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Interaction mechanism between TiO₂ nanostructures and bovine leukemia virus proteins in photoluminescence-based immunosensors

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In this research a mechanism of interaction between a semiconducting TiO_2 layer and bovine leukemia virus protein gp51, applied in the design of photoluminescence-based immunosensors, is proposed and discussed. Protein gp51 was adsorbed on the surface of a nanostructured TiO_2 thin film, formed on glass substrates (TiO_2 /glass). A photoluminescence (PL) peak shift from 517 nm to 499 nm was observed after modification of the TiO_2 /glass by adsorbed gp51 ($gp51/TiO_2$ /glass). After incubation of the $gp51/TiO_2$ /glass in a solution containing anti-gp51, a new structure (anti- $gp51/gp51/TiO_2$ /glass) was formed and the PL peak shifted backwards from 499 nm to 516 nm. The above-mentioned PL shifts are attributed to the variations in the self-trapped exciton energy level, which were induced by the changes of electrostatic interaction between the adsorbed gp51 and the negatively charged TiO_2 surface. The strength of the electric field affecting the photoluminescence centers, was determined from variations between the PL-spectra of TiO_2 /glass, $gp51/TiO_2$ /glass and anti- $gp51/gp51/TiO_2$ /glass. The principle of how these electric field variations are induced has been predicted. The highlighted origin of the changes in the photoluminescence spectra of TiO_2 after its protein modification reveals an understanding of the interaction mechanism between TiO_2 and proteins that is the key issue responsible for biosensor performance.

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1. Introduction

Bovine leukemia is a lethal retroviral infection, which is induced by bovine leukemia virus (BLV). There is a significant risk that BLV can infect the other mammalians as in the case of other retroviruses' – such as, human immunodeficient virus (HIV). Therefore outbreaks of this infectious disease can significantly damage the ecosystem. For this reason the development of advanced bioanalytical systems for the determination of biomarkers of BLV-infection are required. Among many different immunosensors, the photoluminescence-based (PL) immunosensors seems to be the most promising for the improvement in diagnosis of virus induced diseases. In PL-immunosensors nanostructured ZnO or TiO₂ can be used as very efficient photoluminescence transducers. TiO₂ and its composites are extensively used as wide-band gap semiconductors with a unique combination of physical and chemical properties. The case of the provided significant properties.

A good biocompatibility of TiO_2 nanostructures, their applicability at physiological pHs in the range of \sim 5.5–7.0, non-

toxicity and excellent chemical stability have resulted in the extensive application of TiO_2 in electrochemical,⁸⁻¹⁰ electrical¹¹ and optical¹²⁻¹⁴ biosensors. Optical biosensors are increasingly studied class of biosensors because they allow to evaluate some inter-molecular interactions contactless¹⁵ and without any chemical/physical labels.³ The development of immunosensors, based on the optical detection methods, that can be applied for the determination of large variety of analytes in the complex biological samples^{7,12,14,15} is of great interest.

Nanostructured TiO₂ is known as a material of intense photoluminescence at room temperature. ^{16,17} The application of TiO₂ photoluminescence properties in optical biosensors and immunosensors have been reported in the range of works. The changes in the photoluminescence spectra (shift of PL-maximum and the variation of PL-signal intensity) were exploited as analytical signals for the determination of target analyte. ^{18,19} However the interaction mechanism of proteins with TiO₂ and the origin of the changes in the photoluminescence spectra were not discussed, although the mechanism of the interaction between semiconductor and proteins is the key in solving many of problems, which are still arising during the development of TiO₂-based immunosensors, such as an improvement of sensitivity and selectivity.^{3,13,14}

This work is aiming to highlight the origin of the changes in the photoluminescence spectra of TiO₂ resulted after the protein adsorption on its surface during the formation of biosensitive

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layer and after the interaction of biosensitive layer with the analyte. As it is proposed, the reason of the PL shifts observed after modification of TiO₂/glass by gp51 proteins is an electrostatic interaction between adsorbed gp51 and negatively charged TiO₂ surface. The strength of the electric field affecting photoluminescence centers, localized close to the surface of TiO₂/glass, is determined from variations of the PL-spectra of TiO₂/glass, gp51/TiO₂/glass and anti-gp51/gp51/TiO₂/glass. The principle of how these electric field variations are induced is discussed. The influence of several important parameters, including charge density of charged atoms/groups/domains in the specific binding biomolecules, effective coverage area by specific binding biomolecules and variation of the potential barrier are taken into account during the elaboration of the model.

