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1	Microorganisms-based monodisperse microcapsules: encapsulation
2	of the fungicide tebuconazole and its controlled release properties
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23	Abstract: The design of an ideal monodisperse microcapsulation system, which could					
24	meet the need for prolonged and better control of drug administration, is a great					
25	challenge. Herein cyanobacteria cells served as a natural environmentally-friendly					
26	wall material to encapsulate the fungicide tebuconazole (TEB), and then					
27	urea-formaldehyde (UF) resins were automatically coated on it via electrostatic					
28	interactions. By this means, monodisperse TEB-PCC@UF microcapsules were					
29	achieved, which not only can effectively control the drug release rate but also depress					
30	the initial "burst effect" to some degree. A bioactivity experiment showed that					
31	TEB-PCC@UF microcapsules authentically prolonged the antifungal effects, and					
32	were very efficacious in controlling wheat powdery mildew compared with the					
33	commercial formulation.					
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34 35	Keywords:					
	Keywords: Microencapsulation, cyanobacteria, electrostatic interactions, tebuconazole; wheat					
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45 Introduction

Wheat is the most widely cultivated and important food crop in the world as staple 46 crop for about 35% of the human population.¹ Wheat powdery mildew, caused by 47 Blumeria graminis f. sp. Tritici, has been recognized as the main and widespread 48 disease of wheat in the growing areas leading to significant yield decrease and 49 economic loss worldwide.²⁻⁴ The use of pesticides is essential for preventing and 50 controlling it. Tebuconazole (TEB) as a broad-spectrum, high-efficiency, and 51 low-toxicity triazole systemic fungicide is effective against rust, powdery mildew, net 52 blotch, root rot, scab, smut and seed-borne diseases on a variety of cereal crops.⁵ The 53 most common formulations of TEB are emulsifiable concentrates and wettable 54 powders due to its inferior water-solubility (0.032 g/L at 20 °C). There are still serious 55 problems in these formulations due to the immediate release of the active ingredients, 56 which greatly reduce TEB efficacy. Therefore, excessive quantities of TEB are needed 57 to compensate such losses, also resulting in a severe economic loss. Meanwhile, it is 58 harmful to human health as well as the environment. Thus, how to enhance the 59 efficacy of TEB and minimize its environmental impacts is always an important issue. 60 This problem has stimulated interesting in developing new formulations to improve 61 62 them. Especially, microencapsulation formulation is one choice for it.

63 Microencapsulation of pesticides is a versatile technology for controlled drug 64 release in which numerous synthetic⁶⁻¹⁰ and natural materials¹¹⁻¹⁷ have been widely 65 employed as pesticide carriers. Many achievements have been made in the field of 66 pesticide encapsulation for controlled release, and encapsulated pesticides have

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exhibited controlled-release properties, provided enhanced efficacy and reduced the impacts.⁶⁻¹⁷ However, these single-walled microcapsules cannot control the release of the core materials effectively, and lead to high initial burst release because they were often made of thin polymeric membranes. The double-walled microspheres with a drug-encapsulating particle core surrounded by a drug-free shell layer,¹⁸ often exhibit a reduction in the initial burst release and better controlled release properties¹⁹⁻²² as compared to single-walled ones.

Microorganisms such as yeast can be harnessed as biocompatible and 74 biodegradable reservoirs and have been successfully applied in the encapsulation of 75 essential oil,²³ flavor,^{24,25} antioxidant^{26,27} and pharmaceuticals.²⁸⁻³⁰ The cell wall and 76 the plasma membrane of the yeast cell make them an attractive encapsulation 77 matrix.³¹ Prokaryotes, unicellular cyanobacteria have unique highly differentiated 78 internal membrane systems. Like other Gram-negative bacteria, cyanobacteria such as 79 Synechocystis sp. strain PCC 6803 (PCC) have a cell envelope consisting of a plasma 80 membrane, peptidoglycan layer, and outer membrane,³² thus making them an ideal 81 microencapsulation wall material. 82

Urea-formaldehyde (UF) resins via in situ polymerization, in which the capsule wall is formed by condensation polymerization on the phase interface, have been employed as the capsule wall, and attracted attention due to its simplicity, low cost and excellent mechanical strength of the resulting capsules.³³⁻³⁶ In situ polymerization has many advantages, such as feasible size controllability and adjustable shell thickness.

