Accepted Manuscript



This is an *Accepted Manuscript*, which has been through the Royal Society of Chemistry peer review process and has been accepted for publication.

Accepted Manuscripts are published online shortly after acceptance, before technical editing, formatting and proof reading. Using this free service, authors can make their results available to the community, in citable form, before we publish the edited article. We will replace this Accepted Manuscript with the edited and formatted Advance Article as soon as it is available.

You can find more information about *Accepted Manuscripts* in the **Information for Authors**.

Please note that technical editing may introduce minor changes to the text and/or graphics, which may alter content. The journal's standard <u>Terms & Conditions</u> and the <u>Ethical guidelines</u> still apply. In no event shall the Royal Society of Chemistry be held responsible for any errors or omissions in this *Accepted Manuscript* or any consequences arising from the use of any information it contains.



www.rsc.org/chemcomm

Cite this: DOI: 10.1039/x0xx00000x

Received 00thFebruary 2014, Accepted 00thFebruary 2014

DOI: 10.1039/x0xx00000x

www.rsc.org/

Antibacterial polymeric nanostructures for biomedical applications

Jing Chen^a, Fangyingkai Wang^a, Qiuming Liu^a, and Jianzhong Du^{a*}

The high incidence of bacterial infection and the growing resistance of bacteria to conventional antibiotics have resulted in the strong need for the development of new generation of antibiotics. Nano-sized particles have been considered as novel antibacterial agents with high surface area and high reactivity. The overall antibacterial properties of antimicrobial nanostructures can be significantly enhanced compared with conventional antibacterial agents not in a regular nanostructure, showing better effect on inhibiting the growth and reproduction of microbials such as bacteria and fungi, *etc.* In this review, recent advances in the research and applications of antimicrobial polymeric nanostructures have been highlighted, including silver-decorated polymer micelles and vesicles, antimicrobial polymer micelles and vesicles, and antimicrobial peptide-based vesicles, *etc.* Furthermore, we proposed the current challenges and future research directions in the field of antibacterial polymeric nanostructures for the real-world biomedical applications.

Introduction

Antibiotics are naturally occurring or synthetic organic compounds which inhibit or destroy selective bacteria or other microorganisms, generally at low concentrations.¹ Compared with a wide range of active chemical agents (biocides) which have a broad spectrum of activity, antibiotics trend to have specific intracellular targets.¹ Although many generations of antibiotics have been developed, antibiotic-resistant bacteria are becoming a more and more important threat to public health due to the overuse and the improper use of antibiotics. Therefore, new antimicrobial agents are needed and much work has been devoted to developing highly efficient compounds that are also less susceptible to development of resistance by bacteria.^{1, 2}

Among the new antimicrobial agents, silver,³ quaternary ammonium moieties,^{4, 5} silica-based,⁶⁻⁹ carbon-based materials,¹⁰⁻¹² reactive-oxygen-species-generating conjugated polymers,¹³⁻¹⁷ antimicrobial peptides,¹⁸ *etc.* have been widely studied. The antibacterial mechanisms of these agents are varied from cell wall/membrane-damaging abrasiveness, metal ions released to inhibit certain oxidative enzymes, denaturated protein or interfered with DNA/RNA replication, *etc.*¹⁹

The antibacterial activity is related to many factors such as formulation effects, presence of an organic load, synergy, temperature, and dilution.^{1, 20-23} To enhance the antibacterial activities, a great number of work in designing the ideal antibacterial nanoparticles have been investigated. Overall, synthetic chemistry, morphology, size and surface charge of

particles are among the most relevant variables affecting antibacterial activity.²⁴⁻²⁸

In the last decade, growing attention has been paid to antimicrobial polymers and their nanostructures due to their broad applications in human and animal health care.^{13, 14, 29-34} Usually, these polymers can form secondary structures to enrich the antibacterial groups have extra ability for drug delivery. Therefore, they are able to kill bacteria on contact with durable and sustainable antimicrobial activities when covalently attached to the surfaces of a variety of materials.^{35, 36}

In this review, we aim to focus on the antibacterial mechanisms and the recent advances of polymeric nanostructures, including silver-decorated polymeric micelles and vesicles, natural or synthetic cationic antimicrobial agent conjugated polymeric nanostructures, *etc.* We also aim to highlight the approaches to stabilize the silver, to control the shape, to normalize the size, and to reduce the cytotoxicity of silver decorated polymeric nanoparticles. We will discuss the self-assemblies based on cationic antimicrobial polymers and antimicrobial peptides, with the purpose of increasing the antibacterial efficacy and possessing the potential drug delivery capabilities. Finally, we aim to highlight current challenges in the field of antibacterial polymeric nanostructures for the real-world biomedical applications.

Silver-decorated polymeric nanostructures

Silver nanoparticles are some of the most widely commercialized nanomaterials used in clinical care and consumer products,³⁷⁻⁴³ which have shown great toxicity to a

broad range of micro-organisms (Fig. 1) and can effectively kill both Gram-negative and Gram-positive bacteria, such as *Escherichia coli* (*E. coli*) and *Staphylococcus aureus* (*S. aureus*).^{39-41, 44, 45} As a naturally antibacterial metal, a silver nanoparticle likely has multiple mechanisms of antibacterial activity (Fig. 1).⁴⁶



Fig. 1 Silver nanoparticles showing multiple bactericidal actions.⁴⁶



Fig. 2 Synthetic route to silver-decorated polymer vesicles and micelles. Silver nanoparticles are formed *in situ* among the vesicle membrane or the micelle core after introduction of $AgNO_3$ and subsequent reduction by $NaBH_4$. Reproduced from Ref. 47.

First, the membrane permeability of bacteria was thought to be affected by nanoparticles because of the presence of a large number of nanoparticles inside the bacteria. Interaction of silver particles with bacteria membrane and intracellular proteins, particularly sulfur-containing membrane proteins and phosphorus-containing DNA, interferes with cell division and causes cell death. Following, some researches also confirmed the presence of biocidal ionic silver released from nanoparticle surfaces.²⁵ Upon exposure to ionic silver, bacteria DNA conglomeration defense mechanisms protect it from a toxic surrounding environment but this compromises bacteria replication ability. Thus, the responses to ionic silver and nanoparticles are different, but both are essential to a complete understanding of the antibacterial activity of silver nanoparticles.

However, the agglomeration problem of silver nanoparticles has significantly restricted their applications. Once silver nanoparticles agglomerate to form micro particles or aggregates, their antibacterial activities decrease sharply.⁴⁸ Therefore, templates such as polymer micelles, polymer vesicles, microgels and dendrimers have been used to prevent the particle agglomeration.⁴⁹⁻⁵¹ However, for many decades the agglomeration problem has not been solved thoroughly. Therefore, exploring a facile, efficient and controlled template for preparing silver nanoparticles with long-term stability is still of interest for many scientists.⁴⁷

For example, our group reported the design and preparation of water dispersible silver-decorated polymer vesicles and micelles based on an amphiphilic block-statistical copolymer, PEO-*b*-P(DMA-*stat*-*t*BA) (polymer 1 in Fig. 2) and its partially hydrolysed derivative, PEO-*b*-P(DMA-*stat*-*t*BA-*stat*-AA) (polymer 2 in Fig. 2).⁴⁷ In both block copolymers, PDMA chains displayed variable pK_a values due to the interaction of each block in the copolymer chains.⁵²⁻⁵⁵ Therefore, it is possible to prepare different nanostructures by simply changing the pH of the copolymer solution. Then silver nanoparticles were *in situ* generated in the membrane of the polymer vesicles or the core of the micelles (Fig. 2).

