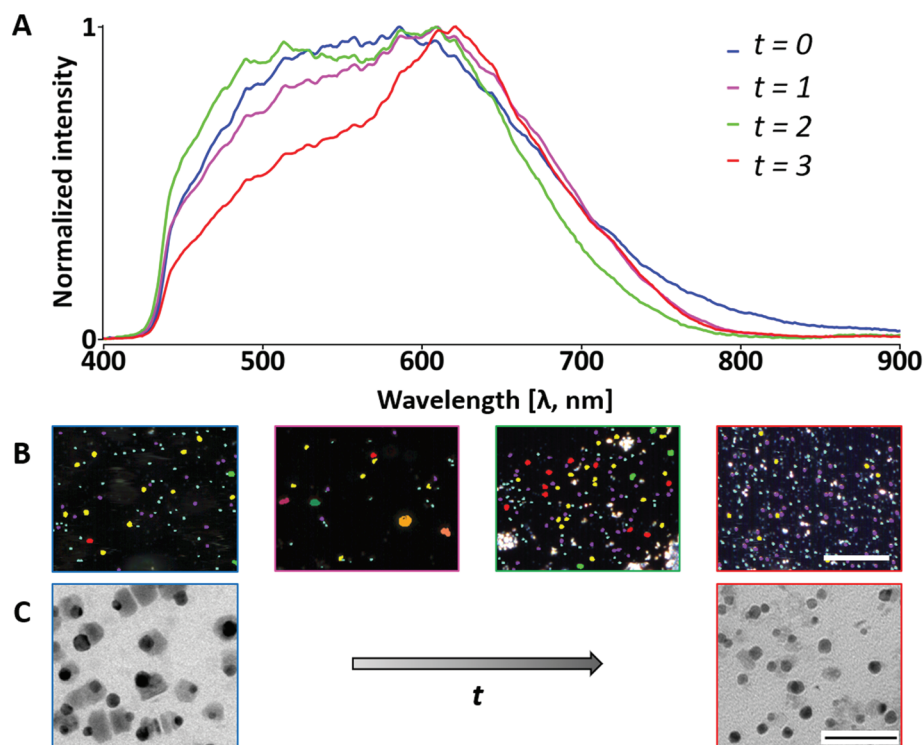


Fig. 6 Spectral analysis of polymer-coated Au/CuS nanoparticles up to 8 months. (A) Mean spectral profiles of a subpopulation of NPs in neutral GM (yellow false-colored ROIs in DFIs) at different time points: $t = 0$, after 2 months ($t = 1$), 5 months ($t = 2$), and 8 months ($t = 3$); (B) DFIs of the NPs at the described time points with the population sorted by light spot sizes (pixels) presented with false-colored ROIs. Scale bar: 10 μm ; (C) respective TEM images of the NPs at $t = 0$ and $t = 3$, where prominent changes in the morphology can be observed. Scale bar: 50 nm.

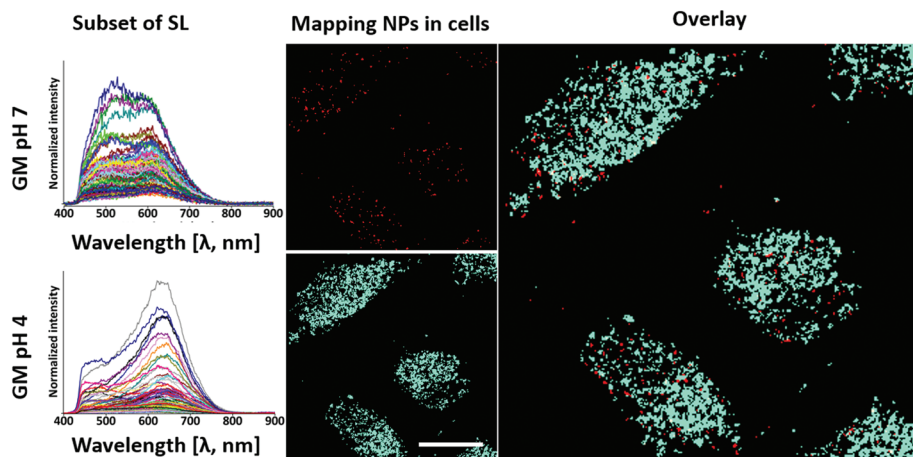


Fig. 7 Spectral mapping and intracellular localization of polymer-coated Au/CuS NPs. Left column: subsets of the SLs of NPs exposed to GM pH 7 and pH 4 used in the spectral mapping procedure; middle column: false-colored mapping image of the NPs exposed to pH 7 (red pixels) and pH 4 (blue pixels); right column: the overlay of the two spectral mappings (red and blue pixels) is shown for extracellular/early endosome and lysosomal particle detection, respectively. Scale bar: 10 μm .

