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Micromagnetic and morphological characterization of heteropolymer human ferritin cores

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The physical properties of *in vitro* iron-reconstituted and genetically engineered human heteropolymer ferritins were investigated. High-angle annular dark-field scanning transmission electron microscopy (HAADF-STEM), electron energy-loss spectroscopy (EELS), and ⁵⁷Fe Mössbauer spectroscopy were employed to ascertain (1) the microstructural, electronic, and micromagnetic properties of the nanosized iron cores, and (2) the effect of the H and L ferritin subunit ratios on these properties. Mössbauer spectroscopic signatures indicate that all iron within the core is in the high spin ferric state. Variable temperature Mössbauer spectroscopy for H-rich (H₂₁/L₃) and L-rich (H₂/L₂₂) ferritins reconstituted at 1000 ⁵⁷Fe/protein indicates superparamagnetic behavior with blocking temperatures of 19 K and 28 K, while HAADF-STEM measurements give average core diameters of (3.7 ± 0.6) nm and (5.9 ± 1.0) nm, respectively. Most significantly, H-rich proteins reveal elongated, dumbbell, and crescent-shaped cores, while L-rich proteins present spherical cores, pointing to a correlation between core shape and protein shell composition. Assuming an attempt time for spin reversal of $\tau_0 = 10^{-11}$ s, the Néel–Brown formula for spin-relaxation time predicts effective magnetic anisotropy energy densities of 6.83×10^4 J m⁻³ and 2.75×10^4 J m⁻³ for H-rich and L-rich proteins, respectively, due to differences in surface and shape contributions to magnetic anisotropy in the two heteropolymers. The observed differences in shape, size, and effective magnetic anisotropies of the derived biomineral cores are discussed in terms of the iron nucleation sites within the interior surface of the heteropolymer shells for H-rich and L-rich proteins. Overall, our results imply that site-directed nucleation and core growth within the protein cavity play a determinant role in the resulting core morphology. Our findings have relevance to iron biomineralization processes in nature and the growth of designer's magnetic nanoparticles within recombinant apoferritin nano-templates for nanotechnology.

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Introduction

Mammalian ferritins are predominantly hetero-polymeric species consisting of 24 structurally similar, but functionally different subunit types named H (for Heavy) and L (for Light).¹ The variability in the composition of heteropolymer ferritins is related to the expressions of H and L subunits,^{2,3} which co-assemble in various H to L ratios, with tissue specific distribution, to form shell-like protein structures of ~12 nm outer diameter and ~8 nm inner cavity diameter, where thousands of

iron atoms can be sequestered.^{1,3-5} The human H-subunit has a dinuclear iron center, known as the ferroxidase center, where fast conversion of Fe²⁺ to Fe³⁺ occurs. In contrast, the human L-subunit lacks such a center but provides sites for iron cluster nucleation and iron mineralization due to a higher density of carboxyl groups exposed on the inner cavity surface.^{1,5-7}

It is generally accepted that after rapid oxidation of Fe²⁺ at the ferroxidase centers of H-subunits, the Fe³⁺ ions migrate to the protein cavity and bind at nucleation sites on the L-subunits where iron cluster nucleation and subsequent growth of the iron biomineral core⁸⁻¹² is initiated. Even though H-subunits lack such nucleation sites, formation of ferritin iron cores inside H-subunit homopolymers does still occur, presumably assisted by acidic residues within the cavity.^{1,8,11,13,14} Despite the widespread occurrence of heteropolymer ferritins in tissues of vertebrates, very little is known about the complementary roles that H- and L-subunits play within the protein, due to a lack of availability of recombinant heteropolymer experimental

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systems. In a groundbreaking study, our research group has successfully engineered a novel ferritin expression system to produce recombinant heteropolymer ferritins with different H/L subunit ratios.¹⁵ Our unique plasmid design can be easily tuned to allow the synthesis of a full spectrum of heteropolymer ferritins, from H-rich to L-rich ferritins and any combinations in-between (isoferritins). The two ferritin subunits appear to play complementary ferroxidation and mineralization functions, since different mixture of subunits affects the rate and the amount of iron deposited inside the protein cavity.¹⁵

Numerous investigations on the structure and morphology of the iron mineral inside ferritin^{16–23} have been reported, but a systematic study of the iron cores in human heteropolymer ferritins has not, yet, been performed. Natural ferritins with different H to L subunit ratios associated with different organs correlate with different rates of ferritin biomineral formation, and likely, with biomineral order, degree of crystallinity, and iron turnover.^{3,24,25} In theory, fewer ferroxidase centers decrease the rate of iron oxidation, and therefore the rate of iron deposition and core formation and should lead to more crystalline iron cores. However, studies have reported that the low percentage of catalytic sites in L-rich ferritins (such as liver ferritin) contributed to a less crystalline and low mineral order iron core.²⁶ Interestingly, ferritins which had amorphous iron cores when isolated from natural sources formed crystalline ferrihydrite cores upon reconstitution, that is when the iron core is reconstituted *in vitro* using native ferritin stripped of iron.^{3,27–29} Once oxidized, ferric ions are stored inside the ferritin cavity as an inorganic hydrated iron oxide ferrihydrite^{30,31} ($5\text{Fe}_2\text{O}_3 \cdot 9\text{H}_2\text{O}$), the morphology of which has been typically investigated by electron microscopy.^{16–20} It was reported that the iron nanoparticles formed inside recombinant homopolymer human H-ferritin (HuHF) are not discrete and exhibited poor contrast, whereas those inside human L-ferritin (HuLF) homopolymers exhibited discrete, electron-dense cores with well-defined spherical shapes.¹⁹ These differences between natural ferritins and recombinant homopolymer ferritins suggest that the morphology of the ferritin iron core depends on the protein shell composition, and the number of nucleation sites present on the protein.¹⁹