Those water dispersible silver-decorated polymer micelles and vesicles showed excellent antibacterial efficacy against *E. coli* with quite low minimum inhibitory concentration (MIC) and minimum bactericidal concentration (MBC).

To further prepare ultrafine water-dispersible silver nanoparticles with long-term stability, a role-switching method was developed based on a soft deformable block copolymer vesicle. As illustrated in Fig. 3,⁵⁶ by vesicle templating, the Ag⁺ ions can be easily absorbed by the PAA segments within the loose vesicle membrane, leading to an even distribution of Ag⁺ ions. During the process of reduction, the pH jump leads to the break-up of the Ag⁺-adsorbed polymer vesicles to afford ultrafine silver nanoparticles without the loss of the uniformity of the distribution of Ag⁺ ions.

Those ultrafine silver nanoparticles showed excellent antibacterial efficacy against both Gram-negative and Grampositive bacteria with quite low MICs of 16.9 μ g/mL and 8.45 μ g/mL, respectively. The key point of this role-switching method is using polymer vesicle as the template and its subsequent deformation into micelles during reduction process of Ag⁺ into Ag(0) to stabilize the final silver nanoparticles. Journal Name



Fig. 3 (A) Preparation of ultrafine antibacterial silver nanoparticles with long term stability by a role-switching method. Green: hydrophilic poly(ethylene oxide) (PEO); blue: pH-responsive poly(acrylic acid) (PAA); purple: hydrophobic poly(*tert*-butylacrylate) (PtBA). (B) Comparison between the handover of vesicle templating to micelle stabilization and micelle templating/stabilization methods. Reproduced from Ref. 56.

Besides the agglomeration problem, the metabolization of silver nanoparticles is another major challenge to their applications, especially for *in vivo* antibacterial treatment. Our group recently reported an enzymatically degradable polymer vesicle decorated with silver nanoparticles (Fig. 4), which showed low cytotoxicity against human normal liver L02 cells near the minimum inhibitory concentrations (MICs) but excellent antibacterial efficacy against both Gram-negative and Gram-positive bacteria with quite low MICs of 3.56 mg/mL and 7.12 mg/mL, respectively, exhibiting promising potential applications in nanomedicine.⁵⁷

Alternatively, to decrease the cytotoxicity of silver nanoparticles and increase the tensile strength of materials, nanocomposites from a waterborne polyetherurethane (PEU) ionomer and silver nanoparticles were prepared without the use of any cross-linker.⁵⁸ The PEU showed high tensile strength and the addition of silver nanoparticles further increased its

thermal stability, and the PEU-Ag nanocomposites had a strong bacteriostatic effect on the growth of *E. coli* and *S. aureus*.



Fig. 4 Silver-decorated biodegradable antibacterial PCL₇₅-b-PAA₂₁ diblock copolymer vesicles. Reproduced from Ref. 57.

Overall, the silver-decorated polymeric nanoparticles have a strong antimicrobial activity against both Gram-positive and Gram-negative bacteria. However, further studies are needed to solve the agglomeration and the cytotoxicity problems to meet various requirements such as higher concentration. In addition, synthetic nanocomposites may have limited biocompatibility, leading to inflammation phenomena and even hazardous immunogenic responses. Such problems have been partially solved by using natural or bio-inspired polymers. Further studies on the silver-decorated polymeric nanoparticles for *in vivo* applications may greatly contribute to this area.

Cationic antimicrobial agent conjugated polymeric nanostructures

Cationic compounds have emerged as promising candidates for developments as antimicrobial agents with decreased potential for resistance development. Among them, cationic surfactants,^{59, 60} lipids,^{61, 62} peptides^{63, 64} and natural or synthetic cationic polymers^{35, 65} have been intensively studied as antimicrobial agents by themselves or in sophisticated formulations.

Usually, the following sequence of events occurs with microorganisms exposed to cationic agents: (i) adsorption and penetration of the agent into the cell wall; (ii) reaction with the cytoplasmic membrane (lipid or protein) followed by membrane disorganization; (iii) leakage of intracellular low-molecular-weight material; (iv) degradation of proteins and nucleic acids; and (v) wall lysis caused by autolytic enzymes. These would be a loss of structural organization and integrity of the cytoplasmic membrane in bacteria, together with other damaging effects to the bacterial cell.^{66, 67}

In this section, polymeric cationic antibacterial agents, synthetic and natural antimicrobial peptides have been highlighted.

Polymeric cationic antibacterial agent

Fig. 5 shows a possible mechanism of polymeric cationic antibacterial activity.⁶⁸ Normal bacterial membranes (panel a) are stabilized by Ca^{2+} ions binding anionic charged phospholipids. Cationic polymer rapidly displaces Ca^{2+} (panel b), leading to loss of fluidity (panel c) and eventual phase separation of different lipids. Domains in the membrane then undergo a transition to more smaller micelles.

Furthermore, antimicrobial cationic polymers can effectively inhibit the growth of bacteria and other microbes without releasing low molecular weight toxic chemicals to environment. It is noteworthy that the common bacterial strains, such as *E. coli* and *S. aureus* do not develop resistance against polymeric biocides.⁶⁹ Antimicrobial polymers usually contain polycationic structures, such as substituted quaternary ammonium compounds,⁷⁰⁻⁷² phosphonium salts,⁷³ *N*-alkyl pyridinium salt⁶⁹ and rhodamine derivative.⁷⁴

Unlike common antimicrobial polymer films, self-assembled cationc polymeric nanoparticles can form a secondary structure before interacting with the microbial membrane, and are expected to have better antimicrobial properties.⁷¹ In the natural cationic antimicrobial polymers, chitosan is one of the most widely applied polymers due to its great biological activities, low toxicity toward mammalian cells,^{75, 76} antibacterial activity in controlling growth of bacteria and inhibiting viral multiplication.⁷⁷⁻⁷⁹

Wang's group investigated the use of chitosan nanoparticles as bactericidal agents in poly(methyl methacrylate) (PMMA) bone cement. To increase the antibacterial activity and solubility of chitosan, quaternary ammonium chitosan derivative nanoparticles have also been prepared. The results showed the chitosan and quaternary ammonium chitosan nanoparticles provided a significant additional bactericidal effect to the bone cement with no cytotoxicity, indicating a new promising strategy for combating joint implant infection.⁸⁰



Fig. 5 A possible mechanism of polymeric cationic antibacterial activity.⁶⁸

Polymers with quaternary ammonium moieties have good antibacterial property, which can be further enhanced when forming nanoparticles because of the increase in the local concentration of cationic charge.

For example, Hedrick *et al.* reported a quaternary ammonium compounds containing biodegradable and *in vivo* applicable antimicrobial polymer nanoparticles synthesized by metal-free organocatalytic ring-opening polymerization of functional cyclic carbonate (Fig. 6A-C).⁷¹ The cationic polymer micelles have a strong effect against growth drug-resistant Gram-positive bacteria, as well as fungi. As shown in the transmission electron microscope (TEM) results (Fig. 6D), the cell walls and membranes of the microorganisms were damaged, and cell lysis was observed after treatment with the micelles. Their MIC values are varied from 4.3-10.8 μ M as cell-type-dependent.

However, quaternary ammonium compounds may lead to haemolysis, which is a major harmful side effect of many cationic polymers. Therefore, polymers without quaternary ammonium have been selected for the preparation of antibacterial polymeric nanoparticles.