89	Herein, we report a controlled drug-delivery system based on UF modified PCC
90	cells in which TEB are loaded into algae cells. In addition, the uncoated algae cells
91	drug-release system was used for comparison to investigate the release property.
92	Specifically, PCC cells used in this work as appropriate candidates for TEB release
93	system have three distinguishing features: (i) Their surface is negatively charged, so
94	they could adsorb and take up positively charged UF prepolymers via electrostatic
95	interactions in acidic solution. (ii) The groups on cell wall are mainly carboxyl,
96	hydroxyl and amine, which are responsible for hydrogen bond formation with TEB.
97	(iii) They are essentially spherical and exhibit narrow size distribution. The uniform
98	property of PCC enables them to be an intelligent drug delivery systems to develop
99	monodispersed microcapsules, which are critical for the precise manipulation of the
100	loading levels and the release kinetics of encapsulated substances. ³⁷

101 Experimental

102 Materials

Technical grade tebuconazole (98.5% purity) was kindly supplied by Jiannong 103 jiangsu Agrochemical & Chemical Co. Ltd. (China). Tebuconazole (45%, WP, 104 105 Elite) was obtained from Bayer Co. (Kansas City Mo.). Isopropanol (99.5%), 106 formaldehyde (37%), urea and triethanolamine were obtained from Sinopharm Chemical Regent Co. (China). PCC cells were obtained from the Department of 107 108 Biology, Shanghai Normal University (China). Double distilled water was used in the experiment. All chemicals were analytic grade and were used without further 109 purification. 110

111 Fabrication of TEB-PCC

112 Cyanobacteria used in the experiments were Synechocystis sp. strain PCC 6803 113 (PCC). The PCC cells were centrifuged, washed with deionized water 3 times, and 114 spray dried at 220 °C. The dried cells (1.0 g), TEB (0.2 g) and absolute ethanol (400 115 mL) were added into 500 mL capped erlenmeyer flasks under continuous shaking for 116 24 h at 30 °C. Then, the cells were centrifuged for 1 min at 10000 rpm, quickly 117 washed three times with small amounts of absolute ethanol-water mixture (5:95, v/v) 118 and freeze dried for 48 h. The TEB-PCC was obtained.

119 Preparation of Urea-formaldehyde Pre-polymer

Recrystallized urea (120 g) and 37% formaldehyde solution (225 mL) were mixed 120 121 in a 250 mL three-neck round-bottomed flask equipped with a mechanical stirrer at 122 room temperature. When urea was dissolved, the pH value of the resultant solution 123 was adjusted to 8~9 by adding suitable amount of triethanolamine, then the solution was gradually heated to 70 $^{\circ}$ C and maintained at that temperature for 1 h. At the end 124 125 of the reaction, this urea-formaldehyde pre-polymer resin was cooled and diluted with 126 distilled water to be 500 mL of UF resin solution. The resin concentration was 0.42 g mL^{-1} . 127

128 Fabrication of TEB-PCC@UF

TEB-PCC (4 g), prepolymer solution (1 g) and double-distilled water (5.0 mL) were mixed by stirring at 200 rpm at 60 $^{\circ}$ C, and the pH of the mixture was adjusted to 1.5~2 with 1% HCl solution. The reaction was continued with a stirring rate of 500 rpm for 4 h. After 4 h, the urea-formaldehyde polymer network is formed at the

TEB-PCC interface. The resultant microcapsules were filtered and washed withdistilled water for three times and dried in a vacuum oven for 20 h.