Ferrihydrite occurs in nature as a nano-phase material with no bulk counterpart.³¹ The iron ions are in the high spin ferric state (Fe^{3+} , $S = 5/2$) octahedrally ($\sim 80\%$) and/or tetrahedrally ($\sim 20\%$) coordinated to oxygen ions and super-exchange-coupled to produce an antiferromagnetically ordered material of various degrees of crystallinity, referred to as 2-line and 6-line ferrihydrite, based on XRD structure determination.³² The antiferromagnetically ordered ferritin core possesses a net magnetic moment due to spin non-compensation at the surface and the possible presence of defects within the interior of the core, as originally proposed by Néel for single-magnetic-domain antiferromagnetic particles.^{33–35} The magnetic moment of the ferritin core of horse spleen ferritin has been measured to be only $300 \mu_{\text{B}}$,³⁶ where μ_{B} is the Bohr magneton. The process of biomineralization in ferritin has been exploited in materials science to produce monodispersed metal and metal-oxide magnetic nanoparticles by biomimetic synthesis within

protein cages and viral capsids.^{37,38} The first magnetic material synthesized within horse spleen apoferritin cages was magnetite³⁹ or maghemite, both of which are ferrimagnetically ordered, and therefore exhibit high magnetization. This material has properly been coined “magnetoferritin” and has found multiple biomedical applications.⁴⁰ The availability of recombinant human heteropolymer apoferritin nanocages of various L/H ratios, made possible *via* our novel ferritin expression system in *E. coli*, afford materials scientists additional protein nano-templates to produce biocompatible magnetic nanoparticles within the confined space of their cavities. Biocompatible magnetic nanoparticles have important applications in nanomedicine and nanobiotechnology for MRI imaging enhancement, magnetically targeted drug delivery, non-viral cell transfection, magnetic hyperthermia, and cell separation applications.^{41,42} In many medical and biotechnological applications, the magnetization and magnetic relaxation properties of the resulting nanoparticles are of interest, as they must be tailored to specific applications. Mössbauer spectroscopy has uniquely contributed to elucidating the electronic and micromagnetic properties of ferritin, magnetoferritin, and other apoferritin derived magnetic nanoparticles,^{43–48} while bioanalytical applications of Mössbauer spectroscopy have been recently reviewed.⁴⁹

Herewith, we present high resolution images obtained *via* high-angle annular dark-field scanning transmission electron microscopy (HAADF-STEM) of recombinant human H-rich heteropolymer (H_{21}/L_3) ferritin, and recombinant human L-rich heteropolymer (H_2/L_{22}) ferritin reconstituted to 1000 Fe/protein, to better understand the effect of protein composition on the shape and crystallinity of the core. We complement these measurements with EELS and ^{57}Fe Mössbauer spectroscopy⁴⁵ to ascertain the iron oxidation state in the biomineral cores and probe their micromagnetic properties. We hypothesize that differences in structural details observed by high resolution electron microscopy ought to be reflected in the micromagnetic properties of the cores, which determine their superparamagnetic properties.⁴² Manipulation of the magnetic relaxation properties of biocompatible magnetic nanoparticles is very desirable for applications in nanomedicine. As expected, the results point to correlations between the microstructural morphology of the derived iron cores and their micromagnetic properties.

Electron microscopy

Fig. 1 compares representative STEM images obtained for the L-rich and H-rich proteins reconstituted at 1000 Fe/protein. Distinctly different core shapes are observed in the two ferritin heteropolymers. The L-rich proteins promote the formation of spherical core shapes (Fig. 1A). In contrast, the H-rich proteins (Fig. 1B) present non-spherical cores; various shapes are seen dominated by elongated, dumbbell, and crescent-shaped cores. Furthermore, the H-rich proteins show a higher degree of crystallinity, as evidenced by the more clearly resolved lattice fringes, which indicated increased crystalline order. Fig. 2 gives the histograms of the particle size



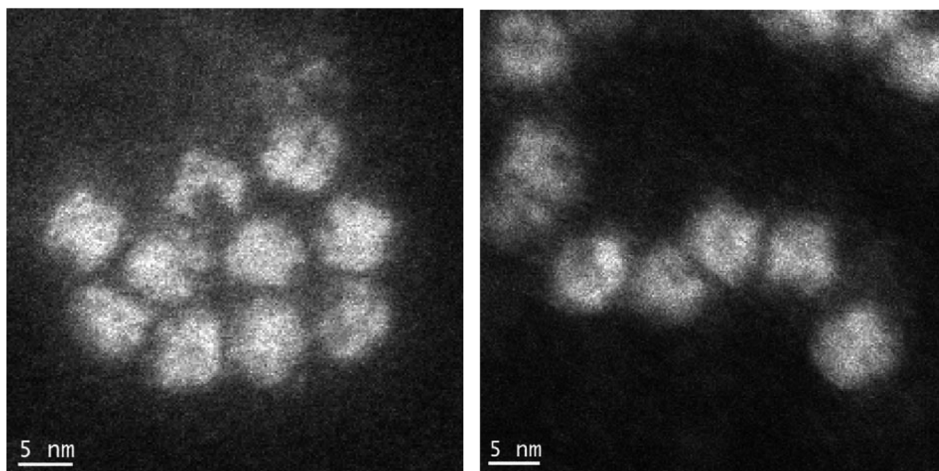
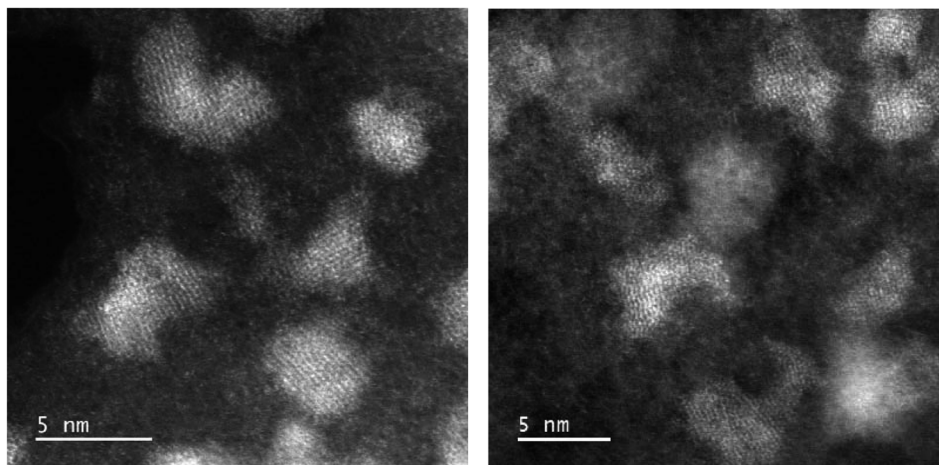
(A) L-Rich (H_2/L_{22}) 1000 Fe/protein(B) H-Rich (H_{21}/L_3) 1000 Fe/protein

