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3 1 Reagent-free and portable detection of *Bacillus anthracis* spores using a microfluidic incubator
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5 2 and smartphone microscope
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9 3 Janine R. Hutchison*^a, Rebecca L. Erikson^b, Allison M. Sheen^c, Richard M. Ozanich^a, Ryan T.
10
11 4 Kelly*^b
12

13
14 5 ^aChemical Biological Signatures Science, National Security Directorate, Pacific Northwest
15
16 6 National Laboratory, P.O. Box 999, Richland, Washington 99352.
17

18
19 7 ^bElectronics and Measurement Systems, National Security Directorate, Pacific Northwest
20
21 8 National Laboratory, P.O. Box 999, Richland, Washington 99352.
22

23
24 9 ^cEnvironmental Molecular Sciences Laboratory, Pacific Northwest National Laboratory, P.O.
25
26 10 Box 999, Richland, Washington 99352.
27

28 11 *Corresponding Email: Janine.Hutchison@pnnl.gov, Phone: 509-372-6301, Fax: 509-375-2227
29

30 12 *Corresponding Email: Ryan.Kelly@pnnl.gov, Phone: 509-371-6525, Fax: 509-371-6445
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32
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34
35 14 Abstract

36
37 15 *Bacillus anthracis* is the causative agent of anthrax and can be contracted by humans and
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39 16 herbivorous mammals by inhalation, ingestion, or cutaneous exposure to bacterial spores. Due to
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41 17 its stability and disease potential, *B. anthracis* is a recognized biothreat agent and robust
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43 18 detection and viability methods are needed to identify spores from unknown samples. Here we
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45 19 report the use of smartphone-based microscopy (SPM) in combination with a simple microfluidic
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47 20 incubation device (MID) to detect 50 to 5000 *B. anthracis* Sterne spores in 3 to 5 hours. This
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49 21 technique relies on optical monitoring of the conversion of the 1 μ m spores to the filamentous
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51 22 vegetative cells that range from tens to hundreds of micrometers in length. This distinguishing
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53 23 filament formation is unique to *B. anthracis* as compared to other members of the *Bacillus*
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3 24 *cereus* group. A unique feature of this approach is that the sample integrity is maintained, and
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5 25 the vegetative biomass can be removed from the chip for secondary molecular analysis such as
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8 26 PCR. Compared with existing chip-based and rapid viability PCR methods, this new approach
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10 27 reduces assay time by almost half, and is highly sensitive, specific, and cost effective.
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15 29 **Introduction**