135 In Vitro Drug-release Study

The different TEB samples containing about 20 mg of TEB were weighted and 136 dispersed in 200 mL of ethanol-water mixture (50:50, v/v) with shaking at100 rpm, 137 25 $^{\circ}$ C, which was used as the release medium in order to dissolve TEB. 2.0 mL of the 138 139 suspension was removed for analysis at given time intervals with a syringe followed by 10 min centrifugation at 10000 rpm. The precipitates from centrifugation and the 140 141 same volume of fresh release medium were returned to the flasks to keep the 142 composition of suspension unchanged. The extracted medium was sufficiently diluted with release medium, and analyzed by UV/Vis spectroscopy at a wavelength of 220 143 144 nm. Blanks containing no TEB and three replicates of each sample were used for each series of experiments. 145

Bioassay Experiments

The bioactivities of TEB-PCC@UF and commercial formulations of TEB on wheat 147 powdery mildew which is one of main wheat diseases were conducted on 2-3 leaf 148 stage of wheat seedlings. Two formulations were dissolved in water to prepare 100 149 150 mg/L of the mother liquors and then diluted into 2.5 ppm, 5 ppm, 10 ppm, 20 ppm, 30 151 ppm and 40 ppm TEB with 0.1% (w/w) Tween 80 solution. The plants were treated homogeneously in a spraying cabin with the pesticides 24 h, 48 h, and 72 h before 152 153 pathogen inoculation. Wheat was inoculated with pathogens Erysiphe graminis (by shaking spore powder over the uninfected plants), and grown in a greenhouse under 154

155	conditions of 18 °C, at 70% relative humidity, with 12 h light and were used for
156	testing after 4, 8 and 12 days, respectively.
157	Characterization
158	The morphology of the samples was characterized by field emission scanning
159	microscopy (FESEM, Hitachi S-4800). Particle size and zeta potential were measured
160	using a Zetasizer Nano-ZS-90 (Malvern Instruments). Fourier transform infrared
161	(FT-IR) spectra were recorded with a Nicolet Magna 550 spectrometer using KBr
162	method. The concentrations of TEB in the adsorption and release experiments were
163	determined by UV-vis spectrophotometer (UV-2000, UNICO (Shanghai) Instruments
164	Co., Ltd.).

Co., Ltd.).

Results and discussion 165

Characterization of microcapusles 166

167 Scheme 1 schematically illustrates the reduction of initial burst and improvement of efficacy on target fungicide of two drug-delivery systems, TEB-PCC@UF and 168 TEB-PCC. In the former one, TEB release is doubly controlled by the PCC cell shell 169 and the UF layer sequentially. The double-walled TEB-PCC@UF system can exhibit 170 a reduction in the initial burst release and better controlled release properties. For the 171 172 TEB-PCC, the PCC cell shell can control the drug diffusion with sustained-release 173 behavior only.

For the TEB-PCC@UF, the TEB-PCC spheres were effectively covered with UF 174 175 due to the electrostatic interaction. As shown in Figure S1, the Zeta potential of 176 TEB-PCC spheres, UF prepolymers, and TEB-PCC@UF were -40.2 mv, 4.32 mv, and

-3.98 mv, respectively, indicating that the TEB-PCC spheres have been successfullycoated with UF.

179 The FT-IR spectrum (Figure 1) was employed to further prove the presence of UF on TEB-PCC spheres surface. As shown in Figure 1d and 1e, the FT-IR spectra of UF 180 resins and TEB-PCC@UF closely match to the characteristic peaks of the N-H 181 stretching vibration at 1543cm⁻¹, C=O stretching vibration at 1650 cm⁻¹, and a C-H 182 stretching vibration at 1389 cm⁻¹. The peaks at 1242 cm⁻¹ and 3357 cm⁻¹ are assigned 183 to stretching vibrations of C-N bonds, and O-H bonds, respectively. This indicates that 184 the UF resin shell was formed on the surface of TEB-PCC. Furthermore, it is 185 noteworthy to mention that the characteristic adsorption bands of PCC (Figure 1a) and 186 TEB (Figure 1b) were not observed at TEB-PCC@UF (Figure 1e) due to the sealing 187 and penetration resistance of the UF shell resins fully filled with TEB-PCC. 33,38,39 188

