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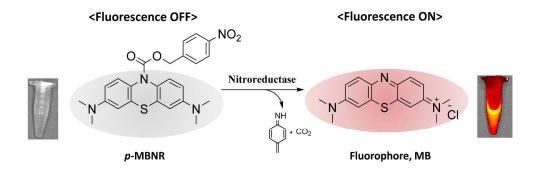
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A new fluorescent probe caged with a p-nitrobenzyl redox switch enables selective switching on of fluorescence by nitroreductase.

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Nitroreductase-triggered activation of a novel caged fluorescent probe obtained from methylene blue

Received 00th January 20xx, Accepted 00th January 20xx Jungeun Bae^a, Louis E. McNamara^b, Manal A. Nael^c, Fakhri Mahdi^d, Robert J. Doerksen^c, Gene L. Bidwell III^d, Nathan I. Hammer^b and Seongbong Jo^{*a}

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A near-infrared fluorescent probe based on methylene blue (*p*-NBMB) was developed for the detection of nitroreductase. Conjugating methylene blue with a *p*-nitrobenzyl moiety enables it to be activated by nitroreductase-catalyzed 1,6-elimination, resulting in the release of an active methylene blue fluorophore.

Nitroreductase (NTR), a flavin mononucleotide (FMN) cofactor dependent protein expressed in Escherichia coli (E. coli), catalyzes reduction of a nitro group to hydroxylamine, which is subsequently converted to an amine in the presence of nicotinamide adenine dinucleotide phosphate (NAD(P)H) as a cofactor.¹ The large electronic change resulting from conversion of the electronwithdrawing nitro group to the electron-donating hydroxylamino group provides a selective 'switch' mechanism for the activation of an inert compound which leads to the subsequent release of the active agent. Based on this switch mechanism, various prodrug or activatable imaging probes have been designed with nitro groups as substrates to be triggered upon reduction by NTR.² The dicoumarin carbonate-based latent fluorophore was devised for the application in imaging to improve selectivity for NTR and aqueous solubility.^{2b} Furthermore, NTR was employed in development of gene-directed enzyme prodrug cancer therapies (GDEPT), antibody-directed enzyme prodrug therapy (ADEPT) and drug screening as exemplified with 2,4-dinitrobenzamide (CB1954).3 The basis of CB1954 activation has been fully elucidated and the molecule has advanced into clinical trials.4

Despite the previous extensive investigation about the use of

nitrobenzyl redox switches for NTR activatable materials, these switches have not been applied for the development of bifunctional compounds, which can serve as a tool for selective imaging and therapy.²⁻⁴ To design NTR activatable agents with combined imaging and therapeutic function, the selection of an appropriate reporter is of great importance. Among various reporters, fluorophores with emission in the far red and near-infrared (NIR), in the range of 600-1000 nm, are widely utilized in relevant research settings to overcome the limitation of poor tissue penetration owing to the interference from background auto-fluorescence from biomolecules.⁵ In addition, NIR fluorophores offer several additional advantages over conventional imaging agents including high resolution, sensitivity and non-invasiveness.⁶ In particular, methylene blue (MB) has been recognized as a sensible starting point for the development of a better NIR fluorophore given MB's strong absorption of broadband red light (550-700 nm, maximum at 664 nm), a wavelength at which absorption and autofluorescence are minimal.⁷ Moreover, MB has been applied for clinical therapeutic purposes including treating methemoglobinemia, Barrett's esophagus, and cervical cancer.8 MB is also known to be photodynamically active so that it can inactivate viruses, destroy



Nitroreductase

Scheme 1 Mechanism of switching on the fluorescence probe, *p*-NBMB, upon reduction of a *p*-nitrobenzyl moiety after nitroreductase-mediated activation.



<Fluorescence ON>

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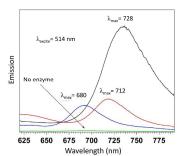


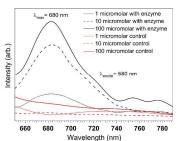
Fig. 1 Heterogeneity of p-NBMB in addition of NTR (1 unit) with NAD(P)H (1 mM). Thin film fluorescence emission spectra were obtained at 541 nm excitation.