18 30 Anthrax is an acute disease caused by the bacterium *Bacillus anthracis* that can be contracted by
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20 31 humans and other animals through ingestion or inhalation of the spores, or by cutaneous
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22 32 introduction through abrasions.¹ While the natural infection of humans and livestock in the
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24 33 United States is rare, anthrax outbreaks are common in many developing countries where
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26 34 effective means of prevention, diagnosis and treatment are lacking. The hardiness of *B. anthracis*
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28 35 – spores can remain viable for decades – and the ability to produce large quantities of the spores
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30 36 *in vitro* have also led to the use of *B. anthracis* as an agent of biological warfare and
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32 37 bioterrorism. In a 2001 case of bioterrorism in the United States, *B. anthracis*-laced letters sent
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34 38 through the postal system infected 22 individuals, 5 of whom died as the result of the attack.²
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38 40 Since the 2001 incident, substantial research efforts have focused on improving viable *B.*
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40 41 *anthracis* spore sampling, recovery, detection and confirmation.^{3–5} Current detection methods
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42 42 include traditional culture plating, immunoassays, DNA-based detection via PCR, and a variety
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44 43 of biosensors, with each approach presenting advantages and challenges.⁶ A particular emphasis
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46 44 has been placed on field-based measurements, where diagnostics can be performed at the point
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48 45 of threat in the case of either a suspected deliberate release or a natural anthrax outbreak. For
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50 46 such field-based measurements, a premium is placed on ruggedness, ease of use and low cost. A
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3 47 noteworthy advance in fieldable detection was recently reported by Harper *et al.*, in which a self-
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5 48 contained credit card sized device enabled remote detection of *B. anthracis*.⁷ The device
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8 49 incorporated on-chip incubation starting with as few as 100 spores for amplification to the $>10^6$
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11 50 spores needed for detection by an integrated lateral flow immunoassay. The time required for the
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13 51 test was in the range of 8–18 h and the device was self-contained, requiring no external power
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15 52 sources or pumps (novel magnetically actuated valves provided fluidic control). The price per
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17 53 assay was estimated to be ~\$5–7, a fivefold reduction compared to current commercial offerings.
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20 54 The reduction in price can dramatically increase the accessibility of the test, particularly in
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22 55 resource-limited settings where natural outbreaks are most common, and additional reductions in
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24 56 assay cost will further promote testing and minimize the impact of outbreaks.
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29 58 An exciting development in recent years has been the adaptation of ubiquitous smartphone
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31 59 technology for portable chemical and biological detection.^{8–16,16–25} Smartphones are now widely
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34 60 available in even the most remote settings, and the combination of high quality cameras and
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36 61 integrated communication capabilities offer tremendous promise for remote and resource-limited
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38 62 analyses. Assays are frequently performed using either paper- or channel-based microfluidic
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41 63 platforms with optical signals being recorded by the smartphone camera. Custom-built
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43 64 applications can then be used for data processing and readout or the acquired images can be
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46 65 transmitted to a centralized facility for further evaluation. Optical attachments can convert
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48 66 smartphone cameras into high powered microscopes for cytological measurements.^{26–33}
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53 68 Here, we have combined a simple microfluidic incubation device (MID) with a high-power,
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55 69 extremely low-cost (< \$0.10) smartphone microscope (SPM) for rapid, sensitive and reagent free
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3 70 detection of viable *B. anthracis* spores. *Bacillus anthracis* spores germinate under appropriate
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5 71 conditions and the metabolically active vegetative cells grow in filamentous rods that can be
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8 72 distinguished visually from other classes of bacteria. Spores are combined with growth media
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10 73 and manually loaded via syringe into a microfluidic incubation chamber. Following incubation,
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12 74 the media is passed through a patterned microfluidic filter where the filamentous rods are
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15 75 retained. The SPM, which has 350× magnification and is based on a Leeuwenhoek design, can
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17 76 readily identify the filamentous rods and confirm the presence of *B. anthracis*.³⁴ Detection of 50
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20 77 to 5,000 spores was achieved in 3 to 5 hours, and the platform is readily compatible with
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22 78 secondary confirmation by PCR providing not only genus/species verification but potentially
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24 79 isolate information. Importantly, aside from the smartphone, the entire platform, including the
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27 80 SPM and the MID has a cost of less than \$1, providing an order of magnitude reduction in per-
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29 81 assay costs relative to current protocols, which should dramatically increase accessibility of the
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32 82 assay and improve response to potential threats.
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36 84 **Materials and methods**

37 85 **Smartphone microscope**

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39 86 The SPM utilized a glass bead as its lens and was attached to the smartphone using a 3D printed
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42 87 lens holder.²³ The lens holders were created on a Makerbot Replicator 2X using PLA filament at
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45 88 a print speed of 60 mm/s (Makerbot, New York, NY, USA). Two designs were evaluated; the
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48 89 first was a ‘clip’ style 100× microscope that fits over most smartphones. The second design,
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51 90 which was the primary microscope for the current study, fits snugly over an iPhone 5 or 5S and
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53 91 provides a magnification of 350×.³⁵ For the 100× SPM, a 3-mm-diameter glass bead was
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56 92 employed (GL0179B/3000; MO-SCI, Rolla, MO, USA), while a 1-mm-diameter glass bead
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3 93 served as the 350× microscope lens (11079110; BioSpec, Bartlesville, OK, USA). The glass
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5 94 bead lens was aligned with the 3D printed lens holder and inserted by compression fitting. The
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8 95 magnification was measured using a chrome-on-glass calibration slide from Motic (Motic,
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10 96 Richmond, British Columbia, Canada). The 350× design weighs 2.1 grams, adds 1mm of
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12 97 thickness to the phone, and has a bill of materials cost of \$0.07 including the optics. All images
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15 98 were captured using an iPhone 5s (Apple, Cupertino, CA) with the default camera application
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17 99 that is included with the phone. No external light sources were used for any images and ambient
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20 100 light conditions both inside and outdoors are sufficient for imaging at the tested magnifications.
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24 102 **Microfluidic Incubation Device (MID) fabrication**