The FT-IR spectrum of the TEB-PCC systems was similar to the spectrum of the 189 PCC cells (Figure 1a and 1c), whilst the IR absorption bands of TEB significantly 190 decreased, nearly disappeared. This observation suggests that the main bands of TEB 191 192 was 'hidden' by the interaction with the inner wall groups of PCC cell components and TEB molecules are rather located inside the PCC cells. The above results 193 correlate well with Shi and Paramera's²⁶⁻²⁸ in which the encapsulation of resveratrol, 194 195 chlorogenic acid and curcumin in yeast cells was studied respectively, and the disappearance of the characteristic IR absorption bands of the substances in the 196 197 microcapsules was attributed to the encapsulation into cells.

198 FESEM and dynamic light scattering (DLS) revealed that PCC cells were almost

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199 monodisperse microspheres (Figure 2a) and the average diameter of PCC is relatively uniform (1.474 µm, Figure S2 in the Supporting Information). Figure 2b shows a 200 201 FESEM micrograph of the PCC after adsorption of TEB molecules (TEB-PCC). No 202 apparent difference can be observed compared to Figure 2a, although TEB-PCC 203 contains a large number of TEB molecules. Moreover, the adsorption kinetics studies of TEB onto PCC showed that the absorption equilibrium was achieved after 24 h. As 204 205 obtained from adsorption isotherms (Figure S3 in the Supporting Information), the 206 maximum adsorbed amount was about 20.1 mg/g at an equilibrium concentration of 207 approximately 500 mg/L. Consequently, the number of TEB molecules encapsulated in PCC cell sphere is 7.99×10^7 (see the Supporting Information S4). From the FESEM 208 images (Figure 2b, c and d), it clearly depicts that TEB-PCC@UF spheres possess a 209 210 roughly spherical structure with an average diameter of 1.773 µm, which perfectly replicate the morphology of the cells. Meanwhile, a uniform thin layer with a 211 212 thickness of around 0.15 µm completely covers the whole outer surface of the 213 TEB-PCC microspheres, which correlate well with the normal FT-IR spectra of 214 TEB-PCC@UF.

To characterize the sustained-release effect, we systematically investigated the release behavior of TEB from the TEB-PCC and TEB-PCC@UF systems in media of ethanol/water mixture (v/v, 1:1). As shown in Figure 3a, the amounts of released free TEB reach about 94.6% in less than 53 h (Figure 3a), and Figure 3b and 3c clearly presented that both systems exhibit sustained-release properties. The TEB-PCC system takes about 76 h to release 72% of TEB into the solvent, which might be

221	attributed to the fact that the plasma membrane, peptidoglycan layer, and outer
222	membrane of the PCC cells act as effective barriers preventing the premature release
223	of the TEB from TEB-PCC system. ^{23,24} In addition, it has been reported ⁴⁰⁻⁴² that the
224	hydrogen bonds interaction between the carrier and the active ingredient can also
225	affect the release of active ingredient from the matrix. A high energy of interaction
226	would result in a slower release of the active ingredient. Consequently, a large number
227	of hydroxyl and amine groups on the PCC cell (Figure 1a) act as proton donors for
228	hydrogen bonds, and the nitrogen atoms and hydroxyl groups of TEB act as acceptors.
229	Thus, the hydrogen bond interaction between TEB and the carrier may also contribute
230	to the slow-release of TEB from TEB-PCC system.
231	For the TEB-PCC@UF system, the TEB release time and rate was obviously
232	decreased compared to TEB-PCC. The release amount only reaches 42% after 76 h.
233	This finding indicates that the UF layer plays an important role and serves as an
234	effective diffusion barrier during the controlled-release process. Furthermore, the t_{50}

respectively. These results can be concluded that the addition of PCC cells is beneficial to slow down the release of TEB from TEB-PCC microcapsules. Moreover, the TEB-PCC@UF system has a much better controlled drug-release property than the TEB-PCC.