Fig. 6 (A) Synthesis of cationic polycarbonates. (B) The formation of micelles was simulated through molecular modelling using Materials StudioSoftware (in the polymer molecule: red, O; white, H; grey, C; blue, N). (C) TEM image of polymer 3

Page 5 of 12

Journal Name

ChemComm

micelle. (D) Comparative TEM images of *Enterococcus faecalis* in the absence and presence of polymer 3. 71

Among these polycationic substances, poly[2-(tertbutylaminoethyl) methacrylate] (PTA) has a high antibacterial activity and a low toxicity to human cells.^{30, 81, 82} It is partially hydrophilic and partially hydrophobic in neutral water as its pK_a is 9.12 and can exchange with the Ca²⁺ or/and Mg²⁺ cation in the outer membrane of bacteria. Once they are displaced by an external agent, the outer membrane is disorganized and the lysis of cell occurs, which results in the death of the bacteria.⁸³, Therefore, PTA exhibits antibacterial activity without quatermization, as is not the case with other amine-containing polycationic substances.^{30, 85, 86} For example, Jang et al. coated PTA chains on the surface of silica nanoparticles, which showed size-dependant antimicrobial efficacy.³²



Fig. 7 Antibacterial PEO-*b*-PCL-*b*-PTA triblock copolymer micelles: (A) Formation of antibacterial micelles and the mechanism of the antibacterial activity. (B) *E. coli* and *S. aureus* growth inhibition results after polymers treatment. Reproduced from Ref. 87.

In 2012, we synthesized PTA-based ABC triblock copolymers (PEO₄₃-*b*-PCL₂₀-*b*-PTA₂₀ and PEO₄₃-*b*-PCL₂₀-*b*-PTA₃₀), which were then self-assembled into water-dispersible and biodegradable polymer micelles with good antibacterial activity in the absence of quaternary ammonium moieties or

loaded biocides.⁸⁷ Upon degradation of PCL, the PEO and PTA blocks were cut off (Fig. 7A).

The self-assembled nanostructure leads to strong interactions between the polymer and cell wall/membrane due to higher local concentrations of positive charges, which eventually translate to effective antimicrobial activities. Micelles from PEO_{43} -*b*-PCL₂₀-*b*-PTA₂₀ (polymer 1) have MBC values of 0.30 and 0.15 mM against *E. coli* and *S. aureus*, respectively (Fig. 4). The MBCs of micelles from PEO_{43} -*b*-PCL₂₀-*b*-PTA₃₀ (polymer 2) are 0.20 and 0.08 mM, respectively (Fig. 7B).⁸⁷



copolymer vesicles: (a) branched cylinders by dissolving PME0₂MA-*b*-PTA diblock copolymer in DMF and dialyzing against water. (b) TEM of images of branched cylinders and high-genus vesicles. (c) Liver cancer cells killing efficacy of DOX-HCI loaded high-genus vesicles. Reproduced from Ref. 89.

Furthermore, we developed a novel thermo- and pHresponsive antimicrobial diblock copolymer, PMEO₂MA₂₀-*b*-PTA₂₀, where PMEO₂MA is thermo-responsive poly[2-(2methoxyethoxy)ethyl methacrylate] and PTA is pH-responsive and antibacterial,⁸⁸ which can be directly dissolved in water to form conventional simple polymer vesicles upon simply raising the temperature.

Compared to the individual polymer chains, polymer vesicles exhibit much better antimicrobial efficacy against both Gramnegative and Gram-positive bacteria under physiological conditions with neither quaternary ammonium moieties nor the

Journal Name

loading of any external antibiotics as a result of their increased local concentration of cationic charge. 88

Moreover, this copolymer can self-assemble into an "armed" high-genus block copolymer vesicle by a solvent switch method, which is different from the above direct dissolution method (Fig. 8a-b).⁸⁹ Interestingly, branched cylinders were formed at 20 °C when the DMF was replaced by pure netural water, which could be eventually transformed into perforated high-genus vesicles when heated to a higher temperature at 37 °C (Fig. 8a-b).⁸⁹

The high-genus vesicles have more internal barriers than the simple polymer vesicles, showing better antibacterial activity against both Gram-positive and Gram-negative bacteria without quaternary ammonium moieties or the loading of any external antibiotics compared to the non-self-assembled individual polymer chains, or the above mentioned conventional simple vesicle.⁸⁹

In addition, the haemolysis experiment confirmed that the H_{50} value of this high-genus vesicle is 4.7 mg/mL, suggesting its excellent blood compatibility.⁸⁹

Moreover, the high-genus vesicle could be also used as an efficient drug delivery carrier with more internal barriers for drug molecules than conventional simple vesicles, which can efficiently kill liver cancer cells (HCCLM3) in a dose-dependent fashion (Fig. 8c). Therefore, this "armed" drug delivery vehicle makes antibacterial and anticancer therapeutic processes proceed spontaneously, representing a safer and more efficient drug delivery system in nanomedicine.⁸⁹

Recently, dendrimers have been received considerable attention for antibacterial applications because of their unique properties such as controlled size, low dispersivity and flexibility of modifying the terminal functional groups.⁹⁰⁻⁹³ Those dendrimers could be also self-assembly into nanoparticles for improving the antibacterial activity.

For example, Yao had modified the poly(amidoamine) (PAMAM) dendrimers with quaternized carboxymethyl chitosan (CM-HTCC). The CM-HTCC/PAMAM nanoparticles exhibited better antibacterial activity against Gram-negative bacteria *E. coli*, but slightly affected the growth of Grampositive bacteria *S. aureus* compared with quaternized chitosan.⁹⁴

Antimicrobial peptides

Antimicrobial peptides (AMPs) are natural, amphiphilic sequences of 5-50 amino acid residues with net positive charges.^{63, 95} They are produced by bacteria, plants and animals (both vertebrates and invertebrates).^{63, 64, 96, 97} Recently, AMPs have been termed "natural antibiotics" because they show broad-spectrum antimicrobial activities against various microorganisms, including Gram-positive and Gram-negative bacteria, fungi and viruses.⁶³ A list of well-studied antibacterial peptides is sumarrized in Table 1.

AMPs is generally accepted that positively charged peptides interact directly with the negatively charged cellular membranes of bacterial cells, resulting in increase of membrane permeability, which leads to a rapid cell death.^{98, 99} The mechanism of the antimicrobial activities of AMPs has been studied for some selected peptides. Functions of these peptides vary from membrane permeabilization to actions on an array of intracellular target molecules including immune-modulatory activities. The peptides can be membrane-disruptive, resulting in cell lysis. Alternatively, the membrane interaction can lead to the formation of transient pores and the transport of peptides inside the cell, bringing them into contact with intracellular targets.