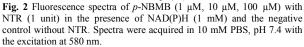
bacteria, and inhibit cancer cell growth.^{7b, 9} Given its advantageous properties, MB may be an ideal compound to use in design of an NTR-switchable probe with both imaging and therapeutic capability.

In this study, we describe a novel NIR fluorescent probe, pnitrobenzyl 3,7-bis(dimethylamino)-10H-phenothiazine-10carboxylate (p-NBMB) which can be triggered by NTR. To obtain a MB-based latent fluorescent probe, which is activatable, a pnitrobenzyl moiety as an NTR switch was conjugated to cage MB at the nitrogen of the phenothiazine ring through a carbamate bond, thereby quenching electron transfer within the molecule (Scheme 1). This ultimately leads to improvements in achievable target-tobackground auto-fluorescence ratios. In the presence of NTR, the resultant caged fluorescent probe is intended to be turned back on undergoing reduction of the aryl nitro group. Subsequently, the benzyl moiety will be removed by a rapid 1,6-elimination (Scheme 1). We primarily assessed the feasibility of whether a novel p-NBMB can be developed into an NTR selective activatable agent. Additionally, a potential therapeutic application of the compound in photodynamic therapy was also addressed.

The caged NIR fluorescent probe *p*-NBMB was synthesized in straightforward steps using MB and *p*-nitrobenzyl as shown in Scheme S1. Initially, MB in toluene (80% v/v in water) was reduced to obtain the activated leuco form of MB (leuco-MB). The yellow toluene phase containing leuco-MB was transferred into 4-nitrobenzyl chloroformate in toluene to afford the caged *p*-NBMB. The orange solid resultant *p*-NBMB was characterized by elemental analysis and ¹H-NMR spectroscopy (ESI[†]). The proton NMR of *p*-NBMB in CDCl₃ in Fig. S1 showed all the characteristic peaks and splitting, which indicated successful *p*-NBMB synthesis. The chemical shift value of the two protons after the reaction was deshielded from 4.82 ppm to 5.32 ppm, which is indicative of the formation of the carbamate bond.

The spectral analysis of *p*-NBMB was compared with that of a fluorophore MB as a reference. In spectroscopic evaluation of MB and *p*-NBMB, MB exhibits maximal absorbance at 665 nm and fluorescence at 685 nm ($\lambda_{ex} = 665$ nm) (Fig. S2). In contrast, *p*-NBMB displayed neither significant absorbance nor fluorescence excitation at 665 nm. This phenomenon appears to be caused by the interruption of π -conjugation system bridging the three rings of MB, which quenches the absorbance between 500 nm to 800 nm. This result indicated that *p*-NBMB exhibits no fluorescence when the signal compound MB is caged with the nitrobenzyl moiety redox





switch as illustrated in Scheme 1, which should lead to diminished noise in clinical imaging applications.

The selective uncaging via nitro reduction was assessed using NfsA, which is the major NTR from E. coli. As expected, p-NBMB exhibited a selective response for NTR, shown in Figure S3. The fluorescence spectrum of the control revealed no emission between 640 and 800 nm when excited by either 580 nm light using a fluorescence spectrometer or by 514.5 nm laser light, unless NTR is added in the solution. Heterogeneities of reduced p-NBMB were further observed with thin film fluorescence emission spectra as shown in Fig. 1. After reduction of p-NBMB by NTR, several different peaks were recovered in addition to the dominant 680 nm peak in the spectrum (Fig. 1). These results might be due to the formation of aggregates and excimers when the reduced p-NBMB interacts with the surface of a glass cover slip. A previous reported study also showed that the fluorophore MB forms dimers in dilute aqueous solutions and aggregates at increasing concentration due to the strong π -interactions among MB molecules.¹⁰ Thus, peaks from dimer and aggregates would appear on the longer wavelength at 712 nm and 728 nm due to the transition dipole moment from the ground state to the lower excited state, called the N-branch.¹¹ Considering the increase in fluorescence intensity in the presence of NTR, we anticipate that uncaging p-NBMB is dependent on nitroreductasemediated two-electron reduction of the nitrobenzyl moiety redox switch.