Materials and methods 2.

2.1. Formation and characterization of TiO₂ samples

Nanostructured TiO₂ layers containing TiO₂ nanoparticles were formed on the glass substrates (TiO2/glass) by the deposition of colloidal suspension of TiO2 nanoparticles (Sigma Aldrich, 99.7%, particle size of 32 nm), dissolved in ethanol. Initial concentration of TiO₂ nanoparticles was about 0.01 mg ml⁻¹. The formed TiO₂/glass structures were dried at room temperature and then annealed at 350 °C. Structural and surface characterization of the obtained samples showed that in TiO2/glass structures the TiO2 kept the anatase structure and TiO2 nanoparticles formed a high surface area porous structure, which was suitable for the formation of biosensitive layer. More detailed description of deposition and characterization procedures, which were applied for the characterization of nanostructured TiO2/glass layers is reported in earlier our researches.18,19

Optical characterization of the nanostructured TiO2/glass layers was performed by photoluminescence measurements using 355 nm solid state laser as the excitation source. Optical setup is described in detail in previous our researches. 19,20 The PL-spectra were recorded in the range of wavelength from 360 to 800 nm.

Fabrication and evaluation of an immunosensor

The immobilization of biological molecules was carried out by incubation in a solution containing leukemia virus proteins gp51, similar to the immobilization procedure described in earlier works. 18-20 Briefly: a solution of PBS containing gp51 antigens at a high concentration was directly immobilized on the surface of TiO₂/glass structure. Then the sample was placed into a Petri plate for the incubation in a medium saturated with water vapor at 25 °C. After 10 min of incubation, the surface of the sample was washed with a PBS solution in order to remove not well adsorbed antigens from the surface of TiO₂/glass structure. As a result, a layered structure of gp51/ TiO₂/glass was formed, which got affinity and selectivity for the one type of bio-molecules - antibodies against leukemia proteins gp51 (anti-gp51). To prevent a nonspecific interaction (i.e., binding of anti-gp51 antibodies directly to unmodified

TiO2 surface), the surface of TiO2/glass was further treated with a solution of bovine serum albumin (BSA), which after the formation of gp51/BSA/TiO2/glass structure filled still freeremaining sites available for non-specific protein-adsorption standing. Thus it was expected that the selectivity of gp51/ BSA/TiO₂/glass structure has been improved in comparison to that of BSA-not modified gp51/TiO₂/glass structure.

3. Results and discussion

Interaction of gp51 proteins with TiO2 surface

Proteins consist of amino acids that might contain positively and/or negatively charged radicals that are determining the charge of different protein domains.21 A large quantity of negatively charged groups such as aldehyde (-CHO), hydroxyl (-OH), carboxyl (-COOH) and positively charged primary amine (-NH₂) and some other groups, which are involved into the structure of amino acids, are responsible for the partial (δ + and δ -) charges of particular protein domains. Therefore the proteins are characterized by electrostatic properties, and sometimes even significant electrostatic 'asymmetry of protein molecule' because the atoms and functional groups, which are forming the protein molecules are charged differently both in charge sign and in absolute charge value. Naturally, the charges in proteins at least partly are compensating each other, but the ternary structure of proteins is relatively rigid and the charged groups have only limited degree of freedom to move within the protein globule. Therefore, in some parts of the protein some uncompensated charge on the surface and inside of the protein still remains.21 The distribution of charged groups on the surface of the protein depends on the sequence of amino acids, which is pre-determined by the genome that was developed during millions or even billions of years lasting evolution of each protein. During the evolution, the genes which are promoting the synthesis of proteins whose structure the most efficiently matches their function, were selected for further generations.