As shown in Fig. 9, the listed models explaining the mechanisms of membrane permebilization include: (A) carpet, peptide chains cover the surface of membranes in a carpet-like manner and dissolves it like a detergent beyond a threshold concentration for which a high peptide-to-lipid ratio is required; (B) barrel stave, the peptides bind to the cell membrane, then the peptides themselves insert into the hydrophobic core of the membrane forming a pore, causing leakage of cytoplasmic material and death of the cell; (C) wormhole or toroidal, the peptides aggregate and tempt the lipid monolayers to bend continuously through the pore so that both the inserted peptides and the lipid head groups line the water core; (D) aggregate channel, the peptides insert into the membrane and then cluster into unstructured aggregates that span the membrane. These aggregates are proposed to have water molecules associated with them providing channels for leakage of ions and possibly larger molecules through the membrane (Fig. 9).¹⁰⁰⁻¹⁰²

Table 1 Representative antibacterial peptides						
Antimicrobial	Structure	Sequence	Antibacterial Activities		Ref.	
Peptide Name		-	Gram+	Gram-		
Magainin	α-helix	GIGKFLHSAKKFGKAFVGEIMNS	+	+	103-105	
β-Defensin3	β-sheet	GIINTLQKYYC1RVRGGRC2AVLSC3LPKEEQIGKC2STRGRKC1C3RRKK ^a	+	+	106-108	
Lactoferricin B	β-hairpin	FKC1RRWQWRMKKLGAPSITC1VRRAFA	+	+	109, 110	
Nisin A	Non-regular polypeptides	I-Dhb-A ₁ -I-Dha-L-A ₁ -Abu ₂ -PG-A ₂ -K-Abu ₃ -GALMG-A ₃ -NMK-Abu ₄ -A-Abu ₅ - A ₄ -N-A ₅ -SIMV-Dha-K ^b	+	-	111, 112	
Polymyxin E (Colistin)	Cyclic polypeptides	Fatty Acid-Dab-T-Dab- Dab ₁ - Dab-dL-L-Dab-Dab-T ₁ ^c	-	+	113-115	

^{*a*}Cysteines forming disulfide bonds are numbered with subscripts to indicate their pairings; ^{*b*}Aminobutyric acid (Abu), 2,3-didehydroalanine (Dha), 2,3-didehydrobutyrine (Dhb); ^{*c*}The fatty acid molecule is 6-methyloctanoic acid for colistin A and 6-methylheptanoic acid for colistin B, diaminobytyric acid (Dab).

FEATURE ARTICLE

RSCPublishing

Fig. 9 Mode of action of antibacterial peptides in Gram-negative bacteria. AMPs are proposed to associate with the negatively charged surface of the outer membrane by either neutralizing the charge over a patch of the outer membrane or by strongly interacting to the divalent cation binding sites on LPS.¹⁰²

However, these natural peptides as well as their peptide analogues are expensive to prepare and difficult to produce in a large scale, limiting their potential use to certain pharmaceutical applications.

Recently, a number of nonnatural peptides with designed sequences have been elaborated to provide biologically active structures;¹¹⁶⁻¹¹⁸ in particular, facially amphiphilic peptides built from amino acids can mimic both the structures and the biological function of natural antimicrobial peptides such as magainins and cecropins.

For example, Tew and co-workers¹¹⁶ have designed a series of facially amphiphilic arylamide polymers that capture the physical and biological properties of this class of antimicrobial peptides synthesized from inexpensive monomers. The design process was aided by molecular calculations with density functional theory-computed torsional potentials. These amphiphilic polymers may be applied in situations where inexpensive antimicrobial agents are required.

In another example, one kind of poly(oxonorbornene)-based synthetic mimics of antimicrobial peptides (SMAMPs) was reported.¹¹⁹ This was achieved by carefully designing the distribution of the chemical functional groups on the polymer backbone, so that the polymers were also facially amphiphilic. It was further demonstrated that such polymer-based SMAMPs also target the bacterial membrane, most likely by a mechanism similar to AMPs. The combined properties of excellent antimicrobial activity, cell selectivity, low resistance formation potential and easy availability make SMAMPs ideal candidates for biomedical applications (Fig. 10).



Fig. 10 Chemical structure of poly(oxonorbornene)-based synthetic mimics of antimicrobial peptides (SMAMPs). (a) SMAMPs with tunable antimicrobial activity and cell-compatibility can be obtained by varying the hydrophobic groups (green, R = methyl to hexyl) and hydrophilic groups (blue) that are attached to the poly(oxonorbornene backbone) (orange). (b) Structure of the SMAMP copolymers; Series 1: R = Propyl, Series 2: R = Butyl.¹¹⁹

The antibacterial efficacy can be enhanced significantly when an individual antibacterial polymer chain self-assembled into polymer micelles or vesicles due to concentration of local positive charges.⁸⁷⁻⁸⁹

For example, Yang and coworkers designed a short amphiphilic peptide (CG₃R₆TAT), which contains a hydrophilic block of cell penetrating peptide TAT and six arginine residues (R₆ or Arg₆) for adding more cationic charges to improve membrane translocation.⁷² Under the driving force of the hydrophobic block of cholesterol the core-shell nanoparticles formed by self-assembly. The nanoparticles showed strong antimicrobial properties against a range of bacteria, yeasts and fungi. What's more, the nanoparticles can also cross the bloodbrain barrier and suppress bacterial growth in infected brains (Fig. 11).

Compared with solid nanoparticles, polymer vesicles are excellent carriers, which can be used to deliver drugs,¹²⁰⁻¹²³ antioxidant agents,¹²⁴ magnetic resonance imaging (MRI) contrast agents,¹²⁵⁻¹²⁷ proteins, DNA and RNA, *etc.*^{128, 129}

To combine the advantages of AMPs' antibacterial capability and the drug delivery capability of polymer vesicles, our group recently reported a novel kind of "armed" carrier: an antibacterial polypeptide-grafted chitosan-based vesicle with an excellent antibacterial efficacy against both Gram-positive and Gram-negative bacteria (Fig. 12).¹³⁰

One sixth of -COOH groups in the acid-functionalized chitosan were grafted by an antibacterial peptide [poly(Lys₁₁-*stat*-Phe₁₀)], providing an excellent antibacterial efficacy for vesicles. Half -COOH groups in the acid-functionalized chitosan were esterified by methanol for enhancement of antibacterial activity. One third of residual -COOH groups in the acid-functionalized chitosan can be further functionalized when necessary.¹³⁰



Fig. 11 Peptide structure and formation of peptide nanoparticles. (a) Chemical structure of the designed peptide with cholesterol, glycine, arginine and TAT. (b) Formation of micelles, simulated through molecular modelling using Materials Studio software. (c) and (d) Scanning electron micrographs of nanoparticles.⁷²



Fig. 12 Antibacterial polypeptide-grafted chitosan-based vesicle as an "armed" carrier of drugs: Vesicles from $[poly(Lys_{11}-stat-Phe_{10})-g-Cs]_x-stat-Cs_{2x}-stat-ECs_{3x}$

have excellent antibacterial activity, while they are capable of delivering anticancer and antiepileptic drugs simultaneously. $^{\rm 130}$



Fig. 13 Dose-dependent growth inhibitions of typical gram-negative (*E. coli*) and gram-positive (*S. aureus*) bacteria in the presence of polymer **8** nanocapsules (vesicles) and polymer **4** chains. OD: optical density.¹³⁰

The membrane of such kind of vesicle is composed of both hydrophobic and entrapped hydrophilic moieties, which has a "fuzzy" boundary between hydrophilic and hydrophobic moieties, providing new opportunities for making a range of functional materials.¹³¹⁻¹³⁴ Drugs are released faster in the presence of protease due to biodegradation of polypeptide in the vesicle membrane.