The major problem in a controlled release system is the obvious initial burst during which a great amount of drug releases, resulting in an acutely high concentration and

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release lose control.^{43,44} As shown in Figure 3, there was an initial burst in the release profile of the free TEB, and it was significantly suppressed in the single-walled TEB-PCC and double-walled TEB-PCC@UF systems. Especially in the double-walled TEB-PCC@UF, its initial burst time is the shortest, suggesting that the double-walled encapsulation of TEB not only can prolong the release time but also depress the initial "burst effect" to some degree.

249 Drug release studies

Finally, the release mechanisms of TEB were investigated for the TEB-PCC and 250 TEB-PCC@UF microcapsules. The release process should involve two steps: i) The 251 252 bulk solution diffuses into the microcapsules and the core TEB dissolves in it. ii) The 253 dissolved TEB molecules spread out. It is expected that at the early release stage the 254 TEB concentration within the microcapsules is close to saturation, and is sustained until the core TEB dissolve completely.⁴⁵ During this period, the permeability of the 255 microcapsule shell is the determining factor controlling the release rates, explaining 256 why the release rate decreases as the microcapsule wall thickness increases.⁴⁶ Here, 257 we analyzed the kinetic release data of the TEB from microcapsules by applying the 258 empirical equation⁴⁷ 259

260

$$M_t / M_0 = K t^n \tag{1}$$

where M_t/M_0 is the percentage of TEB released at time *t*, *K* is a constant that incorporates characteristic of the macromolecular network system and the active ingredient, and *n* is a diffusional parameter, which is indicative of the transport mechanism. The values of *K* and n obtained from the initial 60% of TEB released are

265	presented in Table 1. According to correlation coefficients, we can deduce that the					
266	release profiles of TEB from single-walled TEB-PCC and double-walled					
267	TEB-PCC@UF microcapsules fit well to the empirical equation. The n values are					
268	0.387 and 0.536 for TEB-PCC microcapsule and TEB-PCC@UF microcapsule, which					
269	are very close to 0.5 reported for the diffusion mechanism of spherical formulations in					
270	the ref 47 and 7. For spheres, when corrected for geometry of the device					
271	(microparticle), the diffusion parameter changes to a value of 0.43 when Fickian					
272	diffusion occurs in a spherical monolithic matrix. Value of n close to 0.43 are					
273	indicative of Fickian diffusion. ⁴⁷ The larger n (0.536) may be ascribed to the swelling					
274	of polymer coated carrier ^{42,48} or the interaction between TEB and UF resins induces					
275	the deviation from Fickian diffusion. ⁴⁹ These results suggested that the release					
276	mechanism of TEB from the single or double-walled microcapsules is Fickian					
277	diffusion, that is, the release is diffusion-controlled.					

278 Bioassay Experiment

To further evaluate the controlled release properties of the TEB-PCC@UF 279 microcapsules, we assessed its protective and persistent effects against wheat 280 powdery mildew. For the test of protective effects (Figure 4a, b), the plants were 281 282 inoculated with pathogen of the plant disease for 24 h after spraying with the TEB-PCC@UF microcapsules or the commercial formulation of TEB at doses 283 ranging from 2.5 to 40 mg/L. It was found that the control efficacies of two 284 formulations were increased with the increasing of TEB concentration sampling at the 285 286 4th, 8th and 12th day after TEB application (Figure 4a, b). However, compared to the