It should be taken into account that even if the structure of the most proteins is at some extent 'rigid' there is still some degree of flexibility because proteins in their polymeric structure contains a high number of σ-bonds, around which the rotation of protein-building segments is possible. Moreover, both secondary and tertiary structures of the protein are supported by a large number of hydrogen bonds but many of them are not very strong, therefore this factor adds additional degree of freedom for protein structure.22 The electrostatic interactions, which are based on Coulomb forces between the opposite charges, van der Waals forces and disulfide bonds also play an important role in the formation of both secondary and tertiary structures of protein, but they can be relatively easily disrupted by electrostatic-neutralization and/or displacement of some charged groups/domains, which are forming proteins.

TiO₂ (in its allotropic form of anatase) is a semiconductor of n-type conductivity, usually with an 'upward' band bending of the energy levels when closing the surface of TiO₂ (Fig. 1),^{4,6} which indicates the accumulation of a negative charge (bound at surface levels) on its surface. 6,23 The adsorption of the most of

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molecules is known to introduce an additional charge on the solid state surface and it can change the existing surface energy levels or form the additional ones that are involved in the exchange of charges with the volume of a solid material. It should be taken into account, that in the open air, the oxygen adsorbates (O_{ads}^-) formed on the surface of TiO_2 are resulting in an electron delocalization towards adsorbed oxygen what reduces the conductivity of TiO_2 layer. This process is similar to that, which is well described for $ZnO.^{25}$

Further analysis of the interaction between TiO_2/g lass and gp51 proteins is based on the evaluation of photoluminescence of TiO_2 nanoparticles. The protein gp51 is specifically binding with antibodies against gp51 (anti-gp51) *i.e.* the target-analyte. The photoluminescence properties of the TiO_2 nanoparticles have been previously investigated in some research papers. Moreover, optical effects, which are registered during gp51 protein adsorption on TiO_2/g lass, also where observed and even applied in the development of photoluminescence based immunosensor for the determination of gp51 antibodies. However in these publications no attention was paid to the nature of interaction between protein gp51 and semiconductor TiO_2 and for the prediction of the mechanism of PL-based signal generation.

In a present research the success of immobilization of *gp*51 and the formation of *gp*51/TiO₂/glass structure was similar to that reported in earlier our works.^{19,20} The immobilization of *gp*51 proteins on TiO₂/glass leads to an increase in the intensity of the photoluminescence signal of TiO₂/glass nanostructures and a UV-shift in the position of the maximum of the photoluminescence spectra (Fig. 2a).¹⁹ The application of BSA, which were used to block the free adsorption centers on the TiO₂/glass surface, also leads to a slight increase in the photoluminescence intensity, but the spectrum shift was not observed.

Interaction between $gp51/\text{TiO}_2/g$ lass and anti-gp51 leads to the inverse changes in the photoluminescence spectrum (Fig. 2b), *i.e.* a decrease in the integral intensity of the photoluminescence and the IR-shift of spectra. Therefore, the response of the immunosensor $gp51/\text{TiO}_2/g$ lass to anti-gp51 can be estimated by two parameters: (i) the photoluminescence intensity and (ii) the position of the PL-maximum. The sensitivity of $gp51/\text{TiO}_2/g$ lass based immunosensor towards anti-gp51 was in the range of 2–8 μ g ml⁻¹.19

3.2. Mechanism of interaction between $TiO_2/glass$ and gp51 proteins

A gp51 protein molecule has a molecular mass of 51 kDa. The characteristic geometric size of the gp51 molecules that are adsorbed on the TiO_2 surface is about 6 nm in diameter. The authors, which have published a research on the formation of gp51 protein-based capsid of BLV, have constructed an image of the structure of the gp51 protein from the X-ray crystallography data and they have reported that this protein is extra-flexible, which provides very high functionality and the ability to associate and/or dissociate of mainly on gp51 protein based the capsid of BLV to/from the membrane of BLV infected cell. Therefore, it is expected that on the surface of TiO_2 gp51 protein also forms a well-ordered monolayer. The formation of such layer was confirmed in previous our researches based on the application of spectroscopic ellipsometry.