To verify whether there is a fluorescence response to other redox enzymes, which catalyze two-electron reduction, p-NBMB emission was investigated using DT-diaphorase. As shown in Fig. S4, DTdiaphorase did not induce any noticeable fluorescence signal enhancement from p-NBMB compared to the negative control without the enzyme, over an incubation period up to 48 h. According previous studies on triggerable fluorescent probes, to nitrobenzimidazoles containing aryl nitro groups could be an efficient redox switch that can be turned on by DT-diaphorase.¹² In addition, CB1954, the aforementioned prodrug carrying aryl nitro groups, was found to be activated by both DT-diaphorase and NTR but NTR catalyzed the reduction of CB1954 60 times faster than DT-diaphorase.^{4, 13} However, caged *p*-NBMB with the *p*-nitrobenzyl modification on the phenothiazine ring was not activated by DTdiaphorase. The result indicated that p-NBMB can be selectively reduced in the presence of NTR and hence can be used for NTR detection.

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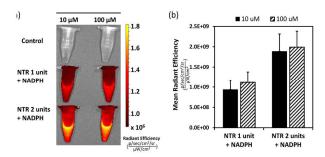


Fig. 3 Fluorescence response of *p*-NBMB to nitroreductase. (a) IVIS fluorescence images of *p*-NBMB (10 μ M, 100 μ M) with nitroreductase (1 and 2 unit/ml, 1 mM NAD(P)H) and the control without nitroreductase. (b) Quantitation of fluorescence from each group. Data shown as mean \pm SD (n = 3). Spectra were acquired after incubation at 37 °C overnight in 10 mM PBS (pH 7.4).

We also examined changes in fluorescence intensity as a function of concentration of p-NBMB, following incubation with one unit/ml of NTR. An increase in fluorescence intensity was observed when the concentration of p-NBMB was increased from 1 to 10 to 100 µM (Fig. 2). This result indicates that fluorescence enhancement is dependent on reduction of a p-nitrobenzyl redox switch by NTR. However, based on qualitative interpretation, the fluorescence intensity was not proportional to the concentration of p-NBMB within the concentration range. From this result, we inferred that the fluorescence enhancement would be more related to the amount of NTR. Hence, two concentrations of NTR, 1 unit/mL and 2 units/mL, were tested to observe the redox enzyme capacity in releasing fluorophore MB from p-NBMB (Fig. S5, ESI⁺). At the lowest p-NBMB concentration, 1 µM, the higher fluorescence emission intensity was similar, regardless of NTR concentrations. This implies that p-NBMB might show a detection limit at p-NBMB concentrations higher than 1 µM. For better visualization, we investigated the imaging capacity of p-NBMB using an in vivo imaging system, a Xenogen IVIS® Spectrum. As expected from the result showing NTR dependent fluorescence release in Fig. 3, images obtained from IVIS® are consistent. When the fluorescence intensity was compared by the released radiance efficiency in vivo, there were no statistically significant differences between the two p-NBMB concentrations. These results suggest that fluorescence emission occurring by p-NBMB reduction was predominantly dependent on the reduction capacity of NTR in the presence of NAD(P)H, providing its potential use for monitoring NTR.

Since we are interested in *p*-NBMB application not only in NTR activatable imaging *in vitro* but also for therapeutic purposes, we primarily focused on the characterization of the NTR selectivity of *p*-NBMB. This can be eventually translated into therapeutic

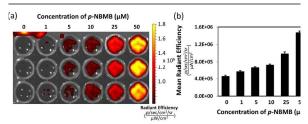


Fig. 4 IVIS fluorescence images of *p*-NBMB (1 - 50 μ M) incubated with intact *E. coli* K12 strain XL1-Blue (10⁹ CFU/mL) at 37 °C for 4 hours.

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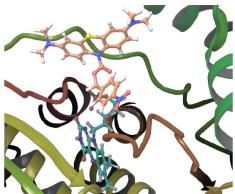


Fig. 5 The best binding pose of *p*-NBMB (orange carbons) to NTR. FMN is shown as cyan carbons. The substrate binding pocket of NTR (PDB 1F5V) was generated using Fred v3.0.0 of OpenEye software suite. The enzyme is represented as cartoon and colored by secondary structure (prepared with Maestro¹⁴).