Fig. 1 Comparison of iron cores grown within the L-rich (A) and H-rich (B) proteins at an iron level loading of 1000 Fe/protein. Distinctly different core shapes are observed. The L-rich proteins present spherical cores, while the H-rich proteins present irregular shaped, elongated, dumbbell, and crescent-like cores. The H-rich protein cores are discrete, while the L-rich cores appear more diffuse and amorphous.

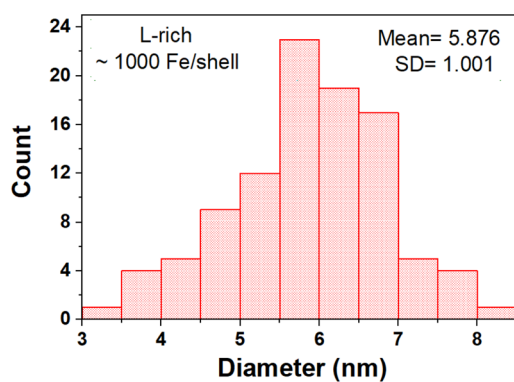
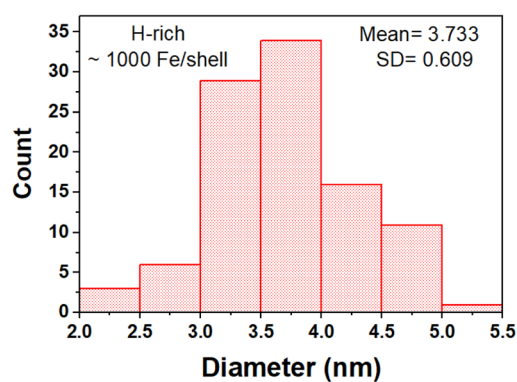
(A) L-Rich (H_2/L_{22})(B) H-Rich (H_{21}/L_3)

Fig. 2 Histograms of the particle size distributions of the ferrihydrite mineral cores grown in (A) L-rich heteropolymers and (B) H-rich heteropolymers, reconstituted to 1000 Fe/protein.



(A) L-Rich (as expressed in *E. coli*, contains ~ 100 Fe/protein)

(B) H-Rich (as expressed in *E. coli*, contains ~ 100 Fe/protein)

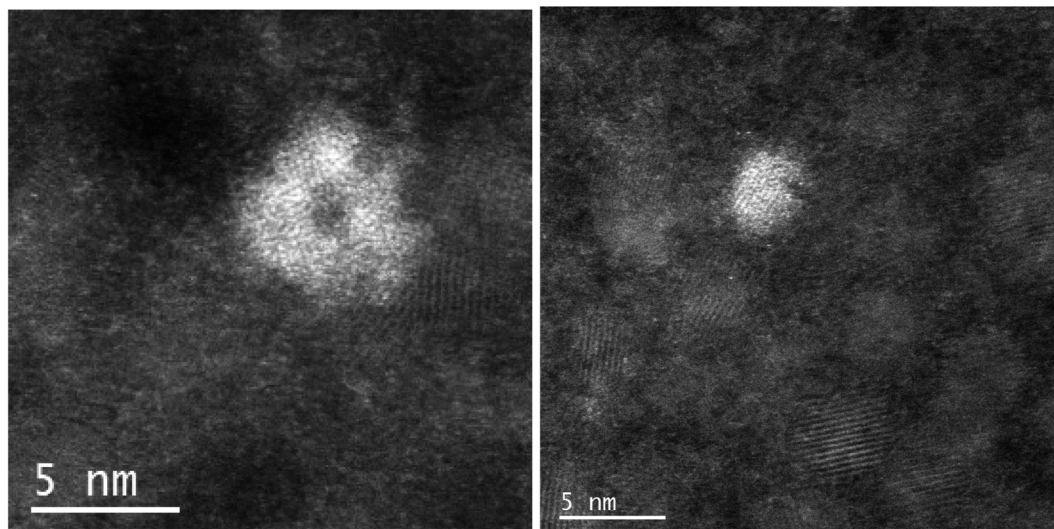


Fig. 3 Comparison of nascent iron cores of ~ 100 Fe/protein loading for (A) L-rich and (B) H-rich heteropolymers. Site-directed iron nucleation produces distinctly different shapes of iron cores (see text for details).

distributions, assuming spherical cores. For the L-rich ferritin cores, the estimated average core diameter, based on 100 particles count and Gaussian particle-size distribution was $\langle d_{L\text{-rich}} \rangle = (5.9 \pm 1.0)$ nm, while that for the H-rich proteins was $\langle d_{H\text{-rich}} \rangle = (3.7 \pm 0.6)$ nm (Fig. 2). This indicates that under identical iron reconstitution conditions, the L-rich heteropolymers promote the formation of larger and more spherical iron cores compared to H-rich heteropolymers.