The gp51 is not a redox-protein therefore the charge transfer between gp51 and TiO_2/g lass is not possible.³⁰ But the gp51 protein, like many other proteins, contains a number of partially charged groups and domains, which in Fig. 3 and 4, are represented as partial charges " δ –" and " δ +". These charges per charged atom or group are mostly lower in value than the total single-electron charge (1.6×10^{-19} coulombs). The presence of

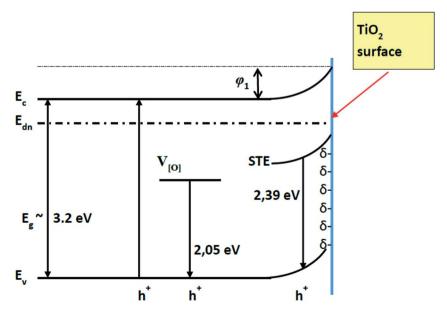


Fig. 1 Energetic levels of pristine TiO_2 (TiO_2 /glass structure). E_c , E_v – conduction and valence band of TiO_2 respectively. E_{dn} – electron demarcation level.

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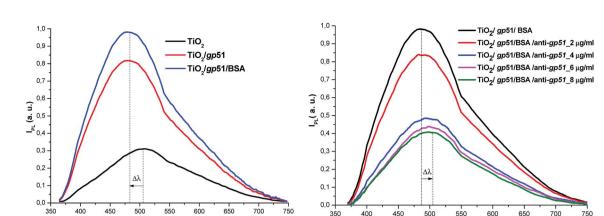


Fig. 2 Photoluminescence spectra of TiO_2 /glass nanoparticles: (a) before and after the immobilization of gp51 on the TiO_2 /glass surface and after BSA deposition; (b) photoluminescence spectra of $gp51/TiO_2$ /glass based immunosensor after the interaction with analyte (anti-gp51), which is present in the aliquots at different concentrations.

these partial charges suggests that the electrostatic influence of gp51 protein on the surface charge of TiO_2/g lass is coming from the side of partially uncompensated charges, which are localized in those parts of the gp51 protein that are located in close proximity to the surface of TiO_2/g lass and are mainly responsible for the adsorption of this protein on the TiO_2/g lass surface. The electrostatic Coulomb interaction, which takes place between charged groups in the gp51 protein and the negatively charged surface of the TiO_2/g lass, are the most strong at a distances ranging from several angstroms to few nanometers. Therefore, among the other interactions such as hydrogen bonds, disulfide bonds, van der Waals interaction, etc., which all also have significant role during the adsorption of proteins,

a)

the electrostatic interaction plays one of the most significant role during the adsorption of proteins onto electrically charged surfaces, such as ${\rm TiO_2}$. In addition, the local electric fields of charged domains of adsorbed proteins are electrostatically affecting the PL-centers of ${\rm TiO_2/glass}$ and it causes the shift in the photoluminescence spectra of ${\rm TiO_2}$ nanoparticles. Therefore, the photoluminescence maximum of $gp51/{\rm TiO_2/glass}$, which is mainly caused by self-trapped excitons (STE), shifts from 517 to 499 nm (*i.e.*, to 18 nm), which corresponds to ~ 0.086 eV that is less than 0.1 eV, and it is one of the proofs of electrostatic interaction based physical adsorption of $gp51.^{24}$

b)

The splitting of the photoluminescence spectra into Gaussian curves at each stage of the experiment shows that after