advances in photodynamic therapy using fluorophores. Hence, we further examined the fluorescence response of p-NBMB to intact E. coli K12 strain XL1-Blue. When incubated with 10⁹ CFU/mL of E. coli, the NIR fluorescent probe p-NBMB was activated and released a fluorophore showing emission as indicated in the images in Fig. 4. In addition, p-NBMB demonstrated a concentration dependent increase in fluorescence intensity in the presence of bacteria. When the p-NBMB concentration is 1 µM as this bacterial concentration, no noticeable change in fluorescence emission was observed, indicating that the detection limit is 1 µM. This result is consistent with Fig. S5. We also used a serial dilution of a bacterial suspension to determine in vitro sensitivity of p-NBMB fluorescence to bacterial number (see ESI⁺). As shown in Fig. S6, the raw fluorescence images and the quantified data indicated that fluorescence intensity from p-NBMB is correlated with an increase in bacterial number. At the concentration and incubation time shown, the detection limit ranged between 10⁷ and 10⁸ CFU/mL. However, optimizing concentration of *p*-NBMB and incubation time could likely increase this limit. These observations implied that E. coli expressing NTR activates reduction of a redox switch in p-NBMB to facilitate release of a fluorophore, MB.

Along with the capacity of p-NBMB for imaging anaerobic bacteria expressing NTR, p-NBMB might be useful for the detection of hypoxia in application for tumor diagnosis based on the recently reported studies demonstrating that molecular probes caged with nitrobenzyl group showed fluorescence enhancement in hypoxia condition $(1\% \text{ pO}_2)$.¹⁵ Moreover, since the fluorophore methylene blue is an effective photosensitizer for photodynamic therapy, the generation of singlet oxygen $({}^{1}O_{2})$ from *p*-NBMB was tested using p-nitrosodimethylaniline (RNO) before and after activation by NTR. It is known that RNO is bleached in the presence of single oxygen, implying that the change in RNO absorbance intensity indicates the generation of ¹O₂¹⁶ Figure S7a shows that the *p*-NBMB incubated with NTR/NAD(P)H exhibited a decrease in RNO absorbance after laser irradiation at a wavelength of 634 nm (110 mW/cm², Hughes Research Laboratories, Culver City, CA). In contrast, no significant change in RNO absorbance was observed from the control after laser exposure (Fig. S7b). This result indicated that free MB released from *p*-NBMB reduction was able to generate ¹O₂ upon an irradiation in a

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NIR range. Based on the work done by Komine *et al.* demonstrating that ${}^{1}O_{2}$ generated from MB (0.01%) with a laser irradiation for 5 min killed *E. faecalis* (>99.9%)¹⁷, *p*-NBMB will be beneficial both for targeted diagnostic and therapeutic applications.

Molecular docking was also exploited to predict the accessability of the active site of NTR to *p*-NBMB.¹⁸ The docking results revealed that the ten generated poses of *p*-NBMB fit well inside the binding pocket of NTR based on FRED Chemgauss 4 scores in the range of -11 to -9 (Fig. 5). By inspecting the binding mode of *p*-NBMB, shown in Fig. S8, we noticed that one phenyl ring of the phenothiazine skeleton forms a π - π stacking interaction with Arg15, the positively charged amino group interacts with the negatively charged carboxylate of Glu162, and the carbamate carbonyl forms a dipole cation interaction with Lys167 (Fig. S8). These results rationally correlate favorable *p*-NBMB binding to the active site of NTR and the experimental observation of efficient *p*-NBMB reduction by NTR.

We have developed a new NIR fluorescent probe *p*-NBMB equipped with a *p*-nitrobenzyl redox switch that enables selective switching on of fluorescence by NTR. Whereas *p*-NBMB shows no fluorescence emission in PBS buffer at pH 7.4, it exhibits remarkable NIR fluorescence intensity after undergoing selective reduction by NTR. Furthermore, *p*-NBMB fluorescence was induced by incubation with live *E. coli* bacteria, indicating that endogenous NTR can activate the nitrobenzyl moiety switch to generate the fluorophore. This collectively indicates that *p*-NBMB would be a suitable imaging sensor to detect bacteria expressing NTR. In addition, *p*-NBMB also possesses potential as an MB prodrug which can be applied for the treatment of various diseases.