As expressed in *E. coli*, purified recombinant heteropolymer ferritins contained a small iron core of ≈ 100 Fe/protein as determined by an iron reductive mobilization assay.⁵⁰ To further probe the observed difference in the morphology of the cores, and to image the initial stages of iron nucleation, we obtained HAADF-STEM micrographs of the heteropolymer H-

rich and L-rich ferritins containing these small and nascent iron cores. The images are shown in Fig. 3 and the histograms of the corresponding size distributions are shown in Fig. 4. It is noted that the distinct difference in morphology has an early onset as it is already apparent in the nascent cores of mean average diameters of $\langle d_{L\text{-rich}} \rangle = (2.9 \pm 1.0)$ nm and $\langle d_{H\text{-rich}} \rangle = (1.8 \pm 0.5)$ nm. This early difference in iron accumulation and core morphology appears to be caused by site-directed iron cluster nucleation^{51,52} at specific nucleation sites on the interior cavity surface of the heteropolymers. The presence of nucleation sites on the interior surface of L-rich proteins produce a crown-looking nascent core, as shown in Fig. 3A. The nucleated iron ions appear to grow from the surface of the interior cavity while the center is void of iron. Upon further core growth,

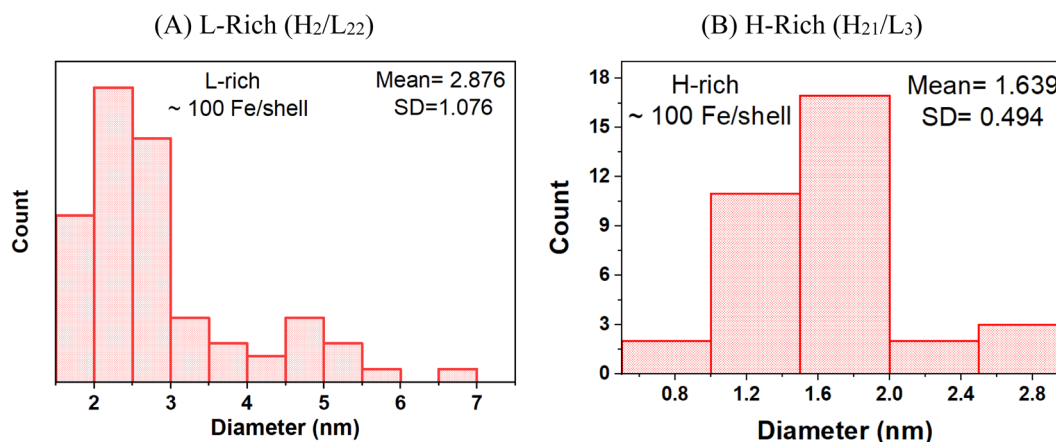


Fig. 4 Histograms of the particle size distributions of the ferrihydrite mineral cores grown in (A) L-rich heteropolymers and (B) H-rich heteropolymers, containing ~ 100 Fe/protein.



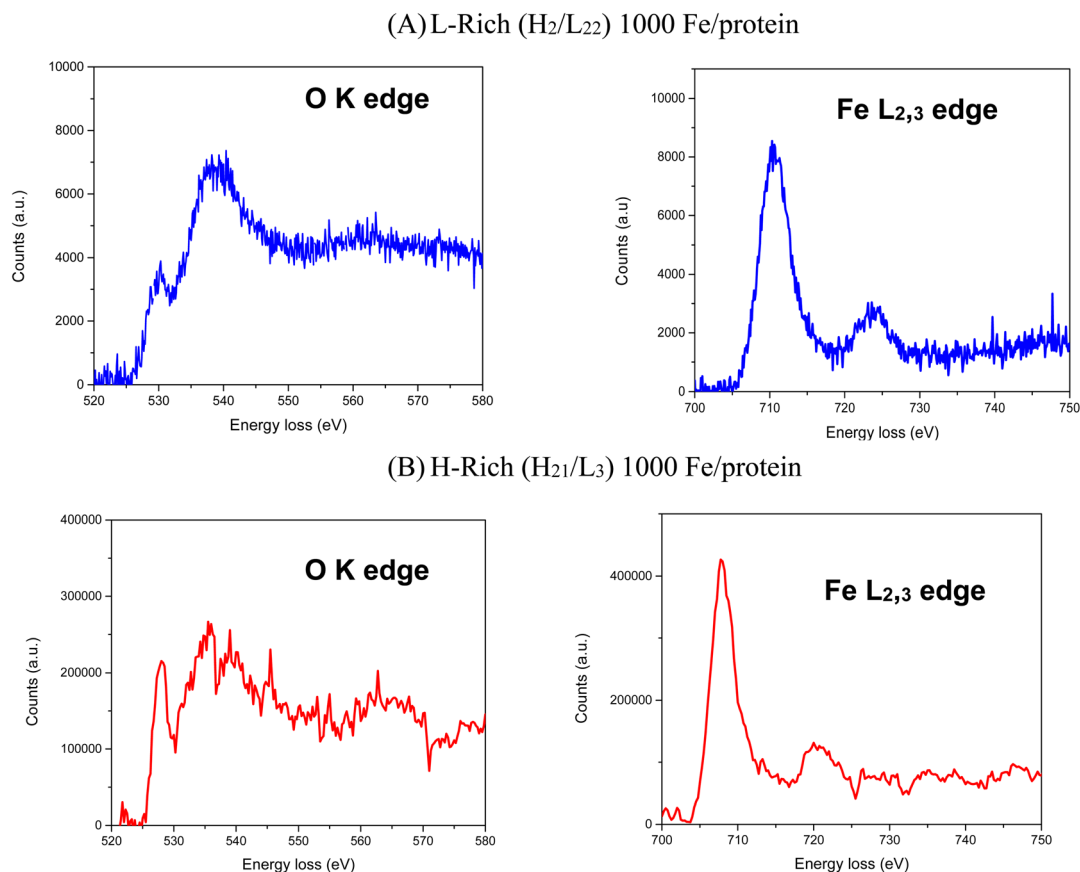


Fig. 5 EELS of the ferrihydrite mineral cores grown in (A) L-rich heteropolymers and (B) H-rich heteropolymers, containing 1000 Fe/protein. The shape of the O K edges combined with the ratio of the L₃/L₂ peaks for Fe are consistent with iron in the ferric state (Fe³⁺).

iron nucleation expands towards the central region to produce the spherical shapes observed in Fig. 1A. Our data corroborate a previously proposed iron-core-growth mechanism influenced by the L/H ratio in heteropolymer proteins.¹⁹ The image shown in Fig. 3A also resembles that of hepatic mineral core obtained from thin sections of a liver biopsy¹⁸ from a patient with hereditary haemochromatosis. It is well known that hepatic ferritin is an L-rich ferritin. In contrast, the nascent mineral core for the H-rich protein is smaller in size and appears to grow from a single nucleation site (Fig. 3B), suggesting a role for the ferritin shell and/or subunit composition as a template for core morphology.