calization (ESI *cf.* Section 6.2 Fig. S19A†). The spectral data from the control cells (without NPs) are filtered out from the SLs to remove possible similar spectra. We also mapped the cells not exposed to NPs and where no NPs were found (ESI *cf.* Section 6.2 Fig. S20†). In this way, we ensure that the spectral profiles compiled in each SL used for cell mapping will only relate to the NPs. MDA-MB-231 human breast cancer cells were

incubated with 5 nM polymer-coated Au/CuS NP solution for 3 hours and the HDC was taken for mapping. Fig. 7 shows false coloured images of the NPs whose spectral profile matches with the SL. Red pixels fit with the spectral profile of the NPs in the neutral (pH 7) environment, whereas blue pixels fit the acidic (pH 4) environment. The overlay image from both mappings indicates the different locations of the



NPs in acidic *versus* neutral environments, corresponding to different cellular environments.

Fig. S19B (ESI *cf.* Section 6.2†) includes the overlay with the DFI of the cells, indicating intracellular or pericellular location. It is worth mentioning that the number of pixels mapped under acidic conditions is much higher (*ca.* a power of ten) than that in the neutral environment (Fig. 8 and ESI *cf.* Section 6.3 Fig. S21†). It is important to note that not all NPs are mapped. We can only map those NPs whose spectral profiles coincide with the SLs selected for mapping, and we cannot correlate the number of pixels with the number of NPs. We could not, for example, track changes of the NPs upon their interaction with the plasma membrane. However, the results obtained previously (Fig. 3) together with these findings support the conclusion of

the lysosomal location of the NPs. Most importantly, we could track the progression of the NPs from neutral to more acidic environments during their internalization, typical of endocytosis.^{80,81,84,124,125} Once we obtained the spectral signatures of the NPs under the different cell-related conditions, changing their physicochemical properties like inducing agglomeration, reshaping or formation of a protein corona, among others, the spectral profiles were the input in the HEDFM system for recognition inside cells. In this way, we can track and predict the cellular behaviour of the NPs.

Conclusions

Biomedical nanomaterials are dynamic systems changing their physicochemical properties upon their interaction with the physiological milieu. Changes in these properties can induce a performance loss. Therefore, it is strictly necessary to elucidate the behavioral patterns of nanostructured materials in the physiological milieu and to correlate this with physicochemical parameters of the materials such as their geometry, size, composition, and charge. This is the only way to anticipate the cellular response, to control the interactions of the material with the physiological environment, and to manufacture robust nanomaterials maintaining their functionality.

HEDFM provides semiquantitative information on how the NP spectra change in a physiological environment. HEDFM imaging provides diffuse reflectance spectra from light-scattering samples and, therefore, contributes to the scope of the NP-environment knowledge at different levels. These are: (i) NP-solvent interactions such as the effect of ionic strength, pH, protein corona and agglomeration state, (ii) NP-time interaction based on ageing and geometrical evolution, and (iii) NP-cell interaction focusing on internalization dynamics and cellular fate.

Our 25 nm polymer-coated Au/CuS NPs facilitate HEDFM imaging. Hyperspectral sensitivity provides detailed spectra compared to multispectral acquisition, emphasizing alterations in NPs. At each pixel, HEDFM collects information on how their spectral signature changes over the whole visible spectrum in different biological environments. We identified unique spectral signatures of polymer-coated Au/CuS NPs under the influence of individual biological parameters that are associated with changes in their morphology, thus, confirming that this methodology has enough sensitivity to accurately detect spectral shifts due to small changes in the biological environment.

Polymer-coated Au/CuS NPs are photothermal agents with improved biocompatibility. We combined HEDFM with CLSM to investigate the NP scenario after exposing TNBC cells to polymer-coated Au/CuS NPs for 3 hours. The NPs are internalized by the cells and accumulated intracellularly, specifically in the lysosomes. At that time and NP dose, no cellular toxicity was observed; therefore the cells were two-photon irradiated and successfully treated with PTT. Regardless of spectral deviations inside the cells, the performance was validated accurately. However long-term effects on the spectral profile of the