commercial formulation, the TEB-PCC@UF microcapsules exhibited excellent

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commercial formulation, the TEB-TCC@OF interocapsules exhibited excenent
control efficacy against wheat powdery mildew, particularly in the concentrations
ranging from 10 to 40 mg/L. This suggested that the TEB-PCC@UF microcapsules
can provide significantly protection effect on wheat. For example, at 40 mg/L
concentration, the control efficacies of TEB-PCC@UF microcapsules at intervals
were 95.75%, 88.25% and 83.75%, but that of the commercial product were merely
91.00%, 75.25% and 51.00% respectively. The preferable protective effect can be
ascribed to the controlled-release ability of the TEB-PCC@UF microcapsules, which
evidently improved the long-term bioavailability of TEB.
For the test of persistent effects, the plants inoculated for 24, 48, or 72 h after spray
different formulations of TEB at the above concentrations was also studied; and the
control efficacies were assessed at the 4th, 8th and 12th day after inoculation,
respectively (Figure 4). TEB-PCC@UF microcapsules also showed a superior
persistent effect due to its advantageous controlled-release property. For example, for
the 72 h after TEB application, the TEB-PCC@UF microcapsules, especially at high
concentrations, exhibited a good control efficacy in 12 d after inoculation. At 40 mg/L
concentration, the control efficacy still reached 80.75% in 12 d after inoculation.
However, the control efficacy of the commercial formulation of TEB only reached
52.25%. Obviously, the TEB-PCC@UF microcapsules had remarkable advantages in

controlling TEB release compared to the commercial formulation of TEB.

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310	In summary, we have successfully developed an efficient cyanobacteria cells-based
311	controlled drug-release system by using UF as a coating shell to modify TEB-loaded
312	PCC cells. Compared to the TEB-PCC system without UF, the TEB-PCC@UF system
313	not only can effectively control the drug release rate but also depress the initial "burst
314	effect" to some degree. The UF layer plays an important role and serves as an
315	effective diffusion barrier during the controlled-release process. Furthermore, the
316	control efficacy of TEB-PCC@UF system against wheat powdery mildew remained
317	over 80% in 12 d after inoculation, due to the slow and persistent release of the active
318	components from the system. In contrast, the control efficacy of the commercial
319	formulation at the same concentration (40 mg/L) only reached 52.25%. Accordingly,
320	the cyanobacteria cells are a promising drug controlled-release platform.

321

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419	List of Figure Legends

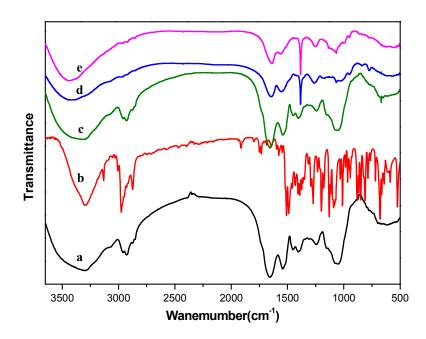
- 420 Fig. 1 FT-IR spectra of (a) PCC, (b) TEB, (c) TEB-PCC, (d) UF resins, and (e)
- 421 TEB-PCC@UF.
- 422 Fig. 2 FESEM micrographs of PCC (a), the TEB-PCC system (b), and the
- 423 TEB-PCC@UF system (c and d)
- 424 Fig. 3 Release profiles of TEB from the free TEB (a), the TEB-PCC system (b), and
- 425 the TEB-PCC@UF system (c) in ethanol/water mixture (v/v, 1:1).
- 426 Fig. 4 Control efficacy of TEB-PCC@UF microcapsules (a, c and e) and commercial
- 427 formulation (b, d and f) on wheat powdery mildew after 4, 8 and 12 day sprayed
- 428 wheat at 24 h (a, b), 48 h (c, d) and 72 h (e, f) before inoculation, respectively.
- 429 Scheme 1. Schematic illustration of two drug-delivery systems which show different
- 430 controlled-release patterns.