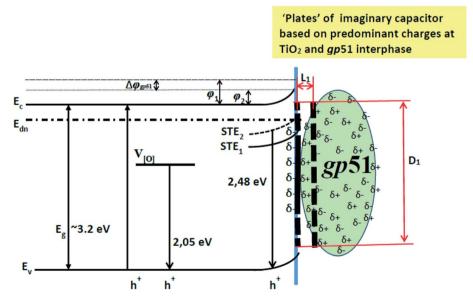


Fig. 3 Energetic levels and the model based on 'imaginary flat capacitor', which represents averaged interaction between charges in $gp51/\text{TiO}_2/$ glass structure: L_1 – 'relative distance' between 'plates' area of imaginary capacitor, D_2 – diameter of imaginary capacitor, which is determined by surface area of gp51 and can be used for the calculation of relative surface area of imaginary capacitor; φ_1 – potential barrier value for surface of TiO_2 interphase with air (air// TiO_2 /glass); φ_2 – potential barrier value for $gp51/TiO_2$ structure at interphase with air (air// $gp51/TiO_2$ /glass); $\Delta \varphi_{gp51}$ – difference of potential barriers between air// TiO_2 /glass and (air// $gp51/TiO_2$ /glass) caused by immobilization of gp51.

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 $V_{[O]} = \frac{\Delta \varphi_{\text{anti-}gp51/gp51}}{\nabla V_{[O]}} = \frac{\nabla V_{[O]}}{\nabla V_{$

Fig. 4 Energetic levels and the model based on 'imaginary flat capacitor', which represents averaged interaction between charges in anti-gp51/ $gp51/TiO_2$ /glass structure: L_2 – 'relative distance' between 'plates' area of imaginary capacitor, D_2 – diameter of imaginary capacitor, which is determined by surface area of gp51 and can be used for the calculation of relative surface area of imaginary capacitor, φ_3 – potential barrier value for anti- $gp51/gp51/TiO_2$ /glass structure at interphase with air (air//anti- $gp51/gp51/TiO_2$ /glass). $\Delta \varphi_{anti-gp51/gp51}$ – difference of potential barriers between air//TiO₂/glass and air//anti- $gp51/gp51/TiO_2$ /glass.

the adsorption of gp51 protein molecules on the TiO2 surface the energy value of excitation levels, which are responsible for the luminescence and associated with oxygen vacancies $I_{V[O]}$, almost does not change remaining at a value of 605 \pm 2 nm. At the same time, the photoluminescence maximum caused by the recombination of STE31-33 shifts to short wavelengths, changing its position from 517 ($I_{\text{STE1}} = 2.39 \text{ eV}$) nm to 499 nm ($I_{\text{STE2}} =$ 2.48 eV). Since the involvement of the STE level in the process of radiative recombination is regulated by the surface, this indicates that STE level is located either on the surface plane or not very deeply within the surface layer of the TiO2. The displacement of the light emitting recombination peak indicates that the energy level of STE is complex and has its 'basic' and 'excited' states.31-33 The appearance of luminescence in the region of 499 nm indicates a radiative transition from the excited STE level. This indicates that the charge at the TiO₂/gp51 boundary controls the energy level of the STE and shows that the electronic demarcation level practically coincides with the position of the STE level, i.e. is approximately 2.39 eV above the valence band. Therefore, the appearance of proteins on the TiO₂ surface leads to a shift in the energy levels, including energy levels of the light emitting centers, relatively to the electron demarcation level $E_{\rm dn}$.

The blue-shift of the photoluminescence maximum by 18 nm as a result of adsorption of the gp51 protein, which corresponds to $\Delta E_{\rm STE} = {\rm STE}_2 - {\rm STE}_1 = 0.086$ eV, also indicates that the initial value of the potential barrier (φ_1) on the ${\rm TiO}_2$ / glass surface has decreased by a value of 0.086 eV to φ_2 . Variation of the potential barrier means that the value of negative charge localized on the ${\rm TiO}_2$ /glass surface has also changed, due to the charge-charge-based interaction with adsorbed