Electron energy-loss spectroscopy (EELS) was also performed on the H-rich and L-rich samples shown in Fig. 5. The O K edge shows 3 distinctive peaks at 529 eV, 540 eV and 564 eV loss. The shape of the O K edges combined with the ratio of the L₃/L₂ peaks for Fe are consistent with iron in the ferric state.^{53,54} This agrees with the Mössbauer results given in the following section.

Mössbauer spectroscopy

Fig. 6 and 7 present selected Mössbauer spectra of L-rich and H-rich proteins, respectively, fit to the core/shell model of the ferrihydrite mineral core of ferritin.⁵⁵ This model treats the core as the superposition of two phases; an interior antiferromagnetically spin-ordered ferrihydrite phase (core) surrounded by a spin

disordered phase (shell) on the surface of the mineral core. At room temperature, both samples present a simple Mössbauer quadrupolar absorption at the central region of the velocity axis range. As the temperature is lowered the spectra become complex, broaden, and eventually split into a six-line magnetic hyperfine absorption spectrum, extending over the full range of the velocity axis. This temperature spectral profile is typical of an ensemble of magnetically ordered, small magnetic particles undergoing superparamagnetic relaxation processes relative to the uniaxial magnetic anisotropy axis of the particle.⁵⁶

At room temperature Mössbauer absorption spectra were fit to the superposition of two quadrupole doublet distributions, corresponding to the ordered interior core phase (green trace) and the disordered shell phase on the surface (purple trace), giving the fitted parameters of the average isomer shift (δ) and average quadrupole splitting (ΔE_q) for each phase, tabulated in Table 1 for the L-rich proteins, and Table 2 for the H-rich proteins. It is seen that at room temperature all phases share the same isomer shift $\delta \approx 0.36 \text{ mm s}^{-1}$, which indicates that iron is in the ferric high spin (Fe³⁺, $S = 5/2$) state. The EELS spectra also indicated iron in the Fe³⁺ state. The smaller quadrupole splitting values $\Delta E_q \approx (0.50\text{--}0.57) \text{ mm s}^{-1}$ are associated with interior iron atoms, and are consistent with higher coordination symmetry, while the larger values of quadrupole splitting $\Delta E_q \approx (0.87\text{--}0.99) \text{ mm s}^{-1}$ are associated



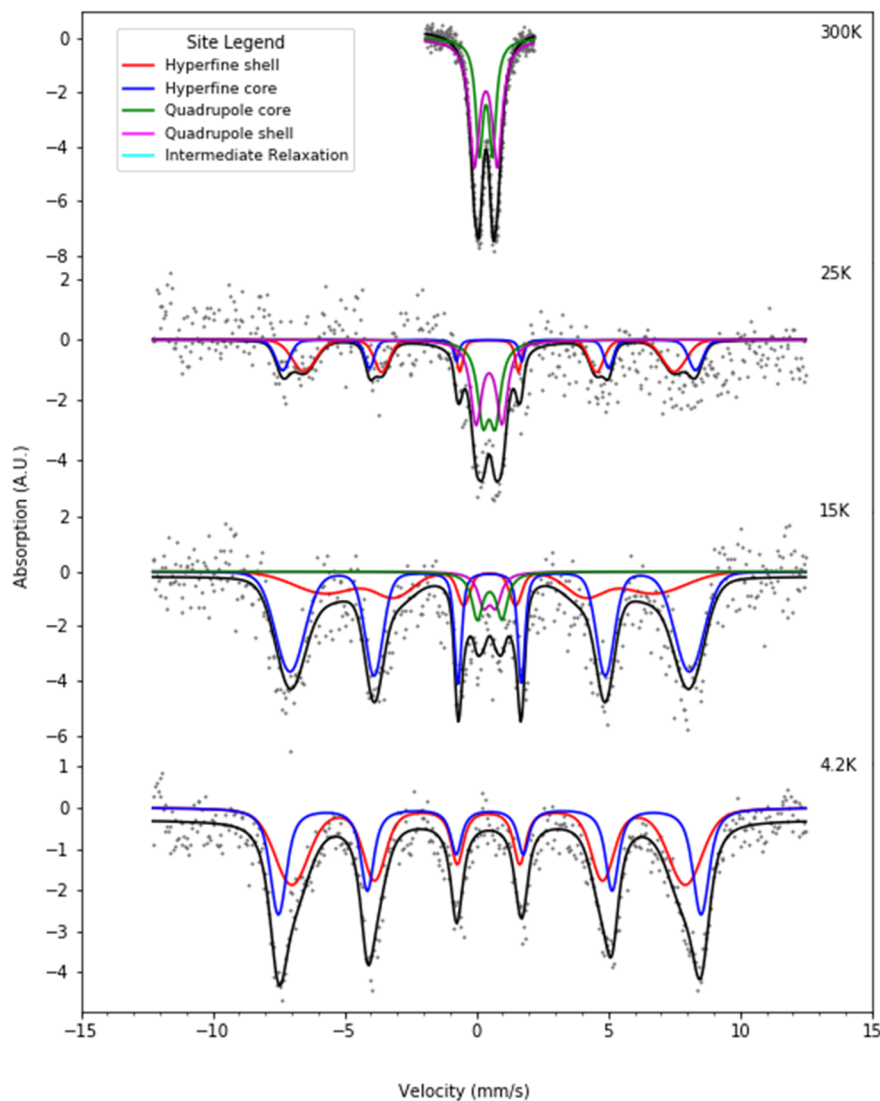
L-rich 1000 ^{57}Fe /protein

Fig. 6 Selected Mössbauer spectra for the L-rich heteropolymer ferritin reconstituted at 1000 ^{57}Fe /protein at various temperatures fitted to the core/shell model of the ferritin biomineral core (see site legend). Selected values of fitted parameters are given in Table 1.