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26
27 103 The MID design is depicted in Fig 1. The template used for soft lithography comprised three
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29 104 different feature heights, two of which were photolithographically patterned.³⁶ A single
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31 105 photomask contained two distinct and aligned layers and was designed and used according to a
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33 106 previously developed procedure.³⁷ The first layer patterned the 10- μm -tall fine filter (Fig. 2) and
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35 107 was created by spin-coating SU-8 2010 (Microchem, Westborough, MA, USA) on a 100-mm-
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37 108 diameter silicon wafer (University Wafer, Boston, MA, USA) at 3000 rpm for 60 sec and soft
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39 109 baking, exposing, post-exposure baking and developing according to manufacturer instructions.
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41 110 The wafer was then hard baked at 180 °C for 15 min. The remaining patterned features were 25
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43 111 μm tall and were made from SU 8 25 (Microchem) spin-coated at 2000 rpm for 30 sec and were
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46 112 also processed according to manufacturer instructions followed by a 180 °C hard bake for 15
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48 113 min. The incubation chamber and waste chamber were made from ~7-mm-tall, 1-cm-diameter
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50 114 cylinders of hot melt adhesive (HMA; Ad tech, Hampton, NH, USA). HMA cylinders were
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53 115 affixed to the template as shown in Fig. 1 by placing the wafer on a hot plate at 85 °C and
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3 116 pressing the HMA in place. This provided an incubation chamber volume of ~500 μ L in the
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5 117 completed devices.
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10 119 Devices were prepared from the patterned templates as described previously.³⁸ Briefly, Sylgard
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12 120 184 (Dow Corning, Midland, MI, USA) was mixed according to manufacturer specifications,
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14 121 poured onto the template to a thickness of ~8 mm, degassed under vacuum and cured at 70 °C
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16 122 for 2 hr. Patterned substrates were then removed from the template and holes were punched at
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18 123 the Inlet and Air Outlet (Fig. 1) using a 20-gauge catheter hole punch (Syneo, West Palm Beach,
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20 124 FL, USA). Substrates were cleaned and irreversibly bonded to 22 mm x 40 mm cover glass
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22 125 (Thermo Fisher, Waltham, MA, USA) by activating the bonding surfaces of the glass and PDMS
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24 126 in an oxygen plasma system. Following activation, the PDMS and glass substrates were brought
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26 127 into contact and then placed in an oven at 70 °C for 1 hr to improve bond strength.
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33 34 129 **Microorganisms**

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36 130 *Bacillus anthracis* Sterne spores were prepared reported in Nutrient Broth with CCY salts for 72
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38 131 hours.³⁷ Two additional spore preparations, derived from *Bacillus atropheus* ATCC 9372 and
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40 132 the filamentous fungus *Neurospora crassa*, were tested and served as negative controls. Spores
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42 133 were diluted in phosphate buffered saline (#10010049 Invitrogen, Waltham, MA, USA)
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44 134 containing 0.02% Tween-80 (#P4780, Sigma-Aldrich, St. Louis, MO, USA) which is denoted
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46 135 PBS-T, to 10 times the target concentration. Spores were then diluted tenfold into germination
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48 136 media [Tryptic Soy Broth (TSB; #286220, BD, Franklin Lakes, NJ, USA) with 10 mM L-alanine
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50 137 (#A7627, Sigma-Aldrich)] to the final concentration (10^6 , 10^4 , 10^3 , or 10^2 , CFU/mL).³⁹ *Bacillus*
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3 138 *atrophaeus* and *N. crassa* spores were tested at a concentration of 10^6 CFU/mL. Viable plating
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6 139 was used to confirm the spore CFU/mL.
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10 141 **Spore germination and optical detection**