protein gp51. Positively charged atoms and groups, which are provided by the gp51 protein, partially compensates the surface charge of TiO2/glass and reduces the energy of electrons localized at the surface levels, which are the most responsible for the generation of PL-signal. Taking into account the fact that the total negative charge predominates on the TiO2/glass surface, the positively charged parts of the gp51 protein electrostatically interact with the negatively charged TiO2/glass surface. As a result, a partial decrease of the surface charge reduces the electric field in the TiO₂/glass surface region. Further interaction of gp51/TiO2/glass structure with analyte - anti-gp51, which is also a protein, leads to the inverse changes in the photoluminescence spectra, i.e., to UV-shift of the spectrum and decrease the photoluminescence intensity to the value that corresponds to the pure TiO₂/glass. The latter effect is based on the formation of an immune complex between immobilized antigens gp51 and anti-gp51 antibodies, which are present in aliquot. The formation of this immune complex besides the van der Waals interaction and other interactions at a very high extent is based on the interaction between oppositely charged domains, functional groups and atoms in gp51 and anti-gp51 molecules (including the formation of number of hydrogen bounds, which can be estimated as specific kind of electrostatic interaction). It can be assumed that uncompensated charges (δ + and δ) of both proteins (gp51 and anti-gp51) are involved in electrostatic interactions during the formation of immune complex. As a result, some of the charged groups of protein gp51 that were originally involved in the interaction between gp51 and TiO2/glass are at least partially compensated by the opposite charge of the anti-gp51 protein groups, thereby reducing the direct electrostatic effect from immobilized gp51 proteins to the charged surface of ${\rm TiO_2}$ and at the same time to PL-light emitting centers.

The effects described above have an effect on the shift of PL-maximum and on the decrease in the potential barrier on $gp51/TiO_2/glass$ interface due to the charge–charge interaction between $TiO_2/glass$ and gp51. The potential barrier at the interface between $TiO_2/glass$ and gp51 has a greater value in $gp51/TiO_2/glass$ structure in comparison with that in anti- $gp51/gp51/TiO_2/glass$ due to partial compensation (decrease in value) and/or delocalization of gp51 charges, which were initially involved into interaction between $TiO_2/glass$ and gp51 after formation of $gp51/TiO_2/glass$ structure.

The changes in the PL intensity from TiO_2 after the protein adsorption can be caused by following reasons. An increase of the PL intensity after immobilization of gp51 proteins on the TiO_2 /glass surface could result from the fact that the oxygen, adsorbed on the surface of TiO_2 , forms a re-oxidized layer that is reduced by the atoms and groups in gp51 proteins. A decrease of the PL intensity after the interaction of biosensitive layer with the target analyte can be caused by both additional dispersion of light from the excitation source and exited PL signal generated from anti-gp51/gp51/ TiO_2 /glass structure.

The distribution of charges in $gp51/\text{TiO}_2/\text{glass}$ structure can also be interpreted as a model based on an 'imaginary capacitor' (Fig. 3), formed as a result of the electrostatic interaction between oppositely charged protein gp51 layer and the $\text{TiO}_2/\text{glass}$ surface. The 'imaginary capacitor' is formed as a result of protein gp51 adsorption on $\text{TiO}_2/\text{glass}$ surface, after which the charges are distributed in energetically most favorable way, partially compensating each other. Consequently, the positive 'imaginary capacitor plate' is based on the positive charges, which are predominant in the protein gp51 surface area that after adsorption appears in close proximity to $gp51/\text{TiO}_2/\text{glass}$ interface and/or due to the negative electrostatic effect of $\text{TiO}_2/\text{glass}$ are induced/attracted closer to negatively charged $\text{TiO}_2/\text{glass}$ surface.

Charged atoms/groups/domains of gp51 that are localized in the close proximity to the TiO_2 /glass surface and they electrostatically affect the TiO_2 emission centers and the energy value of the surface potential barrier. Thus the position of the energy levels of the TiO_2 /glass emission maximum depends on TiO_2 surface modification stage (TiO_2 /glass or $gp51/TiO_2$ /glass) shifts from/backwards the initial position of the demarcation level. Fig. 3 represents an imaginary capacitor consisting of a negatively charged plate on the surface of TiO_2 /glass and an 'imaginary positively charged plate' formed in gp51 protein in close proximity to $gp51/TiO_2$ /glass interphase.