This vesicle has excellent antibacterial activity (Fig. 13), excellent blood compatibility and low cytotoxicity.¹³⁰ To confirm the enhancement of the antibacterial efficacy of [poly(Lys₁₁-*stat*-Phe₁₀)-*g*-Cs]_x-*stat*-Cs_{2x}-*stat*-ECs_{3x} (polymer **8** in Fig. 13) vesicles compared to poly(Lys₁₁-*stat*-Phe₁₀) chain (polymer **4** in Fig. 13, which is the effective antibacterial component in polymer **8**), their MICs against both Gramnegative *E. coli* and Gram-positive *S. aureus* were evaluated (Figure 2): 16 µg/mL (polymer **8** vesicles) and 31 µg/mL (polymer **4** chain which is not in any assembled state). This is due to a higher local positive charge density in vesicles as mentioned before.

Overall, patients after tumor surgery may benefit from this "armed" carrier because it is highly anti-inflammation and is able to deliver anticancer and antiepileptic drugs simultaneously. This concept can be also extended to design a variety of new delivery vehicles with antibacterial, antitumor, and many other functions.

Conclusions and future outlooks

Polymeric nanoparticles have been identified to inhibit a variety of bacterial species *in vitro*, including some multi-drug-resistant microbes. In this review, the recent advances in the antibacterial polymeric nanostructures such as micelles and vesicles have been highlighted.

Compared with the individual polymer chain, the selfassembled nanostructure can significantly improve the antibacterial efficacy resulting from the 2^{nd} or 3^{rd} structureJournal Name

dependent highly concentrated antibacterial agents. Meanwhile, based on this antibacterial enhancement property it is possible to restore the antibacterial activity of some currently less effective or ineffective antibiotics, and to decrease the risk of antibiotic-resistance of new generation of antibiotics in the future.

Nowadays, infection has the trend to happen together with multiple complications, such as cancer, over-reaction of immune system and so on. Also, the complications will seriously threaten patients' lives. Thus, compounded functional or "smart" nanostructures with both excellent antibacterial activity and controlled drug delivery capabilities are desired to solve this problem. For example, our group has recently reported several antibacterial polymeric vesicles with promising capability of delivering anticancer and other drugs simultaneously.^{89, 130} Wang *et al.* revealed that conjugated polymers can provide efficient antimicrobial and anticancer activities by generating reactive oxygen species upon light radiation.¹⁵⁻¹⁷

In general, biocompatibility and biodegradability of nanoparticles are important issues for *in vivo* biomedical applications. Therefore, well-designed biocompatible and biodegradable polymers are needed for further decreasing the cytotoxicity of silver nanoparticles and other conjugated antibacterial agents.

Furthermore, more and more "smart" antibacterial nanocarriers with specific targeting, stable structure, high drug loading efficiency, and conditions sensitivity are needed to be designed to meet various biomedical requirements. Moreover, the overall evaluation based on in vitro and in vivo studies on antibacterial the activity, drug delivery efficacy, biocompatibility and biodegradability of functional antimicrobial polymeric nanostructures are also required to meet the clinic requirements.

Moreover, deeper insight into the observation of more physiologically and biologically relevant modes of bacteria interaction with nano-materials is strongly needed in the future to develop new approaches and materials with broad and persistent microbes killing capability and low toxicity to mammalian cells. Hopefully, antibacterial polymeric nanostructures by self-assembly technique may provide an alternative way to design more effective, more clinically promising, and less antibiotic-resistant multifunctional biomedical nanomaterials.

Abbreviations

aminobutyric acid
antimicrobial peptide
arginine
quaternized carboxymethyl chitosan
carboxyl group
diaminobytyric acid
2,3-didehydroalanine

Dhb	2,3-didehydrobutyrine	
DNA	deoxyribonucleic acid	
E. coli	Escherichia coli	
Gly	glycine	
HCCLM3	a liver cancer cell	
Lys	lysine	
MBC	minimum bactericidal concentration	
MIC	minimum inhibitory concentration	
MRI	magnetic resonance imaging	
PAA	poly(acrylic acid)	
PAMAM	poly(amidoamine)	
PCL	poly(<i>ɛ</i> -caprolactone)	
PDMA	poly(N, N'-dimethylacrylamide)	
PEO	poly(ethylene oxide)	
PEU	polyetherurethane	
Phe	phenylalanine	
PMEO ₂ MA	poly[2-(2-methoxyethoxy)ethyl	
	methacrylate]	
PMMA	poly(methyl methacrylate)	
PTA	poly[2-(tert-butylaminoethyl)	
	methacrylate]	
PtBA	poly(<i>tert</i> -butylacrylate)	
RNA	ribonucleic acid	
S. aureus	Staphylococcus aureus	
SMAMP	synthetic mimics of antimicrobial peptide	
TAT	one kind of cell penetrating peptide	
TEM	transmission electron microscope	

Acknowledgements

J. Du is supported by National Natural Science Foundation of China (21174107 and 21374080), Shanghai 1000 Plan, Eastern Scholar professorship, Ph.D. program Foundation of Ministry of Education (20110072110048), Fok Ying Tong Education Foundation (132018), and the fundamental research funds for the Central Universities.



Jing Chen received her bachelor degree (2001) and PhD degree (2006) in Institute of Genetics, School of Life Science, Fudan University, China. Her PhD involved novel cell penetrating peptides screening & application on protein transduction for stem cell differentiation, and development of oral non-virus gene delivery system by using Chitosan for gene therapy. She is currently working in

School of Materials Science and Engineering at Tongji University as a postdoctoral research associate in the research group of Prof. Jianzhong Du. Her research interests encompass the application of novel multifunctional polymer vesicles in medical molecular biology area.

3.

4.

5.

6.

7.

8.

9.

26.

34.

Page 10 of 12



Fangyingkai Wang received his Bachelor's degree in 2012 from School of Materials Science and Engineering, Tongji University. He is currently a Ph.D. candidate under the supervision of Prof. Jianzhong Du and focusing on the synthesis, self-assembly and biomedical applications of smart polymers.



Qiuming Liu received her bachelor degree in 2010 from Hubei University. In 2013 she received her master degree from Tongji University under the joint supervision of Professors Jianzhong Du and Tianbin Ren. She is currently working for her PhD degree under the supervision of Prof. Jianzhong Du. Her research interests focus on multifunctional polymer

vesicles for biomedical applications.



Prof. Jianzhong Du received his PhD degree in chemistry in 2004 from Institute of Chemistry, Chinese Academy of Sciences. He was appointed as an 'Eastern Scholar' professor at Tongji University in 2009 and a 'Shanghai 1000 Plan' professor in 2011. Before he moved to Tongji, he worked with Prof. Steve Armes at the

University of Sheffield (2004-2008), and Dr Rachel O'Reilly at University of Cambridge (2008-2010) as a postdoctoral research fellow. He was also an Alexander *von* Humboldt Fellow in 2006. He was awarded the Top 50 PhD Dissertations in CAS in 2005 and the Nominated National Top 100 PhD Dissertations in China in 2006, New Century Excellent Talents in Universities of Ministry of Education in 2010, "Best Supervisors in My Eyes" at Tongji University in 2013, and National Award for Contribution of Creative Talents of Returned Overseas Chinese in 2014. His research interests focus on the synthesis, self-assembly and applications of stimuli-responsive polymers with particular interests in polymer vesicles and other complex nanostructures. He also has wide interests in materials science, biomedicine, biocatalysis, water remediation, and antibacterial materials, *etc*.

Notes and references

^a School of Materials Science and Engineering, Tongji University, 4800 Caoan Road, Shanghai, 201804, China. Fax: +86 (021) 6958 4723; Tel: +86 (021) 6958 0239; E-mail: jzdu@tongji.edu.cn

- 1. G. McDonnell and A. D. Russell, *Clin. Microbiol. Rev.*, 1999, **12**, 147-179.
- 2. W. A. Rutala and D. J. Weber, *Clin. Infect. Dis.*, 2004, **39**, 702-709.