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12 142 Five-hundred μ L of spore-containing mixture were loaded into a 1 mL plastic syringe (Becton
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15 143 Dickinson, Franklin Lakes, NJ, USA) and supplied to the MID via Tygon tubing (Cole-Parmer,
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17 144 Vernon Hills, IL, USA) by hand. After the entire sample was loaded, the MID was incubated at
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20 145 37 °C with shaking at 100 rpm for 3 to 5 hours to allow the spores to germinate and form
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22 146 vegetative filaments. Subsequent experiments were conducted at room temperature with no
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24 147 shaking to determine the fieldability of the device. The culture was then injected into the waste
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27 148 chamber to collect the *B. anthracis* vegetative cells on the fine filter. The MID fine filter was
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29 149 aligned with the SPM or a standard light microscope (BX51, Olympus, Waltham, MA, USA) to
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31 150 visualize and record the presence of filamentous bacteria. For SPM operation, the 3D printed
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34 151 lens holder was inserted over the iPhone 5s, auto-aligning with the rear-facing camera on the
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36 152 smartphone. Holding the MID to the lens, with the glass coverslip physically resting on the lens
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39 153 cover, the MID was manually translated relative to the lens until the image on the screen
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41 154 displayed the fine filter region of the device. Once positive pressure was applied to aspirate the
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43 155 sample from the incubation chamber to the waste chamber, an accumulation of filamentous rods
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46 156 was rapidly observed on the fine filter surface.
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50 158 **PCR confirmation**

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53 159 To determine the compatibility of the MID with established *B. anthracis*-specific detection a
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55 160 secondary analysis was performed with real-time PCR. MIDs were seeded with spores in
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3 161 germination media and were incubated for 3 to 5 hr. For each concentration of *B. anthracis*
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5 162 spores tested, a time zero sample in PBS-T was also analyzed to control for false positives. The
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7 163 sample was removed from the single-use MID by piercing a needle into the incubation chamber
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9 164 and aspirating near the fine filter. Real-time PCR was conducted with an Applied Biosystems
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11 165 7500 Fast Real-Time PCR system (Grand Island, NY, USA). The FAST cycling conditions were
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13 166 used but were modified to include a thermal lysis step at 95 °C for 10 min prior to cycling. Each
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15 167 PCR reaction was performed in a final volume of 20 µL (10 µL of 2x TaqMan® Fast Universal
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17 168 Master Mix, 1 µL of 20x Primer/Probe, 4 µL of nuclease free water, and 5 µL of template). Auto
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19 169 baseline and auto threshold were used for all analyses. The primers and probes (CAAX) are
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21 170 specific for a *B. anthracis* chromosome marker and were purchased from IDT as a PrimeTime®
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23 171 qPCR Assays (IDT, Coralville, IA, USA).⁴⁰ The primer sequences were: Forward primer (5' to
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25 172 3') TCC GTT TAC CAA TTC ACT ATG AAT CAA T, reverse primer (5' to 3') ATG CGT
26
27 173 TGT TAA GTA TTG GTA TAA TCA TC and probe (5' to 3') FAM/CC CAC TTG G/Zen/A
28
29 174 TTA TAT CCT GAG TAT CGT GA/3IABkFQ/.

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176 **Results and discussion**

177 **Smartphone microscope characterization**

178 Over the past several years, several research groups have developed a wide array of microscope
179 attachments for smartphones. These attachments range from highly sophisticated systems with
180 multiple components, to relatively simple, low cost arrangements.⁴¹ For the present application, a
181 system was desired that had a footprint comparable to that of a traditional protective cellphone
182 case and that was also inexpensive enough to be considered disposable if contaminated (Fig. 2).
183 Magnification of at least 100× was critical, with the added resolution provided by 300–400×