with lower coordination symmetry of iron ions on/or close to the surface (shell), where the ion coordination symmetry gets increasingly distorted as one approaches the surface. This is due to the interruption of the crystallographic order at the surface of the ferrihydrite biomineral core, or the core/protein interface. Thus, the average quadrupole splitting of the outer iron ions on the shell (or surface) are consistently larger compared to those in the interior of the core. At room temperature, for the L-rich protein 60% of the absorption area is associated with iron ions on the shell (Table 1) with distorted coordination symmetry, while for the H-rich proteins only 40% of sites are distorted (Table 2). This is consistent with a higher crystallinity for the H-rich cores compared to the L-rich cores.

As the temperature of the sample is decreased, the spectra pass slowly from quadrupolar (two-line) to magnetic (six-line). The smaller particles in the distribution, primarily lying at the

core/protein interface, are the last to pass into the magnetic six-line regime, while the larger particles are the first to do so. At room temperature, thermal energy kT prevents observation of the antiferromagnetic order of the ferric ion spins within the crystallographic lattice of the mineral core. The spins fluctuate or flip coherently and continuously between opposite directions of the uniaxial anisotropy axis of the core, with a relaxation time τ_s shorter than the characteristic measuring time for Mössbauer spectroscopy $\tau_{\text{Möss}}$, ($\tau_s < \tau_{\text{Möss}}$, fast relaxation). In this case the nucleus records an average internal magnetic field of zero, resulting in two-line quadrupolar spectra. However, upon lowering the temperature the magnetic order of the mineral is revealed ($\tau_s > \tau_{\text{Möss}}$, slow relaxation). In this case the electronic spin direction, and therefore the internal magnetic fields, persist long enough for the nucleus to record the internal magnetic field before it flips into the opposite direction. This



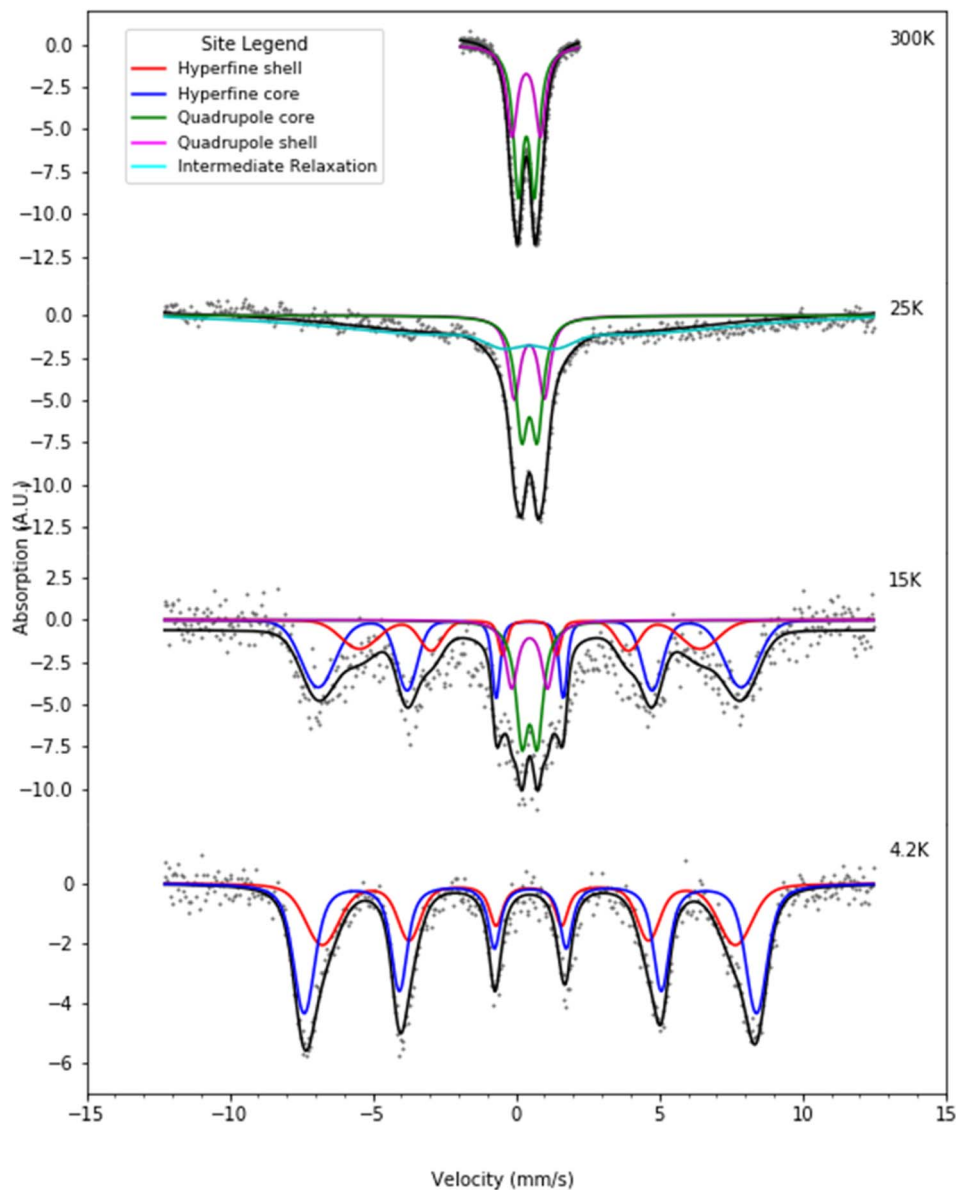


Fig. 7 Selected Mössbauer spectra for the H-rich heteropolymer ferritin reconstituted at 1000 ^{57}Fe /protein at various temperatures fitted to the core/shell model of the ferritin biomineral core (see site legend). Selected values of fitted parameters are given in Table 2.