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- 432 List of Table Titles
- **Table 1:** Characteristic parameters of TEB-loaded microcapsules
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441 Figures



444 Fig.1 FT-IR spectra of PCC (a), TEB (b), TEB-PCC (c), UF resins (d), and445 TEB-PCC@UF (e).

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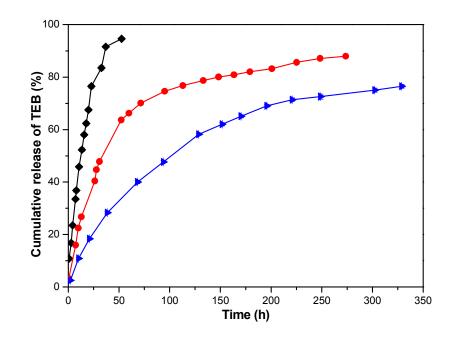
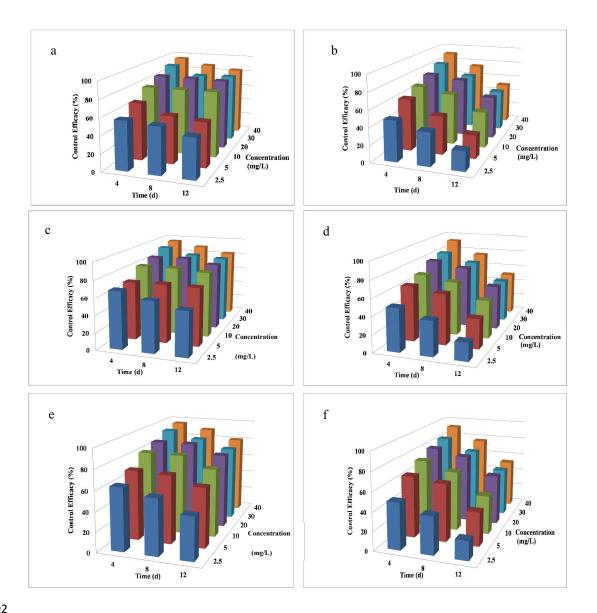
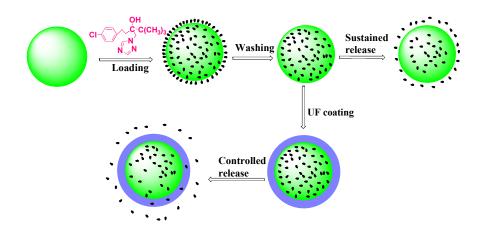


Fig. 3 Release profiles of TEB from the free TEB (a), the TEB-PCC system (b), and
the TEB-PCC@UF system (c) in ethanol/water mixture (v/v, 1:1). (Error bars
represent the standard deviation of three replicates. Where error bars are not shown,
the values of standard deviation are smaller than the data points.).



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Fig. 4 Control efficacy of TEB-PCC@UF microcapsules (a, c and e) and commercial
formulation (b, d and f) on wheat powdery mildew after 4, 8 and 12 day sprayed
wheat at 24 h (a, b), 48 h (c, d) and 72 h (e, f) before inoculation, respectively.



- 498 Scheme 1. Schematic illustration of two drug-delivery systems which show different
- 499 controlled-release patterns.

515	Tables

517	Table 1 Characteristic parameters of TEB-loaded microcapsules				
	Sample	$K(\mathbf{h}^{-1})^{[\mathbf{a}]}$	<i>n</i> ^[b]	$R^{2 [c]}$	t_{50} (h) ^[d]
	TEB-PCC	14.160±1.984	0.387±0.029	0.926	34.23
	TEB-PCC@UF	3.778±0.661	0.536±0.034	0.980	101.62
518	[a] K is the constant that	t incorporates the ma	atrix properties. [b] n	is a diffusion	n parameter. [c] R
519	is a correlation coefficient. [d] t_{50} is the time it takes to release 50% of TEB.				
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