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3 184 magnification being desirable for bacterial morphology inspections. With the small form factor
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5 185 requirement, a Leeuwenhoek design was selected.³⁴ Leeuwenhoek-style microscopes notoriously
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8 186 suffer from aberrations in image quality around the perimeter of the field of view due to the
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10 187 spherical lens being used to view the sample. The center of the field of view, however, provides
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12 188 a more than adequate resolution for cellular morphology and optical viewing of samples.
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17 190 The SPM was initially characterized and compared to other microscope arrangements using an
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19 191 *Aspergillus* specimen. As shown in Fig. 3, the specimen was imaged using the iPhone 5s camera
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21 192 with no microscope (a); 100× SPM (b), 350× SPM (c), KingMas 60× Clip-On Microscope
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23 193 Magnifier (d), and an Olympus BX51 fluorescence phase contrast benchtop microscope at 100×
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25 194 (e) and 400× (f). All images were cropped to the same field of view, and no other image
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27 195 manipulation was performed. Insets in Fig. a, b, d and e provide expanded views of the region
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29 196 displayed in Fig. 3c for resolution and detail comparison. The unassisted iPhone 5s camera (Fig.
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31 197 3a) and the low-cost commercial magnifier (Fig. 3d) are insufficient for resolving the *Aspergillus*
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33 198 conidiophore structures (which range in diameter of 2 to 6 μm) or the ~1 μm diameter *B.*
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35 199 *anthracis* filaments. Similar resolution images were acquired with the 100× SPM (Fig. 3b) and
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37 200 the upright microscope at 100× (Fig. 3e). While individual conidiophore structures can be
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39 201 imaged, there is low resolution of the vesicle at this magnification. As expected, the image
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41 202 quality and structural resolution was the greatest with the 350× SPM (Fig. 3c) and the upright
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43 203 microscope at 400× (Fig. 3f); as both show resolution of distinct conidiophore and vesicle
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45 204 structure of the *Aspergillus* sample. Impressively, the image quality in the center of the field of
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47 205 view of the <\$0.10 SPM is comparable to the ~\$10,000 benchtop microscope. Images taken with
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49 206 the SPM can also be easily transmitted via email or text message allowing sharing of data and
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3 207 input from collaborators on the identification of an unknown sample. Larger magnification SPMs
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5 208 (>350×) can also be developed using smaller diameter lenses, but for the purposes of this study
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8 209 the resolution obtained with the 350× SPM was sufficient to distinguish fungal and bacterial
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10 210 morphology.
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15 212 The use of a 3D printed lens holder increases the ease of use of a Leeuwenhoek style
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17 213 microscope. Previous work by Smith *et al.* demonstrated the utility of a smartphone microscopes
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19 214 using a spherical 1mm glass lens taped to an iPhone camera.²³ The 3D printed lens holder used
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21 215 here allows for the automatic alignment of the microscope lens and the camera, increasing the
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23 216 ease of use. Costs were minimized for the SPM reported here relative to past approaches by
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25 217 employing glass beads that are sold in bulk at a cost of <\$0.01/bead. Similar resolution was
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27 218 achieved with these low cost beads and dedicated optical spheres, and the resulting SPM
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29 219 provides a simple, cost effective microscope for the educational field, environmental sampling,
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31 220 the diagnosis of blood borne diseases, and biothreat detection as described here.
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37 38 39 222 ***Bacillus anthracis* detection by smartphone microscopy**