Hence, the interaction of $gp51/\text{TiO}_2/g$ lass with anti-gp51 antibodies and the formation of gp51/anti-gp51-based immune complex leads to a 'deformation' and the reduction of charge 'stored' on 'the positive imaginary capacitor plate' (Fig. 4). This is mainly due to the redistribution and partial compensation of charges during the formation of the gp51/anti-gp51 immune complex, which in turn reduces the charge of 'the imaginary capacitor plate' based on gp51 ($q_2 < q_1$). This reduced charge can be interpreted as the reduction of the area of the same plate (S_2) and/or the increase of the distance (S_2) between the two

imaginary capacitor plates based on gp51 and $TiO_2/glass$. This effect is observed because some of the gp51 protein charges move from the $gp51/TiO_2/glass$ interface towards interacting anti-gp51 protein and are partially compensated by charge present in anti-gp51, whereby the imaginary positive gp51-based capacitor plate of the capacitor is reduced in imaginary surface area and/or correspondingly moving apart from the negative $TiO_2/glass$ plate. This effect leads to a decrease in the capacitance of this imaginary capacitor and the electric field induced by gp51 becomes reduced. Therefore, after the interaction of $gp51/TiO_2/glass$ with anti-gp51 antibodies and the formation of gp51/anti-gp51 complex, which is involved into anti- $gp51/gp51/TiO_2/glass$ structure, the electrostatic effect of gp51 initially adsorbed on $TiO_2/glass$ towards the TiO_2 surface significantly decreases.

It should be taken into account that after the adsorption of gp51 proteins, the oppositely charged domains build up within a surface layers of both adsorbed-gp51 and TiO₂/glass within the Debye-screening length of both materials. These oppositely charged electric layers forms a double-layered structure with obvious electric capacitance that is dependent on (i) the concentration of charged atoms/groups/domains, (ii) distance of these features from each other and dielectric constant (relative permittivity) of gp51 and space in between adsorbed gp51 and TiO2/glass. Any charge that is emerging within the Debyescreening length on the surfaces of both adsorbed-gp51 and TiO₂/glass is affecting the capacitance of this imaginary capacitor. The variation of both (i) the number and (ii) the localization of charged parts depends on so called 'Debye-screening length' towards all directions of structures and influences the strength of electric field in gp51/TiO₂/glass and anti-gp51/gp51/ TiO₂/glass structures. The relationships among the value of the Debye-screening length (L_D) and the concentration of charged atoms/groups/domains of gp51 are provided in eqn (1) and/or (2):

$$L_{\rm D} = \sqrt{\frac{\varepsilon \varepsilon_0 kT}{2ne^2}} \tag{1}$$

where: ε_0 is the permittivity (dielectric constant of vacuum) in vacuum, ε is the permittivity (dielectric constant) of the TiO_2 (or the relative permittivity of gp51 protein if Debye-screening length is calculated for gp51 protein), T is the absolute temperature (in kelvin), n is the concentration of the electrons, e is the electron charge.

$$k^{-1} = \sqrt{\frac{\varepsilon \varepsilon_{\rm r} k_{\rm B} T}{2N_{\rm A} e^2 I}} \tag{2}$$

where: I is the concentration of charged atoms/groups/domains of the gp51 protein (mol m $^{-3}$), $k_{\rm B}$ is the Boltzmann constant, T is the absolute temperature (in kelvin), $\varepsilon_{\rm r}$ is the relative permittivity of gp51 protein, $N_{\rm A}$ is the Avogadro number, e is the 'averaged elementary charge of electron' and k is the Debye–Hückel screening length in TiO $_2$ or in gp51 protein, which is strongly dependent on the concentration ($N_{\rm d}$) of charged 'defects' in TiO $_2$ or atoms/groups/domains or in gp51 protein, respectively. In this context it should be noted that if Debye-

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screening length is calculated for gp51 protein then 'averaged elementary charge' can vary between elementary charge of electron 1.6×10^{-19} Cb and 0 due to variety of possible δ + and δ -, which are appearing within protein globule. It should be also noted that the exact concentrations of charged atoms or impurities, which is relatively easily calculated for TiO₂, but it is no case for proteins such as gp51 where exact number of charged atoms/groups/domains is not always known and can vary dependably on conformation of protein. Therefore this value should be calculated from the combination of other measurements such as electrochemical impedance spectroscopy,³⁴ etc.