- C. Marambio-Jones and E. M. V. Hoek, J. Nanopart. Res., 2010, 12, 1531-1551.
- S. Buffet-Bataillon, P. Tattevin, M. Bonnaure-Mallet and A. Jolivet-Gougeon, *Int. J. Antimicrob. Ag.*, 2012, **39**, 381-389.
- U. Tezel and S. G. Pavlostathis, in *Antimicrobial Resistance in the Environment*, John Wiley & Sons, Inc., 2011, pp. 349-387.
- J. Song, H. Kim, Y. Jang and J. Jang, ACS Appl. Mater. Interfaces, 2013, 5, 11563-11568.
- G. B. Qi, L. L. Li, F. Q. Yu and H. Wang, ACS Appl. Mater. Interfaces, 2013, 5, 10874-10881.
- A. W. Carpenter, D. L. Slomberg, K. S. Rao and M. H. Schoenfisch, *ACS Nano*, 2011, **5**, 7235-7244.
- E. M. Hetrick, J. H. Shin, N. A. Stasko, C. B. Johnson, D. A. Wespe, E. Holmuhamedov and M. H. Schoenfisch, *ACS Nano*, 2008, **2**, 235-246.
- S. Mitra, S. Chandra, D. Laha, P. Patra, N. Debnath, A. Pramanik, P. Pramanik and A. Goswami, *Mater. Res. Bull.*, 2012, 47, 586-594.
- J. H. Park, K. Y. Yoon, H. Na, Y. S. Kim, J. Hwang, J. Kim and Y. H. Yoon, *Sci. Total Environ.*, 2011, 409, 4132-4138.
- H. S. Abdo, K. A. Khalil, S. S. Al-Deyab, H. Altaleb and E. M. Sherif, *Fibers Polym.*, 2013, 14, 1985-1992.
- L. H. Feng, C. L. Zhu, H. X. Yuan, L. B. Liu, F. T. Lv and S. Wang, *Chem. Soc. Rev.*, 2013, 42, 6620-6633.
- C. L. Zhu, Q. Yang, F. T. Lv, L. B. Liu and S. Wang, *Adv. Mater.*, 2013, 25, 1203-1208.
- H. Chong, C. Y. Nie, C. L. Zhu, Q. Yang, L. B. Liu, F. T. Lv and S. Wang, *Langmuir*, 2012, 28, 2091-2098.
- H. X. Yuan, H. Chong, B. Wang, C. L. Zhu, L. B. Liu, Q. Yang,
 F. T. Lv and S. Wang, J. Am. Chem. Soc., 2012, 134, 13184-13187.
- C. F. Xing, G. M. Yang, L. B. Liu, Q. Yang, F. T. Lv and S. Wang, *Small*, 2012, 8, 525-529.
- G. N. Tew, R. W. Scott, M. L. Klein and W. F. Degrado, Acc. Chem. Res., 2010, 43, 30-39.
- S. L. Percival, P. G. Bowler and D. Russell, J. Hosp. Infect., 2005, 60, 1-7.
- S. P. Denyer, W. Barry Hugo and V. D. Harding, *Int. J. Pharm.*, 1985, 25, 245-253.
- A. H. Linton, W. B. Hugo and A. D. Russell, in *Disinfection in veterinary and farm animal practice*, Blackwell Scientific Publications, Oxford, England, 1987, pp. 12-42.
- A. D. Russell, in *Progress in Medicinal Chemistry*, eds. D. K. L. G.P. Ellis and A. W. Oxford, Elsevier, 1998, pp. 133-197.
- A. D. Russell, W. B. Hugo and G. A. J. Ayliffe, *Principle and practices of disinfection, preservation and sterilization, 2nd ed.*, Blackwell Scientific Publications Ltd, Oxford, England., 1992.
- K. M. Reddy, K. Feris, J. Bell, D. G. Wingett, C. Hanley and A. Punnoose, *Appl. Phys. Lett.*, 2007, 90, DOI: 10.1063/1061.2742324.
- J. R. Morones, J. L. Elechiguerra, A. Camacho, K. Holt, J. B. Kouri, J. T. Ramirez and M. J. Yacaman, *Nanotechnology*, 2005, 16, 2346-2353.
 - S. Pal, Y. K. Tak and J. M. Song, *Appl. Environ. Microbiol.*, 2007, 73, 1712-1720.
- I. Sondi and B. Salopek-Sondi, J. Colloid Interface Sci., 2004, 275, 177-182.
- J. S. Kim, E. Kuk, K. N. Yu, J.-H. Kim, S. J. Park, H. J. Lee, S. H. Kim, Y. K. Park, Y. H. Park, C.-Y. Hwang, Y.-K. Kim, Y.-S. Lee, D. H. Jeong and M.-H. Cho, *Nanomed. Nanotechnol. Biol. Med.*, 2007, **3**, 95-101.
- E.-R. Kenawy, S. D. Worley and R. Broughton, Biomacromolecules, 2007, 8, 1359-1384.
- S. Lenoir, C. Pagnoulle, M. Galleni, P. Comp re, R. J & reme and C. Detrembleur, *Biomacromolecules*, 2006, 7, 2291-2296.
- 31. J. Jang and Y. Kim, *Chem. Commun.*, 2008, 4016-4018.
- J. Song, H. Kong and J. Jang, *Chem. Commun.*, 2009, 5418-5420.
 K. Lienkamp, A. E. Madkour, A. Musante, C. F. Nelson, K
 - K. Lienkamp, A. E. Madkour, A. Musante, C. F. Nelson, K. Nüsslein and G. N. Tew, J. Am. Chem. Soc., 2008, 130, 9836-9843
 - Y. Wang, J. Xu, Y. Zhang, H. Yan and K. Liu, *Macromol. Biosci.*, 2011, **11**, 1499-1504.

Page 11 of 12

Journal Name

77.

78.

80.

85.

86.

87.

88.

89.

90.

91.

92.

93.

94.

95.

96.

97.

98.