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41 223 To explore the utility of the SPM for bacterial pathogen detection, *B. anthracis* spores were
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43 224 selected as a model pathogen. *Bacillus anthracis* has a unique dormant spore structure which can
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45 225 be problematic for detection and viability assessment at low concentrations (for a review see
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47 226 Ireng and Gala, 2012).³ While immunoassays are increasingly popular for rapid detection, they
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49 227 typically require high spore numbers (>10⁴ CFU/mL), and require antibodies that are expensive
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51 228 to develop and that can be cross-reactive, reducing the advantage of the rapid assays. Further,
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53 229 immunoassays cannot provide information on the viability, infectivity, or the genetic potential of
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3 230 the spore. While spores can be imaged directly using the SPM, little information can be gained
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6 231 through optical observation. However, by germinating the spores into the metabolically active
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8 232 vegetative filaments, one can not only determine viability, but sequential molecular assessment
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10 233 can provide valuable information regarding the genetic potential of the organism.
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12 234
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15 235 To detect *B. anthracis* spores without the addition of reagents such as an antibodies, a
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17 236 microfluidic incubation device (MID) was developed for the growth and subsequent imaging of
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19 237 germinated spores. Assay operation was kept as simple as possible as a proof of principle for
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21 238 field-based or resource-limited detection. As such, spores were combined with growth media off-
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23 239 chip prior to loading the MID by hand using a syringe and tubing, such that no equipment
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26 240 besides the MID and the SPM was required. In the process of filling the incubation chamber, the
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28 241 spores were passed through a micropatterned coarse filter (Fig. 1), which consisted of 12 rows of
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30 242 50- μm -diameter pillars with 50- μm spaces in between. The coarse filter was designed to prevent
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32 243 any filamentous, non-spore debris from entering the incubation chamber, as such debris could
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34 244 potentially lead to false positive identifications.
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41 246 Initial tests were conducted at high spore concentrations to verify that germination occurred and
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43 247 that the filaments could be viewed within the MID using the SPM. For the 5×10^5 *B. anthracis*
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45 248 spore samples, numerous vegetative filaments can easily be seen on the fine filter both with
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47 249 standard microscopy and with the SPM (Fig. 4a, 4b, respectively). Similar results were observed
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49 250 for spores at 5×10^3 but were less dense (Fig. 4c, 4d). No filamentous fibers were observed with
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51 251 either the *B. atrophaeus* or the *N. crassa* spores, although the $\sim 5\text{--}8$ μm diameter *N. crassa* spores
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53 252 did aggregate at the coarse filter and tended to clog the MID (Fig. 4e, 4f). Germination and
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3 253 vegetative filament growth was observed for samples incubated at both 37 °C with shaking and
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5 254 static incubation at room temperature (data not shown).
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10 256 Optical detection of 5×10^3 *B. anthracis* spores in 3 hours offers a vast improvement upon
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12 257 traditional culture methods that rely on turbidity measurements and/or colony and bacterial
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14 258 morphology characterization with selective media. However, detection of lower concentrations
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16 259 of spores is desirable for trace analysis. To evaluate the utility of the MID and SPM for low level
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18 260 detection, 500 or 50 CFU were seeded into the MID. After 3 hours no vegetative filaments could
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20 261 be seen, which is not surprising since at lower concentrations additional time is needed to reach
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22 262 an active doubling time. At 4 hours vegetative filaments were observed with MID seeded with
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24 263 500 CFU. At the 5 hour time point vegetative filaments were observed with the 50 CFU samples,
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26 264 as shown in Fig. 4g.
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34 266 In summary, optical detection using the MID and SPM is successful after 3 hours for 5000 CFU,
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36 267 4 hours for 500 CFU, and 5 hours for 50 CFU. The most appropriate comparison for device
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38 268 performance is to Sandia National Lab's credit card-size anthrax detector, BaDx.⁷ The BaDx is a
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40 269 self-contained bio-amplification device that has the capability to detect 500 *B. anthracis* spores
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42 270 within 8 to 18 hours. Overall assay cost is greatly reduced from the \$30 diagnostic cost to ~\$5–7
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44 271 for BaDx. The results presented here show successful detection of 50 to 500 *B. anthracis* spores
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46 272 in 3 to 5 hours with a device cost of less than a dollar. Further advancements in MID design will
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48 273 allow for automated loading and integrated optical detection.
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55 275 **Molecular confirmation**
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3 276 Incubation of an unknown sample for 3 to 5 hours in the germination media is unlikely to lead to
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5 277 rapid growth of filamentous species other than *B. anthracis*. Indeed, filamentous rods were not
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8 278 observed in any negative control (Fig. 4e, 4f). However, in some situations, visual observation of
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10 279 the conversion of bacterial spores to filamentous rods may be considered as a presumptive
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12 280 identification of viable *B. anthracis* spores. In these cases it would be advantageous to confirm
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14 281 the identity and genetic potential of the biological sample using an additional detection method.
15
16 282 One of the fastest methods for molecular detection is real-time PCR (RT-PCR). RT-PCR adds
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18 283 and additional hour to the assay, but provides a conformation of the optical detection method.
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20 284 Three MID experiments at several concentrations were analyzed in triplicate by RT-PCR for n=9
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22 285 measurements, and results are summarized in Table 1. At all concentrations, time zero samples
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24 286 failed to amplify nucleic acid and were considered negative for the presence of viable *B.*
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26 287 *anthracis* cells. Conversely, all samples were positive after incubation in the MID Table 1. These
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28 288 data demonstrate that use of a SPM in combination with a MID allows for rapid detection (3 to 5
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30 289 hours) of low numbers of spores (50 to 5000).
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35 291 Recent advances of microfluidic chip PCR propose on-board field-based detection of biological
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37 292 samples⁴². A challenge with these methods is that the target sample needs to be in a form that
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39 293 can be easily detected. As such, spores are not conducive for direct PCR analysis and require
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41 294 extensive sample prep using, e.g., bead beaters and/or chemical lysis. Rapid viability PCR (RV-
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43 295 PCR) has been utilized to overcome these challenges. In this method, spores are germinated for 9
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45 296 hours in filter cups prior to PCR and PCR is conducted pre- and post- enrichment. The change in
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47 297 CT values from time zero to the final endpoint is used to determine if the sample is positive for
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49 298 *B. anthracis* spores. This method has been extensively used for wipe, swab, and post-decon
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3 299 samples with a reported detection level of 10 to 99 CFU/sample.⁴³⁻⁴⁶ The advantage of using the
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5 300 MID followed by PCR detection is that the overall enrichment time is decreased to 5 hours for
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8 301 50 CFU/sample, allowing rapid turnaround of samples for viability assessment of *B. anthracis*
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10 302 spore samples.
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15 304 **Conclusions**