results in a six-line pattern Zeeman-split Mössbauer spectrum. The characteristic measuring time for Mössbauer, $\tau_{\text{Möss}}$, is given by the Larmor precession time of the iron nuclear spin in the hyperfine magnetic field experienced by the nucleus, due to correlated electronic spins in its vicinity, $\tau_{\text{Möss}} = \tau_L = 10^{-8}$ s. Interior core ions experience on average a larger value of hyperfine magnetic field compared to the shell. Thus, the spectra at 4.2 K are also fit with the superposition of two hyperfine field distribution subsites (core/shell). The relative % absorption areas of the average hyperfine fields for the two subsites are preserved, compared to those observed at room temperature for the quadrupolar subsite % absorption areas (Tables 1 and 2). At intermediate temperatures the spectra are more complex due to the superposition of quadrupolar (fast relaxation), magnetic (slow relaxation) and intermediate

relaxation ($\tau_s \approx \tau_{\text{Möss}}$) processes arising from the presence of particle size distributions (Fig. 2). The temperature spectral profiles observed in Fig. 6 and 7 are characteristic of superparamagnetic particles; they allow estimation the blocking temperature, T_B , of the nanoparticle ensembles.

Experimentally, T_B is defined as the temperature at which the spectral absorption area is equally divided between quadrupolar and magnetic subsites. We calculate T_B (L-rich) = 28 K and T_B (H-rich) = 19 K. Theoretically, spin relaxation in magnetically isolated (non-interacting) nanoparticle ensembles, as is the case for ferritin samples, is governed by the Néel-Brown formula:^{57,58}

$$\tau_s = \tau_0 e^{\frac{K_{\text{eff}} V}{k_B T}} \quad (1)$$



Table 1 Selected Mössbauer fit parameters for the L-rich heteropolymer ferritin^a

<i>T</i> (K)	Site	δ (mm s ⁻¹)	ΔE_q (mm s ⁻¹)	H_{hf} (kOe)	Area (%)	Core or shell
300	1	0.37	0.50	0	39.8	Core
	2	0.36	0.87	0	60.2	Shell
25	1	0.49	0.46	0	23.5	Core
	2	0.49	0.98	0	25.8	Shell
	3	0.49	0	484.2	19.1	Core
	4	0.49	0	434.2	31.7	Shell
4.2	3	0.51	0	495.5	43.6	Core
	4	0.46	0	461.6	56.4	Shell

^a Sites 1 and 2 are associated with quadrupolar spectra (green and purple traces in Fig. 6). The reported parameters correspond to the average values of fitted quadrupole distributions. Sites 3 and 4 are associated with magnetic hyperfine spectra (blue and red traces in Fig. 6). The reported parameters correspond to the average values of fitted hyperfine field distributions. Estimated uncertainties: δ (± 0.02 mm s⁻¹), ΔE_q (± 0.04 mm s⁻¹), H_{hf} (± 2 kOe), area ($\pm 3\%$).

Table 2 Selected Mössbauer fit parameters for the H-rich heteropolymer ferritin^a

<i>T</i> (K)	Site	δ (mm s ⁻¹)	ΔE_q (mm s ⁻¹)	H_{hf} (kOe)	Area (%)	Core or shell
300	1	0.36	0.57	0	59	Core
	2	0.36	0.99	0	41	Shell
15	1	0.48	0.54	0	19.4	Core
	2	0.48	1.25	0	11.6	Shell
	3	0.48	0	484.2	46.9	Core
	4	0.48	0	434.2	22.2	Shell
4.2	3	0.50	0	488.2	59.5	Core
	4	0.45	0	446.0	40.5	Shell

^a Sites 1 and 2 are associated with quadrupolar spectra (green and purple traces in Fig. 7). The reported parameters correspond to the average values of fitted quadrupole distributions. Sites 3 and 4 are associated with magnetic hyperfine spectra (blue and red traces in Fig. 7). The reported parameters correspond to the average values of fitted hyperfine field distributions. Estimated uncertainties: δ (± 0.02 mm s⁻¹), ΔE_q (± 0.04 mm s⁻¹), H_{hf} (± 2 kOe), area ($\pm 3\%$).

Here, τ_s is the spin relaxation time, τ_0 is an attempt time for spin reversal characteristic of the material, K_{eff} is the effective uniaxial magnetic anisotropy density of the particle, V is its volume, k_B is Boltzmann's constant, and T is the temperature in degrees Kelvin. Thus, theoretically, the blocking temperature of a nanoparticle ensemble relative to a measurement technique with characteristic measurement time τ_m is given by the Néel-Brown formula when $\tau_s = \tau_m$ (10^{-8} s for Mössbauer spectroscopy). In addition to Mössbauer many other techniques, of different characteristic measuring times, have been applied to the study of the superparamagnetic properties of ferritin, such as AC susceptibility³⁶ with $\tau_m = (1 \times 10^{-2} - 3 \times 10^{-4})$ s and SQUID magnetization measurements⁵⁹ with $\tau_m = (1-100)$ s. Using the value $\tau_0 = 10^{-11}$ s previously reported for ferritin³⁶ based on AC susceptibility measurements, we can use eqn (1) to estimate the effective magnetic anisotropy densities of the two heteropolymer iron cores.