99

- 35. A. D. Fuchs and J. C. Tiller, Angew. Chem., Int. Ed., 2006, 45, 75. 6759-6762. 76.
- 36. A. M. Klibanov, J. Mater. Chem., 2007, 17, 2479-2482.
- 37. S. Silver, FEMS Microbiol. Rev., 2003, 27, 341-353.
- 38 H. J. Klasen, Burns, 2000, 26, 117-130.
- 39. S. K. Bajpai, Y. M. Mohan, M. Bajpai, R. Tankhiwale and V. Thomas, J. Nanosci. Nanotechnol., 2007, 7, 2994-3010.
- H. Kong and J. Jang, Langmuir, 2008, 24, 2051-2056. 40
- 41. V. K. Sharma, R. A. Yngard and Y. Lin, Adv. Colloid Interface Sci., 2009, 145, 83-96.
- 42. V. Thomas and M. Jayabalan, J. Biomed. Mater. Res. A, 2009, 89A, 192-205.
- 43. K. Vimala, Y. M. Mohan, K. S. Sivudu, K. Varaprasad, S. Ravindra, N. N. Reddy, Y. Padma, B. Sreedhar and K. MohanaRaju, Colloids Surf., B, 2010, 76, 248-258.
- 44 K. A. Juby, C. Dwivedi, M. Kumar, S. Kota, H. S. Misra and P. N. Bajaj, Carbohydr. Polym., 2012, 89, 906-913.
- 45. K. Vasilev, V. Sah, K. Anselme, C. Ndi, M. Mateescu, B. Dollmann, P. Martinek, H. Ys, L. Ploux and H. J. Griesser, Nano Lett., 2010, 10, 202-207.
- 46. M. K. Rai, S. D. Deshmukh, A. P. Ingle and A. K. Gade, J. Appl. Microbiol., 2012, 112, 841-852.
- 47. H. Lu, L. Fan, Q. M. Liu, J. R. Wei, T. B. Ren and J. Z. Du, Polym. Chem., 2012, 3, 2217-2227.
- 48. G. A. Martinez-Castanon, N. Nino-Martinez, F. Martinez-Gutierrez, J. R. Martinez-Mendoza and F. Ruiz, J. Nanopart. Res., 2008, 10, 1343-1348.
- 49. M. Morikawa, K. Kim, H. Kinoshita, K. Yasui, Y. Kasai and N. Kimizuka, Macromolecules, 2010, 43, 8971-8976.
- Y. A. Krutyakov, A. A. Kudrinskiy, A. Y. Olenin and G. V. 50. Lisichkin, Russ. Chem. Rev., 2008, 77, 233-257.
- 51. J. Xu, X. Han, H. Liu and Y. Hu, Colloids Surf., A, 2006, 273, 179-183.
- 52. S. Liu, J. V. M. Weaver, M. Save and S. P. Armes, Langmuir, 2002, 18, 8350-8357.
- 53. Y. F. Chen and M. Yi, Radiat. Phys. Chem., 2001, 61, 65-68.
- 54. L. Zhou, W. Yuan, J. Yuan and X. Hong, Mater. Lett., 2008, 62, 1372-1375.
- 55. Q. Yuan, O. J. Cayre, S. Fujii, S. P. Armes, R. A. Williams and S. Biggs, Langmuir, 2010, 26, 18408-18414.
- H. Lu, L. Yu, Q. M. Liu and J. Z. Du, Polym. Chem., 2013, 4, 56. 3448-3452.
- K. D. Zou, Q. M. Liu, J. Chen and J. Z. Du, Polym. Chem., 2014, 57. 5. 405-411.
- 58. H. L. Liu, S. A. Dai, K. Y. Fu and S. H. Hsu, Int. J. Nanomedicine, 2010, 5, 1017-1028.
- 59. G. Viscardi, P. Quagliotto, C. Barolo, P. Savarino, E. Barni and E. Fisicaro, J. Org. Chem., 2000, 65, 8197-8203.
- 60. J. A. Castillo, A. Pinazo, J. Carilla, M. R. Infante, M. A. Alsina, I. Haro and P. Clapes, Langmuir, 2004, 20, 3379-3387.
- 61. A. Kozubek and J. H. Tyman, Chem. Rev., 1999, 99, 1-26.
- 62. J. J. Kabara and R. Vrable, Lipids, 1977, 12, 753-759.
- M. Zasloff, Nature, 2002, 415, 389-395. 63.
- K. A. Brogden, Nat. Rev. Microbiol., 2005, 3, 238-250. 64.
- 65. J. Song and J. Jang, Adv. Colloid Interface Sci., 2014, 203, 37-50.
- 66. M. R. J. Salton, J. Gen. Physiol., 1968, 52, 227-252.
- 67 S. P. Denyer, Int. Biodeterior. Biodegrad., 1995, 36, 227-245.
- 68. P. Gilbert and L. E. Moore, J. Appl. Microbiol., 2005, 99, 703-715.
- 69. N. M. Milović, J. Wang, K. Lewis and A. M. Klibanov, Biotechnol. Bioeng., 2005, 90, 715-722.
- 70. Y. Qiao, C. Yang, D. J. Coady, Z. Y. Ong, J. L. Hedrick and Y .-Y. Yang, Biomaterials, 2012, 33, 1146-1153.
- 71. F. Nederberg, Y. Zhang, J. P. K. Tan, K. Xu, H. Wang, C. Yang, S. Gao, X. D. Guo, K. Fukushima, L. Li, J. L. Hedrick and Y.-Y. Yang, Nat. Chem., 2011, 3, 409-414.
- 72. L. Liu, K. Xu, H. Wang, P. K. Jeremy Tan, W. Fan, S. S. Venkatraman, L. Li and Y.-Y. Yang, Nat. Nano, 2009, 4, 457-463.
- 73. J. M. Hwang, S. H. Yeom and K. Y. Jung, J. Ind. Eng. Chem., 2007, 13, 474-479.
- 74. M. Lv, S. Su, Y. He, Q. Huang, W. Hu, D. Li, C. Fan and S.-T. Lee, Adv. Mater., 2010, 22, 5463-5467.