Debye-screening length for TiO₂, calculated according to the eqn (1), while applying such values ε – permittivity in TiO₂ (ε = 34), 35 ε_0 – dielectric constant (8.85 × 10⁻¹² F m⁻¹), n – concentration of electrons in TiO₂ (n = 10¹⁹ sm⁻³), e – electron charge (1.6 × 10⁻¹⁹ Cb), k – Boltzmann's constant (1.38 × 10⁻²³ J K⁻¹) and T – absolute temperature (293 K) was estimated to be 15 nm. The estimated value of $L_{\rm D}$ shows that within this distance from TiO₂ surface the PL-centres are affected by electrostatic effects from adsorbed proteins gp51 and anti-gp51/gp51.

The measured PL-peak values determine how the concentration and distribution of charged atoms/groups/domains charge density affect the ${\rm TiO_2}$ surface potential and potential of energetic levels within Debye-screening length, which can be determined using eqn (1) and (2). This effect is similar to that observed on field effect transistors. The sensitivity of ${\rm TiO_2}$ -based PL immunosensor is also influenced by the concentration and distribution of charged atoms/groups/domains (Debye-screening length) in protein gp51 or gp51/anti-gp51-based immune-complex.

4. Conclusions

The main aspects of the interaction mechanism between nanostructured TiO2/glass layer and bovine leukemia virus proteins gp51, during the formation of PL-based immunosensor, have been outlined. Bovine leukemia virus protein gp51, which was adsorbed on the surface of nanostructured TiO₂/ glass thin film, formed the biosensitive layer (gp51/TiO₂/glass) that resulted in the TiO₂ PL peak shift from 517 nm to 499 nm. The interaction gp51/TiO2/glass structure with specific antibodies against gp51 (anti-gp51) has shifted the PL peak backwards from 499 nm to 516 nm. These PL shifts are attributed to the variation of STE energy level, which was induced by changes of electrostatic interaction between adsorbed gp51 and negatively charged TiO₂/glass surface. The displacement of the light emitting recombination peak confirms that the energy of STE level is complex and has its ground and excited states. The blueshift of the photoluminescence maximum by 18 nm as a result of adsorption of the *gp*51 protein, which corresponds to $\Delta E_{\text{STE}} =$ $I_{\rm STE2} - I_{\rm STE1} = 0.086$ eV, indicates that the initial value of the potential barrier on the TiO2/glass surface has decreased by 0.086 eV. The variation of the potential barrier means that the value of negative charge localized on the TiO2/glass surface has changed due to the charge-charge-based interaction with adsorbed protein gp51. Positively charged atoms and groups, provided by the gp51 protein, partially compensate the surface charge of TiO_2 and reduce the energy of electrons localized at the surface levels, which are the most responsible for the generation of PL-signal.

The charge-charge-based interaction in the double charged layers gp51/TiO₂/glass can also be interpreted as a model based on 'imaginary capacitor', formed as a result of the electrostatic interaction between oppositely charged protein gp51 layer and the TiO2/glass surface. The positive charges of protein gp51, attracted to the negatively charged surface, form the positive 'imaginary capacitor plate' in the close proximity to gp51/TiO2/ glass interface. The interaction of gp51/TiO₂/glass with antigp51 antibodies and formation of gp51/anti-gp51-based immune complex leads to a deformation and reduction of charge in 'the positive imaginary capacitor plate', caused by redistribution and partial compensation of charges during the formation of the gp51/anti-gp51 immune complex. Debyescreening length, calculated for TiO2, is in the range of 15 nm, which shows that PL-centres within this distance can be electrostatically affected by adsorbed gp51 and anti-gp51/gp51 complex.

The highlighted origin of the changes in the photoluminescence spectra of ${\rm TiO_2}$ as a result of the formation of biosensitive layer and after its interaction with the analyte, bring us closer to an understanding of the interaction mechanism between ${\rm TiO_2}$ and proteins, that is the key in the solving of many issues related to an improvement of biosensor performance.

In our next work we are going to investigate more in detail some parts of here predicted interaction mechanism using other proteins adsorbed on the surface of TiO₂/glass.

Conflicts of interest

There are no conflicts to declare.

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