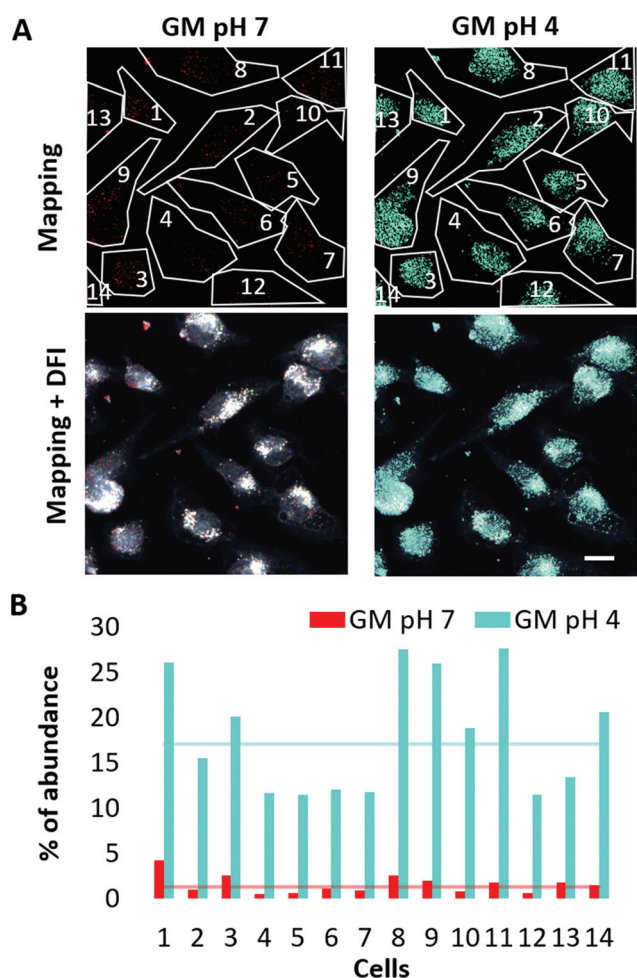


Fig. 8 Relative abundance of polymer-coated Au/CuS NP pixels mapped along internalization. Based on the mapping results from Fig. 7 showing NPs inside the cells at pH 7 and 4, we calculated the relative abundance for each condition, distributed by cells. (A) The upper figures show the different cell ROIs (ROI 1–14). The lower images are the merged image of the pixels mapped inside the cells with the DFI. For each ROI, we quantified the total number of pixels (see the ESI, Section 6.2 Fig. S20†). (B) Graphical representation of the calculated relative abundance of pixels mapped per cell and cellular conditions. Scale bar: 10 μ m.



NPs inside the cells are required to warranty a lack of dysfunctionality.

Thus, combining plasmonic NPs with HEDFM allows (i) evaluating correlations of nanomaterials spectral features in biological matrices and (ii) tracking the dynamic cellular process at the single-cell and single-NP levels but also collectively with the highest resolution (up to 20 nm). Within this work, the spectral change is directly correlated with the alteration of one individual environmental parameter (pH, polarity, protein corona, ionic strength, or time). The concomitant effect of several parameters, as occurring in most physiological fluids, will require further work acquiring the corresponding spectral libraries.

We can conclude that the spectral analysis provides the information of intracellular NP behavior to optimize its functionality for nanomedical applications.

Abbreviations

2PE	Two-photon excitation
Au	Gold
Au/CuS	Gold/copper sulfide
CLSM	Confocal laser scanning microscopy
CuS	Copper sulfide
DFI	Dark field image
GM	Complete cell growth medium
HCl	Hydrochloric acid
HDC	Hyperspectral data cube
HEDFM	Hyperspectral-enhanced dark field microscopy
HER2	Human epidermal growth factor receptor 2
HSI	Hyperspectral imaging system
ICP-MS	Inductive-coupled mass spectrometry
LDA	Laser Doppler anemometry
LSPR	Localized surface plasmon resonance
NIR	Near-infrared
NPs	Nanoparticles
PBS	Phosphate buffered saline
PMA	Poly(maleic- <i>alt</i> -anhydride) modified with dodecylamine
PPDT	Plasmonic photodynamic therapy
PPTT	Plasmonic photothermal therapy
PTT	Photothermal therapy
RI	Refractive index
ROI	Region of interest
SAM	Small angle mapper
SEM	Standard error of the mean
SL	Spectral library
TEM	Transmission electron microscopy
TNBC	Triple-negative breast cancer

Author contributions

PZP: investigation, methodology, visualization, and writing – original draft. BP: investigation, visualization, and writing –

original draft. DT: investigation and visualization. MGS: investigation. WJP: funding acquisition and writing – review and editing. PRG: conceptualization, funding acquisition, methodology, project administration, supervision, writing – original draft, and writing – review and editing.

Conflicts of interest

The authors declare that they have no competing interests.

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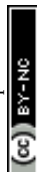
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