- M. N. V. R. Kumar, R. A. A. Muzzarelli, C. Muzzarelli, H. Sashiwa and A. J. Domb, Chem. Rev., 2004, 104, 6017-6084.
- H. Sashiwa and S.-i. Aiba, Prog. Polym. Sci., 2004, 29, 887-908.
- E. I. Rabea, M. E. T. Badawy, C. V. Stevens, G. Smagghe and W. Steurbaut, Biomacromolecules, 2003, 4, 1457-1465.
- H. K. No, N. Y. Park, S. H. Lee and S. P. Meyers, Int. J. Food Microbiol., 2002, 74, 65-72.
- M. W. Huh, I. K. Kang, D. H. Lee, W. S. Kim, D. H. Lee, L. S. 79. Park, K. E. Min and K. H. Seo, J. Appl. Polym. Sci., 2001, 81, 2769-2778.
 - Z. L. Shi, K. G. Neoh, E. T. Kang and W. Wang, Biomaterials, 2006, 27, 2440-2449.
- 81. G. Seyfriedsberger, K. Rametsteiner and W. Kern, Eur. Polym. J., 2006, 42, 3383-3389.
- 82. M. Ignatova, S. Voccia, B. Gilbert, N. Markova, D. Cossement, R. Gouttebaron, R. J érôme and C. J érôme, Langmuir, 2005, 22, 255-262
- M. Schindler and M. J. Osborn, Biochemistry, 1979, 18, 4425-83. 4430.
- D. R. Storm, K. S. Rosenthal and P. E. Swanson, Annu. Rev. 84. Biochem., 1977, 46, 723-763.
 - M. B. Harney, R. R. Pant, P. A. Fulmer and J. H. Wynne, ACS Appl. Mater. Interfaces, 2008, 1, 39-41.
 - O. Bouloussa, F. Rondelez and V. Semetey, Chem. Commun., 2008, 951-953.
 - W. Z. Yuan, J. R. Wei, H. Lu, L. Fan and J. Z. Du, Chem. Commun., 2012, 48, 6857-6859.
 - C. Zhang, Y. Q. Zhu, C. C. Zhou, W. Z. Yuan and J. Z. Du, Polym. Chem., 2013, 4, 255-259.
 - H. S. Zhu, Q. R. Geng, W. Q. Chen, Y. Q. Zhu, J. Chen and J. Z. Du, J. Mater. Chem. B, 2013, 1, 5496-5504.
 - D. A. Tomalia, Prog. Polym. Sci., 2005, 30, 294-324.
 - R. Esfand and D. A. Tomalia, Drug Discov Today, 2001, 6, 427-436
 - S. S. Abkenar and R. M. A. Malek, Cellulose, 2012, 19, 1701-1714.
 - S. J. Strydom, W. E. Rose, D. P. Otto, W. Liebenberg and M. M. de Villiers, Nanomed. Nanotechnol. Biol. Med., 2013, 9, 85-93.
 - Y. Wen, Z. Tan, F. Sun, L. Sheng, X. Zhang and F. Yao, Mater. Sci. Eng., C, 2012, 32, 2026-2036.
 - M. N. Melo, R. Ferre and M. A. R. B. Castanho, Nat. Rev. Microbiol., 2009, 7, 245-250.
 - H. A. Pereira, Curr. Pharm. Biotechnol., 2006, 7, 229-234.
 - L. M. Rossi, P. Rangasamy, J. Zhang, X.-Q. Qiu and G. Y. Wu, J. Pharm. Sci., 2008, 97, 1060-1070.
 - R. E. Hancock and H. G. Sahl, Nat. Biotechnol., 2006, 24, 1551-1557.
 - S. Zhu and B. Gao, Fased J., 2009, 23, 13-20.
- 100. G. Maróti, A. Kereszt, É. Kondorosi and P. Mergaert, Res. Microbiol., 2011, 162, 363-374.
- 101. P. Yang, A. Ramamoorthy and Z. Chen, Langmuir, 2011, 27, 7760-7767.
- 102. A. Giuliani, G. Pirri and S. F. Nicoletto, Cent. Eur. J. Biol., 2007, 2, 1-33.
- 103. F. Porcelli, B. A. Buck-Koehntop, S. Thennarasu, A. Ramamoorthy and G. Veglia, Biochemistry, 2006, 45, 5793-5799.
- 104. L. Yang, T. M. Weiss, R. I. Lehrer and H. W. Huang, Biophys. J., 2000, 79, 2002-2009.
- 105. K. Matsuzaki, Biochim. Biophys. Acta, 1999, 1462, 1-10.
- 106. V. Dhople, A. Krukemeyer and A. Ramamoorthy, Biochim. Biophys. Acta, 2006, 1758, 1499-1512.
- J. K. Lee, S. W. Chang, H. Perinpanayagam, S. M. Lim, Y. J. 107. Park, S. H. Han, S. H. Baek, Q. Zhu, K. S. Bae and K. Y. Kum, J. Endod., 2013, 39, 1625-1629.
- 108. B. Spudy, F. D. Sonnichsen, G. H. Waetzig, J. Grotzinger and S. Jung, Biochem. Biophys. Res. Commun., 2012, 427, 207-211.
- 109. H. J. Vogel, D. J. Schibli, W. Jing, E. M. Lohmeier-Vogel, R. F. Epand and R. M. Epand, Biochem. Cell Biol., 2002, 80, 49-63.
- 110. H. Choi, J. S. Hwang and D. G. Lee, Biochim. Biophys. Acta, 2013, 1828, 2745-2750.
- E. Breukink and B. de Kruijff, Biochim. Biophys. Acta, 1999, 111. **1462**, 223-234.

- E. M. Molloy, D. Field, O. C. PM, P. D. Cotter, C. Hill and R. P. Ross, *PloS one*, 2013, 8, e58530.
- M. E. Falagas and S. K. Kasiakou, *Clin. Infect. Dis.*, 2005, 40, 1333-1341.
- A. Batirel, Balkan, II, O. Karabay, C. Agalar, S. Akalin, O. Alici, E. Alp, F. A. Altay, N. Altin, F. Arslan, T. Aslan, N. Bekiroglu, S. Cesur, A. D. Celik, M. Dogan, B. Durdu, F. Duygu, A. Engin, D. O. Engin, I. Gonen, E. Guclu, T. Guven, C. A. Hatipoglu, S. Hosoglu, M. K. Karahocagil, A. U. Kilic, B. Ormen, D. Ozdemir, S. Ozer, N. Oztoprak, N. Sezak, V. Turhan, N. Turker and H. Yilmaz, *Eur. J. Clin. Microbiol. Infect. Dis.*, 2014, 33, 1311-1322.
- A. F. Mohamed, O. Cars and L. E. Friberg, J. Antimicrob. Chemother., 2014, 69, 1350-1361.
- G. N. Tew, D. Liu, B. Chen, R. J. Doerksen, J. Kaplan, P. J. Carroll, M. L. Klein and W. F. DeGrado, *Proc. Natl. Acad. Sci.*, 2002, 99, 5110-5114.
- 117. B. Findlay, G. G. Zhanel and F. Schweizer, *Antimicrob. Agents Chemother.*, 2010, **54**, 4049-4058.
- 118. C. Chen, J. Hu, S. Zhang, P. Zhou, X. Zhao, H. Xu, X. Zhao, M. Yaseen and J. R. Lu, *Biomaterials*, 2012, **33**, 592-603.
- A. Al-Ahmad, D. Laird, P. Zou, P. Tomakidi, T. Steinberg and K. Lienkamp, *PloS one*, 2013, 8, e73812.
- 120. J. Z. Du and R. K. O'Reilly, *Soft Matter*, 2009, **5**, 3544-3561.
- 121. W. Q. Chen and J. Z. Du, *Sci. Rep.*, 2013, **3**, DOI: 10.1038/srep02162.
- 122. Q. M. Liu, J. Chen and J. Z. Du, *Biomacromolecules*, 2014, DOI: 10.1021/bm500676e.
- 123. X. Hu, J. Hu, J. Tian, Z. Ge, G. Zhang, K. Luo and S. Liu, J. Am. Chem. Soc., 2013, 135, 17617-17629.
- 124. J. Z. Du and H. Sun, ACS Appl. Mater. Interfaces, 2014, DOI: 10.1021/am502663j.
- C. Sanson, O. Diou, J. Thevenot, E. Ibarboure, A. Soum, A. Brulet, S. Miraux, E. Thiaudiere, S. Tan, A. Brisson, V. Dupuis, O. Sandre and S. Lecommandoux, ACS Nano, 2011, 5, 1122-1140.
- 126. T. B. Ren, Q. M. Liu, H. Lu, H. M. Liu, X. Zhang and J. Z. Du, J. Mater. Chem., 2012, 22, 12329-12338.
- 127. Q. M. Liu, H. S. Zhu, J. Y. Qin, H. Q. Dong and J. Z. Du, Biomacromolecules, 2014, 15, 1586-1592.
- 128. H. Lomas, I. Canton, S. MacNeil, J. Z. Du, S. P. Armes, A. J. Ryan, A. L. Lewis and G. Battaglia, *Adv. Mater.*, 2007, **19**, 4238-4243.
- 129. Y. Q. Zhu, F. Y. K. Wang, C. Zhang and J. Z. Du, ACS Nano, 2014, 8, 6644-6654.
- C. C. Zhou, M. Z. Wang, K. D. Zou, J. Chen, Y. Q. Zhu and J. Z. Du, ACS Macro Lett., 2013, 2, 1021-1025.
- Y. Q. Zhu, L. Liu and J. Z. Du, *Macromolecules*, 2013, 46, 194-203.
- L. Fan, H. Lu, K. D. Zou, J. Chen and J. Z. Du, *Chem. Commun.*, 2013, 49, 11521-11523.
- 133. T. T. Liu, W. Tian, Y. Q. Zhu, Y. Bai, H. X. Yan and J. Z. Du, *Polym. Chem.*, 2014, DOI: 10.1039/c1034py00501e.
- 134. Y. Q. Zhu, L. Fan, B. Yang and J. Z. Du, ACS Nano, 2014, 8, 5022-5031.