17 305 In summary, we have developed and implemented a simple microfluidic device with an
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19 306 inexpensive smartphone-based microscope for optical detection of the unique filaments formed
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21 307 by viable *B. anthracis* spores following germination. While *B. anthracis* is closely related to
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23 308 other members of the *Bacillus cereus* group, the vegetative filaments of *B. anthracis* tend to be
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25 309 much longer (>100 μm) and can be used as a distinguishing phenotype from other group
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27 310 members. The approach presented here is simple to use, cost effective, readily implemented in
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29 311 resource-limited settings and is compatible with secondary confirmation assays such as real-time
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31 312 PCR. Only 3 to 5-hour incubation times are required depending on spore concentration, and
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33 313 image collection takes less than 5 minutes. The unique approach also allows data transmission to
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35 314 a subject matter expert for confirmation in minutes. This platform can be modified for the
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37 315 detection of potential biothreat agents in addition to *B. anthracis*.
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7
8 324 located at PNNL.
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11 326 **Notes and references**

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403 **Tables**

404 Table 1. RT-PCR values of biomass recovered from MID when seeded with a target spore
 405 number and sampled at a specific time. Mean CT values are the average of 3 MID chips analyzed
 406 in triplicate for an n=9 PCR measurements.

Target number of <i>B. anthracis</i> spores	Growth time	Mean C _T	Standard deviation of the mean
5x10 ⁵	3 hours	30.31	0.41
5000	3 hours	35.90	0.40
5000*	3 hours	36.76	0.50
500	4 hours	34.02	0.66
50	5 hours	35.62	1.39

407 *In addition to *B. anthracis* Sterne spores, *N. crassa* spores were also seeded into the MID

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4 408 **Figure Legends**

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6 409 Fig. 1. Schematic of the MID. The biological sample is injected into the inlet and passes through
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8 410 a coarse filter to remove large debris and particulates before entering the incubation chamber.
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10 411 After incubation for a pre-determined amount of time, the sample is aspirated to the waste
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12 412 chamber. Vegetative bacterial filaments are trapped and concentrated on a fine filter during
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14 413 aspiration for facile optical monitoring.
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18 415 Fig. 2 Smartphone microscope (SPM) device for iPhone 5 or 5s. Plastic housing is printed using
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20 416 a 3D printer with PLA filament. A 1 mm glass bead that serves as the lens is inserted into the
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22 417 housing after 3D printing.
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26 419 Fig. 3 Comparison images of an *Aspergillus* specimen taken with a) an iPhone 5s using
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28 420 maximum digital zoom and no optical zoom attachment b) iPhone 5s with 100× SPM c) iPhone
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30 421 5s with 350× SPM, d) iPhone 5s with KingMas 60x Smartphone Microscope, e) Olympus
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32 422 BX51 at 100×, f) Olympus BX51 at 400x. Insets in a, b, d and e magnifications of the region
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34 423 displayed in c for resolution and detail comparison.
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38 425 Fig. 4 *B. anthracis* Sterne spores were germinated for 3 hours in a MID prior to imaging with the
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40 426 350× SPM. Thin filamentous vegetative cells were observed only in samples that included *B.*
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42 427 *anthracis* spores, the presence of these filaments was indicative positive viable anthrax. (a) 5×10^5
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44 428 spores imaged using standard microscopy; (b) 5×10^5 spores imaged with SPM; (c) 5×10^3 spores
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46 429 imaged with standard microscopy; (d) 5×10^3 spores imaged using SPM; (e) 5×10^5 *B. atropaenus*
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430 spores; (f) 5×10^5 *N. crassa* spores; (g) 50 spores incubated for 5 hours in MID. Arrows highlight
431 *B. anthracis* vegetative filaments.