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Notes and references

- B. D. Palmer, P. van Zijl, W. A. Denny and W. R. Wilson, J. Med. Chem., 1995, 38, 1229-1241.
- (a) P. F. Searle, M. J. Chen, L. Hu, P. R. Race, A. L. Lovering, J. I. Grove, C. Guise, M. Jaberipour, N. D. James and V. Mautner, *Clin. Exp. Pharmacol. Physiol.*, 2004, **31**, 811-816; (b) H.-C. Huang, K.-L. Wang, S.-T. Huang, H.-Y. Lin and C.-M. Lin, *Biosens. Bioelectron.*, 2011, **26**, 3511-3516.
- 3. W. A. Denny, Curr. Pharm. Des., 2002, 8, 1349-1361.
- R. J. Knox, F. Friedlos, R. F. Sherwood, R. G. Melton and G. M. Anlezark, *Biochem. Pharm.*, 1992, 44, 2297-2301.
- (a) T. Schaeffter, in *Imaging in Drug Discovery and Early Clinical Trials*, Birkhäuser Basel, 2005, vol. 62, ch. 2, pp. 15-81; (b) G. S. Filonov, K. D. Piatkevich, L. M. Ting, J. Zhang, K. Kim and V. V. Verkhusha, *Nat. Biotechnol.*, 2011, **29**, 757-761.

- (a) D. Benaron, *Cancer Metastasis Rev*, 2002, 21, 45-78;
 (b) J. K. Willmann, N. van Bruggen, L. M. Dinkelborg and S. S. Gambhir, *Nat. Rev. Drug Discov.*, 2008, 7, 591-607.
- (a) E. Tanaka, F. Y. Chen, R. Flaumenhaft, G. J. Graham, R. G. Laurence and J. V. Frangioni, *J. Thorac. Cardiovasc. Surg.*, 2009, 138, 133-140;
 (b) W. Tang, H. Xu, R. Kopelman and M. A. Philbert, *Photochem. Photobiol.*, 2005, 81, 242-249.
- (a) W. B. Wendel, J. Clin. Investigation, 1939, 18, 179; (b) N. Ormeci,
 B. Savas, S. Coban, M. Palabiyikoğlu, A. Ensari, I. Kuzu and N. Kursun, Surg. Endosc., 2008, 22, 693-700.
- (a) M. Wagner, E. Suarez, T. Theodoro, C. Machado Filho, M. Gama, J. Tardivo, F. Paschoal and M. Pinhal, *Clin. Exp. Derma.*, 2012, 37, 527-533; (b) R. A. Floyd, J. E. Schneider and D. P. Dittmer, *Antiviral Res.*, 2004, 61, 141-151; (c) J. Perdrau and C. Todd, *Proc. R. Soc. Lond. B Biol. Sci.*, 1933, 288-298; (d) J. P. Tardivo, A. Del Giglio, C. S. de Oliveira, D. S. Gabrielli, H. C. Junqueira, D. B. Tada, D. Severino, R. de Fátima Turchiello and M. S. Baptista, *Photodiagnosis Photodyn. Ther.* 2005, 2, 175-191.
- (a) S. L. Fornili, J. Chem. Soc. Faraday Trans., 1981, 77, 3049; (b) D.
 Heger, J. Phys. Chem. A, 2005, 109, 6702-6709; (c) S. Jockusch, N. J.
 Turro and D. A. Tomalia, Macromolecules, 1995, 28, 7416-7418.
- 11. K. Patil, R. Pawar and P. Talap, *Phys. Chem. Chem. Phys.*, 2000, **2**, 4313-4317.
- Ž. Anusevičius, H. Nivinskas and J. Segura-Aguilar, Arch. of Biochem. Biophys., 1997, 346, 219-229.
- 13. G. M. Anlezark, R. G. Melton, R. F. Sherwood, B. Coles, F. Friedlos and R. J. Knox, *Biochem. Pharm.*, 1992, 44, 2289-2295.
- Schrödinger Release 2015-1: Maestro, version 10.1, Schrödinger, LLC, New York, NY, 2015.
- T. Guo, L. Cui, J. Shen, W. Zhu, Y. Xu and X. Qian, *Chem. Commun.*, 2013, **49**, 10820-10822.
- I. Kraljic, S. E. Mohsni and M. Arvis, *Photochem. Photobiol.*, 1978, 27, 531-537
- 17. C. Komine and Y. Tsujimoto, J. Endodont, 2013, 39, 411-414.
- 18. M. McGann, J. Chem. Info. Model., 2011, 51, 578-596.