$$K_{\text{eff}} = \frac{\ln(\tau_m/\tau_0)k_B T_B}{V} \quad (2)$$

Eqn (2) yields $K_{\text{eff}}(\text{L-rich}) = 2.75 \times 10^4$ J m⁻³ and $K_{\text{eff}}(\text{H-rich}) = 6.83 \times 10^4$ J m⁻³. The value of the magnetic anisotropy density of the H-rich heteropolymer ferritins is larger than that

of the L-rich heteropolymer. Considering the different contributions to K_{eff} ⁶⁰

$$K_{\text{eff}} = K_{\text{mc}} + K_s + K_{\text{sh}} + K_\sigma \quad (3)$$

where the first term (K_{mc}) is the magneto-crystalline anisotropy characteristic of the crystal lattice, the second term (K_s) arises from surface anisotropy due to crystalline structure and its symmetry breaking at the surface. The third term (K_{sh}) is due to shape anisotropy, which notably induces an easy axis along the long axis of an ellipsoid. The fourth term (K_σ) is due to lattice strain due to stress imposed by the support or ligands coordinated on the surface of the particle. K_s is most pronounced for particles whose diameters are smaller than 6 nm⁶¹ and should be more pronounced in the H-rich cores. K_{sh} is present only in the case of non-spherical particles and must contribute significantly to the H-rich cores, which possess a non-spherical morphology, with some of the cores appearing to have an effective acicularity as large as 1.9. The various contributions to the effective magnetic anisotropy may reinforce or oppose each other, making it difficult to calculate their individual contributions to K_{eff} . The different anchoring topology of the cores onto the cavity surface for the L-rich vs. the H-rich heteropolymers implies different values of K_σ for the two cases.



Assuming similar ferrihydrite phases within the cores, contributing similar magneto-crystalline anisotropies, the last three terms must be responsible for the difference in K_{eff} .

Conclusion

Nucleation and growth of magnetic nanoparticles by self-assembly within confined spaces of biological templates is a challenging area of research, but of great current interest due to the many applications in nanotechnology and biomedicine.^{24,42,62–64} In this study we have applied high resolution electron microscopy, electron energy-loss spectroscopy, and Mössbauer spectroscopy to better understand the process of iron biomineralization in two types of recombinant human heteropolymer ferritins (an H-rich and an L-rich), and to characterize the resulting micromagnetic properties of the iron biomineral cores. We observed that data obtained from the three techniques correlate in their findings. Our novel expression system will allow the synthesis of heteropolymer ferritin molecules of any H/L ratio, thus adding to the experimenter's tool kit an additional degree of freedom to probe iron biomineralization in ferritin. The study of these novel experimental systems promises to elucidate the structure–function relationships of different heteropolymer ferritins, which mimic those present in various tissues and organs. Our heteropolymer ferritin templates might be of great interest to nanomedicine and nanobiotechnology and allow researchers the ability to synthesize various metal and metal-oxide nanoparticles, with tailored morphology and magnetic anisotropy densities that dictate the superparamagnetic properties of such nano-systems.

Materials and methods

Ferritin expression and purification

Samples were prepared at the State University of New York, Potsdam, NY. The H-rich and L-rich recombinant human heteropolymer ferritins were produced in *E. coli* Rosetta-gami B strain using a recently engineered pWUR-FtH-TetO-FtL plasmid and different concentrations of inducers.¹⁵ Protein purification and quantification was performed according to established protocols using size exclusion chromatography (Akta Go, GE Healthcare), native and SDS-PAGE, and capillary gel electrophoresis (7100 model from Agilent Technologies).¹⁵ The concentration of protein was determined using the Micro BCA Protein Assay Kit (Thermo Scientific).

Ferritin reconstitution with ^{57}Fe

Ferritin reconstitution was performed at SUNY, Potsdam with 100% iron-57 enriched salts ($^{57}\text{FeSO}_4$). The $^{57}\text{FeSO}_4$ solution was prepared by dissolving 5.9 mg of ^{57}Fe metal (95.1 atom%; U.S. Service, Inc. Summit, NJ, USA) in 500 μL of 0.2 M H_2SO_4 over a period of 3 days, to produce a final solution of 0.207 M FeSO_4 , pH \sim 2.0. Three ^{57}Fe injections of 6.5 μL each (1.34 mM or \sim 335 Fe/shell), 20 min apart, were made to each ferritin sample (4 μM prepared in an aqueous buffer solution of 200 mM Mops, 50 mM NaCl, pH 7.2) to give a total of 1000 ^{57}Fe /

shell, equivalent to 0.228 mg of ^{57}Fe . The ferritin samples were then lyophilized (through freeze-drying) and analyzed by Mössbauer spectroscopy.

Electron microscopy

HAADF-STEM images at 0.63 nm resolution were obtained at the Singh Center for Nanotechnology at the University of Pennsylvania, Philadelphia, PA using an aberration corrected JEOL NEOARM instrument operating at 200 kV. Electron energy-loss spectroscopy (EELS) was performed with a K2 Summit camera provided by Gatan Inc. For STEM imaging, the camera length was 4 cm with a probe current of 150 pA. For EELS, the camera length was 2 cm, and the probe current was 500 pA.

Mössbauer spectroscopy

Mössbauer spectra on freeze-dried, reconstituted heteropolymer ferritins loaded with 1000 ^{57}Fe /protein were collected at Villanova University, Villanova, PA with a SEE Co constant acceleration spectrometer, calibrated with a 6 μm thin metal iron foil enriched in ^{57}Fe . All isomer shifts are referenced to metallic iron. Sample temperature variation from 4.2 to 300 K was achieved using a Janis Veri-Temp cryostat by Janis Research Co and a Lake Shore temperature controller. The radioactive source was ^{57}Co deposited in a Rh matrix (gamma@seeco.com.us). The source was maintained at room temperature. Spectral fits were performed using the WMOSS fitting software package commercially available from SEE Co, Edina, Minnesota.

Conflicts of interest

There are no conflicts to declare.

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